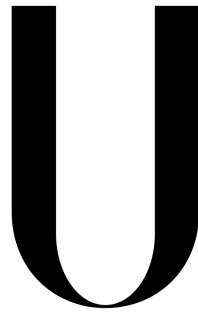


UNIVERSIDADE DE LISBOA
FACULDADE DE CIÊNCIAS
DEPARTAMENTO DE FÍSICA



LISBOA

UNIVERSIDADE
DE LISBOA

Embedded Platform for Electrical Neural Stimulation

Francisco Pargana de Melo

Orientadores

Prof. Dr. Timothy Constandinou

Prof. Ricardo Salvador

Mestrado Integrado em Engenharia Biomédica e Biofísica

Perfil em Engenharia Clínica e Instrumentação Médica

DISSERTAÇÃO

2015

Resumo

Atualmente, o número de tecnologias baseadas em neuro-estimulação está em crescimento, crescimento este que é promovido pelo facto de a neuro-estimulação ser uma área de investigação de elevado interesse devido às várias áreas de possível aplicação, tais como a terapia e tratamento, reabilitação e próteses. Na área da terapia e tratamentos, a possível aplicação da neuro-estimulação está relacionada com a neuro-regulação de órgãos do corpo humano, aplicação que tem sido vista já no campo dos distúrbios do sistema nervoso, tais como a doença de Parkinson e a epilepsia, no tratamento de dor crónica, no controlo do funcionamento cardíaco – no qual se insere uma das tecnologias mais conhecidas, o *pacemaker* – e está ainda a ser investigada para o controlo da libertação de insulina e a absorção renal de sais [1]. Na área da reabilitação, a aplicação da neuro-estimulação tem sido vista em casos de lesões na medula espinal onde a utilização da técnica de estimulação elétrica funcional, ou *FES* de *Funcional Electrical Stimulation*, resultou na recuperação de algumas funções motoras e de controlo de certos órgãos [2]. Relativamente à área das próteses, a neuro-estimulação tem um papel muito importante principalmente no desenvolvimento de próteses funcionais, permitindo que estas próteses não só reajam a informação vinda do sistema de nervoso, realizando os movimentos desejados pelo utilizador, como também forneçam informação ao mesmo, permitindo assim que haja um mecanismo de *feedback* da prótese, aumentando assim a restituição que esta pode dar ao seu utilizador, tanto a nível funcional como emocional. Uma das mais conhecidas próteses que recorrem à neuro-estimulação é o implante coclear que permite uma recuperação parcial da capacidade auditiva recorrendo para isso a um conjunto de microfones no ouvido externo que deteta o som e o transmite à unidade de processamento que por sua vez transforma o som em impulsos elétricos que são direcionados para eléctrodos no interior da cóclea e que irão estimular os nervos auditivos [3].

A neuro-estimulação é então um procedimento baseado na estimulação de células excitáveis, como os neurónios, recorrendo para isso à utilização de eléctrodos, com o objetivo de iniciar ou inibir um potencial de ação. Esta possibilidade de iniciar um estímulo nervoso através de estímulos externos deve-se ao facto da ativação e propagação de um sinal neural ser um fenómeno eletroquímico. Este fator torna possível o desenvolvimento

de tecnologias que resultem numa maior, ou menor, recetividade da célula a um estímulo através da promoção de alterações do meio em que estão inseridas as células excitáveis ou de propriedades da membrana das mesmas.

O desenvolvimento de tecnologias que recorram à neuro-estimulação está dependente de um estudo profundo dos tipos e estratégias de estimulação de forma a obter a estratégia que seja mais eficaz, segura e eficiente, sendo que esta varia de situação para situação, dependendo de fatores como o local de aplicação e mesmo o resultado que se espera do estímulo. Por estes motivos têm de ser realizados estudos comparativos válidos entre estratégias de estimulação e, para um estudo deste tipo ser valido, os vários estudos devem ser feitos nas mesmas condições com distâncias temporais preferencialmente curtas. Assim sendo, no âmbito da neuro-estimulação recorrendo a estímulos eléctricos, criou-se a necessidade de desenvolver sistemas que permitissem uma mais rápida variação dos parâmetros de estimulação comparativamente à montagem experimental clássica. De forma a cumprir estes requisitos, vários sistemas de rápida configuração de parâmetros tem vindo a ser propostos.

O projeto relatado nesta Tese de Mestrado, desenvolvido durante um estágio de seis meses no *Centre for Bio-Inspired Technologies, Imperial College London*, apresenta-se então como uma plataforma de neuro-estimulação eléctrica para a realização de estudos comparativos tendo em vista a otimização da estratégia de estimulação, com o objetivo de ser uma versão melhorada dos sistemas já disponíveis. Esta plataforma é composta por três principais componentes: uma interface utilizador-sistema, que permite ao utilizador configurar a estimulação como pretende controlando características como o tipo de onda, a amplitude, a duração, a frequência, entre outros; um microcontrolador e uma placa de estimulação, em que o primeiro controla o segundo de acordo com o que foi configurado pelo utilizador sendo que a placa têm a responsabilidade de gerar e aplicar um estímulo eléctrico. O principal objetivo deste projeto era então desenvolver uma plataforma de neuro-estimulação eléctrica capaz de gerar e aplicar uma estimulação eléctrica bipolar com capacidade de equilíbrio de cargas, podendo fazê-lo através de quatro canais de estimulação. Ao mesmo tempo era objetivo que esta fosse pequena, de baixo custo, eficaz, eficiente, de fácil utilização proporcionando um maior leque de possibilidades de configuração comparativamente aos sistemas já desenvolvidos e que pudesse também ser facilmente recriado, alterado e, eventualmente, melhorado.

Os resultados obtidos de testes realizados demonstraram que esta plataforma opera corretamente nos dois principais aspetos do seu funcionamento, nomeadamente a capacidade de gerar uma estimulação de acordo com todos os parâmetros tal como configurados pelo utilizador e a capacidade de cumprir os propósitos de equilíbrio de cargas após estimulação, em todos os tipos de ondas definidos.

Existem no entanto ainda algumas limitações no funcionamento da plataforma. Estas limitações estão relacionadas com a amplitude máxima de estimulação que o sistema é capaz de aplicar, mais especificamente a amplitude máxima do *output* do DAC utilizado e também a amplitude máxima que o amplificador operacional escolhido consegue por no seu *output*; com a existência de algumas imprecisões temporais na aplicação do estímulo, resultantes do tempo de execução de algumas funções por parte do microcontrolador; com o consumo energético e ainda o facto de a ligação entre o computador e o microcontrolador ser feita através de um cabo USB, o que limita a mobilidade que se pode ter durante o trabalho experimental.

Comparativamente a plataformas de estimulação elétrica configuráveis existentes, o sistema aqui desenvolvido apresenta diversas vantagens. Para além de vantagens como baixo custo e facilidade de recriação, esta plataforma tem também um maior número de parâmetros da estimulação que o utilizador pode configurar e também permite uma estimulação através de quatro canais, de três formas diferentes: utilizando apenas um canal, utilizando mais do que um canal ao mesmo tempo ou ainda mais do que um canal de forma sequencial. No entanto, alguns dos sistemas já existentes não apresentam as limitações acima referidas e como tal os desafios futuros desta placa passam por ultrapassar essas limitações.

Palavras-Chave: Estimulação Neuronal, Estudo de Estratégias de Estimulação, Sistema para Configuração de Estimulação Elétrica, MATLAB GUI, Microcontrolador KL26Z, Placa de Estimulação.

Abstract

Nowadays, neurostimulation technologies have grown to reach a wide range of applications including therapy and treatment, rehabilitation and prosthetics and its range continues to grow as it still represents an interesting area of research.

Neurostimulation is based on stimulation of excitable cells, such as nerve cells, through the use of electrodes, with the purpose of achieving initiation or inhibition of an action potential. This interaction is possible due to the electrophysiological base of activation and propagation of a neural signal. This neural signal characteristic makes it possible to use external technologies to promote changes in the nerve cell membrane voltage potential or the environment surrounding it, which can lead to the initiation of a neural signal in the cell or simply to a higher, or lower, receptivity of the cell to a stimulus.

The use of neurostimulation technologies in referred areas and future possibility of use in other applications depends on research developments. An important point of this research is the stimulation strategy, more specifically, the characteristics that a stimulation pulse should have to optimize results towards the intended objective and minimize safety risks.

The present thesis reports a project developed during an internship at the Centre for Bio-Inspired Technologies, Imperial College London which consists in designing and building a full system for the study of stimulation strategies. This full system includes a user interface in a computer, so that the user can choose the stimulus characteristics, such as waveform and amplitude, and define the intended strategy, such as repetition rate and inter-stimulus increasing or decreasing rate; and a microcontroller for control of stimulus application through a front-end stimulation-output circuit, which will be responsible for generation of programmed current-controlled stimulus.

The measurement results verify that the main objectives of this project were accomplished, namely, the capacity to generate a stimulation that meets the parameters as configured by the user and the capacity to carry a charge-balanced stimulation in all the preset waveforms.

However, some limitations were also found related namely with the maximum stimulation amplitude, the small time inaccuracy during stimulation, the power consumption and the fact that connection between the computer and microcontroller is done via USB, limiting the mobility of a experimental procedure using this system.

The system developed here presents some advantages compared to existing systems, such as low cost, easy to build, higher number of parameters that can be configured and can apply stimulation through four channels and do it either with only one, with two or more at the same time or with two or more sequentially. However some of these existing systems do not present some of the limitations mentioned and the challenge on the future of this platform is to overcome these limitations.

Keywords: Neural Stimulation, Study of Stimulation Strategies, Platform for Configurable Electric Stimulation, MATLAB GUI, Microcontroller KL26Z, Front-End Stimulation Board.

Acknowledgements

First of all, I would like to say a great thank you to Professor Timothy Constandinou for this amazing opportunity to do my internship at the Imperial College London and also for all the help and guidance given.

I would also like to thank Dr. Yan Liu and Dr. Song Luan for all the help and guidance given through the whole internship. Their help was of utmost importance to achieve the goal of this internship.

A thank you also to Deren Barsakcioglu, for his help during the development of my work, and to Izabella Wojcicka-Grzesiak, whose patience and help was very important to simplify various issues that arose during my stay.

I would like to thank Professor Ricardo Salvador for all the help and support given during the internship and towards the accomplishment of this thesis.

I would also like to thank the people of the Bio-Inspired group, who were very welcoming, always very friendly and were always available to help me.

A great thank you to my friends Filipa Guerreiro and João Tourais for all the companion and good time during my stay in London, to my friend and roommate Nádia Vilhena for helping to make our home in London a cheerful Portuguese home and especially to my lab partner and roommate Célia Fernandes, whose help, patience and friendship were a great support and very important for me, both at work and at home.

I would also like to express the greatest and most special gratitude to my family for all the support, especially for my parents, Sofia e António. Not only for making possible for me to do another internship outside Portugal, for all the support, both moral and financial, and all the help given, but also for everything that is behind, for the academic and personal path that you gave me which brought me here.

Contents

Resumo	i
Abstract	v
Acknowledgements	vii
List of Tables	xi
List of Figures	xiii
Abbreviations	xvii
1 Introduction and Objectives	1
1.1 Objectives	2
1.2 Thesis Structure	3
2 Fundamentals of Neural Stimulation	5
2.1 Neuroanatomy and Neurophysiology	5
2.1.1 Neural Cell	6
2.1.2 Action Potential Generation	7
2.2 External Electrical Neuron Stimulation	12
2.2.1 Electrical Stimulation Principles	12
2.2.2 Electrical Stimulation Application Techniques	16
3 State-of-the-Art of User Configurable Neural Stimulation Technologies	21
4 Software Development	29
4.1 MATLAB-based User-System Interface	29
4.1.1 Choosing between Different Waveforms	31
4.1.2 Configuring Pulse Parameters	34
4.1.3 Configuring Interphasic Delay	40
4.1.4 Configuring Biphasic Ratio	40
4.1.5 Configuring Pulse Repetition and Stimulation Duration	40
4.1.6 Configuring Channels	42
4.1.7 Configuring Maximum Amplitude Voltage	44
4.1.8 Overall Operation and Communication with Microcontroller	45
4.2 <i>Freescale</i> Microcontroller FRDM-KL26Z	48

5	Hardware Development	51
5.1	Requirements	52
5.2	Components	52
5.2.1	Power Supply Circuits	53
5.2.2	Reference Voltage Circuits	56
5.2.3	Stimulation Application Circuits	56
5.2.4	Microcontroller Connections	61
5.3	PCB Design Characteristics	63
5.4	Full Neural Stimulation Board and MCU Compatibility	65
6	Overall Stimulation System Operation	69
6.1	System Analysis	70
6.2	Charge Balancing Analysis	76
7	Conclusion and Future Work	83
	References	87
A	MATLAB Code	91
A.1	User-System Interface Code	91
B	Microcontroller Code	211
B.1	Main Function Code	211

List of Tables

6.1	System Analysis measurements.	74
6.2	Timing measurements.	77
6.3	Charge Balance measurements.	81
7.1	Specifications of the developed platform.	85
7.2	Comparison between this work and existing systems.	86

List of Figures

1.1	Prosthesis Control and Feedback through Neural Signal.	2
2.1	Representation of Neural Cell.	7
2.2	Action Potential Propagation throughout a Nerve Cell.	8
2.3	Variation of Membrane Potential during an Action Potential.	9
2.4	Circuit Model of Cell Membrane.	10
2.5	Electrode-Electrolyte Interface Representation (a) and Circuit Model (b).	12
2.6	Electrode-Electrolyte and Tissue Interface Circuit Model in a Bipolar Montage.	13
2.7	Biphasic Square Pulse Stimulation.	15
2.8	Rectangular Pulse.	18
2.9	Quasi-Trapezoidal Pulse.	18
2.10	Tri-Exponential Pulse.	19
2.11	Sub-threshold Pre-Pulse followed by Pulse.	19
2.12	Bursting Strategy Stimulation.	20
4.1	MATLAB GUIDE interface.	30
4.2	Pushbutton function code.	30
4.3	Waveform Type pop-up menu.	32
4.4	Rectangular waveform-based pulse.	33
4.5	Amplitude and Width edit boxes.	34
4.6	Amplitude and Width edit boxes with secondary parameters locked.	35
4.7	Bi-level Lilly waveform-based pulse.	35
4.8	Edit boxes for Quasi-Trapezoidal exponential characteristics.	35
4.9	Edit boxes for Tri-Exponential exponential characteristics.	36
4.10	Decay Width and Resolution edit boxes.	37
4.11	Quasi-Trapezoidal waveform-based pulse.	37
4.12	Tri-Exponential waveform-based pulse.	39
4.13	Tri-Exponential waveform-based pulse.	39
4.14	Interphasic Delay edit box.	40
4.15	Biphasic Ratio edit box.	40
4.16	Repetition Rate and Repetition Amplitude Ratio edit boxes.	41
4.17	Stimulation Duration edit box.	41
4.18	Axes area and Plot pushbutton.	42
4.19	Channel pop-up menu.	42
4.20	Firing Type pop-up menu.	43
4.21	Time Lag edit box.	43
4.22	Electrode Impedance panel.	44

4.23	Electrode Impedance dialog window.	45
4.24	Warning window when no Electrode Impedance value is input in dialog window.	45
4.25	Full User-System Interface.	46
4.26	User-System Interface Operation Diagram.	46
4.27	Upload pushbutton.	47
4.28	Waiting Bar window.	47
4.29	Apply and Reset pushbuttons.	48
4.30	COM Port pop-up menu.	48
4.31	MCU Operation Diagram.	49
5.1	<i>Altium</i> 3D vision from the board with highlighted components	53
5.2	DC/DC converter circuit schematic.	54
5.3	Placement on the board of VBAT power supply header (black), VDD and VSS jumpers (blue) and Vdd/VssALT alternative supply header (red).	55
5.4	Schematic of DAC's power supply circuit.	55
5.5	Schematic of DAC's reference voltage circuit.	56
5.6	DAC schematic representation.	57
5.7	<i>Cadence</i> OrCAD schematic of V-to-I Converter.	58
5.8	ADG436 switch scheme.	59
5.9	Schematic of circuit with V-to-I Converter and Switch – single stimulation channel.	59
5.10	Schematic of a single stimulation channel circuit with converter, switches and electrode impedances.	60
5.11	<i>Altium</i> schematic of a single stimulation channel circuit.	60
5.12	Electrode placement sites on board.	61
5.13	Input and Output Connection on whole Stimulation Board.	62
5.14	Board Connections on <i>Altium</i>	64
5.15	Layers connections.	64
5.16	3D image of Stimulation Board.	65
5.17	Tracks in the real board without any components.	66
5.18	Full Stimulation Board, with all components.	66
5.19	FRDM-KL26Z connections with Stimulation and Recording Board.	67
6.1	Overall Operation of the Embedded Platform for Neural Electrical Stimulation.	69
6.2	Measured wave for rectangular shaped stimulation.	71
6.3	Measured wave for bi-level Lilly shaped stimulation.	72
6.4	Measured wave for quasi-trapezoidal shaped stimulation	72
6.5	Measured wave tri-exponential shaped stimulation.	73
6.6	Measured wave for bursting strategies based stimulation.	73
6.7	Rectangular shaped repetitive stimulation.	74
6.8	Rectangular shaped repetitive stimulation with amplitude limitation.	75
6.9	Synchronous rectangular-based stimulation.	76
6.10	Asynchronous rectangular-based stimulation.	77
6.11	Intervals for timing measurement.	78
6.12	Charge-balancing results for Rectangular shaped stimulation.	78
6.13	Charge-balancing results for Bi-level Lilly shaped stimulation.	79

6.14	Charge-balancing results for Quasi-Trapezoidal based stimulation.	80
6.15	Charge-balancing results for Tri-Exponential based stimulation.	80
6.16	Charge-balancing results for Bursting Strategies based stimulation.	81

Abbreviations

AC	A lternating C urrent
ADC	A nalog-to- D igital C onverter
ASIC	A pplication S pecific I ntegrated C ircuits
CMOS	C omplementary M etal- O xide- S emiconductor
DAC	D igital-to- A nalog C onverter
DC	D irect C urrent
DCU	D igital C ontrol U nit
FSM	F inite S tate M achine
GUI	G raphical U ser I nterface
GUIDE	G raphical U ser I nterface D evelopment E nvironment
IC	I ntegrated C ircuit
LDO	L ow- D rop O ut R egulator
MCU	M icro C ontroller U nit
OLED	O rganic L ight- E mitting D iode
OpAmp	O perational A mplifier
PCB	P rinted C ircuit B oard
PIC	P rogrammable I nterface C ontroller
RF	R adio- F requency
SAR	S uccessive A pproximation R egister
SMD	S urface- M ount D evice
SPDT	S ingle- P ole D ouble- T hrow
SPI	S erial P eripheral I nterface
SU	S timulation U nit
THD	T otal H armonic D istortion
USB	U niversal S erial B us

Chapter 1

Introduction and Objectives

Neurostimulation technologies are an area of research with a variety of applications, which range from therapy, treatment and rehabilitation to prostheses. Therapy and treatment applications of these technologies are related to neural regulation of the human body's organs and have been seen in the field of brain disorders – both in movement, such as Parkinson's disease, and psychological disorders, for example epilepsy –, in chronic and untreatable pain, in cardiac control – pacemaker – and are also being studied for the control of insulin release and renal salt absorption [1]. Rehabilitation has been seen in cases of spinal cord disorders, such as Spinal Cord Injury, where some motor and control functions are restored through use of Functional Electrical Stimulation [2]. Prosthetic applications of neurostimulation technologies are related to the use of devices to replace malfunctioning motor or sensory neural functions and in this case neurostimulation is used for the transmission of information from prosthesis to the user's nervous system, as represented by the green line in Figure 1.1. One of the most well-known prosthetic applications of neurostimulation is the cochlear implant, which is composed by a first stage of microphones that detect the sounds, then a processing unit that transforms the sound in electric impulses and transmits them to an electrode array inside the cochlea which is responsible for electric stimulation of auditory nerve fibers [3].

For the aforementioned applications, a careful study of stimulation strategies has to be done so that stimulation can be effective, safe and also energy efficient. Effectiveness varies with location where stimulation is applied and also for the purpose it is intended. For these reasons, valid comparative studies between stimulation strategies have to be

made and for such studies to be valid, a faster capacity of variation of strategy parameters is required compared to the classical methods for study of stimulation. In order to meet those needs, numerous alternative methods have been proposed. The project reported in this Master thesis is presented as an improvement of the existent alternative methods for these comparative studies of stimulation strategies.

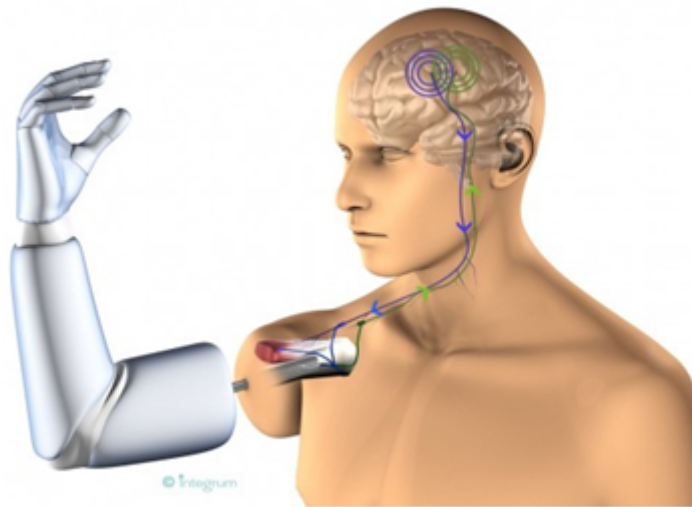


FIGURE 1.1: Prosthesis Control and Feedback through Neural Signal [4].

1.1 Objectives

In this thesis we describe the development of a stimulation system for the study of stimulation strategies that can present itself as an improvement of existing methods that already allow comparative studies of stimulation strategies. In more specific terms, this project is an embedded platform for electrical neural stimulation that allows its user to control the parameters of stimulation, including waveform shape, amplitude, frequency, width and others that will be explained ahead. This system is then capable of generating and applying that stimulation through four different channels. This stimulation system is composed of three main components: a user-system interface, a microcontroller and a front-end circuit board, whose development and operation is described throughout this thesis. The purpose of this project is to obtain a small, low-cost, effective, efficient and easy-to-use stimulation platform that can also be easily recreated, changed and, eventually, improved.

1.2 Thesis Structure

The thesis here presented is divided in six main chapters. The first main chapter is Chapter 2, “Fundamentals of Neural Stimulation”, where the principles behind neural stimulation are explained, namely the anatomy and physiology that lie under the functioning of the nervous system and also the mechanisms behind an external electrical stimulation.

In Chapter 3, “State-of-the-Art of User Configurable Neural Stimulation Technologies”, a state of art of user-controllable systems for electrical neural stimulation is made, including a description of main advantages brought to this field of investigation and also limitations attached to it.

Chapter 4, “Software Development”, is dedicated to the development and operation of the software part of the stimulation system. This chapter is divided in two sections: the first section focuses on the user-system interface, where it is described the options and parameters that user is able to configure, the operation of the interface behind the choices of the user and the interface side of interface-microcontroller communication; the second section focuses on the microcontroller side of interface-microcontroller communication and its operation.

In Chapter 5, “Hardware Development”, the development and operation of hardware part of the system, more specifically the ‘front-end’ circuit board, is described. This includes the requirements, schematics and simulations behind the development up to the schematics and sketches of resulting final board.

Chapter 6, “Overall Stimulation System Operation”, presents a discussion on the embedded platform created, with a specific focus on the results obtained using this system to apply different types of stimulation with different waveform parameters through different channels and on the system charge-balancing capacity.

Lastly, Chapter 7, “Conclusion and Future Work”, presents important conclusions on this project and also perspectives on future work. Following the last chapter are appendices related to Chapter 4, namely the code for the user-system interface, and to Chapter 5, namely the code for the main function of the microcontroller.

Chapter 2

Fundamentals of Neural Stimulation

The major principle of neurostimulation technologies is the activation of excitable neural tissue through use of electrodes. This type of activation of neural tissue is possible due to the electrochemical nature of neural communications in human body. Neural communication via electric pulses is possible due to a series of unique anatomic and physiological characteristics of cells that compose the nervous system, and particularly the neural cell. Thanks to these characteristics, these cells have the ability to receive, conduct and send electrical-based signals throughout the nervous system. These electrical-based signals are called action potentials, i.e., rapid oscillations of the transmembrane potential resulting from ionic currents. The following chapters thoroughly explain these fundamentals of neural stimulation, more particularly, anatomy and physiology behind neural communication, specifically the neural cell and mechanisms of action potential generation, and the mechanisms behind electrical neural stimulation.

2.1 Neuroanatomy and Neurophysiology

As stated previously, the basis of neurostimulation is the electrical nature of neural communication in the nervous system, whose base by its turn is the neural cell. In the following chapters an overview of both these bases is done, more specifically, the

neural cell structure and properties and the mechanisms behind the generation of action potentials.

2.1.1 Neural Cell

The neural cell, also known as neuron, is, as it was mentioned previously, the base of the neural communication and it consists of an electrically excitable cell composed by dendrites, a cell body, an axon and terminal branches, as it is presented in Figure 2.1. For example, the normal path of an electrical signal on the neuron starts by the reception from other cells via the dendrites which is then transmitted to cell body, the metabolic and processing centre, which then sends it through the axon – a fibre that can be surrounded by myelin sheaths with intermittent unmyelinated areas, called nodes of Ranvier, whose conformation allows a higher speed of propagation of electric signal – to the terminal branches where information is passed to other cell via a process called synapse. This direction of propagation is called orthodromic propagation. But signals can also propagate antidromically, i.e., from axon to dendrite. A synapse is an electrical or chemical process, depending on the way the signal is transmitted to the following cells, in which the electrical signal is transmitted from the presynaptic cell to the postsynaptic cell. In an electrical synapse, the electric signal passes from presynaptic to postsynaptic cell through channels that connect the cytoplasm from both cells. These channels are called gap junctions. In a chemical synapse, when the electrical signal coming from the axon reaches the terminal branches it causes a release of neurotransmitters which leave the cell to bond to receptors in the postsynaptic cells. The latter triggers a reaction in ion channels in the post-synaptic membrane which can lead to changes in its membrane potential. [5]

A very important characteristic of the neural cell is the presence on its cell membrane of transmembrane proteins, called ion channels and ion pumps. These proteins are crucial on the cell excitation process since they selectively allow ions to cross the cell membrane, since the phospholipidic layer is impermeable to ions, providing also a control of ion concentration gradient across the cell through ion permeability variations and also active transportation. This excitation process is behind electrical signal generation and propagation as it will be explained in the following chapter. [5]

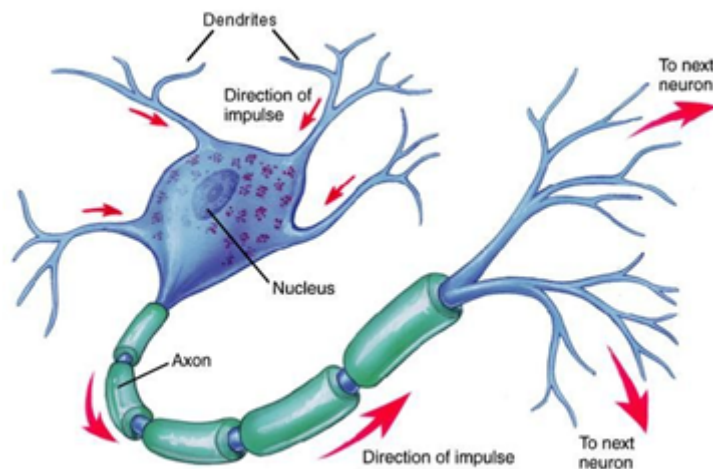


FIGURE 2.1: Representation of Neural Cell [6].

2.1.2 Action Potential Generation

In the absence of external changes, the neuron is found in a resting state where there is a difference between extracellular and intracellular ion concentrations. This difference is caused by a much higher presence of Sodium cations Na^+ and Chloride anions Cl^- on the outside of the cell than on the inside where there is a much higher presence of Potassium cations K^+ and negatively charged particles such as proteins or phosphate compounds. This difference of concentrations is mostly caused by sodium-potassium pumps existent in the neurons membrane since they promote, through active transport, the flux of potassium ions into the cell and sodium ions outside the cell. Besides sodium-potassium pumps, selective permeability of cell membrane also plays an important role in different concentrations since the flux of certain substances is done through active and passive ionic channels. [7]

Due to these different ionic concentrations inside and outside the cell membrane, the inside is a positively-charged medium while the outside is a negatively-charged medium, which creates a voltage potential across the membrane, called resting potential. This resting potential is then a negative value, usually of about -70 mV. When a stimulus is applied to the cell, a variation of this potential occurs originating a local potential on the membrane. If this potential reaches a certain threshold, for example -55 mV – see Figure 2.3 – a sharp increase of the membrane potential occurs, followed by a rapid decrease to restore the resting potential. This is called an action potential and it obeys

to an “all-or-none” principle, which defines that it only occurs if necessary conditions are verified, i.e., only if stimulus intensity is higher than referred threshold. In this situation, other membrane potential variations occur in adjacent places of the membrane, leading to a sequence of potential changes throughout the membrane and, consequently, throughout the neuron. Otherwise, if stimulus does not reach the threshold, there is small variation of the cell membrane potential and no action potential is generated. In this case, there is little or no propagation throughout the membrane. [7]

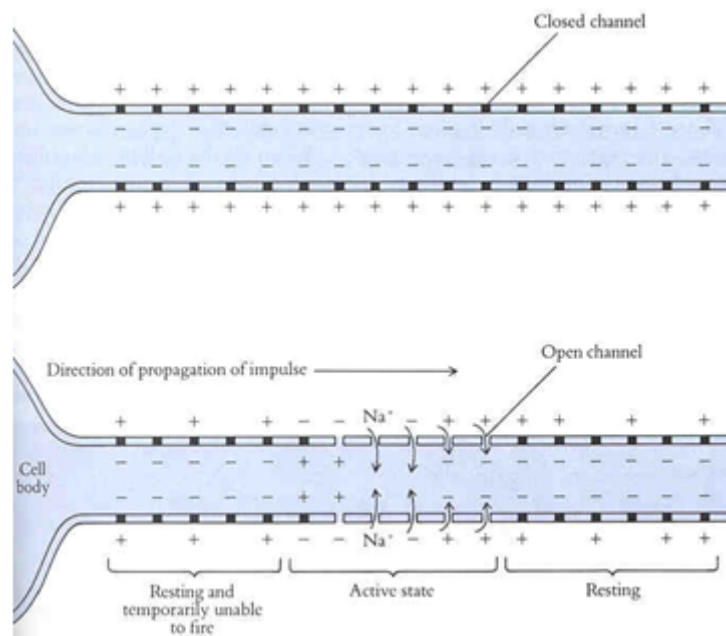


FIGURE 2.2: Action Potential Propagation throughout a Nerve Cell [8].

Despite being a consequence of a stimulus, action potentials are generated by the cell membrane, whose voltage-gated Sodium channels open, allowing influx of Sodium ions, thus increasing the membrane potential. This phase is called membrane depolarization. Voltage-gated channels are channels whose opening and closing for its specific ions depends on the membrane voltage across near the channel. When the membrane potential reaches a certain maximum positive value, the Sodium channels get shut off slowly, reducing its flux. On the other hand, the membrane becomes more permeable to Potassium ions that initially also flow to the inside of the cell and make it even more concentrated there, which then leads to outside diffusion according to the concentration gradient. This diffusion to the outside of the cell will make the intracellular medium negatively-charged and the extracellular medium positively-charged again, in an attempt

to restore the membrane potential – a process called repolarization. After repolarization, Sodium pumps lead Sodium ions back to the outside of the cell, which makes the intracellular medium slightly more negative than its resting state. This slightly negative phase is called refractory period and allows the potassium ions to return to its original place, the inside of the cell, through active transport and diffusion, which restores the membrane to its resting potential. During the refractory period, also called hyperpolarization phase, Sodium and Potassium channels do not react even if a new stimulus is applied. This is important for the unidirectionality of propagation of action potentials in the neuron. [7] An illustration of the previously described events is presented in Figure 2.3. Besides having a role in the membrane resting state potential, the Chloride anion diffusion effect is negligible when an action potential occurs [7].

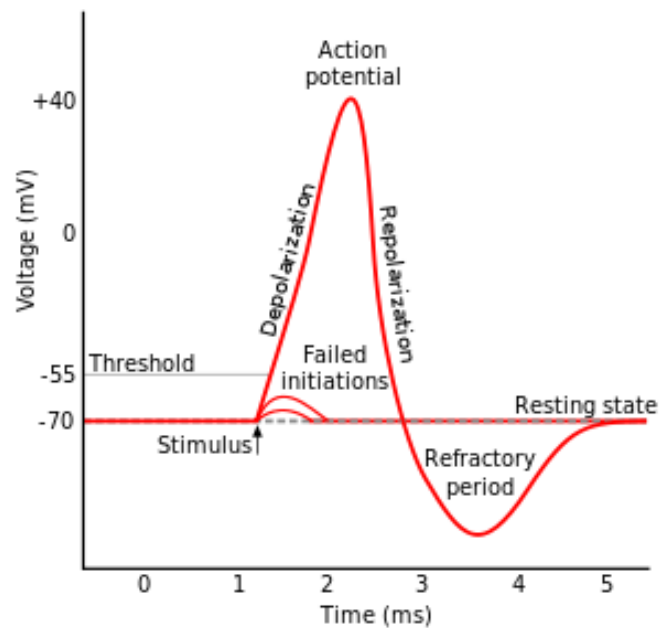


FIGURE 2.3: Variation of Membrane Potential during an Action Potential [9].

The basic mechanism behind neuronal activity was first identified by Hodgkin and Huxley in 1952. They developed a mathematical model for action potential initiation and propagation along the nerve which was based on a circuit model of cell membrane. For this circuit, every component of the cell membrane is represented by an electric component: the dual phospholipid layer is represented by a capacitor C_m , the voltage-dependent ion channels as conductances g_n and the electrochemical gradients as voltages sources E_n , where n represents each of the ions to which the membrane is permeable

to. The circuit is represented in Figure 2.4 and V_m represents the voltage across the cell membrane [7].

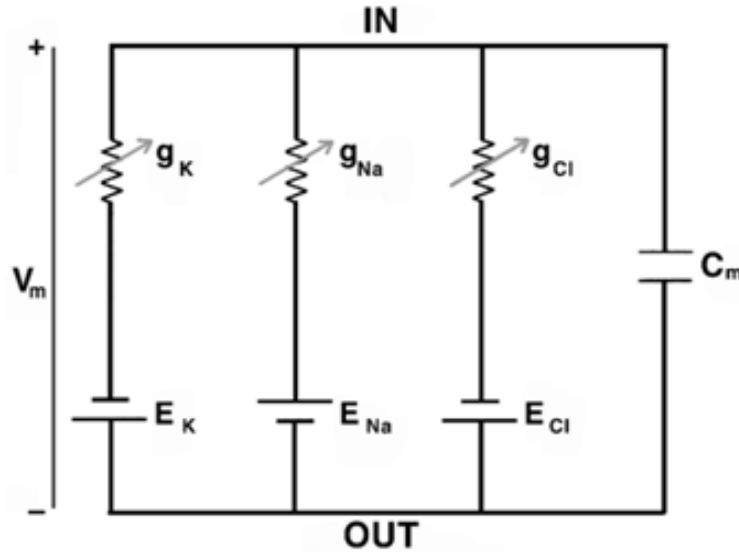


FIGURE 2.4: Circuit Model of Cell Membrane [7].

The Hodgkin and Huxley model then describes the total membrane current I_m as the sum of the ionic currents I_{ion} and capacitive current I_C . This results in Equation 2.1.

$$I_m(t) = I_{ion}(t) + I_C(t) \quad (2.1)$$

In this equation, I_{ion} is given by the sum of the currents that pass through each of the ion channels, as it is on Equation 2.2. In this equation, Na and K represent sodium and potassium channels, respectively, and L is the leakage current which represents the less significant ion channels. Each of ionic currents is time dependent and its value is obtained from the conductance of the ionic channel and the potential difference between membrane potential V_m and Nernst Potential E_n for each ion, as in Equation 2.3. The Nernst Potential is the potential difference across the membrane at equilibrium. Equilibrium is the state where the rate of movement due to diffusion of the ion n in one direction, resulting from ionic concentration differences between the inside and outside of the membrane, is equal to its rate of movement in the opposite direction due to electrical field, which results from the transmembrane potential created by the accumulation of charged ions in the membrane. The capacitive current I_C represents the change of charge inside the cell and is given by Equation 2.4.

$$I_{ion} = \sum I_n = I_{Na} + I_K + I_L \quad (2.2)$$

$$I_n(t) = g_n(t, V_m) \times (V_m(t) - E_n) \quad (2.3)$$

$$I_C(t) = C_m \frac{dV_m(t)}{dt} \quad (2.4)$$

In ionic current equation, Equation 2.3, conductance of ionic channel is given by Equation 2.5, where \bar{g}_n is the maximum conductance of respective ionic channel, and δ and ρ are the probability of existing channel subunits being open. In these, q and k are the number of correspondent subunits existent in the ion channel. For its turn, the probability of subunits being open is given by Equation 2.6, where α_δ are the opening rates and β_δ are the closing rates of the subunits and are both time- and voltage-dependent, δ_0 is the probability of open channels in $t = 0$, and v_m is the reduced membrane potential, which is the difference between the membrane potential V_m and the membrane resting potential V_r .

$$g_n(t, V_m) = \bar{g}_n * \delta^q(t, V_m) * \rho^k(t, V_m) \quad (2.5)$$

$$\frac{d\delta(t, v_m)}{dt} = \alpha_\delta(v_m) * (1 - \delta) - \beta_\delta(v_m) * \delta \quad (2.6)$$

In membrane-ionic dynamics, temperature also plays an important role, namely in membrane kinetics and ionic channel conductance, so a thermic coefficient \emptyset can be included in both Equation 2.3 and 2.6 to represent acceleration in membrane kinetics. This thermic coefficient is multiplied by the referred equations and is given by Equation 2.7. In this equation, Q_{10} is a constant that represents the increase in permeability and kinetics of the membrane when temperature raises $10^\circ C$ and T_0 a reference temperature. [10]

$$\emptyset = Q_{10}^{\left(\frac{(T-T_0)}{10}\right)} \quad (2.7)$$

2.2 External Electrical Neuron Stimulation

As it was mentioned in the previous chapter, nerve stimulation is possible because neural communications are based on electrochemical changes or more precisely, as explained, ionic currents. An intuitive way of inducing nerve stimulation is then to apply an electric current to the excitable nerve tissue. This can be achieved through the placement of at least two electrodes, a positive anode and a negative cathode, in the neural tissue and promote the passage of electrical current from one electrode to the other. These electrodes can also be called sink and drain electrodes since their function is to inject current and then remove it from the tissue. This is known as a bipolar montage. When current is applied to an electrode, free electrons of the electrodes' metallic conductor reach the electrode-biological tissue interface where there is a transduction of charge carriers, from electrons to ions, which allows the current to continue its path [11]. A further description of this phenomenon will be made in the following subsection.

2.2.1 Electrical Stimulation Principles

When an electrical stimulation is applied through the use of electrodes there is one interface to be considered besides the aforementioned electrode-tissue interface - the electrode-electrolyte interface. The two interfaces are represented in Figure 2.5 and Figure 2.6.

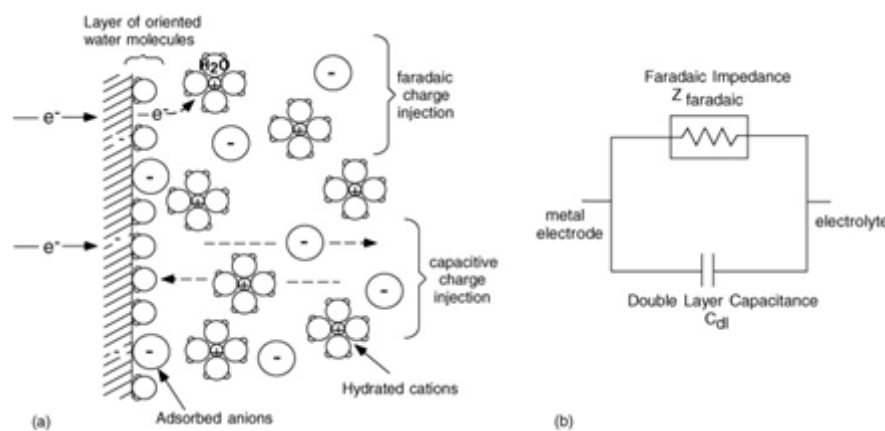


FIGURE 2.5: Electrode-Electrolyte Interface Representation (a) and Circuit Model (b) [12].

On the representation of electrode-electrolyte interface circuit model, Figure 2.5.b., we can see that the interface consists of a resistor $R_{faradaic}$, which represents the Faradaic

resistance, in parallel with a capacitor C_{dl} , which by its turn represents the Helmholtz double-layer capacitor effect at the interface. A Helmholtz double-layer, or to simplify double-layer, is a structure composed of charged particles, and ions attracted to these particles, adsorbed to a structure of an metal object when it is exposed to a fluid – Figure 2.5.a. Due to this capacitor effect, one can infer that the impedance of electrode is frequency dependent. Also contributing to a difficult accurate modelling of this interface is the fact that both C_{dl} and $R_{faradaic}$ are nonlinear time-varying components. [13] A circuit model of a bipolar electrode montage is represented in Figure 2.6, where the resistor R_S is the access resistance and can represent either the electrolyte or the tissue resistance.

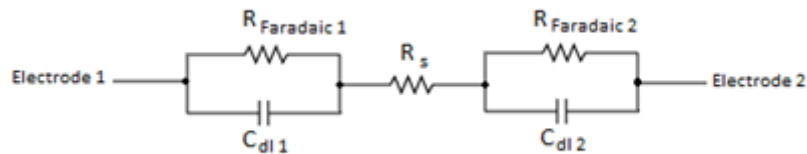


FIGURE 2.6: Electrode-Electrolyte and Tissue Interface Circuit Model in a Bipolar Montage [11].

Half-cell potential for the electrode is also a factor to be considered. Half-cell potential results from chemical reactions in the double-layer that momentarily pumps electric charged particles between the electrode and electrolyte creating a potential difference. The half-cell is simply a structure composed of a conductive electrode and a conductive electrolyte surrounding it where a naturally occurring double-layer separates them. [14] However, in the case of a dipole electrode montage, the half-cell potential of both electrodes can be omitted from the model because it is assumed that they are made of same material and so they cancel each other. [11]

The importance of this model for stimulation designs is that it allows studying each mechanism and reaction behind the application of an electric stimulus through an electrode. There are two main mechanisms that allow the passage of current between two different media: the Faradaic and the non-Faradaic mechanism.

A non-Faradaic mechanism, also known as capacitive charging process, is related to a redistribution of charged chemical species in the electrolyte and the referred Helmholtz double-layer capacitor effect charging and discharging. In this mechanism, charge is

applied on each electrode, creating a capacitor-like effect where the tissue acts as a dielectric layer. This way, charge on the electrode attracts, or repulses, ions from the tissue thus producing stimulating pulses of ionic current. In a perfect non-Faradaic process, there is no charge crossing the electrode-electrolyte interface and a situation close to this is possible as long as charge density is maintained below the electrode's limit. This ideal situation is represented in the circuit model by an $R_{faradaic}$ with infinite value. In this mechanism, it is possible to reverse the charge distribution by reversing the direction of applied current. [11]

In a Faradaic mechanism, also known as electrochemical reaction process or oxidation-reduction reaction process, an injection of charge occurs from electrode to electrolyte and in the opposite direction. An oxidation reaction is verified at the positive electrode, resulting in removal of electrons, and at the negative electrode a reduction reaction occurs, which acquires electrons. It can then be divided in two types of reactions: reversible and irreversible. The reversibility of a Faradaic process is dependent on relative rate of kinetics and mass transport. For a Faradaic process to be reversible, the kinetic rate, which is the electrons transport at the interface, has to be higher than the mass transport rate. In this situation, redox products formed at the interface are stored near the electrode instead of diffusing away and a reversion of stimulus current direction allows the products to return to its original forms. In an irreversible Faradaic process, a smaller kinetic rate is verified and so the redox products are able to diffuse away instead of being stored near the electrode and not even the inversion of current direction is able to reverse the products into their original forms. [13] An irreversible Faradaic is then a process to be avoided since it leads to electrochemical changes in the interface, such as electrode dissolution and gassing or pH variation of electrolyte, which can generate toxic chemical substances to the tissue. [11]

To apply a safe stimulation, a charge balancing phase after the stimulating phase has to exist to avoid irreversible Faradaic charge transfer. This charge balancing phase should be the application of a current with the opposite direction of the stimulating current in order to recover all the charge initially injected, as soon as possible to avoid diffusion of the redox products. [11] However, in most electric stimulation systems an interphase delay between stimulating and charge balancing is used so that stimulation effect can be maximized. [15]. Figure 2.7 exemplifies the referred stimulation by showing a classic square pulse stimuli followed by an interphasic delay and then a charge balancing phase.

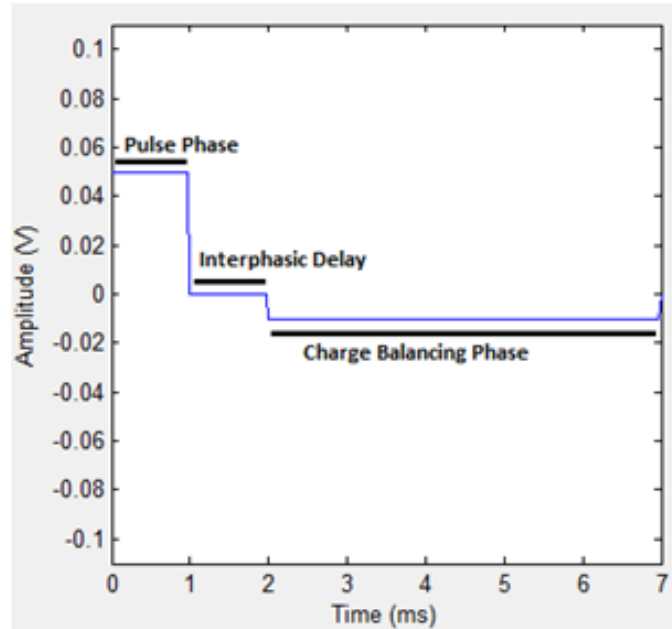


FIGURE 2.7: Biphasic Square Pulse Stimulation.

For the charge balancing phase to be precise so that safety is maximized, the amount of charge in stimulation and charge in this balancing should be the same. However, if amplitude in balancing phase is of the same amplitude as the pulse, a new stimulation or inhibition can occur. To solve this, the amplitude and duration are changed so that the amplitude can be reduced but the amount of charge stays the same. This decrease in amplitude therefore means an increase on duration. This increase and decrease are usually calculated through a ratio, called biphasic ratio, applied to the referred parameters of original pulse. Equation 2.8 and 2.9 present the calculation of charge balancing amplitude A_{cb} and duration T_{cb} , respectively, through the use of biphasic ratio B .

$$A_{cb} = \frac{A_p}{B} \quad (2.8)$$

$$T_{cb} = T_p * B \quad (2.9)$$

A_p and T_p respectively represent the amplitude and duration of the original stimulating pulse.

2.2.2 Electrical Stimulation Application Techniques

The principles described in the previous section are the base of electrical stimulation which essentially consists of applying a potential gradient across the neuron, using electrodes, which will create an intracellular ionic current flow and depolarization or hyperpolarization of cell membrane that can result in neural stimulation or inhibition, respectively.

Application of these potential gradients in the neural tissue is currently achieved through three electrical ways, either by Voltage-Controlled, Current-Controlled or Charge-Controlled stimulators. Voltage-Controlled stimulators' operation is based on application of a voltage between the electrodes. This type of stimulators is a more simple way of applying stimulation and it's the most energy-saving option. However, variations of neural tissue impedance make it difficult to control the actual charge that is injected on the tissue, which can lead to safety concerns. This type of stimulators is currently used in techniques such as Deep Brain Stimulation and devices as pacemakers, where proven efficacy and low power consumption are dominant arguments. [10]

Current-Controlled stimulators apply a current stimulus to the neural tissue which is also controlled by the voltage difference between the electrodes. Difference lays in the fact that in this case voltage difference may vary along stimulation time so that wanted current intensity, or current intensity variation, is applied. However, to obtain this type of control, a higher power waste occurs, compromising not only battery lifetime, which is of great importance in portable implantable devices, but also surrounding tissue damage due to heating. This type of stimulators is used, for example, in Transcranial Direct Current Stimulation, a recently used technique whose effects and applications are still under research. [10]

Finally, Charge-Controlled stimulators are a type of stimulators which basically stimulate with a fixed amount of charge via voltage stimulation. For example, a capacitor can be added to a voltage-controlled stimulator for controlling and limit the charge delivered to the electrodes. This is a better energy-efficient type of stimulator than current-controlled stimulators but worse than voltage-controlled ones and it is not yet a clinically-used technique. [10]

Electrical stimulus application can be used through different strategies which can lead to different results due to ion channels conductance and opening rates time dependence, thus making this an area of current research interest. There are some considerations and limitations that need to be considered when using electrical stimulation, such as selectivity, efficacy, efficiency, electrode size and safety. Main safety concerns include biocompatibility, electrode dissolution and creation of toxic chemical substance, already explained in previous section. Since the last two referred safety concerns are related to control of amount of charge passing through the electrodes, one important area of research in electrical stimulation is the design of safe circuits which nowadays make use of blocking capacitors. Although this solution has proven effective, blocking capacitors have an unattractive size and weight for portable and implantable devices that lead investigation towards capacitor-free circuits. Another safety limitation subject of current research areas is related to stimulation selectivity dependency on electrode size and electrode point of application. Electrode design is directly related to selectivity where smaller electrodes lead to higher stimulation precision but, on the other hand, safety charge levels decrease as electrode surface area reduces. Electrode point of application is also an important issue since electrodes close to target neuron provide higher precision but close-located electrodes require a higher biocompatibility level. [10]

Regarding electrical stimulation consideration of selectivity, efficacy and efficiency, besides the dependency on electrode size and point of application, the dependency on stimulation strategy, more specifically waveform shape, amplitude, frequency or width, among others, is also very important and research has shown that more advanced waveforms lead to better results [16]. In matters of waveform shape, the rectangular pulse, presented in Figure 2.8, is the most used waveform shape in neurostimulation because it provides an effective electrical stimulation of simple implementation, however it has several limitations such as the activation of large-diameter fibres before the smaller ones and indiscriminates stimulation of sensory and motor neurons [16].

More advanced waveform shapes, such as the Quasi-Trapezoidal and Tri-Exponential waveform, can lead to more accurate neuron stimulation. Quasi-Trapezoidal is a waveform with a steep rise followed by an exponential decay as shown in Figure 2.9. Tri-Exponential is a triangular-shaped waveform which consists of a linear rise followed by an exponential decrease, as it is presented in Figure 2.10. These waveforms shapes have been found to activate first small-diameter fibres before large fibres and besides

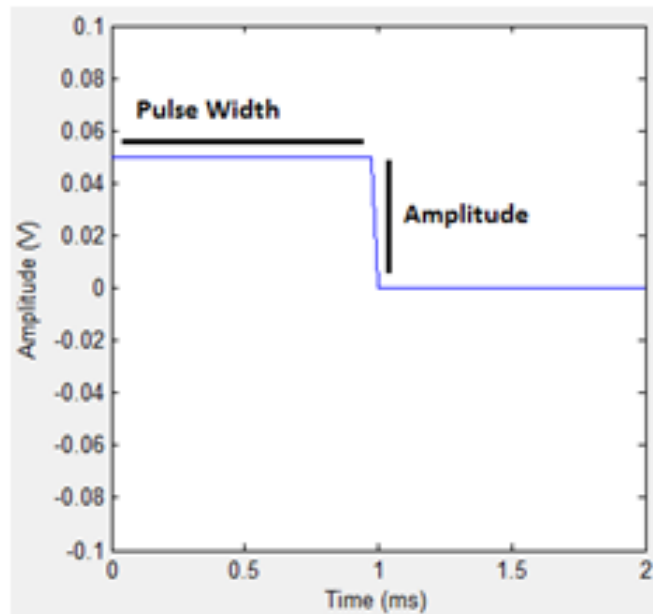


FIGURE 2.8: Rectangular Pulse.

this fibre recruitment characteristic [17, 18], quasi-trapezoidal has also shown success in unidirectional stimulation [19].

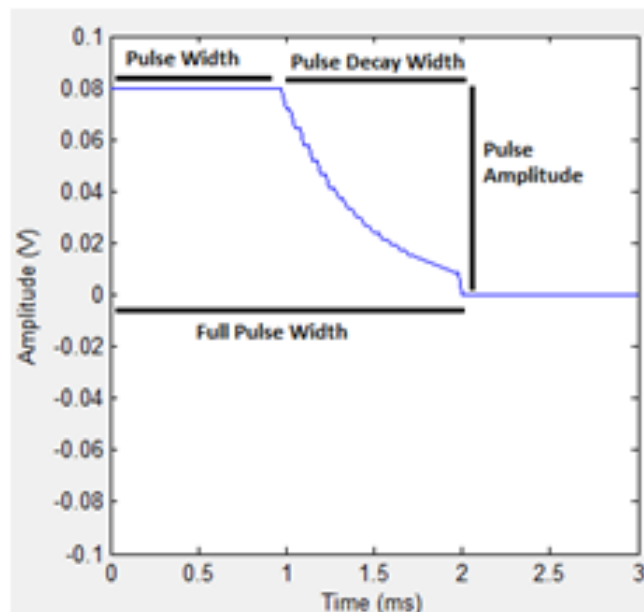


FIGURE 2.9: Quasi-Trapezoidal Pulse.

Activation of medial fibres without activation of lateral fibres is also possible through the use of sub-threshold pre-pulses [20]. An example of a stimulation using this type of strategy is shown in Figure 2.11.

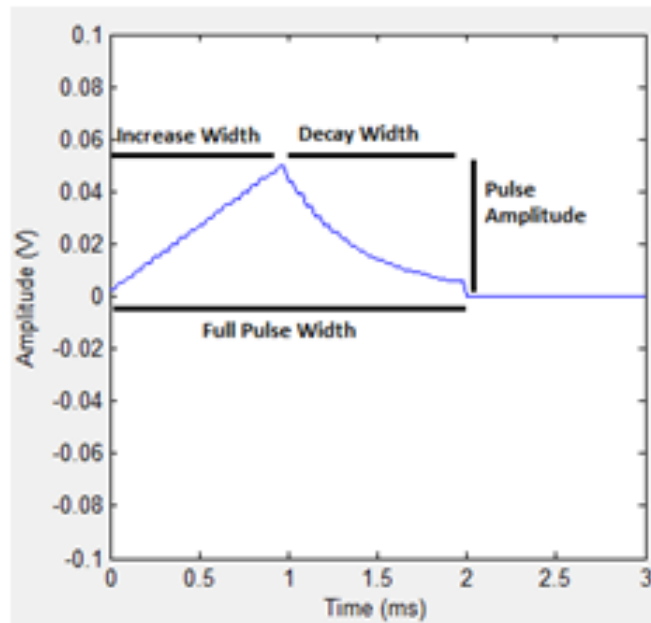


FIGURE 2.10: Tri-Exponential Pulse.

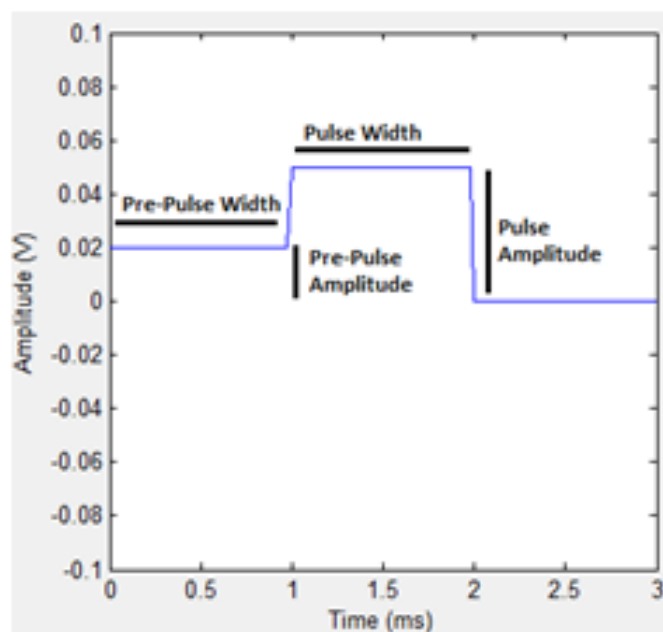


FIGURE 2.11: Sub-threshold Pre-Pulse followed by Pulse.

Other stimulation strategy with good results in selectivity is called bursting strategy, shown in Figure 2.12, which consists of applying smaller rectangular pulses, also called ‘pulsons’, with a small time interval between them instead of a single rectangular pulse. This bursting strategy is understood to improve not only fiber-selectivity but also power efficiency [21, 22].

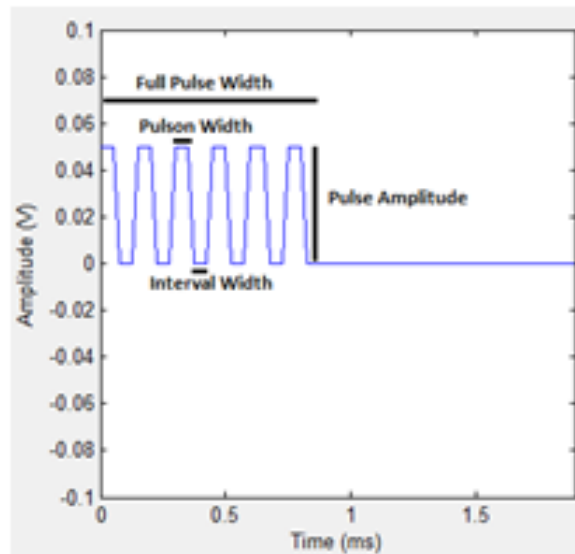


FIGURE 2.12: Bursting Strategy Stimulation.

In summary of waveform parameters, amplitude results in fiber-selectivity, more specifically, the activation of larger fibres with low amplitudes and the blocking of larger fibres previous to smaller ones when an anodal current is applied [17]; frequency causes blocking effects on selected fibre diameters when a high frequency stimulation is applied [23]; and shorter pulse width activates more small-diameter fibres than large ones [24].

Chapter 3

State-of-the-Art of User Configurable Neural Stimulation Technologies

Electrical stimulus application can be used through different strategies for different results due to physiological characteristics of the neuron. When defining a strategy, performance such as selectivity and efficacy, and limitations such as efficiency and safety need to be taken in consideration. The challenge of optimizing the performance of the neurostimulator within the limitations for each specific application is what makes this an area of current research interest.

Towards this goal, research has focused in studying and investigating different types of stimulation strategies in various areas where neural stimulation can be applied. However, with the use of typical neurostimulation experimental methods, changing stimulation strategies is a very time-consuming task and it would not be possible to make a valid comparison between stimulations applied to the same nerve since nerve fatigue could occur and it had to be tested in a new nerve. This way, to allow for further progress in this area, a system that would enable a fast and easy reconfiguration of stimulation parameters was necessary.

In order to respond to this need, new experimental procedures were developed such as the one presented by Grill, W. M., Jr. and J. T. Mortimer (1996) [24] which bypasses this problem through the use of a highly integrated computational model, or the one

presented by Accornero, N., et al. (1977) [18] which uses a common testing platform that integrates a square pulse into a triangular pulse with multiple customized circuits, more specifically, a potentiometer and a switch connected to three different capacitors allowing a control of both amplitude and duration of the triangular pulse. However, in this last procedure it still takes some time to change the configuration, and consequently the parameters, and would also only allow evaluation of a limited number of variables.

Bugbee, M., et al. (2001) [25] developed a programmable implantable stimulator system for selective stimulation of nerves. This system is divided in two parts: one internal and one external. The internal part is placed near the stimulation site and is responsible for the application of stimulation. It is composed by two main integrated circuits (ICs): a Digital Control Unit (DCU) and a Stimulation Unit (SU). SU is the responsible for application of stimulation according to commands from DCU, which receives and decodes radio-frequency information from the external part. The external part of this system is then composed by a computer, a microprocessor-based modulator and a radio-frequency (RF) transmitter. On the computer runs a program that controls the whole system and defines certain parameters for stimulation such as the amplitude, the charge balancing ratio, pulse width, frequency and duration of stimulation. After all parameters are chosen, the program sends that information to the internal part, via the microcontroller and RF transmitter, and then the user can initiate and stop stimulation and save the history of stimulations. This system presented itself has a great advance towards fast and easy reconfiguration of parameters of stimulation and also has the major advantage of allowing programmability with the stimulator already implanted. However there are still limitations namely in the number of parameters that the user is allowed to change and also the options within those parameters. A similar device is reported by Sha, H., et al. (2005) [26] but communication between internal and external part is made via optical transcutaneous communication instead of RF transmission and also the internal part can be composed of more than one stimulator, interacting with only one at a time depending on identification information contained by the light pulse. Here, however, the number of parameters that can be changed is not only limited but also much smaller – about 6 parameters. In Salmons, S., et al. (2001) [27] an analog implantable system is made, but here light is used to select a pre-programmed set of stimulation parameters, which can only be done while the stimulator part is not yet implanted. This therefore means that the number of parameter variations to be tested is limited and to try different

sets or combinations of parameters an extraction and new implantation have to be done, which is a very time-consuming, intrusive and nerve-exhausting procedure.

Constandinou, T. G., et al. (2008) [28] presents an integrated circuit for electrical stimulation which allows user programmability of three bipolar stimulation channels. A continuous interleaving sampling strategy is applied which involves sequencing the stimulation waveforms among active channels. This is a current-controlled stimulation system which allows for programmable asymmetric biphasic stimulation where charge-balancing is obtained through a current-steering circuit that has three circuit configuration phases: one for cathodic pulse, one for anodic pulse and a third one, which occurs between pulses, in which current is not directed to the electrodes but instead to a dummy load. This dummy load phase is used to achieve a smoother transition between pulses by minimizing charge buildup and spiking.

Woods, V. et al. (2008) [29] proposes an experimental setup which consists of a software-controlled automated stimulation-and-recording module. This setup allows the user to specify a number of waveform shapes and the corresponding range of stimulation parameters to be investigated, such as amplitude and duration, through a MATLAB-based interface after which the software starts loading the first waveform into a programmable AC current generator. The current output is converted into voltage using an instrumentation amplifier and is then connected to a data acquisition module. To this data acquisition module is also connected the neural recording amplifier. This way, for each stimulation applied, corresponding to the waveform programmed, an acquisition from the nerve is made and stored. After one stimulation and recording is done, the system updates the following programmed waveform and, after allowing some time for nerve to recover, it applies respective stimulation and recording. This system then presents itself with the advantages of re-configurability, allowing an automatic assessment of different stimulation strategies with very rapid parametric variations on one nerve, and portability. However it still presents some limitations. The high price of main components presents as a limitation since to reproduce this system a programmable AC current generator is needed, whose cost is usually above 6.000€, and also a data acquisition module, whose cost is above 2.000€. Also, although portable, generator and acquisition module are still heavy and bulky instruments. Adding to these limitations is the high power consumption they have even when no stimulation is being applied.

Thurgood, B. K., et al. (2009) [30] presents a stimulation system which can be programmed via wireless transmission. Here the programming is made in a computer, where certain parameters can be changed such as current pulse amplitude, duration, interphasic delay and repetition rate, and this information is sent directly from the computer to the stimulator chip. The system was developed with an array of 100 stimulators and allows programming and control of an individual stimulator at a time. The array of stimulators itself is powered via inductive coils and it is effectively controlled by a global finite state machine (FSM), which is the one that receives and interprets the information from the computer to send it to a stimulator. The stimulator itself is composed of analog and digital components that, after receiving and storing information on referred parameters, make it able, on activation, to apply current-based biphasic stimulation. The system developed here presents the major advance of using wireless, an easy, reliable and widely-used means of data transmission, to communicate with stimulators which lead to an easy, remote and hence isolated configurability, meaning it can be a fully implantable programmable stimulator. However, this system has a very limited number of parameters available to configuration, which can be related to a smaller memory available due to size limitations that an implantable device imposes.

Eftekhari, A., et al. (2009) [31] presents a platform that follows the system presented by Woods, V., et al. [29], but instead of using heavy and bulky instruments such as the AC current generator it designs a small PCB-based stimulator which will be the responsible for generation and application of stimulation. This platform is also software-controlled through a MATLAB-based graphical user interface (GUI) that allows specification of stimulation parameters. The interface created in this article allows the user to choose any waveform type desired not only by presenting a number of predefined waveform shapes but also by allowing the upload of arbitrary waveforms. Besides this, the interface allows to specify parameters such as repetition rate, resolution to built stimulation and also amplitude and duration. The computer is then connected to a PCB-based stimulation module composed by a microcontroller, a digital-to-analog converter (DAC), a voltage-to-current converter and an H-bridge, which are supplied by a standard 9 V battery. In this platform, after stimulation profiles are defined in the computer, they are uploaded to the module where they are stored. To choose a stored profile and use it for stimulation a DIP switch is used, following which a trigger input is used to generate and apply the stimulation. This platform then presents the programmability and current-based

stimulation advantages from the previous device but adds portability, since it not only is a relatively small module but also has a battery power supply and, after the profiles are updated, it can work alone without being connected to the computer. Also, building this platform is relatively easy and much cheaper than obtaining the programmable AC current generator. However, this platform presents one major limitation compared to the previously mentioned system: it can only perform stimulation; neural recording is not possible with this module. Besides this, there are also limitations to the number of channels to apply stimulation – it only has one channel which allows up to a tripolar montage – and it also has lower parameter ranges due to microcontroller memory size and other electronic components limitations, such as voltage compliance in stimulation amplitude. Guilvard, A., et al. (2010) [32] make an approach to build a system with capacity of working through multiple channels and allow multi-polar montages, however this system was designed and simulated but fabrication and testing remains undone.

Laotaveerungrueng, N., et al. (2010) [33] present an 8-channel integrated current and voltage stimulator chip. This stimulator chip allows the user to choose a set of stimulation parameters among which stands out the possibility of choosing to apply either a voltage-controlled stimulation or a current-controlled stimulation, which can be programmed independently for the eight channels. The communication between programmer and stimulator is made via SPI where user chosen information besides stimulation control type is sent, such as pulse width, frequency and amplitude. Waveform shape however is not a controllable option similarly to what occurs with interphasic and biphasic ratio. Regarding waveform shape, this system only applies square-shaped waveforms. Regarding interphasic delay, it is defined to be one clock cycle. And with biphasic ratio, besides the fact that the system allows for user to choose between monophasic or biphasic stimulation, it does not allow user to control the degree of symmetry between original pulse and charge-balancing pulse. After all information is sent and stored in the chip, it starts to generate the squared-shaped stimulation according to the referred parameters by sending a digital code identifying the output channel and an analog value of the waveform amplitude.

Chiu, H.-C., et al. (2014) [34] have developed a two-channel micro-stimulating and neural recording brain-machine interface that provides a monophasic voltage-controlled stimulation based on parameters defined by the user through a GUI in a computer, which are transferred to the biomedical core, processed and sent through a DAC to

the stimulator front-end, and also provides detection of neural activity through probes after which it is amplified, converted to digital by a successive approximation register (SAR) analog-to-digital converter (ADC) and passed to the biomedical core where it will be processed and transmitted. In this system user can control specifications from both recording and stimulation. Regarding recording, specifications include operating voltage, channel, sampling rate, bandwidth and gain. Regarding stimulation, controllable specifications are operating voltage, channel, amplitude, frequency, pulse width, and time. This system presents itself has a very useful tool for neural activity and stimulation studies especially for the fact that it allows for a joint operation of stimulation and recording, where it also allows for configurability of both these modalities, and also because it is done via Bluetooth which makes this a better option for studies where implantation is intended. However, in the stimulation side, there are still a number of limitations in particular with the parameters available for programmability and characteristics of stimulation. Regarding parameters, the fact that it is not possible to control the waveform shape is a major limitation as well as the impossibility of using either a monophasic or biphasic stimulation. Regarding stimulation itself, the monophasic-only limitation referred previously also affects here since it is seen as not so safe type of stimulation. Besides this, the fact that it is a voltage-controlled stimulation can also be seen as a limiting factor since it is more difficult to control the amount of charge injected in the tissue, although a more power efficient method which is an advantage since this is an implantable system.

Besides these devices, some were also developed and made available in open-source platforms such as the open-source platform for electrophysiology called Open Ephys [35]. An available device in this platform is the Pulse Pal [36]. Pulse Pal is an open-source device that allows for users to program and generate sequences of voltage stimulation pulses. It presents four output channels, which can be independently programmed and have unique pulse sequences, and two trigger channels that can control the output of the pulses. This device allows user to control a set of 16 parameters, as the voltage amplitude, the width of the pulse, if it is monophasic or biphasic, the interphasic delay, the charge-balance amplitude and width, the interpulse, or resting, voltage and width. It also allows user to use a bursting strategy instead of plain rectangular pulse and program its pulsions width and inter-pulsions width. Besides this, the device also allows configuring the delay between trigger and beginning of output of the pulses and duration of all pulse train and

it is also possible to program the trigger mode. All these parameters can be configured in the device itself, due to the existence of an OLED screen and a joystick, but can also be connected to computer and be programmed from there through a programming interface such as MATLAB, or via C++ language or Python. In case of being programmed in a computer, it is also possible to generate different and more complex pulse trains and then load them to the device. However, due to memory limitations, this option is only available for a maximum of two channels. With all these referred characteristics, Pulse Pal is a very promising tool for stimulation study. Adding to the fact of having a wide range of parameters available for configuration, the availability of trigger mode and the possibility of programming either in stand-alone mode or through a programming interface, it is the fact of being a low-cost device – it costs about \$ 200 – and the fact that the software and hardware assembly instructions are openly available. However, there are limitations such as the ones resulting from the memory, which results in only two possible custom-made waveforms, and the fact that only a channel at a time can output.

The electrical stimulation devices that were described in this chapter present characteristics that make them very useful tools for the study of electrical stimulation strategies. However, limitations can still be found in all these systems. The development of a programmable electrical stimulation platform which presents the advantages and overcomes the referred limitations of the reported devices is then a major goal intended for the project here developed.

Chapter 4

Software Development

The development of the stimulation platform is described throughout this thesis and it is divided in the two main parts that compose the system: software and hardware. The software part is responsible for receiving the user's configuration, processing them and then control the hardware part so that stimulation can be done accordingly.

This chapter is dedicated to the software part of the system, where the requirements, the software developed and its operation are described. For this part, two different types of software platforms were used namely MATLAB and CodeWarrior which were used, respectively, to create the user-system interface and to program a FRDM-KL26Z Freescale microcontroller. The requirements, development and operation of each of this software will be done separately, starting by a section for user-system and then a section for microcontroller.

4.1 MATLAB-based User-System Interface

As previously stated, MATLAB was the software platform used for the development of the user-system interface. The choice of MATLAB to do such an interface was not only because it is a very powerful and interactive software for numeric computation, data analysis and visualization but also a very intuitive and easy-to-use platform for programming and algorithm development and also has as specific tool for the design and development of user interfaces called GUI Development Environment (GUIDE). Figure 4.1 presents the MATLAB GUIDE interface.

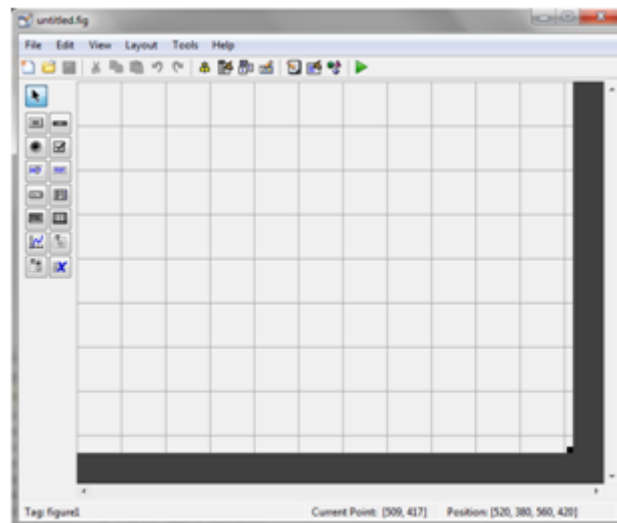


FIGURE 4.1: MATLAB GUIDE interface.

The GUIDE interface allows user to design a GUI with several of predefined components such as pushbuttons, checkboxes, pop-up menus, among others. After placing the wanted components on the GUI design area (grey grid area), MATLAB automatically generates a function to match each of the components placed in a main function that corresponds to running the GUI. Inside these functions can then be written code lines that will define what happens when the respective component is used. Figure 4.2 presents an example of a function generated for a pushbutton.

```
% --- Executes on button press in pushbutton1.  
function pushbutton1_Callback(hObject, eventdata, handles)  
% hObject      handle to pushbutton1 (see GCBO)  
% eventdata    reserved - to be defined in a future version of MATLAB  
% handles      structure with handles and user data (see GUIDATA)
```

FIGURE 4.2: Pushbutton function code.

To develop the user-system interface, there were a number of requirements that were initially defined as necessary for the program to have. These requirements were essentially related with parameters from stimulation that the user should be able to configure and control. The requirements were the following:

- To be able to choose between different waveforms.
- To allow configuration of pulse parameters, such as amplitude and width.
- To allow configuration of interphasic delay.

- To allow configuration of biphasic ratio.
- To allow configuration of pulse repetition.
- To allow control of stimulation duration.

These were defined as priority requirements since they were already implemented by some of the existing configurable stimulation systems [25-34, 36] as it was referred in Chapter 3.

Besides these priority requirements, other requirements for stimulation configuration were also taken into account to be available for user control. The first requirement is related to the control of existing stimulation channels. More specifically, it was desired that this interface would allow user to control four stimulation channels, that each one could be programmed independently and also that it would be possible to use these channels either stimulating individually, stimulating at the same time – synchronously – or stimulating sequentially with a fixed delay between them – asynchronously.

The second requirement was related to voltage amplitude limitations of this stimulation system, more specifically, to the limitations of front-end stimulation circuit. The purpose of this requirement is to warn the user of the maximum amplitude that the stimulation system is able to sustain in order to apply stimulation as user configured in the conditions that stimulation is going to be applied, in this case in particular the electrode impedance.

The following sections provide a description of the user-system interface functionalities created to accomplish the requirements aforementioned.

4.1.1 Choosing between Different Waveforms

Regarding to the first point of requirements, the ability to choose between different types of waveform, it was defined that the available waveforms would be the ones used by Eftekhari, A., et al. [31], which are: Bi-level Lilly, Quasi-Trapezoidal, Tri-Exponential and Bursting Strategies. Besides these four options, it was also included a simple Rectangular pulse thus having a set of five pre-selected waveforms. Besides this five waveforms, it was also included a sixth option which allows user to upload an arbitrary waveform of its choice. To allow the user to perform this selection, a pop-up menu with all the

referred options was created, as can be seen in Figure 4.3.

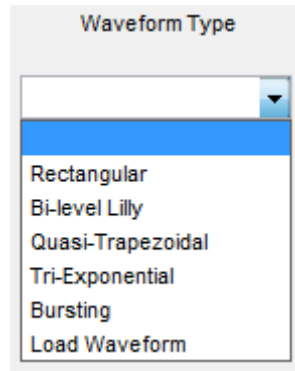


FIGURE 4.3: Waveform Type pop-up menu.

For this pop-up menu, the function written was that when the user chooses one of the five preset waveforms, a one pulse stimulation using the matching waveform is built and saved in an array. Here, the basic necessary parameters are pre-defined to build the respective waveform: amplitude, width, biphasic ratio and interphasic delay. This is done so that user can have an idea of the waveform chosen without having to configure all these referred characteristics. The building of one stimulation pulse is made by concatenation of three arrays – Equation 4.1.

$$pulse = charge\ phase + interphase\ delay + charge\ balancing\ phase \quad (4.1)$$

The first array, which is for charge phase, results of multiplying an array of ones, with length equal to width T_O , in milliseconds (ms), times 40, by the amplitude value A_O , in milliVolts (mV) – see Equation 4.2.

$$charge\ phase = A_O * ones[1, T_O * 40] \quad (4.2)$$

The second array, which is from interphasic delay, is a zero array whose length corresponds to the duration of interphasic delay T_{ID} – see Equation 4.3.

$$interphasic\ delay = zero[1, T_{ID} * 40] \quad (4.3)$$

The final array, which is from charge-balancing phase, is obtained similarly to the first one, with the key differences being the fact that here the charge-balancing amplitude A_{CB} has opposite sign than the original, and the fact that charge-balancing amplitude and width T_{CB} used are obtained by the division and multiplication, respectively, of the original value by the biphasic ratio B – Equation 4.4. Width is multiplied by 40 because it was defined that one array element corresponds to 0.025 ms, hence 40 elements correspond to 1 ms.

$$\text{charge balancing phase} = A_{CB} * \text{ones}[1, T_{CB} * 40] = \frac{-A_O}{B} * \text{ones}[1, B * T_O * 40] \quad (4.4)$$

Here, *ones* and *zeros* are MATLAB functions that generate arrays filled only with one and zero, respectively, whose number of lines is given by the first value inside square brackets and columns by the second value. In this interface it is pre-defined that charge phase, also called cathodic, is represented as negative amplitude and that charge-balancing, also called anodic, is represented by positive amplitude. The equations above presented are the basis of almost every edit box created for parameters, however there are changes in the way charge phase array is calculated depending on the waveform chosen, as it will be explained further. Figure 4.4 shows a rectangular waveform with all the above mentioned phases.

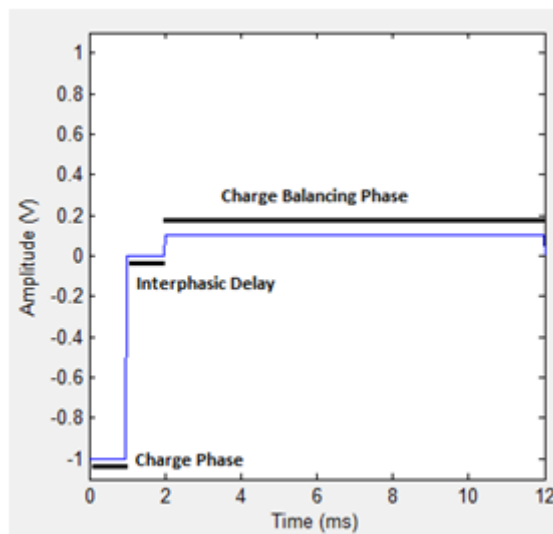
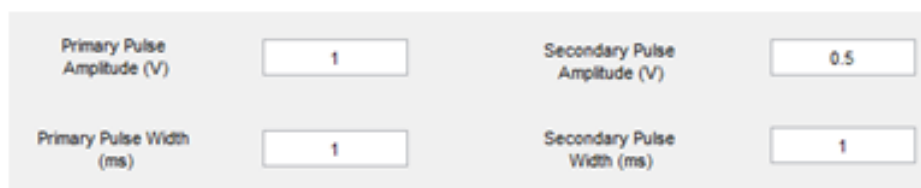


FIGURE 4.4: Rectangular waveform-based pulse.

4.1.2 Configuring Pulse Parameters

Concerning configuration of pulse parameters, edit boxes were created to allow the user to input the desired values. Input boxes were created for control of both pulse amplitude and width. However due to the characteristics of some of the preset waveforms, other input boxes had to be created besides these two. Firstly, we had to create two more edit boxes for amplitude and width for Bi-level Lilly waveform since this waveform can have two different amplitude levels. To differentiate the two, the amplitude edit box that applies to all waveforms is identified as “Primary Pulse Amplitude” and the width is identified as “Primary Pulse Width”, and the amplitude and width edit boxes that only apply to Bi-level Lilly waveform are respectively identified as “Secondary Pulse Amplitude” and “Secondary Pulse Width”. The function activated when primary amplitude and width edit boxes have a new input is similar to the one from waveform type pop-up menu but here the variable of charge phase amplitude and width, A_O and T_O , have the input value. When secondary amplitude and width edit boxes have an input a similar process to the one for primary parameters occurs. The difference between primary and secondary calculation is the addition of one phase array, which follows the existing charge phase. This phase array is also a result of multiplying an array of ones – with length equal to secondary width T_{O2} , in milliseconds (ms), times 40 – by the secondary amplitude value A_{O2} , in milliVolts (mV). Besides this, there is also inclusion of both these secondary parameters in the calculation of amplitude and width of charge balancing phase. To avoid any possible error with the remaining waveforms, these edit boxes are locked and respective variables are set null whenever Bi-level Lilly is not selected. Figure 4.5 shows the mentioned edit boxes with the pre-defined values. Figure 4.6 shows the same edit boxes but with secondary parameters locked.



Primary Pulse Amplitude (V)	1	Secondary Pulse Amplitude (V)	0.5
Primary Pulse Width (ms)	1	Secondary Pulse Width (ms)	1

FIGURE 4.5: Amplitude and Width edit boxes.

Figure 4.7 shows a pulse built with use of Bi-level Lilly waveform type with the preset parameters shown in Figure 4.6.

Primary Pulse Amplitude (V)	<input type="text" value="1"/>	Secondary Pulse Amplitude (V)	<input type="text" value="0.5"/>
Primary Pulse Width (ms)	<input type="text" value="1"/>	Secondary Pulse Width (ms)	<input type="text" value="1"/>

FIGURE 4.6: Amplitude and Width edit boxes with secondary parameters locked.

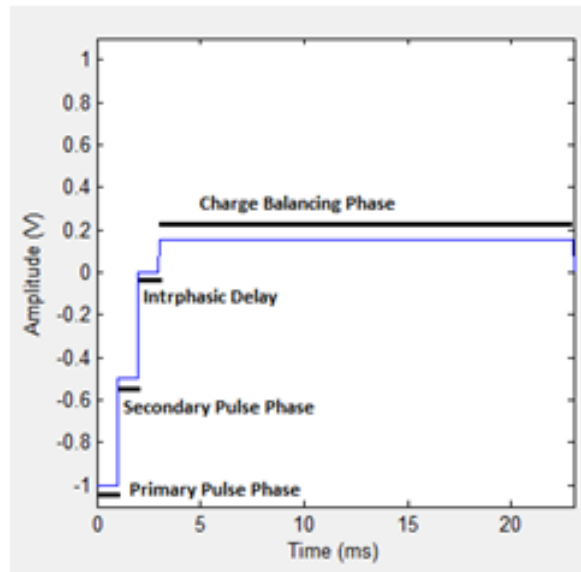


FIGURE 4.7: Bi-level Lilly waveform-based pulse.

Secondly, considering the characteristics of Quasi-Trapezoidal and Tri-Exponential waveforms, more specifically the fact that both these waveforms have an exponential decay, edit boxes for configuration of exponential components were also created, thus giving the user control over the shape of the decay. However, there is a difference between the decays of the referred waveform, this difference being the fact that Quasi-Trapezoidal decay is exponential while Tri-Exponential decay is, has the name implies, tri-exponential. Figure 4.8 and 4.9 show the edit boxes created respectively for Quasi-Trapezoidal and Tri-Exponential waveforms.

Quasi-Trapezoidal Exponential Characteristics

$Q \exp(-qt)$

Q

q

FIGURE 4.8: Edit boxes for Quasi-Trapezoidal exponential characteristics.

Tri-Exponential Characteristics

$A \exp(-at) + B \exp(-bt) + C \exp(-ct)$

A	0.2
a	1.1972e+03
B	0.3
b	2.1972e+03
C	0.5
c	3.1972e+03

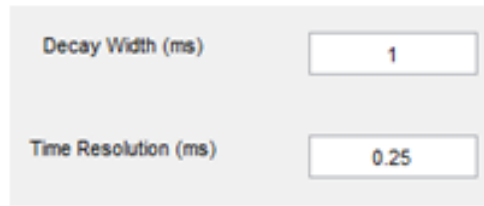
FIGURE 4.9: Edit boxes for Tri-Exponential exponential characteristics.

As it is possible to see in the figures above, an edit box was created for each parameter of the exponential, whose identification is explained in the equation presented above the respective edit boxes. Here, as in previous edit boxes, the functions activated when an input is done have the same Equations 4.1, 4.2, 4.3 and 4.4 as its basis. However, in these cases, building of charge phase array is divided in two parts. In Quasi-Trapezoidal case, the first part of this phase is built the same way, as presented in Equation 4.2, using “Primary Pulse Width” as this phase width; the second part of the phase is built through concatenation of smaller arrays, of length equal to time resolution multiplied by 1ms of array elements, composed by amplitude values obtained by iteration of exponential equation starting from the amplitude value, chosen by the user or pre-defined, until a certain limit of number of iteration steps is reached. The equation used for iteration is presented on the top of Figure 4.8 and can be seen in Equation 4.5. The number of iteration steps is obtained from the division of decay width by resolution and so, to allow a higher user-control over the behavior of the decay, and more specifically of number of steps, edit boxes were also created for configurability of decay width and resolution intended – see Figure 4.10.

$$A_d(T_O + t) = Qe^{-q(T_O+t)} \quad (4.5)$$

In Equation 4.5, the t is the resolution, or time step, and A_d is amplitude in decay phase.

During this second part, summation of amplitude obtained in each iteration is done so that, by adding its result to first phase amplitude, it is possible to calculate correctly the amplitude of charge-balancing phase.



The image shows a software interface with two input fields. The first field is labeled "Decay Width (ms)" and contains the number "1". The second field is labeled "Time Resolution (ms)" and contains the number "0.25".

FIGURE 4.10: Decay Width and Resolution edit boxes.

Figure 4.11 shows a Quasi-Trapezoidal pulse with the referred phases. In Decay Phase it is possible to see the iteration steps, which can be smoothen if resolution is configured to be smaller.

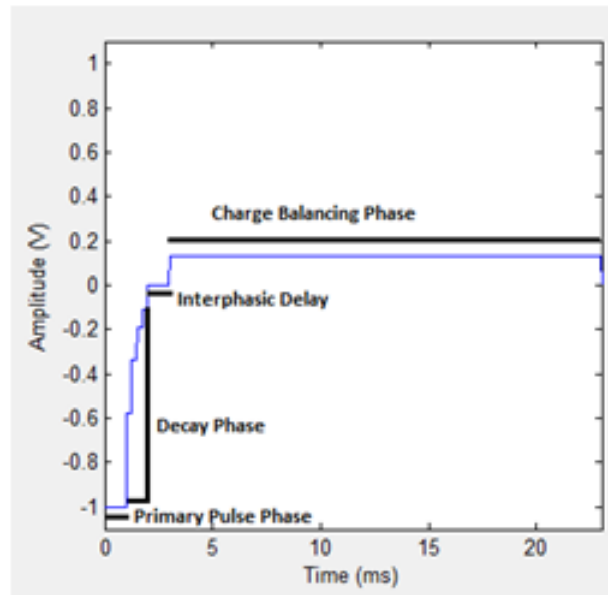


FIGURE 4.11: Quasi-Trapezoidal waveform-based pulse.

Regarding Tri-Exponential case, the first part of charge phase is a linear increase of amplitude so to build this part array Equation 4.6 is used, obtained knowing that the maximum value is the amplitude defined by the user, or pre-defined, that initial amplitude is zero and also that charge pulse starts in beginning, which means when time is zero. Using this equation, iteration is made and all the resolution-length arrays composed of amplitude values, obtained from each iteration, are concatenated together building an array of increasingly higher amplitude values up until it reaches a limit number of iterations. This number of iterations is defined similarly to decay, the difference being

that instead of using decay width value, primary pulse width value is used.

$$A_i(t) = \frac{A_O}{T_O}t + \frac{-A_O}{T_O} \quad (4.6)$$

In Equation 4.6, A_i is amplitude in increase phase and t still is resolution, or time step. The second part of the charge phase, which corresponds to the decay, is built similarly to Quasi-Trapezoidal waveform, meaning it is also obtained through concatenation of smaller arrays, of length equal to time resolution multiplied by 1 ms of array elements, composed by amplitude values obtained by iteration of exponential equation starting from the amplitude value until a certain limit of number of iteration steps is reached. The only difference here, comparing to Quasi-Trapezoidal, is the fact that a tri-exponential equation is used to calculate the decay. This equation can be seen in Figure 4.9 on the top and is presented in Equation 4.7.

$$A_d(T_O + t) = Ae^{-a(T_O+t)} + Be^{-b(T_O+t)} + Ce^{-c(T_O+t)} \quad (4.7)$$

With this waveform, summation of amplitude obtained in each iteration is done, similarly to Quasi-Trapezoidal, but here is done in both part one and two so that by adding both amplitude results, it is possible to calculate correctly the amplitude of charge-balancing phase. Figure 4.12 shows a Tri-Exponential pulse with the referred phases and building characteristics identified.

Besides these two waveforms, it is also important to refer the parameters that can be configured for Bursting Strategies. In here, besides primary pulse amplitude and width, also resolution can be configured since it is an important factor on the building of pulse. In this waveform type, the building of pulse is also done by concatenation of arrays through iteration but in this case each iteration adds an array that can be divided in two parts: the first part is a set of primary amplitude values with length equal to half of the resolution multiplied by 1ms of array elements and the second part is a set of zeros with the same length of the first part. Iteration is done up to a number of steps which is obtained the same ways as in previous waveform, i.e., result of dividing primary pulse width by resolution. Figure 4.13 shows a pulse built making use of Bursting Strategies waveform type.

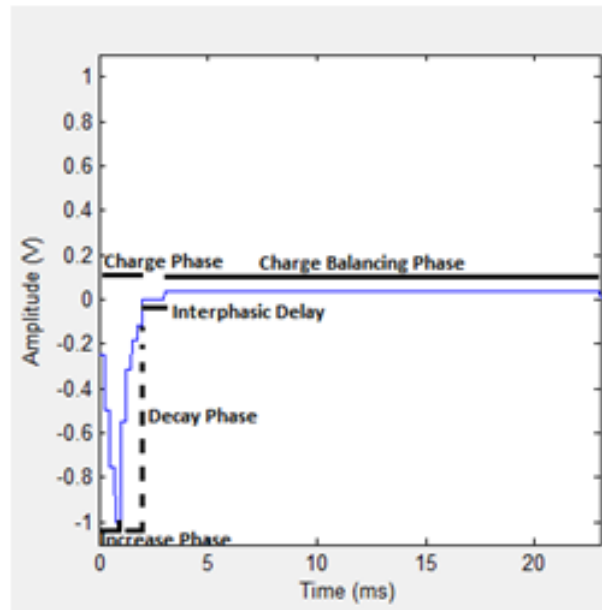


FIGURE 4.12: Tri-Exponential waveform-based pulse.

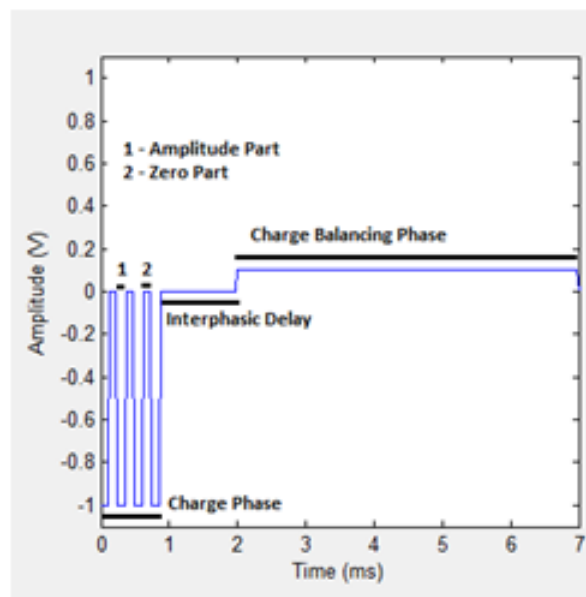


FIGURE 4.13: Tri-Exponential waveform-based pulse.

A common event in the function of all the edit boxes referred is that, when an edit box is used and an input is placed, the initial stored pulse is substituted by a new pulse, built from the beginning, using the new input value and the already stored information, either pre-defined or input, of the other parameters. The pre-defined values for the aforementioned edit boxes can be seen in the figures from edit boxes presented. Similarly to secondary amplitude and width edit boxes, the edit boxes that are specific to a waveform are locked when that waveform is not selected.

4.1.3 Configuring Interphasic Delay

Regarding configuration of interphasic delay, similarly to what was done with the previous parameters, an edit box was created, as it can be seen in Figure 4.14. Equally similar to the boxes, the function behind it is the same as the one behind waveform type pop-up menu, meaning that when a value is input in this box, the pulse is again rebuilt using the Equations 4.1, 4.2, 4.3 and 4.4 according to the new interphasic delay value, taking into account the waveform type selected, which is especially important for the building of charge phase array, and the already input, or pre-defined, relevant parameters.

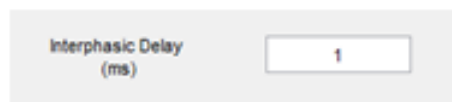


FIGURE 4.14: Interphasic Delay edit box.

The pre-defined value for interphasic delay is, as it can be seen in Figure 4.14, 1 ms.

4.1.4 Configuring Biphasic Ratio

Concerning configuration of biphasic ratio, an edit box was also created as shown in Figure 4.15. The functioning of this edit box is equal to the one from interphasic delay, i.e., the pulse is again rebuilt using the same equations according to the new biphasic ratio value and taking into account the waveform type selected and the remaining relevant parameters already stored.

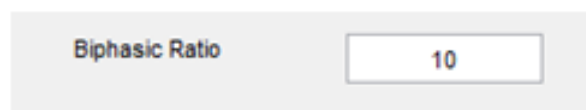


FIGURE 4.15: Biphasic Ratio edit box.

Biphasic Ratio is preset to 10. It is also possible to override Biphasic Ratio in order to have a monophasic pulse by setting it to zero value.

4.1.5 Configuring Pulse Repetition and Stimulation Duration

Regarding configuration of pulse repetition, two configurable parameters were made available: repetition rate and repetition amplitude ratio. Repetition rate is the frequency, in kiloHertz (kHz), at which the whole pulse is repeated throughout the full

stimulation duration. Repetition amplitude ratio is a ratio which is applied to the pulse between every repetition. This allows the user to give a repetitive stimulation with increasingly higher or lower stimulation pulses. For both of these parameters edit boxes were created that allow the user to input desired values and they both work in a similar way, the only difference being the parameter that is changed. Figure 4.16 shows both edit boxes with respective pre-defined values.

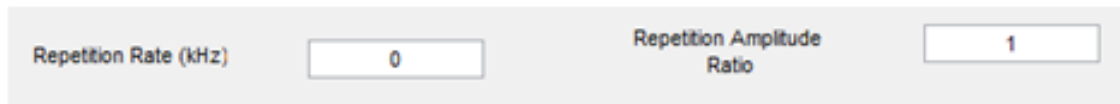


FIGURE 4.16: Repetition Rate and Repetition Amplitude Ratio edit boxes.

The function behind both of these edit boxes is the same and consists of an iteration within which a concatenation of three arrays is done. The first array is the stimulation array which is initially composed by one pulse and is where all the stimulation will be stored; the second array is an array of zeros with length equivalent to the interpulse delay; and the third array is an array of one stimulation pulse multiplied by the repetition amplitude ratio. Interpulse delay is the inverse of repetition rate meaning it is the time between repetitions. The number of iterations done is the result of dividing the duration defined for the whole stimulation by the sum of duration of a pulse with interpulse delay.

Stimulation duration is a very important parameter and can also be programmed through the edit box presented in Figure 4.17. The operation of this edit box is similar to the repetition rate and repetition amplitude ratio, i.e., applying concatenation of the three arrays abovementioned by iteration. The value that is presented in the edit box is automatically calculated whenever a configuration change of the pulse is made.

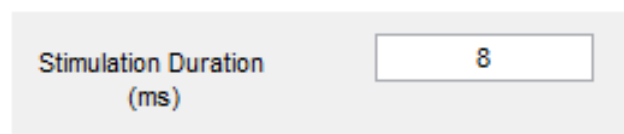


FIGURE 4.17: Stimulation Duration edit box.

The real effect of these parameters on the stimulation profile being configured is however not done in the computer but instead in the microcontroller. In fact, the array here built serves only to create the stimulation profile so that user can see the result. The most important outcome of using these parameters is the number of repetitions, the interpulse

delay and repetition amplitude ratio, information which will be sent to microcontroller and whose use will be explained further, in Section 4.2.

To allow the user to have a better insight on the pulse that is being programmed, a set of axes was also included in the user interface, which responds to when waveform type is changed and is updated when user presses a pushbutton identified as “Plot”. Figure 4.18 shows both the axes area and the plot pushbutton created.

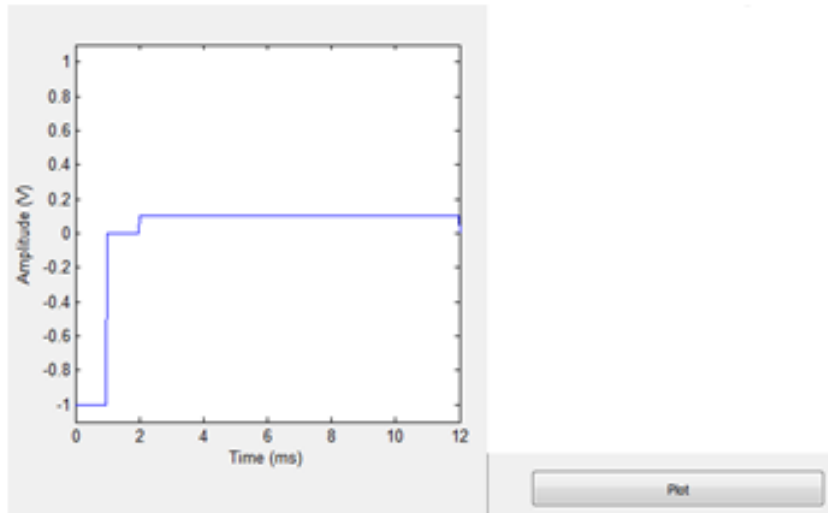


FIGURE 4.18: Axes area and Plot pushbutton.

4.1.6 Configuring Channels

As was mentioned previously, the system here presented is composed by four channels therefore it is of utmost importance that the user-system interface has the capacity to allow the user to control all available stimulation channels. To allow an easy configuration of any of the channels independently, a pop-up menu was created that would allow the user to choose the channel through which the configured stimulation will be applied. Figure 4.19 shows the mentioned pop-up menu.

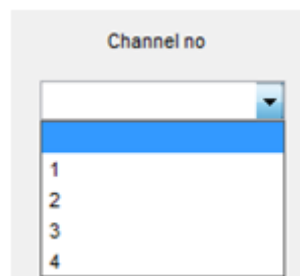


FIGURE 4.19: Channel pop-up menu.

The change of channel does not lead to any changes on the rest of parameters present but instead informs the microcontroller which channel is being programmed.

Another important parameter is control over the way stimulation channels are used, or in other words, the firing type. To this end another pop-up menu was created, as shown in Figure 4.20. This menu allows the user to choose between three different uses of stimulation channels: alone stimulation, synchronous stimulation and asynchronous stimulation.

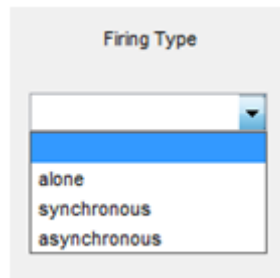


FIGURE 4.20: Firing Type pop-up menu.

Alone stimulation consists of using a single channel to apply stimulation, which can be any of the four channels available. Synchronous stimulation is a stimulation firing type where up to four channels can be used and consists of starting to apply the stimulation at the same time in all channels. Asynchronous stimulation is a type of stimulation firing where users can use up to four channels and its operation consists of applying the stimulation one channel at a time, sequentially, from Channel 1 to Channel 4, with a delay, or time lag, between them. To allow even more configurability of this firing type, an edit box to configure this delay, in milliseconds (ms), was also created – see Figure 4.21.

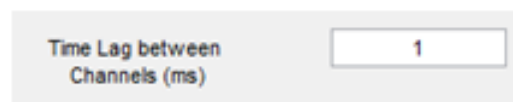


FIGURE 4.21: Time Lag edit box.

It is also important to mention that, in both synchronous and asynchronous firing types, stimulation can be based on different waveforms, different amplitude values and a different number of repetitions. In the synchronous case, however, the repetition rate of stimulations in all the channels used has to be the same.

These firing type definitions don't have any effect on the rest of the waveform parameters, except for the fact that whenever asynchronous is not selected the Time Lag edit box is locked, and its information is sent to the microcontroller.

4.1.7 Configuring Maximum Amplitude Voltage

Due to some electronic limitations of the front-end circuit, which will be described later in Chapter 5, this stimulation system has a maximum amplitude voltage that can be applied during stimulation, beyond which the stimulation profile will not be output as programmed. This maximum voltage is determined to be 5 V but it can vary, and its variation is mainly dependent on the output impedance. Here, the biggest influence comes from the electrode impedance which varies from electrode to electrode, depending on characteristics such as electrode material and size. Hence, with this in mind, a panel with two edit boxes was created: one for user to input the impedance of electrode that is going to be used, if known; a second one, which is locked and not available to be edited, that will only be used to present to the user the calculated maximum amplitude voltage. This panel can be seen in Figure 4.22.



FIGURE 4.22: Electrode Impedance panel.

Due to the importance of this limitation, an additional measure was taken, which consisted in programming a dialog box that warns the user for this limitation and allows him to input the electrode impedance value – see Figure 4.23. In case the user inputs the impedance, the respective values will appear on the panel shown in Figure 4.22. Otherwise, the warning window in Figure 4.24 will appear, to warn the user that maximum amplitude was not calculated.

The calculation of Amplitude Maximum from the Electrode Impedance value is done through Equation 4.8.

$$A_{max} = \frac{A_{max,def} * R_{set}}{Z + R_{set} + 2R_{internal}} \quad (4.8)$$

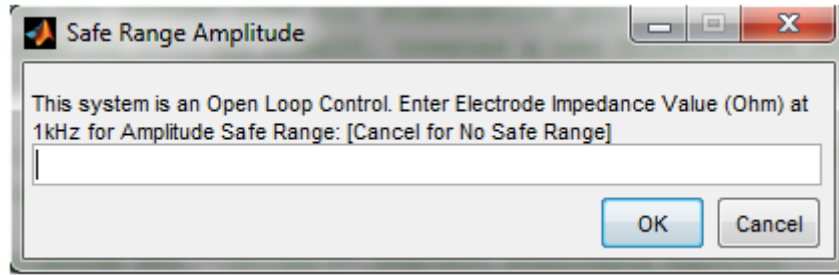


FIGURE 4.23: Electrode Impedance dialog window.

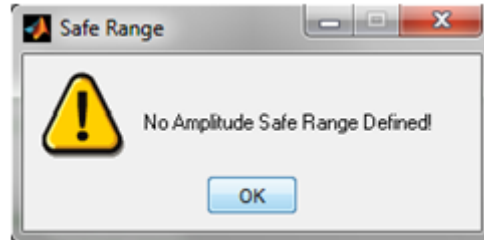


FIGURE 4.24: Warning window when no Electrode Impedance value is input in dialog window.

In Equation 4.8, A_{max} represents Maximum Amplitude calculated, $A_{max,def}$ is the maximum amplitude by definition, both in Volt (V), Z is the electrode impedance, R_{set} is the value of set resistor, which will be explained further in Chapter 5, and $R_{internal}$ is the resistance from the switches used, the three of them in Ohm.

4.1.8 Overall Operation and Communication with Microcontroller

The resulting interface is shown in Figure 4.25 and, as it can be seen, presents all the requirements and respective components referred in the last sections.

As can be seen in Figure 4.25, there are three pushbuttons that were not referred previously. This was because these pushbuttons are not related to the configurability of stimulation profile but instead are used for communication with the microcontroller. The diagram shown in Figure 4.26 represents the operation of the MATLAB-based user-system interface.

The diagram from Figure 4.26 shows that there are three configurations that are of most importance to be chosen first, which are the Firing Type, Waveform Type and Channel Number. While the information on the first and the third configurations are simply stored to be sent later to the microcontroller, the Waveform Type configuration is, as said before, associated to other parameters available for configuration. As can

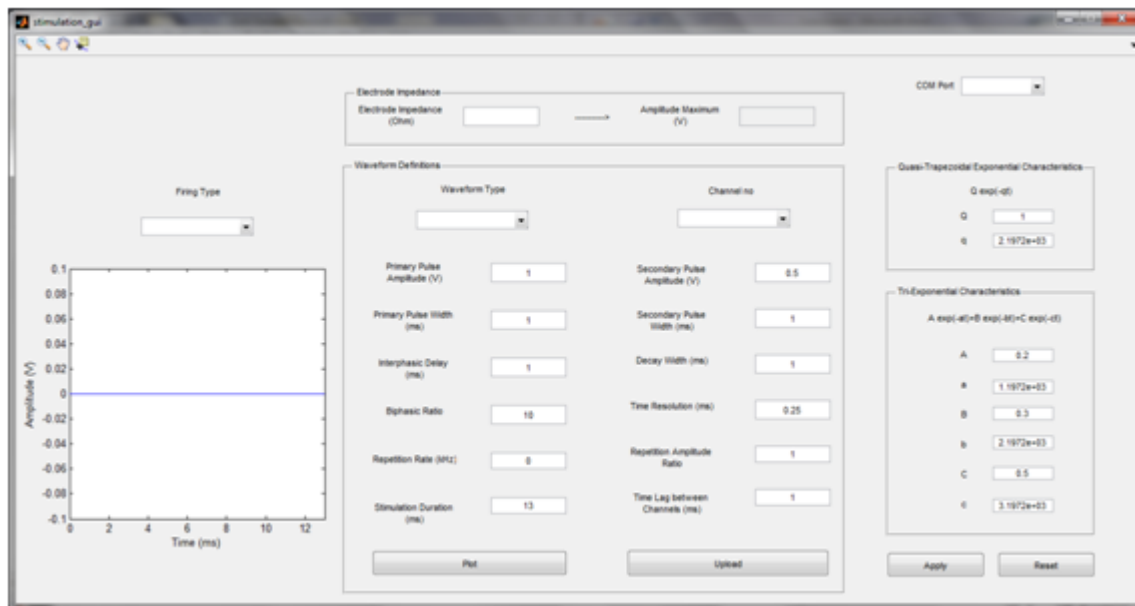


FIGURE 4.25: Full User-System Interface.

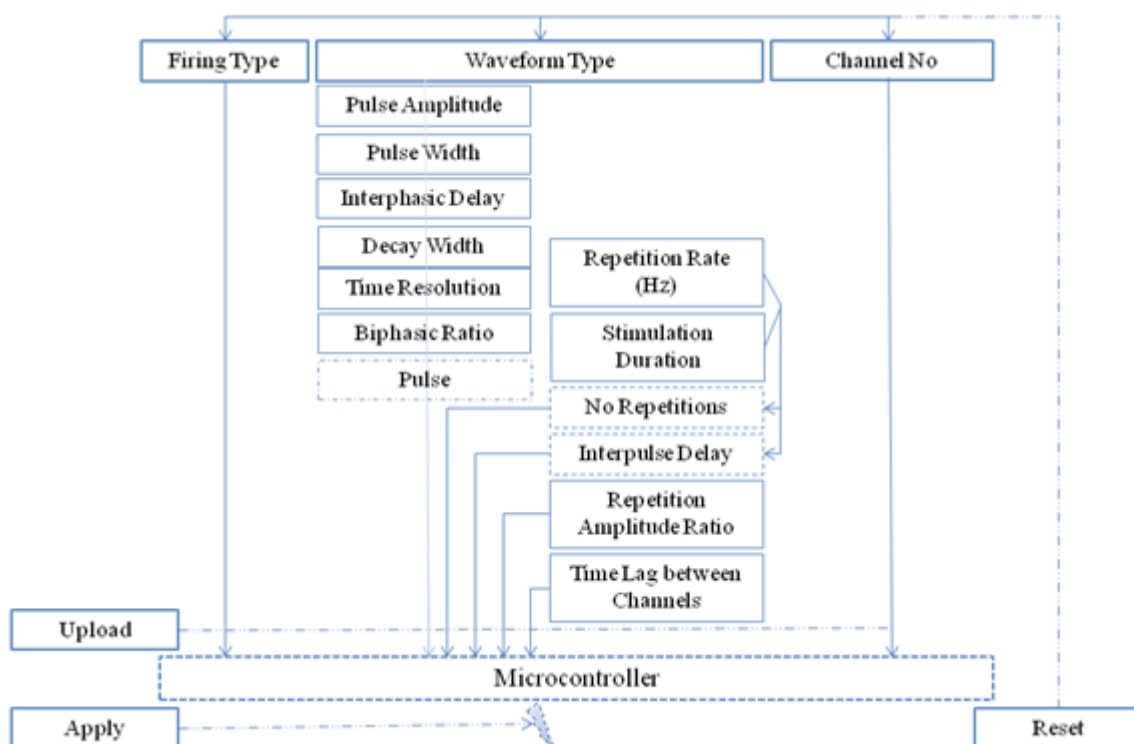


FIGURE 4.26: User-System Interface Operation Diagram.

be seen in the diagram, after choosing the waveform type, a single stimulation pulse is built based on values defined for parameters pulse amplitude, width, interphasic delay, decay width, resolution and biphasic ratio, either pre-defined or defined by the user, which is then stored. Parameters such as Repetition Rate and Stimulation Duration are used to obtain the number of repetitions and the interpulse delay which are then

stored. Also stored with no processing are the values of Repetition Amplitude Ratio and Time Lag between Channels. This stored information can then be transferred to the microcontroller by pushing “Upload” button – see Figure 4.27. When this pushbutton is pressed, MATLAB starts a communication protocol which consists of signaling the piece of information that is going to be sent and then sends it. It is important to refer that, regarding pulse upload, MATLAB sends the absolute values of the pulse and, instead of sending negative values, it sends a signal to the microcontroller of when in the pulse there is a variation from negative to positive, or vice-versa, or a variation to or from zero. The state of the transfer of information is transmitted to the user by a waiting bar, present in Figure 4.28.

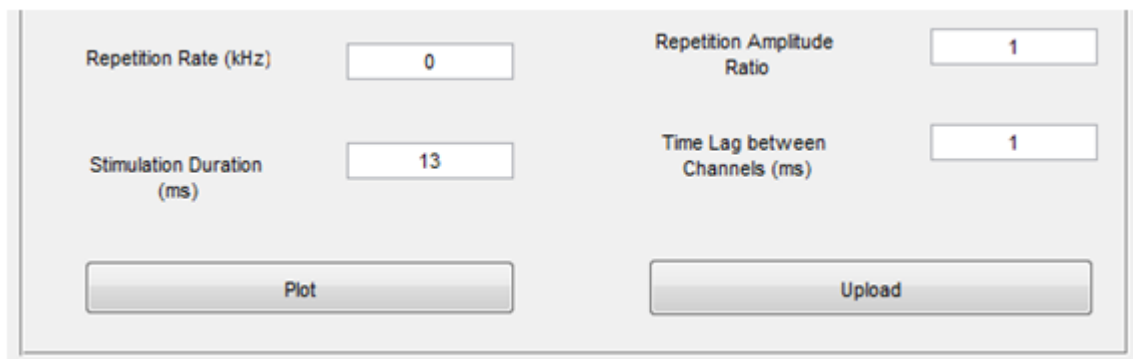


FIGURE 4.27: Upload pushbutton.

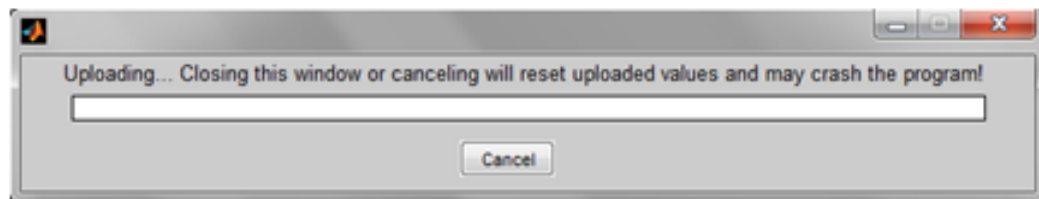


FIGURE 4.28: Waiting Bar window.

After sending all the information, the user can then decide to upload pulses for the other channels, if the firing type is either synchronous or asynchronous, or change the pulse programmed for the same channel. Furthermore, the user can decide if the configurations done are enough and choose to apply the respective stimulation or decide to clear all the information stored in microcontroller. If user decides to apply, the “Apply” pushbutton has to be pushed after which stimulation is applied and the information existent in microcontroller is subsequently cleared. If user decides to clear all the information in the microcontroller, the “Reset” pushbutton has to be pushed, after which no information will remain stored in microcontroller. Figure 4.29 shows these last referred pushbuttons.

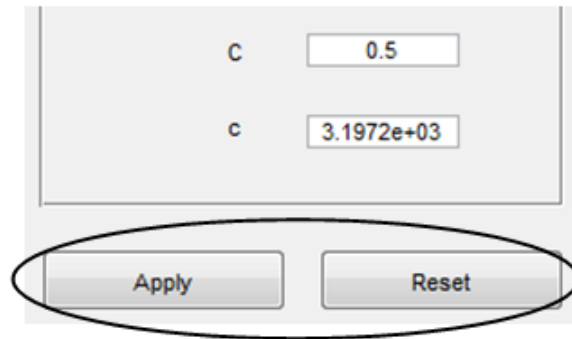


FIGURE 4.29: Apply and Reset pushbuttons.

To allow for a better operation of this user-system interface, other pop-up menu was also included identified as “COM Port” – see Figure 4.30. The reason behind the creation of this menu was the fact that connection of microcontroller to COM ports from computer was many times in the origin of problems related with sending information to the microcontroller, more specifically its misidentification. The pop-up menu here created only shows the COM ports being used at the time and this way allows user to easily change the port or correct if the wrong one is being used.

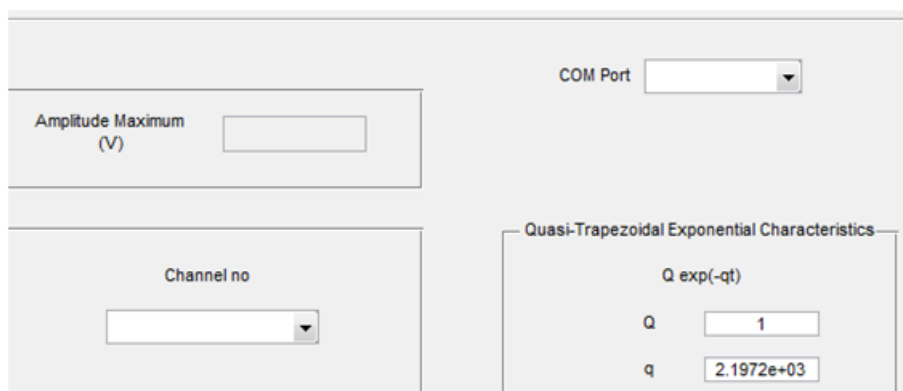


FIGURE 4.30: COM Port pop-up menu.

4.2 *Freescale* Microcontroller FRDM-KL26Z

As already mentioned in the previous chapter, the role of microcontroller is to receive the information about stimulation parameters from MATLAB and then use it to control a front-end stimulation circuit in order to produce stimulation as desired by user. The microcontroller used for this work was a *Freescale* FRDM-KL26Z which was programmed through an integrated development environment (IDE) called CodeWarrior that allows

for software writing, compiling and debugging in C programming language. A diagram representing the operation developed for the MCU is presented in Figure 4.31.

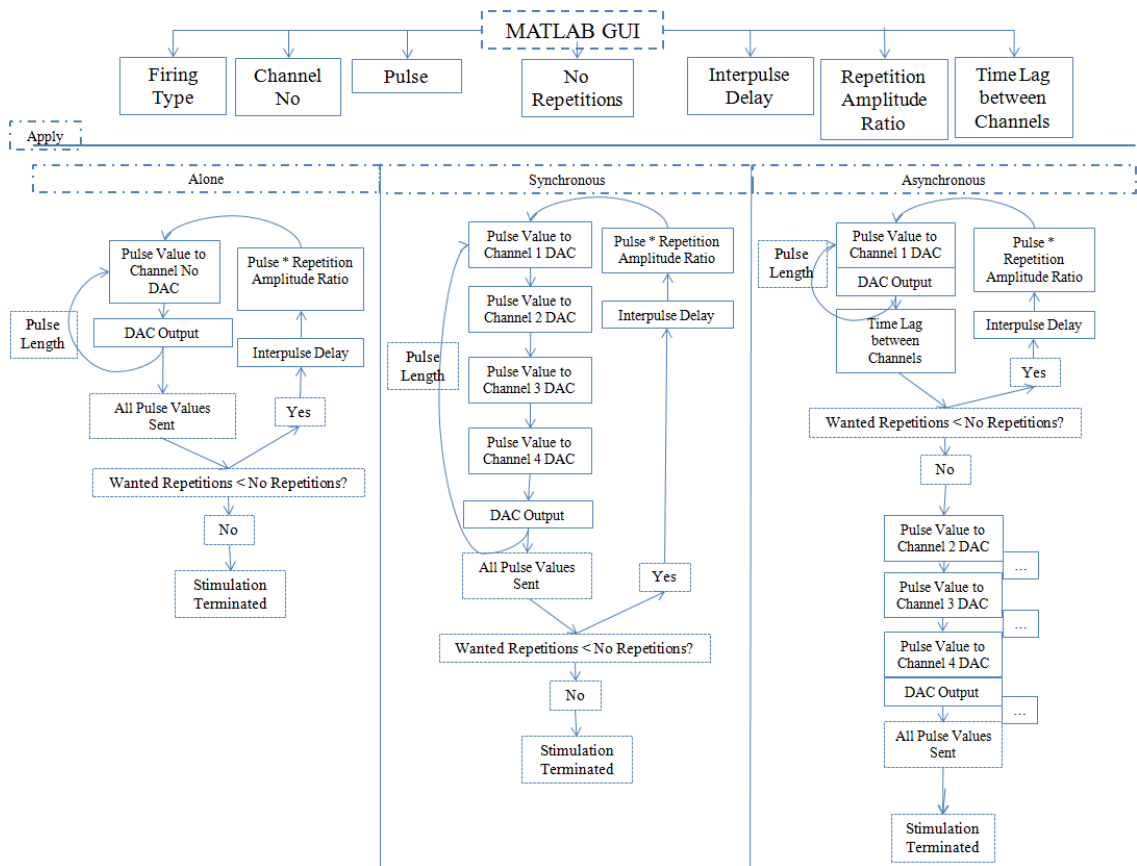


FIGURE 4.31: MCU Operation Diagram.

The microcontroller's role starts when information is being sent by MATLAB. As it is possible to see, the information is: firing type, channel number, single stimulation pulse, number of repetitions, delay between repetitions (interpulse delay), repetition amplitude ratio and time lag between channels.

The first step of the microcontroller is to identify the firing type being used. If it is the alone firing type, then each value from the single stimulation pulse is sent to the DAC via SPI and output by the user-defined DAC channel. After all values from a single pulse are sent, the microcontroller checks if there are repetitions to be done. If not, it ends the program, otherwise it calculates and updates the pulse values, depending on the value of the repetition amplitude ratio, and causes a delay, the interpulse delay, after which it starts sending values to DAC which outputs it. This cycle is repeated until there are no more repetitions to be made.

If the synchronized firing type is chosen, the main difference from the alone firing type is that instead of sending only one value to the DAC, one value per channel used is sent from the respective single stimulation pulse. Only after every used channel has its values, the DAC outputs the values, from all channels at the same time. After all values from a single pulse from all channels are sent and output, the procedure is similar: the microcontroller checks if there are repetitions to be done. If not, it ends the program, otherwise it calculates and updates the pulse values, depending on the value of the repetition amplitude ratio, and causes a delay, the interpulse delay, after which it starts sending values to the DAC which outputs it. This cycle is repeated until there are no more repetitions to be made.

Lastly, if the asynchronous firing type is chosen, the microcontroller essentially produces one alone firing type after the other, one for each of the channels selected, with a delay between them – the time lag between channels. After this the DAC output phase is done. The repetition procedure is the same as previous firing types. Besides the indicated, other information is also received together with the pulse values, as referred to in the previous section, which is the location of signal variations on the pulse. This information is stored along with the pulse and used with it. Its purpose is the activation and deactivation of pins whose function is to control a switch which will allow for change of current direction and thus obtain both cathodic and anodic phases. This is needed because all pulse values stored in the microcontroller are absolute values and also because the DAC used does not output negative voltages. This is further explained in more detail in the following chapter.

It is important to refer that the microcontroller also has LED signaling that is used to indicate its internal state:

- Green LED – no information stored in the microcontroller. This LED turns on when the microcontroller is powered up, after stimulation is applied or if the Reset button is pushed.
- Blue LED – information stored in the microcontroller. This LED turns on after upload is done.
- Red LED – work in process. This can either be when an upload is being done and when stimulation is being applied.

Chapter 5

Hardware Development

As mentioned previously, the stimulation system whose development is being described in this thesis is composed by two main parts, software and hardware. In Chapter 4, a description of the software component of the stimulation system was done. In this chapter we will describe the hardware part of this system. The hardware part of this system is responsible for application of the electrical neural stimulation according to the information that comes from the user configuration done in the software part.

Throughout this chapter a description of the requirements for this hardware platform will be done, the different components that make the platform and the work developed in each of them will be described, and lastly a description of the platform operation will be made.

To design and develop the circuits for the board, simulations of circuits were firstly done through the use of *Cadence OrCAD Capture* and *Texas Instruments TINA*. These are circuit simulators that allow for circuit sketching and simulation using components from external sources, such as the fabricators of the components, thus allowing a more reliable simulation. After this stage the circuits were tested in a breadboard. The actual board was developed using *Altium Designer* program which allows the development of printed circuit boards (PCB) by firstly providing a schematic area where the circuits can be sketched – also with components from external sources – and then, based on those circuits, a 3D workspace is presented where a PCB board appears along with the components defined in the sketch of the circuit. In this 3D workspace the user can then shape the board and place the components in the board where desired. After that the

connections between the components are created, which can be done via auto-routing – where the program tries itself to make the connections – or it can be done by the user. This can be done on the top surface of the board or using any of the layers of the board, a characteristic of a tridimensional board that can also be configured by the user.

5.1 Requirements

As stated before, the hardware part of this system is responsible for the actual application of neural stimulation according to what was configured by the user in the user-system interface. Even though its operation is controlled by the microcontroller, the front-end board should be able to transform that control into a correct stimulation. With this in mind, essential requirements were defined for this board:

- To have its own power supply;
- To have its own voltage reference;
- To be able to receive digital pulse information from MCU and convert it to analog amplitude value;
- To have four equal stimulation channels;
- To apply a current-controlled stimulation;
- To be able to apply bi-directional current.

The following chapters will describe the components chosen and the work developed to accomplish all these requirements for the stimulation system front-end board.

5.2 Components

In order to accomplish a current-controlled stimulation system, the front-end board was defined to be composed by power supply circuits, reference voltage circuits, a 16-bit quad-DAC, opamp-based voltage-to-current converter and a set of switches. In the following sections a description of the referred board components will be done, focusing on

negative and positive output but also because it can do it from a single positive supply with a range from 1.2 V to 15 V. This circuit, and the values of additional parts used, is based on recommendations from the datasheet of DC/DC converter used in order to obtain an output in negative supply (VSS) of -9 V and in positive supply (VDD) of +9 V and it was successfully tested with a external supply (VBAT) of 5.5 V.

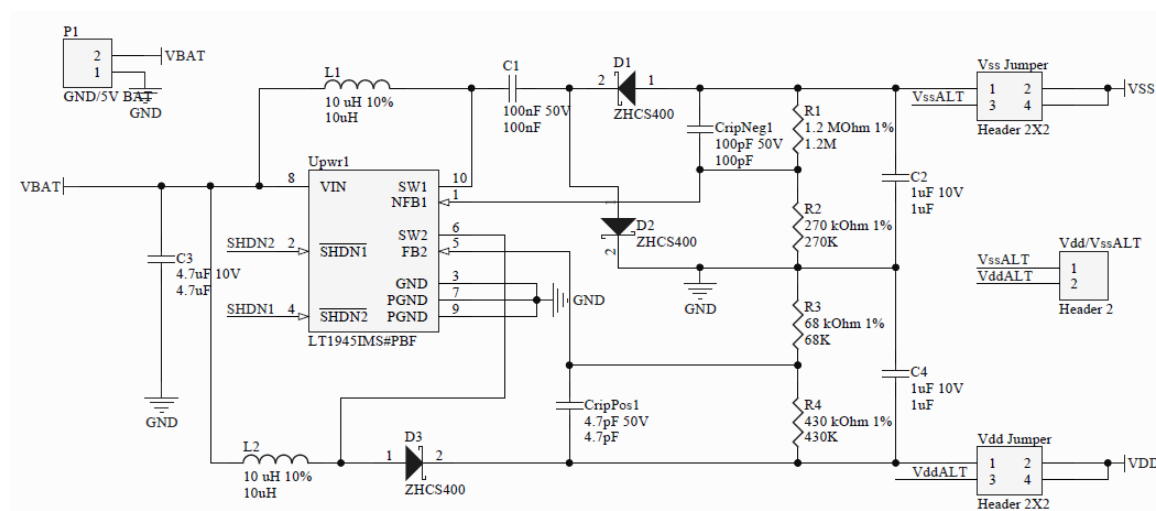


FIGURE 5.2: DC/DC converter circuit schematic.

As it is possible to see in the schematics presented in Figure 5.2, four headers were used in this circuit. The first one, 'P1', is the one where the external power supply should be connected to power up the DC/DC converter. At the end of the DC/DC converter circuit there are 2 headers, 'Vss_Jumper' and 'Vdd_Jumper', which are here placed with the purpose of allowing the user to choose between using the DC/DC converter supply to the components or a different external supply. The 'Vdd/VssALT' header is then to allow the user to connect the external supply. The placements in the board are shown in Figure 5.3 and highlighted by the black, blue and red circle, respectively.

These defined positive and negative values output by the DC/DC converter circuit are suitable for supply of most electronic parts used in this board except for the DAC which, in turn, needs a supply voltage of 5 V. In this case, the voltage supply is given by the LP3985 LDO voltage regulator whose schematic is in Figure 5.4. A LDO regulator is a linear voltage regulator which can have a steady output voltage from a defined range of input voltage and whose difference between input and output can be small – low dropout. This LDO in particular, the LP3985, was chosen because it is low power, has low noise and very low-dropout voltage and it can have a 5 V output from an input

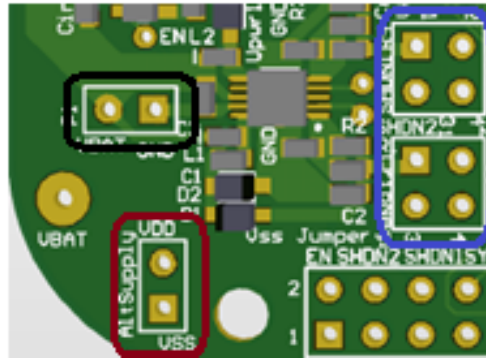


FIGURE 5.3: Placement on the board of VBAT power supply header (black), VDD and VSS jumpers (blue) and Vdd/VssALT alternative supply header (red).

range of 5 V plus dropout voltage, which was of 100 mV, up to 6 V. This input range is included in the range of DC/DC converter input which is important for the definition of external source voltage.

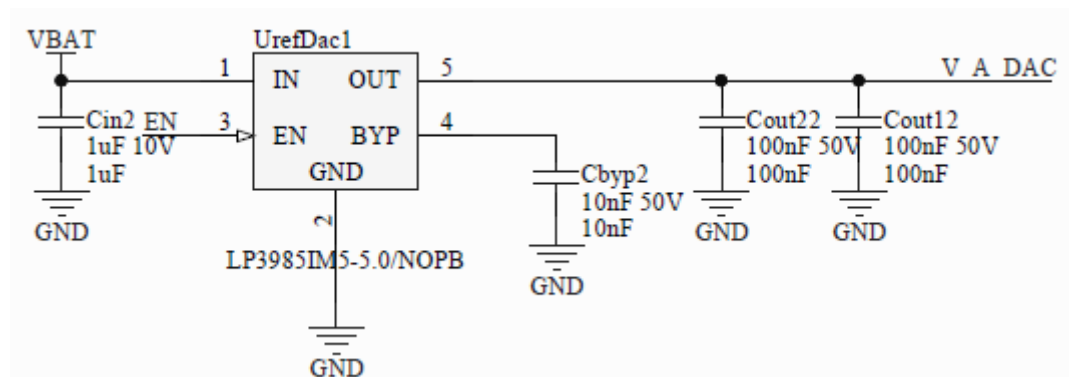


FIGURE 5.4: Schematic of DAC's power supply circuit.

Other important characteristic of the DC/DC converter and LDO chosen is the possibility of shutting down the output until desired through an enabling pin. In the DC/DC converter, there are two enabling pins, identified as SHDN1 and SHDN2, and in the LDO there is one, identified as EN. These are logical pins which enable output when they are high and disable when low and are connected to the MCU which is programmed to only enable them when MCU is completely functional. This way, by controlling these pins, there is no need to wait for the MCU to be on to connect the board to the battery to avoid any unintentional charge delivery.

It is important to refer that a misnaming happened in the designing of the board. In Figure 5.4, the name of the component should be 'UpwrDac1' instead of 'UrefDac1', and

the inverse problem is verified in the reference circuit for the DAC.

5.2.2 Reference Voltage Circuits

Identified by the red line in Figure 5.1 is the reference voltage circuit. As previously mentioned, it was a requirement that this board could have its own reference voltage, distinct from the power supply circuits. This circuit is equal to the one responsible for the DAC power supply, with the same source from the battery and an output of 5 V as well, as this was defined as the voltage reference value. DAC's power supply and reference voltage could be connected to the same LDO output however it was decided to have one for each so that higher stability could be obtained. Figure 5.5 shows the schematic of the circuit. It is important to remind, once again, of the misnaming of LDO in the schematic and in the board.

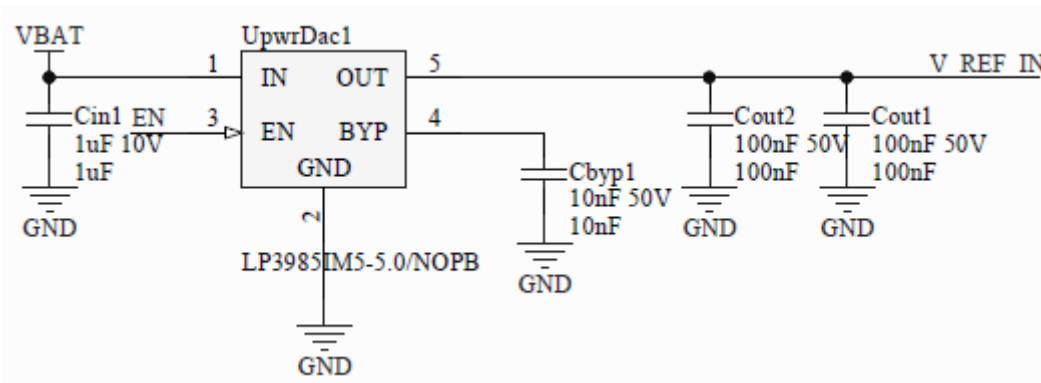


FIGURE 5.5: Schematic of DAC's reference voltage circuit.

5.2.3 Stimulation Application Circuits

Highlighted by the black, blue and white lines in Figure 5.1 are, respectively, the DAC, voltage-to-current (V-to-I) converter and switches. As initially mentioned, it was a requirement that this board would be able to receive digital pulse information from MCU and convert it to analog amplitude value and also that would have four equal stimulation channels. To accomplish this, there were two options: either to have four DAC, one DAC for each channel, or a DAC with four outputs, called quad-DAC. For this board the second option was decided, with the DAC124S085 Quad-DAC being the chosen one. The choice of this DAC is due to the fact that it is based in a 16-bit serial communication,

which is the same communication type of MCU and also because, of the sixteen bits, twelve are for the digital values, meaning it allows to have a good amplitude resolution – approximately 1.2 mV for this case since the DAC can output a voltage amplitude up to voltage reference which is 5 V – and the remaining four bits are for channel selection and mode of operation, which include important options such as sending information to a specified DAC channel and output it or not, or to send an information to all the channels and output it. However, when output is done, all channels give an output and it is not possible to have only one at a time. The connections of DAC used are represented in the schematic of Figure 5.6.

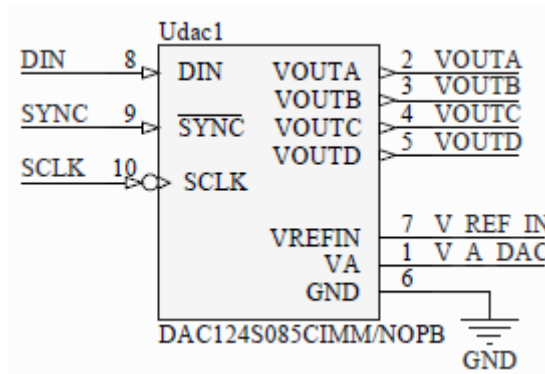


FIGURE 5.6: DAC schematic representation.

After the DAC, is then a V-to-I converter followed by a switch. The V-to-I converter is necessary because it is a requirement to be a current-controlled stimulation system and the DAC output is voltage amplitude. It was desired that this V-to-I converter could be as simple as possible so it was initially considered to use the *Texas Instruments* XTR111 V-to-I converter, however this product was only available as Surface Mount Device (SMD) and so to test it in a breadboard would mean that other electronic parts had also to be bought making this an expensive option. The least expensive alternative thought was then to design our own V-to-I converter based on an opamp, this way allowing for easier and cheaper testing on a breadboard. To maintain as simple as possible, the circuit designed was simply an opamp-based V-to-I converter, as it is presented in Figure 5.7. The opamp chosen was the AD744 due to its fast-settling, relatively good slew-rate, low total harmonic distortion (THD) and external compensation for stable operation.

In a V-to-I converter such as the one in Figure 5.7, the current amplitude generated by

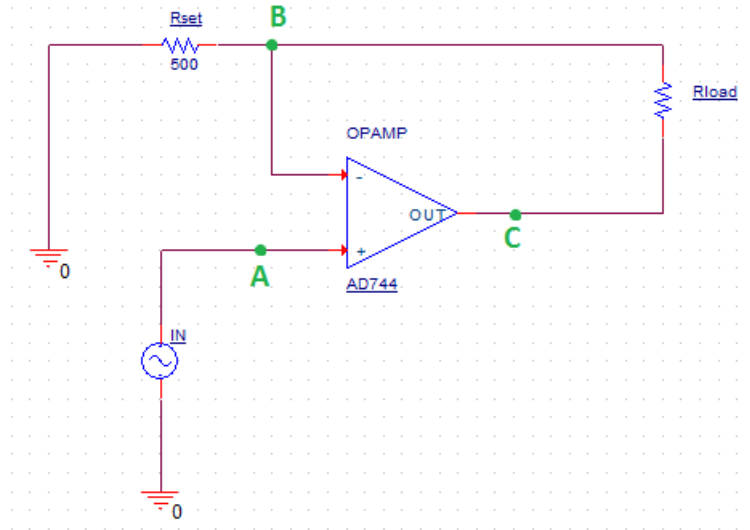


FIGURE 5.7: Cadence OrCAD schematic of V-to-I Converter.

the input voltage amplitude is defined by the setting resistor R_{set} , since the voltage potential in inverting input V_B is the same as in non-inverting input V_A , which corresponds to the input voltage coming from the DAC, and R_{set} is between V_B and ground. As current entering the opamp input is substantial, the current in R_{set} is the same in R_{load} which in this situation represents the impedance from switches, electrodes and tissue. However, this also means that the voltage potential on the output of the opamp, V_C , is dependent on the value of R_{load} and this simplicity of the V-to-I converter circuit leads to a major limitation which is related to the maximum amplitude that can be at opamp output, i.e., the opamp saturation limits which are given by the power supply. This means that R_{set} had to be chosen carefully so that it could have a good current range but could also handle reasonable values of load impedance. The maximum current amplitude was defined as 10 mA with a 500 Ohm setting resistor, since the maximum DAC output is 5 V. This limitation here referred is the reason why in user-system interface there is maximum voltage amplitude warning. As tissue impedance is very small compared to electrode it is neglected and only switch and electrode impedance is considered as load impedance in calculation of maximum amplitude voltage – see Equation 4.8 in Software Development chapter.

By its turn, the switch is necessary to allow for bi-directional current as required, namely cathodic and anodic current which are very important for charge-balancing. The switch used is an ADG436 Dual Single Pole, Double Throw (SPDT) Switch and its scheme is presented in Figure 5.8. The scheme of this switch then allows designing the circuit so

that not only switching the direction of the current going through the electrodes can be done but also there is a conformation where no current is directed to the tissue.

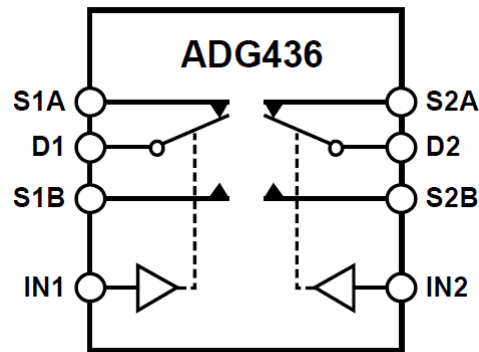


FIGURE 5.8: ADG436 switch scheme.

In this switch, when its Logic Control Input (IN_x) is low the D_x pin is connected to S_xB , when IN_x is high D_x pin is connected to S_xA . The schematic of the circuit designed is presented in Figure 5.9. This means that when $IN1$ is low and $IN2$ is high, and so $S1A$ is connected to $D1$ and $D2$ is connected to $S2B$, cathodic current is obtained. When $IN1$ is high and $IN2$ is low, and so $S1B$ is connected to $D1$ and $D2$ is connected to $S2A$, the opposite current, anodic, is obtained. When both $IN1$ and $IN2$ are low, $D1$ is connected to $S1B$ and $D2$ is connected to $S2B$, and there is no feedback circuit which leads to absence of current going to the tissue and may also allow some remaining charge on the tissue to be dissipated.

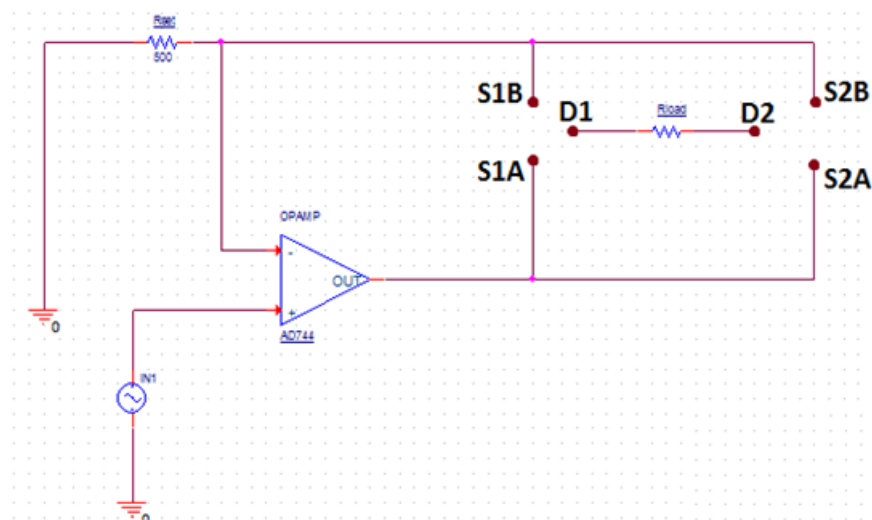


FIGURE 5.9: Schematic of circuit with V-to-I Converter and Switch – single stimulation channel.

In Figure 5.10 is shown the full schematic of a single current-controlled stimulation channel, with both the opamp-based V-to-I converter and switch, in which are included the impedance from the switch – R_{swtA} , C_{stwA} from switch bridge A and R_{swtB} , C_{swtB} from switch bridge B – and also the impedance from the electrode and tissue as described by the Electrode-Electrolyte Model – R_{farad1} , C_{dl1} from electrode 1, R_s of electrolyte or tissue resistance, and R_{farad2} , C_{dl2} from electrode 2.

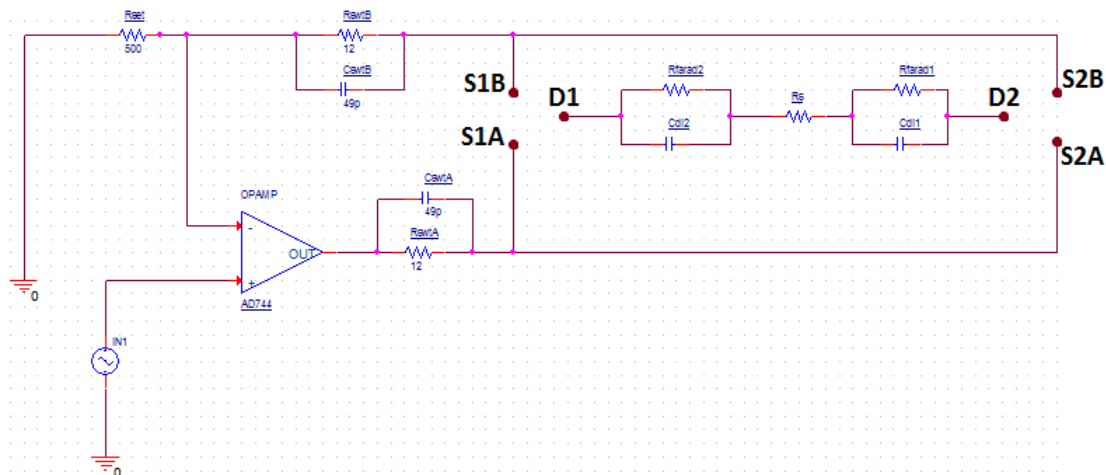


FIGURE 5.10: Schematic of a single stimulation channel circuit with converter, switches and electrode impedances.

In Figure 5.11 is shown the same single stimulation channel but in the Altium schematic.

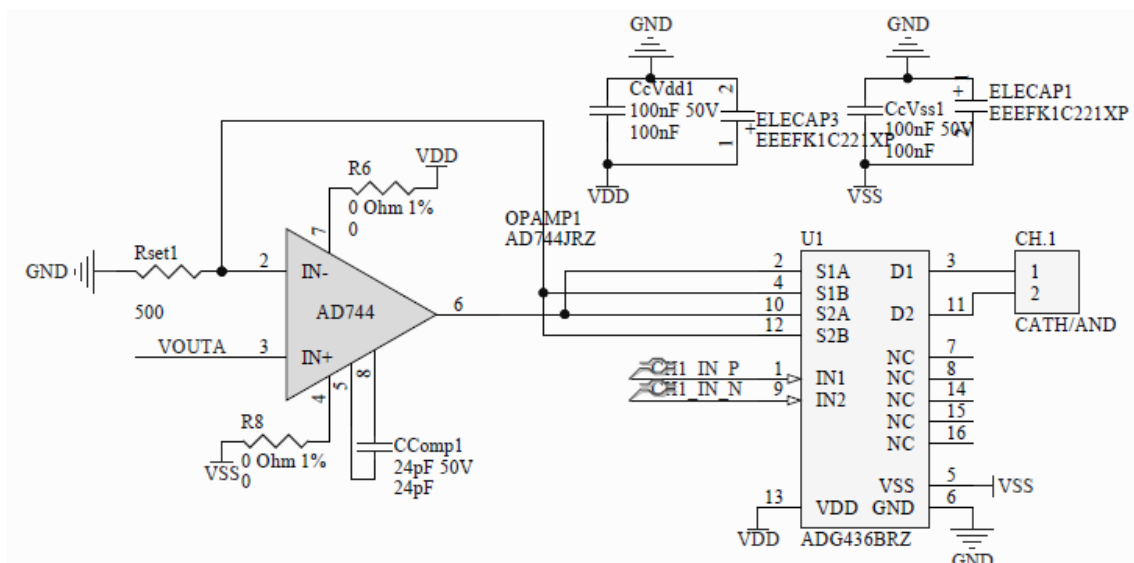


FIGURE 5.11: Altium schematic of a single stimulation channel circuit.

On the top right of the schematic are represented the decoupling capacitors for the VDD and VSS sources. On the left is then the V-to-I converter and on the right, under the

decoupling capacitors, is the switch. Zero Ohm resistors were also placed between the opamp power connections and the power sources in order to allow easy disconnection of a channel and board debugging. It is also possible to see in the schematic the header where the electrodes should be connected, called CH.x, where x will be the number of the channel (1, 2, 3 or 4), which is the place where current will be output from the board to the stimulation site. Their placement on the board is shown in Figure 5.12.

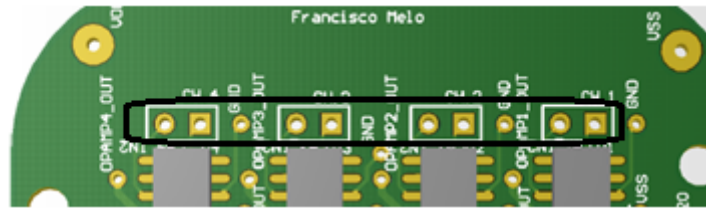


FIGURE 5.12: Electrode placement sites on board.

5.2.4 Microcontroller Connections

The front-end stimulation board here developed is, as it has been mentioned throughout the thesis, essentially controlled by the FDRM-KL26Z microcontroller. To accomplish that control, sites for input and output connections had to be created to allow connection to the specific components. Figure 5.13 presents a 3D vision of the whole stimulation board created with these connections properly identified.

Identified on the Figure 5.13 are then the following board connections to the KL26Z:

- CHx_INxk – is the point of connection between microcontroller and the switch's logic control input.
- DIN – DAC's Serial Data Input.
- SYNC – DAC's Synchronization Input for data input.
- SHDNx – Enable pins (also, shutdown pins) for DC/DC converter.
- UART_TX – connection point to UART transmitter.
- UART_RX – connection point for UART receiver.
- EN – Enable pin for LDOs.
- SCLK – DAC's Serial Clock Input.

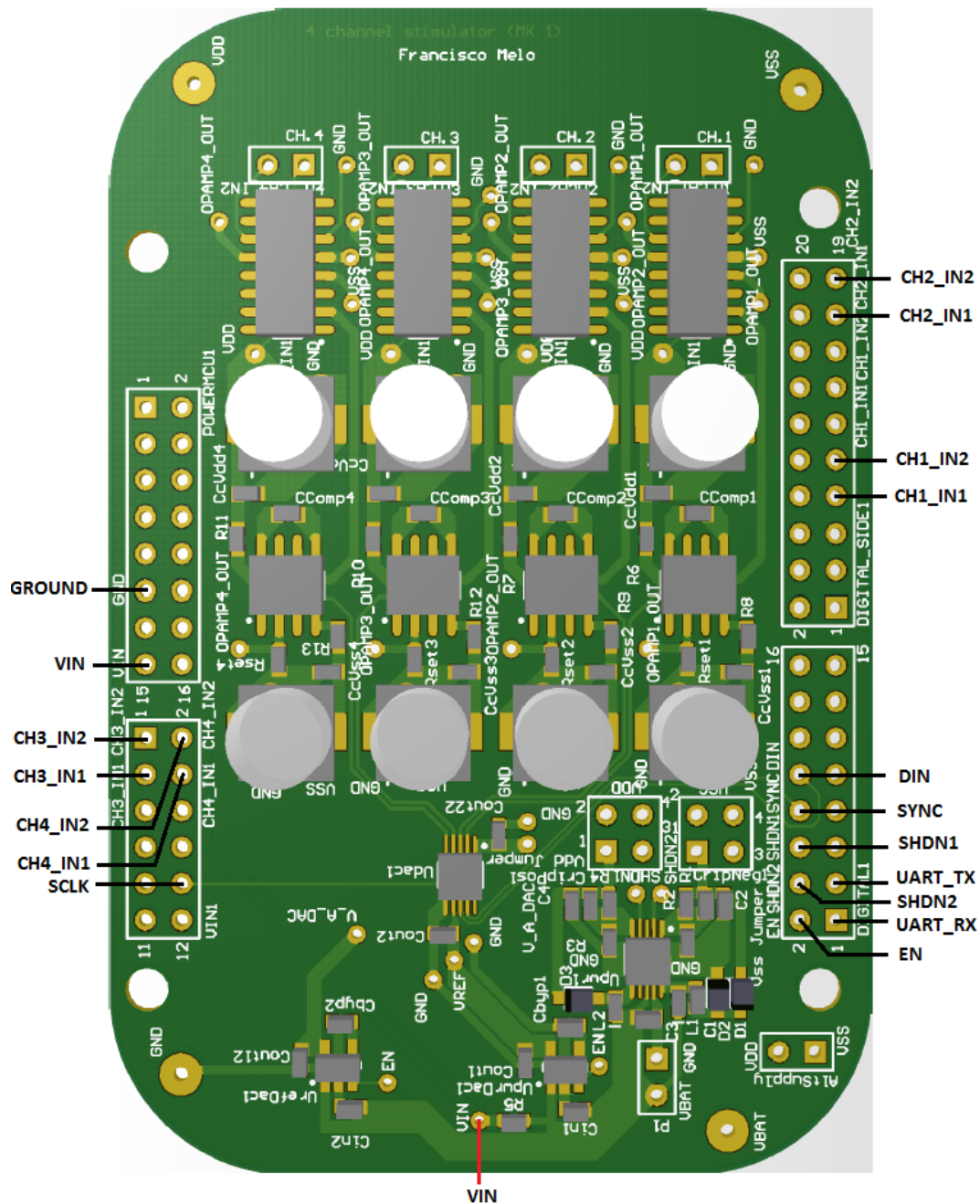


FIGURE 5.13: Input and Output Connection on whole Stimulation Board.

- GROUND – provides ground to the whole system.
- VIN – used to power the microcontroller if it is not connected via USB. In this case, a wire has to be used to connect the connection pin VIN (identified in black) to the power pin (identified in red).

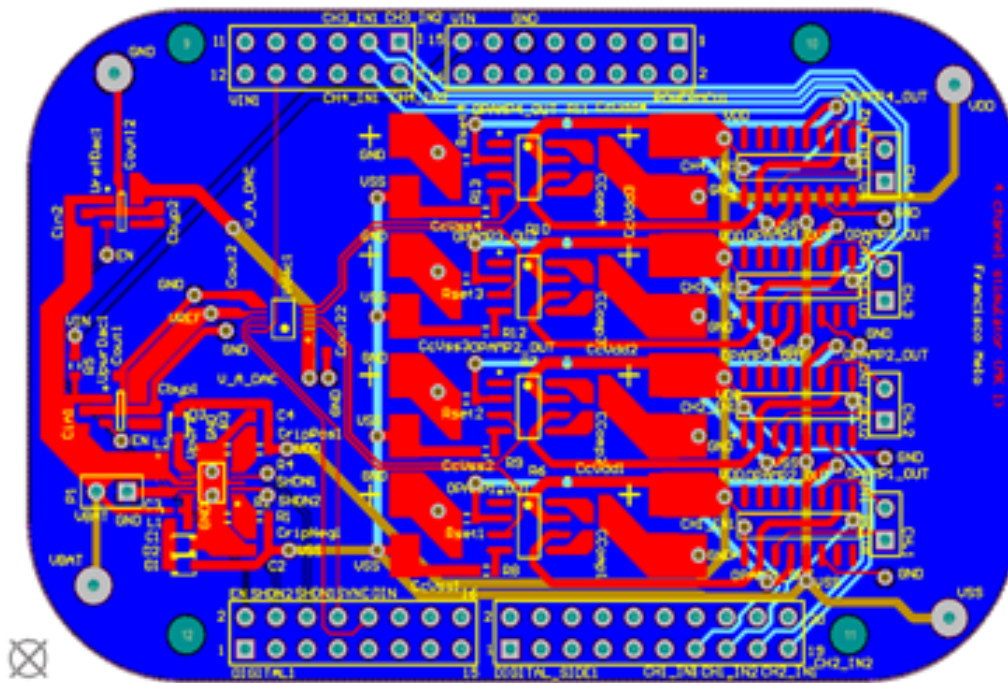
5.3 PCB Design Characteristics

Besides the component placement on the PCB board, there are other very important characteristics that have to be defined to make a perfectly operational board. These characteristics are the connections between the components and the board layers.

As previously mentioned, the connections can be done via auto-routing or can be done by the user. In auto-routing mode the program tries itself to make the connections which, although fast and convenient, have significant limitations. A particular and very important limitation is related to the lack of knowledge of the program regarding the type and amplitude of signals that will pass in each of the connections which is an important concern in order to avoid interference and contamination of signals, also called signal cross-talk. This can occur for example when a wire carrying an analog signal passes near a track carrying a digital signal. It can also occur for example when a high amplitude signal passes near a lower amplitude signal. Another important concern is the width of the tracks carrying the signal, where the greater the signal current intensity, the wider the track should be. This relation comes from the fact that current passing causes a temperature rise on the track which increases with the increasing of the current intensity. This way a wider track allows a better heat dissipation, keeping the temperature within safe and less-damaging limits. For all these reasons, the connections were made by hand.

In Figure 5.14, the connections made between all the components on the board, including the input and output sites, are shown. As it is possible to see, there are tracks that are much wider than the others. These tracks are the ones related to the power supplies circuits since these are the circuits that are required to conduct higher currents. Following these are the voltage reference circuits, which have slightly wider tracks than the remaining connections.

It is also possible to see in Figure 5.14 that the tracks have different colors: red, brown, light blue and dark blue. This color difference is related to the layer where the tracks were made. The red tracks are on the top layer, the brown tracks are on a top-internal layer, the light blue tracks are on a bottom-internal layer, and the dark blue tracks are on the bottom layer. The role of each layer is shown in Figure 5.15 and, as it is indicated, the top layer is mainly for analog signals, the top-internal layer for digital signals, the bottom-internal layer for power connections and the bottom layer for ground

FIGURE 5.14: Board Connections on *Altium*.

connections. The possibility of multilayer routing not only facilitates the hand routing, by allowing that tracks can pass through the same point, bi-dimensionally speaking, but also because it provides isolation to avoid cross-talk between the tracks. Figure 5.15 also shows how the communication between layers is made in a multilayer routing. As it is possible to see, the communication is made through holes that cross the entire board, called “through-holes”, which then connect to a defined layer. In this example, the left ‘through-hole’ allows for connection between a top-layer track and top-internal layer, without connecting with either the bottom-internal or the bottom-layer track. On the ‘through-hole’ on the right however, the top-layer track is connected to both the bottom-internal and the bottom-layer track, but not to the top-internal layer. In between these layers there are non-conductive layers to isolate the conductive ones.



FIGURE 5.15: Layers connections.

It is also important to refer that a pouring layer was placed in the bottom layer, covering the free area of this layer, thus the reason why the board looks dark blue making it hard to understand where the bottom-layer tracks are. The reason to include such a layer is related to the expected use of this board, i.e., since the board is intended to be used with the microcontroller, being installed on the top of it, this pouring layer then acts as a protective layer, between the board and the microcontroller, to avoid interferences between them.

5.4 Full Neural Stimulation Board and MCU Compatibility

The result of the front-end stimulation board here developed is shown in Figures 5.16, 5.17 and 5.18. In Figure 5.16 it is possible to see a 3D image of the full stimulation board with all its components. In Figure 5.17 the real version of the stimulation board is shown only with the tracks and connections for the components. Finally, in Figure 5.18, the full stimulation system with all components already placed and soldered to the board is shown.

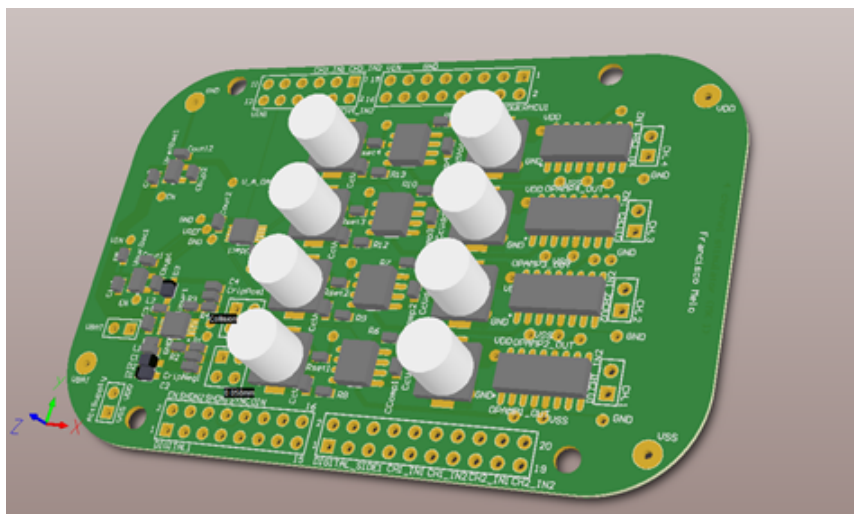


FIGURE 5.16: 3D image of Stimulation Board.

Figure 5.19 shows an image of FRDM-KL26Z microcontroller with its input/output connectors highlighted. For each connector, their connection to the inputs of the front-end stimulation board are identified.

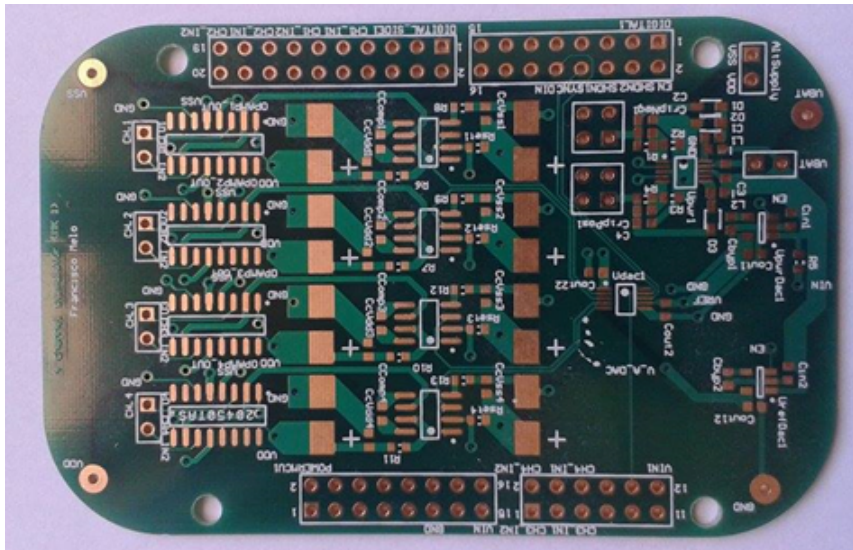


FIGURE 5.17: Tracks in the real board without any components.

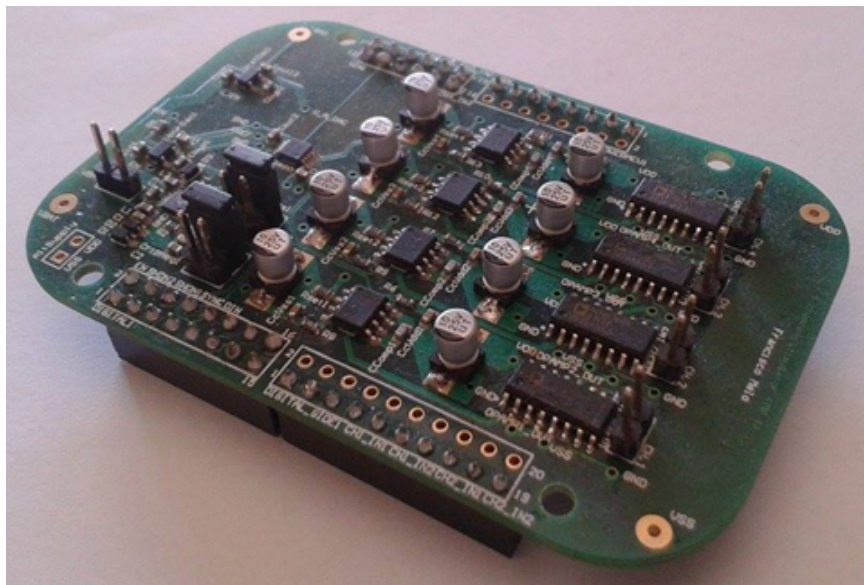


FIGURE 5.18: Full Stimulation Board, with all components.

It is important to refer that this system was built with the future plan of being used together with a neural recording system with a structure and control similar to this stimulation board. So, when defining the connections of the MCU to the stimulation board, attention had to be given to the connections that would be required by the recording system. This way, overlapping of connectors would not occur, except for connections in which communication could be made through the same inputs without affecting the functioning of the connections of either the stimulation or the recording systems to the microcontroller. These connectors are the UART connection pins, the LED connection and the MCU power supply pin.

Chapter 6

Overall Stimulation System Operation

Throughout this thesis, the three main components of an embedded platform for electrical neural stimulation were described, namely the User-System Interface, the Microcontroller – Chapter 4 – and the Front-End Board – Chapter 5. The result of the developed work was an operational current-controlled stimulation system whose stimulation profiles are configurable by the created user-system interface. Figure 6.1 shows the overall operation of this stimulation system.



FIGURE 6.1: Overall Operation of the Embedded Platform for Neural Electrical Stimulation.

As it is possible to see in Figure 6.1, the operation of the system starts with the user programming the stimulation profiles from which results the stimulation information, such as one pulse stimulation and other parameters. That information is then sent to the FRDM-KL26Z microcontroller via the USB connection when the user presses ‘Upload’ in the interface. The microcontroller then stores that information and starts to process

it when ‘Apply’ is pressed. The processing in the microcontroller consists of controlling the Front-End board in accordance with the stored information from the interface. This includes sending pulse values to the DAC, controlling its output according to information on firing type and stimulation channel, and controlling the switches according to the phase of the pulse. The end of the operation resulting from a stimulation profile uploaded and applied is then at the Front-End board, which is responsible for converting the digital pulse value coming from microcontroller into voltage amplitude, with the DAC. The voltage is then converted into current, via the voltage-to-current converter, which is then routed to the switch, whose conformation depends of pulse phase and is finally output through one of the two electrodes and recollected by the other one.

6.1 System Analysis

To check the operation of the built stimulation system, tests were made with the use of an oscilloscope. The tests consisted essentially in applying the various possible types of stimulation profiles and measuring the output on the electrode sites of the front-end board. Figures 6.2, 6.3, 6.4, 6.5 and 6.6 show, respectively, the output of the board when a single stimulation pulse is done with a profile based on a rectangular waveform, bi-level Lilly waveform, quasi-trapezoidal waveform, tri-exponential waveform and bursting strategies. All waveforms were configured to deliver a 850 mV primary amplitude and a secondary amplitude of 425 mV, when applicable, with the remaining parameters left with the preset values referred in Chapter 4. These signals were measured between the entry of a dummy load composed by a 150 Ohm resistor and the anodic electrode site of Channel 1. The reason for choosing this point for the measures was the fact that, since charge-balancing values are smaller, the differences between the expected value and the measured one, resulting from the impedance of the dummy load, would be smaller as well. This would allow for a better evaluation of the similarity between the stimulation and what was configured. These figures show not only the voltage measured at the dummy load entry, in yellow, but also the voltage at the input entry of the switch, in pink. The latter is up for anodic current, so that it could be easier to see the low amplitude in anode phase. In these testing conditions it was expected to obtain, for the rectangular shaped stimulation, a charge voltage amplitude of 850 mV and a charge-balancing amplitude of 110 mV. The latter amplitude is slightly higher than the calculated 85 mV since in the

charge-balancing conformation the anodic site is the opamp output. Values similar to the ones expected were obtained, as it can be seen in Figure 6.2.



FIGURE 6.2: Measured wave for rectangular shaped stimulation.

For the bi-level Lilly shaped stimulation it was expected to obtain a primary charge voltage amplitude of 850 mV, a secondary amplitude of 425 mV and a charge-balancing amplitude of 164 mV. The latter was, again, slightly higher than the calculated value of 127.5 mV, for the same reason explained before. Values similar to the expected ones were obtained as it can be seen in Figure 6.3.

For the quasi-trapezoidal shaped stimulation it was expected to obtain a primary charge voltage amplitude of 850 mV and a charge-balancing amplitude slightly higher than the 110.8 mV: 142.7 mV. Values similar to the expected ones were obtained as it can be seen in Figure 6.4.

For the tri-exponential shaped stimulation it was expected to obtain a primary charge voltage amplitude of 850 mV and a charge-balancing amplitude slightly higher than the 28.5 mV: 38 mV. In this case, as it can be seen in Figure 6.5, the charge-balancing values obtained were also similar to the ones expected. The charge values, however, were smaller than the expected.

For the "bursting strategies" based stimulation it was expected to obtain a primary charge voltage amplitude of 850 mV and a charge-balancing amplitude slightly higher

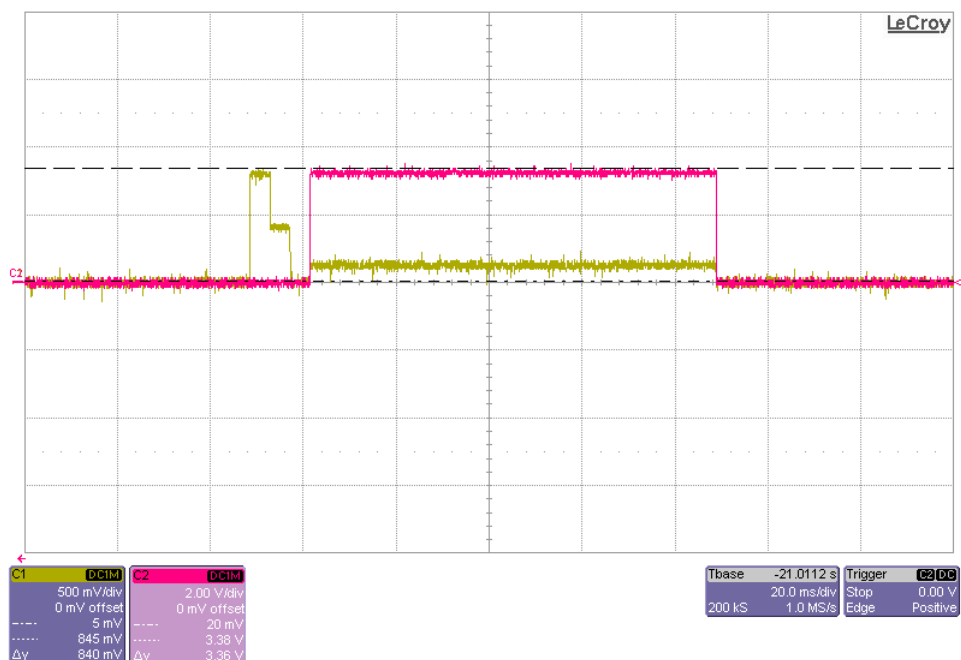


FIGURE 6.3: Measured wave for bi-level Lilly shaped stimulation.

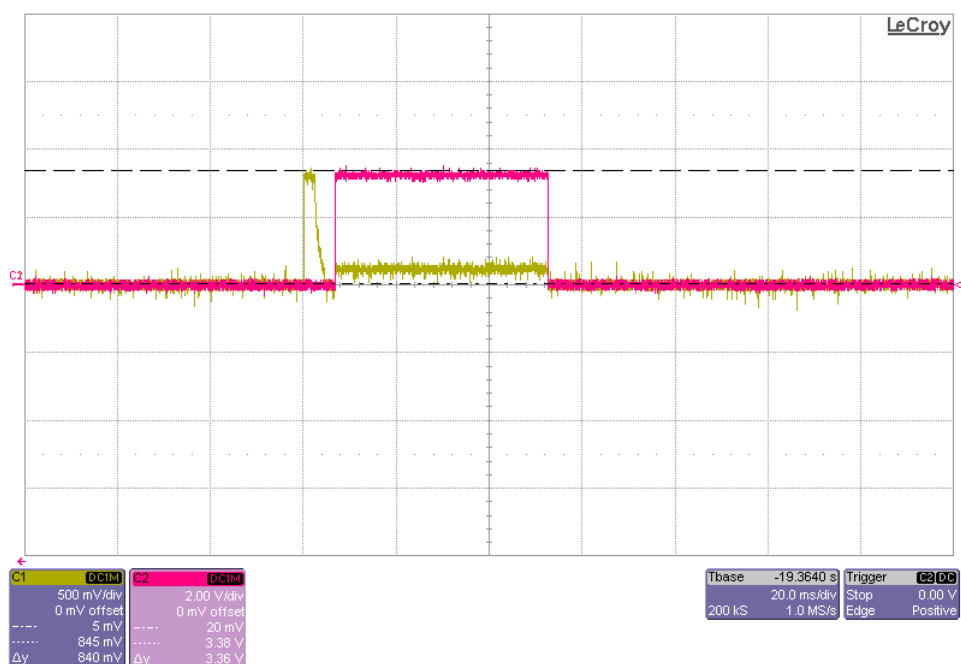


FIGURE 6.4: Measured wave for quasi-trapezoidal shaped stimulation

than the 85 mV: 110 mV. Here, the values obtained were once again similar to the ones expected as it can be seen in Figure 6.6.

Table 6.1 summarizes the results of obtained from previous measures. It can be seen the charge amplitude programmed in the user-system interface and resulting charge-balancing amplitude, the expected charge-balancing amplitude due to the measuring

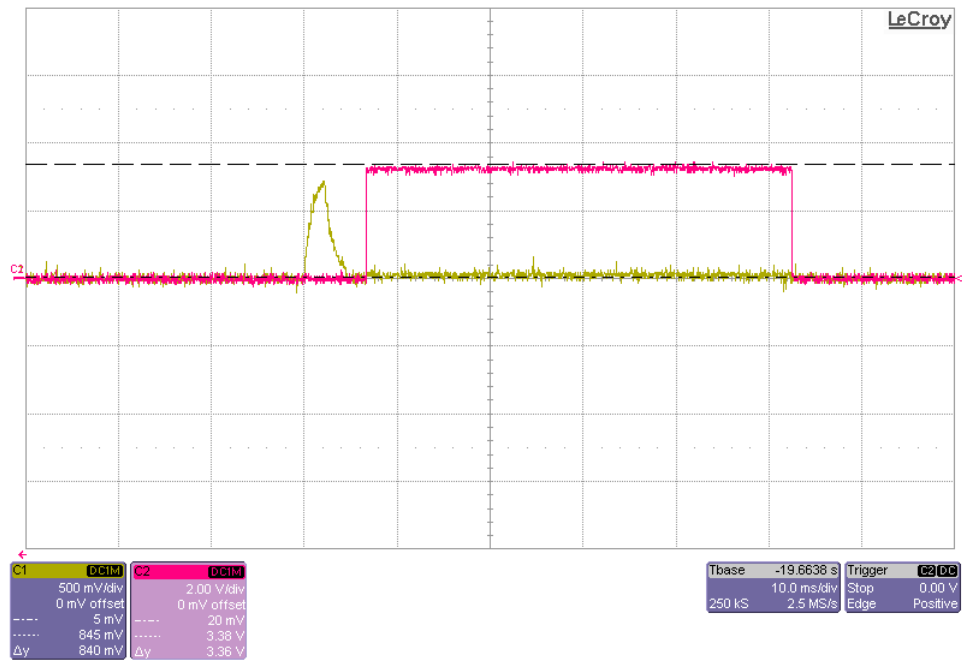


FIGURE 6.5: Measured wave tri-exponential shaped stimulation.

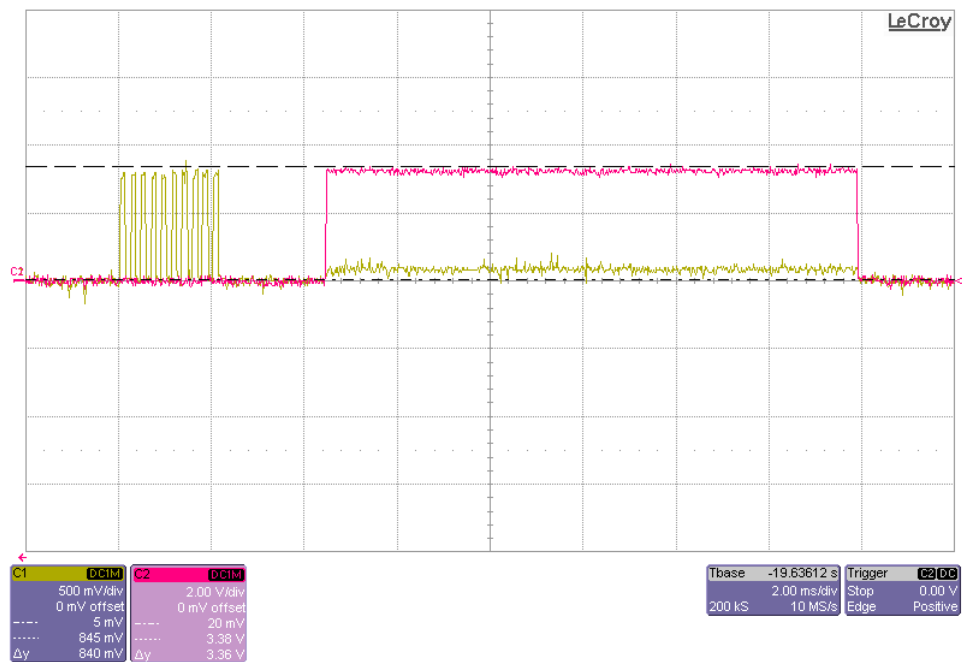


FIGURE 6.6: Measured wave for bursting strategies based stimulation.

conditions, and the approximate measurement values for charge and charge-balancing. Bi-level Lilly presents two values in charge amplitude, the first for the first step amplitude and the second for the second step amplitude. The referred proximity between the values expected and measured can be clearly observed, excepted for the Tri-Exponential waveform, where a slight difference between charge amplitude programmed and measured can be seen.

TABLE 6.1: System Analysis measurements.

Waveform Type	Programmed Charge Amplitude [mV]	Programmed Charge-Balancing Amplitude [mV]	Expected Charge-Balancing Amplitude [mV]	Measured Charge Amplitude [mV]	Measured Charge-Balancing Amplitude [mV]
Rectangular	850	85	110	840	100
Bi-level Lilly	850 ¹ 420 ²	127.5	164	840 ¹ 400 ²	150
Quasi-Trapezoidal	850	110.8	142.7	840	130
Tri-Exponential	850	28.5	38	700	30
Bursting Strategy	850	85	110	840	100

¹ First step amplitude. ² Second step amplitude.

The same procedure was also done for the remaining channels and the same results were obtained. Besides single pulse stimulations, the other possible stimulation configurations were also tested. Figure 6.7 shows a rectangular-based repetitive stimulation – in yellow – with a primary amplitude of 700 mV, a repetition rate of 10 kHz, a repetition amplitude ratio of 2 and a stimulation duration of 40 ms. The blue and pink traces represent the cathodic and anodic phases, respectively, since they are sampling the corresponding switch inputs. The remaining configuration were left as preset.

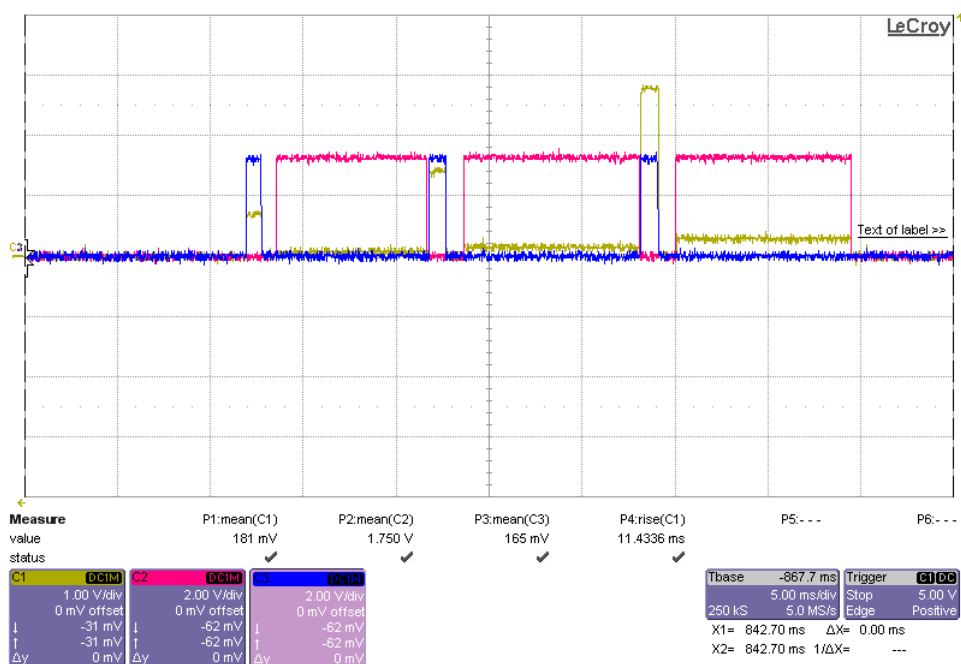


FIGURE 6.7: Rectangular shaped repetitive stimulation.

Figure 6.8 shows a similar stimulation but where, along the repetition, the maximum amplitude voltage is reached as it is possible to understand by the fact that in the last two pulses the amplitude does not increase. To obtain a stimulation as the one presented in Figure 6.8, the following parameters were chosen in the interface: rectangular-based stimulation with a primary amplitude of 100 mV, a repetition rate of 10 kHz, a repetition amplitude ratio of 2 and a stimulation duration of 90ms. All the remaining parameters were left as preset. Also, to test the systems capacity to comply with the calculated voltage maximum, it was configured in the interface that the electrode impedance would be of 900 Ohm, which leads to a voltage maximum of approximately 3.2 V. The result is shown in Figure 6.8 with a stimulation composed by seven repetitions with increasingly higher amplitude until the sixth one, from where the amplitude does not increase more due to the amplitude limitations.

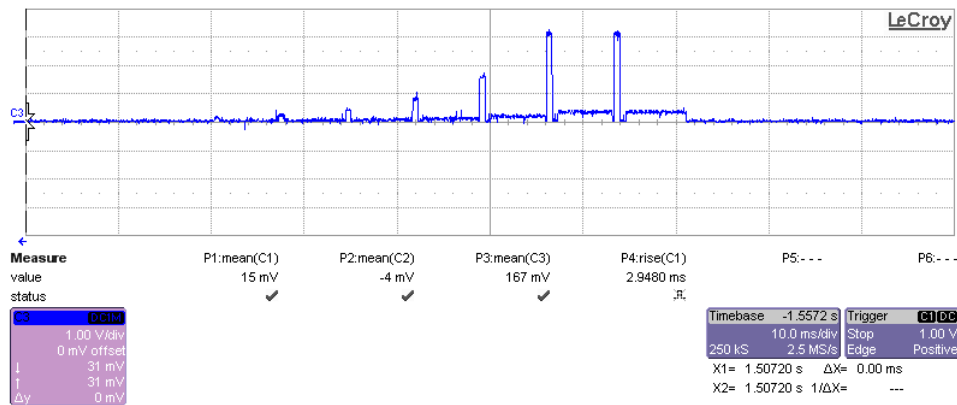


FIGURE 6.8: Rectangular shaped repetitive stimulation with amplitude limitation.

Figure 6.9 shows a synchronous rectangular-based stimulation through two different channels, namely Channel 3 – blue tracing – and Channel 4 – yellow tracing , both with a primary amplitude of 700 mV and the remaining parameters left as preset.

Figure 6.10 shows an asynchronous rectangular-based stimulation through the same two channels, Channel 3 and 4, the first represented by the blue tracing and the second by the yellow tracing. In this case the stimulation pulse has the same parameters of the previous demonstration, namely a primary amplitude of 700 mV and the remaining parameters left as preset.

The reason why Figures 6.9 and 6.10 have a different look than the other results is because they were obtained with a different oscilloscope.

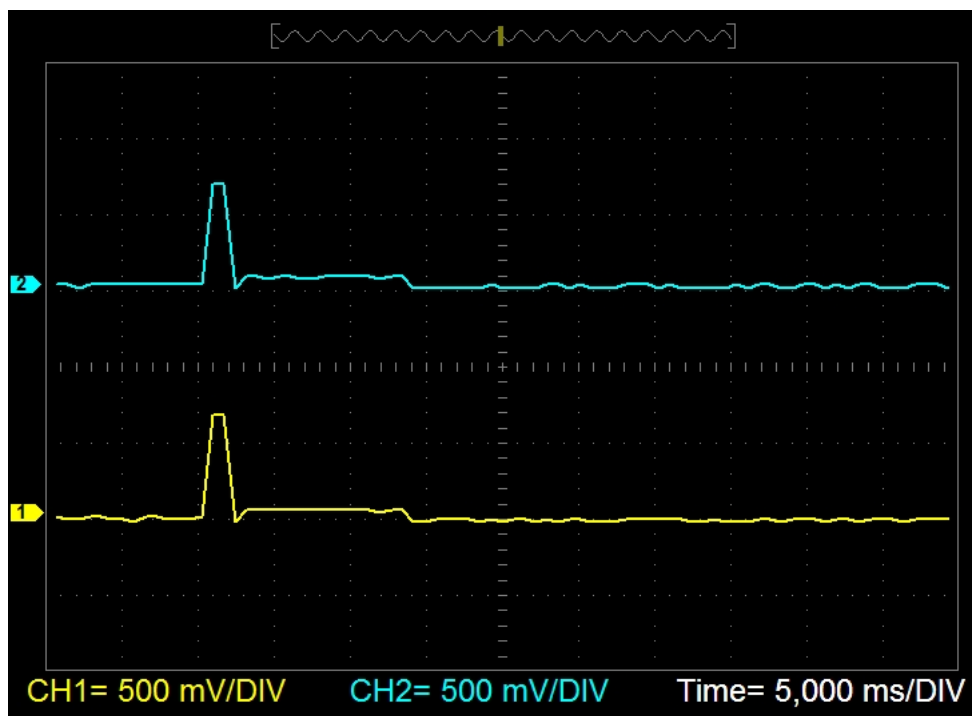


FIGURE 6.9: Synchronous rectangular-based stimulation.

From the results shown in Figure 6.7, a measure of the duration of the phases was also made to check that the configured timings were being met. The measured timings were the widths of the charge and charge-balancing phases from the three pulses, as can be seen in Figure 6.11. The results obtained are shown in Table 6.2. As the values for the charge width was left as preset, i.e., a width of 1 ms, with an also preset biphasic ratio of 10, the expected charge-balancing was of 10 ms. However, as it is possible to see in Table 6.2, these widths were not met in the first pulse but were approximately correct in the following ones. Besides this, it is possible to see that the widths show a trend to increase along the repetitions. The cause for these differences is related to the clock frequency of the microcontroller and also the delay caused by some functions of the microcontroller.

6.2 Charge Balancing Analysis

The charge-balancing capacity of this system was also tested by applying a simple stimulation profile to a dummy load composed of an 8.2 kOhm resistor and an 8.8 μF capacitor in series and measuring the voltage across the capacitor. Ideally, at the end of the application of stimulation, the result of this test should be that the voltage potential on one

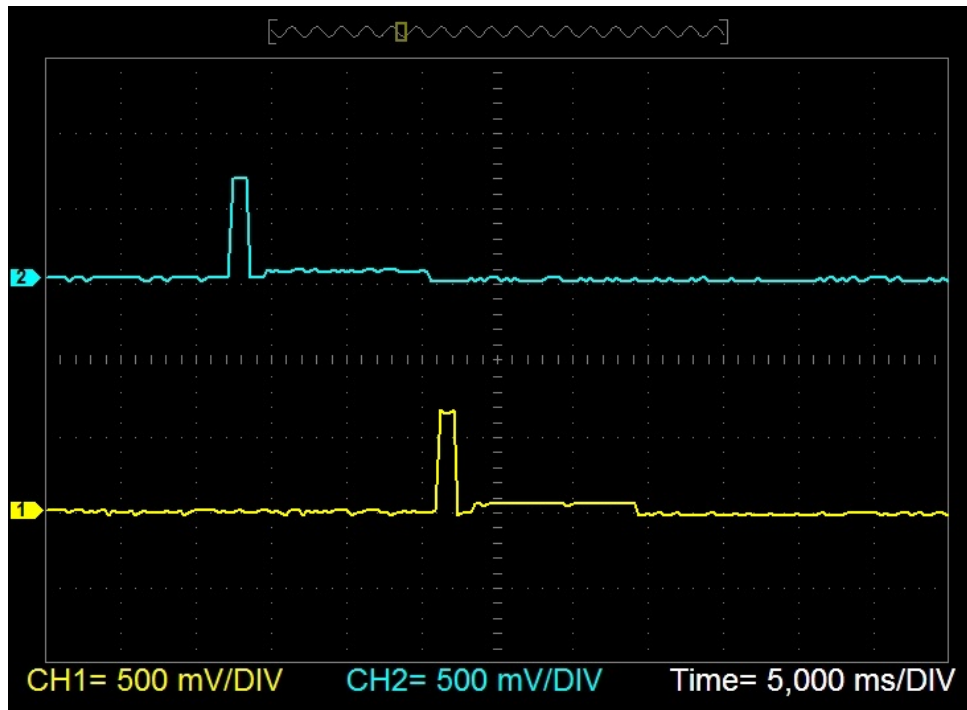


FIGURE 6.10: Asynchronous rectangular-based stimulation.

TABLE 6.2: Timing measurements. The definition of the intervals is shown previously in Figure 6.11.

Interval	Width [ms]
A	0.780
B	8.08
C	1.08
D	10.50
E	1.08
F	10.72

side of the capacitor would be the same as on the other side, that is, there is no potential difference across it meaning that there is no charge accumulated in the capacitor. For this test, four probes were used: a green one for the switch input corresponding to cathodic conformation, a yellow one for the switch input corresponding to anodic conformation, a blue one for the cathode side of the capacitor and a pink one for the anode side of the capacitor. It is important to mention that the green probe was multiplying the signal by 10 and this option could not be switched off. Also it is important to refer that some charge can escape through the probes. Figures 6.12, 6.13, 6.14, 6.15 and 6.16 show the results obtained for the five preset waveforms.

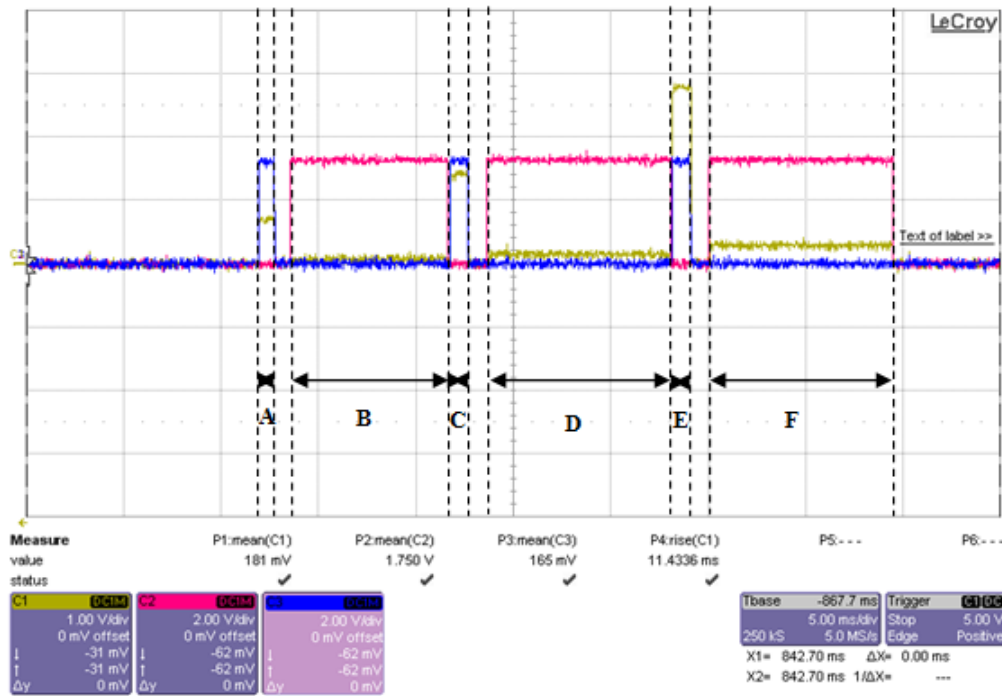


FIGURE 6.11: Intervals for timing measurement.

In Figure 6.12 the results from a single rectangular shaped stimulation are presented. As it is possible to see, at the end of the stimulation, which corresponds to the end of the yellow line, the blue and pink probes measure approximately the same voltage level, meaning that charge-balancing across the capacitor is correctly achieved.

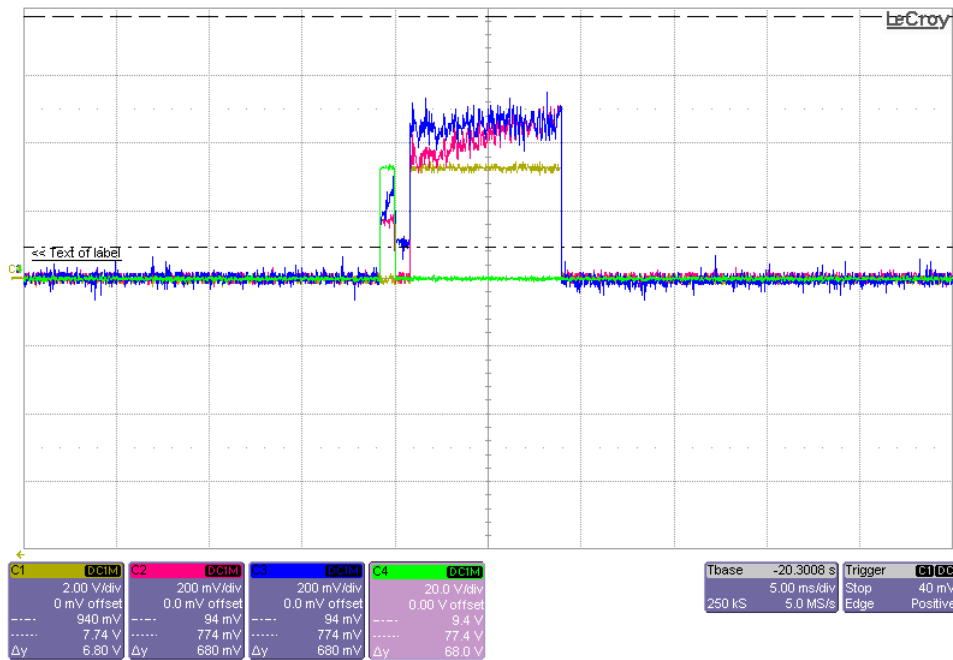


FIGURE 6.12: Charge-balancing results for Rectangular shaped stimulation.

In Figure 6.13 the results from a single bi-level Lilly shaped stimulation are presented. As it is possible to see in this case, at the end of the stimulation, the blue and pink probes measure a slightly different voltage, meaning that some charge build-up occurs on the capacitor and thus a correct charge-balancing is not completely achieved.

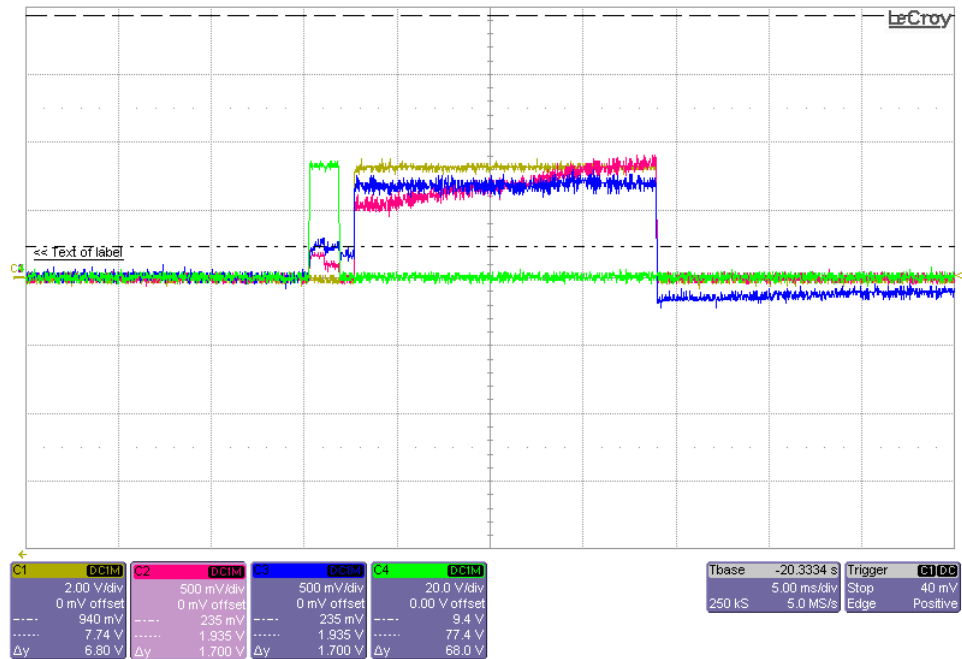


FIGURE 6.13: Charge-balancing results for Bi-level Lilly shaped stimulation.

In Figure 6.14 the results from a single quasi-trapezoidal shaped stimulation are presented. As it is possible to see in this case, at the end of the stimulation, the blue and pink probes measure a slightly different voltage, meaning that some charge build-up occurs on the capacitor and thus a correct charge-balancing is not completely achieved.

In Figure 6.15 the results from a single tri-exponential shaped stimulation are presented. As it is possible to see, at the end of the stimulation, the blue and pink probes measure approximately the same voltage level, meaning that charge-balancing across the capacitor is correctly achieved.

In Figure 6.16 the results from single bursting strategy based stimulation are presented. As it is possible to see, at the end of all stimulation, blue and pink probes measure approximately the same voltage level, meaning that charge-balancing across the capacitor is correctly achieved.

The results from this charge-balancing test are presented in Table 6.3. In this table are the approximate amplitude values measured at the end of the stimulation for both

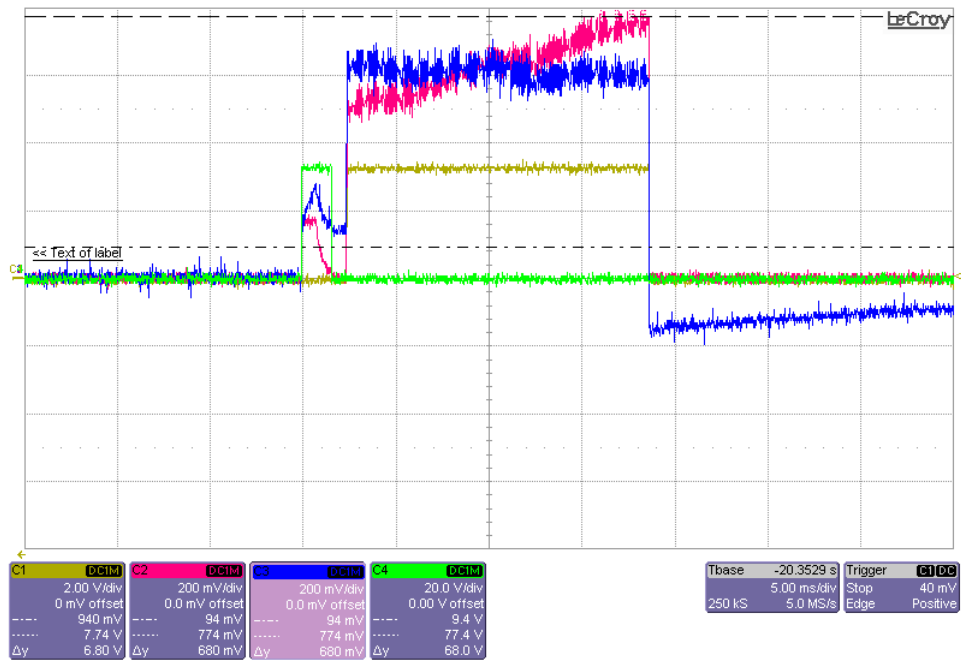


FIGURE 6.14: Charge-balancing results for Quasi-Trapezoidal based stimulation.

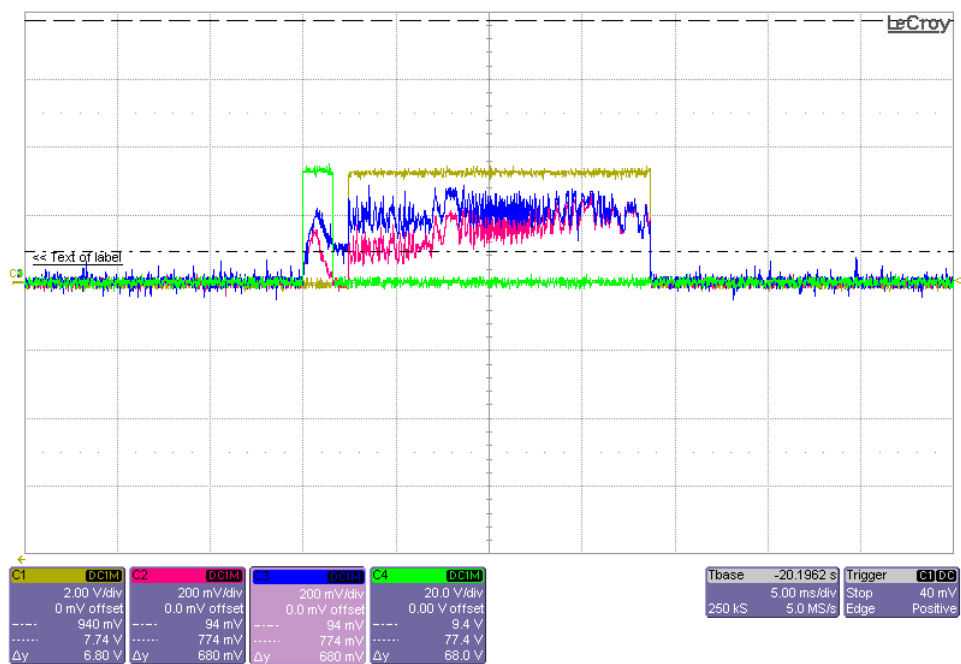


FIGURE 6.15: Charge-balancing results for Tri-Exponential based stimulation.

cathodic and anodic measuring sites, the difference between them and the corresponding residual charge in the capacitor.



FIGURE 6.16: Charge-balancing results for Bursting Strategies based stimulation.

TABLE 6.3: Charge Balance measurements.

Waveform Type	Cathodic Value [mV]	Anodic Value [mV]	Cathodic-Anodic	Residue Charge [μC]
Rectangular	500	500	0	0
Bi-level Lilly	700	800	- 100	- 0.9
Quasi-Trapezoidal	600	774	- 100	- 1
Tri-Exponential	200	200	0	0
Bursting Strategy	450	450	0	0

These results show that this system can provide a correctly charge-balanced stimulation in three of the five stimulation based on preset waveforms, namely with Rectangular waveform, Tri-Exponential and Bursting Strategies. In Bi-level Lilly and Quasi-Trapezoidal however, there is a difference between the voltages on both sides of the capacitor, meaning that there is some charge being accumulated there, more precisely, a charge of $-0.9 \mu\text{C}$ for Bi-level Lilly waveform and $-1 \mu\text{C}$ for Quasi-Trapezoidal. Despite the existence of this residual charge, it is not considered big enough to dismiss the charge-balancing capacity for both waveforms. The reason for not dismissing its capacity is the fact that safety range, known as water window, for example for a platinum electrode and a Ag/AgCl reference electrode is from -0.6 V to 0.8 V , and when a Hg/HgCl₂ reference electrode, also known calomel electrode, is used the range goes

from -0.8 V up to 1.2 V [11]. Beyond the limits of the water window, hydrolysis and electrode dissolution can occur. Since the voltage difference for Bi-level Lilly and Quasi-Trapezoidal waveforms is of -100 mV and -144 mV, respectively, it means that it would be within these safety limits. Besides this, the fact that repetition of stimulation was found to lead to increasingly smaller charge difference [37] gives reasons to believe that this result can be improved.

Chapter 7

Conclusion and Future Work

As an area of major interest due to its various possible applications, from therapy to treatment, to rehabilitation and also prosthetics, neurostimulation research has led to the development of many currently used technologies in the aforementioned areas. Some of the resulting technologies are nowadays well-known and widely used such as the pacemaker for cardiac control and the cochlear implant for people with hearing loss. Besides these two technologies others less known are also already being used for therapies, treatments and rehabilitation and in functional prostheses and more are on the way.

For the development of these technologies in its mentioned applications, careful studies of stimulation strategies have to be done so that an effective, safe and energy-efficient stimulation can be obtained for each specific use. For an optimal stimulation to be obtained, comparative studies have to be done between different stimulation strategies which ideally should be within a relatively small period of time, so that the nerve's conditions do not change, and with the minimum changes to the experimental apparatus, so that the conditions of the experience stay the same. However, the classical methods for neural stimulation studies did not enable these requirements to be met since it took time and amendments to the apparatus to change the parameters of the stimulation. To meet the comparative studies requirements, new stimulation experimental apparatus have been developed firstly with testing platforms with multiple customized circuits for stimulations with different amplitude and duration for a specific waveform [18] and computational models [24], and then more advanced systems that allowed for an increasingly

easier and faster programmability of stimulation with an higher number of parameters available for configuration [25-34, 36].

The project reported in this thesis is an approach to create an improved, small, low-cost, effective, efficient and easy-to-use version of a programmable stimulation system for these comparative studies of stimulation strategies. In addition to this it is also a purpose that this project can be easily recreated, changed and, eventually, improved.

Throughout this thesis we have described the development of an embedded platform for electrical neural stimulation that allows its user to control the parameters of stimulation through a MATLAB-based user-system interface, as explained in Chapter 4.1, and is then capable of generating and applying a charge-balancing bipolar stimulation via four different channels thanks to a microcontroller and a front-end circuit board, as explained in Chapter 4.2 and 5. The results reported in Chapter 6 show that the platform here developed can operate correctly in both the main aspects of its functioning: the capacity to generate the stimulation according to all the parameters as configured by the user and the capacity to provide a charge-balancing stimulation in all the preset waveforms.

When compared to the existing programmable stimulation platforms, the system here developed presents several advantages. Besides being a small, low-cost, easy-to-build, effective and easy-to-use stimulation system, the platform developed for this thesis also presents to its users a higher level of programmability. Regarding the configuration of stimulation characteristics, this system allows users to choose between five preset waveforms or upload a arbitrary waveform, to control pulse parameters such as amplitude, width, decay width, exponential level of decay and time resolution, to control the delay between charge phase and charge-balancing phase – interphasic delay, the ratio between charge amplitude and charge-balancing amplitude – biphasic ratio, to define the repetition ratio and the possibility of the pulse amplitude vary in each repetition – repetition amplitude ratio, and the duration intended for the full stimulation. In addition to this, the platform here developed allows the user to apply stimulation in three different ways with the possible use of the four available stimulation channels, namely using only one channel, using more than one sequentially or more than one at the same time.

However, there are still some significant limitations to the platform here developed. One significant limitation is related to the maximum output that the system can provide. The first output limitation comes from the DAC which can only output a maximum of

5 V which means that users cannot configure in this system stimulations with voltage amplitude higher than 5 V. The second output limitation comes from the opamp voltage compliance, which is of ± 9 V – the power supply values. This is a limiting factor because it means that the electrode impedance has major role on the maximum voltage that the user can configure for the stimulation since that beyond the voltage compliance point the opamp saturates and the configurations defined are not met. However, this limitation may not be so significant because this platform was originally thought for experimental setups where the electrodes are placed closer to the target nerve where stimulation usually has lower amplitudes. Table 7.1 presents all the ranges and specifications of the platform developed.

TABLE 7.1: Specifications of the developed platform.

Parameter	Value	Units
Amplitude Maximum	5	[V]
Amplitude Resolution	0.01	[V]
Charge Phase Width	0.1 - 11.6	[ms]
Interphasic Delay	0 – 11.6	[ms]
Time Resolution	0.025 – 1	[ms]
Biphasic Ratio	0 – 221	-
Repetition Frequency	0.001 – 40	[kHz]

A second limitation is related to its failure to comply exactly with the pulse widths and the fact that these widths increase along the repetitions. These width problems are thought to be caused by the clock frequency of the microcontroller and also the delay caused by some functions of the microcontroller, meaning that an optimization of the microcontroller’s code together with its clock frequency is necessary.

A third limitation of this system is the energy consumption it presents. During the tests performed the operation of the front-end board alone, including when a stimulation was done, the current consume was of about 300 mA, with peaks reaching 500 mA. Although this is not problematic for the experimental procedure itself, it means a high energy consume from the power source and consequently a shorter lifetime.

Another limitation of the system here developed is the fact that all connections, between computer, microcontroller and the front-end board, is done through wires. This presents

as a limiting factor because it reduces the liberty of movements and maneuver that can be done in an experimental setup using this platform.

Table 7.2 presents a comparison between the embedded platform described in this thesis and the five most recent stimulation systems mentioned in Chapter 3. For this table focus was made on the following characteristics: number of waveforms available for user choice; the possibility of creating a custom waveform, different from the available ones; the number of parameters available for configuration; if the system allows for biphasic stimulation; the number of channels available to apply stimulation; the number of modes for applying stimulation – firing modes; the electric mode of applying stimulation; if the system can work in stand-alone mode, i.e., if it does not need for a computer controlling its operation; and if the communication can be made wirelessly.

TABLE 7.2: Comparison between this work and existing systems.

Characteristics	This Work	[30]	[31]	[33]	[34]	[36]
No Waveforms	5	1	5	1	1	2
Custom Waveform	Yes	No	Yes	No	No	Yes
No Parameters	20	4	5	4	6	16
Biphasic	Yes	Yes	Yes	Yes	No	Yes
No Channels	4	100	1	8	2	4
Firing Modes	3	2	3	1	1	2
Electric Mode	Current -Controlled	Current -Controlled	Current -Controlled	Voltage or Current	Voltage -Controlled	Voltage -Controlled
Stand-Alone Mode	No	No	Yes	No	No	Yes
Wireless	No	Yes	No	No	Yes	No

The challenges for the future of this platform are then the search for the solutions for these limitations: to improve its output capacity both by a different, more powerful DAC and an improved V-to-I converter circuit that can overcome these voltage compliance limits, to optimize the microcontroller code together with its clock frequency so that stimulations width can be exactly as intended by the user, and finally to make it less power consuming and make the communication between computer and microcontroller wireless so that microcontroller and front-end board can be used for example as an implantable stimulating platform.

References

- [1] Famm, K., et al. (2013). "Drug discovery: a jump-start for electroceuticals." *Nature* 496(7444): 159-161.
- [2] Ragnarsson, K. T. (2008). "Functional electrical stimulation after spinal cord injury: current use, therapeutic effects and future directions." *Spinal Cord* 46(4): 255-274.
- [3] Yawn, R., et al. (2015). "Cochlear implantation: a biomechanical prosthesis for hearing loss." *F1000Prime Rep* 7: 45.
- [4] "A diagram of Chalmers' implanted prosthetics system" from <http://www.gizmag.com/thought-controlled-prosthetic-arm/25216/> in 07/12/2014
- [5] Seely R., Stephens T., Tate P. (2011). "Anatomia e Fisiologia" (8th ed.). Loures: Lusociência.
- [6] "Neuron diagram" from <https://www.pinterest.com/beverleycain9/neuroscience/> in 12/06/2015
- [7] Plonsey, R. and R.C. Barr (2007). *Bioelectricity, a quantitative approach.*, Springer, 3rd ed
- [8] "Diagram of an action potential" from <http://www.cog.brown.edu/courses/cg0001/lectures/visualpaths.html> in 29/11/2014
- [9] "Variation of Membrane Potential during an Action Potential" from <http://hmpphysiology.blogspot.pt/p/nervous-system.html> in 02/09/2015
- [10] Luan, S., et al. (2014). "Neuromodulation: present and emerging methods." *Front Neuroeng* 7: 27.

-
- [11] Liu, X., A. Demosthenous, N. Donaldson. (2011). "Neural Interfaces for Implanted Stimulators." In: Springer Handbook of Medical Technology., Springer: 749-766.
- [12] Merrill, D. R., et al. (2005). "Electrical stimulation of excitable tissue: design of efficacious and safe protocols." *J Neurosci Methods* 141(2): 171-198.
- [13] Dymond, A. M. (1976). "Characteristics of the metal-tissue interface of stimulation electrodes." *IEEE Trans Biomed Eng* 23(4): 274-280.
- [14] de Voogt, W. G., et al. (2004). "Understanding capture detection." *Europace* 6(6): 561-569.
- [15] Prado-Guitierrez, P., et al. (2006). "Effect of interphase gap and pulse duration on electrically evoked potentials is correlated with auditory nerve survival." *Hear Res* 215(1-2): 47-55.
- [16] W. M. Grill and J. T. Mortimer (1995), "Stimulus waveforms for selective neural stimulation," *IEEE Eng. Med. Biol. Mag.*, 14(4): 375–385.
- [17] Fang, Z. P. and J. T. Mortimer (1991). "Selective activation of small motor axons by quasi-trapezoidal current pulses." *IEEE Trans Biomed Eng* 38(2): 168-174.
- [18] Accornero, N., et al. (1977). "Selective Activation of peripheral nerve fibre groups of different diameter by triangular shaped stimulus pulses." *J Physiol* 273(3): 539-560.
- [19] van den Honert, C. and J. T. Mortimer (1979). "Generation of unidirectionally propagated action potentials in a peripheral nerve by brief stimuli." *Science* 206(4424): 1311-1312.
- [20] Grill, W. M. and J. T. Mortimer (1997). "Inversion of the current-distance relationship by transient depolarization." *IEEE Trans Biomed Eng* 44(1): 1-9.
- [21] Qing, K., et al. (2015). "Burst-modulated waveforms optimize electrical stimuli for charge efficiency and fiber selectivity." *IEEE Trans Neural Syst Rehabil Eng*.
- [22] Qing, K. (2013). "Electrical stimulation with burst-modulated pulse waveforms improves efficiency and fiber-selectivity." In 6th International IEEE EMBS Conference on Neural Engineering. San Diego, CA, November 6-8 2013. USA: IEEE. 1.
- [23] Kilgore, K. L. and N. Bhadra (2004). "Nerve conduction block utilising high-frequency alternating current." *Med Biol Eng Comput* 42(3): 394-406.

- [24] Grill, W. M., Jr. and J. T. Mortimer (1996). "The effect of stimulus pulse duration on selectivity of neural stimulation." *IEEE Trans Biomed Eng* 43(2): 161-166.
- [25] Bugbee, M., et al. (2001). "An implant for chronic selective stimulation of nerves." *Med Eng Phys* 23(1): 29-36.
- [26] Sha, H., et al. (2005). "A microcontroller-based implantable nerve stimulator used for rats." *Conf Proc IEEE Eng Med Biol Soc* 6: 6176-6179.
- [27] Salmons, S., et al. (2001). "ASIC or PIC? Implantable stimulators based on semi-custom CMOS technology or low-power microcontroller architecture." *Med Eng Phys* 23(1): 37-43.
- [28] Constandinou, T. G., et al. (2008). "A partial-current-steering biphasic stimulation driver for vestibular prostheses." *IEEE Trans Biomed Circuits Syst* 2(2): 106-113.
- [29] Woods, V., et al. (2008). "A Reconfigurable and Automated System for the study of Stimulus Waveform Parameters." *Conf Proc IFESS 2008*
- [30] Thurgood, B. K., et al. (2009). "A wireless integrated circuit for 100-channel charge-balanced neural stimulation." *IEEE Trans Biomed Circuits Syst* 3(6): 405-414.
- [31] Eftekhar, A., et al. (2009). "A Programmable Neural Interface for Investigating Arbitrary Stimulation Strategies" *Conf Proc IFESS 2009*
- [32] Guilvard, A., et al. (2010) "A Fully-Programmable Neural Interface for Multi-Polar, Multi-Channel Stimulation Strategies." *IEEE Circuits Sys* 2010: 2235-2238.
- [33] Laotaveerungrueng, N., et al. (2010). "A high-voltage, high-current CMOS pulse generator ASIC for deep brain stimulation." *Conf Proc IEEE Eng Med Biol Soc* 2010: 1519-1522.
- [34] Chiu, H.-C., et al. (2014). "An Intelligent Brain Machine Interface with Wireless Micro-Stimulation and Neural Recording." *IEEE Biomed Health Inform* 2014.
- [35] <http://www.open-ephys.org/> in 23/09/2015
- [36] <https://sites.google.com/site/pulsepalwiki/home> in 23/09/2015

-
- [37] Williams, I. and T. Constandinou (2013). "An energy-efficient, dynamic voltage scaling neural stimulator for a proprioceptive prosthesis." *IEEE Trans Biomed Circuits Syst* 7(2): 129-139.

Appendix A

MATLAB Code

A.1 User-System Interface Code

```
1 function varargout = stimulation_gui(varargin)
2 % STIMULATION_GUI MATLAB code for stimulation_gui.fig
3 %     STIMULATION_GUI, by itself, creates a new STIMULATION_GUI or raises the
4 %     existing
5 %     singleton*.
6 %     H = STIMULATION_GUI returns the handle to a new STIMULATION_GUI or the
7 %     handle to
8 %     the existing singleton*.
9 %     STIMULATION_GUI('CALLBACK',hObject,eventData,handles,...) calls the local
10 %    function named CALLBACK in STIMULATION_GUI.M with the given input
11 %    arguments.
12 %     STIMULATION_GUI('Property','Value',...) creates a new STIMULATION_GUI or
13 %    raises the
14 %    existing singleton*. Starting from the left, property value pairs are
15 %    applied to the GUI before stimulation_gui_OpeningFcn gets called. An
16 %    unrecognized property name or invalid value makes property application
17 %    stop. All inputs are passed to stimulation_gui_OpeningFcn via varargin.
18 %     *See GUI Options on GUIDE's Tools menu. Choose "GUI allows only one
19 %     instance to run (singleton)".
20 %
21 % See also: GUIDE, GUIDATA, GUIHANDLES
22
23 % edit the above text to modify the response to help stimulation_gui
24
```

```
25 % Last Modified by GUIDE v2.5 17-Mar-2015 11:56:17
26
27 % Begin initialization code - DO NOT EDIT
28 gui_Singleton = 1;
29 gui_State = struct('gui_Name',       mfilename, ...
30     'gui_Singleton',  gui_Singleton, ...
31     'gui_OpeningFcn', @stimulation_gui_OpeningFcn, ...
32     'gui_OutputFcn',  @stimulation_gui_OutputFcn, ...
33     'gui_LayoutFcn',  [] , ...
34     'gui_Callback',   []);
35 if nargin && ischar(varargin{1})
36     gui_State.gui_Callback = str2func(varargin{1});
37 end
38
39 if nargin
40     [varargout{1:nargout}] = gui_mainfcn(gui_State, varargin{:});
41 else
42     gui_mainfcn(gui_State, varargin{:});
43 end
44 % End initialization code - DO NOT EDIT
45
46
47 % --- Executes just before stimulation_gui is made visible.
48 function stimulation_gui_OpeningFcn(hObject, eventdata, handles, varargin)
49 % This function has no output args, see OutputFcn.
50 % hObject    handle to figure
51 % eventdata  reserved - to be defined in a future version of MATLAB
52 % handles    structure with handles and user data (see GUIDATA)
53 % varargin   command line arguments to stimulation_gui (see VARARGIN)
54
55 % Initial Considerations
56
57 handles.t_i = 0; %1; % just to see the initial fase of the stimulus
58 handles.t_f = 0; %2; % just to see the end of the stimulus
59 handles.amplitude_1 = 1;
60 handles.amplitude_2 = 0;
61 handles.duration_1 = 1; % 1ms (100/1000) stimulation
62 handles.duration_2 = 0;
63 handles.amplitude_I0 = 0.01; % for tri-exponential growth, since I0 cannot be
    zero is a value aprox. zero
64 handles.delay = 1;
65 handles.decay = 1;
66 handles.biphasic = 10;
67 handles.resolution = 0.25;
68 handles.time_ms_s = 1/1000;
69 handles.time_s_ms = 1000;
70 handles.time_ms_us = 1000;
71 handles.q = 1;
```



```
72 handles.q2 = 2.197e+03;
73 handles.a = 0.2;
74 handles.a2 = 1.197e+03;
75 handles.b = 0.3;
76 handles.b2 = 2.197e+03;
77 handles.c = 0.5;
78 handles.c2 = 3.197e+03;
79 handles.decay_steps = handles.decay/handles.resolution;
80 handles.burst_steps = handles.duration_1/handles.resolution;
81 handles.increase_steps = handles.duration_1/handles.resolution;
82 handles.repetition = 0; % starts with no repetition, just the original wave
83 handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
84 handles.duration_balance_2 = handles.biphasic.*handles.duration_2;
85 handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
    duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
86 handles.time_resolution = 40; % so 0,025ms * 40 = 1 time sample
87 handles.timescale = (0:(1/handles.time_resolution):(handles.stimulation_fulltime+
    handles.t_f));
88 handles.current_data_I = zeros(1,length(handles.timescale));
89 handles.stimulation_data_I = zeros(1,length(handles.timescale));
90 handles.fullstimulation_duration = handles.stimulation_fulltime;
91 handles.rep_amp_ratio = 1;
92 handles.time_lag = 1;
93 handles.number_sent_channels = 1;
94 handles.old_channel = 0;
95 handles.interstimulus_time = 0;
96 handles.n_repetitions = 0;
97 handles.old_firing = 0;
98 handles.amplitude_max = 0;
99 handles.reps_max = 0;
100
101 handles.resistance = 0;
102 handles.DAC_amplitude_limit = 5; % CHANGE HERE IF HIGHER LIMIT IS DESIRED
103 handles.opamp_max_output_voltage = 9;
104 handles.R_set = 510; % it was initially thought with 500 but the actual resistor
    is 510
105 handles.R_internal = 12;
106
107
108
109 set(handles.stim_duration_edit, 'enable', 'on','String', handles.
    fullstimulation_duration)
110
111 serialInfo = instrhwinfo('serial');
112 if isempty(serialInfo.SerialPorts) == 1
113     % Nothing happens and program moves on
114 else
115     % if finds COM ports being used, reports them and makes them available
```

```

116     % for user selection
117     n_coms = 1;
118     for n_coms = 1:length(serialInfo.SerialPorts)
119         string_list(n_coms+1) = serialInfo.SerialPorts(n_coms);
120     end
121     set(handles.COM_popup, 'String', string_list);
122 end
123
124 % User notification of Type of System
125 input_answer = inputdlg('This system is an Open Loop Control. Enter Electrode
    Impedance Value (Ohm) at 1kHz for Amplitude Safe Range: [Cancel for No Safe
    Range]', 'Safe Range Amplitude');
126 if isempty(input_answer) == 1
127     % If the User chooses not to have a Safe Range
128     wd = warndlg('No Amplitude Safe Range Defined!', 'Safe Range');
129     waitfor(wd);
130 else
131     % Calculates the Amplitude Maximum for a Safety
132     try
133         handles.resistance = str2num(cell2mat(input_answer));
134         handles.amplitude_max = (handles.opamp_max_output_voltage * handles.R_set
    )/(handles.resistance + handles.R_set + (2*handles.R_internal));
135         set(handles.electrode_impedit, 'enable', 'on', 'String', handles.
    resistance)
136         set(handles.amplitude_maximum_edit, 'enable', 'off', 'String', handles.
    amplitude_max)
137     catch err
138         wd = warndlg('No Amplitude Safe Range Defined!', 'Safe Range');
139         waitfor(wd);
140         handles.resistance = 0;
141         handles.amplitude_max = 0;
142     end
143 end
144
145
146
147
148 % Waveform signals
149
150 % Pulse Waveform
151 handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-handles.
    amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
152     zeros(1,(handles.delay*handles.time_resolution))...
153     ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones(1,handles.
    duration_balance_1*handles.time_resolution)...
154     zeros(1,(length(handles.timescale)-handles.t_i*handles.time_resolution)...
155     -((handles.stimulation_fulltime)*handles.time_resolution))];
156

```

```

157
158 % Bi-Level Lilly Waveform
159 % amplitude_CB is the amplitude needed for charge balance
160 amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.amplitude_2*
    handles.duration_2)/handles.biphasic;
161 handles.duration_balance_total = handles.biphasic.*(handles.duration_1 + handles.
    duration_2);
162 handles.stimulation_fulltime = handles.duration_1+handles.duration_balance_total+
    handles.delay+handles.decay;
163 handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-handles.
    amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
164 (-handles.amplitude_2).*ones(1,handles.duration_2*handles.time_resolution)
    zeros(1,(handles.delay*handles.time_resolution))...
165 amplitude_CB.*ones(1,handles.duration_balance_total*handles.time_resolution)
    ...
166 zeros(1,(length(handles.timescale)-handles.t_i*handles.time_resolution)...
167 -((handles.stimulation_fulltime)*handles.time_resolution))];
168
169
170
171 % Quasi-Trapezoidal Waveform
172 handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-handles.
    amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
173 i=1;
174 total_decay_amplitude = 0;
175 %Building of the decay part of wave
176 for i=1:handles.decay_steps
177     handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.amplitude_1*handles
    .q*...
178         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s)).*...
179         ones(1,handles.resolution*handles.time_resolution));
180     total_decay_amplitude = total_decay_amplitude + (handles.amplitude_1*handles.
    q*...
181         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
182 end
183 %Building of Discharge Phase
184 amplitude_CB = (handles.amplitude_1*handles.duration_1 + total_decay_amplitude*
    handles.resolution)/handles.biphasic;
185 handles.duration_balance_total = handles.biphasic.*(handles.duration_1 + handles.
    decay);
186 handles.stimulation_fulltime = handles.duration_1+handles.duration_balance_total+
    handles.delay+handles.decay;
187 handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.delay*handles.
    time_resolution))...
188     amplitude_CB.*ones(1,handles.duration_balance_total*handles.time_resolution)
    ...
189     zeros(1,(length(handles.timescale)-handles.t_i*handles.time_resolution)...
190     -((handles.stimulation_fulltime)*handles.time_resolution))]);

```

```

191
192
193 % Tri-Exponential Waveform
194
195 handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
196 j_i = 1;
197 j_d = 1;
198 total_increase_amplitude = 0;
199 total_decay_amplitude = 0;
200 %Building of the increase part of wave
201 for j_i=1:handles.increase_steps
202     handles.tri_exp = horzcat(handles.tri_exp, (((-handles.amplitude_1)/((
        handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.resolution*handles
        .time_resolution)...
203         +((-handles.amplitude_1*handles.t_i)/(handles.duration_1+handles.t_i)-
        handles.t_i))/handles.time_resolution).*...
204         ones(1,handles.resolution*handles.time_resolution));
205     total_increase_amplitude = total_increase_amplitude + ((handles.amplitude_1)
        /((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.resolution*
        handles.time_resolution)...
206         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+handles.t_i)-
        handles.t_i))/handles.time_resolution);
207
208 end
209 %Building of the decay part of wave
210 for j_d=1:handles.decay_steps
211     handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((handles.t_i+
        handles.duration_1)*handles.time_resolution)*((handles.a*...
212         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))+handles.b
        *...
213         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))+handles.c
        *...
214         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s))))).*...
215         ones(1,handles.resolution*handles.time_resolution));
216     total_decay_amplitude = total_decay_amplitude + (handles.tri_exp((handles.t_i+
        handles.duration_1)*handles.time_resolution)*((handles.a*...
217         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))+handles.b
        *...
218         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))+handles.c
        *...
219         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s))));
220 end
221 %Building of Discharge Phase
222 amplitude_CB = (total_increase_amplitude*handles.resolution +
        total_decay_amplitude*handles.resolution)/handles.biphasic;
223 handles.duration_balance_total = handles.biphasic.*(handles.duration_1 + handles.
        decay);

```

```

224 handles.stimulation_fulltime = handles.duration_1+handles.duration_balance_total+
    handles.delay+handles.decay;
225 handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*handles.
    time_resolution))...
226     amplitude_CB.*ones(1,handles.duration_balance_total*handles.time_resolution)
    ...
227     zeros(1,(length(handles.timescale)-handles.t_i*handles.time_resolution)...
228     -((handles.stimulation_fulltime)*handles.time_resolution)]];
229
230
231 % Bursting Waveform
232 handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
233 k=1;
234 %Building of the steps
235 for k=1:handles.burst_steps
236     handles.bursting = horzcat(handles.bursting,[-handles.amplitude_1.*...
237         ones(1,(handles.resolution/2)*handles.time_resolution) ...
238         zeros(1,(handles.resolution/2)*handles.time_resolution)]);
239 end
240 %Building of Discharge Phase
241 handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*handles.
    time_resolution))...
242     ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones(1,handles.
    duration_balance_1*handles.time_resolution)...
243     zeros(1,(length(handles.timescale)-handles.t_i*handles.time_resolution)...
244     -((handles.stimulation_fulltime)*handles.time_resolution)]];
245
246
247 % Initial Plot Output Look
248 axes(handles.plot_axes);
249 plot(handles.timescale,handles.current_data_I);
250 ylim([(min(handles.current_data_I)-0.1),-(min(handles.current_data_I)-0.1)]);
251 xlim([0,((length(handles.current_data_I)-1)/handles.time_resolution)]);
252 ylabel('Amplitude (V)');
253 xlabel('Time (ms)');
254
255 % Choose default command line output for stimulation_gui
256 handles.output = hObject;
257
258 % Update handles structure
259 guidata(hObject, handles);
260
261 % UIWAIT makes stimulation_gui wait for user response (see UIRESUME)
262 % uiwait(handles.figure1);
263
264
265 % --- Outputs from this function are returned to the command line.
266 function varargout = stimulation_gui_OutputFcn(hObject, eventdata, handles)

```

```
267 % varargin    cell array for returning output args (see VARARGOUT);
268 % hObject     handle to figure
269 % eventdata   reserved - to be defined in a future version of MATLAB
270 % handles     structure with handles and user data (see GUIDATA)
271
272 % Get default command line output from handles structure
273 varargin{1} = handles.output;
274
275
276 % --- Executes on selection change in plot_popup.
277 function plot_popup_Callback(hObject, eventdata, handles)
278 % hObject     handle to plot_popup (see GCBO)
279 % eventdata   reserved - to be defined in a future version of MATLAB
280 % handles     structure with handles and user data (see GUIDATA)
281
282 % Hints: contents = cellstr(get(hObject,'String')) returns plot_popup contents as
        cell array
283 %           contents{get(hObject,'Value')} returns selected item from plot_popup
284
285 % DO NOT CHANGE THIS POPUP PART IN .FIG AGAIN
286
287 val = get(handles.plot_popup, 'Value');
288 handles.plot_popup_value = val;
289 str = get(handles.plot_popup, 'String');
290 handles.plot_popup_string = str;
291 switch str{val}
292     case 'Rectangular' % User selects pulse wave
293
294         % Defines variables to the original value
295         handles.amplitude_1 = 1;
296         handles.duration_1 = 1;
297         handles.amplitude_2 = 0;
298         handles.duration_2 = 0;
299         handles.biphasic = 10;
300         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
301         handles.duration_balance_2 = 0;
302         handles.decay = 0;
303         handles.delay = 1;
304         handles.resolution = 0.25;
305         handles.repetition = 0;
306         handles.rep_amp_ratio = 1;
307         handles.stimulation_fulltime = handles.duration_1+handles.duration_2+
handles.duration_balance_1+handles.duration_balance_2+handles.delay+handles.
decay;
308         handles.fullstimulation_duration = handles.stimulation_fulltime;
309         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
310
```

```

311     %Building the pulse wave
312     handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-handles.
amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
313         zeros(1,(handles.delay*handles.time_resolution))...
314         ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones(1,
handles.duration_balance_1*handles.time_resolution)...
315         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution)...
316         -((handles.stimulation_fulltime)*handles.time_resolution))];
317     %
318     handles.current_data_I = handles.pulse;
319     handles.stimulation_data_I = handles.pulse;
320
321     % Define which edit fields should work and define its initial values
322     set(handles.amplitude1_edit, 'enable', 'on','String', handles.amplitude_1
)
323     set(handles.duration1_edit, 'enable', 'on','String', handles.duration_1)
324     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
325     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
326     set(handles.amplitude2_edit, 'enable', 'off')
327     set(handles.duration2_edit, 'enable', 'off')
328     set(handles.decay_edit, 'enable', 'off')
329     set(handles.resolution_edit, 'enable', 'off')
330     set(handles.repetition_edit, 'enable', 'on','String', handles.repetition)
331     set(handles.Q_exp_edit, 'enable', 'off')
332     set(handles.Q2_exp_edit, 'enable', 'off')
333     set(handles.A_exp_edit, 'enable', 'off')
334     set(handles.A2_exp_edit, 'enable', 'off')
335     set(handles.B_exp_edit, 'enable', 'off')
336     set(handles.B2_exp_edit, 'enable', 'off')
337     set(handles.C_exp_edit, 'enable', 'off')
338     set(handles.C2_exp_edit, 'enable', 'off')
339     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
340     set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
341
342     case 'Bi-level Lilly' % User selects bilevel Lilly
343         handles.amplitude_1 = 1;
344         handles.duration_1 = 1;
345         handles.amplitude_2 = 0.5;
346         handles.duration_2 = 1;
347         handles.biphasic = 10;
348         handles.delay = 1;
349         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
350         handles.duration_balance_2 = handles.biphasic.*handles.duration_2;
351         handles.decay = 0;
352         handles.resolution = 0.25;

```

```

353     handles.repetition = 0;
354     handles.rep_amp_ratio = 1;
355
356     % Building the Bilevel Lilly
357     amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
amplitude_2*handles.duration_2)/handles.biphasic;
358     handles.duration_balance_total = handles.biphasic.*(handles.duration_1 +
handles.duration_2);
359     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
360     handles.fullstimulation_duration = handles.stimulation_fulltime;
361     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
362     handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
363         (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
364         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
365         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...
366         -((handles.stimulation_fulltime)*handles.time_resolution)];
367     %
368     handles.current_data_I = handles.bi_level;
369     handles.stimulation_data_I = handles.bi_level;
370
371     % Define which edit fields should work and define its initial values
372     set(handles.amplitude1_edit, 'enable', 'on','String', handles.amplitude_1
)
373     set(handles.duration1_edit, 'enable', 'on','String', handles.duration_1)
374     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
375     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
376     set(handles.amplitude2_edit, 'enable', 'on','String', handles.amplitude_2
)
377     set(handles.duration2_edit, 'enable', 'on','String', handles.duration_2 )
378     set(handles.decay_edit, 'enable', 'off')
379     set(handles.resolution_edit, 'enable', 'off')
380     set(handles.repetition_edit, 'enable', 'on','String', handles.repetition)
381     set(handles.Q_exp_edit, 'enable', 'off')
382     set(handles.Q2_exp_edit, 'enable', 'off')
383     set(handles.A_exp_edit, 'enable', 'off')
384     set(handles.A2_exp_edit, 'enable', 'off')
385     set(handles.B_exp_edit, 'enable', 'off')
386     set(handles.B2_exp_edit, 'enable', 'off')
387     set(handles.C_exp_edit, 'enable', 'off')
388     set(handles.C2_exp_edit, 'enable', 'off')
389     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)

```



```

390     set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
391
392 case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
393     handles.amplitude_1 = 1;
394     handles.duration_1 = 1;
395     handles.amplitude_2 = 0.5;
396     handles.duration_2 = 1;
397     handles.biphasic = 10;
398     handles.delay = 1;
399     handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
400     handles.duration_balance_2 = 0;
401     handles.decay = 1;
402     handles.repetition = 0;
403     handles.q = 1;
404     handles.q2 = 2.1972e+03;
405     handles.rep_amp_ratio = 1;
406
407     % Building the Quasi-Trapezoidal Wave
408     handles.decay_steps = handles.decay/handles.resolution;
409     handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
410     i=1;
411     total_decay_amplitude = 0;
412     for i=1:handles.decay_steps
413         handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.amplitude_1
*handles.q*...
414             exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s)).*...
415             ones(1,handles.resolution*handles.time_resolution));
416         total_decay_amplitude = total_decay_amplitude + (handles.amplitude_1*
handles.q*...
417             exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
418     end
419     amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
420     handles.duration_balance_total = handles.biphasic.*(handles.duration_1 +
handles.decay);
421     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
422     handles.fullstimulation_duration = handles.stimulation_fulltime;
423     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
424     handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.delay*
handles.time_resolution))...
425         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
426         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...

```

```

427         -((handles.stimulation_fulltime)*handles.time_resolution)]]);
428     %
429     handles.current_data_I = handles.quasi_trap;
430     handles.stimulation_data_I = handles.quasi_trap;
431
432     % Define which edit fields should work and define its initial values
433     set(handles.amplitude1_edit, 'enable', 'on','String', handles.amplitude_1
)
434     set(handles.duration1_edit, 'enable', 'on','String', handles.duration_1)
435     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
436     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
437     set(handles.amplitude2_edit, 'enable', 'off')
438     set(handles.duration2_edit, 'enable', 'off')
439     set(handles.decay_edit, 'enable', 'on','String', handles.decay)
440     set(handles.resolution_edit, 'enable', 'on','String', handles.resolution)
441     set(handles.repetition_edit, 'enable', 'on','String', handles.repetition)
442     set(handles.Q_exp_edit, 'enable', 'on','String', handles.q)
443     set(handles.Q2_exp_edit, 'enable', 'on', 'String', handles.q2)
444     set(handles.A_exp_edit, 'enable', 'off')
445     set(handles.A2_exp_edit, 'enable', 'off')
446     set(handles.B_exp_edit, 'enable', 'off')
447     set(handles.B2_exp_edit, 'enable', 'off')
448     set(handles.C_exp_edit, 'enable', 'off')
449     set(handles.C2_exp_edit, 'enable', 'off')
450     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
451     set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
452
453     case 'Tri-Exponential' % User selects tri-exponential
454         handles.amplitude_1 = 1;
455         handles.duration_1 = 1;
456         handles.amplitude_2 = 0.5;
457         handles.duration_2 = 1;
458         handles.biphasic = 10;
459         handles.delay = 1;
460         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
461         handles.duration_balance_2 = 0;
462         handles.decay = 1;
463         handles.repetition = 0;
464         handles.resolution = 0.25;
465         handles.a = 0.2;
466         handles.a2 = 1.197e+03;
467         handles.b = 0.3;
468         handles.b2 = 2.197e+03;
469         handles.c = 0.5;
470         handles.c2 = 3.197e+03;
471         handles.repetition = 0;

```

```

472     handles.rep_amp_ratio = 1;
473
474     % Building the Tri-Exponential Wave
475     handles.increase_steps = handles.duration_1/handles.resolution;
476     handles.decay_steps = handles.decay/handles.resolution;
477     handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
478     j_i = 1;
479     j_d = 1;
480     total_increase_amplitude = 0;
481     total_decay_amplitude = 0;
482     for j_i=1:handles.increase_steps
483         handles.tri_exp = horzcat(handles.tri_exp, (((-handles.amplitude_1)
/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.resolution*
handles.time_resolution)...
484             +(-((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
485             ones(1,handles.resolution*handles.time_resolution));
486         total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
487             -((handles.amplitude_1*handles.t_i)/(handles.duration_1+handles.
t_i)-handles.t_i))/handles.time_resolution);
488     end
489     for j_d=1:handles.decay_steps
490         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((handles.
t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
491             exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))+
handles.b*...
492             exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))+
handles.c*...
493             exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
.*...
494             ones(1,handles.resolution*handles.time_resolution));
495         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
496             exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))+
handles.b*...
497             exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))+
handles.c*...
498             exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)));
499     end
500     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
501     handles.duration_balance_total = handles.biphasic.*(handles.duration_1 +
handles.decay);
502     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
503     handles.fullstimulation_duration = handles.stimulation_fulltime;

```

```

504     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
505     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
506         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
507         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution)...
508         -((handles.stimulation_fulltime)*handles.time_resolution))]);
509     %
510     handles.current_data_I = handles.tri_exp;
511     handles.stimulation_data_I = handles.tri_exp;
512
513     % Define which edit fields should work and define its initial values
514     set(handles.amplitude1_edit, 'enable', 'on','String', handles.amplitude_1
)
515     set(handles.duration1_edit, 'enable', 'on','String', handles.duration_1)
516     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
517     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
518     set(handles.amplitude2_edit, 'enable', 'off')
519     set(handles.duration2_edit, 'enable', 'off')
520     set(handles.decay_edit, 'enable', 'on','String', handles.decay)
521     set(handles.resolution_edit, 'enable', 'on','String', handles.resolution)
522     set(handles.repetition_edit, 'enable', 'on','String', handles.repetition)
523     set(handles.Q_exp_edit, 'enable', 'off')
524     set(handles.Q2_exp_edit, 'enable', 'off')
525     set(handles.A_exp_edit, 'enable', 'on','String', handles.a)
526     set(handles.A2_exp_edit, 'enable', 'on', 'String', handles.a2)
527     set(handles.B_exp_edit, 'enable', 'on','String', handles.b)
528     set(handles.B2_exp_edit, 'enable', 'on', 'String', handles.b2)
529     set(handles.C_exp_edit, 'enable', 'on','String', handles.c)
530     set(handles.C2_exp_edit, 'enable', 'on', 'String', handles.c2)
531     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
532     set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
533
534     case 'Bursting' % User selects bursting strategies
535         handles.amplitude_1 = 1;
536         handles.duration_1 = 1;
537         handles.amplitude_2 = 0.5;
538         handles.duration_2 = 1;
539         handles.biphasic = 10;
540         handles.delay = 1;
541         handles.duration_balance_2 = 0;
542         handles.decay = 0;
543         handles.duration_balance_1 = handles.biphasic.*(handles.duration_1/2);
544         handles.resolution = 0.25;

```

```

545     handles.repetition = 0;
546     handles.rep_amp_ratio = 1;
547     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+
handles.duration_balance_1+handles.duration_balance_2+handles.delay+handles.
decay;
548     handles.fullstimulation_duration = handles.stimulation_fulltime;
549     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
550
551     % Building the Bursting Wave
552     handles.burst_steps = handles.duration_1/handles.resolution;
553     handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
554     k=1;
555     for k=1:handles.burst_steps
556         handles.bursting = horzcat(handles.bursting,[-handles.amplitude_1
.*...
557             ones(1,(handles.resolution/2)*handles.time_resolution) ...
558             zeros(1,(handles.resolution/2)*handles.time_resolution)]);
559     end
560     handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*
handles.time_resolution))...
561         ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones(1,
handles.duration_balance_1*handles.time_resolution)...
562         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution)...
563         -((handles.stimulation_fulltime)*handles.time_resolution))]);
564     %
565     handles.current_data_I = handles.bursting;
566     handles.stimulation_data_I = handles.bursting;
567
568     % Define which edit fields should work and define its initial values
569     set(handles.amplitude1_edit, 'enable', 'on','String', handles.amplitude_1
)
570     set(handles.duration1_edit, 'enable', 'on','String', handles.duration_1)
571     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
572     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
573     set(handles.amplitude2_edit, 'enable', 'off')
574     set(handles.duration2_edit, 'enable', 'off')
575     set(handles.decay_edit, 'enable', 'off')
576     set(handles.resolution_edit, 'enable', 'on','String', handles.resolution)
577     set(handles.repetition_edit, 'enable', 'on','String', handles.repetition)
578     set(handles.Q_exp_edit, 'enable', 'off')
579     set(handles.Q2_exp_edit, 'enable', 'off')
580     set(handles.A_exp_edit, 'enable', 'off')
581     set(handles.A2_exp_edit, 'enable', 'off')
582     set(handles.B_exp_edit, 'enable', 'off')
583     set(handles.B2_exp_edit, 'enable', 'off')
584     set(handles.C_exp_edit, 'enable', 'off')

```

```

585     set(handles.C2_exp_edit, 'enable', 'off')
586     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
587     set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
588
589
590 case 'Load Waveform' % User selects to load an arbitrary waveform
591     final_answer = questdlg('Loaded Waveform can only have a maximum of 930
data points. Timings and Discharge Phase are of user responsibility.
Amplitude is a multiplication value in this case',...
592         'Load Waveform...', 'OK', 'Cancel', 'Cancel');
593     switch final_answer
594         case 'OK'
595             handles.amplitude_1 = 1;
596             handles.repetition = 0;
597             handles.rep_amp_ratio = 1;
598
599             % Define which edit fields should work and define its initial
values
600             set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
601             set(handles.duration1_edit, 'enable', 'off')
602             set(handles.amplitude2_edit, 'enable', 'off')
603             set(handles.duration1_edit, 'enable', 'off')
604             set(handles.duration2_edit, 'enable', 'off')
605             set(handles.decay_edit, 'enable', 'off')
606             set(handles.delay_edit, 'enable', 'off')
607             set(handles.biphasic_edit, 'enable', 'off');
608             set(handles.resolution_edit, 'enable', 'off')
609             set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
610             set(handles.Q_exp_edit, 'enable', 'off')
611             set(handles.Q2_exp_edit, 'enable', 'off')
612             set(handles.A_exp_edit, 'enable', 'off')
613             set(handles.A2_exp_edit, 'enable', 'off')
614             set(handles.B_exp_edit, 'enable', 'off')
615             set(handles.B2_exp_edit, 'enable', 'off')
616             set(handles.C_exp_edit, 'enable', 'off')
617             set(handles.C2_exp_edit, 'enable', 'off')
618             set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
619
620             % Allows the use to choose the file to load
621             try
622                 [FileName,PathName] = uigetfile('*.*txt','Select the TXT file'
);
623                 filename = [PathName FileName];

```

```

624         delimiterIn = ' ';
625         handles.current_data_I = importdata(filename,delimiterIn);
626     catch err
627         % Case the user doesnt want to load waveform afterall
628         errordlg('Something went wrong',...
629             'Invalid Input','modal')
630         uicontrol(hObject)
631         return
632     end
633
634     % Checks is data has the limit size
635     if length(handles.current_data_I) > 930
636         errordlg('Too many data points!','Invalid TXT File','modal')
637         uicontrol(hObject)
638         return
639     else
640         handles.stimulation_data_I = handles.current_data_I;
641         set(handles.stim_duration_edit, 'enable', 'on','String',
(0:(1/handles.time_resolution):(length(handles.current_data_I)/handles.
time_resolution)))
642     end
643     case ' Cancel'
644     end
645
646 end
647
648 guidata(hObject, handles);
649
650
651 % --- Executes during object creation, after setting all properties.
652 function plot_popup_CreateFcn(hObject, eventdata, handles)
653 % hObject    handle to plot_popup (see GCBO)
654 % eventdata  reserved - to be defined in a future version of MATLAB
655 % handles    empty - handles not created until after all CreateFcns called
656
657 % Hint: popupmenu controls usually have a white background on Windows.
658 %       See ISPC and COMPUTER.
659 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
660     set(hObject,'BackgroundColor','white');
661 end
662
663
664
665 function amplitude1_edit_Callback(hObject, eventdata, handles)
666 % hObject    handle to amplitude1_edit (see GCBO)
667 % eventdata  reserved - to be defined in a future version of MATLAB
668 % handles    structure with handles and user data (see GUIDATA)

```

```
669
670 % Hints: get(hObject,'String') returns contents of amplitude1_edit as text
671 %         str2double(get(hObject,'String')) returns contents of amplitude1_edit as
        a double
672
673 % Data input by user
674 amplitude_1_input = str2double(get(hObject,'string'));
675
676 if isfield(handles, 'plot_popup_value' )
677     % handles.plot_popup_value exists - you may access it
678 else
679     % handles.plot_popup_value does not exist
680     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
681     uicontrol(hObject)
682     return
683 end
684
685 % If there is no amplitude input, if it is non-numeric, or if the input is 0,
        error
686 if isnan(amplitude_1_input) || amplitude_1_input == 0
687     errordlg('You must enter a numeric value bigger than 0 (zero)','Invalid Input
        ','modal')
688     uicontrol(hObject)
689     return
690 % If there is a maximum amplitude calculated, it confirms if its below it
        otherwise error
691 elseif handles.amplitude_max ~=0 && amplitude_1_input > handles.amplitude_max
692     errordlg('That value breaches the Safe Limit Range','Invalid Input','modal')
693     uicontrol(hObject)
694     return
695 % The Quad-DAC maximum Output is 5V
696 elseif amplitude_1_input > 5
697     errordlg('DACs higher output is 5V','Invalid Input','modal')
698     uicontrol(hObject)
699     return
700 % If the value doesnt have any 'problem', builds the Waveforms with the
701 % inputed value
702 else
703     handles.amplitude_1 = amplitude_1_input;
704     value = handles.plot_popup_value;
705     string = handles.plot_popup_string;
706     switch string{value}
707         case 'Bi-level Lilly' % Case user has selected bilevel Lilly
708             amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
        amplitude_2*handles.duration_2)/handles.biphasic;
709             handles.duration_balance_total = handles.biphasic.*(handles.
        duration_1 + handles.duration_2);
```



```

710         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
711         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
712         handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
713         (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
714         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
715         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
716         -((handles.stimulation_fulltime)*handles.time_resolution))]];
717         handles.current_data_I = handles.bi_level;
718         handles.stimulation_data_I = handles.bi_level;
719         case 'Quasi-Trapezoidal' % Case user has selected quasi-trapezoidal
720         handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
721         i=1;
722         total_decay_amplitude = 0;
723         for i=1:handles.decay_steps
724             handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
725                 exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
726                 ones(1,handles.resolution*handles.time_resolution));
727             total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
728                 exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
729         end
730         amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
731         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
732         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
733         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
734         handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
735         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
736         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
737         -((handles.stimulation_fulltime)*handles.time_resolution))]];
738         handles.current_data_I = handles.quasi_trap;
739         handles.stimulation_data_I = handles.quasi_trap;
740         case 'Tri-Exponential' % Case user has selected tri-exponential

```

```

741         handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
742         j_i = 1;
743         j_d = 1;
744         total_increase_amplitude = 0;
745         total_decay_amplitude = 0;
746         for j_i=1:handles.increase_steps
747             handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
748                 +((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
749                 ones(1,handles.resolution*handles.time_resolution));
750             total_increase_amplitude = total_increase_amplitude + (((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
751                 -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
752         end
753         for j_d=1:handles.decay_steps
754             handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
755                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
756                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
757                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
758                 ones(1,handles.resolution*handles.time_resolution));
759             total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
760                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
761                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
762                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
763         end
764         amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
765         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
766         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
767         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
768         handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...

```

```

769         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
770         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
771         -((handles.stimulation_fulltime)*handles.time_resolution))))];
772         handles.current_data_I = handles.tri_exp;
773         handles.stimulation_data_I = handles.tri_exp;
774         case 'Bursting' % Case user has selected bursting strategies
775             handles.duration_balance_1 = handles.biphasic.*(handles.duration_1/2)
;
776             handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
777             k=1;
778             for k=1:handles.burst_steps
779                 handles.bursting = horzcat(handles.bursting,[-handles.amplitude_1
.*...
780                 ones(1,(handles.resolution/2)*handles.time_resolution) ...
781                 zeros(1,(handles.resolution/2)*handles.time_resolution)]);
782             end
783             handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*
handles.time_resolution))...
784             ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
785             zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
786             -((handles.stimulation_fulltime)*handles.time_resolution))))];
787             handles.current_data_I = handles.bursting;
788             handles.stimulation_data_I = handles.bursting;
789             case 'Rectangular' % Case user has selected pulse
790                 handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
791                 zeros(1,(handles.delay*handles.time_resolution))...
792                 ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
793                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
794                 -((handles.stimulation_fulltime)*handles.time_resolution))))];
795                 handles.current_data_I = handles.pulse;
796                 handles.stimulation_data_I = handles.pulse;
797             case 'Load Waveform' % Case user has loaded its own waveform
798                 handles.current_data_I = handles.amplitude_1.* handles.current_data_I
;
799                 handles.stimulation_data_I = handles.current_data_I;
800         end
801
802         % If there is a repetition defined, it rebuilds the waveform with the
803         % repetitions
804         handles.reps_max = 0;
805         if handles.repetition ~= 0

```

```

806     for n_reps = 1:handles.n_repetitions
807         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
            amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
            handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
            reps_max == 0)...
808             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
                <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
                DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
                +1)) ) && handles.reps_max == 0)
809                 handles.reps_max = n_reps;
810         end
811         if handles.reps_max ~=0
812             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
                handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
                .^(handles.reps_max)).*handles.stimulation_data_I);
813         else
814             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
                handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
                .^(n_reps)).*handles.stimulation_data_I);
815         end
816     end
817 end
818
819 % If time stimulation created is bigger than the chosen value of stimulation,
    it
820 % replaces it on the GUI
821 if handles.fullstimulation_duration < handles.stimulation_fulltime
822     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
        stimulation_fulltime)
823 end
824
825 end
826
827 guidata(hObject, handles);
828
829
830 % --- Executes during object creation, after setting all properties.
831 function amplitude1_edit_CreateFcn(hObject, eventdata, handles)
832 % hObject    handle to amplitude1_edit (see GCBO)
833 % eventdata  reserved - to be defined in a future version of MATLAB
834 % handles    empty - handles not created until after all CreateFcns called
835
836 % Hint: edit controls usually have a white background on Windows.
837 %         See ISPC and COMPUTER.
838 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
        defaultUicontrolBackgroundColor'))
839     set(hObject,'BackgroundColor','white');
840 end

```

```
841
842
843
844 function duration1_edit_Callback(hObject, eventdata, handles)
845 % hObject    handle to duration1_edit (see GCBO)
846 % eventdata  reserved - to be defined in a future version of MATLAB
847 % handles    structure with handles and user data (see GUIDATA)
848
849 % Hints: get(hObject,'String') returns contents of duration1_edit as text
850 %         str2double(get(hObject,'String')) returns contents of duration1_edit as
      a double
851
852 % Data input by user
853 duration_1_input = str2double(get(hObject,'string'));
854
855 if isfield(handles, 'plot_popup_value' )
856     % handles.plot_popup_value exists - you may access it
857 else
858     % handles.plot_popup_value does not exist
859     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
860     uicontrol(hObject)
861     return
862 end
863
864 % If there is no duration value, if it is non-numeric, or if it is smaller than
      0.1ms, error
865 if isnan(duration_1_input) || duration_1_input < 0.1
866     errordlg('You must enter a numeric value bigger than 0.1','Invalid Input','
      modal')
867     uicontrol(hObject)
868     return
869 % If the input value leads to a non-integer value when multiplied by the
870 % time resolution it throws error because it would lead to a array error
871 elseif ((duration_1_input*handles.time_resolution) - floor(duration_1_input*
      handles.time_resolution)) ~= 0
872     errordlg('Invalid input','Invalid Input','modal')
873     uicontrol(hObject)
874     return
875 % If the length of the one pulse stimulation is bigger than the MCU maximum,
876 % do to its memory limitations, error
877 elseif length((0:(1/handles.time_resolution):(duration_1_input+handles.duration_2
      +(handles.biphasic*duration_1_input)+(handles.biphasic*handles.decay)+(
      handles.biphasic*handles.duration_2)+handles.delay+handles.decay))) > 930
878     errordlg('The full duration of the pulse has to be smaller','Invalid Input','
      modal')
879     uicontrol(hObject)
880     return
881 % Else, it starts building the waveform
```

```

882 else
883     handles.duration_1 = duration_1_input;
884     handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
885     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
886     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
887     handles.burst_steps = handles.duration_1/handles.resolution;
888     handles.increase_steps = handles.duration_1/handles.resolution;
889     value = handles.plot_popup_value;
890     string = handles.plot_popup_string;
891     switch string{value}
892         case 'Bi-level Lilly' % Case user has selected bilevel Lilly
893             amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
amplitude_2*handles.duration_2)/handles.biphasic;
894             handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.duration_2);
895             handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
896             handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
897             handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
898                 (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
899                 amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
900                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
901                     -((handles.stimulation_fulltime)*handles.time_resolution)))]];
902             handles.current_data_I = handles.bi_level;
903             handles.stimulation_data_I = handles.bi_level;
904             case 'Quasi-Trapezoidal' % Case user has selected quasi-trapezoidal
905                 handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
906                 i=1;
907                 total_decay_amplitude = 0;
908                 for i=1:handles.decay_steps
909                     handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
910                         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
911                             ones(1,handles.resolution*handles.time_resolution));
912                     total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
913                         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
914                 end

```

```

915         amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
916         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
917         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
918         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
919         handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
920         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
921         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
922         -((handles.stimulation_fulltime)*handles.time_resolution))]);
923         handles.current_data_I = handles.quasi_trap;
924         handles.stimulation_data_I = handles.quasi_trap;
925         case 'Tri-Exponential' % Case user has selected tri-exponential
926         handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
927         j_i = 1;
928         j_d = 1;
929         total_increase_amplitude = 0;
930         total_decay_amplitude = 0;
931         for j_i=1:handles.increase_steps
932         handles.tri_exp = horzcat(handles.tri_exp, ((((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
933         +(-((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
934         ones(1,handles.resolution*handles.time_resolution));
935         total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
936         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
937         end
938         for j_d=1:handles.decay_steps
939         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
940         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
941         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
942         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
943         ones(1,handles.resolution*handles.time_resolution));
944         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...

```

```

945         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
946         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
947         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
948     end
949     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
950     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
951     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
952     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
953     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
954     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
955     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
956     -((handles.stimulation_fulltime)*handles.time_resolution))]);
957     handles.current_data_I = handles.tri_exp;
958     handles.stimulation_data_I = handles.tri_exp;
959     case 'Bursting' % Case user has selected bursting strategies
960     handles.duration_balance_1 = handles.biphasic.*(handles.duration_1/2)
;
961     handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
962     k=1;
963     for k=1:handles.burst_steps
964     handles.bursting = horzcat(handles.bursting,[-handles.amplitude_1
.*...
965     ones(1,(handles.resolution/2)*handles.time_resolution) ...
966     zeros(1,(handles.resolution/2)*handles.time_resolution)]);
967     end
968     handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*
handles.time_resolution))...
969     ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
970     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
971     -((handles.stimulation_fulltime)*handles.time_resolution))]);
972     handles.current_data_I = handles.bursting;
973     handles.stimulation_data_I = handles.bursting;
974     case 'Rectangular' % Case user has selected pulse
975     handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
976     zeros(1,(handles.delay*handles.time_resolution))...

```



```

977         ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
978         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
979         -((handles.stimulation_fulltime)*handles.time_resolution)))]];
980         handles.current_data_I = handles.pulse;
981         handles.stimulation_data_I = handles.pulse;
982     end
983
984     % If there is a repetition defined, it rebuilds the waveform with the
985     % repetitions
986     handles.reps_max = 0;
987     if handles.repetition ~= 0
988         for n_reps = 1:handles.n_repetitions
989             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
990                 || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
991                 handles.reps_max = n_reps;
992             end
993             if handles.reps_max ~=0
994                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
995             else
996                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
997             end
998         end
999     end
1000
1001     % If time stimulation created is bigger than the chosen value of stimulation,
1002     % it
1003     % replaces it on the GUI
1004     if handles.fullstimulation_duration < handles.stimulation_fulltime
1005         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
1006     end
1007 end
1008
1009
1010 guidata(hObject, handles);

```

```
1011
1012
1013 % --- Executes during object creation, after setting all properties.
1014 function duration1_edit_CreateFcn(hObject, eventdata, handles)
1015 % hObject    handle to duration1_edit (see GCBO)
1016 % eventdata  reserved - to be defined in a future version of MATLAB
1017 % handles    empty - handles not created until after all CreateFcns called
1018
1019 % Hint: edit controls usually have a white background on Windows.
1020 %         See ISPC and COMPUTER.
1021 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
    defaultUicontrolBackgroundColor'))
1022     set(hObject,'BackgroundColor','white');
1023 end
1024
1025
1026
1027 function delay_edit_Callback(hObject, eventdata, handles)
1028 % hObject    handle to delay_edit (see GCBO)
1029 % eventdata  reserved - to be defined in a future version of MATLAB
1030 % handles    structure with handles and user data (see GUIDATA)
1031
1032 % Hints: get(hObject,'String') returns contents of delay_edit as text
1033 %         str2double(get(hObject,'String')) returns contents of delay_edit as a
    double
1034
1035 % Data input by user
1036 delay_input = str2double(get(hObject,'string'));
1037
1038 if isfield(handles, 'plot_popup_value' )
1039     % handles.firing_popup_value exists - you may access it
1040 else
1041     % handles.firing_popup_value does not exist
1042     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
1043     uicontrol(hObject)
1044     return
1045 end
1046
1047 % If there is no delay value or has a non-number value, error
1048 if isnan(delay_input)
1049     errordlg('You must enter a numeric value','Invalid Input','modal')
1050     uicontrol(hObject)
1051     return
1052 % If the input value leads to a non-integer value when multiplied by the
1053 % time resolution it throws error because it would lead to a array error
1054 elseif ((delay_input*handles.time_resolution) - floor(delay_input*handles.
    time_resolution)) ~= 0
1055     errordlg('Invalid input','Invalid Input','modal')
```

```

1056     uicontrol(hObject)
1057     return
1058 % If the length of the one pulse stimulation is bigger than the MCU maximum,
1059 % do to its memory limitations, error
1060 elseif length((0:(1/handles.time_resolution):(handles.duration_1+handles.
    duration_2+(handles.biphasic*(handles.duration_1 + handles.duration_2+handles
    .delay))+delay_input+handles.decay))) > 930
1061     errordlg('The full duration of the pulse has to be smaller','Invalid Input',
    'modal')
1062     uicontrol(hObject)
1063     return
1064 % Else, waveform is build
1065 else
1066     handles.delay = delay_input;
1067     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
    duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
1068     handles.timescale = (0:(1/handles.time_resolution):(handles.
    stimulation_fulltime+handles.t_f));
1069     handles.duration_balance_1 = handles.biphasic*handles.duration_1;
1070     value = handles.plot_popup_value;
1071     string = handles.plot_popup_string;
1072     switch string{value}
1073         case 'Bi-level Lilly' % User selects bilevel Lilly
1074             amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
    amplitude_2*handles.duration_2)/handles.biphasic;
1075             handles.duration_balance_total = handles.biphasic.*(handles.
    duration_1 + handles.duration_2);
1076             handles.stimulation_fulltime = handles.duration_1+handles.
    duration_balance_total+handles.delay+handles.decay;
1077             handles.timescale = (0:(1/handles.time_resolution):(handles.
    stimulation_fulltime+handles.t_f));
1078             handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
    handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
1079                 (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
    time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
1080                 amplitude_CB.*ones(1,handles.duration_balance_total*handles.
    time_resolution)...
1081                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
    time_resolution)...
1082                 -((handles.stimulation_fulltime)*handles.time_resolution))]];
1083             handles.current_data_I = handles.bi_level;
1084             handles.stimulation_data_I = handles.bi_level;
1085         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
1086             handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
    handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
1087             i=1;
1088             total_decay_amplitude = 0;
1089             for i=1:handles.decay_steps

```

```

1090         handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
1091         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
1092         ones(1,handles.resolution*handles.time_resolution));
1093         total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
1094         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
1095     end
1096     amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
1097     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
1098     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
1099     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1100     handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
1101     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1102     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
1103     -((handles.stimulation_fulltime)*handles.time_resolution))]);
1104     handles.current_data_I = handles.quasi_trap;
1105     handles.stimulation_data_I = handles.quasi_trap;
1106     case 'Tri-Exponential' % User selects tri-exponential
1107         handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
1108         j_i = 1;
1109         j_d = 1;
1110         total_increase_amplitude = 0;
1111         total_decay_amplitude = 0;
1112         for j_i=1:handles.increase_steps
1113             handles.tri_exp = horzcat(handles.tri_exp, ((((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution))...
1114             +((-(-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
1115             ones(1,handles.resolution*handles.time_resolution));
1116             total_increase_amplitude = total_increase_amplitude + (((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution))...
1117             -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
1118         end
1119         for j_d=1:handles.decay_steps
1120             handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...

```

```

1121         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
    +(handles.b*...
1122         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
    +(handles.c*...
1123         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
    )*. ...
1124         ones(1,handles.resolution*handles.time_resolution));
1125         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
    ((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
1126         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
    +(handles.b*...
1127         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
    +(handles.c*...
1128         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
    );
1129         end
1130         amplitude_CB = (total_increase_amplitude*handles.resolution +
    total_decay_amplitude*handles.resolution)/handles.biphasic;
1131         handles.duration_balance_total = handles.biphasic.*(handles.
    duration_1 + handles.decay);
1132         handles.stimulation_fulltime = handles.duration_1+handles.
    duration_balance_total+handles.delay+handles.decay;
1133         handles.timescale = (0:(1/handles.time_resolution):(handles.
    stimulation_fulltime+handles.t_f));
1134         handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
    handles.time_resolution))...
1135         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
    time_resolution)...
1136         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
    time_resolution))...
1137         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1138         handles.current_data_I = handles.tri_exp;
1139         handles.stimulation_data_I = handles.tri_exp;
1140         case 'Bursting' % User selects bursting strategies
1141             handles.duration_balance_1 = handles.biphasic.*(handles.duration_1/2)
    ;
1142             handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
1143             k=1;
1144             for k=1:handles.burst_steps
1145                 handles.bursting = horzcat(handles.bursting,[-handles.amplitude_1
    .*...
1146                 ones(1,(handles.resolution/2)*handles.time_resolution) ...
1147                 zeros(1,(handles.resolution/2)*handles.time_resolution)]);
1148             end
1149             handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*
    handles.time_resolution))...
1150             ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
    (1,handles.duration_balance_1*handles.time_resolution)...

```

```

1151         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
1152         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1153         handles.current_data_I = handles.bursting;
1154         handles.stimulation_data_I = handles.bursting;
1155         case 'Rectangular' % User selects squar
1156             handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
1157                 zeros(1,(handles.delay*handles.time_resolution))...
1158                 ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
1159                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
1160                 -((handles.stimulation_fulltime)*handles.time_resolution))]);
1161             handles.current_data_I = handles.pulse;
1162             handles.stimulation_data_I = handles.pulse;
1163         end
1164
1165         % If there is a repetition defined, it rebuilds the waveform with the
1166         % repetitions
1167         handles.reps_max = 0;
1168         if handles.repetition ~= 0
1169             for n_reps = 1:handles.n_repetitions
1170                 if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^n_reps+1)) && handles.
reps_max == 0)...
1171                 || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^n_reps
+1)) ) && handles.reps_max == 0)
1172                     handles.reps_max = n_reps;
1173                 end
1174                 if handles.reps_max ~=0
1175                     handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
1176                 else
1177                     handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
1178                 end
1179             end
1180         end
1181
1182         % If time stimulation created is bigger than the chosen value of stimulation,
it
1183         % replaces it on the GUI

```

```
1184     if handles.fullstimulation_duration < handles.stimulation_fulltime
1185         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
            stimulation_fulltime)
1186     end
1187
1188 end
1189
1190 guidata(hObject, handles);
1191
1192
1193 % --- Executes during object creation, after setting all properties.
1194 function delay_edit_CreateFcn(hObject, eventdata, handles)
1195 % hObject    handle to delay_edit (see GCBO)
1196 % eventdata  reserved - to be defined in a future version of MATLAB
1197 % handles    empty - handles not created until after all CreateFcns called
1198
1199 % Hint: edit controls usually have a white background on Windows.
1200 %       See ISPC and COMPUTER.
1201 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
            defaultUicontrolBackgroundColor'))
1202     set(hObject,'BackgroundColor','white');
1203 end
1204
1205
1206
1207 function biphasic_edit_Callback(hObject, eventdata, handles)
1208 % hObject    handle to biphasic_edit (see GCBO)
1209 % eventdata  reserved - to be defined in a future version of MATLAB
1210 % handles    structure with handles and user data (see GUIDATA)
1211
1212 % Hints: get(hObject,'String') returns contents of biphasic_edit as text
1213 %       str2double(get(hObject,'String')) returns contents of biphasic_edit as a
            double
1214
1215 % Data input by user
1216 biphasic_input = str2double(get(hObject,'string'));
1217
1218 if isfield(handles, 'plot_popup_value' )
1219     % handles.firing_popup_value exists - you may access it
1220 else
1221     % handles.firing_popup_value does not exist
1222     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
1223     uicontrol(hObject)
1224     return
1225 end
1226
1227 % If there is no biphasic value or its non-numeric
1228 if isnan(biphasic_input) %|| biphasic_input == 0
```

```

1229     errordlg('You must enter a numeric value','Invalid Input','modal')
1230     uicontrol(hObject)
1231     return
1232 elseif length((0:(1/handles.time_resolution):(handles.duration_1+handles.
    duration_2+(biphasic_input*handles.duration_1)+(biphasic_input*handles.
    duration_2)+(biphasic_input*handles.decay)+handles.delay+handles.decay))) >
    930
1233     errordlg('The full duration of the pulse has to be smaller','Invalid Input','
    modal')
1234     uicontrol(hObject)
1235     return
1236 else
1237     handles.biphasic = biphasic_input;
1238     handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
1239     handles.duration_balance_2 = handles.biphasic*handles.duration_2;
1240     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
    duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
1241     handles.timescale = (0:(1/handles.time_resolution):(handles.
    stimulation_fulltime+handles.t_f));
1242     value = handles.plot_popup_value;
1243     string = handles.plot_popup_string;
1244     switch string{value}
1245         case 'Bi-level Lilly' % User selects bilevel Lilly
1246             amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
    amplitude_2*handles.duration_2)/handles.biphasic;
1247             handles.duration_balance_total = handles.biphasic.*(handles.
    duration_1 + handles.duration_2);
1248             handles.stimulation_fulltime = handles.duration_1+handles.
    duration_balance_total+handles.delay+handles.decay;
1249             handles.timescale = (0:(1/handles.time_resolution):(handles.
    stimulation_fulltime+handles.t_f));
1250             handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
    handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
1251             (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
    time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
1252             amplitude_CB.*ones(1,handles.duration_balance_total*handles.
    time_resolution)...
1253             zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
    time_resolution)...
1254             -((handles.stimulation_fulltime)*handles.time_resolution))]];
1255             handles.current_data_I = handles.bi_level;
1256             handles.stimulation_data_I = handles.bi_level;
1257         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
1258             handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
    handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
1259             i=1;
1260             total_decay_amplitude = 0;
1261             for i=1:handles.decay_steps

```



```

1262         handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
1263         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
1264         ones(1,handles.resolution*handles.time_resolution));
1265         total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
1266         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
1267     end
1268     amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
1269     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
1270     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
1271     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1272     handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
1273     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1274     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
1275     -((handles.stimulation_fulltime)*handles.time_resolution))]);
1276     handles.current_data_I = handles.quasi_trap;
1277     handles.stimulation_data_I = handles.quasi_trap;
1278     case 'Tri-Exponential' % User selects tri-exponential
1279         handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
1280         j_i = 1;
1281         j_d = 1;
1282         total_increase_amplitude = 0;
1283         total_decay_amplitude = 0;
1284         for j_i=1:handles.increase_steps
1285             handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
1286             +(-((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
1287             ones(1,handles.resolution*handles.time_resolution));
1288             total_increase_amplitude = total_increase_amplitude + (((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
1289             -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
1290         end
1291         for j_d=1:handles.decay_steps
1292             handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...

```

```

1293         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+ (handles.b*...
1294         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+ (handles.c*...
1295         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
1296         ones(1,handles.resolution*handles.time_resolution));
1297         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
1298         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+ (handles.b*...
1299         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+ (handles.c*...
1300         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
1301         end
1302         amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
1303         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
1304         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
1305         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1306         handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
1307         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1308         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
1309         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1310         handles.current_data_I = handles.tri_exp;
1311         handles.stimulation_data_I = handles.tri_exp;
1312         case 'Bursting' % User selects bursting strategies
1313         handles.duration_balance_1 = handles.biphasic.*(handles.duration_1/2)
;
1314         handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
1315         k=1;
1316         for k=1:handles.burst_steps
1317         handles.bursting = horzcat(handles.bursting,[-handles.amplitude_1
.*...
1318         ones(1,(handles.resolution/2)*handles.time_resolution) ...
1319         zeros(1,(handles.resolution/2)*handles.time_resolution)]);
1320         end
1321         handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*
handles.time_resolution))...
1322         ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...

```

```

1323         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
1324         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1325         handles.current_data_I = handles.bursting;
1326         handles.stimulation_data_I = handles.bursting;
1327         case 'Rectangular' % User selects square
1328             handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
1329                 zeros(1,(handles.delay*handles.time_resolution))...
1330                 ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
1331                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
1332                 -((handles.stimulation_fulltime)*handles.time_resolution))]);
1333             handles.current_data_I = handles.pulse;
1334             handles.stimulation_data_I = handles.pulse;
1335         end
1336
1337         % If there is a repetition defined, it rebuilds the waveform with the
1338         % repetitions
1339         handles.reps_max = 0;
1340         if handles.repetition ~= 0
1341             for n_reps = 1:handles.n_repetitions
1342                 if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^n_reps+1)) && handles.
reps_max == 0)...
1343                 || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^n_reps
+1)) ) && handles.reps_max == 0)
1344                 handles.reps_max = n_reps;
1345             end
1346             if handles.reps_max ~=0
1347                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
1348             else
1349                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
1350             end
1351         end
1352     end
1353
1354     % If time stimulation created is bigger than the chosen value of stimulation,
it
1355     % replaces it on the GUI

```

```
1356     if handles.fullstimulation_duration < handles.stimulation_fulltime
1357         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
            stimulation_fulltime)
1358     end
1359
1360 end
1361
1362 set(handles.stim_duration_edit, 'enable', 'on','String', handles.
            stimulation_fulltime)
1363
1364
1365 guidata(hObject, handles);
1366
1367
1368 % --- Executes during object creation, after setting all properties.
1369 function biphasic_edit_CreateFcn(hObject, eventdata, handles)
1370 % hObject    handle to biphasic_edit (see GCBO)
1371 % eventdata  reserved - to be defined in a future version of MATLAB
1372 % handles    empty - handles not created until after all CreateFcns called
1373
1374 % Hint: edit controls usually have a white background on Windows.
1375 %         See ISPC and COMPUTER.
1376 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
            defaultUicontrolBackgroundColor'))
1377     set(hObject,'BackgroundColor','white');
1378 end
1379
1380
1381
1382 function repetition_edit_Callback(hObject, eventdata, handles)
1383 % hObject    handle to repetition_edit (see GCBO)
1384 % eventdata  reserved - to be defined in a future version of MATLAB
1385 % handles    structure with handles and user data (see GUIDATA)
1386
1387 % Hints: get(hObject,'String') returns contents of repetition_edit as text
1388 %         str2double(get(hObject,'String')) returns contents of repetition_edit as
            a double
1389
1390 % Data input by user
1391 repetition_input = str2double(get(hObject,'string'));
1392
1393 if isfield(handles, 'plot_popup_value' )
1394     % handles.firing_popup_value exists - you may access it
1395 else
1396     % handles.firing_popup_value does not exist
1397     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
1398     uicontrol(hObject)
1399     return
```

```
1400 end
1401
1402 % If there is no repetition value or if it is bigger than 40kHz
1403 if isnan(repetition_input) || repetition_input > 40
1404     errordlg('You must enter a numeric value smaller or equal to 40kHz','Invalid
1405             Input','modal')
1406     uicontrol(hObject)
1407     return
1408 % resolution
1409 elseif rem(handles.time_resolution,repetition_input) ~= 0 && rem(repetition_input
1410             ,handles.time_resolution) ~= 0
1411     errordlg('Invalid input','Invalid Input','modal')
1412     uicontrol(hObject)
1413     return
1414 % If input is 0, waveform is build with no repetition
1415 elseif repetition_input == 0
1416     handles.interstimulus_time = 0;
1417     handles.n_repetitions = 1;
1418     value = handles.plot_popup_value;
1419     string = handles.plot_popup_string;
1420     switch string{value}
1421         case 'Bi-level Lilly' % User selects bilevel Lilly
1422             handles.current_data_I = handles.bi_level;
1423             handles.stimulation_data_I = handles.bi_level;
1424         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
1425             handles.current_data_I = handles.quasi_trap;
1426             handles.stimulation_data_I = handles.quasi_trap;
1427         case 'Tri-Exponential' % User selects tri-exponential
1428             handles.current_data_I = handles.tri_exp;
1429             handles.stimulation_data_I = handles.tri_exp;
1430         case 'Bursting' % User selects bursting strategies
1431             handles.current_data_I = handles.bursting;
1432             handles.stimulation_data_I = handles.bursting;
1433         case 'Rectangular' % User selects pulse
1434             handles.current_data_I = handles.pulse;
1435             handles.stimulation_data_I = handles.pulse;
1436         case 'Load Waveform'
1437             handles.current_data_I = handles.current_data_I;
1438             handles.stimulation_data_I = handles.current_data_I;
1439     end
1440     return
1441 % If interstimulus time is smaller than stimulation duration, no repetition
1442 % is made
1443 elseif ((1/(repetition_input)) > handles.fullstimulation_duration)
1444     warndlg('Repetition Cycle bigger than Stimulation Duration! No Repetition
1445             will be made.','Value Selection','modal');
1446     uicontrol(hObject)
```

```

1445     return
1446 % Else, build waveform with the calculated number of repetitions
1447 % The built waveform is just for the plot, since the MATLAB sense only
1448 % one pulse and the information on no of repetitions and interstimulus time
1449 else
1450     handles.repetition = repetition_input;
1451     value = handles.plot_popup_value;
1452     string = handles.plot_popup_string;
1453     n_reps = 1;
1454     handles.reps_max = 0;
1455     handles.interstimulus_time = 1/handles.repetition;
1456     handles.n_repetitions = (floor(handles.fullstimulation_duration/(handles.
stimulation_fulltime+handles.interstimulus_time))-1);
1457     switch string{value}
1458         case 'Bi-level Lilly' % User selects bilevel Lilly
1459             handles.current_data_I = handles.bi_level;
1460             handles.stimulation_data_I = handles.bi_level;
1461             for n_reps = 1:handles.n_repetitions
1462                 if (handles.amplitude_max ~=0 && handles.reps_max == 0 && (
handles.amplitude_max <= handles.amplitude_1*((handles.rep_amp_ratio).^(
n_reps+1)) || handles.amplitude_max <= handles.amplitude_2*((handles.
rep_amp_ratio).^(n_reps+1))))...
1463                     || (handles.amplitude_max ==0 && (handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) || handles.DAC_amplitude_limit <= handles.amplitude_2*((handles.
rep_amp_ratio).^(n_reps+1)) ) && handles.reps_max == 0)
1464                         handles.reps_max = n_reps;
1465                     end
1466                 if handles.reps_max ~=0
1467                     handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.bi_level);
1468                 else
1469                     handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.bi_level);
1470                 end
1471             end
1472         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
1473             handles.current_data_I = handles.quasi_trap;
1474             handles.stimulation_data_I = handles.quasi_trap;
1475             for n_reps = 1:handles.n_repetitions
1476                 if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
1477                     || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)

```

```

1478         handles.reps_max = n_reps;
1479     end
1480     if handles.reps_max ~=0
1481         handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.quasi_trap);
1482     else
1483         handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.quasi_trap);
1484     end
1485     end
1486     case 'Tri-Exponential' % User selects tri-exponential
1487         handles.current_data_I = handles.tri_exp;
1488         handles.stimulation_data_I = handles.tri_exp;
1489         for n_reps = 1:handles.n_repetitions
1490             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
1491                 || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
1492                 handles.reps_max = n_reps;
1493             end
1494             if handles.reps_max ~=0
1495                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.tri_exp);
1496             else
1497                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.tri_exp);
1498             end
1499         end
1500     case 'Bursting' % User selects bursting strategies
1501         handles.current_data_I = handles.bursting;
1502         handles.stimulation_data_I = handles.bursting;
1503         for n_reps = 1:handles.n_repetitions
1504             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
1505                 || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
1506                 handles.reps_max = n_reps;
1507             end
1508             if handles.reps_max ~=0

```

```

1509             handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.bursting);
1510         else
1511             handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(n_reps)).*handles.bursting);
1512         end
1513     end
1514     case 'Rectangular' % User selects pulse
1515         handles.current_data_I = handles.pulse;
1516         handles.stimulation_data_I = handles.pulse;
1517         for n_reps = 1:handles.n_repetitions
1518             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
1519                 || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
1520                 handles.reps_max = n_reps;
1521             end
1522             if handles.reps_max ~=0
1523                 handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.pulse);
1524             else
1525                 handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(n_reps)).*handles.pulse);
1526             end
1527         end
1528     case 'Load Waveform'
1529         handles.current_data_I = handles.current_data_I;
1530         handles.stimulation_data_I = handles.current_data_I;
1531         for n_reps = 1:handles.n_repetitions
1532             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= max(
handles.stimulation_data_I)*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
amplitude_max <= abs(min(handles.stimulation_data_I))*((handles.rep_amp_ratio
).^(n_reps+1))) && handles.reps_max == 0)...
1533                 || (handles.amplitude_max ==0 && (handles.
DAC_amplitude_limit <= max(handles.stimulation_data_I)*((handles.
rep_amp_ratio).^(n_reps+1)) || handles.DAC_amplitude_limit <= abs(min(handles
.stimulation_data_I))*((handles.rep_amp_ratio).^(n_reps+1))) && handles.
reps_max == 0)
1534                 handles.reps_max = n_reps;
1535             end
1536             if handles.reps_max ~=0

```



```
1537             handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(n_reps)).*handles.stimulation_data_I);
1538         else
1539             handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(n_reps)).*handles.stimulation_data_I);
1540         end
1541     end
1542 end
1543
1544
1545 end
1546
1547 guidata(hObject, handles);
1548
1549
1550 % --- Executes during object creation, after setting all properties.
1551 function repetition_edit_CreateFcn(hObject, eventdata, handles)
1552 % hObject    handle to repetition_edit (see GCBO)
1553 % eventdata  reserved - to be defined in a future version of MATLAB
1554 % handles    empty - handles not created until after all CreateFcns called
1555
1556 % Hint: edit controls usually have a white background on Windows.
1557 %         See ISPC and COMPUTER.
1558 if ispc && isequal(get(hObject, 'BackgroundColor'), get(0, '
defaultUicontrolBackgroundColor'))
1559     set(hObject, 'BackgroundColor', 'white');
1560 end
1561
1562
1563 function amplitude2_edit_Callback(hObject, eventdata, handles)
1564 % hObject    handle to amplitude2_edit (see GCBO)
1565 % eventdata  reserved - to be defined in a future version of MATLAB
1566 % handles    structure with handles and user data (see GUIDATA)
1567
1568 % Hints: get(hObject, 'String') returns contents of amplitude2_edit as text
1569 %         str2double(get(hObject, 'String')) returns contents of amplitude2_edit as
a double
1570
1571 % Data input by user
1572 amplitude_2_input = str2double(get(hObject, 'string'));
1573
1574 if isfield(handles, 'plot_popup_value' )
1575     % handles.firing_popup_value exists - you may access it
1576 else
1577     % handles.firing_popup_value does not exist
1578     errordlg('You must choose a Waverform Type!', 'Invalid Input', 'modal')
```

```

1579     uicontrol(hObject)
1580     return
1581 end
1582
1583 if isnan(amplitude_2_input)
1584     errordlg('You must enter a numeric value','Invalid Input','modal')
1585     uicontrol(hObject)
1586     return
1587 elseif handles.amplitude_max ~=0 && amplitude_2_input > handles.amplitude_max
1588     errordlg('That value breaches the Safe Limit Range','Invalid Input','modal')
1589     uicontrol(hObject)
1590     return
1591 elseif amplitude_2_input > 5
1592     errordlg('DACs higher output is 5V','Invalid Input','modal')
1593     uicontrol(hObject)
1594     return
1595 else
1596     handles.amplitude_2 = amplitude_2_input;
1597     value = handles.plot_popup_value;
1598     string = handles.plot_popup_string;
1599     switch string{value}
1600         case 'Bi-level Lilly' % User selects bilevel Lilly
1601             amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
amplitude_2*handles.duration_2)/handles.biphasic;
1602             handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.duration_2);
1603             handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
1604             handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1605             handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
1606                 (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
1607                 amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1608                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
1609                     -((handles.stimulation_fulltime)*handles.time_resolution)))]];
1610             handles.current_data_I = handles.bi_level;
1611             handles.stimulation_data_I = handles.bi_level;
1612         end
1613
1614     handles.reps_max = 0;
1615     if handles.repetition ~= 0
1616         for n_reps = 1:handles.n_repetitions

```

```

1617         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
1618             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
1619             handles.reps_max = n_reps;
1620         end
1621         if handles.reps_max ~=0
1622             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
1623         else
1624             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
1625         end
1626     end
1627 end
1628
1629 if handles.fullstimulation_duration < handles.stimulation_fulltime
1630     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
1631 end
1632
1633 end
1634
1635 guidata(hObject, handles);
1636
1637
1638 % --- Executes during object creation, after setting all properties.
1639 function amplitude2_edit_CreateFcn(hObject, eventdata, handles)
1640 % hObject    handle to amplitude2_edit (see GCBO)
1641 % eventdata  reserved - to be defined in a future version of MATLAB
1642 % handles    empty - handles not created until after all CreateFcns called
1643
1644 % Hint: edit controls usually have a white background on Windows.
1645 %         See ISPC and COMPUTER.
1646 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
1647     set(hObject,'BackgroundColor','white');
1648 end
1649
1650
1651
1652 function duration2_edit_Callback(hObject, eventdata, handles)

```

```
1653 % hObject    handle to duration2_edit (see GCBO)
1654 % eventdata  reserved - to be defined in a future version of MATLAB
1655 % handles     structure with handles and user data (see GUIDATA)
1656
1657 % Hints: get(hObject,'String') returns contents of duration2_edit as text
1658 %           str2double(get(hObject,'String')) returns contents of duration2_edit as
           a double
1659
1660 % Data input by user
1661 duration_2_input = str2double(get(hObject,'string'));
1662
1663 if isfield(handles, 'plot_popup_value' )
1664     % handles.firing_popup_value exists - you may access it
1665 else
1666     % handles.firing_popup_value does not exist
1667     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
1668     uicontrol(hObject)
1669     return
1670 end
1671
1672 if isnan(duration_2_input)
1673     errordlg('You must enter a numeric value','Invalid Input','modal')
1674     uicontrol(hObject)
1675     return
1676 elseif ((duration_2_input*handles.time_resolution) - floor(duration_2_input*
           handles.time_resolution)) ~= 0
1677     errordlg('Invalid input','Invalid Input','modal')
1678     uicontrol(hObject)
1679     return
1680 elseif length((0:(1/handles.time_resolution):(handles.duration_1+duration_2_input
           +(handles.biphasic*handles.duration_1)+(handles.biphasic*duration_2_input)+(
           handles.biphasic*handles.delay)+handles.delay+handles.decay))) > 930
1681     errordlg('The full duration of the pulse has to be smaller','Invalid Input','
           modal')
1682     uicontrol(hObject)
1683     return
1684 else
1685     handles.duration_2 = duration_2_input;
1686     handles.duration_balance_2 = handles.biphasic.*handles.duration_2;
1687     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
           duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
1688     handles.timescale = (0:(1/handles.time_resolution):(handles.
           stimulation_fulltime+handles.t_f));
1689     value = handles.plot_popup_value;
1690     string = handles.plot_popup_string;
1691     switch string{value}
1692         case 'Bi-level Lilly' % User selects bilevel Lilly
```

```

1693         amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
amplitude_2*handles.duration_2)/handles.biphasic;
1694         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.duration_2);
1695         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
1696         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1697         handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
1698         (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
1699         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1700         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
1701         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1702         handles.current_data_I = handles.bi_level;
1703         handles.stimulation_data_I = handles.bi_level;
1704     end
1705
1706     handles.reps_max = 0;
1707     if handles.repetition ~= 0
1708         for n_reps = 1:handles.n_repetitions
1709             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
1710             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
1711                 handles.reps_max = n_reps;
1712             end
1713             if handles.reps_max ~=0
1714                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
1715             else
1716                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
1717             end
1718         end
1719     end
1720
1721     if handles.fullstimulation_duration < handles.stimulation_fulltime

```

```
1722     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
        stimulation_fulltime)
1723     end
1724
1725 end
1726
1727 set(handles.stim_duration_edit, 'enable', 'on','String', handles.
        stimulation_fulltime)
1728
1729 guidata(hObject, handles);
1730
1731 % --- Executes during object creation, after setting all properties.
1732 function duration2_edit_CreateFcn(hObject, eventdata, handles)
1733 % hObject    handle to duration2_edit (see GCBO)
1734 % eventdata  reserved - to be defined in a future version of MATLAB
1735 % handles    empty - handles not created until after all CreateFcns called
1736
1737 % Hint: edit controls usually have a white background on Windows.
1738 %         See ISPC and COMPUTER.
1739 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
        defaultUicontrolBackgroundColor'))
1740     set(hObject,'BackgroundColor','white');
1741 end
1742
1743
1744
1745 function decay_edit_Callback(hObject, eventdata, handles)
1746 % hObject    handle to decay_edit (see GCBO)
1747 % eventdata  reserved - to be defined in a future version of MATLAB
1748 % handles    structure with handles and user data (see GUIDATA)
1749
1750 % Hints: get(hObject,'String') returns contents of decay_edit as text
1751 %         str2double(get(hObject,'String')) returns contents of decay_edit as a
        double
1752
1753 % Data input by user
1754 decay_input = str2double(get(hObject,'string'));
1755
1756 if isfield(handles, 'plot_popup_value' )
1757     % handles.firing_popup_value exists - you may access it
1758 else
1759     % handles.firing_popup_value does not exist
1760     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
1761     uicontrol(hObject)
1762     return
1763 end
1764
```

```

1765 if isnan(decay_input) || decay_input == 0 || rem(decay_input,handles.resolution)
      ~= 0
1766     errordlg('You must enter a numeric value bigger than 0 and remainder of
      division by Resolution is 0',...
1767             'Invalid Input','modal')
1768     uicontrol(hObject)
1769     return
1770 elseif length((0:(1/handles.time_resolution):(handles.duration_1+(handles.
      biphasic*(handles.duration_1+decay_input))+handles.delay+decay_input))) > 930
1771     errordlg('The full duration of the pulse has to be smaller','Invalid Input','
      modal')
1772     uicontrol(hObject)
1773     return
1774 else
1775     handles.decay = decay_input;
1776     handles.decay_steps = handles.decay/handles.resolution;
1777     handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
1778     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
      duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
1779     handles.timescale = (0:(1/handles.time_resolution):(handles.
      stimulation_fulltime+handles.t_f));
1780     value = handles.plot_popup_value;
1781     string = handles.plot_popup_string;
1782     switch string{value}
1783         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
1784             handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
      handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
1785             i=1;
1786             total_decay_amplitude = 0;
1787             for i=1:handles.decay_steps
1788                 handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
      amplitude_1*handles.q*...
1789                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
      .*...
1790                     ones(1,handles.resolution*handles.time_resolution));
1791                 total_decay_amplitude = total_decay_amplitude + (handles.
      amplitude_1*handles.q*...
1792                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
1793             end
1794             amplitude_CB = (handles.amplitude_1*handles.duration_1 +
      total_decay_amplitude*handles.resolution)/handles.biphasic;
1795             handles.duration_balance_total = handles.biphasic.*(handles.
      duration_1 + handles.decay);
1796             handles.stimulation_fulltime = handles.duration_1+handles.
      duration_balance_total+handles.delay+handles.decay;
1797             handles.timescale = (0:(1/handles.time_resolution):(handles.
      stimulation_fulltime+handles.t_f));

```

```

1798         handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
1799         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1800         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
1801         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1802         handles.current_data_I = handles.quasi_trap;
1803         handles.stimulation_data_I = handles.quasi_trap;
1804         case 'Tri-Exponential' % User selects tri-exponential
1805             handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
1806             j_i = 1;
1807             j_d = 1;
1808             total_increase_amplitude = 0;
1809             total_decay_amplitude = 0;
1810             for j_i=1:handles.increase_steps
1811                 handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
1812                 +((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
1813                 ones(1,handles.resolution*handles.time_resolution));
1814                 total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
1815                 -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
1816             end
1817             for j_d=1:handles.decay_steps
1818                 handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
1819                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
1820                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
1821                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
1822                 ones(1,handles.resolution*handles.time_resolution));
1823                 total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
1824                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
1825                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
1826                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
1827             end

```



```

1828         amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
1829         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
1830         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
1831         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1832         handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
1833         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1834         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
1835         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1836         handles.current_data_I = handles.tri_exp;
1837         handles.stimulation_data_I = handles.tri_exp;
1838     end
1839
1840     handles.reps_max = 0;
1841     if handles.repetition ~= 0
1842         for n_reps = 1:handles.n_repetitions
1843             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^n_reps+1)) && handles.
reps_max == 0)...
1844             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^n_reps
+1)) ) && handles.reps_max == 0)
1845                 handles.reps_max = n_reps;
1846             end
1847             if handles.reps_max ~=0
1848                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
1849             else
1850                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
1851             end
1852         end
1853     end
1854
1855     if handles.fullstimulation_duration < handles.stimulation_fulltime
1856         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
1857     end

```

```
1858
1859 end
1860
1861 set(handles.stim_duration_edit, 'enable', 'on','String', handles.
    stimulation_fulltime)
1862
1863 guidata(hObject, handles);
1864
1865 % --- Executes during object creation, after setting all properties.
1866 function decay_edit_CreateFcn(hObject, eventdata, handles)
1867 % hObject    handle to decay_edit (see GCBO)
1868 % eventdata  reserved - to be defined in a future version of MATLAB
1869 % handles    empty - handles not created until after all CreateFcns called
1870
1871 % Hint: edit controls usually have a white background on Windows.
1872 %         See ISPC and COMPUTER.
1873 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
    defaultUicontrolBackgroundColor'))
1874     set(hObject,'BackgroundColor','white');
1875 end
1876
1877
1878
1879 function resolution_edit_Callback(hObject, eventdata, handles)
1880 % hObject    handle to resolution_edit (see GCBO)
1881 % eventdata  reserved - to be defined in a future version of MATLAB
1882 % handles    structure with handles and user data (see GUIDATA)
1883
1884 % Hints: get(hObject,'String') returns contents of resolution_edit as text
1885 %         str2double(get(hObject,'String')) returns contents of resolution_edit as
    a double
1886
1887 % Data input by user
1888 resolution_input = str2double(get(hObject,'string'));
1889
1890 if isfield(handles, 'plot_popup_value' )
1891     % handles.firing_popup_value exists - you may access it
1892 else
1893     % handles.firing_popup_value does not exist
1894     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
1895     uicontrol(hObject)
1896     return
1897 end
1898
1899 if isnan(resolution_input) || resolution_input == 0 || rem(handles.decay,
    resolution_input) ~= 0 ||...
1900     ((resolution_input*handles.time_resolution) > 0 && (resolution_input*
    handles.time_resolution) < 1)
```

```

1901     errordlg('You must enter a numeric value between ]0,1], whos remainder of
dividing Decay is 0 and product by Time Resolution (40 by defenition) is an
integer',...
1902         'Invalid Input','modal')
1903     uicontrol(hObject)
1904     return
1905 else
1906     handles.resolution = resolution_input;
1907     handles.decay_steps = handles.decay/handles.resolution;
1908     handles.burst_steps = handles.duration_1/handles.resolution;
1909     handles.increase_steps = handles.duration_1/handles.resolution;
1910     handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
1911     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
1912     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1913     value = handles.plot_popup_value;
1914     string = handles.plot_popup_string;
1915     switch string{value}
1916         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
1917             handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
1918             i=1;
1919             total_decay_amplitude = 0;
1920             for i=1:handles.decay_steps
1921                 handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
1922                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
1923                     ones(1,handles.resolution*handles.time_resolution));
1924                 total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
1925                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
1926             end
1927             amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
1928             handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
1929             handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
1930             handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1931             handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
1932                 amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1933                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...

```

```

1934         -((handles.stimulation_fulltime)*handles.time_resolution))]);
1935     handles.current_data_I = handles.quasi_trap;
1936     handles.stimulation_data_I = handles.quasi_trap;
1937     case 'Tri-Exponential' % User selects tri-exponential
1938         handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
1939         j_i = 1;
1940         j_d = 1;
1941         total_increase_amplitude = 0;
1942         total_decay_amplitude = 0;
1943         for j_i=1:handles.increase_steps
1944             handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
1945                 +(-((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
1946                 ones(1,handles.resolution*handles.time_resolution));
1947             total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
1948                 -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
1949         end
1950         for j_d=1:handles.decay_steps
1951             handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
1952                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
1953                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
1954                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
1955                 ones(1,handles.resolution*handles.time_resolution));
1956             total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
1957                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
1958                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
1959                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
1960         end
1961         amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
1962         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
1963         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;

```

```

1964         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
1965         handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
1966             amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
1967             zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
1968                 -((handles.stimulation_fulltime)*handles.time_resolution))]);
1969         handles.current_data_I = handles.tri_exp;
1970         handles.stimulation_data_I = handles.tri_exp;
1971         case 'Bursting' % User selects bursting strategies
1972             if ((resolution_input/2)*handles.time_resolution) > 0 && ((
resolution_input/2)*handles.time_resolution) < 1)
1973                 errordlg('You must enter a numeric value whos division by 2
followed of multiplication by Time Resolution (100 by defenition) is an
integer',...
1974                     'Invalid Input','modal')
1975                 uicontrol(hObject)
1976                 return
1977             else
1978                 handles.duration_balance_1 = handles.biphasic.*(handles.
duration_1/2);
1979                 handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
1980                 k=1;
1981                 for k=1:handles.burst_steps
1982                     handles.bursting = horzcat(handles.bursting,[-handles.
amplitude_1.*...
1983                         ones(1,(handles.resolution/2)*handles.time_resolution)
...
1984                         zeros(1,(handles.resolution/2)*handles.time_resolution)]]
;
1985                 end
1986                 handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.
delay*handles.time_resolution))...
1987                     ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*
ones(1,handles.duration_balance_1*handles.time_resolution)...
1988                     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
1989                         -((handles.stimulation_fulltime)*handles.time_resolution))]]
;
1990                 handles.current_data_I = handles.bursting;
1991                 handles.stimulation_data_I = handles.bursting;
1992             end
1993         end
1994
1995         handles.reps_max = 0;
1996         if handles.repetition ~= 0

```

```

1997     for n_reps = 1:handles.n_repetitions
1998         if handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps)) ) && handles.reps_max
== 0
1999             handles.reps_max = n_reps;
2000         end
2001         if handles.reps_max ~=0
2002             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
2003         else
2004             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
2005         end
2006     end
2007 end
2008
2009 if handles.fullstimulation_duration < handles.stimulation_fulltime
2010     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2011 end
2012
2013 end
2014
2015 guidata(hObject, handles);
2016
2017 % --- Executes during object creation, after setting all properties.
2018 function resolution_edit_CreateFcn(hObject, eventdata, handles)
2019 % hObject    handle to resolution_edit (see GCBO)
2020 % eventdata  reserved - to be defined in a future version of MATLAB
2021 % handles    empty - handles not created until after all CreateFcns called
2022
2023 % Hint: edit controls usually have a white background on Windows.
2024 %         See ISPC and COMPUTER.
2025 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
2026     set(hObject,'BackgroundColor','white');
2027 end
2028
2029 % --- Executes on button press in plot_pushbutton.
2030 function plot_pushbutton_Callback(hObject, eventdata, handles)
2031 % hObject    handle to plot_pushbutton (see GCBO)
2032 % eventdata  reserved - to be defined in a future version of MATLAB
2033 % handles    structure with handles and user data (see GUIDATA)
2034
2035 % Display surf plot of the currently selected data

```

```

2036 handles.timescale = (0:(1/handles.time_resolution):(length(handles.current_data_I
    )-1)/handles.time_resolution);
2037 % handles.timescale = (0:(1/handles.time_resolution):(handles.
    stimulation_fulltime+handles.t_f));
2038 axes(handles.plot_axes);
2039 plot(handles.timescale,handles.current_data_I);
2040 if (min(handles.current_data_I)-0.1) > -(min(handles.current_data_I)-0.1)
2041     ylim([(min(handles.current_data_I)-0.1),(max(handles.current_data_I)-0.1)]);
2042 else
2043     ylim([(min(handles.current_data_I)-0.1),-(min(handles.current_data_I)-0.1)]);
2044 end
2045 xlim([0,((length(handles.current_data_I)-1)/handles.time_resolution)]);
2046 %xlim([0,((length(handles.current_data_I)-1)/handles.time_resolution)]);
2047 ylabel('Amplitude (V)');
2048 xlabel('Time (ms)');
2049
2050 length(handles.stimulation_data_I);
2051
2052 if length(handles.stimulation_data_I) > 930
2053     errordlg('An unknown error occurred. Probably related to length of pulse.
    Values in boxes were reseted. If problem pressists, change waveform once',...
2054         'Unknown Error','modal')
2055     switch handles.plot_popup_string{handles.plot_popup_value}
2056         case 'Rectangular' % User selects pulse wave
2057             % Define non interest variables to the original value
2058             handles.amplitude_1 = 1;
2059             handles.duration_1 = 1;
2060             handles.amplitude_2 = 0;
2061             handles.duration_2 = 0;
2062             handles.biphasic = 10;
2063             handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
2064             handles.duration_balance_2 = 0;
2065             handles.decay = 0;
2066             handles.delay = 1;
2067             handles.resolution = 0.25;
2068             handles.repetition = 0;
2069             handles.rep_amp_ratio = 1;
2070             handles.stimulation_fulltime = handles.duration_1+handles.duration_2+
handles.duration_balance_1+handles.duration_balance_2+handles.delay+handles.
decay;
2071             handles.fullstimulation_duration = handles.stimulation_fulltime;
2072             handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2073             %Building the pulse wave
2074             handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
2075                 zeros(1,(handles.delay*handles.time_resolution))...

```

```

2076         ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
2077         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution)...
2078         -((handles.stimulation_fulltime)*handles.time_resolution))];
2079     %
2080     handles.current_data_I = handles.pulse;
2081     handles.stimulation_data_I = handles.pulse;
2082     % Define with edit fields should work and define its initial values
2083     set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2084     set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2085     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2086     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2087     set(handles.amplitude2_edit, 'enable', 'off')
2088     set(handles.duration2_edit, 'enable', 'off')
2089     set(handles.decay_edit, 'enable', 'off')
2090     set(handles.resolution_edit, 'enable', 'off')
2091     set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2092     set(handles.Q_exp_edit, 'enable', 'off')
2093     set(handles.Q2_exp_edit, 'enable', 'off')
2094     set(handles.A_exp_edit, 'enable', 'off')
2095     set(handles.A2_exp_edit, 'enable', 'off')
2096     set(handles.B_exp_edit, 'enable', 'off')
2097     set(handles.B2_exp_edit, 'enable', 'off')
2098     set(handles.C_exp_edit, 'enable', 'off')
2099     set(handles.C2_exp_edit, 'enable', 'off')
2100     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2101     set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2102
2103     case 'Bi-level Lilly' % User selects bilevel Lilly
2104         handles.amplitude_1 = 1;
2105         handles.duration_1 = 1;
2106         handles.amplitude_2 = 0.5;
2107         handles.duration_2 = 1;
2108         handles.biphasic = 10;
2109         handles.delay = 1;
2110         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
2111         handles.duration_balance_2 = handles.biphasic.*handles.duration_2;
2112         handles.decay = 0;
2113         handles.resolution = 0.25;
2114         handles.repetition = 0;
2115         handles.rep_amp_ratio = 1;
2116         % Building the Bilevel Lilly

```



```

2117         amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
amplitude_2*handles.duration_2)/handles.biphasic;
2118         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.duration_2);
2119         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
2120         handles.fullstimulation_duration = handles.stimulation_fulltime;
2121         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2122         handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
2123         (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
2124         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
2125         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...
2126         -((handles.stimulation_fulltime)*handles.time_resolution)]];
2127         %
2128         handles.current_data_I = handles.bi_level;
2129         handles.stimulation_data_I = handles.bi_level;
2130         set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2131         set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2132         set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2133         set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2134         set(handles.amplitude2_edit, 'enable', 'on','String', handles.
amplitude_2)
2135         set(handles.duration2_edit, 'enable', 'on','String', handles.
duration_2 )
2136         set(handles.decay_edit, 'enable', 'off')
2137         set(handles.resolution_edit, 'enable', 'off')
2138         set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2139         set(handles.Q_exp_edit, 'enable', 'off')
2140         set(handles.Q2_exp_edit, 'enable', 'off')
2141         set(handles.A_exp_edit, 'enable', 'off')
2142         set(handles.A2_exp_edit, 'enable', 'off')
2143         set(handles.B_exp_edit, 'enable', 'off')
2144         set(handles.B2_exp_edit, 'enable', 'off')
2145         set(handles.C_exp_edit, 'enable', 'off')
2146         set(handles.C2_exp_edit, 'enable', 'off')
2147         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2148         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2149

```

```

2150     case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
2151         handles.amplitude_1 = 1;
2152         handles.duration_1 = 1;
2153         handles.amplitude_2 = 0.5;
2154         handles.duration_2 = 1;
2155         handles.biphasic = 10;
2156         handles.delay = 1;
2157         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
2158         handles.duration_balance_2 = 0;
2159         handles.decay = 1;
2160         handles.resolution = 0.25;
2161         handles.repetition = 0;
2162         handles.q = 1;
2163         handles.q2 = 2.1972e+03;
2164         handles.rep_amp_ratio = 1;
2165         % Building the Quasi-Trapezoidal Wave
2166         handles.decay_steps = handles.decay/handles.resolution;
2167         handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
2168         i=1;
2169         total_decay_amplitude = 0;
2170         for i=1:handles.decay_steps
2171             handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
2172                 exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
2173                 ones(1,handles.resolution*handles.time_resolution));
2174             total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
2175                 exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
2176         end
2177         amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
2178         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
2179         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
2180         handles.fullstimulation_duration = handles.stimulation_fulltime;
2181         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2182         handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
2183             amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
2184             zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...
2185             -((handles.stimulation_fulltime)*handles.time_resolution)]];
2186         %

```

```
2187         handles.current_data_I = handles.quasi_trap;
2188         handles.stimulation_data_I = handles.quasi_trap;
2189         set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2190         set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2191         set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2192         set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2193         set(handles.amplitude2_edit, 'enable', 'off')
2194         set(handles.duration2_edit, 'enable', 'off')
2195         set(handles.decay_edit, 'enable', 'on','String', handles.decay)
2196         set(handles.resolution_edit, 'enable', 'on','String', handles.
resolution)
2197         set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2198         set(handles.Q_exp_edit, 'enable', 'on','String', handles.q)
2199         set(handles.Q2_exp_edit, 'enable', 'on', 'String', handles.q2)
2200         set(handles.A_exp_edit, 'enable', 'off')
2201         set(handles.A2_exp_edit, 'enable', 'off')
2202         set(handles.B_exp_edit, 'enable', 'off')
2203         set(handles.B2_exp_edit, 'enable', 'off')
2204         set(handles.C_exp_edit, 'enable', 'off')
2205         set(handles.C2_exp_edit, 'enable', 'off')
2206         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2207         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2208
2209     case 'Tri-Exponential' % User selects tri-exponential
2210         handles.amplitude_1 = 1;
2211         handles.duration_1 = 1;
2212         handles.amplitude_2 = 0.5;
2213         handles.duration_2 = 1;
2214         handles.biphasic = 10;
2215         handles.delay = 1;
2216         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
2217         handles.duration_balance_2 = 0;
2218         handles.decay = 1;
2219         handles.repetition = 0;
2220         handles.resolution = 0.25;
2221         handles.a = 0.2;
2222         handles.a2 = 1.197e+03;
2223         handles.b = 0.3;
2224         handles.b2 = 2.197e+03;
2225         handles.c = 0.5;
2226         handles.c2 = 3.197e+03;
2227         handles.repetition = 0;
2228         handles.rep_amp_ratio = 1;
```

```

2229         % Building the Tri-Exponential Wave
2230         handles.increase_steps = handles.duration_1/handles.resolution;
2231         handles.decay_steps = handles.decay/handles.resolution;
2232         handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
2233         j_i = 1;
2234         j_d = 1;
2235         total_increase_amplitude = 0;
2236         total_decay_amplitude = 0;
2237         for j_i=1:handles.increase_steps
2238             handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
2239                 +((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
2240                 ones(1,handles.resolution*handles.time_resolution));
2241             total_increase_amplitude = total_increase_amplitude + (((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
2242                 -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
2243         end
2244         for j_d=1:handles.decay_steps
2245             handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
2246                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
2247                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
2248                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
2249                 ones(1,handles.resolution*handles.time_resolution));
2250             total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
2251                 exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
2252                 exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
2253                 exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
2254         end
2255         amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
2256         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
2257         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
2258         handles.fullstimulation_duration = handles.stimulation_fulltime;

```

```

2259         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2260         handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
2261             amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
2262             zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution)...
2263             -((handles.stimulation_fulltime)*handles.time_resolution))]);
2264         %
2265         handles.current_data_I = handles.tri_exp;
2266         handles.stimulation_data_I = handles.tri_exp;
2267         set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2268         set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2269         set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2270         set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2271         set(handles.amplitude2_edit, 'enable', 'off')
2272         set(handles.duration2_edit, 'enable', 'off')
2273         set(handles.decay_edit, 'enable', 'on','String', handles.decay)
2274         set(handles.resolution_edit, 'enable', 'on','String', handles.
resolution)
2275         set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2276         set(handles.Q_exp_edit, 'enable', 'off')
2277         set(handles.Q2_exp_edit, 'enable', 'off')
2278         set(handles.A_exp_edit, 'enable', 'on','String', handles.a)
2279         set(handles.A2_exp_edit, 'enable', 'on', 'String', handles.a2)
2280         set(handles.B_exp_edit, 'enable', 'on','String', handles.b)
2281         set(handles.B2_exp_edit, 'enable', 'on', 'String', handles.b2)
2282         set(handles.C_exp_edit, 'enable', 'on','String', handles.c)
2283         set(handles.C2_exp_edit, 'enable', 'on', 'String', handles.c2)
2284         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2285         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2286
2287     case 'Bursting' % User selects bursting strategies
2288         handles.amplitude_1 = 1;
2289         handles.duration_1 = 1;
2290         handles.amplitude_2 = 0.5;
2291         handles.duration_2 = 1;
2292         handles.biphasic = 10;
2293         handles.delay = 1;
2294         handles.duration_balance_2 = 0;
2295         handles.decay = 0;

```

```

2296         handles.duration_balance_1 = handles.biphasic.*(handles.duration_1/2)
;
2297         handles.resolution = 0.25;
2298         handles.repetition = 0;
2299         handles.rep_amp_ratio = 1;
2300         handles.stimulation_fulltime = handles.duration_1+handles.duration_2+
handles.duration_balance_1+handles.duration_balance_2+handles.delay+handles.
decay;
2301         handles.fullstimulation_duration = handles.stimulation_fulltime;
2302         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2303         % Building the Bursting Wave
2304         handles.burst_steps = handles.duration_1/handles.resolution;
2305         handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
2306         k=1;
2307         for k=1:handles.burst_steps
2308             handles.bursting = horzcat(handles.bursting,[-handles.amplitude_1
.*...
2309                 ones(1,(handles.resolution/2)*handles.time_resolution) ...
2310                 zeros(1,(handles.resolution/2)*handles.time_resolution)]);
2311         end
2312         handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*
handles.time_resolution))...
2313             ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
2314             zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution)...
2315             -((handles.stimulation_fulltime)*handles.time_resolution))]);
2316         %
2317         handles.current_data_I = handles.bursting;
2318         handles.stimulation_data_I = handles.bursting;
2319         set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2320         set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2321         set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2322         set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2323         set(handles.amplitude2_edit, 'enable', 'off')
2324         set(handles.duration2_edit, 'enable', 'off')
2325         set(handles.decay_edit, 'enable', 'off')
2326         set(handles.resolution_edit, 'enable', 'on','String', handles.
resolution)
2327         set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2328         set(handles.Q_exp_edit, 'enable', 'off')
2329         set(handles.Q2_exp_edit, 'enable', 'off')
2330         set(handles.A_exp_edit, 'enable', 'off')
2331         set(handles.A2_exp_edit, 'enable', 'off')

```

```
2332         set(handles.B_exp_edit, 'enable', 'off')
2333         set(handles.B2_exp_edit, 'enable', 'off')
2334         set(handles.C_exp_edit, 'enable', 'off')
2335         set(handles.C2_exp_edit, 'enable', 'off')
2336         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2337         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2338         uicontrol(hObject)
2339         return
2340     end
2341 end
2342
2343
2344
2345
2346
2347
2348
2349 % --- Executes on button press in upload_pushbutton.
2350 function upload_pushbutton_Callback(hObject, eventdata, handles)
2351 % hObject    handle to upload_pushbutton (see GCBO)
2352 % eventdata  reserved - to be defined in a future version of MATLAB
2353 % handles    structure with handles and user data (see GUIDATA)
2354
2355 if isfield(handles, 'plot_popup_value' )
2356     % handles.plot_popup_value exists - you may access it
2357 else
2358     % handles.plot_popup_value does not exist returns to interface without
2359     % any action
2360     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
2361     uicontrol(hObject)
2362     return
2363 end
2364
2365 if isfield(handles, 'firing_popup_value' )
2366     % handles.firing_popup_value exists - you may access it
2367 else
2368     % handles.firing_popup_value does not exist returns to interface without
2369     % any action
2370     errordlg('You must choose a Firing Type!','Invalid Input','modal')
2371     uicontrol(hObject)
2372     return
2373 end
2374
2375 if isfield(handles, 'channel_popup_value' )
2376     % handles.channel_popup_value exists - you may access it
2377 else
```

```
2378     % handles.channel_popup_value does not exist returns to interface without
2379     % any action
2380     errordlg('You must choose a Channel!','Invalid Input','modal')
2381     uicontrol(hObject)
2382     return
2383 end
2384
2385 if isfield(handles, 'COM_popup_value' )
2386     % handles.COM_popup_value exists - you may access it
2387 else
2388     % handles.COM_popup_value does not exist
2389     errordlg('No COM port selected!','Invalid Input','modal')
2390     % searches for new COM ports
2391     serialInfo = instrhwinfo('serial');
2392     % if there are no ports returns to interface without
2393     % any action
2394     if isempty(serialInfo.SerialPorts) == 1
2395         errordlg('There are no available COM ports','Invalid Input','modal')
2396         uicontrol(hObject)
2397         return
2398     else % if there is ports, makes them available to user choice and also
2399         % returns to interface with no action
2400         n_coms = 1;
2401         for n_coms = 1:length(serialInfo.SerialPorts)
2402             string_list(n_coms+1) = serialInfo.SerialPorts(n_coms);
2403         end
2404         set(handles.COM_popup,'String',string_list);
2405     end
2406
2407     uicontrol(hObject)
2408     return
2409 end
2410
2411 % if, for some reason, the control of length as failed throughout the
2412 % interface, this is a last control point. If is bigger than the maximum
2413 % length allowed, resets all options
2414 if length(handles.stimulation_data_I) > 930
2415     errordlg('An unknown error occurred. Values in boxes were reseted.','Unknown
2416     Error','modal')
2417     switch handles.plot_popup_string{handles.plot_popup_value}
2418     case 'Rectangular' % User selects pulse wave
2419         % Define non interest variables to the original value
2420         handles.amplitude_1 = 1;
2421         handles.duration_1 = 1;
2422         handles.amplitude_2 = 0;
2423         handles.duration_2 = 0;
2424         handles.biphasic = 10;
2425         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
```



```

2425         handles.duration_balance_2 = 0;
2426         handles.decay = 0;
2427         handles.delay = 1;
2428         handles.resolution = 0.25;
2429         handles.repetition = 0;
2430         handles.rep_amp_ratio = 1;
2431         handles.stimulation_fulltime = handles.duration_1+handles.duration_2+
handles.duration_balance_1+handles.duration_balance_2+handles.delay+handles.
decay;
2432         handles.fullstimulation_duration = handles.stimulation_fulltime;
2433         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2434         %Building the pulse wave
2435         handles.pulse = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
2436             zeros(1,(handles.delay*handles.time_resolution))...
2437             ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
2438             zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...
2439             -((handles.stimulation_fulltime)*handles.time_resolution)]];
2440         %
2441         handles.current_data_I = handles.pulse;
2442         handles.stimulation_data_I = handles.pulse;
2443         % Define with edit fields should work and define its initial values
2444         set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2445         set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2446         set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2447         set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2448         set(handles.amplitude2_edit, 'enable', 'off')
2449         set(handles.duration2_edit, 'enable', 'off')
2450         set(handles.decay_edit, 'enable', 'off')
2451         set(handles.resolution_edit, 'enable', 'off')
2452         set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2453         set(handles.Q_exp_edit, 'enable', 'off')
2454         set(handles.Q2_exp_edit, 'enable', 'off')
2455         set(handles.A_exp_edit, 'enable', 'off')
2456         set(handles.A2_exp_edit, 'enable', 'off')
2457         set(handles.B_exp_edit, 'enable', 'off')
2458         set(handles.B2_exp_edit, 'enable', 'off')
2459         set(handles.C_exp_edit, 'enable', 'off')
2460         set(handles.C2_exp_edit, 'enable', 'off')
2461         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)

```

```

2462         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2463
2464     case 'Bi-level Lilly' % User selects bilevel Lilly
2465         handles.amplitude_1 = 1;
2466         handles.duration_1 = 1;
2467         handles.amplitude_2 = 0.5;
2468         handles.duration_2 = 1;
2469         handles.biphasic = 10;
2470         handles.delay = 1;
2471         handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
2472         handles.duration_balance_2 = handles.biphasic.*handles.duration_2;
2473         handles.decay = 0;
2474         handles.resolution = 0.25;
2475         handles.repetition = 0;
2476         handles.rep_amp_ratio = 1;
2477         % Building the Bilevel Lilly
2478         amplitude_CB = (handles.amplitude_1*handles.duration_1 + handles.
amplitude_2*handles.duration_2)/handles.biphasic;
2479         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.duration_2);
2480         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
2481         handles.fullstimulation_duration = handles.stimulation_fulltime;
2482         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2483         handles.bi_level = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)...
2484         (-handles.amplitude_2).*ones(1,handles.duration_2*handles.
time_resolution) zeros(1,(handles.delay*handles.time_resolution))...
2485         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
2486         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...
2487         -((handles.stimulation_fulltime)*handles.time_resolution)]];
2488     %
2489     handles.current_data_I = handles.bi_level;
2490     handles.stimulation_data_I = handles.bi_level;
2491     set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2492     set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2493     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2494     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2495     set(handles.amplitude2_edit, 'enable', 'on','String', handles.
amplitude_2)
2496     set(handles.duration2_edit, 'enable', 'on','String', handles.
duration_2 )

```

```

2497         set(handles.decay_edit, 'enable', 'off')
2498         set(handles.resolution_edit, 'enable', 'off')
2499         set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2500         set(handles.Q_exp_edit, 'enable', 'off')
2501         set(handles.Q2_exp_edit, 'enable', 'off')
2502         set(handles.A_exp_edit, 'enable', 'off')
2503         set(handles.A2_exp_edit, 'enable', 'off')
2504         set(handles.B_exp_edit, 'enable', 'off')
2505         set(handles.B2_exp_edit, 'enable', 'off')
2506         set(handles.C_exp_edit, 'enable', 'off')
2507         set(handles.C2_exp_edit, 'enable', 'off')
2508         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2509         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2510
2511         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
2512             handles.amplitude_1 = 1;
2513             handles.duration_1 = 1;
2514             handles.amplitude_2 = 0.5;
2515             handles.duration_2 = 1;
2516             handles.biphasic = 10;
2517             handles.delay = 1;
2518             handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
2519             handles.duration_balance_2 = 0;
2520             handles.decay = 1;
2521             handles.repetition = 0;
2522             handles.q = 1;
2523             handles.q2 = 2.1972e+03;
2524             handles.rep_amp_ratio = 1;
2525             % Building the Quasi-Trapezoidal Wave
2526             handles.decay_steps = handles.decay/handles.resolution;
2527             handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
2528             i=1;
2529             total_decay_amplitude = 0;
2530             for i=1:handles.decay_steps
2531                 handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
2532                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
2533                     ones(1,handles.resolution*handles.time_resolution));
2534                 total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
2535                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
2536             end

```

```

2537         amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
2538         handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
2539         handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
2540         handles.fullstimulation_duration = handles.stimulation_fulltime;
2541         handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2542         handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
2543         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
2544         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...
2545         -((handles.stimulation_fulltime)*handles.time_resolution)]];
2546         %
2547         handles.current_data_I = handles.quasi_trap;
2548         handles.stimulation_data_I = handles.quasi_trap;
2549         set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2550         set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2551         set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2552         set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2553         set(handles.amplitude2_edit, 'enable', 'off')
2554         set(handles.duration2_edit, 'enable', 'off')
2555         set(handles.decay_edit, 'enable', 'on','String', handles.decay)
2556         set(handles.resolution_edit, 'enable', 'on','String', handles.
resolution)
2557         set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2558         set(handles.Q_exp_edit, 'enable', 'on','String', handles.q)
2559         set(handles.Q2_exp_edit, 'enable', 'on', 'String', handles.q2)
2560         set(handles.A_exp_edit, 'enable', 'off')
2561         set(handles.A2_exp_edit, 'enable', 'off')
2562         set(handles.B_exp_edit, 'enable', 'off')
2563         set(handles.B2_exp_edit, 'enable', 'off')
2564         set(handles.C_exp_edit, 'enable', 'off')
2565         set(handles.C2_exp_edit, 'enable', 'off')
2566         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
2567         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.
rep_amp_ratio)
2568
2569         case 'Tri-Exponential' % User selects tri-exponential
2570             handles.amplitude_1 = 1;
2571             handles.duration_1 = 1;

```

```

2572     handles.amplitude_2 = 0.5;
2573     handles.duration_2 = 1;
2574     handles.biphasic = 10;
2575     handles.delay = 1;
2576     handles.duration_balance_1 = handles.biphasic.*handles.duration_1;
2577     handles.duration_balance_2 = 0;
2578     handles.decay = 1;
2579     handles.repetition = 0;
2580     handles.resolution = 0.25;
2581     handles.a = 0.2;
2582     handles.a2 = 1.197e+03;
2583     handles.b = 0.3;
2584     handles.b2 = 2.197e+03;
2585     handles.c = 0.5;
2586     handles.c2 = 3.197e+03;
2587     handles.repetition = 0;
2588     handles.rep_amp_ratio = 1;
2589     % Building the Tri-Exponential Wave
2590     handles.increase_steps = handles.duration_1/handles.resolution;
2591     handles.decay_steps = handles.decay/handles.resolution;
2592     handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
2593     j_i = 1;
2594     j_d = 1;
2595     total_increase_amplitude = 0;
2596     total_decay_amplitude = 0;
2597     for j_i=1:handles.increase_steps
2598         handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution)...
2599             +((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
2600             ones(1,handles.resolution*handles.time_resolution));
2601         total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
2602             -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
2603     end
2604     for j_d=1:handles.decay_steps
2605         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
2606             exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
2607             exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
2608             exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
2609         ones(1,handles.resolution*handles.time_resolution));

```

```

2610         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
2611             exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
2612             exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
2613             exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
2614     end
2615     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
2616     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
2617     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
2618     handles.fullstimulation_duration = handles.stimulation_fulltime;
2619     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2620     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
2621         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
2622         zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution))...
2623         -((handles.stimulation_fulltime)*handles.time_resolution)]];
2624     %
2625     handles.current_data_I = handles.tri_exp;
2626     handles.stimulation_data_I = handles.tri_exp;
2627     set(handles.amplitude1_edit, 'enable', 'on','String', handles.
amplitude_1)
2628     set(handles.duration1_edit, 'enable', 'on','String', handles.
duration_1)
2629     set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)
2630     set(handles.delay_edit, 'enable', 'on','String', handles.delay)
2631     set(handles.amplitude2_edit, 'enable', 'off')
2632     set(handles.duration2_edit, 'enable', 'off')
2633     set(handles.decay_edit, 'enable', 'on','String', handles.decay)
2634     set(handles.resolution_edit, 'enable', 'on','String', handles.
resolution)
2635     set(handles.repetition_edit, 'enable', 'on','String', handles.
repetition)
2636     set(handles.Q_exp_edit, 'enable', 'off')
2637     set(handles.Q2_exp_edit, 'enable', 'off')
2638     set(handles.A_exp_edit, 'enable', 'on','String', handles.a)
2639     set(handles.A2_exp_edit, 'enable', 'on', 'String', handles.a2)
2640     set(handles.B_exp_edit, 'enable', 'on','String', handles.b)
2641     set(handles.B2_exp_edit, 'enable', 'on', 'String', handles.b2)
2642     set(handles.C_exp_edit, 'enable', 'on','String', handles.c)

```

```

2643         set(handles.C2_exp_edit, 'enable', 'on', 'String', handles.c2)
2644         set(handles.stim_duration_edit, 'enable', 'on', 'String', handles.
stimulation_fulltime)
2645         set(handles.rep_amp_ratio_edit, 'enable', 'on', 'String', handles.
rep_amp_ratio)
2646
2647         case 'Bursting' % User selects bursting strategies
2648             handles.amplitude_1 = 1;
2649             handles.duration_1 = 1;
2650             handles.amplitude_2 = 0.5;
2651             handles.duration_2 = 1;
2652             handles.biphasic = 10;
2653             handles.delay = 1;
2654             handles.duration_balance_2 = 0;
2655             handles.decay = 0;
2656             handles.duration_balance_1 = handles.biphasic.*(handles.duration_1/2)
;
2657             handles.resolution = 0.25;
2658             handles.repetition = 0;
2659             handles.rep_amp_ratio = 1;
2660             handles.stimulation_fulltime = handles.duration_1+handles.duration_2+
handles.duration_balance_1+handles.duration_balance_2+handles.delay+handles.
decay;
2661             handles.fullstimulation_duration = handles.stimulation_fulltime;
2662             handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2663             % Building the Bursting Wave
2664             handles.burst_steps = handles.duration_1/handles.resolution;
2665             handles.bursting = zeros(1,handles.t_i*handles.time_resolution);
2666             k=1;
2667             for k=1:handles.burst_steps
2668                 handles.bursting = horzcat(handles.bursting, [-handles.amplitude_1
.*...
2669                     ones(1,(handles.resolution/2)*handles.time_resolution) ...
2670                     zeros(1,(handles.resolution/2)*handles.time_resolution)]);
2671             end
2672             handles.bursting = horzcat(handles.bursting, [zeros(1,(handles.delay*
handles.time_resolution))...
2673                 ((handles.amplitude_1*handles.duration_1)/handles.biphasic).*ones
(1,handles.duration_balance_1*handles.time_resolution)...
2674                 zeros(1,(length(handles.timescale)-handles.t_i*handles.
time_resolution)...
2675                 -((handles.stimulation_fulltime)*handles.time_resolution))]);
2676             %
2677             handles.current_data_I = handles.bursting;
2678             handles.stimulation_data_I = handles.bursting;
2679             set(handles.amplitude1_edit, 'enable', 'on', 'String', handles.
amplitude_1)

```

```
2680         set(handles.duration1_edit, 'enable', 'on','String', handles.  
duration_1)  
2681         set(handles.biphasic_edit, 'enable', 'on','String', handles.biphasic)  
2682         set(handles.delay_edit, 'enable', 'on','String', handles.delay)  
2683         set(handles.amplitude2_edit, 'enable', 'off')  
2684         set(handles.duration2_edit, 'enable', 'off')  
2685         set(handles.decay_edit, 'enable', 'off')  
2686         set(handles.resolution_edit, 'enable', 'on','String', handles.  
resolution)  
2687         set(handles.repetition_edit, 'enable', 'on','String', handles.  
repetition)  
2688         set(handles.Q_exp_edit, 'enable', 'off')  
2689         set(handles.Q2_exp_edit, 'enable', 'off')  
2690         set(handles.A_exp_edit, 'enable', 'off')  
2691         set(handles.A2_exp_edit, 'enable', 'off')  
2692         set(handles.B_exp_edit, 'enable', 'off')  
2693         set(handles.B2_exp_edit, 'enable', 'off')  
2694         set(handles.C_exp_edit, 'enable', 'off')  
2695         set(handles.C2_exp_edit, 'enable', 'off')  
2696         set(handles.stim_duration_edit, 'enable', 'on','String', handles.  
stimulation_fulltime)  
2697         set(handles.rep_amp_ratio_edit, 'enable', 'on','String', handles.  
rep_amp_ratio)  
2698         uicontrol(hObject)  
2699         return  
2700     end  
2701 end  
2702  
2703  
2704 % Attempt Communication with Microcontroller  
2705 priorPorts = instrfind; % finds any existing Serial Ports in MATLAB  
2706 delete(priorPorts) % and deletes them  
2707  
2708 % Define Serial Port has the one chosen by user in COM pop up  
2709 s = serial(handles.COM_popup_string{handles.COM_popup_value});  
2710  
2711 % s = serial('COM6'); %assigns the object s to serial port  
2712  
2713 % Definitions of Serial Communication  
2714 set(s, 'InputBufferSize', 1);  
2715 set(s, 'FlowControl', 'none');  
2716 set(s, 'BaudRate', 38400);  
2717 set(s, 'Parity', 'none');  
2718 set(s, 'DataBits', 8);  
2719 set(s, 'StopBit', 1);  
2720 set(s, 'Timeout', 100);  
2721 %clc;  
2722
```



```
2723 % Display of the above definitons in Command Window
2724 % disp(get(s,'Name'));
2725 % prop(1)=(get(s,'BaudRate'));
2726 % prop(2)=(get(s,'DataBits'));
2727 % prop(3)=(get(s, 'StopBit'));
2728 % prop(4)=(get(s, 'InputBufferSize'));
2729 % disp([num2str(prop)]);
2730
2731 % newobjs = instrfind
2732
2733 % tries to open serial port
2734 try
2735     fopen(s);
2736 catch err % if some error occurs while trying to open serial port
2737     errordlg('Something went wrong with the connection. Maybe another program
2738             using the device? If not, try re-connect the device',...
2739             'Invalid Input','modal')
2740     uicontrol(hObject)
2741     return
2742 end
2743
2744 % Firing Type Sending
2745 send_firing_type = handles.firing_type;
2746 % if user is programming another channel when Alone option is selected and
2747 % has not yet applied the previous programmed stimulation
2748 if send_firing_type == 1 && isempty(find(handles.old_channel == handles.
2749     channel_no , 1)) == 1 && handles.number_sent_channels > 1
2750     final_answer = questdlg('You are changing the channel to use alone. Are you
2751     sure?','Firing Channel','Yes','No','No');
2752     switch final_answer
2753     case 'Yes'
2754         fprintf(s, '%d\r', -13) % -13 is the value chosen to control Firing
2755         Type in mcu
2756         pause(0.02);
2757         fprintf(s, '%d\r', send_firing_type) % sends the Firing Type
2758         corresponding number
2759         pause(0.02);
2760     case 'No'
2761         return
2762     end
2763 % if user is changing the firing type after already uploading a different
2764 % firing type but has not applied it yet
2765 elseif send_firing_type ~= handles.old_firing && (handles.old_firing == 1 ||
2766     handles.old_firing == 2 || handles.old_firing == 3)
```

```
2763     final_answer = questdlg('You are changing the firing type from the
    definitions already uploaded without applying any stimulus. Are you sure?','
    Firing Channel','Yes','No','No');
2764     switch final_answer
2765         case 'Yes'
2766             fprintf(s, '%d\r', -13) % -13 is the value chosen to control Firing
    Type in mcu
2767             pause(0.02);
2768             fprintf(s, '%d\r', send_firing_type) % sends the Firing Type
    corresponding number
2769             pause(0.02);
2770         case 'No'
2771             return
2772     end
2773 else
2774     fprintf(s, '%d\r', -13) % -13 is the value chosen to control repetition
    amplitude ratio in mcu
2775     pause(0.02);
2776     fprintf(s, '%d\r', send_firing_type) % sends the Firing Type corresponding
    number
2777     pause(0.02);
2778     % to remember the used firing type
2779     handles.old_firing = send_firing_type;
2780 end
2781
2782
2783 % Channel Sending
2784 send_channel = handles.channel_no;
2785 % if user is uploading values for the same channel before applying the one
2786 % previously uploaded
2787 if isempty(find(handles.old_channel == send_channel , 1)) == 0
2788     final_answer = questdlg('You are reprogramming a channel. Are you sure?','
    Channel','Yes','No','No');
2789     switch final_answer
2790         case 'Yes'
2791             fprintf(s, '%d\r', -7) % -7 is the value chosen to control channel in
    mcu
2792             pause(0.02);
2793             fprintf(s, '%d\r', send_channel) % sends the channel number
2794             pause(0.02);
2795         case 'No'
2796             return
2797     end
2798 else
2799     fprintf(s, '%d\r', -7) % -7 is the value chosen to control channel in mcu
2800     pause(0.02);
2801     fprintf(s, '%d\r', send_channel) % sends the channel number
2802     pause(0.02);
```

```
2803     % to remember the previous channel and know how many channels were
2804     % programmed
2805     handles.old_channel(handles.number_sent_channels) = send_channel;
2806     handles.number_sent_channels = handles.number_sent_channels + 1;
2807 end
2808
2809
2810 h = waitbar(0,'Uploading... Closing this window or canceling will reset uploaded
      values and may crash the program!','CreateCancelBtn',...
2811     'setappdata(gcf,'canceling',1)');
2812 setappdata(h,'canceling',0);
2813
2814
2815
2816 handles.timescale = (0:(1/handles.time_resolution):(length(handles.current_data_I
      )-1)/handles.time_resolution);
2817 handles.timescale_stimulation = (0:(1/handles.time_resolution):(length(handles.
      stimulation_data_I)-1)/handles.time_resolution);
2818
2819 length(handles.stimulation_data_I);
2820
2821 u = handles.stimulation_data_I;
2822 data=round((u*(4095))/5); % use 3.3 if it is just for testing with KL26
      incorporated DAC
2823
2824 % Waveform Sending
2825 mj = 1;
2826 rep = 0;
2827 for mj=1:length(data)
2828     value = data(mj);
2829
2830     % if user tries to cancel upload
2831     if getappdata(h,'canceling')
2832         fprintf(s, '%d\r', -4)
2833         pause(0.02);
2834         break
2835     end
2836
2837     if(value==0 && rep~=0) %if numbers are zero
2838         fprintf(s, '%d\r', -1)
2839         rep=0;
2840         pause(0.02);
2841     elseif(value>0 && rep~=1) %if numbers return to positive, and only then, then
      is >. As we want only during negative then >=
2842         fprintf(s, '%d\r', -2)
2843         rep=1;
2844         pause(0.02);
```

```
2845     elseif(value<0 && rep~=2) %if numbers return to positive, and only then, then
        is >. As we want only during negative then >=
2846         fprintf(s, '%d\r', -3)
2847         rep=2;
2848         pause(0.02);
2849     end
2850
2851     fprintf(s, '%d\r', abs(value))
2852
2853     pause(0.02);
2854     % a small pause is used because MATLAB was sending it to fast for
2855     % the MCU
2856
2857     waitbar(mj / length(data));
2858 end
2859
2860 % if user pressed 'Cancel' in waitbar
2861 if getappdata(h,'canceling')
2862     errordlg('All settings already uploaded were reseted',...
2863             'Uploading Cancelled','modal')
2864     uicontrol(hObject)
2865     fprintf(s, '%d\r', -14)
2866     pause(0.02);
2867     fprintf(s, '%d\r', -6)
2868     pause(0.02);
2869     delete(h);
2870
2871 else
2872     fprintf(s, '%d\r', -4) % after every sample data sent, -4 acts as a
        terminator
2873
2874     % Repetition Rate Sending
2875     send_repetitions = handles.n_repetitions+1;
2876     send_interstimulus = round(handles.interstimulus_time*handles.time_ms_us);
2877     send_reps_max = handles.reps_max;
2878     fprintf(s, '%d\r', -10) % -10 is the value chosen to control repetition rate
        in mcu
2879     pause(0.02);
2880     fprintf(s, '%d\r', send_repetitions) % sends the repetition rate
2881     pause(0.02);
2882     fprintf(s, '%d\r', send_interstimulus) % sends the interstimulus time
2883     pause(0.02);
2884     fprintf(s, '%d\r', send_reps_max) % sends the maximum repetitons it can make
2885         % before value is gets bigger than
2886         % maximum amplitude
2887     pause(0.02);
2888
2889
```

```
2890     % Repetition Amplitude Ratio Sending
2891     send_rep_amp_ratio = handles.rep_amp_ratio;
2892     fprintf(s, '%d\r', -11) % -11 is the value chosen to control repetition
    amplitude ratio in mcu
2893     pause(0.02);
2894     if send_rep_amp_ratio > 0 && send_rep_amp_ratio < 1
2895         fprintf(s, '%d\r', -15) % -15 is the value chosen to signal the mcu that
    repetition amplitude ratio is smaller than 1
2896         pause(0.02);
2897         fprintf(s, '%d\r', ((1/send_rep_amp_ratio)*10)) % sends an inverted
    repetition amplitude ratio multiplied by 10
2898                                     % so it can send value
    smaller than 1 and with one decimal point
2899         pause(0.02);
2900     else
2901         fprintf(s, '%d\r', -16) % -16 is the value chosen to signal the mcu that
    repetition amplitude ratio is bigger than 1
2902         pause(0.02);
2903         fprintf(s, '%d\r', (send_rep_amp_ratio*10)) % sends the repetition
    amplitude ratio multiplied by 10
2904                                     % so it can send value
    smaller than 1 and with one decimal point
2905         pause(0.02);
2906     end
2907
2908
2909
2910     % Time Lag Sending
2911     send_time_lag = handles.time_lag;
2912     fprintf(s, '%d\r', -12) % -11 is the value chosen to control repetition
    amplitude ratio in mcu
2913     pause(0.02);
2914     fprintf(s, '%d\r', send_time_lag) % sends the repetition amplitude ratio
2915     pause(0.02);
2916
2917
2918     % End of Transmission - however transmission is only really finished
2919     % with 'Apply' or 'Reset'
2920
2921 end
2922 delete(h); % close waitbat
2923 fclose(s); %close the serial port
2924 delete(s) % deleting and cleaning of variable. it is more efective
2925 clear s;
2926
2927 guidata(hObject, handles);
2928
2929
```

```

2930
2931 function Q_exp_edit_Callback(hObject, eventdata, handles)
2932 % hObject    handle to Q_exp_edit (see GCBO)
2933 % eventdata  reserved - to be defined in a future version of MATLAB
2934 % handles    structure with handles and user data (see GUIDATA)
2935
2936 % Hints: get(hObject,'String') returns contents of Q_exp_edit as text
2937 %         str2double(get(hObject,'String')) returns contents of Q_exp_edit as a
           double
2938
2939 q_exp_input = str2double(get(hObject,'string'));
2940
2941 if isfield(handles, 'plot_popup_value' )
2942     % handles.firing_popup_value exists - you may access it
2943 else
2944     % handles.firing_popup_value does not exist
2945     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
2946     uicontrol(hObject)
2947     return
2948 end
2949
2950 if isnan(q_exp_input) || q_exp_input > 1
2951     errordlg('You must enter a numeric value smaller or equal to 1','Invalid
           Input','modal')
2952     uicontrol(hObject)
2953     return
2954 else
2955     handles.q = q_exp_input;
2956     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
           duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
2957     handles.timescale = (0:(1/handles.time_resolution):(handles.
           stimulation_fulltime+handles.t_f));
2958     value = handles.plot_popup_value;
2959     string = handles.plot_popup_string;
2960     switch string{value}
2961         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
2962             handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
           handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
2963             i=1;
2964             total_decay_amplitude = 0;
2965             for i=1:handles.decay_steps
2966                 handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
           amplitude_1*handles.q*...
2967                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
           .*...
2968                     ones(1,handles.resolution*handles.time_resolution));
2969                 total_decay_amplitude = total_decay_amplitude + (handles.
           amplitude_1*handles.q*...

```

```

2970         exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
2971     end
2972     amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
2973     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
2974     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
2975     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
2976     handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
2977         amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
2978         zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
2979         -((handles.stimulation_fulltime)*handles.time_resolution))]);
2980     handles.current_data_I = handles.quasi_trap;
2981     handles.stimulation_data_I = handles.quasi_trap;
2982 end
2983
2984 handles.reps_max = 0;
2985 if handles.repetition ~= 0
2986     for n_reps = 1:handles.n_repetitions
2987         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
2988         || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
2989             handles.reps_max = n_reps;
2990         end
2991         if handles.reps_max ~=0
2992             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
2993         else
2994             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
2995         end
2996     end
2997 end
2998
2999 if handles.fullstimulation_duration < handles.stimulation_fulltime

```

```
3000         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
           stimulation_fulltime)
3001     end
3002
3003 end
3004
3005 guidata(hObject, handles);
3006
3007
3008 % --- Executes during object creation, after setting all properties.
3009 function Q_exp_edit_CreateFcn(hObject, eventdata, handles)
3010 % hObject    handle to Q_exp_edit (see GCBO)
3011 % eventdata  reserved - to be defined in a future version of MATLAB
3012 % handles    empty - handles not created until after all CreateFcns called
3013
3014 % Hint: edit controls usually have a white background on Windows.
3015 %         See ISPC and COMPUTER.
3016 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
           defaultUicontrolBackgroundColor'))
3017     set(hObject,'BackgroundColor','white');
3018 end
3019
3020
3021
3022 function Q2_exp_edit_Callback(hObject, eventdata, handles)
3023 % hObject    handle to Q2_exp_edit (see GCBO)
3024 % eventdata  reserved - to be defined in a future version of MATLAB
3025 % handles    structure with handles and user data (see GUIDATA)
3026
3027 % Hints: get(hObject,'String') returns contents of Q2_exp_edit as text
3028 %         str2double(get(hObject,'String')) returns contents of Q2_exp_edit as a
           double
3029 q2_exp_input = str2double(get(hObject,'string'));
3030
3031 if isfield(handles, 'plot_popup_value' )
3032     % handles.firing_popup_value exists - you may access it
3033 else
3034     % handles.firing_popup_value does not exist
3035     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3036     uicontrol(hObject)
3037     return
3038 end
3039
3040 if isnan(q2_exp_input)
3041     errordlg('You must enter a numeric value','Invalid Input','modal')
3042     uicontrol(hObject)
3043     return
3044 else
```



```

3045     handles.q2 = q2_exp_input;
3046     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
3047     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3048     value = handles.plot_popup_value;
3049     string = handles.plot_popup_string;
3050     switch string{value}
3051         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
3052             handles.quasi_trap = [zeros(1,handles.t_i*handles.time_resolution) (-
handles.amplitude_1).*ones(1,handles.duration_1*handles.time_resolution)];
3053             i=1;
3054             total_decay_amplitude = 0;
3055             for i=1:handles.decay_steps
3056                 handles.quasi_trap = horzcat(handles.quasi_trap,(-handles.
amplitude_1*handles.q*...
3057                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s))
.*...
3058                     ones(1,handles.resolution*handles.time_resolution));
3059                 total_decay_amplitude = total_decay_amplitude + (handles.
amplitude_1*handles.q*...
3060                     exp(-handles.q2*(i*handles.resolution)*handles.time_ms_s));
3061             end
3062             amplitude_CB = (handles.amplitude_1*handles.duration_1 +
total_decay_amplitude*handles.resolution)/handles.biphasic;
3063             handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
3064             handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
3065             handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3066             handles.quasi_trap = horzcat(handles.quasi_trap, [zeros(1,(handles.
delay*handles.time_resolution))...
3067                 amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
3068                 zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution)...
3069                     -((handles.stimulation_fulltime)*handles.time_resolution)))]);
3070             handles.current_data_I = handles.quasi_trap;
3071             handles.stimulation_data_I = handles.quasi_trap;
3072         end
3073
3074     handles.reps_max = 0;
3075     if handles.repetition ~= 0
3076         for n_reps = 1:handles.n_repetitions

```

```

3077         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
3078             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
3079             handles.reps_max = n_reps;
3080         end
3081         if handles.reps_max ~=0
3082             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
3083         else
3084             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
3085         end
3086     end
3087 end
3088
3089 if handles.fullstimulation_duration < handles.stimulation_fulltime
3090     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
3091 end
3092
3093 end
3094
3095
3096 % --- Executes during object creation, after setting all properties.
3097 function Q2_exp_edit_CreateFcn(hObject, eventdata, handles)
3098 % hObject    handle to Q2_exp_edit (see GCBO)
3099 % eventdata  reserved - to be defined in a future version of MATLAB
3100 % handles    empty - handles not created until after all CreateFcns called
3101
3102 % Hint: edit controls usually have a white background on Windows.
3103 %         See ISPC and COMPUTER.
3104 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
3105     set(hObject,'BackgroundColor','white');
3106 end
3107
3108
3109
3110 function A_exp_edit_Callback(hObject, eventdata, handles)
3111 % hObject    handle to A_exp_edit (see GCBO)
3112 % eventdata  reserved - to be defined in a future version of MATLAB

```

```

3113 % handles      structure with handles and user data (see GUIDATA)
3114
3115 % Hints: get(hObject,'String') returns contents of A_exp_edit as text
3116 %      str2double(get(hObject,'String')) returns contents of A_exp_edit as a
           double
3117
3118 a_exp_input = str2double(get(hObject,'string'));
3119
3120 if isfield(handles, 'plot_popup_value' )
3121     % handles.firing_popup_value exists - you may access it
3122 else
3123     % handles.firing_popup_value does not exist
3124     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3125     uicontrol(hObject)
3126     return
3127 end
3128
3129 if isnan(a_exp_input)
3130     errordlg('You must enter a numeric value','Invalid Input','modal')
3131     uicontrol(hObject)
3132     return
3133 elseif (a_exp_input + handles.b + handles.c) > 1 % This condition was created
           because if
3134     % the sum of these 3 parameters is bigger than 1, the wave as a step
3135     % between end of increase and begin of decay
3136     errordlg('Sum of A, B and C cannot be bigger than 1','Invalid Input','modal')
3137     uicontrol(hObject)
3138     return
3139 else
3140     handles.a = a_exp_input;
3141     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
           duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
3142     handles.timescale = (0:(1/handles.time_resolution):(handles.
           stimulation_fulltime+handles.t_f));
3143     value = handles.plot_popup_value;
3144     string = handles.plot_popup_string;
3145     switch string{value}
3146         case 'Tri-Exponential' % User selects tri-exponential
3147             handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
3148             j_i = 1;
3149             j_d = 1;
3150             total_increase_amplitude = 0;
3151             total_decay_amplitude = 0;
3152             for j_i=1:handles.increase_steps
3153                 handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
           amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
           resolution*handles.time_resolution))...

```

```

3154         +(-((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
3155         ones(1,handles.resolution*handles.time_resolution));
3156         total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
3157         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
3158     end
3159     for j_d=1:handles.decay_steps
3160         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3161         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3162         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3163         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
3164         ones(1,handles.resolution*handles.time_resolution));
3165         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3166         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3167         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3168         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
3169     end
3170     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
3171     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
3172     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
3173     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3174     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
3175     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
3176     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
3177     -((handles.stimulation_fulltime)*handles.time_resolution))]);
3178     handles.current_data_I = handles.tri_exp;
3179     handles.stimulation_data_I = handles.tri_exp;
3180 end
3181
3182 handles.reps_max = 0;

```

```

3183     if handles.repetition ~= 0
3184         for n_reps = 1:handles.n_repetitions
3185             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
3186                 || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
3187                 handles.reps_max = n_reps;
3188             end
3189             if handles.reps_max ~=0
3190                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
3191             else
3192                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
3193             end
3194         end
3195     end
3196
3197     if handles.fullstimulation_duration < handles.stimulation_fulltime
3198         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
3199     end
3200
3201 end
3202
3203 guidata(hObject, handles);
3204
3205
3206 % --- Executes during object creation, after setting all properties.
3207 function A_exp_edit_CreateFcn(hObject, eventdata, handles)
3208 % hObject    handle to A_exp_edit (see GCBO)
3209 % eventdata  reserved - to be defined in a future version of MATLAB
3210 % handles    empty - handles not created until after all CreateFcns called
3211
3212 % Hint: edit controls usually have a white background on Windows.
3213 %         See ISPC and COMPUTER.
3214 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
3215     set(hObject,'BackgroundColor','white');
3216 end
3217
3218

```

```

3219
3220 function A2_exp_edit_Callback(hObject, eventdata, handles)
3221 % hObject    handle to A2_exp_edit (see GCBO)
3222 % eventdata  reserved - to be defined in a future version of MATLAB
3223 % handles    structure with handles and user data (see GUIDATA)
3224
3225 % Hints: get(hObject,'String') returns contents of A2_exp_edit as text
3226 %         str2double(get(hObject,'String')) returns contents of A2_exp_edit as a
           double
3227
3228 a2_exp_input = str2double(get(hObject,'string'));
3229
3230 if isfield(handles, 'plot_popup_value' )
3231     % handles.firing_popup_value exists - you may access it
3232 else
3233     % handles.firing_popup_value does not exist
3234     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3235     uicontrol(hObject)
3236     return
3237 end
3238
3239 if isnan(a2_exp_input)
3240     errordlg('You must enter a numeric value','Invalid Input','modal')
3241     uicontrol(hObject)
3242     return
3243 else
3244     handles.a2 = a2_exp_input;
3245     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
           duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
3246     handles.timescale = (0:(1/handles.time_resolution):(handles.
           stimulation_fulltime+handles.t_f));
3247     value = handles.plot_popup_value;
3248     string = handles.plot_popup_string;
3249     switch string{value}
3250         case 'Tri-Exponential' % User selects tri-exponential
3251             handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
3252             j_i = 1;
3253             j_d = 1;
3254             total_increase_amplitude = 0;
3255             total_decay_amplitude = 0;
3256             for j_i=1:handles.increase_steps
3257                 handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
           amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
           resolution*handles.time_resolution)...
3258                     +((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
           handles.t_i)-handles.t_i))/handles.time_resolution).*...
3259                 ones(1,handles.resolution*handles.time_resolution));

```

```

3260         total_increase_amplitude = total_increase_amplitude + (((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
3261         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
3262     end
3263     for j_d=1:handles.decay_steps
3264         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3265         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3266         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3267         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
3268         ones(1,handles.resolution*handles.time_resolution));
3269         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3270         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3271         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3272         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
3273     end
3274     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
3275     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
3276     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
3277     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3278     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
3279     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
3280     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
3281     -((handles.stimulation_fulltime)*handles.time_resolution))]);
3282     handles.current_data_I = handles.tri_exp;
3283     handles.stimulation_data_I = handles.tri_exp;
3284 end
3285
3286 handles.reps_max = 0;
3287 if handles.repetition ~= 0
3288     for n_reps = 1:handles.n_repetitions

```

```

3289         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
3290             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
3291             handles.reps_max = n_reps;
3292         end
3293         if handles.reps_max ~=0
3294             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
3295         else
3296             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
3297         end
3298     end
3299 end
3300
3301 if handles.fullstimulation_duration < handles.stimulation_fulltime
3302     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
3303 end
3304
3305 end
3306
3307 guidata(hObject, handles);
3308
3309
3310 % --- Executes during object creation, after setting all properties.
3311 function A2_exp_edit_CreateFcn(hObject, eventdata, handles)
3312 % hObject    handle to A2_exp_edit (see GCBO)
3313 % eventdata  reserved - to be defined in a future version of MATLAB
3314 % handles    empty - handles not created until after all CreateFcns called
3315
3316 % Hint: edit controls usually have a white background on Windows.
3317 %         See ISPC and COMPUTER.
3318 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
3319     set(hObject,'BackgroundColor','white');
3320 end
3321
3322
3323
3324 function B_exp_edit_Callback(hObject, eventdata, handles)

```



```

3325 % hObject    handle to B_exp_edit (see GCBO)
3326 % eventdata  reserved - to be defined in a future version of MATLAB
3327 % handles    structure with handles and user data (see GUIDATA)
3328
3329 % Hints: get(hObject,'String') returns contents of B_exp_edit as text
3330 %         str2double(get(hObject,'String')) returns contents of B_exp_edit as a
           double
3331
3332 b_exp_input = str2double(get(hObject,'string'));
3333
3334 if isfield(handles, 'plot_popup_value' )
3335     % handles.firing_popup_value exists - you may access it
3336 else
3337     % handles.firing_popup_value does not exist
3338     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3339     uicontrol(hObject)
3340     return
3341 end
3342
3343 if isnan(b_exp_input)
3344     errordlg('You must enter a numeric value','Invalid Input','modal')
3345     uicontrol(hObject)
3346     return
3347 elseif (b_exp_input + handles.a + handles.c) > 1
3348     errordlg('Sum of A, B and C cannot be bigger than 1','Invalid Input','modal')
3349     uicontrol(hObject)
3350     return
3351 else
3352     handles.b = b_exp_input;
3353     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
           duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
3354     handles.timescale = (0:(1/handles.time_resolution):(handles.
           stimulation_fulltime+handles.t_f));
3355     value = handles.plot_popup_value;
3356     string = handles.plot_popup_string;
3357     switch string{value}
3358         case 'Tri-Exponential' % User selects tri-exponential
3359             handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
3360             j_i = 1;
3361             j_d = 1;
3362             total_increase_amplitude = 0;
3363             total_decay_amplitude = 0;
3364             for j_i=1:handles.increase_steps
3365                 handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
           amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
           resolution*handles.time_resolution)...
3366                 +(-((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
           handles.t_i)-handles.t_i))/handles.time_resolution).*...

```

```

3367         ones(1,handles.resolution*handles.time_resolution));
3368         total_increase_amplitude = total_increase_amplitude + (((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
3369         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i)/handles.time_resolution);
3370     end
3371     for j_d=1:handles.decay_steps
3372         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3373         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3374         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3375         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
3376         ones(1,handles.resolution*handles.time_resolution));
3377         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3378         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3379         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3380         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
3381     end
3382     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
3383     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
3384     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
3385     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3386     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
3387     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
3388     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
3389     -((handles.stimulation_fulltime)*handles.time_resolution))]);
3390     handles.current_data_I = handles.tri_exp;
3391     handles.stimulation_data_I = handles.tri_exp;
3392 end
3393
3394 handles.reps_max = 0;
3395 if handles.repetition ~= 0
3396     for n_reps = 1:handles.n_repetitions

```

```

3397         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
3398             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)                handles.reps_max = n_reps
;
3399         end
3400         if handles.reps_max ~=0
3401             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
3402         else
3403             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
3404         end
3405     end
3406 end
3407
3408 if handles.fullstimulation_duration < handles.stimulation_fulltime
3409     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
3410 end
3411
3412 end
3413
3414 guidata(hObject, handles);
3415
3416
3417
3418 % --- Executes during object creation, after setting all properties.
3419 function B_exp_edit_CreateFcn(hObject, eventdata, handles)
3420 % hObject    handle to B_exp_edit (see GCBO)
3421 % eventdata  reserved - to be defined in a future version of MATLAB
3422 % handles    empty - handles not created until after all CreateFcns called
3423
3424 % Hint: edit controls usually have a white background on Windows.
3425 %         See ISPC and COMPUTER.
3426 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
3427     set(hObject,'BackgroundColor','white');
3428 end
3429
3430
3431

```

```

3432 function B2_exp_edit_Callback(hObject, eventdata, handles)
3433 % hObject    handle to B2_exp_edit (see GCBO)
3434 % eventdata  reserved - to be defined in a future version of MATLAB
3435 % handles    structure with handles and user data (see GUIDATA)
3436
3437 % Hints: get(hObject,'String') returns contents of B2_exp_edit as text
3438 %         str2double(get(hObject,'String')) returns contents of B2_exp_edit as a
           double
3439
3440 b2_exp_input = str2double(get(hObject,'string'));
3441
3442 if isfield(handles, 'plot_popup_value' )
3443     % handles.firing_popup_value exists - you may access it
3444 else
3445     % handles.firing_popup_value does not exist
3446     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3447     uicontrol(hObject)
3448     return
3449 end
3450
3451 if isnan(b2_exp_input)
3452     errordlg('You must enter a numeric value','Invalid Input','modal')
3453     uicontrol(hObject)
3454     return
3455 else
3456     handles.b2 = b2_exp_input;
3457     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
           duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
3458     handles.timescale = (0:(1/handles.time_resolution):(handles.
           stimulation_fulltime+handles.t_f));
3459     value = handles.plot_popup_value;
3460     string = handles.plot_popup_string;
3461     switch string{value}
3462         case 'Tri-Exponential' % User selects tri-exponential
3463             handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
3464             j_i = 1;
3465             j_d = 1;
3466             total_increase_amplitude = 0;
3467             total_decay_amplitude = 0;
3468             for j_i=1:handles.increase_steps
3469                 handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
           amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
           resolution*handles.time_resolution)...
3470                     +((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
           handles.t_i)-handles.t_i))/handles.time_resolution).*...
3471                 ones(1,handles.resolution*handles.time_resolution));

```

```

3472         total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
3473         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i)/handles.time_resolution);
3474     end
3475     for j_d=1:handles.decay_steps
3476         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3477         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3478         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3479         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
3480         ones(1,handles.resolution*handles.time_resolution));
3481         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3482         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3483         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3484         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
3485     end
3486     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
3487     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
3488     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
3489     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3490     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
3491     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
3492     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
3493     -((handles.stimulation_fulltime)*handles.time_resolution))]);
3494     handles.current_data_I = handles.tri_exp;
3495     handles.stimulation_data_I = handles.tri_exp;
3496 end
3497
3498 handles.reps_max = 0;
3499 if handles.repetition ~= 0
3500     for n_reps = 1:handles.n_repetitions

```

```

3501         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
3502             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
3503             handles.reps_max = n_reps;
3504         end
3505         if handles.reps_max ~=0
3506             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
3507         else
3508             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
3509         end
3510     end
3511 end
3512
3513 if handles.fullstimulation_duration < handles.stimulation_fulltime
3514     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
3515 end
3516
3517 end
3518
3519 guidata(hObject, handles);
3520
3521
3522
3523 % --- Executes during object creation, after setting all properties.
3524 function B2_exp_edit_CreateFcn(hObject, eventdata, handles)
3525 % hObject    handle to B2_exp_edit (see GCBO)
3526 % eventdata  reserved - to be defined in a future version of MATLAB
3527 % handles    empty - handles not created until after all CreateFcns called
3528
3529 % Hint: edit controls usually have a white background on Windows.
3530 %         See ISPC and COMPUTER.
3531 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
3532     set(hObject,'BackgroundColor','white');
3533 end
3534
3535
3536

```

```

3537 function C_exp_edit_Callback(hObject, eventdata, handles)
3538 % hObject    handle to C_exp_edit (see GCBO)
3539 % eventdata  reserved - to be defined in a future version of MATLAB
3540 % handles    structure with handles and user data (see GUIDATA)
3541
3542 % Hints: get(hObject,'String') returns contents of C_exp_edit as text
3543 %         str2double(get(hObject,'String')) returns contents of C_exp_edit as a
           double
3544
3545 c_exp_input = str2double(get(hObject,'string'));
3546
3547 if isfield(handles, 'plot_popup_value' )
3548     % handles.firing_popup_value exists - you may access it
3549 else
3550     % handles.firing_popup_value does not exist
3551     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3552     uicontrol(hObject)
3553     return
3554 end
3555
3556 if isnan(c_exp_input)
3557     errordlg('You must enter a numeric value','Invalid Input','modal')
3558     uicontrol(hObject)
3559     return
3560 elseif (c_exp_input + handles.a + handles.b) > 1
3561     errordlg('Sum of A, B and C cannot be bigger than 1','Invalid Input','modal')
3562     uicontrol(hObject)
3563     return
3564 else
3565     handles.c = c_exp_input;
3566     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
3567     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3568     value = handles.plot_popup_value;
3569     string = handles.plot_popup_string;
3570     switch string{value}
3571         case 'Tri-Exponential' % User selects tri-exponential
3572             handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
3573             j_i = 1;
3574             j_d = 1;
3575             total_increase_amplitude = 0;
3576             total_decay_amplitude = 0;
3577             for j_i=1:handles.increase_steps
3578                 handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
resolution*handles.time_resolution))...

```

```

3579         +(-((-handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution).*...
3580         ones(1,handles.resolution*handles.time_resolution));
3581         total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
3582         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i))/handles.time_resolution);
3583     end
3584     for j_d=1:handles.decay_steps
3585         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3586         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3587         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3588         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
3589         ones(1,handles.resolution*handles.time_resolution));
3590         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3591         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3592         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3593         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
3594     end
3595     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
3596     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
3597     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
3598     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3599     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
3600     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
3601     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
3602     -((handles.stimulation_fulltime)*handles.time_resolution))]);
3603     handles.current_data_I = handles.tri_exp;
3604     handles.stimulation_data_I = handles.tri_exp;
3605 end
3606
3607 handles.reps_max = 0;

```



```

3608     if handles.repetition ~= 0
3609         for n_reps = 1:handles.n_repetitions
3610             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
3611                 || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
3612                 handles.reps_max = n_reps;
3613             end
3614             if handles.reps_max ~=0
3615                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
3616             else
3617                 handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
3618             end
3619         end
3620     end
3621
3622     if handles.fullstimulation_duration < handles.stimulation_fulltime
3623         set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
3624     end
3625
3626 end
3627
3628 guidata(hObject, handles);
3629
3630
3631
3632 % --- Executes during object creation, after setting all properties.
3633 function C_exp_edit_CreateFcn(hObject, eventdata, handles)
3634 % hObject    handle to C_exp_edit (see GCBO)
3635 % eventdata  reserved - to be defined in a future version of MATLAB
3636 % handles    empty - handles not created until after all CreateFcns called
3637
3638 % Hint: edit controls usually have a white background on Windows.
3639 %         See ISPC and COMPUTER.
3640 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
3641     set(hObject,'BackgroundColor','white');
3642 end
3643

```

```

3644
3645
3646 function C2_exp_edit_Callback(hObject, eventdata, handles)
3647 % hObject    handle to C2_exp_edit (see GCBO)
3648 % eventdata  reserved - to be defined in a future version of MATLAB
3649 % handles    structure with handles and user data (see GUIDATA)
3650
3651 % Hints: get(hObject,'String') returns contents of C2_exp_edit as text
3652 %         str2double(get(hObject,'String')) returns contents of C2_exp_edit as a
           double
3653
3654 c2_exp_input = str2double(get(hObject,'string'));
3655
3656 if isfield(handles, 'plot_popup_value' )
3657     % handles.firing_popup_value exists - you may access it
3658 else
3659     % handles.firing_popup_value does not exist
3660     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3661     uicontrol(hObject)
3662     return
3663 end
3664
3665 if isnan(c2_exp_input)
3666     errordlg('You must enter a numeric value','Invalid Input','modal')
3667     uicontrol(hObject)
3668     return
3669 else
3670     handles.c2 = c2_exp_input;
3671     handles.stimulation_fulltime = handles.duration_1+handles.duration_2+handles.
           duration_balance_1+handles.duration_balance_2+handles.delay+handles.decay;
3672     handles.timescale = (0:(1/handles.time_resolution):(handles.
           stimulation_fulltime+handles.t_f));
3673     value = handles.plot_popup_value;
3674     string = handles.plot_popup_string;
3675     switch string{value}
3676         case 'Tri-Exponential' % User selects tri-exponential
3677             handles.tri_exp = zeros(1,handles.t_i*handles.time_resolution);
3678             j_i = 1;
3679             j_d = 1;
3680             total_increase_amplitude = 0;
3681             total_decay_amplitude = 0;
3682             for j_i=1:handles.increase_steps
3683                 handles.tri_exp = horzcat(handles.tri_exp, (((-handles.
           amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i))*(j_i*handles.
           resolution*handles.time_resolution)...
3684                 +((-(-handles.amplitude_1*handles.t_i)/(handles.duration_1+
           handles.t_i)-handles.t_i))/handles.time_resolution).*...
3685                 ones(1,handles.resolution*handles.time_resolution));

```

```

3686         total_increase_amplitude = total_increase_amplitude + ((handles.
amplitude_1)/((handles.duration_1+handles.t_i)-handles.t_i)*(j_i*handles.
resolution*handles.time_resolution)...
3687         -((handles.amplitude_1*handles.t_i)/(handles.duration_1+
handles.t_i)-handles.t_i)/handles.time_resolution);
3688     end
3689     for j_d=1:handles.decay_steps
3690         handles.tri_exp = horzcat(handles.tri_exp,(handles.tri_exp((
handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3691         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3692         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3693         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
).*...
3694         ones(1,handles.resolution*handles.time_resolution));
3695         total_decay_amplitude = total_decay_amplitude + (handles.tri_exp
((handles.t_i+handles.duration_1)*handles.time_resolution)*((handles.a*...
3696         exp(-handles.a2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.b*...
3697         exp(-handles.b2*(j_d*handles.resolution)*handles.time_ms_s))
+(handles.c*...
3698         exp(-handles.c2*(j_d*handles.resolution)*handles.time_ms_s)))
);
3699     end
3700     amplitude_CB = (total_increase_amplitude*handles.resolution +
total_decay_amplitude*handles.resolution)/handles.biphasic;
3701     handles.duration_balance_total = handles.biphasic.*(handles.
duration_1 + handles.decay);
3702     handles.stimulation_fulltime = handles.duration_1+handles.
duration_balance_total+handles.delay+handles.decay;
3703     handles.timescale = (0:(1/handles.time_resolution):(handles.
stimulation_fulltime+handles.t_f));
3704     handles.tri_exp = horzcat(handles.tri_exp, [zeros(1,(handles.delay*
handles.time_resolution))...
3705     amplitude_CB.*ones(1,handles.duration_balance_total*handles.
time_resolution)...
3706     zeros(1,floor((length(handles.timescale)-handles.t_i*handles.
time_resolution))...
3707     -((handles.stimulation_fulltime)*handles.time_resolution))]);
3708     handles.current_data_I = handles.tri_exp;
3709     handles.stimulation_data_I = handles.tri_exp;
3710 end
3711
3712 handles.reps_max = 0;
3713 if handles.repetition ~= 0
3714     for n_reps = 1:handles.n_repetitions

```

```

3715         if (handles.amplitude_max ~=0 && (handles.amplitude_max <= handles.
amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.amplitude_max <=
handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) ) && handles.
reps_max == 0)...
3716             || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
3717             handles.reps_max = n_reps;
3718         end
3719         if handles.reps_max ~=0
3720             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(handles.reps_max)).*handles.stimulation_data_I);
3721         else
3722             handles.current_data_I = horzcat(handles.current_data_I,zeros(1,(
handles.interstimulus_time*handles.time_resolution)),((handles.rep_amp_ratio)
.^(n_reps)).*handles.stimulation_data_I);
3723         end
3724     end
3725 end
3726
3727 if handles.fullstimulation_duration < handles.stimulation_fulltime
3728     set(handles.stim_duration_edit, 'enable', 'on','String', handles.
stimulation_fulltime)
3729 end
3730
3731 end
3732
3733 guidata(hObject, handles);
3734
3735
3736
3737 % --- Executes during object creation, after setting all properties.
3738 function C2_exp_edit_CreateFcn(hObject, eventdata, handles)
3739 % hObject    handle to C2_exp_edit (see GCBO)
3740 % eventdata  reserved - to be defined in a future version of MATLAB
3741 % handles    empty - handles not created until after all CreateFcns called
3742
3743 % Hint: edit controls usually have a white background on Windows.
3744 %         See ISPC and COMPUTER.
3745 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
3746     set(hObject,'BackgroundColor','white');
3747 end
3748
3749
3750

```

```
3751 function stim_duration_edit_Callback(hObject, eventdata, handles)
3752 % hObject    handle to stim_duration_edit (see GCBO)
3753 % eventdata  reserved - to be defined in a future version of MATLAB
3754 % handles    structure with handles and user data (see GUIDATA)
3755
3756 % Hints: get(hObject,'String') returns contents of stim_duration_edit as text
3757 %         str2double(get(hObject,'String')) returns contents of stim_duration_edit
           as a double
3758
3759 stim_duration_input = str2double(get(hObject,'string'));
3760
3761 if isfield(handles, 'plot_popup_value' )
3762     % handles.firing_popup_value exists - you may access it
3763 else
3764     % handles.firing_popup_value does not exist
3765     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3766     uicontrol(hObject)
3767     return
3768 end
3769
3770 if isnan(stim_duration_input) || stim_duration_input == 0
3771     errordlg('You must enter a numeric value bigger than zero','Invalid Input','
modal')
3772     uicontrol(hObject)
3773     return
3774 elseif stim_duration_input < handles.stimulation_fulltime
3775     errordlg('You must enter a value equal or bigger than the duration of a
single pulse','Invalid Input','modal')
3776     uicontrol(hObject)
3777     return
3778 elseif handles.repetition ~= 0 && (1/(handles.repetition)) > stim_duration_input
3779     warndlg('Repetition Cycle bigger than Stimulation Duration! No Repetition
will be made.','Value Selection', 'modal');
3780     uicontrol(hObject)
3781     return
3782 else
3783     handles.fullstimulation_duration = stim_duration_input;
3784     value = handles.plot_popup_value;
3785     string = handles.plot_popup_string;
3786     handles.reps_max = 0;
3787     n_reps = 1;
3788     handles.interstimulus_time = (1/(handles.repetition));
3789     handles.n_repetitions = (floor(handles.fullstimulation_duration/(handles.
stimulation_fulltime+handles.interstimulus_time))-1);
3790     switch string{value}
3791         case 'Bi-level Lilly' % User selects bilevel Lilly
3792             handles.current_data_I = handles.bi_level;
3793             handles.stimulation_data_I = handles.bi_level;
```

```

3794         for n_reps = 1:handles.n_repetitions
3795             if handles.amplitude_max ~=0 && handles.reps_max == 0 && (handles
                .amplitude_max <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps)) ||
                handles.amplitude_max <= handles.amplitude_2*((handles.rep_amp_ratio).^(
                n_reps)))
3796                 handles.reps_max = n_reps;
3797             end
3798             if handles.reps_max ~=0
3799                 handles.current_data_I = horzcat(handles.current_data_I,zeros
                (1,(handles.interstimulus_time*handles.time_resolution)),((handles.
                rep_amp_ratio).^(handles.reps_max)).*handles.bi_level);
3800             else
3801                 handles.current_data_I = horzcat(handles.current_data_I,zeros
                (1,(handles.interstimulus_time*handles.time_resolution)),((handles.
                rep_amp_ratio).^(n_reps)).*handles.bi_level);
3802             end
3803         end
3804         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
3805             handles.current_data_I = handles.quasi_trap;
3806             handles.stimulation_data_I = handles.quasi_trap;
3807             for n_reps = 1:handles.n_repetitions
3808                 if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
                .amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
                ...
3809                 || (handles.amplitude_max ==0 && handles.
                DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
                +1)) && handles.reps_max == 0)
3810                 handles.reps_max = n_reps;
3811             end
3812             if handles.reps_max ~=0
3813                 handles.current_data_I = horzcat(handles.current_data_I,zeros
                (1,(handles.interstimulus_time*handles.time_resolution)),((handles.
                rep_amp_ratio).^(handles.reps_max)).*handles.quasi_trap);
3814             else
3815                 handles.current_data_I = horzcat(handles.current_data_I,zeros
                (1,(handles.interstimulus_time*handles.time_resolution)),((handles.
                rep_amp_ratio).^(n_reps)).*handles.quasi_trap);
3816             end
3817         end
3818         case 'Tri-Exponential' % User selects tri-exponential
3819             handles.current_data_I = handles.tri_exp;
3820             handles.stimulation_data_I = handles.tri_exp;
3821             for n_reps = 1:handles.n_repetitions
3822                 if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
                .amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
                ...

```

```

3823         || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
3824             handles.reps_max = n_reps;
3825         end
3826         if handles.reps_max ~=0
3827             handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.tri_exp);
3828         else
3829             handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.tri_exp);
3830         end
3831     end
3832     case 'Bursting' % User selects bursting strategies
3833         handles.current_data_I = handles.bursting;
3834         handles.stimulation_data_I = handles.bursting;
3835         for n_reps = 1:handles.n_repetitions
3836             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
3837         || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
3838             handles.reps_max = n_reps;
3839         end
3840         if handles.reps_max ~=0
3841             handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.bursting);
3842         else
3843             handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.bursting);
3844         end
3845     end
3846     case 'Rectangular' % User selects pulse
3847         handles.current_data_I = handles.pulse;
3848         handles.stimulation_data_I = handles.pulse;
3849         for n_reps = 1:handles.n_repetitions
3850             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
3851         || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
3852             handles.reps_max = n_reps;

```

```

3853         end
3854         if handles.reps_max ~=0
3855             handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.pulse);
3856         else
3857             handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.pulse);
3858         end
3859     end
3860     case 'Load Waveform'
3861         handles.current_data_I = handles.current_data_I;
3862         handles.stimulation_data_I = handles.current_data_I;
3863         for n_reps = 1:handles.n_repetitions
3864             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= max(
handles.stimulation_data_I)*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
amplitude_max <= abs(min(handles.stimulation_data_I))*((handles.rep_amp_ratio
).^(n_reps+1))) && handles.reps_max == 0)...
3865                 || (handles.amplitude_max ==0 && (handles.
DAC_amplitude_limit <= max(handles.stimulation_data_I)*((handles.
rep_amp_ratio).^(n_reps+1)) || handles.DAC_amplitude_limit <= abs(min(handles
.stimulation_data_I))*((handles.rep_amp_ratio).^(n_reps+1))) && handles.
reps_max == 0)
3866                 handles.reps_max = n_reps;
3867             end
3868             if handles.reps_max ~=0
3869                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.stimulation_data_I);
3870             else
3871                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.stimulation_data_I);
3872             end
3873         end
3874     end
3875
3876 end
3877
3878 guidata(hObject, handles);
3879
3880
3881
3882
3883 % --- Executes during object creation, after setting all properties.
3884 function stim_duration_edit_CreateFcn(hObject, eventdata, handles)
3885 % hObject    handle to stim_duration_edit (see GCBO)

```



```
3886 % eventdata reserved - to be defined in a future version of MATLAB
3887 % handles empty - handles not created until after all CreateFcns called
3888
3889 % Hint: edit controls usually have a white background on Windows.
3890 % See ISPC and COMPUTER.
3891 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
    defaultUicontrolBackgroundColor'))
3892     set(hObject,'BackgroundColor','white');
3893 end
3894
3895
3896
3897 function rep_amp_ratio_edit_Callback(hObject, eventdata, handles)
3898 % hObject handle to rep_amp_ratio_edit (see GCBO)
3899 % eventdata reserved - to be defined in a future version of MATLAB
3900 % handles structure with handles and user data (see GUIDATA)
3901
3902 % Hints: get(hObject,'String') returns contents of rep_amp_ratio_edit as text
3903 % str2double(get(hObject,'String')) returns contents of rep_amp_ratio_edit
    as a double
3904
3905 rep_amp_ratio_input = str2double(get(hObject,'string'));
3906
3907 if isfield(handles, 'plot_popup_value' )
3908     % handles.firing_popup_value exists - you may access it
3909 else
3910     % handles.firing_popup_value does not exist
3911     errordlg('You must choose a Waverform Type!','Invalid Input','modal')
3912     uicontrol(hObject)
3913     return
3914 end
3915
3916 if isnan(rep_amp_ratio_input) || rep_amp_ratio_input == 0 || rem(
    rep_amp_ratio_input , 0.1) ~= 0
3917     errordlg('You must enter a numeric value bigger than zero','Invalid Input','
    modal')
3918     uicontrol(hObject)
3919     return
3920 elseif rep_amp_ratio_input == 0 && handles.repetition == 0
3921     wd = warndlg('There will be no Repetition Cycle','Input','modal')
3922     waitfor(wd);
3923     uicontrol(hObject)
3924     return
3925 elseif handles.repetition == 0
3926     ed = errordlg('There is no Repetition Cycle','Input','modal')
3927     waitfor(ed);
3928     handles.interstimulus_time = 0;
3929     handles.n_repetitions = 1;
```

```

3930     value = handles.plot_popup_value;
3931     string = handles.plot_popup_string;
3932     switch string{value}
3933         case 'Bi-level Lilly' % User selects bilevel Lilly
3934             handles.current_data_I = handles.bi_level;
3935             handles.stimulation_data_I = handles.bi_level;
3936         case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
3937             handles.current_data_I = handles.quasi_trap;
3938             handles.stimulation_data_I = handles.quasi_trap;
3939         case 'Tri-Exponential' % User selects tri-exponential
3940             handles.current_data_I = handles.tri_exp;
3941             handles.stimulation_data_I = handles.tri_exp;
3942         case 'Bursting' % User selects bursting strategies
3943             handles.current_data_I = handles.bursting;
3944             handles.stimulation_data_I = handles.bursting;
3945         case 'Rectangular' % User selects pulse
3946             handles.current_data_I = handles.pulse;
3947             handles.stimulation_data_I = handles.pulse;
3948         case 'Load Waveform'
3949             handles.current_data_I = handles.current_data_I;
3950             handles.stimulation_data_I = handles.current_data_I;
3951     end
3952     return
3953 else
3954     handles.rep_amp_ratio = rep_amp_ratio_input;
3955     value = handles.plot_popup_value;
3956     string = handles.plot_popup_string;
3957     handles.reps_max = 0;
3958     n_reps = 1;
3959     switch string{value}
3960         case 'Bi-level Lilly' % User selects bilevel Lilly
3961             handles.current_data_I = handles.bi_level;
3962             handles.stimulation_data_I = handles.bi_level;
3963             for n_reps = 1:handles.n_repetitions
3964                 if (handles.amplitude_max ~=0 && (handles.amplitude_max <=
handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
amplitude_max <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps+1)) )
&& handles.reps_max == 0)...
3965                     || (handles.amplitude_max ==0 && (handles.DAC_amplitude_limit
<= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
DAC_amplitude_limit <= handles.amplitude_2*((handles.rep_amp_ratio).^(n_reps
+1)) ) && handles.reps_max == 0)
3966                     handles.reps_max = n_reps;
3967                 end
3968                 if handles.reps_max ~=0
3969                     handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.bi_level);

```

```

3970         else
3971             handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(n_reps)).*handles.bi_level);
3972         end
3973     end
3974     case 'Quasi-Trapezoidal' % User selects quasi-trapezoidal
3975         handles.current_data_I = handles.quasi_trap;
3976         handles.stimulation_data_I = handles.quasi_trap;
3977         for n_reps = 1:handles.n_repetitions
3978             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
3979                 || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
3980                 handles.reps_max = n_reps;
3981             end
3982             if handles.reps_max ~=0
3983                 handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.quasi_trap);
3984             else
3985                 handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(n_reps)).*handles.quasi_trap);
3986             end
3987         end
3988     case 'Tri-Exponential' % User selects tri-exponential
3989         handles.current_data_I = handles.tri_exp;
3990         handles.stimulation_data_I = handles.tri_exp;
3991         for n_reps = 1:handles.n_repetitions
3992             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
3993                 || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
3994                 handles.reps_max = n_reps;
3995             end
3996             if handles.reps_max ~=0
3997                 handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.tri_exp);
3998             else
3999                 handles.current_data_I = horzcat(handles.current_data_I, zeros
(1, (handles.interstimulus_time*handles.time_resolution)), ((handles.
rep_amp_ratio).^(n_reps)).*handles.tri_exp);

```

```

4000         end
4001     end
4002     case 'Bursting' % User selects bursting strategies
4003         handles.current_data_I = handles.bursting;
4004         handles.stimulation_data_I = handles.bursting;
4005         for n_reps = 1:handles.n_repetitions
4006             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
4007                 || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
4008                 handles.reps_max = n_reps;
4009             end
4010             if handles.reps_max ~=0
4011                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.bursting);
4012             else
4013                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.bursting);
4014             end
4015         end
4016     case 'Rectangular' % User selects pulse
4017         handles.current_data_I = handles.pulse;
4018         handles.stimulation_data_I = handles.pulse;
4019         for n_reps = 1:handles.n_repetitions
4020             if (handles.amplitude_max ~=0 && handles.amplitude_max <= handles
.amplitude_1*((handles.rep_amp_ratio).^(n_reps+1)) && handles.reps_max == 0)
...
4021                 || (handles.amplitude_max ==0 && handles.
DAC_amplitude_limit <= handles.amplitude_1*((handles.rep_amp_ratio).^(n_reps
+1)) && handles.reps_max == 0)
4022                 handles.reps_max = n_reps;
4023             end
4024             if handles.reps_max ~=0
4025                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(handles.reps_max)).*handles.pulse);
4026             else
4027                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.pulse);
4028             end
4029         end
4030     case 'Load Waveform'
4031         handles.current_data_I = handles.current_data_I;

```

```

4032         handles.stimulation_data_I = handles.current_data_I;
4033         for n_reps = 1:handles.n_repetitions
4034             if (handles.amplitude_max ~=0 && (handles.amplitude_max <= max(
handles.stimulation_data_I)*((handles.rep_amp_ratio).^(n_reps+1)) || handles.
amplitude_max <= abs(min(handles.stimulation_data_I))*((handles.rep_amp_ratio
).^(n_reps+1))) && handles.reps_max == 0)...
4035                 || (handles.amplitude_max ==0 && (handles.
DAC_amplitude_limit <= max(handles.stimulation_data_I)*((handles.
rep_amp_ratio).^(n_reps+1)) || handles.DAC_amplitude_limit <= abs(min(handles
.stimulation_data_I))*((handles.rep_amp_ratio).^(n_reps+1))) && handles.
reps_max == 0)
4036                 handles.reps_max = n_reps;
4037             end
4038             if handles.reps_max ~=0
4039                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.stimulation_data_I);
4040             else
4041                 handles.current_data_I = horzcat(handles.current_data_I,zeros
(1,(handles.interstimulus_time*handles.time_resolution)),((handles.
rep_amp_ratio).^(n_reps)).*handles.stimulation_data_I);
4042             end
4043         end
4044     end
4045 end
4046
4047 guidata(hObject, handles);
4048
4049
4050
4051
4052
4053 % --- Executes during object creation, after setting all properties.
4054 function rep_amp_ratio_edit_CreateFcn(hObject, eventdata, handles)
4055 % hObject    handle to rep_amp_ratio_edit (see GCBO)
4056 % eventdata  reserved - to be defined in a future version of MATLAB
4057 % handles    empty - handles not created until after all CreateFcns called
4058
4059 % Hint: edit controls usually have a white background on Windows.
4060 %         See ISPC and COMPUTER.
4061 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
defaultUicontrolBackgroundColor'))
4062     set(hObject,'BackgroundColor','white');
4063 end
4064
4065
4066
4067 function time_lag_edit_Callback(hObject, eventdata, handles)

```

```
4068 % hObject    handle to time_lag_edit (see GCBO)
4069 % eventdata  reserved - to be defined in a future version of MATLAB
4070 % handles    structure with handles and user data (see GUIDATA)
4071
4072 % Hints: get(hObject,'String') returns contents of time_lag_edit as text
4073 %          str2double(get(hObject,'String')) returns contents of time_lag_edit as a
         double
4074
4075 time_lag_input = str2double(get(hObject,'string'));
4076 wd = warndlg('This value applies for all channels. Always.','Safe Range');
4077 waitfor(wd);
4078
4079 if isnan(time_lag_input) || time_lag_input == 0
4080     errordlg('You must enter a numeric value bigger than zero','Invalid Input','
         modal')
4081     uicontrol(hObject)
4082     return
4083 else
4084     handles.time_lag = time_lag_input;
4085 end
4086
4087 guidata(hObject, handles);
4088
4089
4090
4091 % --- Executes during object creation, after setting all properties.
4092 function time_lag_edit_CreateFcn(hObject, eventdata, handles)
4093 % hObject    handle to time_lag_edit (see GCBO)
4094 % eventdata  reserved - to be defined in a future version of MATLAB
4095 % handles    empty - handles not created until after all CreateFcns called
4096
4097 % Hint: edit controls usually have a white background on Windows.
4098 %          See ISPC and COMPUTER.
4099 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
         defaultUicontrolBackgroundColor'))
4100     set(hObject,'BackgroundColor','white');
4101 end
4102
4103
4104 % --- Executes on selection change in channel_popup.
4105 function channel_popup_Callback(hObject, eventdata, handles)
4106 % hObject    handle to channel_popup (see GCBO)
4107 % eventdata  reserved - to be defined in a future version of MATLAB
4108 % handles    structure with handles and user data (see GUIDATA)
4109
4110 % Hints: contents = cellstr(get(hObject,'String')) returns channel_popup contents
         as cell array
4111 %          contents{get(hObject,'Value')} returns selected item from channel_popup
```

```
4112
4113 val = get(handles.channel_popup, 'Value');
4114 handles.channel_popup_value = val;
4115 str = get(hObject, 'String');
4116 handles.channel_popup_string = str;
4117 switch str{val}
4118     case '1'
4119         handles.channel_no = 1;
4120     case '2'
4121         handles.channel_no = 2;
4122     case '3'
4123         handles.channel_no = 3;
4124     case '4'
4125         handles.channel_no = 4;
4126 end
4127
4128 guidata(hObject, handles);
4129
4130
4131 % --- Executes during object creation, after setting all properties.
4132 function channel_popup_CreateFcn(hObject, eventdata, handles)
4133 % hObject    handle to channel_popup (see GCBO)
4134 % eventdata  reserved - to be defined in a future version of MATLAB
4135 % handles    empty - handles not created until after all CreateFcns called
4136
4137 % Hint: popupmenu controls usually have a white background on Windows.
4138 %         See ISPC and COMPUTER.
4139 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
    defaultUicontrolBackgroundColor'))
4140     set(hObject,'BackgroundColor','white');
4141 end
4142
4143
4144 % --- Executes on selection change in firing_popup.
4145 function firing_popup_Callback(hObject, eventdata, handles)
4146 % hObject    handle to firing_popup (see GCBO)
4147 % eventdata  reserved - to be defined in a future version of MATLAB
4148 % handles    structure with handles and user data (see GUIDATA)
4149
4150 % Hints: contents = cellstr(get(hObject,'String')) returns firing_popup contents
    as cell array
4151 %         contents{get(hObject,'Value')} returns selected item from firing_popup
4152
4153 val = get(handles.firing_popup, 'Value');
4154 handles.firing_popup_value = val;
4155 str = get(hObject, 'String');
4156 handles.firing_popup_string = str;
4157 switch str{val}
```

```
4158     case 'alone'
4159         handles.firing_type = 1;
4160         set(handles.time_lag_edit, 'enable', 'off')
4161     case 'synchronous'
4162         handles.firing_type = 2;
4163         set(handles.time_lag_edit, 'enable', 'off')
4164     case 'asynchronous'
4165         handles.firing_type = 3;
4166         set(handles.time_lag_edit, 'enable', 'on','String', '1')
4167
4168 end
4169
4170 guidata(hObject, handles);
4171
4172
4173 % --- Executes during object creation, after setting all properties.
4174 function firing_popup_CreateFcn(hObject, eventdata, handles)
4175 % hObject    handle to firing_popup (see GCBO)
4176 % eventdata  reserved - to be defined in a future version of MATLAB
4177 % handles    empty - handles not created until after all CreateFcns called
4178
4179 % Hint: popupmenu controls usually have a white background on Windows.
4180 %         See ISPC and COMPUTER.
4181 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
         defaultUicontrolBackgroundColor'))
4182     set(hObject,'BackgroundColor','white');
4183 end
4184
4185
4186 % --- Executes on selection change in COM_popup.
4187 function COM_popup_Callback(hObject, eventdata, handles)
4188 % hObject    handle to COM_popup (see GCBO)
4189 % eventdata  reserved - to be defined in a future version of MATLAB
4190 % handles    structure with handles and user data (see GUIDATA)
4191
4192 % Hints: contents = cellstr(get(hObject,'String')) returns COM_popup contents as
         cell array
4193 %         contents{get(hObject,'Value')} returns selected item from COM_popup
4194
4195 serialInfo = instrhwinfo('serial');
4196
4197 if isempty(serialInfo.SerialPorts) == 1
4198     errordlg('There are no available COM ports','Invalid Input','modal')
4199     uicontrol(hObject)
4200     return
4201 else
4202     n_coms = 1;
4203     for n_coms = 1:length(serialInfo.SerialPorts)
```



```
4204         string_list(n_coms+1) = serialInfo.SerialPorts(n_coms);
4205     end
4206     set(handles.COM_popup, 'String', string_list);
4207 end
4208
4209 val = get(handles.COM_popup, 'Value');
4210 handles.COM_popup_value = val;
4211 str = get(hObject, 'String');
4212 handles.COM_popup_string = str;
4213
4214 guidata(hObject, handles);
4215
4216
4217
4218
4219
4220 % --- Executes during object creation, after setting all properties.
4221 function COM_popup_CreateFcn(hObject, eventdata, handles)
4222 % hObject    handle to COM_popup (see GCBO)
4223 % eventdata  reserved - to be defined in a future version of MATLAB
4224 % handles    empty - handles not created until after all CreateFcns called
4225
4226 % Hint: popupmenu controls usually have a white background on Windows.
4227 %         See ISPC and COMPUTER.
4228 if ispc && isequal(get(hObject, 'BackgroundColor'), get(0, '
    defaultUicontrolBackgroundColor'))
4229     set(hObject, 'BackgroundColor', 'white');
4230 end
4231
4232
4233 % --- Executes on button press in apply_pushbutton.
4234 function apply_pushbutton_Callback(hObject, eventdata, handles)
4235 % hObject    handle to apply_pushbutton (see GCBO)
4236 % eventdata  reserved - to be defined in a future version of MATLAB
4237 % handles    structure with handles and user data (see GUIDATA)
4238
4239 if handles.old_channel == 0
4240     errordlg('Nothing uploaded to apply', 'Invalid Input', 'modal')
4241     uicontrol(hObject)
4242 else
4243
4244     if isfield(handles, 'COM_popup_value' )
4245         % handles.firing_popup_value exists - you may access it
4246     else
4247         % handles.firing_popup_value does not exist
4248         errordlg('No COM port selected!', 'Invalid Input', 'modal')
4249         uicontrol(hObject)
4250
```

```
4251     serialInfo = instrhwinfo('serial');
4252     if isempty(serialInfo.SerialPorts) == 1
4253         errordlg('There are no available COM ports','Invalid Input','modal')
4254         uicontrol(hObject)
4255         return
4256     else
4257         n_coms = 1;
4258         for n_coms = 1:length(serialInfo.SerialPorts)
4259             string_list(n_coms+1) = serialInfo.SerialPorts(n_coms);
4260         end
4261         set(handles.COM_popup,'String',string_list);
4262     end
4263
4264     return
4265 end
4266
4267
4268 % Attempt Communication with Microcontroller
4269 priorPorts = instrfind; % finds any existing Serial Ports in MATLAB
4270 delete(priorPorts) % and deletes them
4271
4272 s = serial(handles.COM_popup_string{handles.COM_popup_value});
4273
4274 % s = serial('COM6'); %assigns the object s to serial port
4275
4276 set(s, 'InputBufferSize', 1); %128 originally %number of bytes in inout
buffer
4277 set(s, 'FlowControl', 'none');
4278 set(s, 'BaudRate', 38400);
4279 set(s, 'Parity', 'none');
4280 set(s, 'DataBits', 8);
4281 set(s, 'StopBit', 1);
4282 set(s, 'Timeout',100);
4283 %clc;
4284
4285 try
4286     fopen(s);
4287 catch err
4288     errordlg('Something went wrong with the connection. Maybe another program
using the device? If not, try re-connect the device',...
4289         'Invalid Input','modal')
4290     uicontrol(hObject)
4291     return
4292 end
4293
4294
4295 final_answer = questdlg('Are you sure you want to apply stimulation?','
Stimulation','Apply','Cancel','Cancel');
```

```
4296     switch final_answer
4297         case 'Apply'
4298             fprintf(s, '%d\r', -14)
4299             pause(0.02);
4300             fprintf(s, '%d\r', -5)
4301             pause(0.02);
4302             handles.number_sent_channels = 1;
4303             handles.old_channel = 0;
4304             handles.old_firing = 0;
4305         case 'Cancel'
4306     end
4307
4308     fclose(s);
4309     delete(s)
4310     clear s;
4311 end
4312 guidata(hObject, handles);
4313
4314
4315
4316 % --- Executes on button press in reset_pushbutton.
4317 function reset_pushbutton_Callback(hObject, eventdata, handles)
4318 % hObject    handle to reset_pushbutton (see GCBO)
4319 % eventdata  reserved - to be defined in a future version of MATLAB
4320 % handles    structure with handles and user data (see GUIDATA)
4321
4322 if isfield(handles, 'COM_popup_value' )
4323     % handles.firing_popup_value exists - you may access it
4324 else
4325     % handles.firing_popup_value does not exist
4326     errordlg('No COM port selected!', 'Invalid Input', 'modal')
4327     uicontrol(hObject)
4328
4329     serialInfo = instrhwininfo('serial');
4330     if isempty(serialInfo.SerialPorts) == 1
4331         errordlg('There are no available COM ports', 'Invalid Input', 'modal')
4332         uicontrol(hObject)
4333         return
4334     else
4335         n_coms = 1;
4336         for n_coms = 1:length(serialInfo.SerialPorts)
4337             string_list(n_coms+1) = serialInfo.SerialPorts(n_coms);
4338         end
4339         set(handles.COM_popup, 'String', string_list);
4340     end
4341
4342     return
4343 end
```

```
4344
4345
4346 % Attempt Communication with Microcontroller
4347 priorPorts = instrfind; % finds any existing Serial Ports in MATLAB
4348 delete(priorPorts) % and deletes them
4349
4350 s = serial(handles.COM_popup_string{handles.COM_popup_value});
4351
4352 % s = serial('COM6'); %assigns the object s to serial port
4353
4354 set(s, 'InputBufferSize', 1); %128 originally %number of bytes in inout buffer
4355 set(s, 'FlowControl', 'none');
4356 set(s, 'BaudRate', 38400);
4357 set(s, 'Parity', 'none');
4358 set(s, 'DataBits', 8);
4359 set(s, 'StopBit', 1);
4360 set(s, 'Timeout', 100);
4361 %clc;
4362
4363 try
4364     fopen(s);
4365 catch err
4366     errordlg('Something went wrong with the connection. Maybe another program
4367             using the device? If not, try re-connect the device',...
4368             'Invalid Input','modal')
4369     uicontrol(hObject)
4370     return
4371 end
4372
4373 final_answer = questdlg('Are you sure you want to reset ALL the settings already
4374                         uploaded?', 'Stimulation', 'Reset', 'Cancel', 'Cancel');
4375 switch final_answer
4376     case 'Reset'
4377         fprintf(s, '%d\r', -14) %because the upload cycle only ends when user '
4378         Apply's or 'Reset's
4379         pause(0.02);
4380         fprintf(s, '%d\r', -6)
4381         pause(0.02);
4382         handles.number_sent_channels = 1;
4383         handles.old_channel = 0;
4384         handles.old_firing = 0;
4385     case 'Cancel'
4386 end
4387 fclose(s);
4388 delete(s)
4389 clear s;
```

```
4389
4390 guidata(hObject, handles);
4391
4392
4393 function electrode_impedit_Callback(hObject, eventdata, handles)
4394 % hObject    handle to electrode_impedit (see GCBO)
4395 % eventdata  reserved - to be defined in a future version of MATLAB
4396 % handles    structure with handles and user data (see GUIDATA)
4397
4398 % Hints: get(hObject,'String') returns contents of electrode_impedit as text
4399 %          str2double(get(hObject,'String')) returns contents of
           electrode_impedit as a double
4400 electrode_impedit_input = str2double(get(hObject,'string'));
4401 if isnan(electrode_impedit_input)
4402     wd = warndlg('No Amplitude Safe Range Defined!','Safe Range');
4403     waitfor(wd);
4404     handles.amplitude_max = 0;
4405     set(handles.amplitude_maximum_edit, 'enable', 'off','String', ' ')
4406 else
4407     handles.resistance = electrode_impedit_input;
4408     handles.amplitude_max = (handles.opamp_max_output_voltage * handles.R_set)/(
           handles.resistance + handles.R_set + (2*handles.R_internal));
4409     set(handles.amplitude_maximum_edit, 'enable', 'off','String', handles.
           amplitude_max)
4410 end
4411
4412 guidata(hObject, handles);
4413
4414
4415 % --- Executes during object creation, after setting all properties.
4416 function electrode_impedit_CreateFcn(hObject, eventdata, handles)
4417 % hObject    handle to electrode_impedit (see GCBO)
4418 % eventdata  reserved - to be defined in a future version of MATLAB
4419 % handles    empty - handles not created until after all CreateFcns called
4420
4421 % Hint: edit controls usually have a white background on Windows.
4422 %       See ISPC and COMPUTER.
4423 if ispc && isequal(get(hObject,'BackgroundColor'), get(0, '
           defaultUicontrolBackgroundColor'))
4424     set(hObject,'BackgroundColor','white');
4425 end
4426
4427
4428
4429 function amplitude_maximum_edit_Callback(hObject, eventdata, handles)
4430 % hObject    handle to amplitude_maximum_edit (see GCBO)
4431 % eventdata  reserved - to be defined in a future version of MATLAB
4432 % handles    structure with handles and user data (see GUIDATA)
```

```
4433
4434 % Hints: get(hObject,'String') returns contents of amplitude_maximum_edit as text
4435 %         str2double(get(hObject,'String')) returns contents of
           amplitude_maximum_edit as a double
4436
4437
4438 % --- Executes during object creation, after setting all properties.
4439 function amplitude_maximum_edit_CreateFcn(hObject, eventdata, handles)
4440 % hObject    handle to amplitude_maximum_edit (see GCBO)
4441 % eventdata  reserved - to be defined in a future version of MATLAB
4442 % handles    empty - handles not created until after all CreateFcns called
4443
4444 % Hint: edit controls usually have a white background on Windows.
4445 %         See ISPC and COMPUTER.
4446 if ispc && isequal(get(hObject,'BackgroundColor'), get(0,'
           defaultUicontrolBackgroundColor'))
4447     set(hObject,'BackgroundColor','white');
4448 end
```

Appendix B

Microcontroller Code

B.1 Main Function Code

```
1 /* #####
2 **      Filename      : main.c
3 **      Project       : Send_Num
4 **      Processor     : MKL26Z128VLH4
5 **      Version       : Driver 01.01
6 **      Compiler      : GNU C Compiler
7 **      Date/Time    : 2014-11-19, 12:12, # CodeGen: 0
8 **      Abstract      :
9 **          Main module.
10 **          This module contains user's application code.
11 **      Settings     :
12 **      Contents     :
13 **          No public methods
14 **
15 ** #####*/
16 /*!
17 ** @file main.c
18 ** @version 01.01
19 ** @brief
20 **          Main module.
21 **          This module contains user's application code.
22 */
23 /*!
24 ** @addtogroup main_module main module documentation
25 ** @{
26 */
27 /* MODULE main */
28
```

```
29
30 /*
    #####
31 ATTENTION: For this program to run correctly, the WAIT component has to be
    downloaded
32 Please search 'MCUonEclipse' and 'Processor Expert Component *.PEupd Files on
    GitHub'
33 to understando how to add WAIT component
34 #####
    */
35
36
37 /* Including needed modules to compile this module/procedure */
38 #include "Cpu.h"
39 #include "Events.h"
40 #include "CsIO1.h"
41 #include "IO1.h"
42 #include "WAIT1.h"
43 #include "BLUE.h"
44 #include "IN11.h"
45 #include "GREEN.h"
46 #include "RED.h"
47 #include "IN21.h"
48 #include "IN12.h"
49 #include "IN22.h"
50 #include "IN13.h"
51 #include "IN23.h"
52 #include "IN14.h"
53 #include "IN24.h"
54 #include "SHDN1.h"
55 #include "SHDN2.h"
56 #include "EN.h"
57 /* Including shared modules, which are used for whole project */
58 #include "PE_Types.h"
59 #include "PE_Error.h"
60 #include "PE_Const.h"
61 #include "IO_Map.h"
62
63 /* User includes (#include below this line is not maintained by Processor Expert)
    */
64 #include <stdio.h>
65 #include <stdlib.h>
66
67 /* Constant definition */
68 #define DATA_LENGTH_MAX 930 // Value bigger than this gives memory-related error
69 #define CHANNELS 5 // Array 0 (zero) + 4 channels
70 #define SWITCHOFF 0
```



```
71 #define SWITCHON01 1
72 #define SWITCHON10 2
73
74 /* This definition speeds up these ON/OFF outputs */
75 #define IN11_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN11_MODULE_BASE_ADDRESS,
76                    IN11_PORT_MASK)
77 #define IN11_Set()     GPIO_PDD_SetPortDataOutputMask(IN11_MODULE_BASE_ADDRESS,
78                    IN11_PORT_MASK)
79
80 #define IN21_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN21_MODULE_BASE_ADDRESS,
81                    IN21_PORT_MASK)
82 #define IN21_Set()     GPIO_PDD_SetPortDataOutputMask(IN21_MODULE_BASE_ADDRESS,
83                    IN21_PORT_MASK)
84
85 #define IN12_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN12_MODULE_BASE_ADDRESS,
86                    IN12_PORT_MASK)
87 #define IN12_Set()     GPIO_PDD_SetPortDataOutputMask(IN12_MODULE_BASE_ADDRESS,
88                    IN12_PORT_MASK)
89
90 #define IN22_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN22_MODULE_BASE_ADDRESS,
91                    IN22_PORT_MASK)
92 #define IN22_Set()     GPIO_PDD_SetPortDataOutputMask(IN22_MODULE_BASE_ADDRESS,
93                    IN22_PORT_MASK)
94
95
96 #define IN13_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN13_MODULE_BASE_ADDRESS,
97                    IN13_PORT_MASK)
98 #define IN13_Set()     GPIO_PDD_SetPortDataOutputMask(IN13_MODULE_BASE_ADDRESS,
99                    IN13_PORT_MASK)
100 #define IN23_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN23_MODULE_BASE_ADDRESS,
101                    IN23_PORT_MASK)
102 #define IN23_Set()     GPIO_PDD_SetPortDataOutputMask(IN23_MODULE_BASE_ADDRESS,
103                    IN23_PORT_MASK)
104
105
106 #define IN14_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN14_MODULE_BASE_ADDRESS,
107                    IN14_PORT_MASK)
108 #define IN14_Set()     GPIO_PDD_SetPortDataOutputMask(IN14_MODULE_BASE_ADDRESS,
109                    IN14_PORT_MASK)
110 #define IN24_Clr()      GPIO_PDD_ClearPortDataOutputMask(IN24_MODULE_BASE_ADDRESS,
111                    IN24_PORT_MASK)
112 #define IN24_Set()     GPIO_PDD_SetPortDataOutputMask(IN24_MODULE_BASE_ADDRESS,
113                    IN24_PORT_MASK)
114
115
116 void MCU_Init(void)
117 {
118     //SPI0 module initialization
119     SIM_SCGC4 |= SIM_SCGC4_SPI0_MASK;           // Turn on clock to SPI0 module
120     SIM_SCGC5 |= SIM_SCGC5_PORTC_MASK;         // Turn on clock to Port D module
121     PORTC_PCR5 = PORT_PCR_MUX(0x02);           // PTC5 pin is SPI0 CLK line
122     PORTC_PCR6 = PORT_PCR_MUX(0x02);           // PTC6 pin is SPI0 MOSI line
```

```

103     PORTC_PCR7 = PORT_PCR_MUX(0x02);           // PTC7 pin is SPIO MISO line
104     PORTC_PCR4 = PORT_PCR_MUX(0x02);           // PTC4 pin is configured SSbar
105
106     SPIO_C1 = SPI_C1_SPE_MASK | SPI_C1_MSTR_MASK | SPI_C1_SSOE_MASK;    //
Enable SPIO module, master mode, SS low active mode
107     SPIO_C2 = SPI_C2_SPIMODE_MASK | SPI_C2_MODFEN_MASK;
108     SPIO_BR = SPI_BR_SPPR(0x00) | SPI_BR_SPR(0x00);    // BaudRate = BusClock /
((SPPR+1) * 2^(SPR+1)) = 20970000 / ((1+1) * 2^(0+1)) = 5.2425 MHz
109     SPIO_S = SPI_S_SPTEF_MASK;
110
111 }
112
113
114
115 /*lint -save -e970 Disable MISRA rule (6.3) checking. */
116 int main(void)
117 /*lint -restore Enable MISRA rule (6.3) checking. */
118 {
119
120     /* Write your local variable definition here */
121
122
123     /*** Processor Expert internal initialization. DON'T REMOVE THIS CODE!!!
124     ***/
125     PE_low_level_init();
126     /*** End of Processor Expert internal initialization.
127     ***/
128
129     /* SPI initialization */
130     MCU_Init();
131
132     /* Turn ON Power Supplies */
133     SHDN1_SetVal(SHDN1_DeviceData);
134     SHDN2_SetVal(SHDN1_DeviceData);
135     EN_SetVal(EN_DeviceData);
136
137     for(;;) {
138
139         /* Variables initialization */
140
141         //MATLAB information variables
142         int value = 0;
143         int swtvalue = 0; //needed only if switch is intended to stay on
the all time instead of just a peak
144         int channel = 0;
145         int timeLag = 0;
146         int firingType = 0;

```

```
146         int repetitonAmpRatio[CHANNELS] = {0};
147         int invRatio[CHANNELS] = {0}; //needed because transmission of
float values through UART leads to errors
148         int interstimulusTime[CHANNELS] = {0}; // applicable for Alone
and Asynchronous Fire
149         int nRepetitions[CHANNELS] = {0}; // in here channels is
possible because one can terminate earlier than the others
150         int RepsMax[CHANNELS] = {0};
151         int interstimulusTimeSynch = 0; // applicable only for
Synchronous Fire
152
153         // Counters
154         int pwr = 0;
155         int n = 0;
156         int i = 0;
157         int rep = 0;
158         int rep1 = 0;
159         int rep2 = 0;
160         int rep3 = 0;
161         int rep4 = 0;
162         int nRepts = 0;
163
164         // Output Arrays
165         uint8_t data = {0};
166         uint8_t addressData = {0};
167
168         // One Pulse Data Arrays - they are defined as 16-bit but only
use up to 12-bit numbers because that is the DAC maximum
169         uint16_t current1[DATA_LENGTH_MAX] = {0}; //Due to memory
overload, it has to be like this, can't be a [channel][DATA_LENGTH_MAX]
170         uint16_t current2[DATA_LENGTH_MAX] = {0};
171         uint16_t current3[DATA_LENGTH_MAX] = {0};
172         uint16_t current4[DATA_LENGTH_MAX] = {0};
173         uint16_t controller1[DATA_LENGTH_MAX] = {0};
174         uint16_t controller2[DATA_LENGTH_MAX] = {0};
175         uint16_t controller3[DATA_LENGTH_MAX] = {0};
176         uint16_t controller4[DATA_LENGTH_MAX] = {0};
177
178         // LED OFF and Switch Controllers LOW
179         BLUE_SetVal(BLUE_DeviceData); // turn OFF blue led
180         RED_SetVal(RED_DeviceData); // turn OFF red led
181         GREEN_ClrVal(GREEN_DeviceData); // turn ON green led - this is
the only one ON, to let the user know that it is working
182         IN11_Clr(); // turn LOW switch 1 from channel 1
183         IN21_Clr(); // turn LOW switch 2 from channel 1
184         IN12_Clr(); // turn LOW switch 1 from channel 2
185         IN22_Clr(); // turn LOW switch 2 from channel 2
186         IN13_Clr(); // turn LOW switch 1 from channel 3
```

```

187         IN23_Clr();      // turn LOW switch 2 from channel 3
188         IN14_Clr();      // turn LOW switch 1 from channel 4
189         IN24_Clr();      // turn LOW      switch 2 from channel 4
190
191         // To Power Down the DAC Output
192         data = (0x00 & 0xFF); // least significant byte (8-bit from the
           right)
193         addressData = (0x00 >> 8) + 0x70; // shift to get the
remaining 4-bits of the 12-bit
194         while(!(SPIO_S)); // A wait cycle while SPI information is not
sent
195         SPIO_DH=addressData; //DAC select A[1:0], State select OP[1:0],
Data bits D[11:8]
196         SPIO_DL=data; // Data bits D[7:0]
197
198
199         /* Cycle to receive the information and data values from MATLAB
*/
200         /*** Communication protocol between MATLAB and MCU is based in
negative values because all important information and data is sent in
positive integers ***/
201         for(;;){
202
203             // Reading from UART. Blocks cycle until a value is
received
204             char line[20];
205             fgets(line, sizeof(line), stdin);
206             sscanf(line, "%d", &value);
207
208             // When a value is received is, green and blue leds are
OFF, red led turns ON
209             GREEN_SetVal(GREEN_DeviceData);
210             BLUE_SetVal(BLUE_DeviceData);
211             RED_ClrVal(RED_DeviceData);
212
213             // The MATLAB 'pre-warns' the MCU of what is the
information that is going to send.
214             if (value == -7){ // MATLAB is going to send information
on the Channel and values from one pulser
215
216                 char line[20];
217                 fgets(line, sizeof(line), stdin);
218                 sscanf(line, "%d", &value);
219
220                 channel = value;
221
222                 // If are data values regarding the channel 1
223                 if (channel == 1) {

```

```
224         n = 0;
225         while (1){
226             char line[20];
227             fgets(line, sizeof(line), stdin);
228             sscanf(line, "%d", &value);
229
230             if (n > DATA_LENGTH_MAX){ // If,
somehow, the length of one pulse is bigger than the possible
231                 break;
                // the cycle breaks and a restart of the system will occur
232             }
233             else if (value == -1){ //If in
the pulse there will be a zero phase (interphasic delay)
234
235                 swtvalue = SWITCHOFF;
                // the value that means switch off (0) is saved
236
237             }
238             else if (value == -2){ //If in
the pulse there is a variation to a positive phase
239
240                 swtvalue = SWITCHON01;
                // the value that means the respective switch on (1) is saved
241
242             }
243             else if (value == -3){ //If in
the pulse there is a variation to a negative phase
244
245                 swtvalue = SWITCHON10;
                // the value that means the respective switch on (2) is saved
246
247             }
248             else if (value == -4){ //If it
is the end of data on one pulse
249
250                 break; // the cycle
breaks and a restart of the system will occur
251             }
252
253             else { //If it is not any
information on variation or to break cycle then it is data of the pulse to
store
254
255                 controller1[n] = swtvalue
                ; // Stores the 'configuration' of the switches in the same place where the
respective phase starts
256
257                 current1[n] = value;
                // Stores the value of the pulse
258
259                 n++;
```

```
257
258         }
259     }
260
261     }
262
263
264
265     if (channel == 2) {
266         n = 0;
267         while (1){
268             char line[20];
269             fgets(line, sizeof(line), stdin);
270             sscanf(line, "%d", &value);
271
272             if (n > DATA_LENGTH_MAX){
273                 break;
274             }
275             else if (value == -1){ //
shorting phase - interphase
276
277                 swtvalue = SWITCHOFF;
278
279             }
280             else if (value == -2){ //
positive phase
281
282                 swtvalue = SWITCHON01;
283
284             }
285             else if (value == -3){ //
negative phase
286
287                 swtvalue = SWITCHON10;
288
289             }
290             else if (value == -4){
291
292                 break;
293             }
294
295             else {
296                 controller2[n] = swtvalue
;
297                 current2[n] = value;
298                 n++;
299
300             }
```

```
301         }
302
303     }
304
305
306
307
308     if (channel == 3) {
309         n = 0;
310         while (1){
311             char line[20];
312             fgets(line, sizeof(line), stdin);
313             sscanf(line, "%d", &value);
314
315             if (n > DATA_LENGTH_MAX){
316                 break;
317             }
318             else if (value == -1){ //
319
320                 shorting phase - interphase
321
322                 swtvalue = SWITCHOFF;
323
324             }
325             else if (value == -2){ //
326
327                 positive phase
328
329                 swtvalue = SWITCHON01;
330
331             }
332             else if (value == -3){ //
333
334                 negative phase
335
336                 swtvalue = SWITCHON10;
337
338             }
339             else if (value == -4){
340
341                 break;
342             }
343             else {
344                 controller3[n] = swtvalue
345
346                 current3[n] = value;
347                 n++;
348             }
349         }
350     }
```

```
345
346         }
347
348
349
350         if (channel == 4) {
351             n = 0;
352             while (1){
353                 char line[20];
354                 fgets(line, sizeof(line), stdin);
355                 sscanf(line, "%d", &value);
356
357                 if (n > DATA_LENGTH_MAX){
358                     break;
359                 }
360                 else if (value == -1){ //
361
362                     shorting phase - interphase
363
364                     swtvalue = SWITCHOFF;
365
366                 }
367                 else if (value == -2){ //
368
369                     positive phase
370
371                     swtvalue = SWITCHON01;
372
373                 }
374                 else if (value == -3){ //
375
376                     negative phase
377
378                     swtvalue = SWITCHON10;
379
380                 }
381                 else if (value == -4){
382                     break;
383                 }
384                 else {
385                     controller4[n] = swtvalue
386
387                     current4[n] = value;
388                     n++;
389                 }
390             }
391         }
392     }
```



```
389
390         }
391
392         else if (value == -10){ // MATLAB is going to send
information on the Repetition Rate
393
394             char line[20];
395             fgets(line, sizeof(line), stdin);
396             sscanf(line, "%d", &value);
397
398             nRepetitions[channel] = value; // Saves the
number of repetitions of the respective channel
399
400
401             char line2[20];
402             fgets(line2, sizeof(line2), stdin);
403             sscanf(line2, "%d", &value);
404
405             if (firingType == 2){
406                 interstimulusTimeSynch = value; // Saves
the interstimulus time of all channels in synchronised firing
407             }
408             else {
409                 interstimulusTime[channel] = value;
// Saves the interstimulus time of each channel in alone and asynchronous
firing
410             }
411
412
413             char line3[20];
414             fgets(line3, sizeof(line3), stdin);
415             sscanf(line3, "%d", &value);
416
417             RepsMax[channel] = value;
418
419         }
420         else if (value == -11){ // MATLAB is going to send
information on the Repetition Amplitude Ratio
421
422             char line[20];
423             fgets(line, sizeof(line), stdin);
424             sscanf(line, "%d", &value);
425
426             if (value == -15){ // If the Repetition
Amplitude Ratio is between 1 and 0
427                 invRatio[channel] = -1;
428             }
```

```
429             else if (value == -16){ // If the Repetition
Amplitude Ratio is higher than 1
430                 invRatio[channel] = 1;
431             }
432
433             char line2[20];
434             fgets(line2, sizeof(line2), stdin);
435             sscanf(line2, "%d", &value);
436
437             repetitonAmpRatio[channel] = value; // Saves the
Repetition Amplitude Ratio of each channel
438         }
439         else if (value == -12){ // MATLAB is going to send
information on Time Lag
440
441             char line[20];
442             fgets(line, sizeof(line), stdin);
443             sscanf(line, "%d", &value);
444
445             timeLag = value; // Saves the Time Lag between
all channel in asynchronous firing
446
447             RED_SetVal(RED_DeviceData); // turn off red
LED
448             BLUE_ClrVal(BLUE_DeviceData); // turn on blue LED
- this is located here because it is the last information on a channel sent
by MATLAB
449
450         }
451         else if (value == -13){ // MATLAB is going to send
information on the Firing Type
452
453             char line[20];
454             fgets(line, sizeof(line), stdin);
455             sscanf(line, "%d", &value);
456
457             firingType = value; // Saves which Firing Type is
going to be used
458         }
459         else if (value == -14 || n > DATA_LENGTH_MAX){ // User
in MALTAB has finished programming the channels or wants to reset all
information already uploaded
460
461             RED_SetVal(RED_DeviceData); // turn off red LED
462             BLUE_SetVal(BLUE_DeviceData); // turn off blue
LED
463             break; // terminates all communication cycle
464         }
```

```
465
466     }
467
468
469     /// THIS PART STILL HAVE CHANGES TO BE MADE. IN FIRING TYPE = 1,
CHANNEL 1 AND 2 HAVE DIFFERENT OUTPUT FROM 3 AND 4 ///
470     // This is due to time testing being made in order to minimize
delay between the output of the original sample and the output of the sample
multiplied by amplitude repetition ratio //
471
472
473     /* Code to use the information and data values previously saved
to obtain a stimulation according to user preferences */
474     char line[20];
475     fgets(line, sizeof(line), stdin);
476     sscanf(line, "%d", &value);
477
478
479     if (n > (DATA_LENGTH_MAX+1) || value == -6){ // If amount of
data is incorrect (due to some transfer error) or user wants to reset all
informantion
480
// skips everything and go to the beginning (to
communication with MATLAB)
481     }
482     else if (value == -5) { // If user wants to apply the stimulation
uploaded
483
RED_ClrVal(RED_DeviceData); // turn off red LED
484
485     // If user chose an Alone Firing
486     if (firingType == 1){
487         nRepts = 0;
488         pwr = 0;
489
490         // One stimulation pulse (stored in MCU) is
repeated for the number of repetitions intended in only one channel
491         while (nRepts < nRepetitions[channel]) {
492             i = 0;
493             rep = 0;
494
495             // If user chose an Channel 1 for Firing
496             if (channel == 1){
497                 for (i = 0; i <= (n-1); i++) { // For the
length of the pulse uploaded
498
499
if(controller1[i] == SWITCHOFF &&
rep!=0){ // If it is a zero phase and it was a variation to zero (this way
avoiding entering in this condition with every SWITCHOFF)
```

```

500                                     IN11_Clr(); // Switch 1
    to LOW
501                                     IN21_Clr(); // Switch 2
    to LOW
502                                     rep = 0; // just to avoid
    entering in this condition with every SWITCHOFF
503                                     }
504                                     else if(controller1[i] ==
SWITCHON01 && rep!=1){ //positive phase
505                                     IN11_Set(); // Switch 1
    to UP
506                                     IN21_Clr(); // Switch 2
    to LOW
507                                     rep = 1; // just to avoid
    entering in this condition with every SWITCHON01
508                                     }
509                                     else if(controller1[i] ==
SWITCHON10 && rep!=2){ //negative phase
510                                     IN11_Clr(); // Switch 1
    to LOW
511                                     IN21_Set(); // Switch 2
    to UP
512                                     rep = 2;          // just
    to avoid entering in this condition with every SWITCHON10
513                                     }
514
515
516                                     //Condition for application of
Repetition Amplitude Ratio
517                                     if (pwr > 0 && invRatio[channel]
== 1 && nRepts <= RepsMax[channel]) { // if ratio is bigger than 1
518                                     current1[i] = current1[i]
    * (repetitonAmpRatio[channel]/10); // the ratio is divided by 10 because in
MATLAB is multiplied by 10 to allow user one decimal values
519
520                                     }
521                                     else if (pwr > 0 && invRatio[
channel] == -1 && nRepts <= RepsMax[channel]) { //if ratio is between 1 and 0
522                                     current1[i] = current1[i]
    / (repetitonAmpRatio[channel]/10);
523
524                                     }
525                                     else { // this is included so
that the delay between repetitions wont be so big
526                                     current1[i] = current1[i]
    * ((repetitonAmpRatio[channel])/ (repetitonAmpRatio[channel]));
527                                     }
528

```

```

529             data = (current1[i] & 0xFF);
// least significant byte of the data value (8-bit from the right)
530             addressData = (current1[i] >> 8) + 0
x10; // shift to get the remaining 4-bits of the 12-bit value
531             // for the DAC A and when it is
alone fire need to add DAC:00 and OP:01 to addressData
532
533             while(!(SPIO_S));
534             SPIO_DH=addressData; //DAC
select A[1:0], State select OP[1:0], Data bits D[11:8]
535             SPIO_DL=data; // Data bits D
[7:0]
536         }
537
538         IN11_Clr(); // Switch 1 to LOW
539         IN21_Clr(); // Switch 2 to LOW
540
541         data = (0x00 & 0xFF); // least
significant byte (8-bit from the right)
542         addressData = (0x00 >> 8) + 0x10;
// shift to get the remaining 4-bits of the 12-bit
543         // for the DAC A and when it is alone
fire need to add DAC:00 and OP:01 to addressData
544
545         while(!(SPIO_S));
546         SPIO_DH=addressData; //DAC select A
[1:0], State select OP[1:0], Data bits D[11:8]
547         SPIO_DL=data; // Data bits D[7:0]
548
549     }
550     else if (channel == 2) {
551         for (i = 0; i <= (n-1); i++) {
552
553             if(controller2[i] ==
SWITCHOFF && rep!=0){
554                 IN12_Clr();
555                 IN22_Clr();
556                 rep = 0;
557             }
558             else if(controller2[i] ==
SWITCHON01 && rep!=1){ //positive phase
559                 IN12_Set();
560                 IN22_Clr();
561                 rep = 1;
562             }
563             else if(controller2[i] ==
SWITCHON10 && rep!=2){ //negative phase
564                 IN12_Clr();

```



```

599                                     SPIO_DH=addressData; //DAC
select A[1:0], State select OP[1:0], Data bits D[11:8]
600                                     SPIO_DL=data; // Data bits D
[7:0]
601
602                                     }
603                                     else if (channel == 3) {
604                                         for (i = 0; i <= (n-1); i++) {
605
606                                             if(controller3[i] ==
SWITCHOFF && rep!=0){
607                                                 IN13_Clr();
608                                                 IN23_Clr();
609                                                 rep = 0;
610                                             }
611                                             else if(controller3[i] ==
SWITCHON01 && rep!=1){ //positive phase
612                                                 IN13_Set();
613                                                 IN23_Clr();
614                                                 rep = 1;
615                                             }
616                                             else if(controller3[i] ==
SWITCHON10 && rep!=2){ //negative phase
617                                                 IN13_Clr();
618                                                 IN23_Set();
619                                                 rep = 2;
620                                             }
621
622
623                                     if (pwr > 0 && invRatio[
channel] == 1 && nRepts <= RepsMax[channel]) { // if is not the first pulse
and ratio is bigger than 1 - application of Repetition Amplitude Ratio
624                                         current3[i] =
current3[i] * (repetitonAmpRatio[channel]/10); // the ratio is divided by 10
because in MATLAB is multiplied by 10 to allow user one decimal values
625
626                                     }
627                                     else if (pwr > 0 &&
invRatio[channel] == -1 && nRepts <= RepsMax[channel]) { // if is not the
first pulse and ratio is between 0 and 1 - application of Repetition
Amplitude Ratio
628                                         current3[i] =
current3[i] / (repetitonAmpRatio[channel]/10);
629
630                                     }
631                                     else { // this is
included so that the delay between repetitions wont be so big

```



```

667                                     }
668                                     else if(controller4[i] ==
        SWITCHON10 && rep!=2){ //negative phase
669                                     IN14_Clr();
670                                     IN24_Set();
671                                     rep = 2;
672                                     }
673
674
675                                     if (pwr > 0 && invRatio[
channel] == 1 && nRepts <= RepsMax[channel]) {
676                                     current4[i] =
current4[i] * (repetitonAmpRatio[channel]/10);
677
678                                     }
679                                     else if (pwr > 0 &&
invRatio[channel] == -1 && nRepts <= RepsMax[channel]) {
680                                     current4[i] =
current4[i] / (repetitonAmpRatio[channel]/10);
681
682                                     }
683                                     else { //included this so
        that the delay between repetitions wont be so big
684                                     current4[i] =
current4[i] * ((repetitonAmpRatio[channel]*10)/ (repetitonAmpRatio[channel]
]*10));
685                                     }
686
687                                     data = (current4[i] & 0
xFF); // least significant byte (8-bit from the right)
688                                     addressData = (current4[i
] >> 8) + 0xD0; // shift to get the remaining 4-bits of the
12-bit
689                                     // for the DAC D and when
        it is alone fire need to add DAC:11 and OP:01 to addressData
690
691                                     while(!(SPIO_S));
692                                     SPIO_DH=addressData; //
DAC select A[1:0], State select OP[1:0], Data bits D[11:8]
693                                     SPIO_DL=data; // Data
        bits D[7:0]
694
        }
695
696                                     IN14_Clr();
697                                     IN24_Clr();
698
699                                     data = (0x00 & 0xFF); // least
        significant byte (8-bit from the right)

```



```

740                                     else if(controller1[i] ==
SWITCHON10 && rep1!=2){ //negative phase
741                                     IN11_Clr();
742                                     IN21_Set();
743                                     rep1 = 2;
744                                     }
745
746
747                                     if (pwr > 0 && invRatio
[1] == 1 && nRepts <= RepsMax[1]) {
748                                     current1[i] =
current1[i] * (repetitonAmpRatio[1]/10);
749
750                                     }
751                                     else if (pwr > 0 &&
invRatio[1] == -1 && nRepts <= RepsMax[1]) {
752                                     current1[i] =
current1[i] / (repetitonAmpRatio[1]/10);
753
754                                     }
755                                     else { //included this so
that the delay between repetitions wont be so big
756                                     current1[i] =
current1[i] * ((repetitonAmpRatio[1]*10)/ (repetitonAmpRatio[1]*10));
757                                     }
758
759                                     data = (current1[i] & 0xFF);
// least significant byte (8-bit from the right)
760                                     addressData = (current1[i] >>
8); // shift to get the remaining 4-bits of the 12-bit
761                                     // for the DAC A and when it is
synchronous fire no need to add nothing to addressData
762
763                                     while(!(SPI0_S));
764                                     SPI0_DH=addressData; //DAC
select A[1:0], State select OP[1:0], Data bits D[11:8]
765                                     SPI0_DL=data; // Data bits D
[7:0]
766
767                                     }
768
769
770
771                                     if (nRepts < nRepetitions[2]){
772
773                                     if(controller2[i] == SWITCHOFF
&& rep2!=0){
774                                     IN12_Clr();

```

```

775                                     IN22_Clr();
776                                     rep2 = 0;
777                                     }
778                                     else if(controller2[i] ==
SWITCHON01 && rep2!=1){ //positive phase
779                                     IN12_Set();
780                                     IN22_Clr();
781                                     rep2 = 1;
782                                     }
783                                     else if(controller2[i] ==
SWITCHON10 && rep2!=2){ //negative phase
784                                     IN12_Clr();
785                                     IN22_Set();
786                                     rep2 = 2;
787                                     }
788
789                                     if (pwr > 0 && invRatio
[2] == 1 && nRepts <= RepsMax[2]) {
790                                     current2[i] =
current2[i] * (repetitonAmpRatio[2]/10);
791
792                                     }
793                                     else if (pwr > 0 &&
invRatio[2] == -1 && nRepts <= RepsMax[2]) {
794                                     current2[i] =
current2[i] / (repetitonAmpRatio[2]/10);
795
796                                     }
797                                     else { //included this so
that the delay between repetitions wont be so big
798                                     current2[i] =
current2[i] * ((repetitonAmpRatio[2]*10) / (repetitonAmpRatio[2]*10));
799                                     }
800
801                                     // for the DAC B and when it is
synchronous fire no need to add nothing to addressData
802                                     data = (current2[i] & 0xFF);
// least significant byte (8-bit from the right)
803                                     addressData = (current2[i] >>
8) + 0x40; //adds DAC:01 and OP:00
804
805                                     while(!(SPI0_S));
806                                     SPI0_DH=addressData; //DAC
select A[1:0], State select OP[1:0], Data bits D[11:8]
807                                     SPI0_DL=data; // Data bits D
[7:0]
808
809                                     }

```

```

810
811
812
813                                     if (nRepts < nRepetitions[3]){
814
815                                     if(controller3[i] == SWITCHOFF
&& rep3!=0){
816
817                                         IN13_Clr();
818                                         IN23_Clr();
819                                         rep3 = 0;
820                                     }
SWITCHON01 && rep3!=1){ //positive phase
821
822                                         IN13_Set();
823                                         IN23_Clr();
824                                         rep3 = 1;
825                                     }
SWITCHON10 && rep3!=2){ //negative phase
826
827                                         IN13_Clr();
828                                         IN23_Set();
829                                         rep3 = 2;
830                                     }
831
832                                     if (pwr > 0 && invRatio
[3] == 1 && nRepts <= RepsMax[3]) {
833
834                                         current3[i] =
current3[i] * (repetitonAmpRatio[3]/10);
835                                     }
836                                     else if (pwr > 0 &&
invRatio[3] == -1 && nRepts <= RepsMax[3]) {
837
838                                         current3[i] =
current3[i] / (repetitonAmpRatio[3]/10);
839                                     }
840                                     else { //included this so
that the delay between repetitions wont be so big
841
842                                         current3[i] =
current3[i] * ((repetitonAmpRatio[3]*10)/ (repetitonAmpRatio[3]*10));
843                                     }
844                                     // for the DAC C and when
it is synchronous fire have to add address
845                                     data = (current3[i] & 0xFF);
// least significant byte (8-bit from the right)

```

```

846                                     addressData = (current3[i] >>
8) + 0x80;           //adds DAC:10 and OP:00
847
848                                     while(!(SPI0_S));
849                                     SPI0_DH=addressData; //DAC
select A[1:0], State select OP[1:0], Data bits D[11:8]
850                                     SPI0_DL=data; // Data bits D
[7:0]
851
852                                     }
853
854
855
856                                     if (nRepts < nRepetitions[4]){
857
858                                     if(controller4[i] ==
SWITCHOFF && rep4!=0){
859                                     IN14_Clr();
860                                     IN24_Clr();
861                                     rep4 = 0;
862                                     }
863                                     else if(controller4[i] ==
SWITCHON01 && rep4!=1){ //positive phase
864                                     IN14_Set();
865                                     IN24_Clr();
866                                     rep4 = 1;
867                                     }
868                                     else if(controller4[i] ==
SWITCHON10 && rep4!=2){ //negative phase
869                                     IN14_Clr();
870                                     IN24_Set();
871                                     rep4 = 2;
872                                     }
873
874
875                                     if (pwr > 0 && invRatio
[4] == 1 && nRepts <= RepsMax[4]) {
876                                     current4[i] =
current4[i] * (repetitonAmpRatio[4]/10);
877
878                                     }
879                                     else if (pwr > 0 &&
invRatio[4] == -1 && nRepts <= RepsMax[4]) {
880                                     current4[i] =
current4[i] / (repetitonAmpRatio[4]/10);
881
882                                     }

```

```

883                                     else { //included this so
      that the delay between repetitions wont be so big
884                                     current4[i] =
current4[i] * ((repetitonAmpRatio[4]*10)/ (repetitonAmpRatio[4]*10));
885                                     }
886
887                                     // for the DAC D and when
      it is synchronous fire have to add address and update outputs
888                                     data = (current4[i] & 0
xFF); // least significant byte (8-bit from the right)
889                                     addressData = (current4[i
] >> 8) + 0xD0; //adds DAC:11 and OP:01
890
891                                     while(!(SPIO_S));
892                                     SPIO_DH=addressData; //
DAC select A[1:0], State select OP[1:0], Data bits D[11:8]
893                                     SPIO_DL=data; // Data
bits D[7:0]
894
895                                     }
896
897
898                                     /// This condition is here for
the case when stimulation in some channel is shorter than others, to reassure
the output ///
899                                     /// the will be 0. These
conditions are of most importance in the case where Channel 4 doesn't exist
because otherwise it is ///
900                                     /// the one which updates DAC
outputs and if stops occurring the digital order to update DAC outputs would
also not occur ///
901
902                                     if (nRepts >= nRepetitions[1]){
903
904                                     IN11_Clr();
905                                     IN21_Clr();
906
907                                     data = (0x00 & 0xFF);
// least significant byte (8-bit from the right)
908                                     addressData = (0x00 >>
8); // shift to get the remaining 4-bits of the 12-bit
909                                     // for the DAC A and
when it is synchronous fire no need to add nothing to addressData
910
911                                     while(!(SPIO_S));
912                                     SPIO_DH=addressData;
//DAC select A[1:0], State select OP[1:0], Data bits D[11:8]

```

```
913                                     SPI0_DL=data; // Data
    bits D[7:0]
914
915                                     }
916
917                                     if (nRepts >= nRepetitions[2]){
918                                         IN12_Clr();
919                                         IN22_Clr();
920
921                                     data = (0x00 & 0xFF);
    // least significant byte (8-bit from the right)
922                                     addressData = (0x00 >>
    8) + 0x40; //adds DAC:01 and OP:00
923
924                                     while(!(SPI0_S));
925                                     SPI0_DH=addressData;
    //DAC select A[1:0], State select OP[1:0], Data bits D[11:8]
926                                     SPI0_DL=data; // Data
    bits D[7:0]
927                                     }
928
929                                     if (nRepts >= nRepetitions[3]){
930                                         IN13_Clr();
931                                         IN23_Clr();
932
933                                     data = (0x00 & 0xFF);
    // least significant byte (8-bit from the right)
934                                     addressData = (0x00 >>
    8) + 0x80; //adds DAC:10 and OP:00
935
936                                     while(!(SPI0_S));
937                                     SPI0_DH=addressData;
    //DAC select A[1:0], State select OP[1:0], Data bits D[11:8]
938                                     SPI0_DL=data; // Data
    bits D[7:0]
939                                     }
940
941                                     if (nRepts >= nRepetitions[4] ||
    nRepetitions[4] == 0){
942                                         IN14_Clr();
943                                         IN24_Clr();
944
945                                     data = (0x00 & 0xFF);
    // least significant byte (8-bit from the right)
946                                     addressData = (0x00 >> 8)
    + 0xD0; //adds DAC:11 and OP:01
947
948                                     while(!(SPI0_S));
```



```

991                                     if (pwr > 0 && invRatio[1] == 1
&& nRepts <= RepsMax[1]) {
992                                     current1[i] = current1[i]
* (repetitonAmpRatio[1]/10);
993
994                                     }
995                                     else if (pwr > 0 && invRatio[1]
== -1 && nRepts <= RepsMax[1]) {
996                                     current1[i] = current1[i]
/ (repetitonAmpRatio[1]/10);
997
998                                     }
999                                     else { //included this so that
the delay between repetitions wont be so big
1000                                     current1[i] = current1[i]
* ((repetitonAmpRatio[1]*10)/ (repetitonAmpRatio[1]*10));
1001                                     }
1002
1003                                     data = (current1[i] & 0xFF);
// least significant byte (8-bit from the right)
1004                                     addressData = (current1[i] >> 8)
+ 0x10; // shift to get the remaining 4-bits of the 12-bit
1005                                     // for the DAC A and when it is
alone fire need to add DAC:00 and OP:01 to addressData
1006
1007                                     while(!(SPIO_S));
1008                                     SPIO_DH=addressData; //DAC select
A[1:0], State select OP[1:0], Data bits D[11:8]
1009                                     SPIO_DL=data; // Data bits D
[7:0]
1010                                     }
1011
1012                                     IN11_Clr();
1013                                     IN21_Clr();
1014
1015                                     data = (0x00 & 0xFF); // least
significant byte (8-bit from the right)
1016                                     addressData = (0x00 >> 8) + 0x10;
// shift to get the remaining 4-bits of the 12-bit
1017                                     // for the DAC A and when it is alone
fire need to add DAC:00 and OP:01 to addressData
1018
1019                                     while(!(SPIO_S));
1020                                     SPIO_DH=addressData; //DAC select A
[1:0], State select OP[1:0], Data bits D[11:8]
1021                                     SPIO_DL=data; // Data bits D[7:0]
1022
1023                                     nRepts++;

```

```

1024                                     //// WAIT FOR INTERSTIMULUS TIME ////
1025                                     WAIT1_Waitus(interstimulusTime[1]);
1026                                     }
1027
1028
1029                                     //// WAIT FOR TIME_LAG ///
1030                                     WAIT1_Waitms(timeLag);
1031
1032                                     nRepts = 0;
1033                                     while (nRepts < nRepetitions[2]){
1034
1035                                         i = 0;
1036                                         rep = 0;
1037                                         for (i = 0; i <= (n-1); i++) {
1038
1039                                             if(controller2[i] == SWITCHOFF &&
1040 rep!=0){
1041
1042                                                 IN12_Clr();
1043                                                 IN22_Clr();
1044                                                 rep = 0;
1045                                             }
1046                                             else if(controller2[i] ==
1047 SWITCHON01 && rep!=1){ //positive phase
1048
1049                                                 IN12_Set();
1050                                                 IN22_Clr();
1051                                                 rep = 1;
1052                                             }
1053                                             else if(controller2[i] ==
1054 SWITCHON10 && rep!=2){ //negative phase
1055
1056                                                 IN12_Clr();
1057                                                 IN22_Set();
1058                                                 rep = 2;
1059                                             }
1060
1061                                             if (pwr > 0 && invRatio[2] == 1
1062 && nRepts <= RepsMax[2]) {
1063
1064                                                 current2[i] = current2[i]
1065 * (repetitonAmpRatio[2]/10);
1066                                             }
1067                                             else if (pwr > 0 && invRatio[2]
1068 == -1 && nRepts <= RepsMax[2]) {
1069
1070                                                 current2[i] = current2[i]
1071 / (repetitonAmpRatio[2]/10);
1072                                             }
1073

```

```

1064         else { //included this so that
the delay between repetitions wont be so big
1065             current2[i] = current2[i]
* ((repetitonAmpRatio[2]*10) / (repetitonAmpRatio[2]*10));
1066         }
1067
1068         data = (current2[i] & 0xFF);
// least significant byte (8-bit from the right)
1069         addressData = (current2[i] >> 8)
+ 0x50;           // shift to get the remaining 4-bits of the 12-bit
1070                 // for the DAC B and when it is
alone fire need to add DAC:01 and OP:01 to addressData
1071
1072                 while(!(SPIO_S));
1073                 SPIO_DH=addressData; //DAC select
A[1:0], State select OP[1:0], Data bits D[11:8]
1074                 SPIO_DL=data;    // Data bits D
[7:0]
1075             }
1076
1077             IN12_Clr();
1078             IN22_Clr();
1079
1080             data = (0x00 & 0xFF); // least
significant byte (8-bit from the right)
1081             addressData = (0x00 >> 8) + 0x50;
//adds DAC:01 and OP:00
1082
1083             while(!(SPIO_S));
1084             SPIO_DH=addressData; //DAC select A
[1:0], State select OP[1:0], Data bits D[11:8]
1085             SPIO_DL=data;    // Data bits D[7:0]
1086
1087             nRepts++;
1088             //// WAIT FOR INTERSTIMULUS TIME ////
1089             WAIT1_Waitus(interstimulusTime[2]);
1090         }
1091
1092
1093         //// WAIT FOR TIME_LAG ///
1094         WAIT1_Waitms(timeLag);
1095
1096         nRepts = 0;
1097         while (nRepts < nRepetitions[3]){
1098             i = 0;
1099             rep = 0;
1100             for (i = 0; i <= (n-1); i++) {
1101

```

```

1102                                     if(controller3[i] == SWITCHOFF &&
rep!=0){
1103                                     IN13_Clr();
1104                                     IN23_Clr();
1105                                     rep = 0;
1106                                     }
1107                                     else if(controller3[i] ==
SWITCHON01 && rep!=1){ //positive phase
1108                                     IN13_Set();
1109                                     IN23_Clr();
1110                                     rep = 1;
1111                                     }
1112                                     else if(controller3[i] ==
SWITCHON10 && rep!=2){ //negative phase
1113                                     IN13_Clr();
1114                                     IN23_Set();
1115                                     rep = 2;
1116                                     }
1117
1118
1119                                     if (pwr > 0 && invRatio[3] == 1
&& nRepts <= RepsMax[3]) {
1120                                     current3[i] = current3[i]
* (repetitonAmpRatio[3]/10);
1121
1122                                     }
1123                                     else if (pwr > 0 && invRatio[3]
== -1 && nRepts <= RepsMax[3]) {
1124                                     current3[i] = current3[i]
/ (repetitonAmpRatio[3]/10);
1125
1126                                     }
1127                                     else { //included this so that
the delay between repetitions wont be so big
1128                                     current3[i] = current3[i]
* ((repetitonAmpRatio[3]*10)/ (repetitonAmpRatio[3]*10));
1129                                     }
1130
1131                                     data = (current3[i] & 0xFF);
// least significant byte (8-bit from the right)
1132                                     addressData = (current3[i] >> 8)
+ 0x90; // shift to get the remaining 4-bits of the 12-bit
1133                                     // for the DAC C and when it is
alone fire need to add DAC:10 and OP:01 to addressData
1134
1135                                     while(!(SPI0_S));
1136                                     SPI0_DH=addressData; //0xC3 //DAC
select A[1:0], State select OP[1:0], Data bits D[11:8]

```

```

1137             SPIO_DL=data;    //0x3D // Data
bits D[7:0]
1138         }
1139
1140         IN13_Clr();
1141         IN23_Clr();
1142
1143         data = (0x00 & 0xFF);    // least
significant byte (8-bit from the right)
1144         addressData = (0x00 >> 8) + 0x90;
//adds DAC:10 and OP:00
1145
1146         while(!(SPIO_S));
1147         SPIO_DH=addressData; //DAC select A
[1:0], State select OP[1:0], Data bits D[11:8]
1148         SPIO_DL=data;    // Data bits D[7:0]
1149
1150         nRepts++;
1151         //// WAIT FOR INTERSTIMULUS TIME ////
1152         WAIT1_Waitus(interstimulusTime[3]);
1153
1154     }
1155
1156     //// WAIT FOR TIME_LAG ///
1157     WAIT1_Waitms(timeLag);
1158
1159
1160     nRepts = 0;
1161     while (nRepts < nRepetitions[4]){
1162
1163         i = 0;
1164         rep = 0;
1165         for (i = 0; i <= (n-1); i++) {
1166
1167             if(controller4[i] == SWITCHOFF &&
rep!=0){
1168                 IN12_Clr();
1169                 IN22_Clr();
1170                 rep = 0;
1171             }
1172             else if(controller4[i] ==
SWITCHON01 && rep!=1){ //positive phase
1173                 IN12_Set();
1174                 IN22_Clr();
1175                 rep = 1;
1176             }
1177             else if(controller4[i] ==
SWITCHON10 && rep!=2){ //negative phase

```



```

1212             SPIO_DH=addressData; //DAC select A
[1:0], State select OP[1:0], Data bits D[11:8]
1213             SPIO_DL=data; // Data bits D[7:0]
1214
1215             nRepts++;
1216             //// WAIT FOR INTERSTIMULUS TIME ////
1217             WAIT1_Waitus(interstimulusTime[4]);
1218         }
1219
1220     }
1221
1222
1223         // Turns OFF all the switches - just as an insurance
1224         IN11_Clr();
1225         IN21_Clr();
1226         IN12_Clr();
1227         IN22_Clr();
1228         IN13_Clr();
1229         IN23_Clr();
1230         IN14_Clr();
1231         IN24_Clr();
1232
1233         // to power down the outputs
1234         addressData = (current1[i] >> 8) + 0x70; //adds DAC:00 and
OP:11
1235         while(!(SPIO_S));
1236         SPIO_DH=addressData; //0xC3 //DAC select A[1:0], State select
OP[1:0], Data bits D[11:8]
1237         SPIO_DL=data; //0x3D // Data bits D[7:0]
1238
1239         //BLUE_SetVal(BLUE_DeviceData); /* turn off blue LED */
1240         RED_SetVal(RED_DeviceData);
1241
1242     }
1243
1244 }
1245
1246 /** Don't write any code pass this line, or it will be deleted during code
generation. ***/
1247 /** RTOS startup code. Macro PEX_RTOS_START is defined by the RTOS component.
DON'T MODIFY THIS CODE!!! ***/
1248 #ifdef PEX_RTOS_START
1249     PEX_RTOS_START(); /* Startup of the selected RTOS. Macro is
defined by the RTOS component. */
1250 #endif
1251 /** End of RTOS startup code. ***/
1252 /** Processor Expert end of main routine. DON'T MODIFY THIS CODE!!! ***/
1253 for(;;){}

```



```
1254  /** Processor Expert end of main routine. DON'T WRITE CODE BELOW!!! **/  
1255  } /** End of main routine. DO NOT MODIFY THIS TEXT!!! **/  
1256  
1257  /* END main */  
1258  /*!  
1259  ** @}  
1260  */  
1261  /*  
1262  ** #####  
1263  **  
1264  **      This file was created by Processor Expert 10.3 [05.09]  
1265  **      for the Freescale Kinetis series of microcontrollers.  
1266  **  
1267  ** #####  
1268  */
```
