



Reliability of Corneal Dynamic Scheimpflug Analyser Measurements in Virgin and Post-PRK Eyes

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Abstract

Purpose: To determine the measurement reliability of CorVis ST, a dynamic Scheimpflug analyser, in virgin and post-photorefractive keratectomy (PRK) eyes and compare the results between these two groups.

Methods: Forty virgin eyes and 42 post-PRK eyes underwent CorVis ST measurements performed by two technicians. Repeatability was evaluated by comparing three consecutive measurements by technician A. Reproducibility was determined by comparing the first measurement by technician A with one performed by technician B. Intraobserver and interobserver intraclass correlation coefficients (ICCs) were calculated. Univariate analysis of covariance (ANCOVA) was used to compare measured parameters between virgin and post-PRK eyes.

Results: The intraocular pressure (IOP), central corneal thickness (CCT) and 1_{st} applanation time demonstrated good intraobserver repeatability and interobserver reproducibility ($ICC \geq 0.90$) in virgin and post-PRK eyes. The deformation amplitude showed a good or close to good repeatability and reproducibility in both groups ($ICC \geq 0.88$). The CCT correlated positively with 1_{st} applanation time ($r = 0.437$ and 0.483 , respectively, $p < 0.05$) and negatively with deformation amplitude ($r = -0.384$ and -0.375 , respectively, $p < 0.05$) in both groups. Compared to post-PRK eyes, virgin eyes showed longer 1_{st} applanation time (7.29 ± 0.21 vs. 6.96 ± 0.17 ms, $p < 0.05$) and lower deformation amplitude (1.06 ± 0.07 vs. 1.17 ± 0.08 mm, $p < 0.05$).

Conclusions: CorVis ST demonstrated reliable measurements for CCT, IOP, and 1_{st} applanation time, as well as relatively reliable measurement for deformation amplitude in both virgin and post-PRK eyes. There were differences in 1_{st} applanation time and deformation amplitude between virgin and post-PRK eyes, which may reflect corneal biomechanical changes occurring after the surgery in the latter.

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Introduction

The cornea is a viscoelastic structure with quantifiable biomechanical properties [1]. These properties are related to corneal thickness, age, intraocular pressure (IOP), hydration, and various pathologies [2–5]. The cornea's biomechanical behaviour is mostly dictated by the stroma, which encompasses 90% of the total corneal thickness and has a greater mechanical stiffness than the other corneal layers [6].

Corneal biomechanical failure is the basis of keratectatic diseases [7] such as keratoconus and pellucid marginal degeneration. The ability to quantify corneal biomechanical failure represents an important step towards better understanding and treatment of keratectatic diseases. In addition, corneal refractive laser ablation in virgin eyes weakens the cornea mechanically due

to tissue removal, leading to deterioration in corneal biomechanical strength [8]. Biomechanical changes may also affect the refractive outcome [9]. Moreover, biomechanical weakening after corneal refractive laser treatment may potentially induce iatrogenic keratectasia [10]. Therefore, knowledge of corneal biomechanical properties is important in predicting clinical outcomes [11] and in identifying cases with high risk for postoperative keratectasia after corneal refractive surgery.

Most of the earlier studies concerning corneal biomechanical properties were performed *in vitro* [12–14]. The Ocular Response Analyser (ORA, Reichert, Inc., Depew, NY) was the first device available to evaluate *in vivo* corneal biomechanical response to an air-puff [1]. It employs a quantitative electro-optical system to monitor the pressures at which the cornea flattens inward and outward by registering the corneal reflex of infrared light. The

recently introduced ultra-high-speed Scheimpflug video-imaging device (CorVis ST; Oculus, Wetzlar, Germany) is the first instrument allowing visualization and measurement of corneal deformation in response to a standardized air-puff pressure. Data evaluating the intraobserver repeatability and interobserver reproducibility of measurements with this relatively new device are scarce [15,16]. Furthermore, such studies as are available concern only healthy virgin eyes. The main goal of the present study was to test the hypothesis that the CorVis ST performs reliable measurements in both virgin and post-refractive surgery eyes. To our knowledge, this is the first study to evaluate the repeatability and reproducibility of CorVis ST measurements in post-refractive surgery eyes. The secondary purpose was to test the hypothesis that the measurements can reveal differences in biomechanical properties between these two groups.

CorVis ST

The CorVis ST utilizes an ultraviolet free blue (455 nm wavelength) light emitting diode (LED) and an ultra-high-speed (4330 frames per second) Scheimpflug camera to record the corneal deformation response to a high intensity air impulse. The air impulse originates from a metered, symmetrical, and fixed maximal internal pump generating a pressure of 25 kilopascal [16]. When the eye is aligned and the Scheimpflug image is in focus, the air puff gets released automatically and the cornea is imaged during the deformation event. The air pulse (lasting approximately 20 ms) forces the cornea inwards through appplanation until it achieves its highest concavity (concavity phase). On its way back, the cornea undergoes a second appplanation before achieving its natural shape.

A total of approximately 140 images of the cornea's two-dimensional cross-section are collected. By software tracing of the anterior and posterior corneal boundaries in individual image frames, parameters describing the corneal deformation response are automatically generated by the instrument. The CorVis ST software version 1.00r30 rev. 771 was used in the current study.

With the CorVis ST the biomechanical response of the cornea is characterized by three phases: 1st appplanation, highest concavity, and 2nd appplanation. In addition to intraocular pressure (IOP) and central corneal thickness (CCT) values, time (time to reach appplanation), length (the length of the flattened central cornea), and velocity (the velocity of the corneal apex movement during appplanation) at the moment of both the 1st and 2nd appplanation events are recorded. The following characteristics at the point of highest concavity are also presented: the highest concavity time, the deformation amplitude, the distance between bending points of the cornea (peak distance), and the concave radius of curvature. (Figure 1.)

Patients and Methods

Forty candidates for laser refractive surgery (virgin-eye group: 28 males and 12 females) and 42 subjects treated for myopia and astigmatism with photorefractive keratectomy (PRK) earlier (post-PRK group: 23 males and 19 females) were recruited. The PRK treatments were performed using topography-guided transepithelial surface ablation with the iRES system (iRES, iVIS Technology, Taranto, Italy) at SynsLaser Clinic in Tromsø, Norway, 12.69±10.08 months (range: 2 to 48) prior to the current examination. All participants received an extensive ophthalmic examination including Placido-based topography (Nidek OPD Scan II, Nidek Co. Ltd., Aichi, Japan), Scheimpflug topo/tomography (Precisio, iVIS Technology, Taranto, Italy), slit-lamp biomicroscopy and tonometry (Icare tonometer, Revenio Group

Corporation, Helsinki, Finland) to exclude corneal and other ocular pathologies. The Regional Committee for Medical and Health Research Ethics in Norway approved the study entitled "2013/762 - Biomechanical cornea measurements by means of CorVis ST". The research complied with the tenets of the Declaration of Helsinki and written informed consent was obtained from each participant before examination. Only the data from the right eye of each participant was used for the present study.

The CorVis ST measurements were performed three times by technician A and one time by technician B. The measurement sequence between the technicians was randomized using a randomization table. A one-minute pause was given between each measurement. Repeatability was evaluated by comparing the three consecutive measurements performed by technician A. Reproducibility was determined by comparing the first measurement by technician A with the one performed by technician B. Mean CorVis ST measured values obtained from the three measurements by technician A were used to compare the differences between the virgin and post-PRK eyes groups, as well as for the correlation analysis.

Statistical Analysis

MedCalc software 11.4.2 (MedCalc Software, Ostend, Belgium) and SPSS for Mac software (version 19, SPSS, Inc) were used for statistical analysis. A *p*-value of less than 0.05 was considered statistically significant. Descriptive statistical results were expressed as mean ± standard deviation (SD). The within-subject standard deviation (S_w), within-subject coefficient of variation (COV), and intraclass correlation coefficient (ICC) were determined to assess the intraobserver repeatability. Interobserver S_w , COV, and ICC were calculated to assess interobserver reproducibility. Independent sample *t*-test was used to compare the CorVis measured parameters in virgin and post-PRK eyes groups. For the parameters that showed significant differences, univariate analysis of covariance (ANCOVA) was then applied to adjust for selected covariates (age, CCT measured by the CorVis ST, and mean simulated keratometry (simK) value measured by OPD Scan II) to control for potentially confounding factors. Pearson or Spearman correlations were applied to examine the relationship between CCT, manifest refraction spherical equivalent (MRSE) and the deformation parameters.

Results

Patient Demographics

The mean age of the participants at the time of the examination was 27.6±9.0 (range, 18 to 48) and 31.8±6.7 years (range, 20 to 48) for the virgin-eye and post-PRK groups, respectively. In the virgin-eye group, the values of central corneal thickness (CCT) measured by Precisio, IOP measured by Icare rebound tonometer, and mean simK measured by OPD Scan II were not significantly different from the preoperative values of the post-PRK group (Table 1). The mean manifest refraction spherical equivalent (MRSE) in the virgin-eye and its preoperative value in the post-PRK groups were $-2.15±2.28$ D and $-3.52±1.93$ D, respectively. In the post-PRK group, the mean maximum ablation depth was $66.71±27.84$ μm (range: 18 to 129).

Intraobserver Repeatability and Interobserver Reproducibility

Tables 2 and 3 present the intraobserver repeatability of the CorVis ST measurements. In the virgin-eye group, the IOP, CCT, 1st appplanation time, and 2nd appplanation time demonstrated good

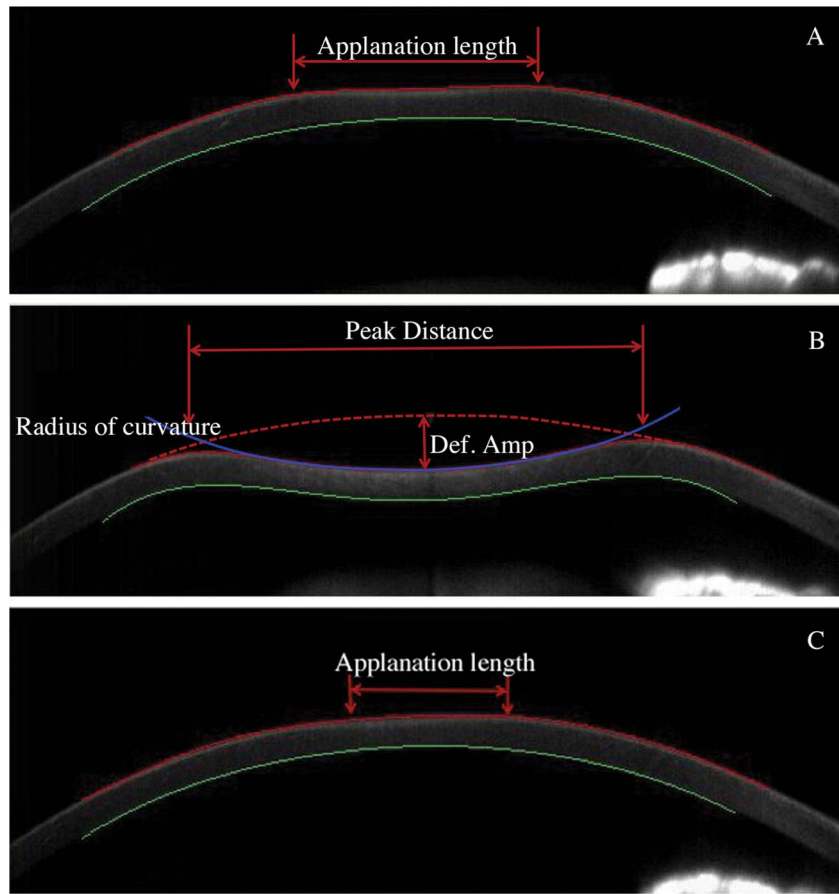


Figure 1. The CorVis ST utilizes the Scheimpflug camera to record the dynamic procedure of the corneal response to an air puff. A) The 1st applanation is achieved. B) The cornea reaches its highest concavity. C) The 2nd applanation is achieved when the cornea rebounds to its original position from the highest concavity. doi:10.1371/journal.pone.0109577.g001

repeatability (ICC ≥ 0.92), followed by deformation amplitude (ICC: 0.88), Radius of Curvature (ICC: 0.70), 2nd applanation velocity (ICC: 0.65), and highest concavity time (ICC: 0.64). The other parameters showed poor repeatability with large COVs and low ICCs. In the post-PRK group, the IOP, CCT, 1st applanation time, and deformation amplitude demonstrated good repeatability (ICC ≥ 0.90), followed by 2nd applanation time (ICC: 0.89), 2nd applanation velocity (ICC: 0.79), highest concavity time (ICC: 0.66), and radius of curvature (ICC: 0.63). The other parameters showed poor repeatability with large COVs and low ICCs.

When comparing the interobserver reproducibility of the CorVis ST parameters, the IOP, CCT, 1st applanation time, and 2nd applanation time demonstrated good reproducibility (ICC ≥ 0.91), followed by deformation amplitude (ICC: 0.88), radius of curvature (ICC: 0.64) and 2nd applanation velocity (ICC: 0.59) in the virgin-eye group. In the post-PRK group, the IOP, CCT, and 1st applanation time demonstrated good reproducibility (ICC ≥ 0.90), followed by deformation amplitude (ICC: 0.88), radius of curvature (ICC: 0.83), 2nd applanation time (ICC: 0.79), highest concavity time (ICC: 0.63), 2nd applanation velocity (ICC:

Table 1. Demographic Data of Participants.

| | Virgin eyes (n = 40) | Post-PRK eyes (n = 42) | p |
|----------------------------|----------------------|--|--------------|
| Age, years | 27.9 ± 9.0 (18, 48) | 31.8 ± 6.9 (20, 48) | 0.03 |
| CCT (Precisio), μm | 547.82 ± 26.78 | preop 542.02 ± 30.68 postop 485.00 ± 40.10 | 0.30* 0.000* |
| IOP (Icare), mmHg | 15.20 ± 2.57 | preop 15.81 ± 3.29 postop 12.71 ± 2.77 | 0.46* 0.000* |
| MRSE, D | -2.15 ± 2.28 | preop -3.52 ± 1.93 postop 0.01 ± 0.48 | 0.03* 0.000* |
| Mean simK (OPD Scan II), D | 43.47 ± 1.38 | preop 43.81 ± 1.58 postop 40.87 ± 1.63 | 0.18* 0.000* |

CCT = central corneal thickness; IOP = intraocular pressure; MRSE = manifest refraction spherical equivalent; simK = simulated keratometry. * p values were adjusted for age-difference. doi:10.1371/journal.pone.0109577.t001

Table 2. Intraobserver Repeatability of Parameters Obtained by Corvis in Virgin-Eye Group (n = 40).

| Parameters | Mean ± SD | Sw | 2.77Sw | COV (%) | ICC (95%CI) |
|--------------------------------------|--------------|------|--------|---------|--------------------|
| IOP (mmHg) | 14.46±1.33 | 0.59 | 1.62 | 3.59 | 0.93 (0.89~0.96) |
| CCT (μm) | 543.32±25.08 | 5.34 | 12.56 | 0.69 | 0.99 (0.98~0.99) |
| 1 _{st} appl. time (ms) | 7.29±0.21 | 0.09 | 0.24 | 1.09 | 0.94 (0.90~0.97) |
| 1 _{st} appl. length (mm) | 1.83±0.18 | 0.29 | 0.81 | 13.94 | 0.10 (-0.52~0.49) |
| 1 _{st} appl. velocity (m/s) | 0.14±0.02 | 0.03 | 0.08 | 18.82 | 0.25 (-0.26~0.57) |
| 2 _{nd} appl. time (ms) | 21.65±0.34 | 0.17 | 0.48 | 0.71 | 0.92 (0.87~0.95) |
| 2 _{nd} appl. length (mm) | 1.89±0.29 | 0.45 | 1.24 | 21.53 | 0.17 (-0.39~0.53) |
| 2 _{nd} appl. velocity (m/s) | -0.34±0.04 | 0.04 | 0.10 | -9.77 | 0.65 (0.42~0.80) |
| Highest concavity time (ms) | 16.40±0.37 | 0.37 | 1.02 | 2.02 | 0.64 (0.40~0.80) |
| Peak distance (mm) | 4.36±0.66 | 1.17 | 3.23 | 21.80 | -0.04 (-0.74~0.41) |
| Radius of curvature (mm) | 7.49±0.60 | 0.55 | 1.51 | 6.31 | 0.70 (0.49~0.83) |
| Deformation amplitude (mm) | 1.06±0.07 | 0.04 | 0.11 | 3.34 | 0.88 (0.81~0.93) |

SD = standard deviation, ICC = intraclass correlation coefficient, CI = confidence interval, Sw = within-subject standard deviation, COV = within-subject coefficient of variation, IOP = intraocular pressure, CCT = central corneal thickness.
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0.60), and 2_{nd} applanation length (ICC: 0.52), (Table 4 and 5). The other parameters showed poor reproducibility.

The IOP, CCT, and 1_{st} applanation time demonstrated good intraobserver repeatability and interobserver reproducibility in both groups. The 2_{nd} applanation time had good repeatability and reproducibility in the virgin eyes, with close to good repeatability but not good reproducibility in post-PRK eyes. The deformation amplitude showed a good or close to good repeatability and reproducibility in both groups.

Comparison of the Measurements between Virgin-Eye and Post-PRK Groups

Differences in the CorVis ST measured parameters between the virgin and post-PRK eyes are listed in Table 6. After adjustment for age, CCT, and mean simK, the differences in the mean values of IOP, 1_{st} applanation time, 2_{nd} applanation time, radius of curvature, and deformation amplitude remained significant.

Compared to the virgin-eye group, the post-PRK group demonstrated a shorter 1_{st} applanation time, longer 2_{nd} applanation time, smaller radius of curvature, and larger deformation amplitude. The CCT demonstrated a confounding effect in the above-mentioned parameters ($p < 0.05$ in all analyses), while age and simK did not show statistically significant confounding effects ($p > 0.05$ in all analyses).

Central corneal thickness measured with the CorVis ST correlated to IOP, 1_{st} applanation time, radius of curvature, and deformation amplitude ($r = 0.439, 0.437, 0.357, \text{ and } -0.384$, respectively, $p < 0.05$), without significant correlation to other parameters in the virgin-eye group. In the post-PRK group, it correlated to IOP, 1_{st} applanation time, 1_{st} applanation velocity, 2_{nd} applanation length, 2_{nd} applanation velocity, radius of curvature, and deformation amplitude ($r = 0.482, 0.483, 0.401, 0.440, 0.395, 0.583, -0.375$, respectively, $p < 0.05$). The MRSE correlated to IOP, 1_{st} applanation time, and 2_{nd} applanation time, without significant correlation to other parameters in the virgin-eye group.

Table 3. Intraobserver Repeatability of Parameters Obtained by Corvis in Post-PRK Group (n = 42).

| Parameters | Mean ± SD | Sw | 2.77Sw | COV (%) | ICC (95%CI) |
|--------------------------------------|--------------|------|--------|---------|--------------------|
| IOP (mmHg) | 12.38±1.02 | 0.55 | 1.52 | 3.85 | 0.90 (0.84~0.94) |
| CCT (μm) | 481.18±42.45 | 8.16 | 22.61 | 2.29 | 0.99 (0.98~0.99) |
| 1 _{st} appl. time (ms) | 6.96±0.17 | 0.09 | 0.25 | 1.11 | 0.91 (0.85~0.95) |
| 1 _{st} appl. length (mm) | 1.82±0.22 | 0.36 | 0.99 | 17.65 | 0.08 (-0.54~0.47) |
| 1 _{st} appl. velocity (m/s) | 0.13±0.02 | 0.03 | 0.09 | 23.30 | -0.27 (-1.14~0.28) |
| 2 _{nd} appl. time (ms) | 21.96±0.31 | 0.18 | 0.49 | 0.69 | 0.89 (0.81~0.94) |
| 2 _{nd} appl. length (mm) | 1.70±0.39 | 0.49 | 1.37 | 26.01 | 0.48 (0.12~0.70) |
| 2 _{nd} appl. velocity (m/s) | -0.40±0.06 | 0.04 | 0.12 | -10.35 | 0.79 (0.65~0.88) |
| Highest concavity time (ms) | 16.48±0.35 | 0.41 | 1.15 | 2.12 | 0.66 (0.43~0.81) |
| Peak distance (mm) | 4.56±0.77 | 1.12 | 3.10 | 18.34 | 0.30 (-0.18~0.60) |
| Radius of curvature (mm) | 6.43±0.66 | 0.70 | 1.94 | 6.76 | 0.63 (0.38~0.79) |
| Deformation amplitude (mm) | 1.17±0.08 | 0.04 | 0.12 | 3.16 | 0.92 (0.86~0.95) |

SD = standard deviation, ICC = intraclass correlation coefficient, CI = confidence interval, Sw = within-subject standard deviation, COV = within-subject coefficient of variation, IOP = intraocular pressure, CCT = central corneal thickness.
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Table 4. Interobserver Reproducibility of Parameters Obtained by Corvis in Virgin-Eye Group (n = 40).

| Parameters | Mean Difference ± SD | Sw | 2.77Sw | COV (%) | ICC (95%CI) |
|--------------------------------------|----------------------|------|--------|---------|-------------------|
| IOP (mmHg) | -0.01±0.82 | 0.58 | 1.60 | 3.25 | 0.92 (0.86~0.96) |
| CCT (µm) | -1.49±6.76 | 4.78 | 13.24 | 0.72 | 0.98 (0.97~0.99) |
| 1 st appl. time (ms) | 0.01±0.12 | 0.08 | 0.23 | 0.96 | 0.93 (0.88~0.96) |
| 1 st appl. length (mm) | -0.02±0.38 | 0.27 | 0.73 | 11.67 | 0.29 (-0.35(0.63) |
| 1 st appl. velocity (m/s) | (0.005±0.05 | 0.03 | 0.09 | 19.10 | 0.08 ((0.75(0.51) |
| 2 nd appl. time (ms) | (0.01±0.24 | 0.17 | 0.47 | 0.61 | 0.91 (0.82(0.95) |
| 2 nd appl. length (mm) | (0.10±0.58 | 0.44 | 1.14 | 17.37 | 0.12 ((0.65(0.53) |
| 2 nd appl. velocity (m/s) | (0.01±0.06 | 0.04 | 0.11 | (9.63 | 0.59 (0.25(0.78) |
| Highest concavity time (ms) | (0.02±0.54 | 0.38 | 1.06 | 1.81 | 0.47 (0.00(0.72) |
| Peak distance (mm) | 0.11±1.47 | 1.04 | 2.89 | 13.08 | 0.06 ((1.45(0.63) |
| Radius of curvature (mm) | 0.01±0.81 | 0.57 | 1.58 | 5.01 | 0.64 (0.31~0.81) |
| Deformation amplitude (mm) | -0.002±0.06 | 0.04 | 0.11 | 1.95 | 0.88 (0.78~0.94) |

SD = standard deviation, ICC = intraclass correlation coefficient, CI = confidence interval, Sw = within-subject standard deviation, COV = within-subject coefficient of variation, IOP = intraocular pressure, CCT = central corneal thickness.
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($r = -0.485$, -0.492 , and 0.420 , respectively, $p < 0.05$). The postoperative MRSE was found to correlate only to radius of curvature in the post-PRK group ($r = 0.583$, $p < 0.05$).

Discussion

In vitro experiments [12,13] as well as theoretical mathematical models [17,18] have demonstrated that the cornea exhibits both elastic and viscoelastic properties. When loaded, the cornea shows instantaneous deformation (purely elastic behaviour) followed by a time-dependent deformation response (viscoelastic behaviour) [19]. The ideal device for measuring corneal biomechanical properties *in vivo* should be accurate, provide repeatable and reproducible results, and be minimally invasive. In the current study, the intraobserver repeatability and interobserver reproducibility of CorVis ST measurements in virgin eyes and post-PRK eyes were investigated.

Similar to the studies performed by Nemeth *et al.* [16] and Hon *et al.* [15], we found that the following parameters had the best repeatability in both groups: CCT, IOP, 1st appplanation time, and deformation amplitude. The current study also presented good repeatability for 2nd appplanation time. In addition, the ICCs in the current study were generally higher than in the mentioned studies for most of the parameters measured. The differences between the studies may be attributed to different patient populations and software versions. For example, in the study by Nemeth *et al.*, the mean age was 61.24 ± 15.72 years (95% CI: 57.62 to 64.86 years), while the population in the current study was much younger. In the study by Hon *et al.*, the software did not offer values for radius of curvature and peak distance. When comparing reproducibility, Hon *et al.* found a statistically significant difference in the CCT measurement between the two sessions. However, the intersession difference was calculated by comparing the examinations performed in the morning (9:00–10:99 am) and afternoon (3:99–5:99 pm) by the same observer. This time difference may have

Table 5. Interobserver Reproducibility of Parameters Obtained by Corvis in Post-PRK Group (n = 42).

| Parameters | Mean Difference ± SD | Sw | 2.77Sw | COV (%) | ICC (95%CI) |
|--------------------------------------|----------------------|------|--------|---------|-------------------|
| IOP (mmHg) | -0.17±0.70 | 0.50 | 1.38 | 2.81 | 0.90 (0.81~0.95) |
| CCT (µm) | 0.43±5.05 | 3.57 | 9.89 | 0.58 | 1.00 (0.99~1.00) |
| 1 st appl. time (ms) | -0.02±0.11 | 0.08 | 0.23 | 0.84 | 0.90 (0.82~0.95) |
| 1 st appl. length (mm) | 0.08±0.46 | 0.32 | 0.90 | 14.45 | 0.27 (-0.36~0.60) |
| 1 st appl. velocity (m/s) | -0.01±0.04 | 0.03 | 0.09 | 17.54 | 0.45 (-0.03~0.70) |
| 2 nd appl. time (ms) | 0.04±0.28 | 0.20 | 0.55 | 0.64 | 0.79 (0.61~0.89) |
| 2 nd appl. length (mm) | -0.11±0.64 | 0.45 | 1.25 | 20.23 | 0.52 (0.12~0.74) |
| 2 nd appl. velocity (m/s) | 0.01±0.07 | 0.05 | 0.15 | -11.03 | 0.60 (0.26~0.78) |
| Highest concavity time (ms) | 0.05±0.49 | 0.35 | 0.97 | 1.54 | 0.63 (0.31~0.80) |
| Peak distance (mm) | 0.001±1.57 | 1.11 | 3.08 | 15.23 | 0.26 (-0.39~0.61) |
| Radius of curvature (mm) | -0.06±0.49 | 0.35 | 0.97 | 4.27 | 0.83 (0.68~0.91) |
| Deformation amplitude (mm) | -0.02±0.15 | 0.04 | 0.12 | 3.89 | 0.88 (0.78~0.94) |

SD = standard deviation, ICC = intraclass correlation coefficient, CI = confidence interval, Sw = within-subject standard deviation, COV = within-subject coefficient of variation, IOP = intraocular pressure, CCT = central corneal thickness.
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Table 6. Comparison of The CorVis ST Measurements Between Virgin-Eye and Post-PRK Groups.

| | Virgin-eye (n = 40) | post-PRK (n = 42) | Difference (mean ± SE) | p | Adjusted p* | Adjusted R ² |
|-----------------------------------|---------------------|-------------------|------------------------|-------|-------------|-------------------------|
| IOP (mmHg) | 14.46±1.33 | 12.38±1.02 | 2.08±0.26 | 0.000 | 0.002 | 0.520 |
| CCT (μm) | 543.32 ±25.08 | 485.41±39.00 | 57.90±7.28 | 0.000 | | |
| 1_{st} applanation | | | | | | |
| Time (ms) | 7.29±0.21 | 6.96±0.17 | 0.33±0.04 | 0.000 | 0.003 | 0.519 |
| Length (mm) | 1.83±0.18 | 1.81±0.22 | 0.01±0.04 | 0.832 | | |
| Velocity (m/s) | 0.14±0.02 | 0.13±0.02 | 0.01±0.00 | 0.010 | 0.614 | 0.160 |
| 2_{nd} applanation | | | | | | |
| Time (ms) | 21.65±0.34 | 21.96±0.31 | -0.31±0.07 | 0.000 | 0.032 | 0.221 |
| Length (mm) | 1.89±0.29 | 1.70±0.39 | 0.19±0.08 | 0.013 | 0.958 | 0.133 |
| Velocity (m/s) | -0.34±0.04 | -0.40±0.06 | 0.07±0.01 | 0.000 | 0.053 | 0.372 |
| Highest concavity | | | | | | |
| Time (ms) | 16.40±0.37 | 16.48±0.41 | -0.07±0.09 | 0.374 | | |
| Peak distance | 4.36±0.66 | 4.56±0.77 | -0.20±0.16 | 0.216 | | |
| Radius (mm) | 7.49±0.60 | 6.43±0.66 | 1.06±0.14 | 0.000 | 0.001 | 0.551 |
| Deformation amplitude (mm) | 1.06±0.07 | 1.17±0.08 | -0.10±0.02 | 0.000 | 0.005 | 0.402 |

SE = standard error, IOP = intraocular pressure, CCT = central corneal thickness.

p* values were adjusted for the effect of the age, CCT, mean simK difference between the virgin-eye and post-PRK groups.

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affected the reproducibility evaluation, as corneal thickness demonstrates diurnal variation [20]. The other parameters measured with the CorVis ST did not show satisfactory reliability. The ICCs varied between the virgin and post-PRK eyes.

It is conceivable that the cornea would be more difficult to deform and would deform less in eyes with a greater CCT. In line with other studies [15,21], we revealed a negative correlation between CCT and deformation amplitude in both groups. In addition, the CCT correlated positively with 1_{st} applanation time and radius of curvature in both virgin and post-PRK eyes. However, correlations between CCT and 1_{st} applanation velocity, 2_{nd} applanation time, length, and velocity were only found in post-PRK eyes. This may imply that CCT in normal virgin eyes does not introduce much variation to some of the CorVis ST parameters, while affecting those measurements in biomechanically compromised corneas. The MRSE in our virgin-eyes group demonstrated correlation with some of the parameters measured by CorVis ST. This may need to be taken into consideration if a database of “healthy corneas” is built for the purpose of identifying biomechanically weaker corneas.

The IOP measured with the CorVis ST was significantly lower in the post-PRK eye group compared to the virgin-eye group, while the historical preoperative data (IOP measured by Icare, CCT, and corneal curvature) of the post-PRK group showed no significant difference compared to the respective data in the virgin-eye group. The CorVis ST measurements in our post-PRK group were performed a minimum of two months postoperatively, by which time the patients had discontinued the use of local steroids for at least three weeks, to exclude a possible pharmacological effect on their IOP. Some studies have demonstrated that IOP measured with the CorVis ST is more reliable compared to Goldmann applanation tonometry (GAT) and Topcon noncontact tonometry in virgin eyes (Topcon CT-80A Computerized Tonometer; Topcon, Tokyo, Japan) [22]. Still, in the version of CorVis ST used in this study, IOP is calculated based on the timing of the 1_{st} applanation event and is not adjusted for corneal

biomechanical properties. Both CCT and corneal biomechanical properties can affect IOP measurements, with the latter suggested to be more influential [18]. The difference in the CorVis ST measured IOP between the groups was most likely caused by changes in corneal biomechanical properties and CCT after PRK.

Interestingly, before being adjusted for age, CCT, and simK, the CorVis ST parameters that demonstrated differences between the virgin and post-PRK eyes (1_{st} applanation time, 1_{st} applanation velocity, 2_{nd} applanation time, 2_{nd} applanation velocity, deformation amplitude and radius of curvature) were the same parameters as those showing differences between normal eyes and keratoconus eyes in the study conducted by Ali *et al.* [23]. It seems that these parameters may be of value in evaluating corneal biomechanical properties.

The earlier start of the apex indentation (shorter 1_{st} applanation time) and greater deformation amplitude in post-PRK eyes indicates a lower resistance to deformation due to a decrease in corneal stiffness [24,25]. Shen *et al.* [26] compared corneal deformation parameters after femtosecond laser small incision lenticule extraction (SMILE), laser-assisted sub-epithelial keratomileusis (LASEK), and femtosecond laser-assisted LASIK (FS-LASIK). They found greater deformation amplitude and shorter 1_{st} applanation time in the FS-LASIK group compared to the LASEK group. However, those parameters did not differ significantly between the SMILE and LASEK groups, or between SMILE and FS-LASIK groups. This indicates that corneal refractive surgery alters the stiffness of the cornea to different degrees with respect to different surgical approaches.

In the current study the CorVis ST measurements in virgin- and post-PRK eyes were taken from two groups of unrelated populations. Pre- and postoperative comparison of the same population would have been better suited to evaluate the changes in biomechanical properties caused by the surgery. We attempted to compensate for this by applying age, CCT, and simK as covariates to adjust for potential confounding factors. For the sake of this discussion we also introduced a separate group of 28 eyes of

16 patients who underwent PRK for myopic astigmatism (mean preoperative MRSE: -3.35 ± 1.98 D, mean postoperative time 9.21 ± 5.09 months) with both pre- and postoperative CorVis ST measurements. The pre- and postoperative CorVis ST measurements of CCT and IOP in that group [547.53 ± 28.89 μm vs. 460.32 ± 48.57 μm ($p < 0.05$), and 15.00 ± 1.48 mmHg vs. 13.48 ± 1.24 mmHg ($p < 0.001$), respectively] were similar to the differences found in the virgin and post-PRK eyes in the current study. Comparable similarity was also found for the I_{st} appplanation time [7.37 ± 0.23 vs. 7.14 ± 0.20 ms ($p < 0.001$)], I_{nd} appplanation time (21.39 ± 0.32 vs. 21.57 ± 0.25 ms ($p < 0.05$), radius of curvature [7.76 ± 0.83 vs. 6.55 ± 0.66 mm ($p < 0.001$)] and deformation amplitude [1.03 ± 0.08 vs. 1.10 ± 0.08 mm, ($p < 0.05$)]. Still, a separate study measuring pre- and post-PRK parameters with a larger population is warranted.

References

- Dupps WJ Jr (2005) Biomechanical modeling of corneal ectasia. *J Refract Surg* 21: 186–190.
- Sullivan-Mee M, Billingsley SC, Patel AD, Halverson KD, Alldredge BR, et al. (2008) Ocular Response Analyzer in subjects with and without glaucoma. *Optometry and Vision Science* 85: 463–470.
- del Buoy MA, Cristobal JA, Ascaso EJ, Lavilla L, Lanchares E (2009) Biomechanical properties of the cornea in Fuchs' corneal dystrophy. *Investigative Ophthalmology and Visual Science* 50: 3199–3202.
- Kida T, Liu JHK, Weinreb RN (2008) Effects of aging on corneal biomechanical properties and their impact on 24-hour measurement of intraocular pressure. *American Journal of Ophthalmology* 146: 567–572.
- Ortiz D, Pinero D, Shabayek MH, Arnalich-Montiel F, Alio JL (2007) Corneal biomechanical properties in normal, post-laser in situ keratomileusis, and keratoconic eyes. *Journal of Cataract and Refractive Surgery* 33: 1371–1375.
- Elsheikh A, Alhasso D, Rama P (2008) Assessment of the epithelium's contribution to corneal biomechanics. *Experimental Eye Research* 86: 445–451.
- Roy AS, Shetty R, Kummelil MK (2013) Keratoconus: a biomechanical perspective on loss of corneal stiffness. *Indian J Ophthalmol* 61: 392–393.
- Guirao A (2005) Theoretical elastic response of the cornea to refractive surgery: risk factors for keratectasia. *J Refract Surg* 21: 176–185.
- Roberts C (2005) Biomechanical customization: the next generation of laser refractive surgery. *Journal of Cataract and Refractive Surgery* 31: 2–5.
- Klein SR, Epstein RJ, Randleman JB, Stulting RD (2006) Corneal ectasia after laser in situ keratomileusis in patients without apparent preoperative risk factors. *Cornea* 25: 388–403.
- Roy AS, Dupps WJ Jr (2009) Effects of altered corneal stiffness on native and postoperative LASIK corneal biomechanical behavior: A whole-eye finite element analysis. *J Refract Surg* 25: 875–887.
- Asejczyk-Widlicka M, Pierscionek BK (2008) The elasticity and rigidity of the outer coats of the eye. *Br J Ophthalmol* 92: 1415–1418.
- Boyce BL, Grazier JM, Jones RE, Nguyen TD (2008) Full-field deformation of bovine cornea under constrained inflation conditions. *Biomaterials* 29: 3896–3904.
- Elsheikh A, Brown M, Alhasso D, Rama P, Campanelli M, et al. (2008) Experimental assessment of corneal anisotropy. *J Refract Surg* 24: 178–187.
- Hon Y, Lam AK (2013) Corneal deformation measurement using Scheimpflug noncontact tonometry. *Optom Vis Sci* 90: e1–8.
- Nemeth G, Hassan Z, Csutak A, Szalai E, Berta A, et al. (2013) Repeatability of ocular biomechanical data measurements with a Scheimpflug-based noncontact device on normal corneas. *J Refract Surg* 29: 558–563.
- Glass DH, Roberts CJ, Litsky AS, Weber PA (2008) A viscoelastic biomechanical model of the cornea describing the effect of viscosity and elasticity on hysteresis. *Investigative Ophthalmology and Visual Science* 49: 3919–3926.
- Liu J, Roberts CJ (2005) Influence of corneal biomechanical properties on intraocular pressure measurement: quantitative analysis. *Journal of Cataract and Refractive Surgery* 31: 146–155.
- Nash IS, Greene PR, Foster CS (1982) Comparison of mechanical properties of keratoconus and normal corneas. *Experimental Eye Research* 35: 413–424.
- Read SA, Collins MJ (2009) Diurnal variation of corneal shape and thickness. *Optom Vis Sci* 86: 170–180.
- Leung CK, Ye C, Weinreb RN (2013) An ultra-high-speed Scheimpflug camera for evaluation of corneal deformation response and its impact on IOP measurement. *Investigative Ophthalmology and Visual Science* 54: 2885–2892.
- Reznicek L, Muth D, Kampik A, Neubauer AS, Hirneiss C (2013) Evaluation of a novel Scheimpflug-based non-contact tonometer in healthy subjects and patients with ocular hypertension and glaucoma. *Br J Ophthalmol* 97: 1410–1414.
- Ali NQ, Patel DV, McGhee CN (2014) Biomechanical responses of healthy and keratoconic corneas measured using a non contact Scheimpflug tonometer. *Investigative Ophthalmology and Visual Science*.
- Han Z, Tao C, Zhou D, Sun Y, Zhou C, et al. (2014) Air puff induced corneal vibrations: theoretical simulations and clinical observations. *J Refract Surg* 30: 208–213.
- Kling S, Marcos S (2013) Contributing factors to corneal deformation in air puff measurements. *Investigative Ophthalmology and Visual Science* 54: 5078–5085.
- Shen Y, Chen Z, Knorz MC, Li M, Zhao J, et al. (2014) Comparison of Corneal Deformation Parameters After SMILE, LASEK, and Femtosecond Laser-Assisted LASIK. *J Refract Surg* 30: 310–318.

The current study demonstrated that, in addition to measurements of CCT and IOP, the CorVis ST showed relatively good reliability in measurements of I_{st} appplanation time and deformation amplitude in both virgin- and post-PRK eyes. The differences in I_{st} appplanation time and deformation amplitude between virgin and post-PRK eyes may imply that the CorVis ST's direct view of the corneal deformation may offer information that promises to yield clinically relevant parameters correlated with corneal biomechanical properties.

Author Contributions

Conceived and designed the experiments: XC AS TPU. Performed the experiments: DH JW. Analyzed the data: XC YH JRE. Contributed reagents/materials/analysis tools: XC AS YH JRE. Wrote the paper: XC AS YH JRE DH JW TPU.