# WEARABLE CHEMICAL SENSORS: CHARACTERIZATION OF HEART RATE ELECTRODES USING ELECTROCHEMICAL IMPEDANCE SPECTROSCOPY

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# Introduction

Wearable monitoring systems have flooded the health and sports industry in recent years. With a continued focus on comfort and cross platform use, it is important that accuracy also remains a priority. Standard disposable hospital monitoring electrodes are accurate in large part due to the reduction-oxidation reaction of Ag/AgCl. The following work presents a testing method to compare future generations of heart rate monitoring devices to the current standard of disposable Ag/AgCl electrodes using electrochemical impedance spectroscopy.







## **Blocking and Non-Blocking Electrodes**



R2 strongly influences impedance at low frequencies suggesting that this parameter determines the effectiveness of the electrode as a heart rate monitor. The CPE data supports this interpretation, illustrating the differences in capacitive and resistive tendencies of the textile and 3M electrodes, respectively.

Standard Ag/AgCl disposable monitoring electrodes rely on the wellknown AgCl + e-  $\leftrightarrow$ Ag + Cl- reduction-oxidation reaction to produce clear, reliable electrocardiogram (ECG) signals for inpatient monitoring. However, these electrodes are not suitable for athletic monitoring for many reasons, most notably the discomfort of the user and the preparation needed before application. However, silver coated fabrics could overcome the comfort issue, and provide the solution for continuous, real-time motion and non-motion measurements in daily life.

#### Impedance Measurements 10 10<sup>4</sup> 10<sup>3</sup> 3M electrodes Ň 10<sup>2</sup> 10 **Textile electrodes** 1°C $10^{0}$ 13°C $10^{2}$ 10 10<sup>-3</sup> 10<sup>4</sup> 10<sup>v</sup> 25°C Frequency (Hz) 37°C 49°C 3M electrodes

# **On-body Testing**





Impedance measurements of adidas textile strap electrodes were compared to 3M Red Dot 2230 diaphoretic monitoring electrodes measurements. An impedance sweep from 1MHz to 1mHz was conducted on the samples at 1°C, 13°C, 25°C, 37°C and 49°C. The data for each temperature was then modeled to the appropriate equivalent circuit.

Resting ECG measurements were taken on a healthy adult male with both electrodes simultaneously. Without electrode gel, the textile electrodes showed erratic behavior, with sudden increases and decreases in heart rate that were not present with the 3M electrodes.

# Conclusions

Wearable sensors are the key to continuous monitoring for health, sports and exercise. Heart rate monitors are essential to the realization of whole body monitoring systems. With the addition of a significant R2 component, the accuracy of textile based sensors can be dramatically improved and whole body monitoring systems could be created.

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