

# Thin Film Gallium Nitride (GaN) Based Acoustofluidic Tweezer: Modelling and Microparticle Manipulation

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1 ABSTRACT

2 Gallium nitride (GaN) is a compound semiconductor which shows advantages in new  
3 functionalities and applications due to its piezoelectric, optoelectronic, and piezo-resistive  
4 properties. This study develops a thin film GaN-based acoustic tweezer (GaNAT) using surface  
5 acoustic waves (SAWs) and demonstrates its acoustofluidic ability to pattern and manipulate  
6 microparticles. Although the piezoelectric performance of the GaNAT is compromised  
7 compared with conventional lithium niobate-based SAW devices, the inherited properties of  
8 GaN allow higher input powers and superior thermal stability. This study shows for the first  
9 time that thin film GaN is suitable for the fabrication of the acoustofluidic devices to manipulate  
10 microparticles with excellent performance. Numerical modelling of the acoustic pressure fields  
11 and the trajectories of mixtures of microparticles driven by the GaNAT was performed and the  
12 results were verified from the experimental studies using samples of polystyrene microspheres.  
13 The work has proved the robustness of thin film GaN as a candidate material to develop high-  
14 power acoustic tweezers, with the potential of monolithical integration with electronics to offer  
15 diverse microsystem applications.

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25 KEY WORDS

26 GaN, thin film, SAW, microfluidics, particle manipulation, IDT

## 1 1. INTRODUCTION

2 Surface acoustic wave (SAW)-based acoustic tweezers are [recently](#) developed for manipulating  
3 micro- [1, 2] and nano-particles [3], cancer cells [4, 5], [blood cells and platelets](#) [6, 7], bacteria  
4 [8, 9], exosomes [10], droplets [11], lipoproteins [12] [and studying intracellular signaling](#) [13].  
5 They show superior advantages and effectiveness as a contactless, label-free, biocompatible,  
6 and versatile tool for biomedical applications [14]. Studies have demonstrated improved label-  
7 free manipulation efficiency realized by integrating acoustic tweezers with dielectrophoresis  
8 [15, 16] and optics [17]. Lithium niobate ( $\text{LiNbO}_3$ ) is a commonly used piezoelectric material  
9 for fabricating SAW-based acoustic tweezers due to its outstanding electromechanical coupling  
10 coefficient.  $\text{LiNbO}_3$  has a very low thermal conductivity ( $0.044 \text{ W}/(\text{cm}\cdot\text{K})$ ) [18] which causes  
11 challenges for operating the acoustic tweezer at high powers for high-throughput manipulation  
12 of biological cells. The high power applied to the interdigital transducers (IDTs) patterned on  
13 the  $\text{LiNbO}_3$  wafer can generate considerable joule heating, which is [often](#) not dissipated  
14 efficiently [through  \$\text{LiNbO}\_3\$](#) , [thus](#) resulting in damage to the  $\text{LiNbO}_3$  substrate and biological  
15 samples [19]. Future acoustofluidic development is desirable to integrate with multi-physical  
16 properties such as optoelectronics and semiconductor circuitry for realizing multi-functional  
17 lab-on-a-chip (LOC). Since  $\text{LiNbO}_3$  does not have such [a](#) versatility to fulfill this purpose, it is  
18 timely to investigate other potential materials with versatile capabilities and robustness for  
19 manufacturing acoustofluidic devices.

20

21 Gallium nitride (GaN) is one of the key compound semiconductor materials for semiconductor  
22 industry after silicon due to its wide band gap, high breakdown electric field, and high electron  
23 mobility [20]. These distinct properties make GaN one of the best materials for optoelectronic  
24 devices e.g., light-emitting diodes (LEDs), and high power and high-temperature electronics,  
25 e.g., high-electron-mobility transistors (HEMT) [21-23]. [A comparison of material properties](#)  
26 [between GaN and  \$\text{LiNbO}\_3\$](#)  are given in Table 1. Although GaN has a lower effective

1 electromechanical coupling coefficient which can be compensated by increasing the applied  
 2 electrical energy, other key attributes such as good thermal conductivity, mechanical, and  
 3 semiconductor properties of GaN make it a superior material for working in high power, low-  
 4 loss, harsh environment and integration in a multifunctional platform. GaN possesses good  
 5 piezoelectric properties and has been applied to make SAW devices for RF filters [24] and  
 6 resonators [25]. The combination of piezoelectric, optoelectronic and semiconducting  
 7 properties provides GaN unique opportunities for nano- and microelectromechanical systems  
 8 (N/MEMS) applications, with a great potential for low cost scaled-up manufacture of  
 9 monolithic electronic devices using large sizes of GaN wafers [26].

10 Table 1 Comparisons of properties between GaN and LiNbO<sub>3</sub>

	Effective coupling coefficient, $k_{\text{eff}}^2(\%)$	Acoustic velocity (m/s)	Refractive index	Thermal Conductivity (W/(cm·K))	Elastic Modulus $c_{33}(\text{GPa})$	Bandgap (eV)	Electron mobility( $\text{cm}^2/\text{V}\cdot\text{sec}$ )
GaN	2 [27]	8044 [20]	2.3-2.5 [29]	1.3 [28]	398 [20]	3.4 [20]	2000 [20]
LiNbO <sub>3</sub>	5-12 [29]	3900 [20]	2.29 [29]	0.044 [18]	60 [30]	N/A	N/A

11

12 Comparing with GaN, there are other types of commonly used thin film piezoelectric materials  
 13 such as ZnO and AlN, which possess high coupling coefficient and good thermal conductivity  
 14 to apply in SAW-based microfluidics and LOC applications [29]. AlN-based SAW devices  
 15 show high leakage current which constrains its applications on high frequencies (e.g. above 10  
 16 GHz [31]). Whereas for ZnO, zinc is a dopant of silicon and a contaminant element, which  
 17 makes ZnO challenging to be integrated with silicon complementary metal-oxide-  
 18 semiconductor (CMOS) [32]. By applying different dopants of GaN [33] and enhancing  
 19 photoconductivity through modifying the surface functionalization, GaN can be used to induce  
 20 physiological responses in yeast [34], improve the adhesion of PC12 cells [35], enhance cell  
 21 growth [36] and differentiation [37]. As GaN possesses a good biocompatibility, it would be of  
 22 great interest to investigate the feasibility of using GaN for fabricating SAW devices to  
 23 manipulate microparticles or biological cells. In addition, GaN can be fabricated as thin film

1 piezoelectrics with similar benefits as ZnO and AlN for next generation acoustofluidic chips  
2 and LOC devices [29]. Thin film GaN-based devices can also overcome the expensiveness and  
3 brittleness of bulk LiNbO<sub>3</sub> materials and allow SAW functionalities to be realised by depositing  
4 the thin piezoelectric film onto wherever the acoustic wave is required [38]. GaN has a higher  
5 speed of sound than that of LiNbO<sub>3</sub>, which allows a GaN-based SAW device to achieve a higher  
6 resonant frequency than that of LiNbO<sub>3</sub>-based device using the same IDT period. In addition,  
7 the two-dimensional electron gases on which GaN HEMTs are based, can be used as IDTs to  
8 eliminate the mass loading and signal reflection [39]. Such excellent properties along with the  
9 maturity of GaN device manufacturing on large wafer sizes makes GaN the perfect choice for  
10 next generation SAW devices.

11

12 In this study, we developed an acoustic tweezer using thin film GaN, e.g., GaNAT, based on  
13 its good thermal and piezoelectric properties. The GaNAT was modelled and tested for  
14 patterning and manipulations of microparticles in order to prove the concept of using GaN as  
15 an alternative material for manufacturing acoustofluidic devices.

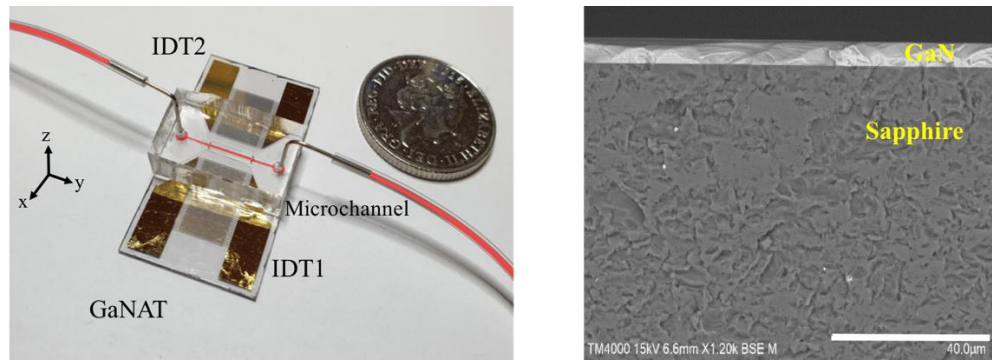
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## 17 2. MATERIAL AND METHODS

### 18 2.1 Fabrication of GaNAT

19 Fig. 1a shows a photo of the fabricated GaNAT comprising a polydimethylsiloxane (PDMS)  
20 microchannel and a GaN-based SAW device. The SAW device was made by a GaN/sapphire  
21 wafer patterned with a pair of IDTs, between which the microchannel was bonded to form the  
22 GaNAT. The GaN thin film was grown on a sapphire substrate in [0001] direction, and Fig. 1b  
23 shows its cross-section image obtained using a scanning electron microscope (SEM,  
24 TM4000PLUS, HITACHI, Japan). The GaN and sapphire layers are measured to be ~4.5 μm  
25 and ~600 μm thick, respectively. The GaN surface was patterned by bilayers of chromium/gold  
26 (30 nm/150 nm-thick) as electrodes using a magnetron sputtering system (LLJGP-560, SKY

1 technology development, China) after a conventional photolithography process. The GaN wafer  
2 was then placed into acetone in an ultrasound bath to perform the lift-off process. Then it was  
3 cleaned with ethanol, deionized water and then dried with nitrogen gas. The pitch of the finger  
4 electrodes,  $p$ , determines the wavelength,  $\lambda$ , of the generated SAW, i.e.,  $\lambda = 4p$ . Both the width  
5 and pitch of the finger electrodes are  $70\ \mu\text{m}$ , which produce SAWs with a wavelength of  $280\ \mu\text{m}$ . Each IDT  
6 contains 40 pairs of finger electrodes with an aperture size of  $7\ \text{mm}$ . The  
7 Rayleigh-mode SAW velocity in the GaN/Sapphire is  $5,486\ \text{m/s}$  in the  $[0001]$  direction [40]  
8 resulting in a Rayleigh-mode frequency  $f = v/\lambda \approx 19.6\ \text{MHz}$ . For the same IDT period, the  
9 higher velocity of the GaN/Sapphire allows a higher resonant frequency compared with that of  
10  $\text{LiNbO}_3$ , which could achieve more precise and effective manipulation of the microparticles.



11  
12 Fig. 1. GaNAT. (a) Photo of the GaNAT device. (b) The scanning electron microscopic image of the undoped  
13 GaN film on a sapphire substrate. The scale bar is  $40\ \mu\text{m}$ .

14

15 The PDMS microchannel with a dimension of  $280\ \mu\text{m}$  (W)  $\times$   $60\ \mu\text{m}$  (H)  $\times$   $1\ \text{cm}$  (L) was  
16 fabricated using a standard soft lithography process and a mold-replica procedure. The degassed  
17 mixture of the base and curing agent (Dow Corning, UK) with a mass ratio of 10:1 was poured  
18 onto the mold, left cured at  $65^\circ\text{C}$  for 2 hours to form the microchannel.

19

## 20 2.2 Characterization of GaNAT

21 The reflection functions of the two IDTs in terms of  $S_{11}$  (reflection coefficient) were measured  
22 using a vector network analyzer (VNA, E5061B ENA Series, Keysight, US). To reduce the  
23 power reflections from the IDTs, impedance matching networks were designed for the IDTs to

1 maximize the power transmission and reduce the risk of damaging the power amplifier when  
 2 operated at high powers. The experimental setup is shown in Fig. 2. The radio frequency (RF)  
 3 signals are amplified by a power amplifier (100A250A, Amplifier Research) to drive the  
 4 GaNAT. A power meter (U2004A, Keysight Technologies, UK) monitor the real-time incident  
 5 and reflected powers of each IDT. To quantify the amplitude of SAWs produced on the surface  
 6 of the GaN thin film with and without the matching networks, a laser vibrometer (PSV-500-  
 7 VH, Polytec, Germany) was used to measure the vibration on the GaN surface. To investigate  
 8 the thermal stability of the GaNAT, the temperatures of the two IDTs were recorded using an  
 9 infrared thermal camera (ETS320, FLIR, US) while changing the input power. For each power,  
 10 the temperature was measured for three times. The temperature values were recorded two  
 11 minutes after each power level, when the temperature becomes stabilized.

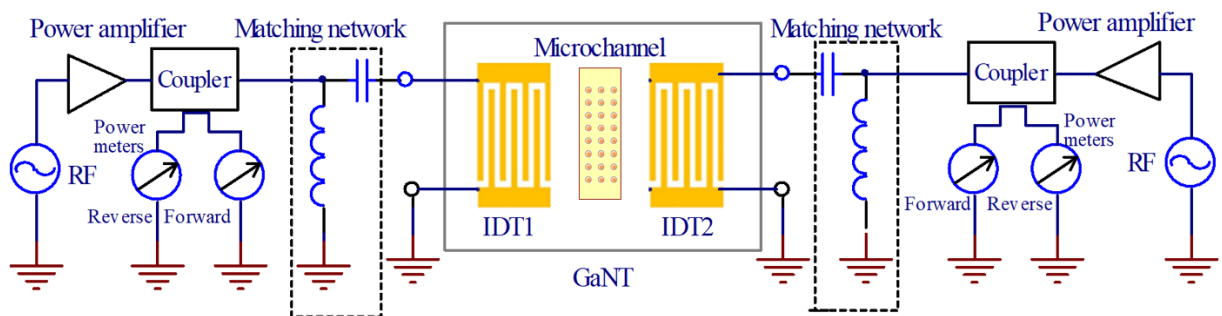


Fig. 2. The experimental setup of the GaNAT.

### 2.3 Experimental design of particle manipulation

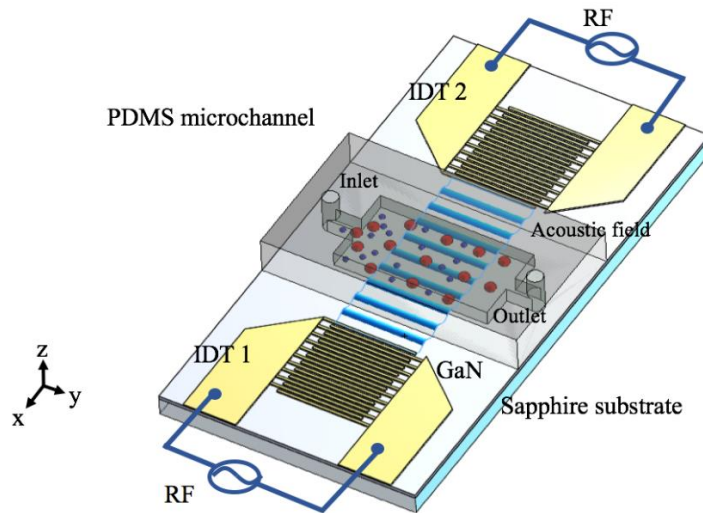
To study particle manipulation using the GaNAT, two batches of mixture polystyrene microspheres samples, e.g., 15  $\mu\text{m}$  and 5  $\mu\text{m}$ , as well as 15  $\mu\text{m}$  and 1  $\mu\text{m}$ , were prepared and injected separately into the microchannel using a syringe pump. When the sample was evenly dispersed inside the microchannel, an RF signal was applied to the GaNAT. The input power of the GaNAT for actuating particles was set to 40 dBm (10W).

## 3. THEORETICAL and NUMERICAL ANALYSIS

1 Fig. 3 shows the schematic of the GaNAT consisting of the SAW device and the PDMS  
 2 microchannel. Applying RF signals to the two IDTs will produce counter-propagating SAWs  
 3 along the surface of GaN and form standing surface acoustic waves (SSAWs). Once the SAWs  
 4 interact with the fluid inside the microchannel, leaky SAWs will be produced, thus exerting  
 5 acoustic radiation force, which is against a drag force on the microparticles inside the  
 6 microchannel. Along the SSAW propagation, a series of pressure nodes (PNs) with minimal  
 7 pressure amplitudes and pressure antinodes (ANs) with maximal pressure amplitudes are  
 8 generated. Microparticles with different signs of acoustic contrast factor  $\phi(\beta, \rho)$  are attracted  
 9 to either PNs (if  $\phi(\beta, \rho) > 0$ ) or ANs (if  $\phi(\beta, \rho) < 0$ ) [41].  $\phi(\beta, \rho)$  is a term determined by  
 10 compressibility and density given by,

$$11 \quad \phi(\beta, \rho) = \frac{5\rho_p - 2\rho_f}{2\rho_p + \rho_f} - \frac{\beta_p}{\beta_f} \quad (1)$$

12 where  $\rho_p, \rho_f, \beta_p,$  and  $\beta_f$  are the densities of the microparticle and the fluid, and the  
 13 compressibilities of the microparticle and the fluid, respectively.



14 Fig. 3. Schematic drawing of the GaNAT device consisting of a GaN-based SAW device bonded with a PDMS  
 15 microchannel.  
 16

17 A finite element method (FEM) was applied to analyze vibration modes of the GaN thin film  
 18 by solving the Newton and Maxwell equations in the two dimensional (2D) model [42]. Using  
 19 the parameters of the c-orientation GaN in Table S1, the numerical results of the Rayleigh  
 20 vibration modes of the GaN/sapphire at  $\lambda = 280 \mu\text{m}$  are obtained which are shown in Fig. S1.



1

2 A numerical simulation as described in Ref [43, 44] was further performed to study the  
3 acoustofluidic condition of the GaNAT device. COMSOL Multiphysics was used to investigate  
4 the acoustic pressure distributions inside the GaNAT device and the particle trajectories within  
5 the microchannel. Briefly, the SSAW generates a pressure disturbance in the fluid inside the  
6 microchannel. The perturbation induced by acoustic vibration is assumed to be much smaller  
7 than the characteristic length scale of the fluid domain [45]. Thus, the perturbation  
8 approximation is applied to numerically solve the acoustic pressure and particle velocity. Any  
9 particles whose size is much less than the height and the width of the microchannel experience  
10 acoustic radiation force  $\mathbf{F}^{\text{rad}}$  and Stokes drag force  $\mathbf{F}^{\text{drag}}$  [46],

$$11 \quad \mathbf{F}^{\text{rad}} = - \left( \frac{\pi p_0^2 V_p \beta_f}{2\lambda} \right) \phi(\rho, \beta) \sin(2kx) \quad (2)$$

$$12 \quad \mathbf{F}^{\text{drag}} = 6\pi\mu a (\langle \mathbf{v}_2 \rangle - \mathbf{v}_p) \quad (3)$$

13 where  $p_0, V_p, \beta_f, \lambda, \phi(\rho, \beta), k, x, \mu, a, \langle \mathbf{v}_2 \rangle$ , and  $\mathbf{v}_p$  denote acoustic pressure, volume of the  
14 microparticle, compressibility of the fluid, wavelength of the SAW, acoustic contrast factor (Eq.  
15 1), wave number, distance from the particle to the closest PN, fluid viscosity, radius of the  
16 particle, time-averaged second-order streaming velocity, and velocity of the microparticle,  
17 respectively. Using the boundary condition of acoustic impedance (parameters shown in Table  
18 S1),  $\mathbf{F}^{\text{rad}}$  and  $\langle \mathbf{v}_2 \rangle$  are determined numerically by solving the time harmonic first order- and the  
19 second order- acoustic perturbation of the continuous and the Navier-Stokes equations.  
20 Generally, the gravitational and buoyancy forces are negligible. Based on Newton's second law  
21 of motion, the governing equation for the particle movement can be written [47],

$$22 \quad \frac{d(m_p \mathbf{v}_p)}{dt} = \mathbf{F}^{\text{rad}} + \mathbf{F}^{\text{drag}} \quad (4)$$

23 where  $m_p$  is the microparticle mass. The net force of the  $\mathbf{F}^{\text{rad}}$  and  $\mathbf{F}^{\text{drag}}$  determines the  
24 trajectory of the suspended microparticles in the fluid and the microparticles trajectories  $\mathbf{v}_p$  can  
25 be solved by combining Eqs. 2-4. The inertia of the particles is generally neglected because the

1 characteristic time of acceleration is small in comparison to the time scale of the motion of the  
2 particles [46]. Thus,

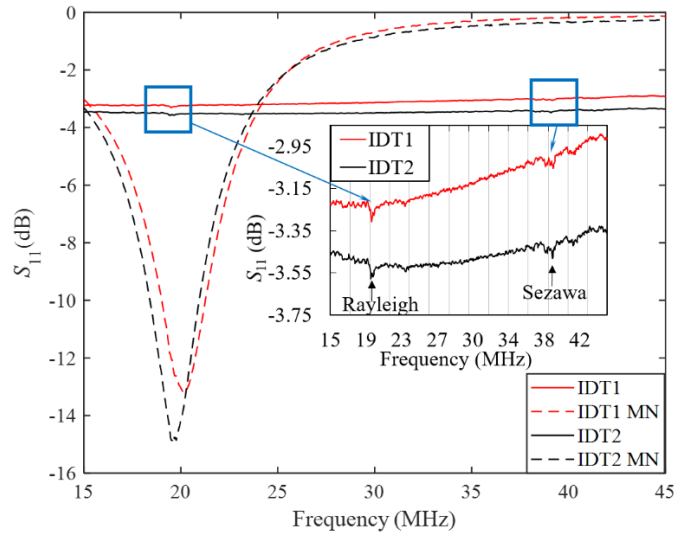
$$3 \quad \mathbf{v}_p = \frac{\mathbf{F}^{\text{rad}}}{6\pi\mu a} + \langle \mathbf{v}_2 \rangle \quad (5)$$

4  $\mathbf{F}^{\text{rad}}$  and  $\mathbf{F}^{\text{drag}}$  scale differently with particle radius;  $\mathbf{F}^{\text{rad}}$  is proportional to the volume of the  
5 particles ( $a^3$ ), whereas  $\mathbf{F}^{\text{drag}}$  is proportional to the radius of the particles. Thus, a particle  
6 transition size,  $d_c$ , exists, which determines whether the exerted force on the microparticle is  
7  $\mathbf{F}^{\text{rad}}$  dominated, i.e., the particle moves towards PN / ANs when  $a > d_c$ , or  $\mathbf{F}^{\text{drag}}$  dominated,  
8 i.e., the particle moves in a pattern of streaming vortex ( $a < d_c$ ) [48]. Given the parameters of  
9 the above GaNAT, the transition size  $d_c$  for the polystyrene microspheres was calculated to be  
10 0.8  $\mu\text{m}$  using the equations in Ref [49]. Microspheres larger than 0.8  $\mu\text{m}$  are driven mainly by  
11  $\mathbf{F}^{\text{rad}}$  inside the microchannel, otherwise they will be mainly driven by  $\mathbf{F}^{\text{drag}}$ .

## 13 4. RESULTS AND DISCUSSION

### 14 4.1 The characterization of the GaNAT

15 The transfer functions of the two IDTs in terms of  $S_{11}$  (reflection coefficient) with and without  
16 the matching networks are denoted by the solid lines in Fig. 4. The inset shows the zoom-in  
17 spectra of  $S_{11}$  parameters, where the device shows two peaks at 19.4 MHz and 38.9 MHz  
18 corresponding to the Rayleigh and Sezawa modes, respectively. By applying the matching  
19 networks, as the  $S_{11}$  spectra denoted by the dashed lines, the minimum  $S_{11}$  of the two IDTs on  
20 Rayleigh mode were reduced from -3.3 dB to -13.2 dB and from -3.6 dB to -14.9 dB,  
21 respectively. The addition of the matching networks significantly reduces the power reflection  
22 of the IDTs, which can effectively assist the operation of the GaNAT.

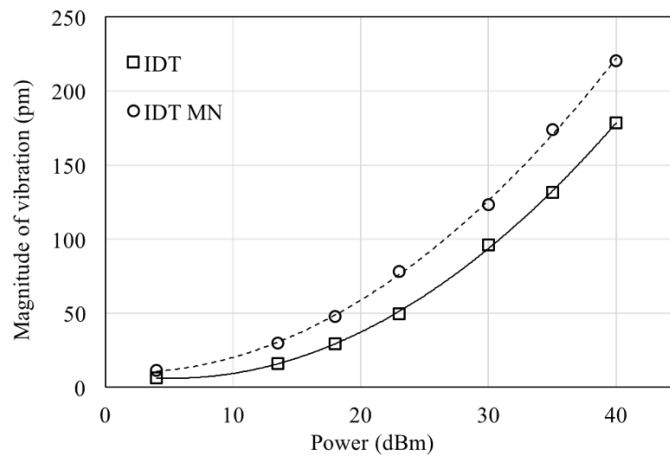


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2 Fig. 4. The reflection parameter ( $S_{11}$ ) of the GaNAT with the matching networks (MNs) and without the MNs. The  
 3 inset is the  $S_{11}$  spectra of the GaNAT without the MNs, showing both the Rayleigh and Sezawa modes.

4

5 Fig. 5 shows the magnitude of SAW vibration produced by the GaNAT with and without the  
 6 matching networks at various input powers. The use of the matching networks in the GaNAT  
 7 considerably increased the amplitude of the SAW, e.g. the maximum magnitudes of the SAW  
 8 at the maximum power of 40 dBm were found to be 220.6 pm and 178.4 pm with and without  
 9 the matching networks, respectively.

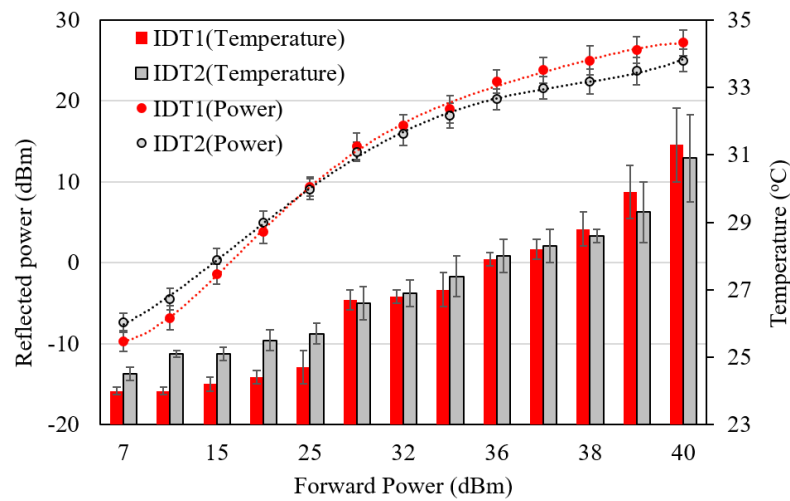


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11 Fig. 5. The magnitude of SAW vibration produced by the GaNAT with and without the MNs.

12 The relationship between the incident and reflected powers of the GaNAT is shown in Fig. 6,  
 13 together with the device temperatures at various input powers measured after thermal  
 14 stabilization. The reflected power accounts for  $\sim 3.2\%$  of the incident power which indicates an

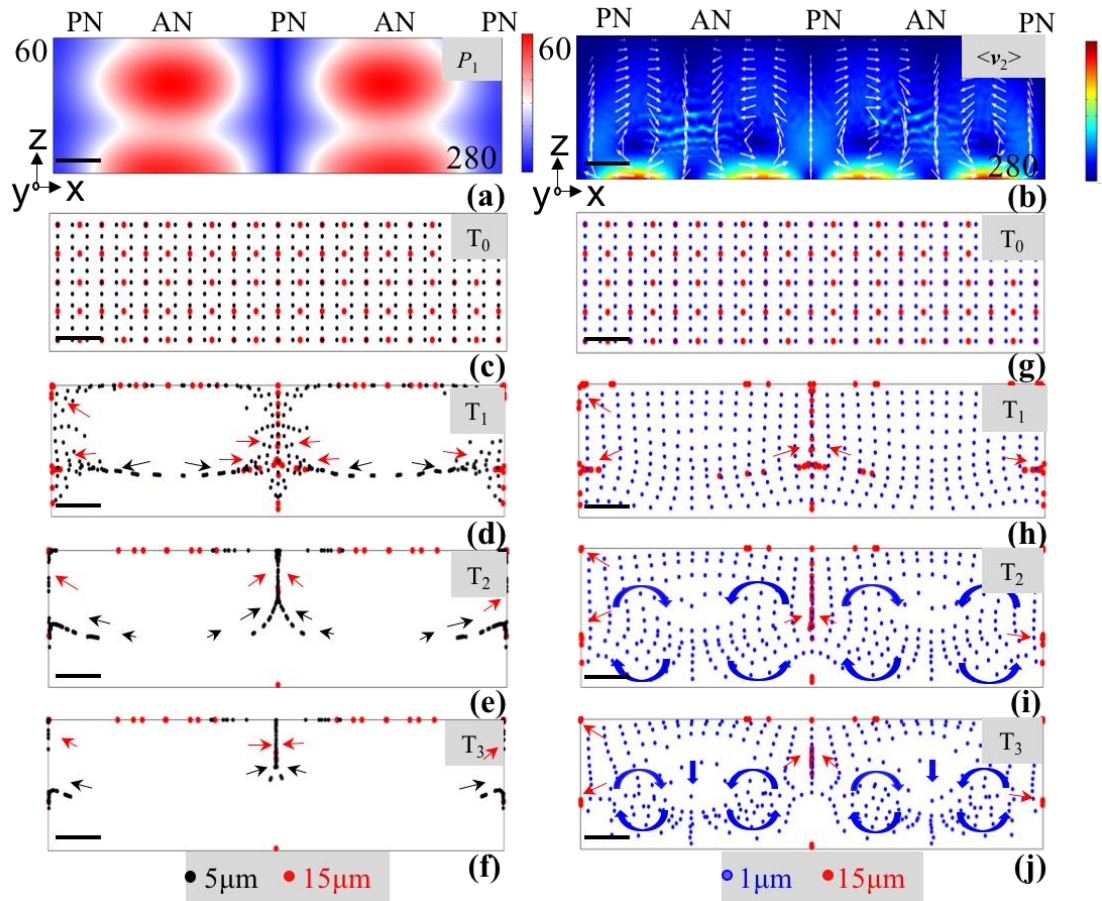
1 efficient energy conversion was achieved by adding the matching networks to the GaNAT [50].  
 2 The temperature on the IDTs is found increasing from  $\sim 24^\circ\text{C}$  to  $\sim 32^\circ\text{C}$  when the input power  
 3 increased from 7 dBm to 40 dBm. The temperature is gradually increased when the applied  
 4 power is increased (30 dBm to 40 dBm) indicating that the high thermal conductivities of the  
 5 thin film GaN and sapphire substrate facilitate efficient heat dissipation through the materials.  
 6 The good thermal stability can simplify system cooling and keep the sample temperature during  
 7 the operation using the GaNAT below the biological limit.



8  
 9 Fig. 6. Power evaluation of the GaNAT shows a high energy conversion on the device when using the matching  
 10 networks. The temperature rises of the IDTs at different input powers are within the biological limits.

## 12 4.2 Numerical analysis of pressure and trajectory of microparticles

13 As shown in Fig. 7a, three PNs and two ANs are generated inside the microchannel. The  
 14 corresponding time-averaged second-order velocity  $\langle v_2 \rangle$  is shown in Fig. 7b with four  
 15 streaming vortices formed. This boundary-driven streaming is induced by the substrate  
 16 vibration with the maximum streaming velocity close to the bottom substrate (the four high  
 17 velocity regions at the bottom in Fig. 7b). The resultant gradients of the streaming velocity in  
 18 both  $x$  and  $z$  directions lead to the streaming vortex moving from the near field to the far field,  
 19 and its directions are indicated by the white arrows as shown in Fig. 7b. At the PNs the  
 20 streaming flows upward while at the ANs the streaming flows downward [51].



1

2 Fig. 7. Numerical simulation of the acoustic pressure, time-averaged second-order velocity and microparticles  
 3 trajectories of the GaNAT device. (a) The first-order acoustic pressure  $p_1$  inside the microchannel. (b) The time-  
 4 averaged second-order velocity field  $\langle v_2 \rangle$ . (c-f) The microparticle trajectories of the mixture of 5  $\mu\text{m}$  (black) and  
 5 15  $\mu\text{m}$  (red) at a series of time points. (g-j) The microparticle trajectories of the mixture of 1  $\mu\text{m}$  (blue) and 15  $\mu\text{m}$   
 6 (red) at a series of points. The scale bar is 20  $\mu\text{m}$ .

7

8 To investigate the trajectory of microparticles with different sizes inside the GaNAT, two  
 9 batches of microparticle mixtures, e.g., 15  $\mu\text{m}$  and 5  $\mu\text{m}$ , as well as 15  $\mu\text{m}$  and 1  $\mu\text{m}$ , were used  
 10 for simulation, and the obtained results shown in Figs. 7c-7f, and Figs. 7g-7j, respectively. For  
 11 the mixture of 15  $\mu\text{m}$  and 5  $\mu\text{m}$  microparticles, since they are both larger than the transition size  
 12 of 0.8  $\mu\text{m}$ , their motions are mainly driven by the  $F^{\text{rad}}$ , thus the particles are moving towards  
 13 the nearest PNs. Two transient moments shown in Figs. 7d and 7e clearly indicate that the 15  
 14  $\mu\text{m}$  microparticles are moving faster than 5  $\mu\text{m}$  ones. For example, there are considerable  
 15 amounts of 5  $\mu\text{m}$  microparticles still moving in the channel while most of 15  $\mu\text{m}$  microparticles

1 have already arrived at the PNs in the moment shown in Fig.7e. Both the microparticles are  
2 able to be aggregated at the PNs as their final positions given enough time as shown in Fig. 7f.  
3 Whereas for the mixture of 15  $\mu\text{m}$  and 1  $\mu\text{m}$  microparticles, since the latter ones are very close  
4 to the transition size, their motion is driven by both the  $F^{\text{rad}}$  and  $F^{\text{drag}}$ , thus resulting in strong  
5 streaming vortex as shown in Fig. 7i, while 15  $\mu\text{m}$  microparticles are already aggregated at the  
6 PNs. Results also show that 1  $\mu\text{m}$  microparticles only follow the streaming pattern to achieve  
7 partial aggregation phenomenon as shown in Fig. 7j. It is worthwhile noting that the numerical  
8 simulation results of the GaNAT show similar streaming patterns as those achieved by  
9 acoustofluidic devices made of  $\text{LiNbO}_3$  working at a frequency of  $\sim 6$  MHz [46, 47]. The only  
10 difference is that a smaller input power is required for the  $\text{LiNbO}_3$ -based SAW devices owing  
11 to their large electromechanical coupling coefficient.

12

### 13 **4.3 Experimental validation of particle manipulation using GaNAT**

14 For the mixture of 15  $\mu\text{m}$  and 5  $\mu\text{m}$  polystyrene microspheres (Fig. 8a-d), the microscope  
15 images were captured on 0 s, 5 s, 15 s, and 1 min after the application of SSAWs. 5  $\mu\text{m}$   
16 microspheres are found to move slower than 15  $\mu\text{m}$  microspheres towards the PNs due to the  
17 smaller  $F^{\text{rad}}$ . This can be seen in Fig. 8b, in which 15  $\mu\text{m}$  microspheres are already aggregated  
18 at PNs after 5 s (red arrows) whereas a large number of 5  $\mu\text{m}$  microspheres are still dispersed  
19 across the microchannel (black arrows). On 15 s, both sizes of microspheres are aggregated at  
20 the PNs with a notable number of 5  $\mu\text{m}$  microspheres are still moving towards the PNs (Fig.  
21 8c). The experimental results show that both sizes of particles can be effectively actuated by  
22 the  $F^{\text{rad}}$  to migrate towards PNs. Due to their size differences, 5  $\mu\text{m}$  and 15  $\mu\text{m}$  experience  
23 different magnitudes of acoustic radiation forces, thus achieving different moving velocities.  
24 Most of these microspheres can be found to form three traces of microspheres at the PNs as  
25 their final positions at  $\sim 1$  min, which prove that particles larger than the transition size are

1 mainly driven by  $F^{\text{rad}}$  in the GaNAT. The experimental results are in good agreements with the  
2 simulation ones shown in Figs. 7c-7f.  
3  
4 For the mixture of 15  $\mu\text{m}$  and 1  $\mu\text{m}$  microspheres (Fig. 8e-h), most of the 15  $\mu\text{m}$  microspheres  
5 are quickly migrated to the PNs after 5 s and well aligned after 15 s (red arrows). However, 1  
6  $\mu\text{m}$  microspheres show no obvious aggregation pattern in 5 s (Fig. 8f) which agrees with Fig.  
7 7h. After 15 s, 1  $\mu\text{m}$  microspheres experience a notable streaming effect and form four  
8 streaming vortices as shown in Fig. 8g (see blue arrows). It is worthwhile to note that two traces  
9 of 1  $\mu\text{m}$  microspheres are formed next to the center PNs after 1 min (Fig. 8h), which are also  
10 well predicted by the simulation as shown in Fig. 7j. The times required to drive different sizes  
11 to arrive their final positions are different, which demonstrates the potential of using the  
12 GaNAT for separating microspheres or cells with different sizes or mechanical properties.  
13 During the experiment, the GaNAT showed its robustness in high power handling and thermal  
14 stability, which can benefit for thermophoresis applications with the biological samples.

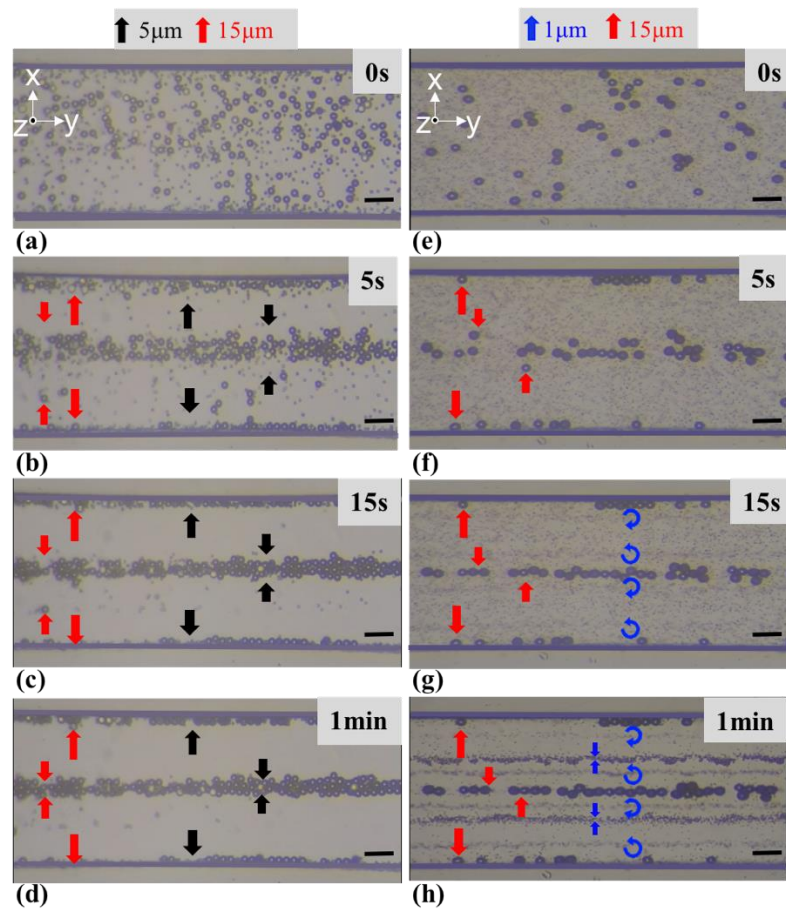


Fig. 8. Experimental results of the mixture of 5  $\mu\text{m}$  and 15  $\mu\text{m}$  polystyrene microspheres and the mixture of 1  $\mu\text{m}$  and 15  $\mu\text{m}$  polystyrene microspheres. (a-d) The distribution of 5  $\mu\text{m}$  and 15  $\mu\text{m}$  microspheres driven by the SSAW field within the microchannel between 0 s to 1 min. (e-h) The distribution of 1  $\mu\text{m}$  and 15  $\mu\text{m}$  microspheres driven by the SSAW field within the microchannel between 0 s to 1 min. The scale bar is 50  $\mu\text{m}$ .

## 5. CONCLUSION

In summary, for the first time, thin film GaN-based acoustofluidic chip was developed for manipulating microparticles, which proved that GaN is an alternative piezoelectric material for producing SAWs for efficient manipulation of microparticles, despite that the electromechanical coupling coefficient of GaN is lower than that of the LiNbO<sub>3</sub>. Grown on sapphire, GaN thin film is a thermally robust material for high power SAW generation. By using matching networks, the GaNAT demonstrated efficient SAWs produced on the surface with less power reflected, which is invaluable to handle biological samples when using high input power for high-throughput applications. The thermal performance can be further



1 improved by replacing the sapphire substrate with either SiC or Si as used in many GaN  
2 electronic device applications. The experimental results of particle manipulation using the  
3 GaNAT were well predicted by the simulation results. By testing with two mixtures of  
4 microspheres, the GaNAT was proven to be able to be used as an acoustic tweezer, and more  
5 importantly, with the potential in making acoustofluidic devices to monolithically integrate  
6 with compound semiconductors to allow miniature, robust, and multi-physical applications.

7

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