

Fluorescent nuclear track detectors as a tool for ion- beam therapy research

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dkfz.

GERMAN
CANCER RESEARCH CENTER
IN THE HELMHOLTZ ASSOCIATION



50 Years – Research for
A Life Without Cancer

Photons or charged particles?

Conventional radiotherapy



- *cost:* € 3 million
- *space:* 500 m³
- *staff:* 3 employees

Particle therapy

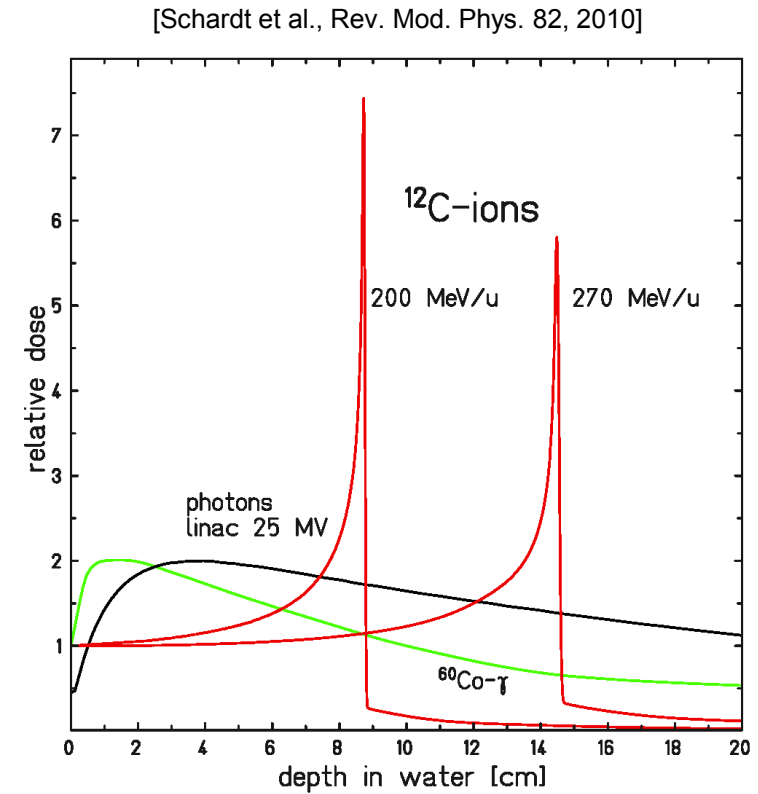


- *cost:* € 120 million
- *space:* 50,000 m³
- *staff:* 40 employees



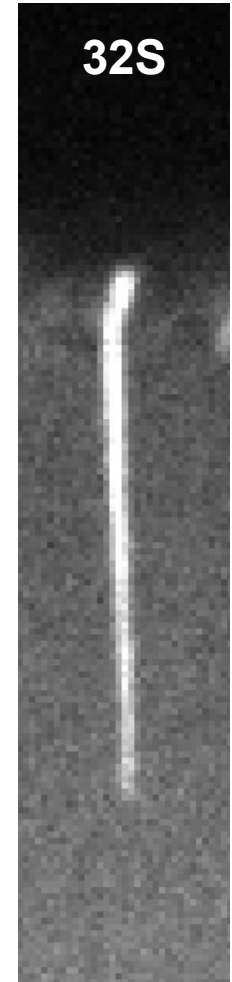
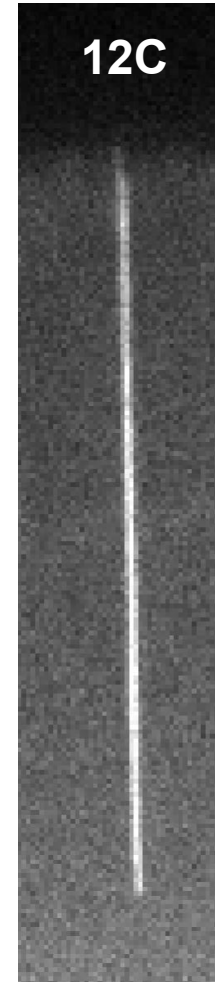
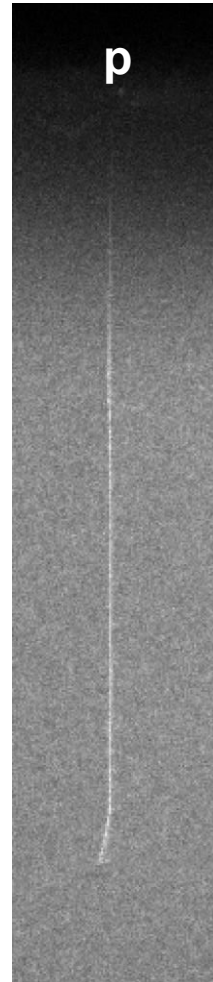
Main characteristics

- inverse depth-dose profile (Bragg peak)



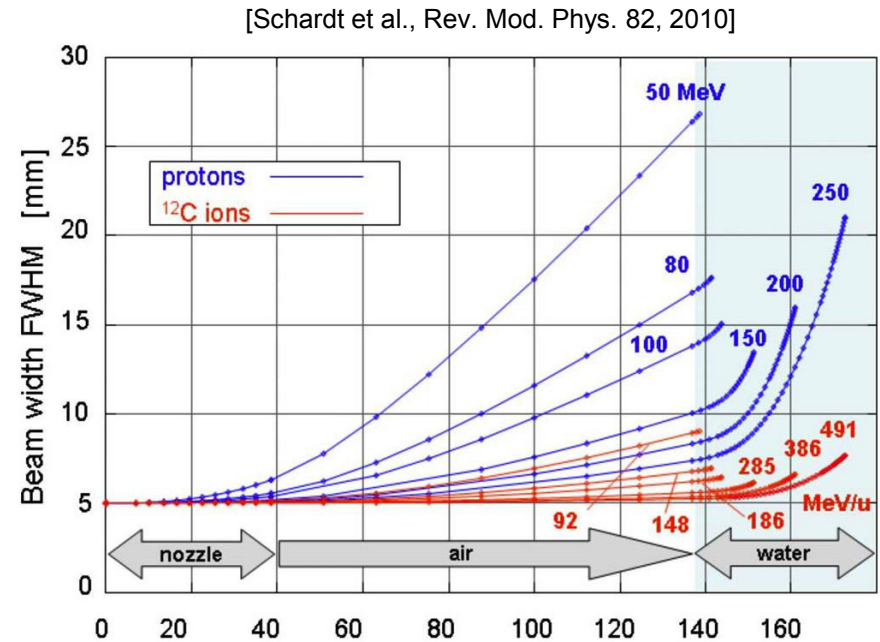
Main characteristics

- inverse depth-dose profile (Bragg peak)
- high ionization density (LET)



Main characteristics

- inverse depth-dose profile (Bragg peak)
- high ionization density (LET)
- reduced lateral scattering



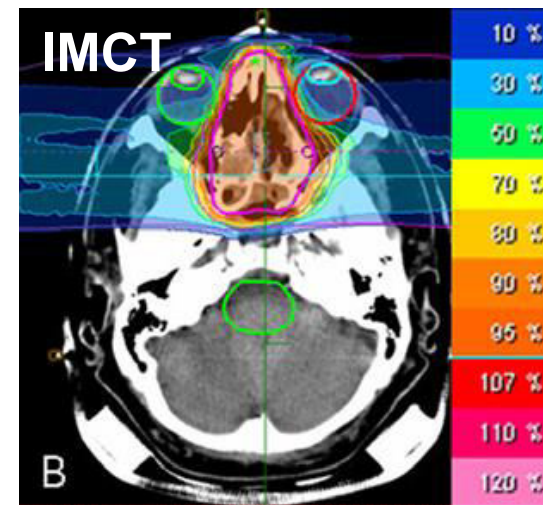
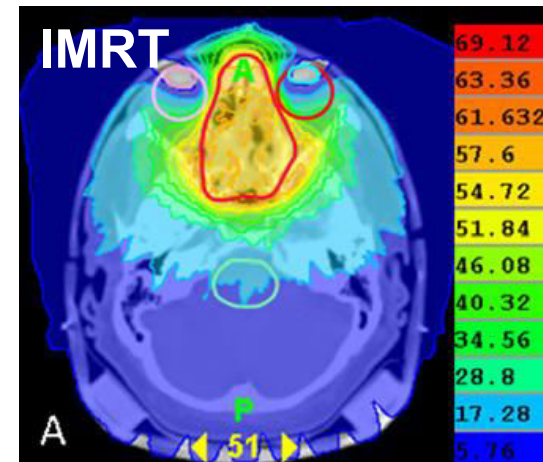
Main characteristics

- inverse depth-dose profile (Bragg peak)
- high ionization density (LET)
- reduced lateral scattering

Consequences

- superior dose conformity

[Kosaki et al., Radiat. Oncol. 7, 2012]

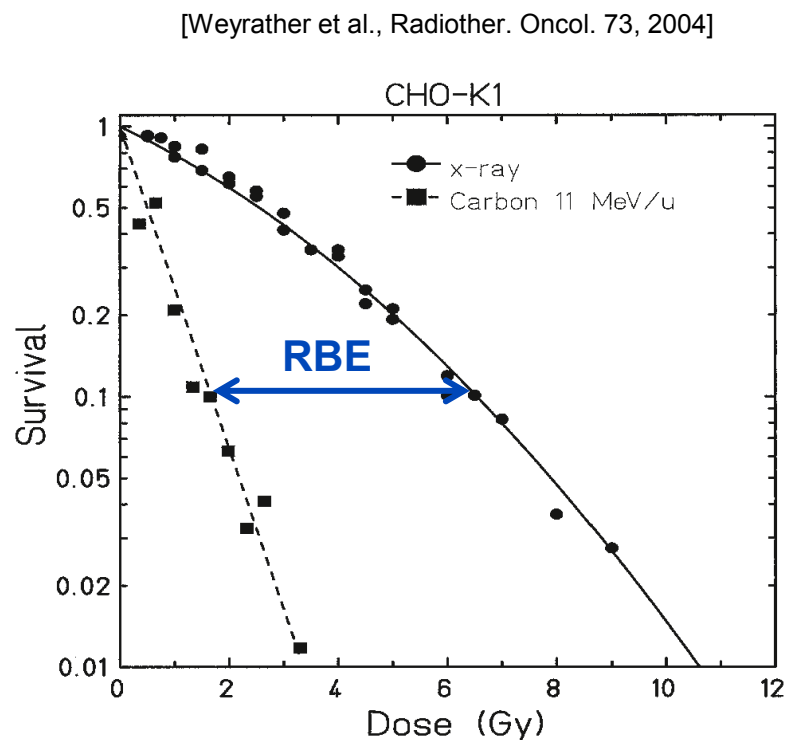


Main characteristics

- inverse depth-dose profile (Bragg peak)
- high ionization density (LET)
- reduced lateral scattering

Consequences

- superior dose conformity
- enhanced relative biological effectiveness (RBE)



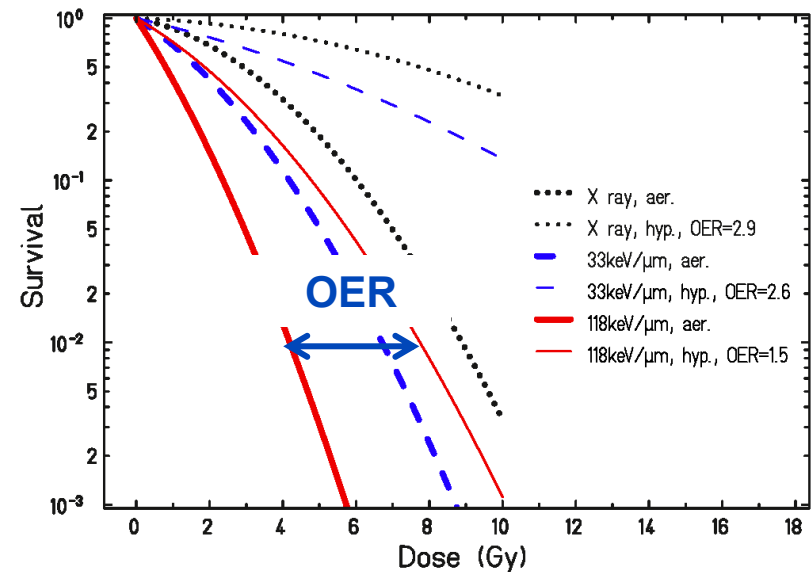
Main characteristics

- inverse depth-dose profile (Bragg peak)
- high ionization density (LET)
- reduced lateral scattering

Consequences

- superior dose conformity
- enhanced relative biological effectiveness (RBE)
- reduced oxygen enhancement ratio (OER)

[data: Blakely et al., Radiat. Res. 80, 1979]
[plot: Schardt et al., Rev. Mod. Phys. 82, 2010]



Main characteristics

- inverse depth-dose profile (Bragg peak)
- high ionization density (LET)
- reduced lateral scattering

Consequences

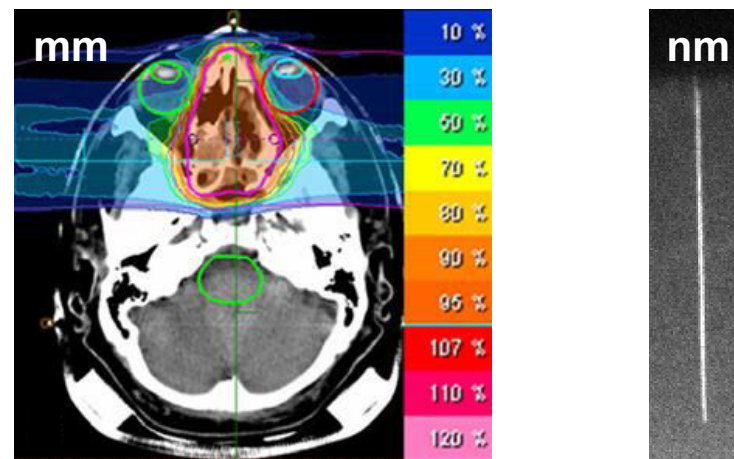
- superior dose conformity
- enhanced relative biological effectiveness (RBE)
- reduced oxygen enhancement ratio (OER)

Expected clinical benefits

- sparing of critical structures
- higher local control for
 - (a) radioresistant, slow-growing tumors
 - (b) hypoxic tumors

Main characteristics

- inverse depth-dose profile (Bragg peak)
- high ionization density (LET)
- reduced lateral scattering



Large dose gradients on mm and nm scale

Ion-beam therapy research requires
detectors that function on both scales.

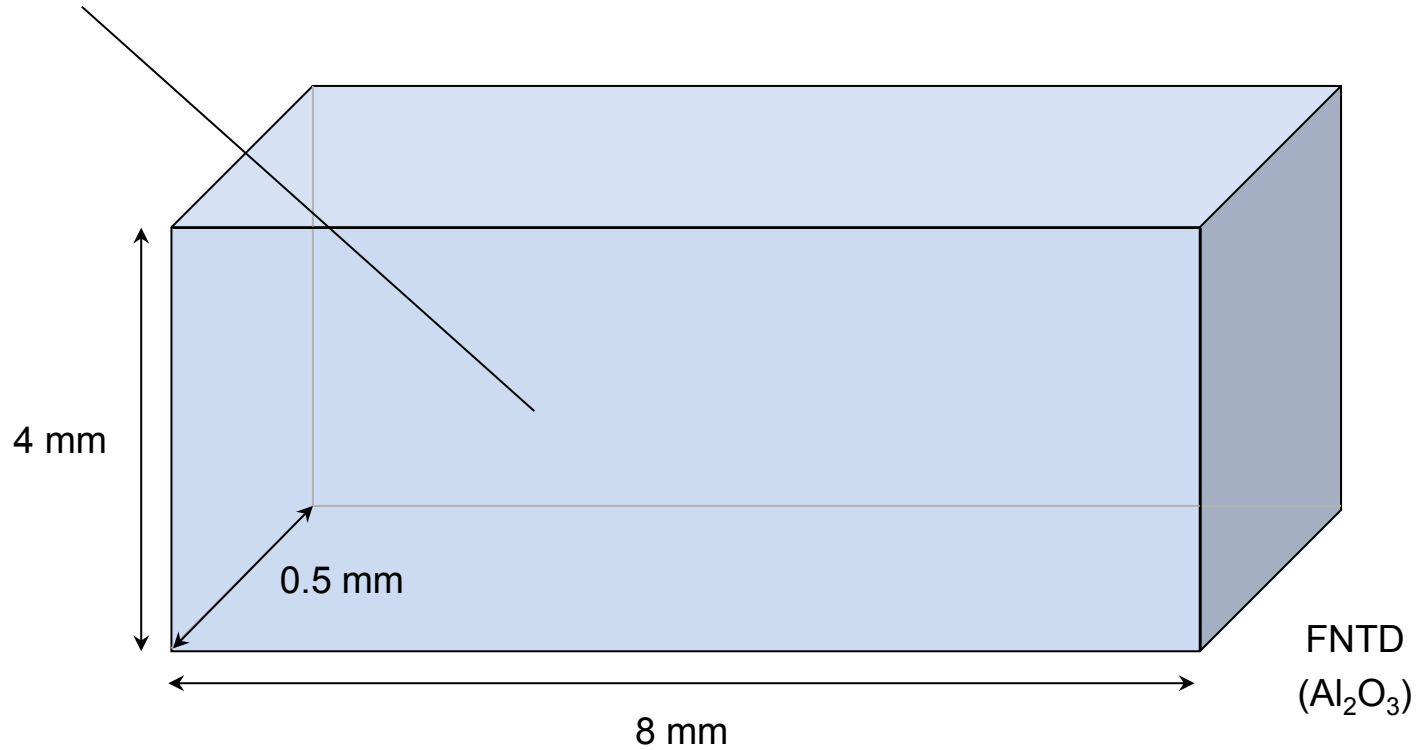
A vertical black line is positioned to the left of the text.

INTRODUCTION

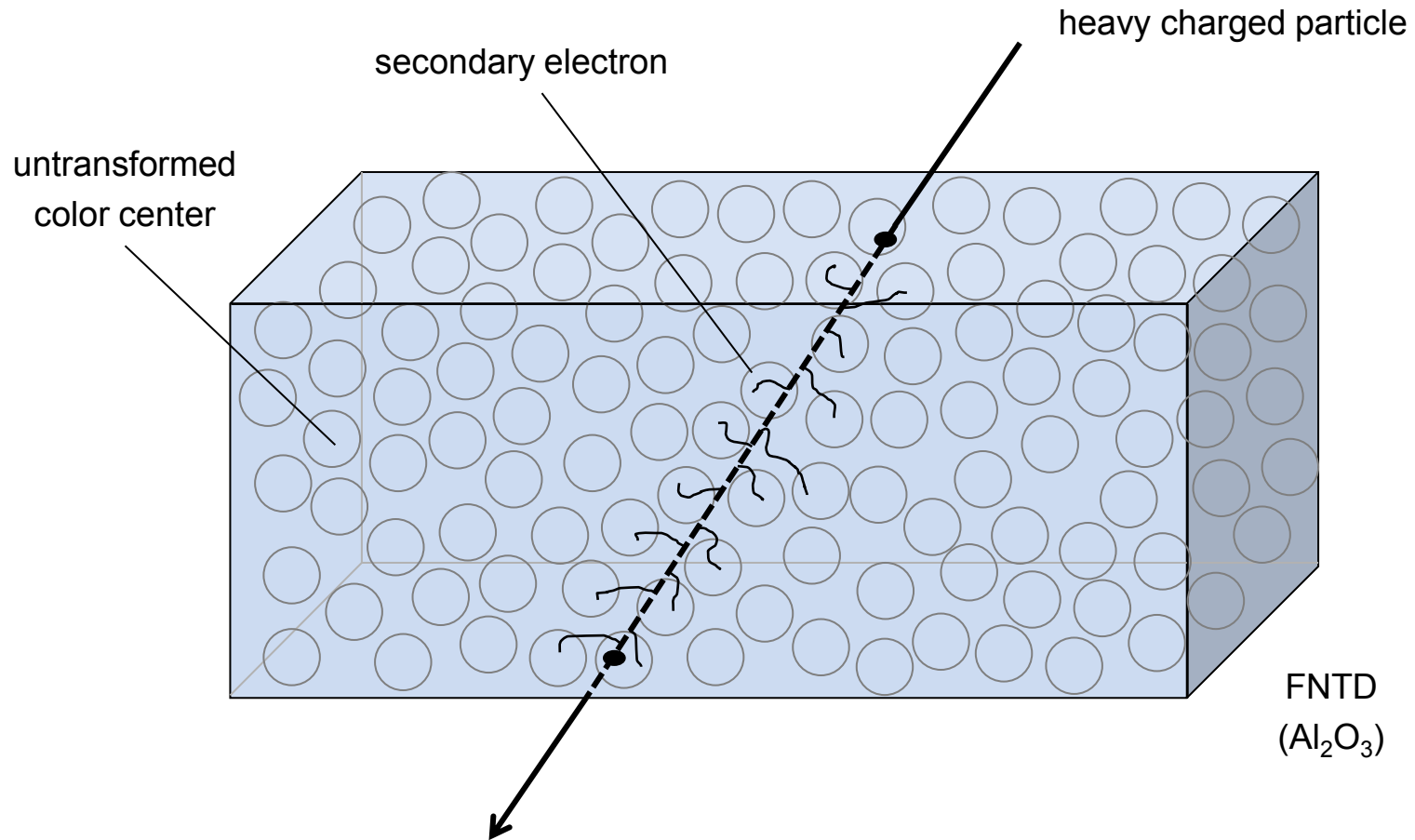
Detector principle

FNTD technology

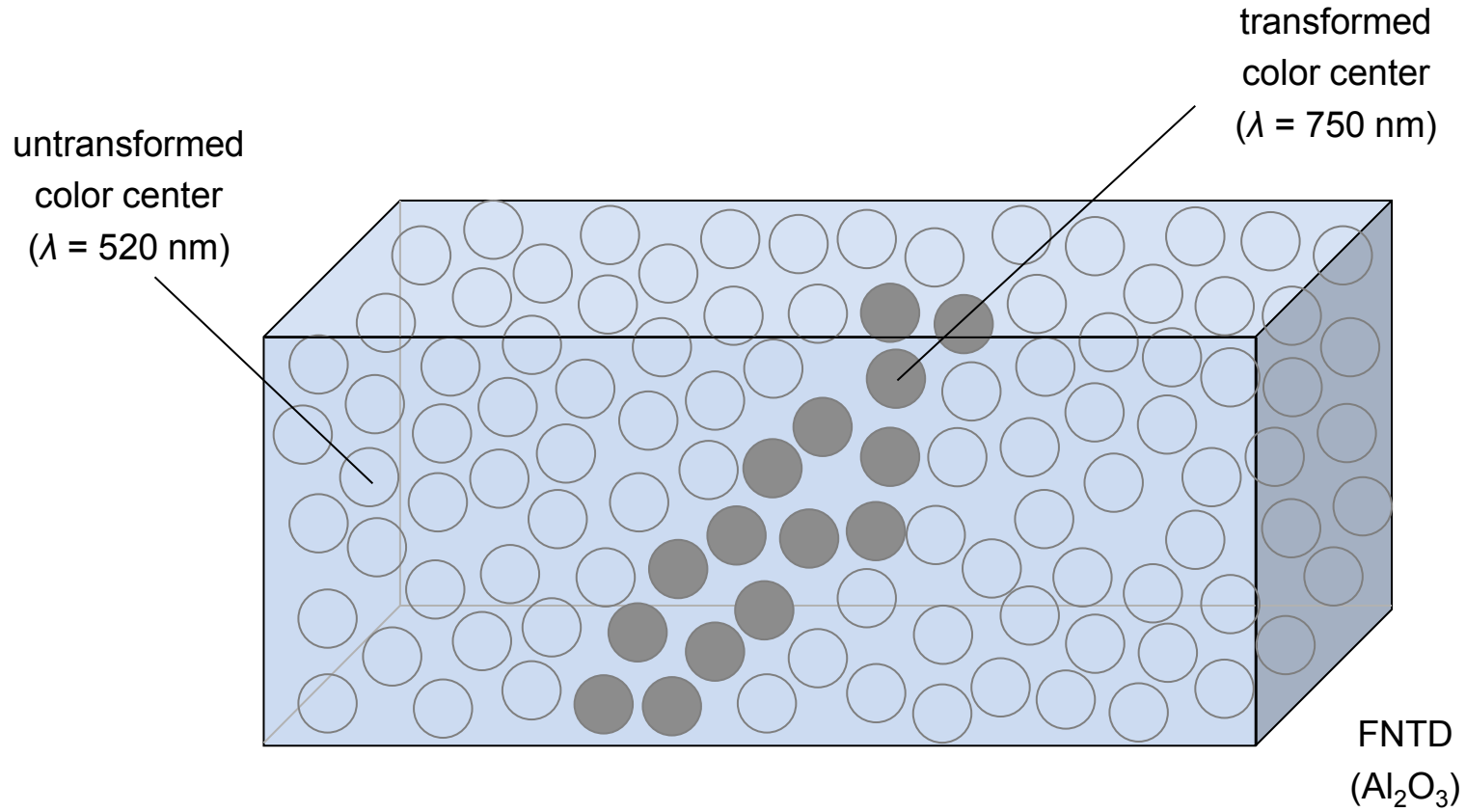
developed and produced by
Landauer Inc., Stillwater (OK), USA



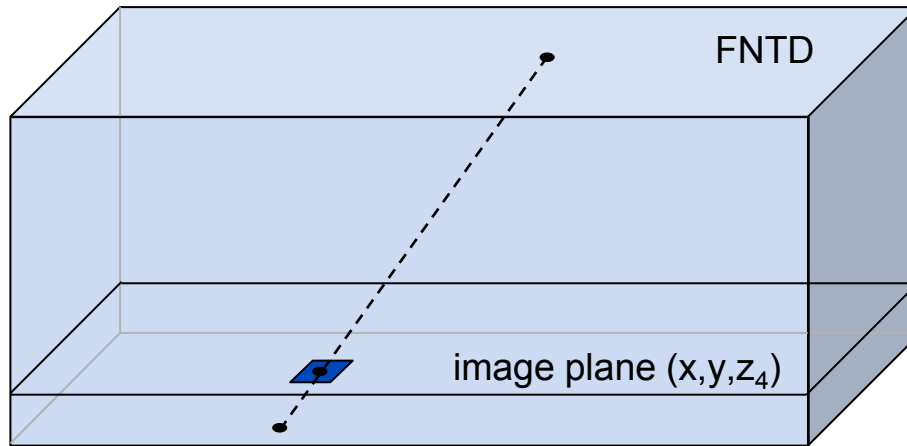
FNTD technology



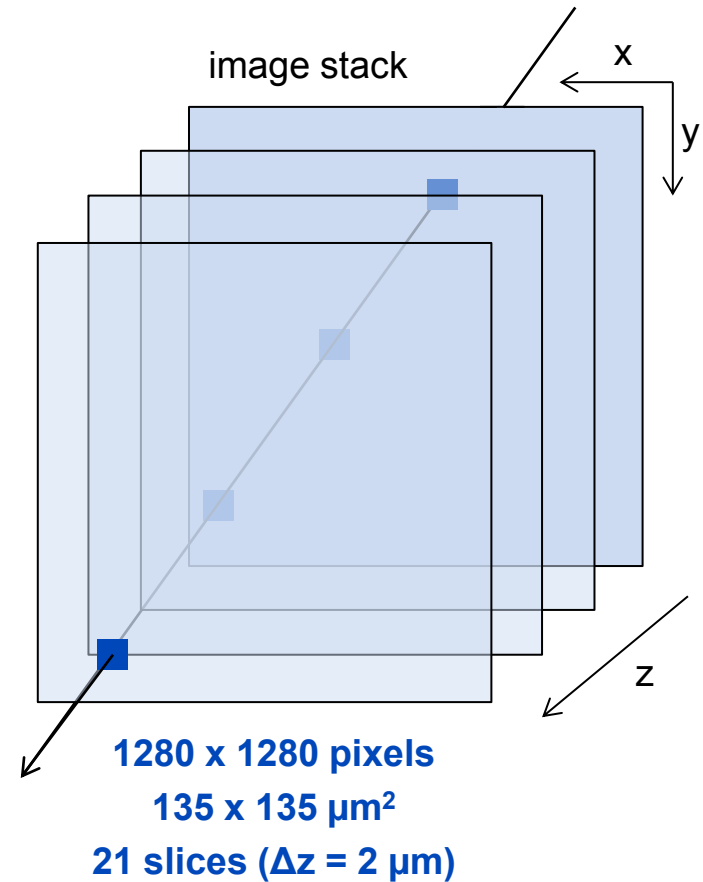
FNTD technology



Readout principle

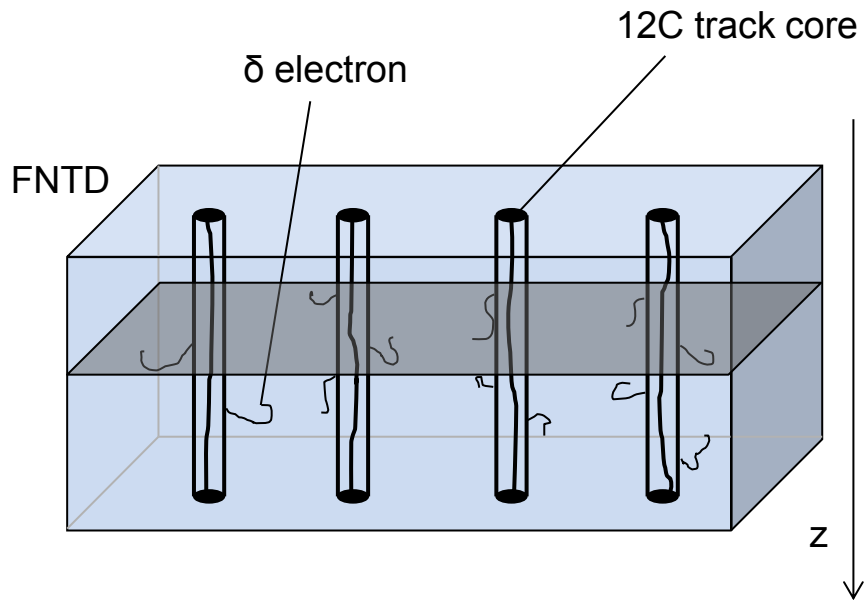


- detector stores trajectory information of traversing ions
- access information via confocal microscopy
 - scan focus plane laterally
 - change focus depth
- image stack contains full 3D information on individual ion tracks

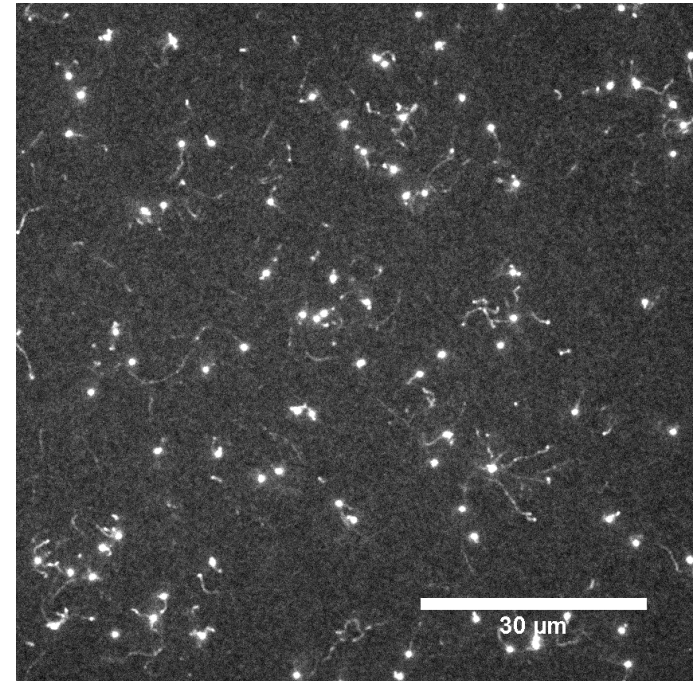


Unidirectional field

12C irradiation (entrance channel)



FNTD readout (Zeiss LSM 710)



I

1st APPLICATION

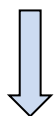
Particle counter

project of J.-M. Osinga

Quality assurance and verification

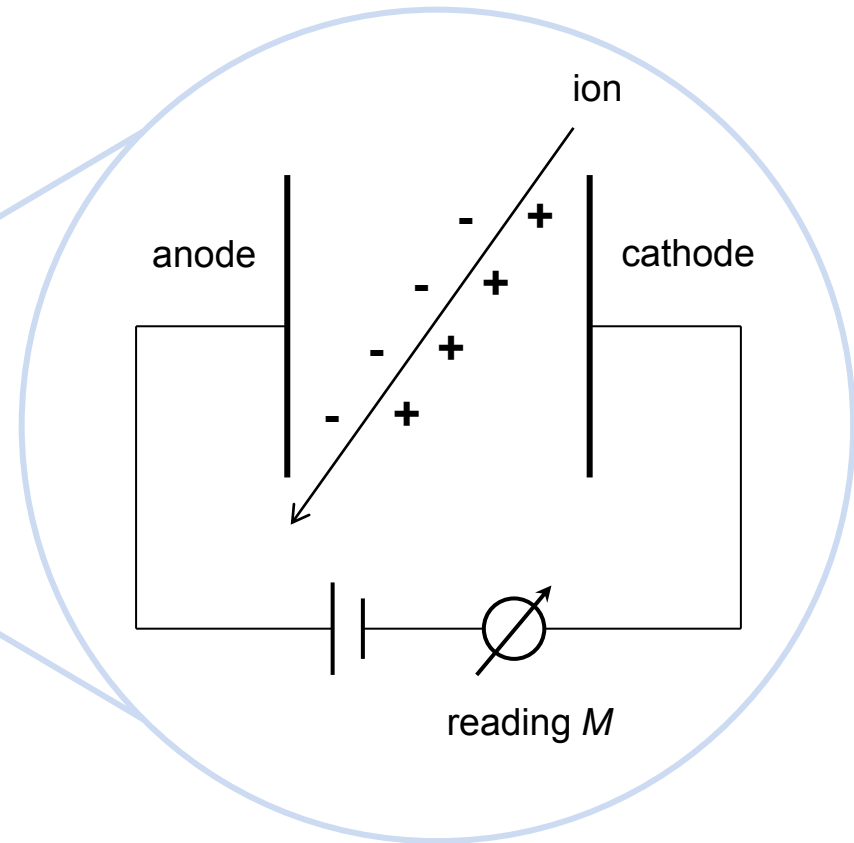


ionization chamber



dose to water:

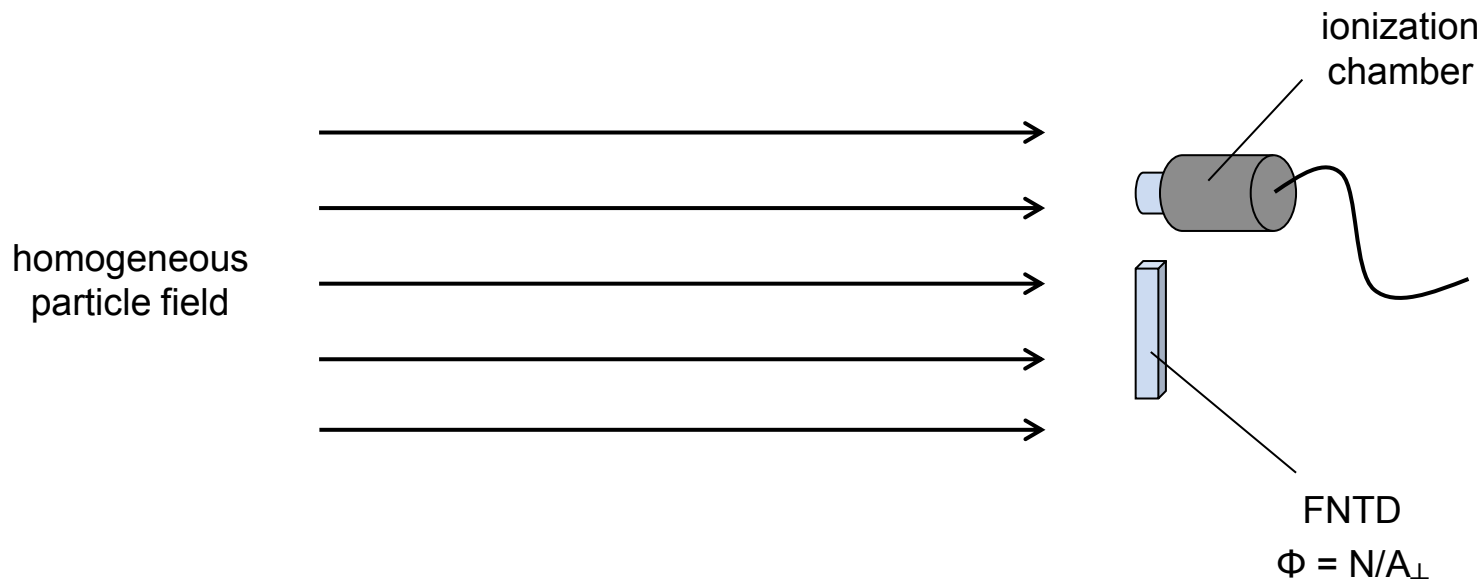
$$D_{IC} = \underbrace{M_{Q,k_i}}_{\text{reading}} \times \underbrace{N_{D,Q_0}}_{\text{calibration}} \times \underbrace{k_{Q,Q_0}}_{\text{correction}}$$



~ 3% uncertainty for carbon ions

Comparison experiment

Novel fluence-based dosimetry approach



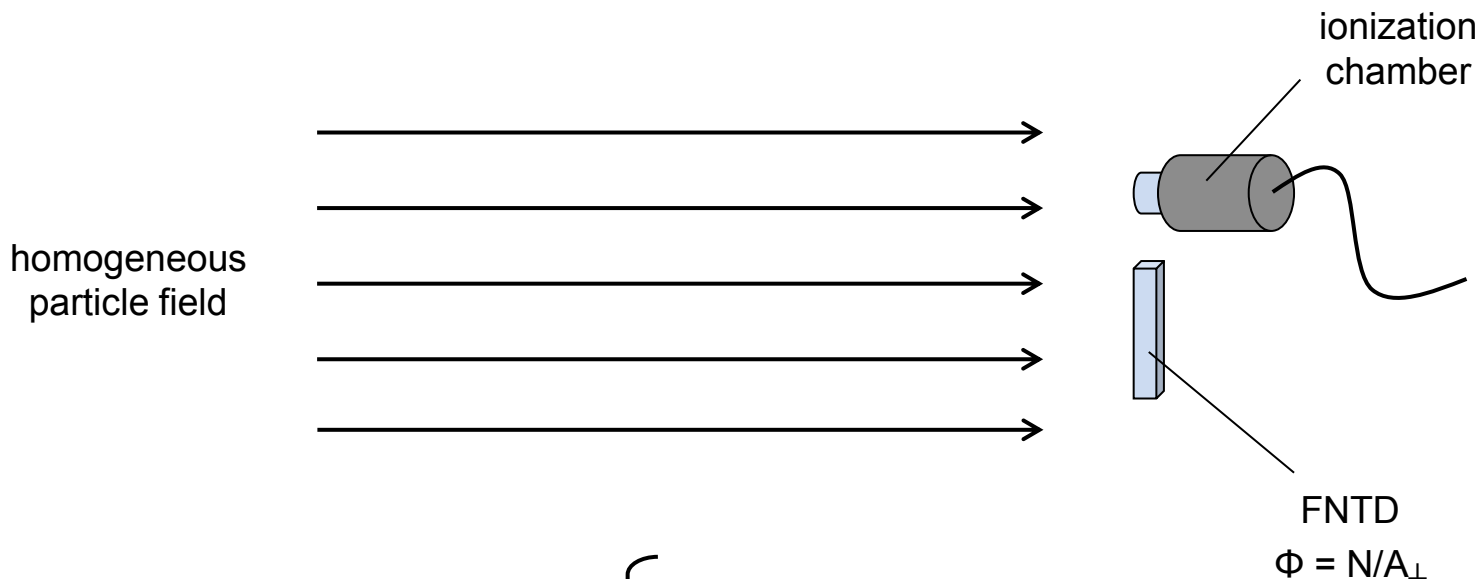
$$D_{FNTD} = \frac{1}{\rho} \Phi S_{eff}$$

nuclear interactions:

- **protons:** energy straggling and target fragmentation
- **carbon ions:** projectile fragmentation; build-up of lower-Z secondary ions

Comparison experiment

Novel fluence-based dosimetry approach

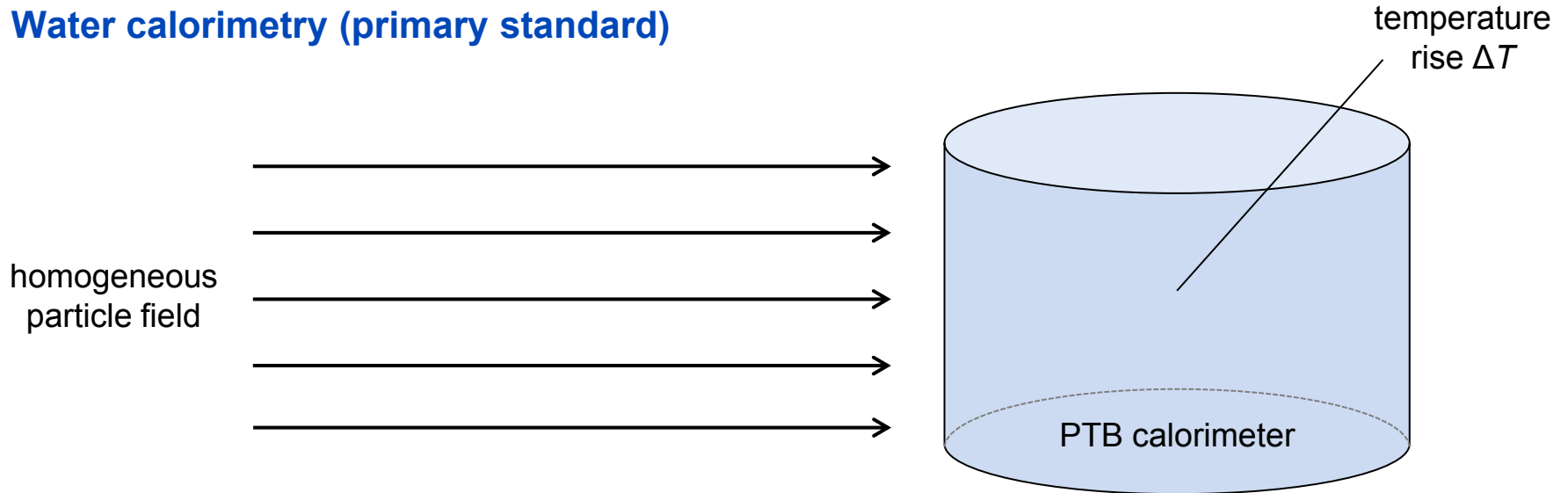


$$\Delta = \frac{D_{IC} - D_{FNTD}}{D_{IC}} \left\{ \begin{array}{l} \bullet \text{ protons: } \Delta_p = + 2.4\% \\ \bullet \text{ carbons: } \Delta_C = + 4.5\% \end{array} \right.$$

k_Q uncertainty?

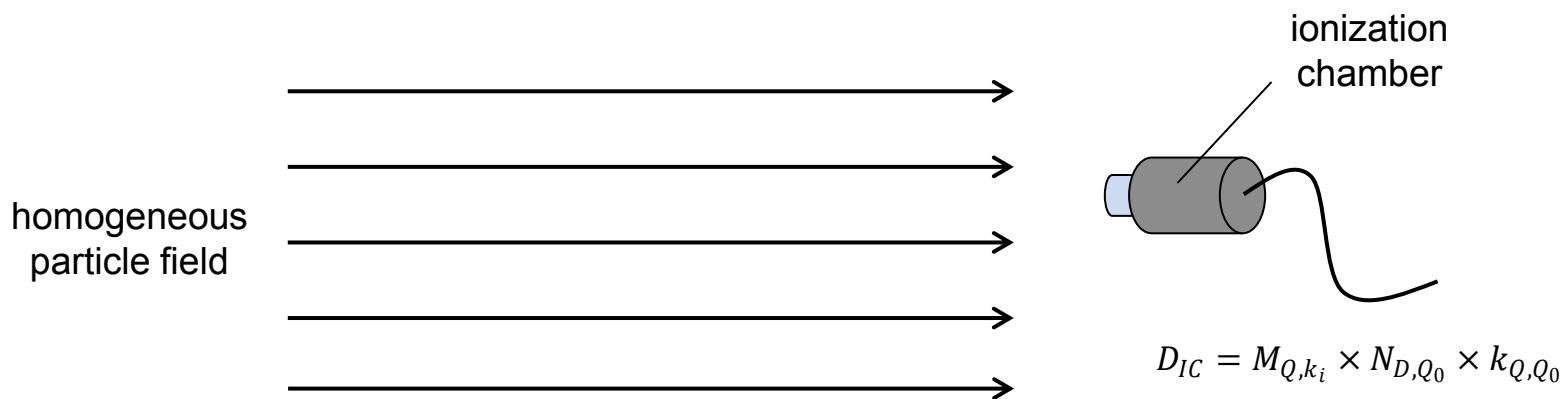
[Osinga et al., Radiat. Prot. Dosim., 2014]

Water calorimetry (primary standard)



$$D_{WC} = \Delta T c_P \prod_i k_i$$

Water calorimetry (primary standard)



$$D_{WC} = \Delta T c_P \prod_i k_i = D_{IC}$$



$$k_{Q,Q_0} = \frac{D_{WC}}{M_{Q,k_i} \times N_{D,Q_0}}$$

II

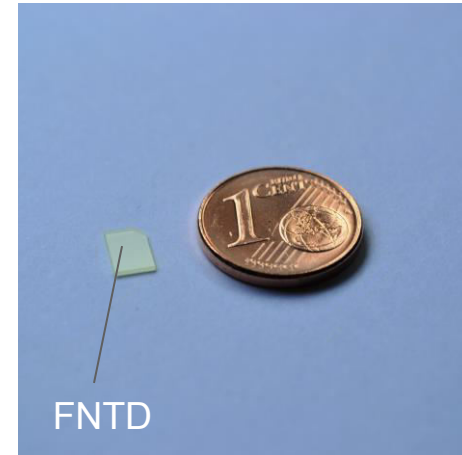
2nd APPLICATION

In vivo dosimeter

project of G. Klimpki

**with fluorescent nuclear
track detectors (FNTDs):**

- measure dose *in vivo*
- estimate biological effect



measured quantities:

$$D_{biol} = f(\Phi, S, Z)$$

particle fluence Φ

calculated from

normalized particle
number N/A_{\perp}

stopping power S

calculated from

track
intensity I

atomic number Z

attributed to

track intensity
distribution

$$D_{biol} = f(\Phi, S, Z)$$

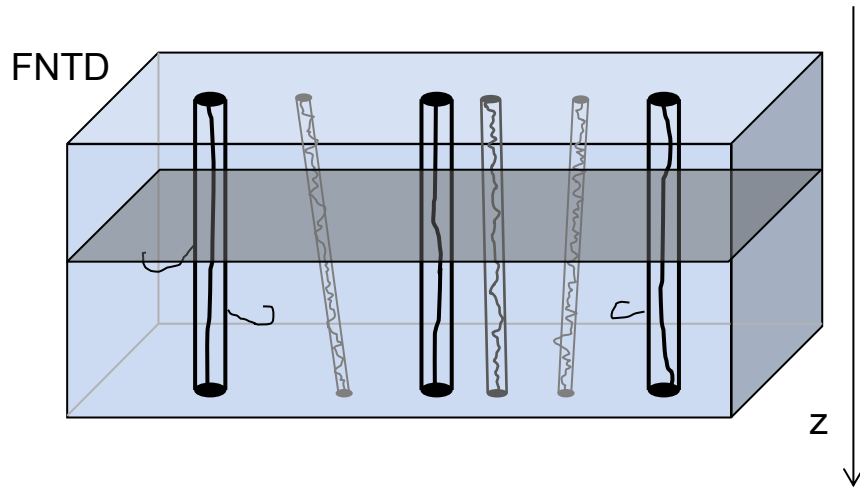
(a) particle fluence Φ

(b) stopping power S

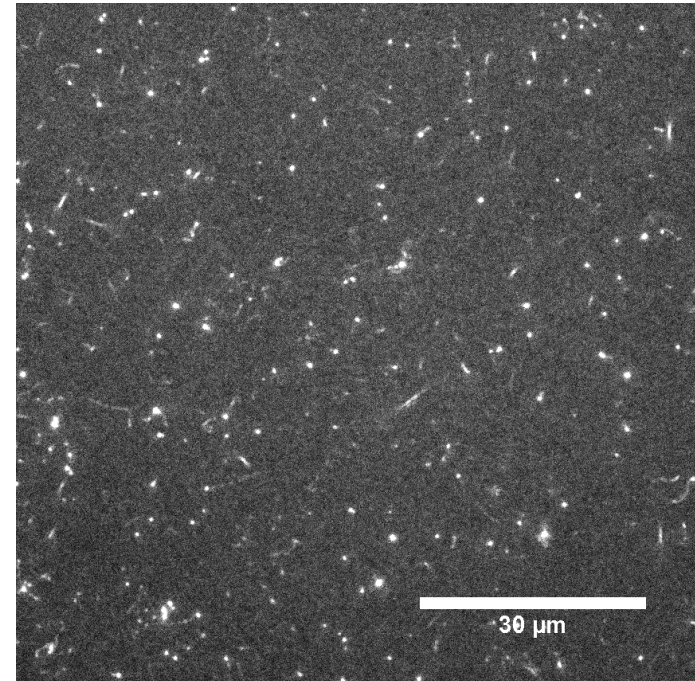
(c) atomic number Z

Multidirectional field

12C irradiation (Bragg peak)



FNTD readout (Zeiss LSM 710)

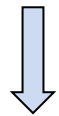


Irradiation

Heidelberg Ion-Beam Therapy Center

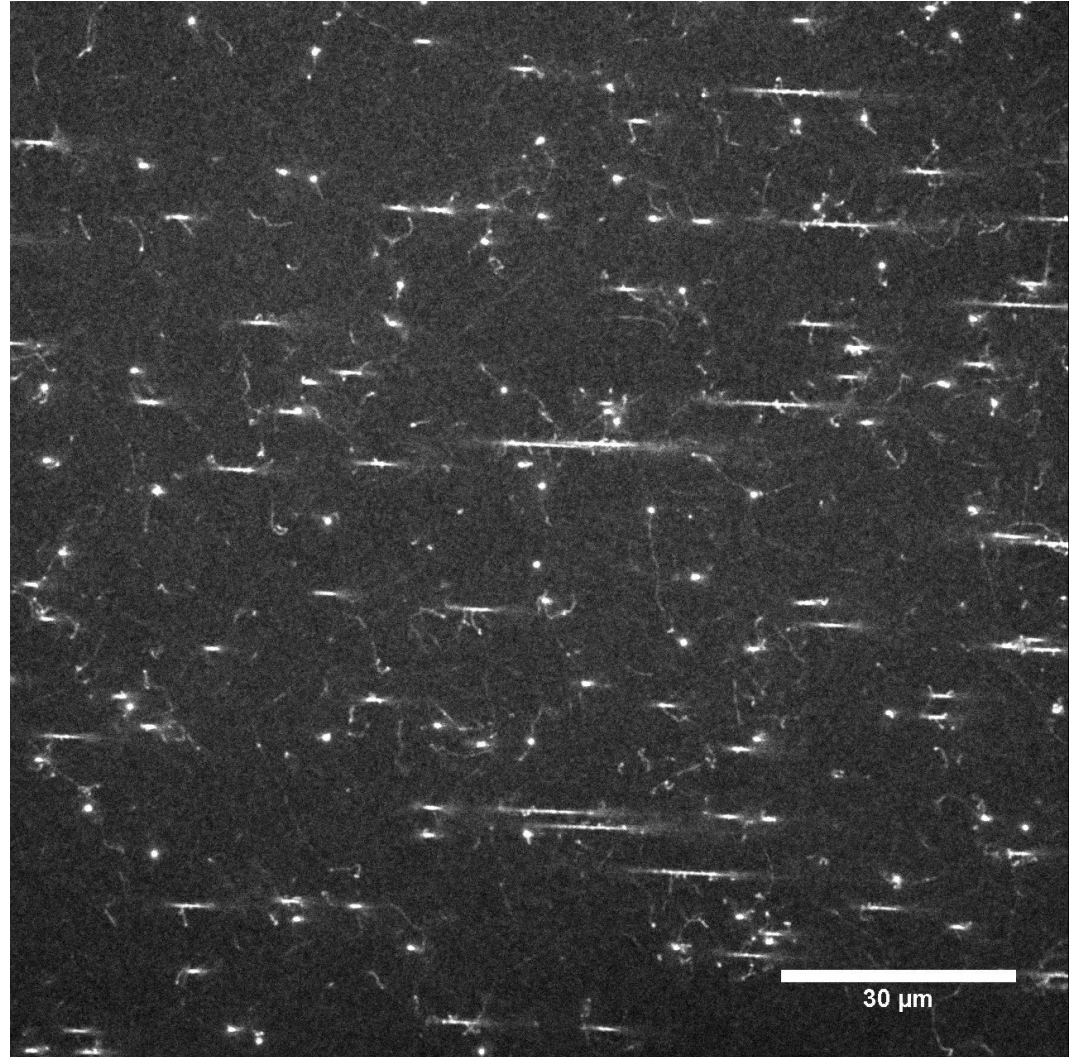
1 detector under 6 angles:
($\vartheta = 0^\circ, 15^\circ, 30^\circ, 45^\circ, 60^\circ, 75^\circ$)

- ion type: ^{12}C
- energy: 90 MeV/u
- total fluence:
 $1.2 \times 10^6 \text{ cm}^{-2}$



Readout

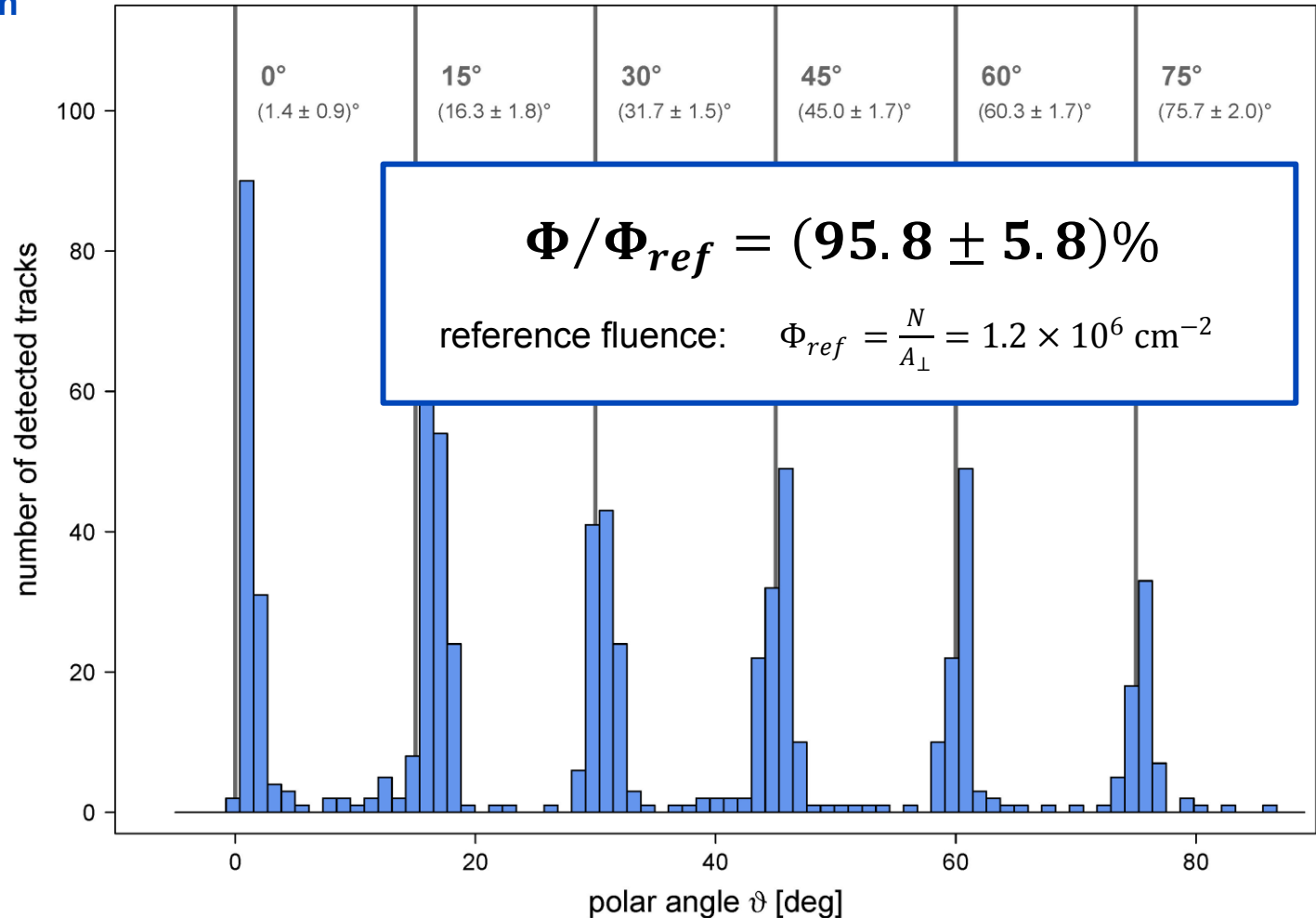
Zeiss LSM 710 microscope (30 min)



Angular distribution

ϑ histogram

701 carbon ion
trajectories



$$D_{biol} = f(\Phi, S, Z)$$

(a) particle fluence Φ

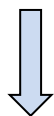
(b) stopping power S

(c) atomic number Z

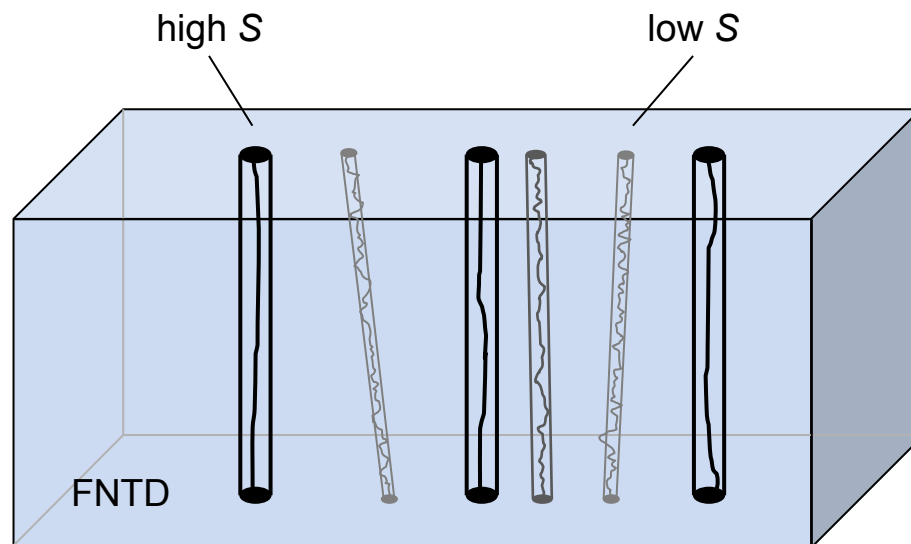
FNTD in mixed field

- high linear stopping power
- large number of secondary electrons
- large number of transformed color centers
- high local track intensity

[Sykora et al., Radiat. Meas. 43, 2008]



correlate stopping power and intensity

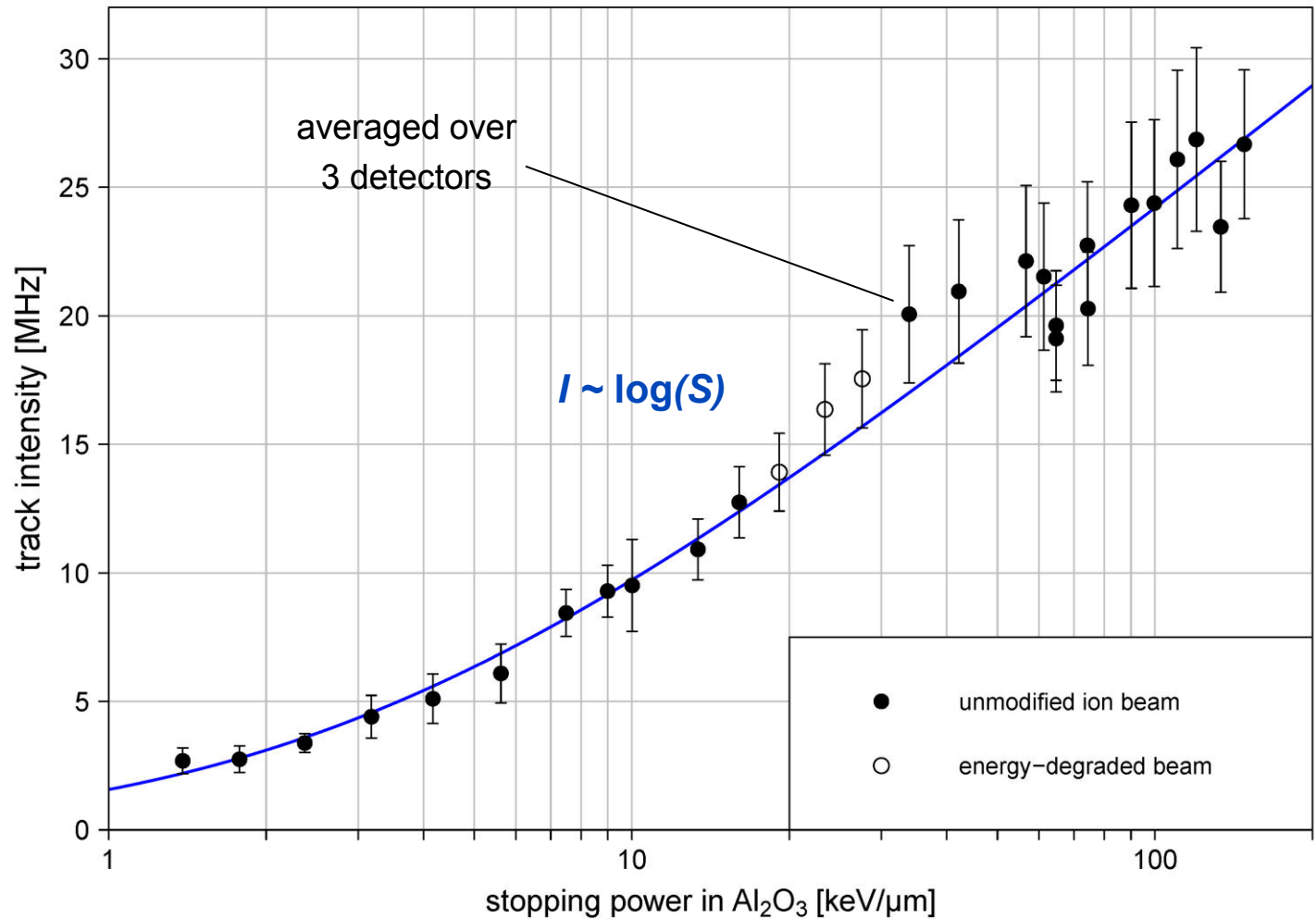


list of limitations:

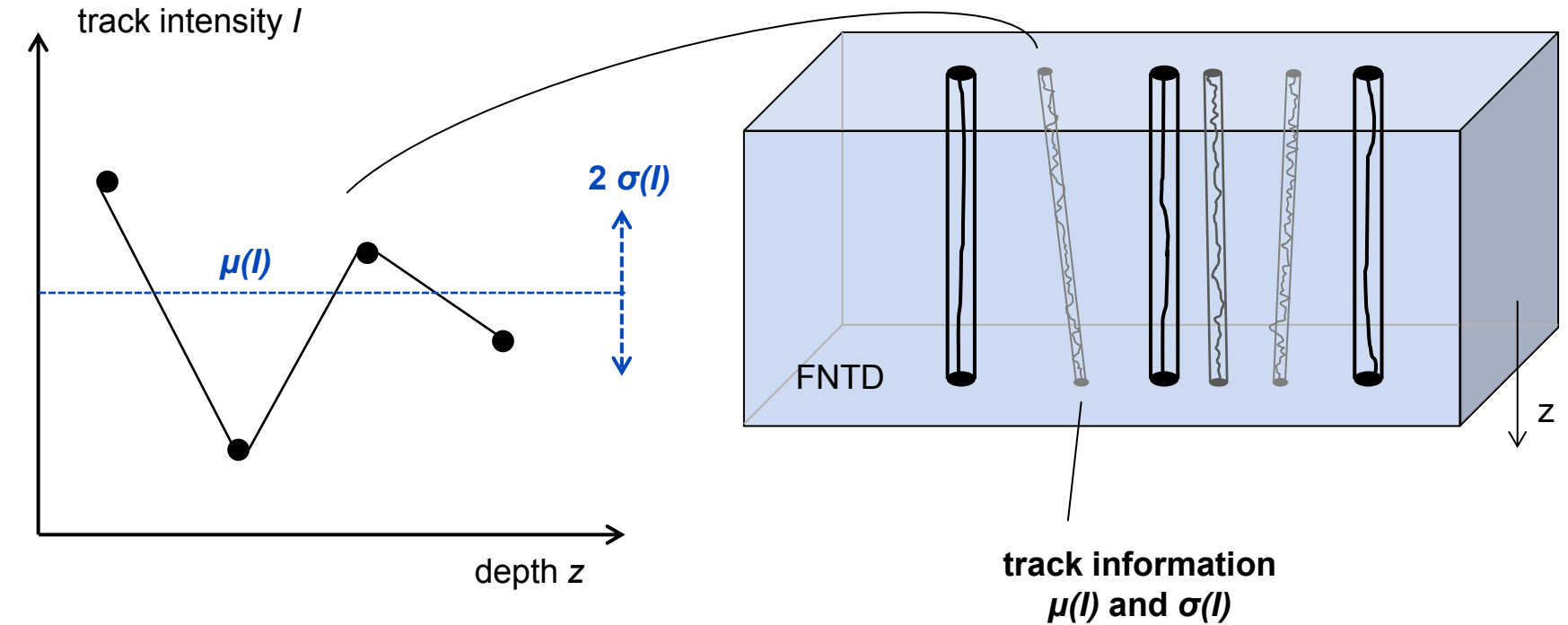
- **FNTD:** detector sensitivity fluctuations; ...
- **PHYSICS:** stochastic energy deposition; intensity loss of angular tracks; intensity measurements itself (maximum, Gauss peak, mean); ...
- **MICROSCOPE:** flat field correction; spherical aberration; ...

$I \sim S$ plot based on 28 irradiations

[H. Mescher, Bachelor's Thesis, DKFZ, 2014]



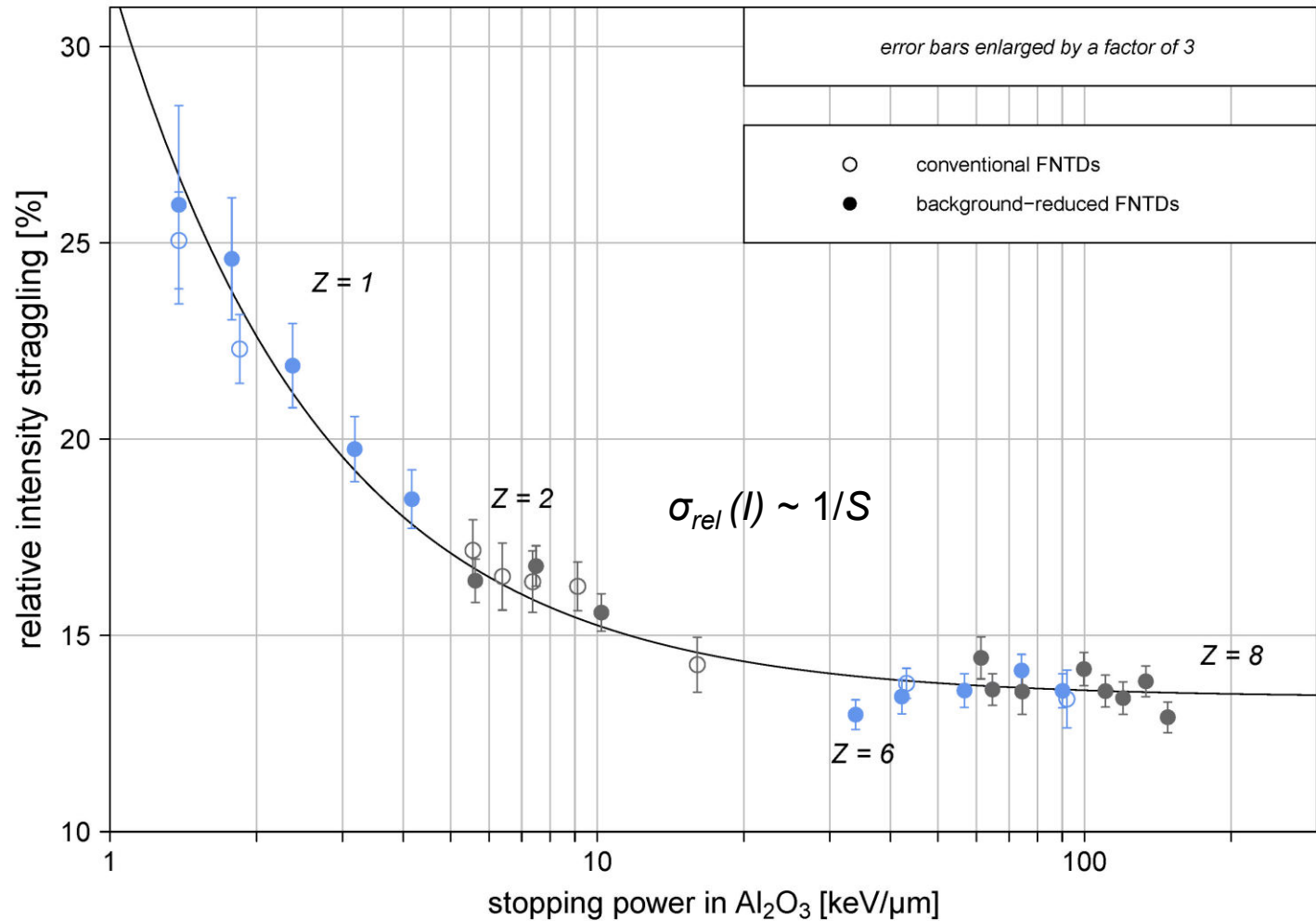
Sensitivity correction



$$\sigma_{rel}(I) = f(S, Z, \dots)?$$

Relative intensity straggling

$\sigma_{rel}(I) \sim S$ plot
based on 31
irradiations



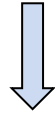
$$D_{biol} = f(\Phi, S, Z)$$

(a) particle fluence Φ

(b) stopping power S

(c) atomic number Z

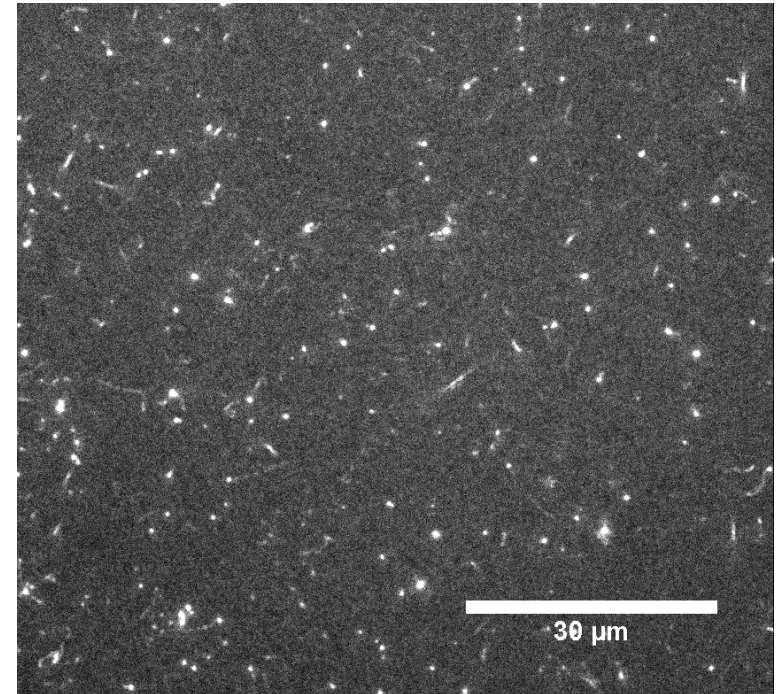
1. correlate Z and track width



information on track width lost
during confocal readout

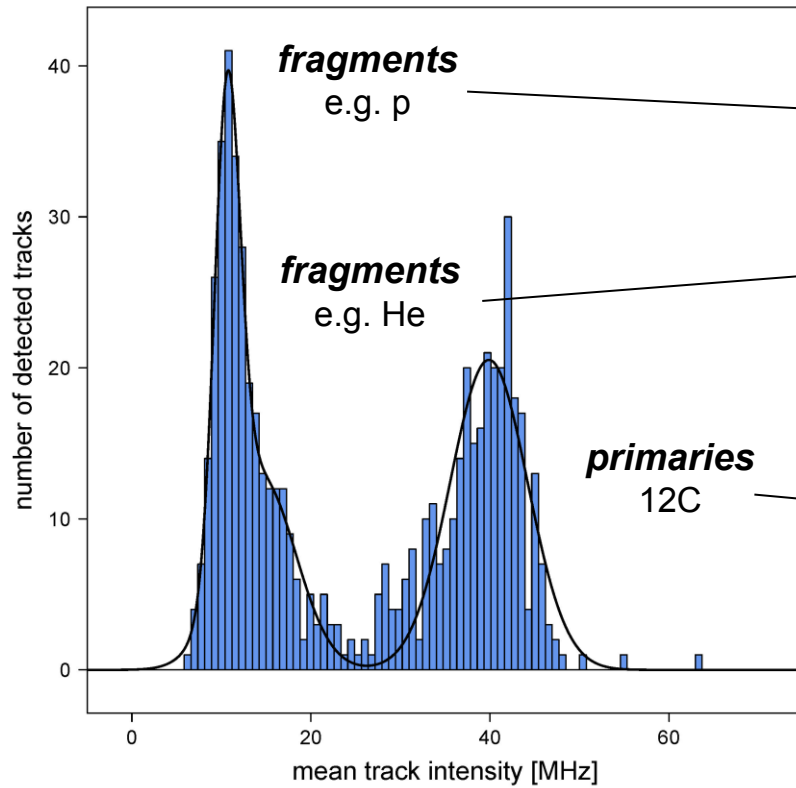
[Niklas et al., Radiat. Meas. 56, 2013]

FNTD placed in mixed heavy ion field

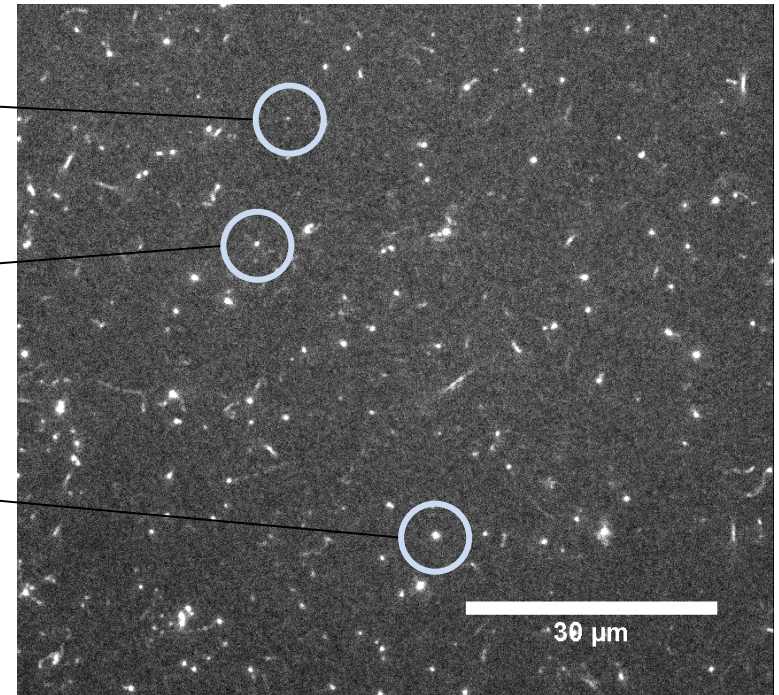


Charge spectroscopy

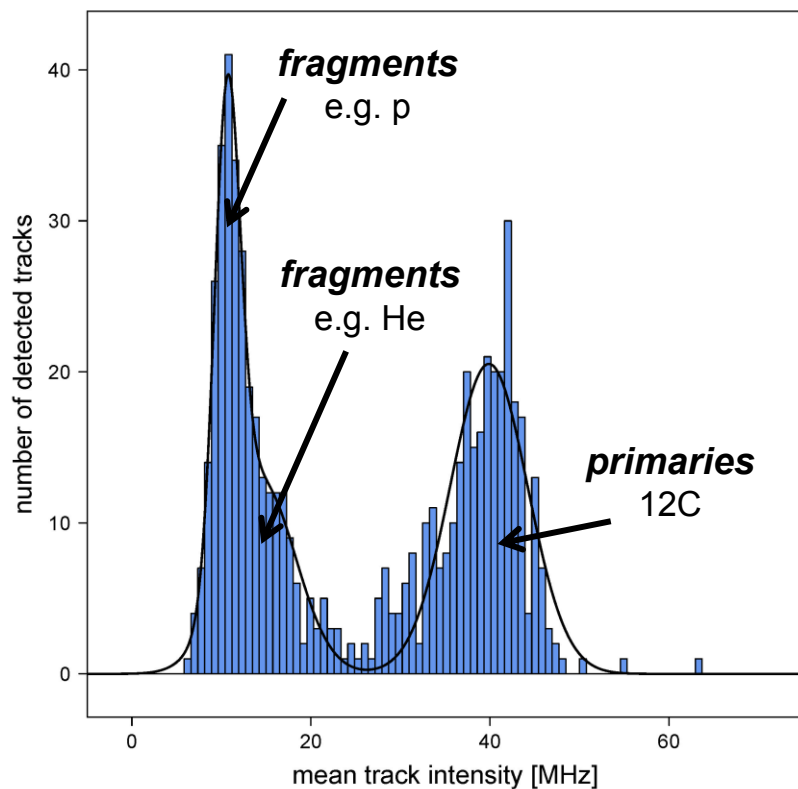
2. attribute Z to intensity spectrum



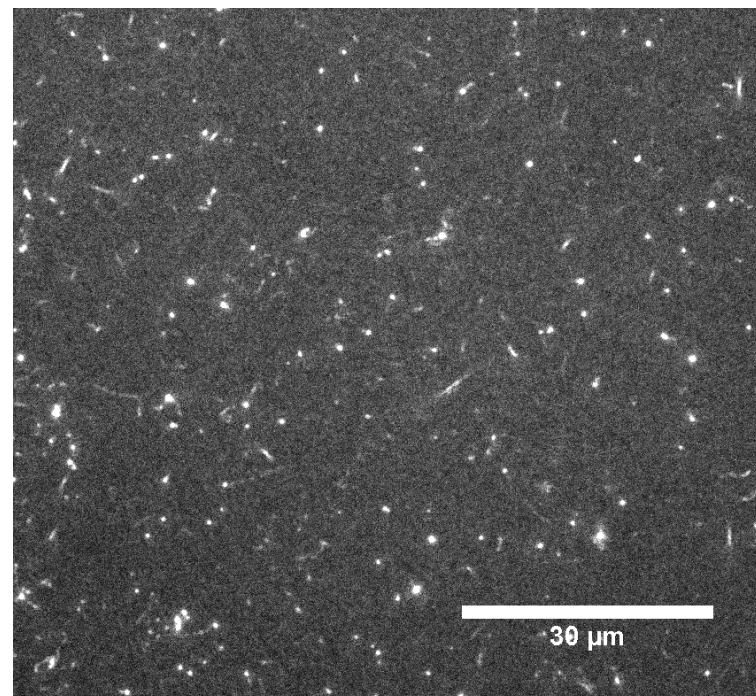
FNTD placed in mixed heavy ion field



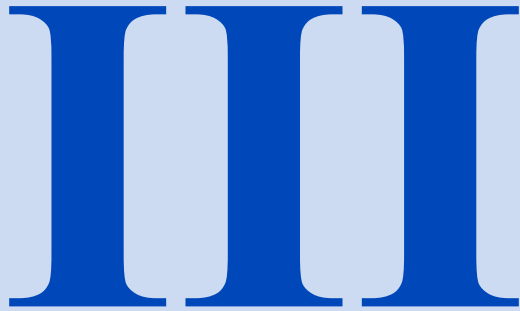
2. attribute Z to intensity spectrum



FNTD placed in mixed heavy ion field



attribution feasible if knowledge on primary beam is available

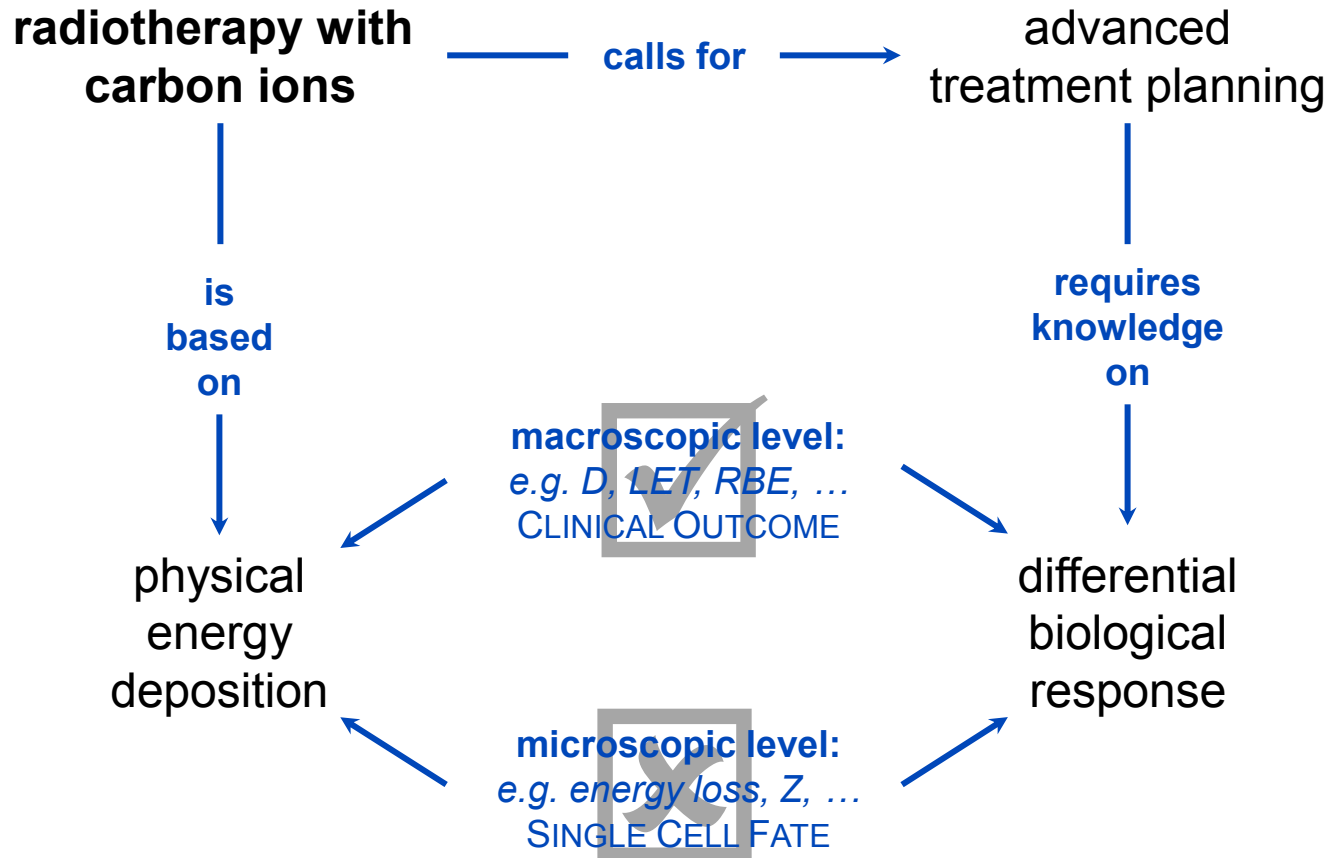


3rd APPLICATION

Hybrid detector

project of M. Niklas

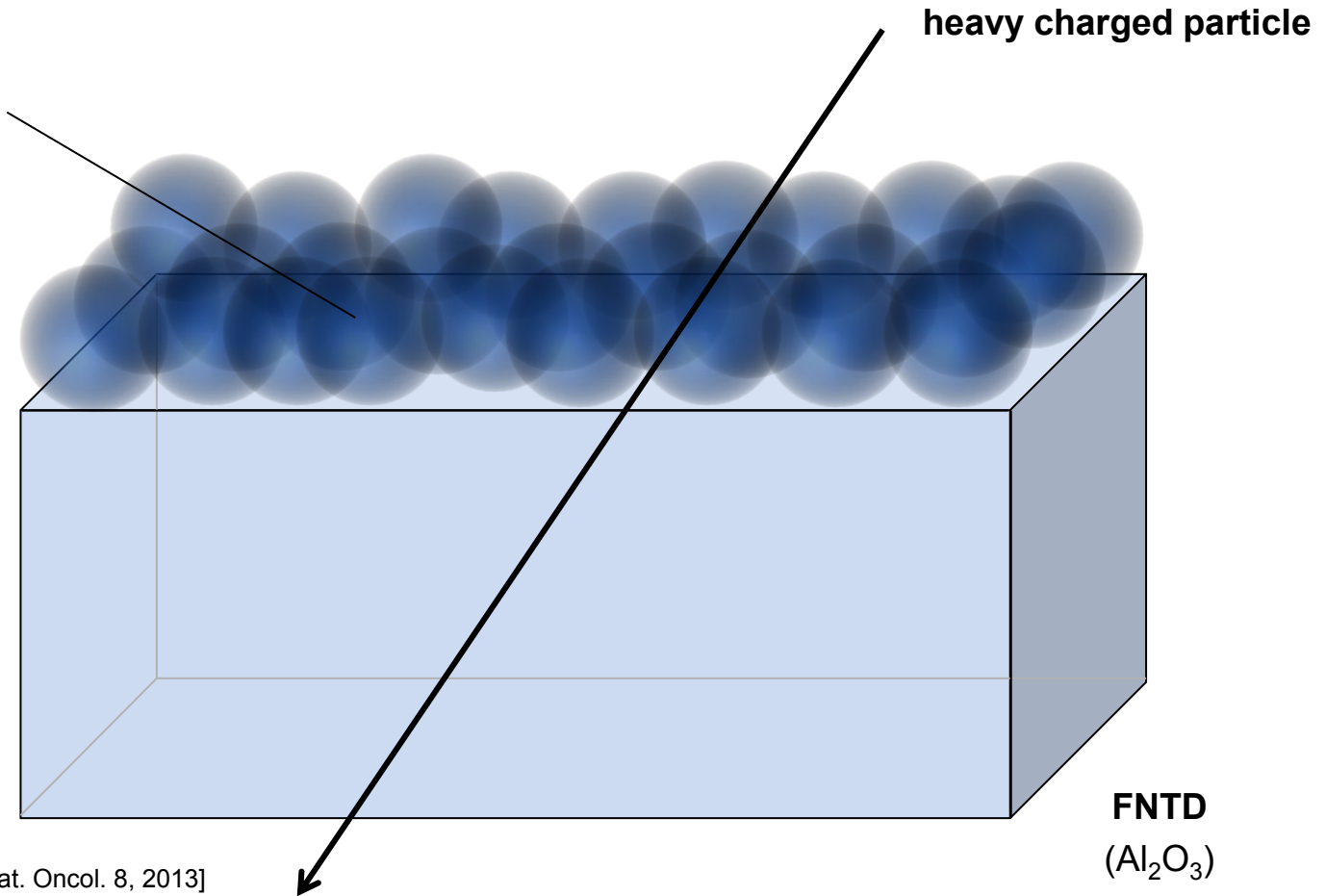
Fundamental principle of ion RT



Hybrid detector system

A549 cell layer

- tightly packed
- monolayer
- immobilization
- little overlap

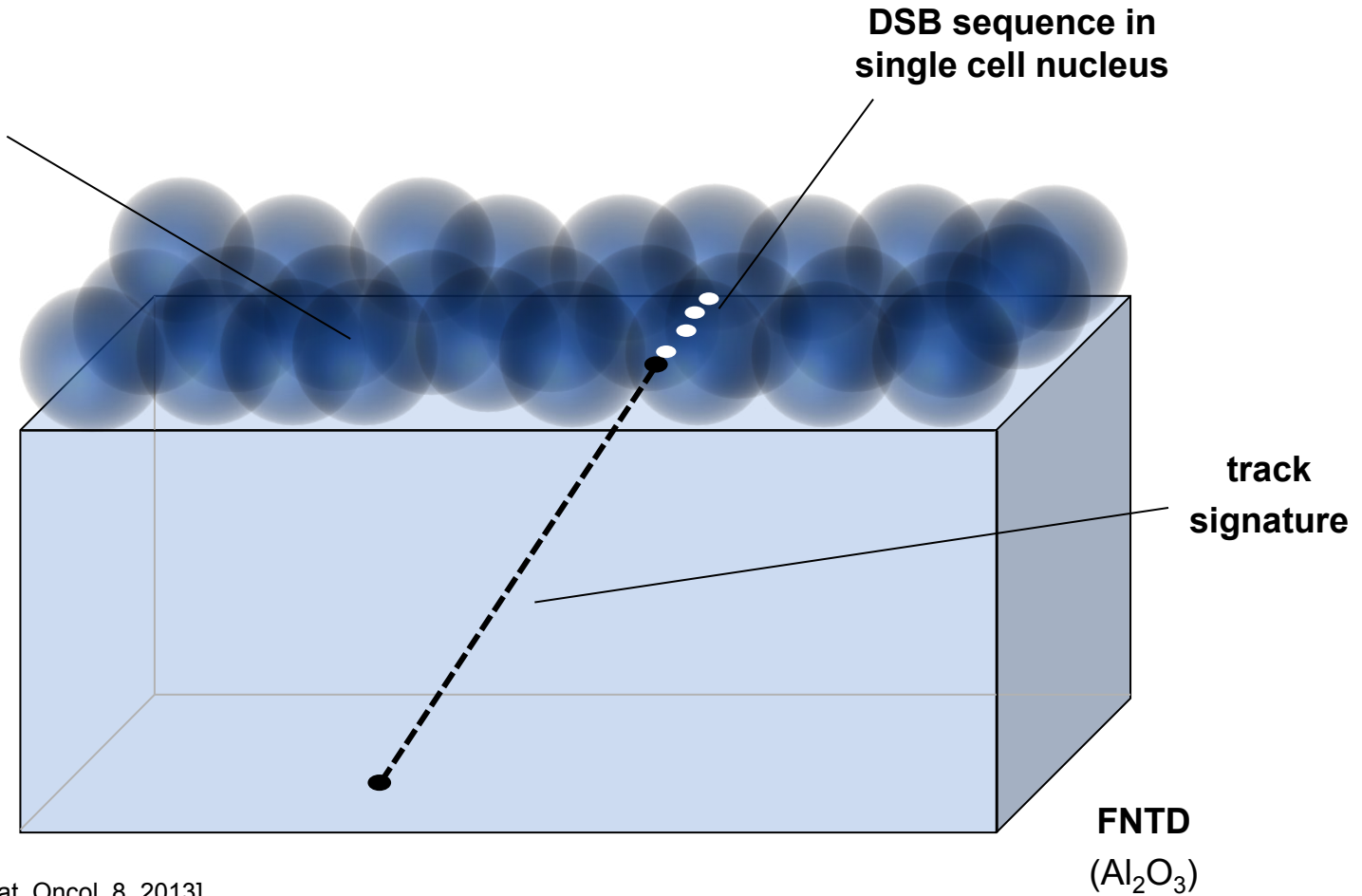


[Niklas et al., Radiat. Oncol. 8, 2013]

Hybrid detector system

A549 cell layer

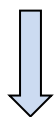
- tightly packed
- monolayer
- immobilization
- little overlap



[Niklas et al., Radiat. Oncol. 8, 2013]

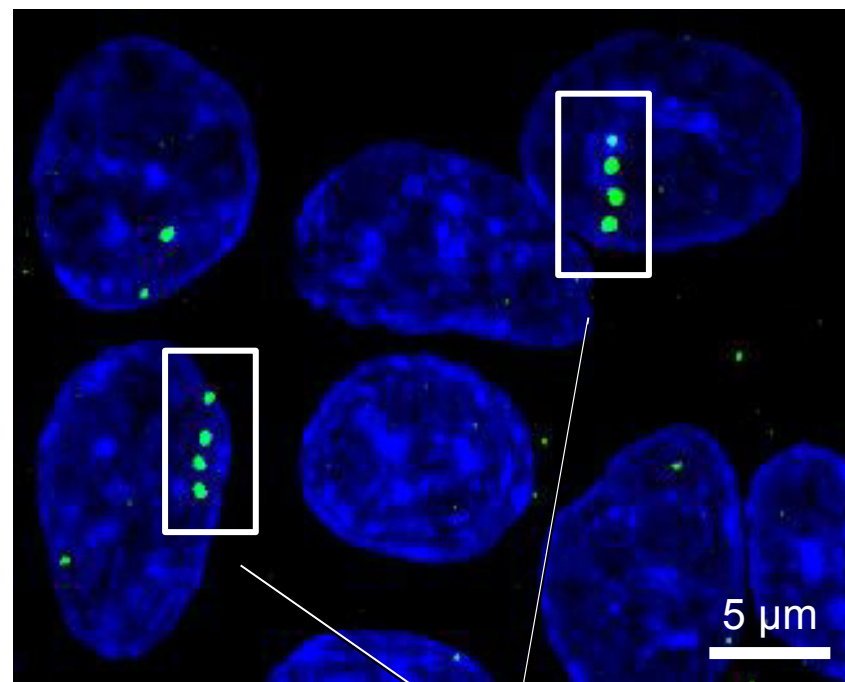
Experiment overview

- irradiation with 270 MeV/u carbon ions
- 360 analyzed cells
- 100 detected nucleus hits
- 16 DSB sequences



correlation of all DSB sequences to ion tracks

[Niklas et al., Int. J. Radiat. Oncol. 87, 2013]



DSB sequences

A vertical black line is positioned to the left of the text.

SUMMARY

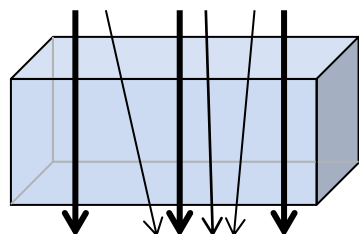
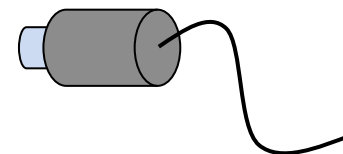
and outlook

I

1st APPLICATION

FNTDs as particle counters

J.-M. Osinga



II

2nd APPLICATION

FNTDs as in vivo dosimeters

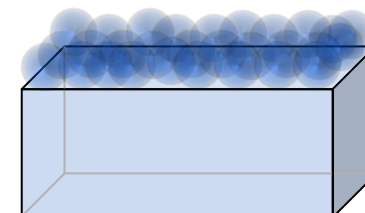
G. Klimpki

III

3rd APPLICATION

FNTDs as hybrid detectors

M. Niklas



Thank you for
your attention!



dkfz.

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CANCER RESEARCH CENTER
IN THE HELMHOLTZ ASSOCIATION



50 Years – Research for
A Life Without Cancer