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Thermoplastic Resins used in Dentistry

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Abstract

Thermoplastic materials such as polyamides (nylon), acetal resins, epoxy resins, polystyrene, polycarbonate resins, polyurethane and acrylic thermoplastic resins were introduced in dentistry as an alternative to classic resins, which have major disadvantages such as the toxicity of the residual monomer, awkward wrapping system and difficult processing.

Indications for thermoplastic resins include partial dentures, preformed clasps, partial denture frameworks, temporary or provisional crowns and bridges, full dentures, orthodontic appliances, anti-snoring devices, different types of mouth guards and splints. Some flexible myofunctional therapy devices, used for orthodontic purposes, may also be made of thermoplastic silicone polycarbonate-urethane.

The main characteristics of thermoplastic resins used in dentistry are as follows: they are monomer free and consequently nontoxic and nonallergenic, they are injected by using special devices, they are biocompatible, they have enhanced esthetics and they are comfortable to wear.

Keywords: Thermoplastic resins, injection devices, metal-free removable partial dentures

1. Introduction

Continuous development and progress of polymer's industry with applications in general and dental medicine was of great importance for the health domain. Using various types of resins for restorations in the oral cavity is beneficial from childhood till geriatric period [1-4].



Thermopolymerizable acrylic resins were first used in dental technique in 1936, this being a great step forward. Acrylic resins are also known as polymethylmethacrylate or PMMA. These synthetically obtained materials can be modeled, packed or injected into molds during the plastic phase and become solid after chemical polymerization [5, 6]. Thermopolymerisable acrylic resins have many disadvantages as increased porosity, high water retention, volume variations and irritating effect due to the residual monomer, awkward wrapping system and difficult processing. Because of these, once polymers developed, alternative materials such as polyamides (nylon), acetal resins, epoxy resins, polystyrene, polycarbonate resins etc. [7-9] came on the market.

The main characteristics of the thermoplastic resins used in dentistry are as follows: they are monomer-free and consequently nontoxic and nonallergenic, they are injected by using special devices, they are biocompatible, they have enhanced esthetics and they are comfortable to wear [10].

2. Types of thermoplastic resins used in dentistry

The classification of resins according to DIN EN ISO 1567 is presented in Table 1:

Type	Class (manufacturing)	Group (presentation form)		
Type 1	Thermopolymerizable resins (>65°C)	Group 1: bicomponent powder and liquid Group 2: monocomponent		
Type 2	Autopolymerizable resins (<65°C)	Group 1: bicomponent powder and liquid Group 2: bicomponent powder and casting liquid		
Type 3	Thermoplastic resins	Monocomponent system grains in cartridges		
Type 4	Light-cured resins	Monocomponent system		
Type 5	Microwave cured resins	Bicomponent system		

Table 1. The classification of resins according to DIN EN ISO 1567

Among the technologies for manufacturing removable complete and partial dentures we distinguish: heat-curing, self-curing, injection, light-curing, casting and microwave use [11].

Thermoplastic resins may be classified by their composition, as acetal resins, polycarbonate resins (belonging to the group of polyester resins), acrylic resins and polyamides (nylons).

The use of thermoplastic resins in dental medicine is continuously growing. The material is thermally plasticized and no chemical reaction takes place. The injection of plasticized resins into a mold represents a new technology in manufacturing complete and removable partial dentures [12].

At present, due to successive alterations in the chemical composition, thermoplastic materials are suitable for manufacturing removable partial dentures with no metallic components, resulting in the so-called "metal-free removable partial dentures" [13].

Indications for thermoplastic resins include removable partial dentures, preformed clasps [14], partial denture frameworks, temporary or provisional crowns and bridges, complete dentures, orthodontic appliances, anti-snoring devices, different types of mouth guards and splints. Some flexible myofunctional therapy devices, used for orthodontic purposes, may also be made of thermoplastic silicone polycarbonate-urethane.

2.1. Thermoplastic acetal

Thermoplastic acetal is a poly(oxy-methylene)-based material, which as a homopolymer has good short-term mechanical properties but as a copolymer has better long-term stability [15]. Due to its resistance to wear and fracture, combined with a certain amount of flexibility, acetal resin is an ideal material for preformed clasps for partial dentures, single-pressed unilateral partial dentures, partial denture frameworks (Figure 1), provisional bridges, occlusal splints and implant abutments, artificial teeth for removable dentures and orthodontic appliances [16].

Because of their resistance to occlusal wear, acetal resins are also well suited for maintaining vertical dimension during provisional restorative therapy. Acetal is not translucent and does not match the esthetic appearance of thermoplastic acrylic and polycarbonate [17].



Figure 1. Removable partial denture with acetal frame and clasps

2.2. Thermoplastic polyamide (nylon)

Thermoplastic polyamide (nylon) is a resin derived from diamine and dibasic acid monomers. Versatility is one of its characteristics and makes it suitable for various applications. Nylon

exhibits high flexibility, physical strength, heat and chemical resistance. It can be easily modified to increase stiffness and wear resistance. Because of its excellent balance of strength, ductility and heat resistance, nylon is an outstanding candidate for metal replacement applications [18]. Nylon is mainly used for tissue supported removable dentures. Its stiffness makes it unsuitable for usage as occlusal rests or denture elements that need to be rigid [7, 13]. Because it is flexible, it cannot maintain vertical dimension when used in direct occlusal forces. Adjustment and polishing is difficult but provides excellent esthetics due to its semitranslucency [19, 20].

Nylon is specially indicated for patients allergic to methyl metacrylate, being monomer-free, lightweight and impervious to oral fluids [21]. Some may also be combined with a metal framework (Figure 2).



Figure 2. Removable partial denture of polyamide combined with metal

Comparative properties of thermoplastic acetal and polyamide, the two types of resins suitable for manufacturing removable partial dentures, are shown in Table 2.

Resin type	Main substance	Resistance	Durity	Flexibility	Esthetics	Biocompatibility
Acetalic resin	polioximetylen	very good	very high	medium	good	very good
Polyamidic resin	diamine	good	high	medium or very high	very good	very good

Table 2. Comparative aspects of acetalic and polyamidic thermoplastic resins

2.3. Thermoplastic polyester

Thermoplastic polyester resins are also used in dentistry. They melt between 230°C and 290°C and the technology implies casting into molds. Polycarbonate resins are particularly polyester

materials. They have good fracture strength and flexibility, but the wear resistance is lower 213aThermoplastis.polyesterbonates have a natural translucency and finishes very well, which recommends them for temporary restorations, but they are not suitable for partial denture Thermoplastic polyester resins are also used in dentistry. They melt between 230°C and 290°C and the frameworks [22] frameworks [22], technology implies casting into molds. Polycarbonate resins are particularly polyester materials. They have good fracture strength and flexibility, but the wear resistance is lower than acetal resins. 2 dy Tabona or lative acrydated translucency and finishes very well, which recommends them for temporary restorations, but they are not suitable for partial denture frameworks [22].

Thermoplastic acrylate consists of fully polymerized acrylate, its base component being acrylic. This material was developed for manufacturing complete dentures. It is not elastic, but Thermoplastic acrylate consists of fully polymerized acrylate, its base component being methylits flexibility makes it practically unbreakable. The material has long-term stability, its surface metacrylate, the special blend of polymers giving it the highest impace rating of any acrylic. This ataucture being clease and amount turing to the lets and a chief the property of the lets and th is practically durbleakhout unthe asaterial gas delignization and tability abecause uncabering tension and smooth. Duritoath bobscoes of residual monomerfits biocompatibility in yone soud. The 1deau re has very good long-term adaptability because water retention is limited. You can bounce such denture off the floor without cracking the base [7,21,23]. 2.5. Presentation form and injection

2.5 Presentation form and injectionThermoplastic materials can be polymerized or prepolymerized and they can be found in Themson a form markital dran molecular riveight, prepared menterpand the cartiful growth at in ligain ate florage iterriors (Figure and A). weight, already wrapped in cartridges that eliminate dosage errors (Figure 3).



Figure 3. (a, b) Cartridges of different thermoplastic resins (c) The granular aspect of the material

Figure 3. (a, b) Cartridges of different thermoplastic resins (c) The granular aspect of the material They exhibit a high rigidity despite their low molecular weight. Their plasticizing temperature is low (200°C=350°C). hThermal interioristation etakes whas recial the vines realist ward in the empterial is injected under pressure into a mold without any chemical reactions. After heating the metallic cartridges containing thermoplastic grains are set in place into the injecting unit and the plasticized material is injected under pressure into a mold, without any chemical reactions. After heating resin is forced into the mold at a pressure of 6-8 bars. Pressure, temperature and injecting time are the matelling contributes by the injectific umendenticies obtained estrip unla recintorable injectification. estbethes plat tionecompatibility (%) 12 mold at a pressure of 6-8 bars. Pressure, temperature Injecting thermonlastic resimminate carolds in motta dominan it related by in. Contact laboratories decause the need of expensive equipment and this could be a disadvantage lity [7, 12, 13, 22]. The special injection devices we use are Polyapress (Bredent) and R-3C (Flexite) injectors (Figure 4).

Injecting thermoplastic resins into molds is not a common technology in dental laboratories because the need of expensive equipment and this could be a disadvantage.

The special injection devices we use are Polyapress (Bredent) and R-3C (Flexite) injectors (Figure 4).



tree and consequently nontoxic and nonallergenic, they are injected by using special devices, they are 3. Prosthotacolderejaste made defilencem oplastic resines wear. Figure 4x fairlike Rolly appears juicities in additionally vice in Bradentil (higher Rastinian Chief lexite)

partial edentations, with removable partial dentures without metallic framework, or combining the The maintain denture of the properties o



saddles (Figure 4). However, the resistance values for the acetal resin framework do not reach those of a metal one [16], consequently the main connector, the classes and the spure need to be oversized figure 5 in the classes and the spure need to be oversized figure 5 in the classes are connected to the consequently the main connected that has five preset programs, as

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3.1 Removable partial dentures with acetal framework

The acetal resin has optimal physical and chemical properties and it is indicated in making frameworks and clasps for removable partial dentures, being available in tooth color and pink [12]. Experimentally, in some cases, we combined an acetal resin frames with classic acrylic resins for the saddles (Figure 4). However, the resistance values for the acetal resin framework do not reach those of a metal one [16], consequently the main connector, the clasps and the spurs need to be oversized

3.1. Removable partial dentures with acetal framework

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Figure Figure & Actal framework and class and removable partial dentures with acetal framework and clasps

The maintenance, support and stabilizing systems used are metal-free ones. The maintenance, support and stabilizing systems used are metal-free ones.

The significant aspects to the technical extract of the technology of governmental danturated and extract of the significant aspects to the technical extraction of the significant aspects to the significan thermoplastic materials are described.

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In order to assess its arms of the clasp are placed a parallelograph analysis is made (Figure 8). The abutment teem are selected and the position of the cast is chosen and recorded so that a favorable path of insertion is obtained. To record the position of the cast tripod marks are used. The contour heights on the abutment teeth and the retentive muco-osseous tissues are marked. The abutments undercuts are measured and the engagement of the terminal third of the retentive arms of the clasps is established.

After the parallelograph analysis is carried out, the future frame design is drawn, including all extensions of saddles, major connector, retentive and bracing arms of the clasps, occlusal rests and minor connectors of Ackers circumferential clasps on abutment teeth. The design starts with the saddles, following the main connector, the retentive and opposing clasp arms, the spurs and the secondary connectors of the Ackers circular clasps [12, 13].

In order to assess its retentiveness and to determine the place where the active arms of the clasp are placed a parallelograph analysis is made (Figure 8). The abutment teeth are selected and the position of the cast is chosen and recorded so that a favorable path of insertion is obtained. To record the position of the cast tripod marks are used. The contour heights on the abutment teeth and the retentive muco-osseous tissues are marked. The abutments undercuts are measured and the engagement of the terminal third of the retentive arms of the clasps is established.

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After designing the framework, the master model is prepared for duplication, including After liestigning the traffic wire, the hospital the prepared plans the giogram with the prepared plans the giogram by the giogram

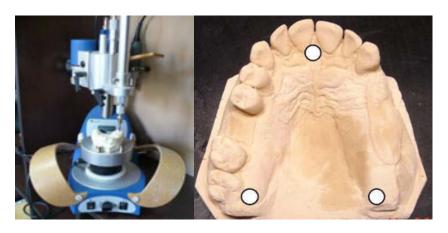


Figure 8. Parallelograph analysis

Figure 8. Parallelograph analysis



Block-out wax is applied between teem cervices and gingival margin of the drawing representing the clasps arms. The block-out wax meets the spacing wax in a smooth joint.

In order to duplicate the model, a vinyl-polysiloxane silicone placed in a flask is used. After its setting, the duplicate model is poured (Figure 10), using class IV hard plaster.





Block-out wax is applied between retentivisation of the impled margin of the drawing representing the clasps arms. The block-out wax meets the spacing wax in a smooth joint. In order Block-out wax is applied between teeth cervices and gingival margin of the drawing representing the clasps arms. The block-out wax meets the spacing wax in a smooth joint. In order clasps arms, the block-out wax meets the spacing wax in a smooth joint. In oratting at the idea transportable partial (figure of the stines of special data of the its setting, the duplicate model is poured (Figure 10), using class IV hard plaster.

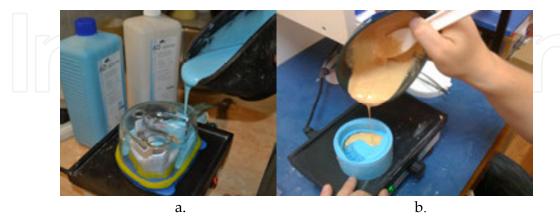


Figure 10. (a) Duplication of the model (b) Casting of the duplicate model using class IV hard plaster Figure 10. (a) Duplication of the model (b) Casting of the duplicate model using class IV hard plaster

The elements of removable partial denture's wax pattern are as follows (Figure 11a): the main connector, made of red wax (so that its thickness is twice as normal), the saddles and the Ackers
The elements of removable partial denture's wax pattern are as follows (Figure 11a): the main
circular clasps, made of blue wax. Injection bars are also required for those areas of the
connector, made of red wax (so that its thickness is twice as normal), the saddles and the Ackers
framework that are not visible in the finite piece. A large central shaft is necessary in order to
circular clasps, made of blue wax. Injection bars are also required for those areas of the framework
connect with the main connector, through which the initial injection takes place. Unlike the
that are not visible in the finite piece. A large central shaft is necessary in order to connect with the
main connector, through which the patterns of the metal-free framework have to be 50%
main connector, through which the initial injection takes place. Unlike the pattern of a metallic
framework, the patterns of the metal-free framework have to be 50% thicker (clasps, occlusal rests and major connected is performed using minor sprues of 2.5 mm calibrated wax connected Spruing the framework is performed using minor sprues of 2.5 mm calibrated wax connected to one major sprue (Figure 11a).



Figure gule (a) a Wrapping the awax pattern frame of the removable partial denture (b) Insulation of the investment

Surface tension reducing solution is applied and the wax pattern is then invested in a vaseline insulated aluminum flask (Figure 11b). Class III hard stone is used as an investment. The gypsum paste is poured into one of the two halves of the flask and the duplicated model containing the framework pattern with sprues attached is centrally dipped base-face down. After setting, the gypsum surface is insulated and the second half of the flask is assembled. Class III hard stone is once more anarad and the fleely is submarged in warm water in a thermostatic container. The two helves of the

Surface tension reducing solution is applied and the wax pattern is then invested in a vaseline insulated aluminum flask (Figure 11b). Class III hard stone is used as an investment. The gypsum paste is poured into one of the two halves of the flask and the duplicated model containing the framework pattern with sprues attached is centrally dipped base-face down. After setting, the gypsum surface is insulated and the second half of the flask is assembled. Class III hard stone is once more prepared and the flask is submerged in warm water in a thermostatic container. The two halves of the flask are disassembled and the wax is boiled out using clean hot water. The surface of the mold is then insulated and treated with a light-curing transparent varnish in order to obtain a shining aspect [12, 13].

Injection is carried out with the R-3C (Flexite) injector (Figure 4b), which does not take up much space as it can be mounted on a wall as well. The device has the following parameters: digital control, preset programs for different types of thermoplastic resins and programs that can be individually set by the user. The pressure developed is 6-8 Bar [23].



Figure 12. Schedule of "G" program of injecting the thermoplastic material (a) Start (b) Heating ooling (c) Injecting (d) Cooling

Before investing in remark, strews are loosened and the flask is gently disassembled (Figure 13) e the injecting pressure is according to procedure demands (7.2-7.5 Bar). Proheating temperature and time are also checked (15 minutes at 220°C). The selected cartridge (quantity and color) is



cartridge is separated and the flask is then released and pulled out. In order to achieve optimal quality of the solution of t

Before investment removal, screws are loosened and the flask is gently disassembled (Figure 13). Before investment removal, screws are loosened and the flask is gently disassembled (Figure 13).

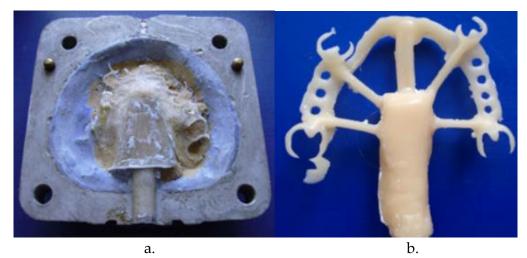


Figure 13. Disassembling the framework of the acetal resin removable partial denture (a) The Figure 13. Disassembling in a mount of the flask (b) Disassembling is complete. The flask (b) Disassembling is complete.

The sprues are cut off using low-pressure carbide and diamond burs to avoid overheating the material. Finishing and polishing is performed using soft brushes, ragwheel and polishing paste (Figure 14).

Disassembling the framework of the future removable partial denture is followed by matching it to the model, processing and finishing this component of the removable partial denture (Figure 15).

Once the framework is ready, the artificial teeth are set up. Wax patterns of the saddles are constructed by dropping pink wax over the framework. Teeth set up starts with the most mesial tooth, which is polished until it esthetically fits onto the arch [24].

After properly setting of all the teeth are the wax pattern is invested in order to obtain the acrylic saddles. An impression of the wax pattern placed on the master model is made by using a putty condensation silicone.

The sprues are cut off using low-pressure carbide and diamond burs to avoid overheating the material. Finishing and polishing is performed using soft brushes, ragwheel and polishing paste (Figure 14).



apolishing the acetal frameworkb(c) Special polishing paste c.

Figure 14. (a) Tools used for processing the acetal framework (b) Tools used for finishing and Disassemblings the frameworkliphidesting and the modely processing and distributions this component of the removable partial denture (Figure 15).

Disassembling the framework of the future removable partial denture is followed by matching it to the mo

Figure 15. (a) Matching the acetal framework to the model (b) The finished acetal framework Figure 15. (a) Matching the acetal framework to the model (b) The finished acetal framework Figure 15. (a) Matching the acetal framework to the model (b) The finished acetal framework

Once the framework is ready the artificial teeth are set up. Wax patterns of the saddles are constructed by drapping paths wax ever the framework is ready, the artificial teeth are set up. Wax patterns of the saddles are constructed by drapping paths wax ever the framework of the set up starts with the most mestal tooth, which is polished in the framework of the framework of the lateral sides of the impression After properly setting of all the feeth are the wax pattern is invested in order to drain the acceptance and the master model as imade by variety and the master model as imade by variety and place the model of the framework is placed and the impression set in its original place. It is condensationed to the departure is war appeal as usual, using rectangular flocks and a class II.

After sections supposed the denture is wrapped as usual using rectangular flasks and a class II are thomography districted penings and being control of the denture is wrapped as usual using rectangular flasks and a class II are thomography districted penings and being control of the denture set in the impression rectangular penings across the property of the denture of the denture of the impression of the denture is wrapped as usual penings of the impression of the denture is wrapped as usual penings of the denture of 50°C and a pressure of 6 bars for 10 minutes to avoid bubble development. Once the resin is cured,

and a pressure of 6 bars for 10 minutes to avoid bubble development. Once the resin is cured, the impression is removed [12, 13]. Burs, brushes, ragwheels and pumice are used to remove the excess, to polish and finish the removable partial denture (Figure 16b).



The cast is introduced into a heat-pressure-curing unit setting a temperature of 50°C and a pressure of 6 bars for Figure in the Wrapped was pattern with teeth (b) Partial dentures made of acetal resinand acrylicsion is removed 12,13 Burs, brushes, ragwheels and pumice are used to remove the excess, to polish and finish the removable partial denture (Figure 16b) red inside the impression through the lateral openings. The result is a consistent removable partial denture inverting a tenacroud picture function with the finishest 0.3-0.5 mm areas of clasps, which means the fective force the thinnest 0.3-0.5 mm areas of clasps, which means the fective force the impression is

removed [12,13]. Burs, brushes, ragwheels and pumice are used to remove the excess, to polish and

3.26 Remayable partial deatures made of different types of polyamides
10 vable partial dentures made of different types of polyamides
The result is a consistent removable partial denture with no macroscopic deficiency even in the 3.2 Remo

Makingest of Salari damenias conclusable which about three classical seguines and intermediary Making spolyamide resineremovable partial dentures dons not irequire so emany intermediary, steps as those madi 2018 protected representation made pointiffer for those of only a middle of a gry life identifies the with thermoplastic materials the difference procedure its used file lasts are made of the same material as the denture polyamide resin removable partial dentures does not require so many intermediary steps as using medium-low they believe the steps are all last the denture flow they believe the steps are using medium-low they believe the steps are similar to those followed for acrylic dentures, but with medium-low flexibility polyamide [12] (Figure 17) in the class are made of the same material as the denture base, when using superflexible polyamide or ready-made clasps, in the case of using

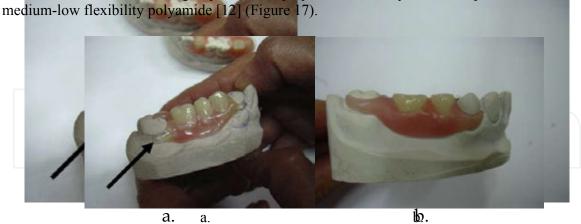


Figure 17. Figure and led remide auto yable and the hereweight has pre-formed class of the least as pade at the of the Figure 17. Polyamide removable partial personal material as the depture have specified as the

Using flexible polyamide is indicated in cases of retentive dental fields (Figure 18). Using flexible polyamide is indicated in cases of retentive dental fields (Figure 18). Using flexible polyamide is indicated in cases of retentive dental fields (Figure 18).

When manufacturing polyamidic dentures, the support elements blend in with the rest of the denture, as they are made of the same material [25, 26].



retentive tuberosity embedded in the flask (b) The denture immediately after unwrapping (c, d) The Figure 18. Removable partial with the flask (b) The identure immediately after unwrapping (c, d) The model with Figure 18. Removable partial with the flask (b) The identure immediately after unwrapping (c, d) The model with Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The Figure 18. Removable partial with the identure immediately after unwrapping (c, d) The iden

When manufacturing polyamidic dentures, the support elements blend in with the rest of the denture,



Figure 19. Medium-low flexibility thermoplastic polyamide denture

The superflexible polyamide resin is extremely elastic, virtually, unbreakable, monomer-free, lightweight and implications is extremely elastic. The meanly minore akable, monomer-free, lightweight and implications is extremely elastic. The meanly minore akable, monomer-free, lightweight and implications is extremely elastic. The meanly minore akable, monomer-free, lightweight and implications in the meanly of the meanly o

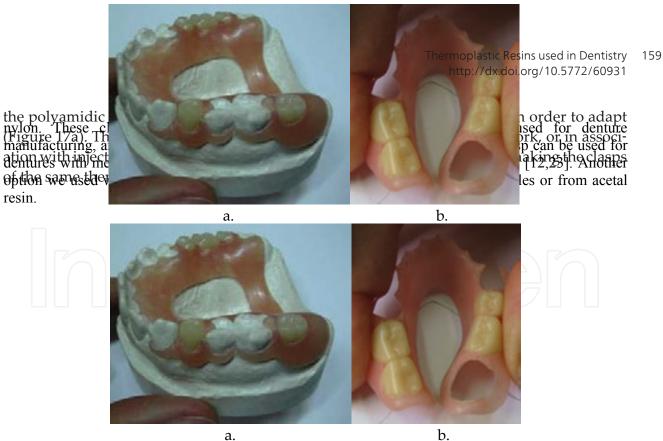


Figure 20 (a) Medium-low flexibility polyamide partial dentures (b) Superflexible polyamide partial dentures (b) Superflexible polyamide partial dentures



dentures Figure 21. (a) The superflexible polyamide denture (b) The final flexibility test

Figure 21. (a) The superflexible polyamide denture (b) The final flexibility test

3.3 Kemeny-type removable partial dentures made of acetal

3.3. Kemeny-type removable partial dentures made of

As an experiment, we managed partial reduced edentations with acetal Kemeny-type dentures (Figures 22 and 23) as an alternative to fixed social dentures, mainly in order to test the physiognomic aspect, having the advantage of a minimal loss of hard dental substance, located only at the level of the occlusal rims, in case of posterior teeth.

Figure 22 shows wax patterning aspects and manufacturing a molar unidental Kemeny denture of argual zesia) while bishes how at the way in the way in the third and the properties and the contract of the contra can be managed. The effectiveness of the technology is ensured by making artificial teeth of 8.3 Kamenyatypearemovable partial dentures made of acetal

160

As an experiment, we managed partial reduced edentations with acetal Kemeny-type dentures (Figures 22 and 23) as an alternative to fixed partial dentures, mainly in order to test the physiognomic aspect, having the advantage of a minimal loss of hard dental substance, located only at As an experiment, we managed partial reduced edentations with acetal Kemeny-type dentures the representative of the partial dentures, mainly in order to test the regure 22 and 23) as an alternative to fixed partial dentures, mainly in order to test the right of 22 shows wax patterning aspects and manufacturing a molar unidental Kemeny denture of physiognomic aspect, having the advantage of a minimal loss of hard dental substance, located only at acetal resin, while Figure 23 shows the way in which a frontal bidental edentation can be managed. The effectiveness of the technology is ensured by making artificial teeth of the same material. He was a property of the partial dental partial dental edentation of the same material. The effectiveness of the technology is ensured by making artificial teeth of the same material acetal resin while figure 23 is not translucent, it is mainly suitable for dealing with lateral edentations. It can, as the material is not translucent, it is mainly suitable for dealing with lateral edentations. It can, as the material is not translucent, it is mainly suitable for dealing with lateral edentations. It can,

As the material is not translucent, it is mainly suitable for dealing with lateral edentations. It can, however, be used temporarily, in the frontal area as well, in those clinical cases where short-term

esthetic aspect is irrelevant [12,23,27].



Figure 22. Kemeny dentures: (a) Unimglar denture wax pattern (b) Denture made of acetal resin

Figure 22. Kemeny dentures: (a) Unimolar denture wax pattern (b) Denture made of acetal resin



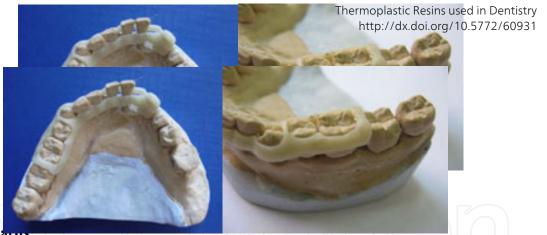
3.4 Splints made of acetar resin

Figure 23. Kemeny-type frontal denture Therhoplastic resins are also indicated for manufacturing antisnoring devices, different types of mouthquards and splints. Parodonthotic teeth after surgery need immobilization. We experimentally manufactured acted resin splints (Figure 24) which turned out to be a viable solution because it matches the color of the teeth and thereby represents a temporary postoperative esthetic choice thermoplastic resins are also indicated for manufacturing antisnoring devices, different types of morthqualating espirator Palsolindiotite teeth and activiting antisnoring devices, different types of morthqualating espirator Palsolindiotite teeth and activities out go by neviable solution absolution and the reby represents a temporary postoperative esthetic choice [18, 23].

3.5. Mouth guards

Mouth guards are dental appliances that can be manufactured using thermoplastic resins. The most satisfactory mouth protectors are custom-made mouth guards. This type of mouth guards is designed by the dentist. They adapt well and provide good retention and comfort. Being custom-made they interfere the least with speaking and have virtually no effect on breathing

rd



3.5 Mouth guarus

Nouth 4 und sure dental tappulatices that can be manufactured using thermoplastic resins.

The most satisfactory mouth protectors are custom-made mouth guards. This type of mouth guards is the four district of the grant with a peaking and have virtually no effect on breathing [28]. Custom-made Mouth guards in any be classified into two types, the year of mouth guards and fire pressure-laminated The most surjection, mouth guards are custom-made mouth guards and fire pressure-laminated The most surjection, mouth projectors are custom-made mouth guards and fire pressure-laminated The most surjection, mouth guards are custom-made mouth guards and fire pressure-laminated the mouth guards. They adapt well and provide good retention and company of mouth guards is is designed by the dentils. They adapt well and provide good retention and company of provide surjections and have a mouth guard and provide good retention and company of provide and they interfere the grant will be adapted they interfere the grant will be adapted to the provide grant gran

We manufactured laminated custom-made mouth guards for 3 layers, with the inner layer made of a thermoplastic polyurethane which increases discoloration resistance and creates a soft inner surface feel (Figure 25).

Figure 2

We manufactured annuated custom-made mouth guards for 3 layers with the inner layer Figure 25. Laminating the custom-made mouth guard. Custom made mouth guard made of a thermoplastic polyurethane which increases discoloration resistance and creates a **3.6 Mivimor tional chical (Figure 25**).

3.6. Myofunctional therapy devices

Controlling dentofacial growth interferences is an important issue. The negative effects of mouth breathing, abnormal lip and tongue function and incorrect swallowing patterns on craniofacial development in the mixed dentition period is well known. Correcting these myofunctional habits improves craniofacial growth and decreases the severity of malocclusion [12].

Myofunctional therapy retrains the muscles of swallowing, synchronizes the swallowing movements obtaining a normal resting posture of the tongue, lips, and jaw. Myofunctional therapy may be rescheduled before, during or after orthodontic treatment [30]. The most typical age range for this type of therapy is between 8 and 16 years.

The main objective of the myofunctional appliances is to eliminate oral dysfunction and to establish muscular balance. These appliances play a certain role in orthodontics because they are simple and economical. The selection of the cases needs to be thorough and the specialist needs to be well trained in their use.

The universal size products, suitable for children between 6 and 11 years old (mixed dentition stage), allow implementing the orthodontic treatment earlier and at lower cost. These are made of a flexible thermoplastic silicone polycarbonate-urethane, a ground-breaking copolymer that combines the biocompatibility and biostability of conventional silicone elastomers with the processability and toughness of thermoplastic polycarbonate-urethanes. This type of appliances has good in vitro and in vivo stability. Its strength is comparable to traditional polycarbonate-urethanes, and the biostability is due to the silicone soft segment and end groups. Various fabrication techniques may be used in order to obtain to different. Additional surface processing after fabrication is not needed [12].

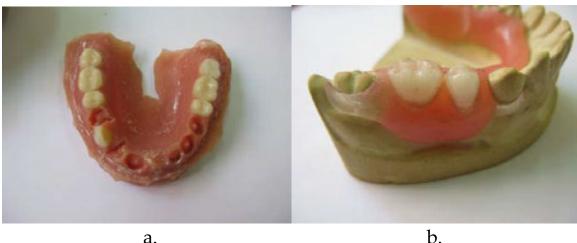
4. Errors in manufacturing thermoplastic resins dentures

Errors might occur when manufacturing thermoplastic resins dentures: the insufficient pressure at injection, which leads to lack of substance, poor polishing, or too thick saddles being some of the causes (Figure 26). These errors lead to deficiencies of the denture, which might be unusable because of esthetic deficiencies, occlusal dysmorphia, exaggerated elasticity, and decubitus areas [31].

5. Conclusions

Thermoplastics used in dentistry have known a great diversification in the last years. Processing principles are similar to the injecting technology of chemoplastics, the main difference consisting in their chemical composition, liquefying temperature of grains, injecting pressure and the fact that thermoplastic resins are monocomponent.

Errors might occur when manufacturing thermoplastic resins dentures: the insufficient pressure at injection, which leads to lack of substance, poor polishing, or too thick saddles being some of the causes (Figure 26). These errors lead to deficiencies of the denture, which reighted unusable because of esthetic deficiencies, occlusal dysmorphia, exaggerated elasticity, and decubitus areas [31].



a.

Figure 26. Errors that might occur when manufacturing dentures from thermoplastic resins (a) Lack Figure 26. Errors that might occur when manufacturing berpures from the might resins (a) Lack of substance (b) Poor polishing

5. Conclusions essing technology is based on the thermal plasticization of the material, in the absence of any chemical reaction. The technology of injection molding is not widely used in dental Thermoplasticsniquedaba ydentistrye haives kproiwhdavigreabudilversificaethore vin petropetaiste y earthe Processing principles attentional and the air feeting received logger of the main difference consisting in their chemical composition, liquefying temperature of grains, injecting pressure and the fact that thermoplastic resins arounonecomponentetal framework dentures, having the advantage of being

lightweight, flexible and much more comfortable for the patient. Metal-free removable partial dentures made of thermoplastic materials are biocompatible, nonirritant, sure, nontoxic, biologically inert, with superior esthetics, which make them rapidly integrate in dentomaxillary structure. They offer quality static and dynamic stability.

The clasps are made of the same material as the denture base or ready-made clasps from the same material may be used. Where the mechanical resistance of the structure comes first, the choice is an acetal resin for making the framework. Superflexible polyamide resin is especially indicated for retentive dental fields, which would normally create problems with the insertion and disinsertion of the removable partial dentures. The removable partial dentures with acetal resin frame are the most laborious to manufacture, requiring most working steps. Manufacturing the acetal framework is first, followed by the acrylic saddles and artificial teeth. A removable partial denture with an acetal resin frame is rapidly integrated into the dentomaxillary system and accepted by the patient. Such a removable denture is a comfortable solution for the partial edentulous patient, achieving the principles of static and dynamic maintenance and stability. These types of partial dentures are not bulky, the frameworks being 0.3-0.5 mm thin, and clasps are flexible and esthetic.

A particular advantage of a removable partial denture made of acetal resin applies to patients with large oral defects as a result of a maxillectomy procedure, who are due to have postoperative radiotherapy and need to have the density of the defect restored to ensure standardized radiation distribution. Different types of boluses may be used for restoration but a stent is usually needed as a support. Traditional metal-clasp retained stents are discarded in such cases as the clasps cause backscatter of the radiation beams. Acetal resin is a radiolucent material suitable for making a stent with clasps or even a removable partial denture to retain the bolus.

In the case of Kemeny-type acetalic dentures, the artificial teeth are made of the same material and in the same step as the rest of the denture. Because it is not translucent, its first indication is lateral edentations but it can be used for short periods, in the frontal area as well, if short-term esthetic aspect is not important.

Thermoplastic resins have several advantages: long-term performance, stability, resistance to deformation, resistance to wear, excellent tolerance, resistance to solvents, absence or low quantity of allergy-inducing residual monomer, and lack of porosity, thus preventing the development of microorganisms and deposits, all of which, together with maintaining size and color in time are very important characteristics, presenting a high degree of flexibility and resistance, permitting the addition of elastomers for increased elasticity or reinforcement with fiberglass, in order to increase their physical splinter quality; some of them can also be repaired or rebased.

The advantages of using the molding-injection system lay in the fact that the resin is delivered in a cartridge, thus excluding mixture errors with long-term shape stability, reduces contraction, and gives mechanical resistance to ageing.

As this class of materials, as well as the processing devices, has been continuously perfected, their future applicability in dental medicine will keep spreading.

Most probably, further chemical development of elastomeric and polymeric materials will enlarge the domain of clinical applications of thermoplastics in dentistry.

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