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## LOCAL ENDOTHELIAL DNA REPAIR DEFICIENCY CAUSES AGING-

#### RESEMBLING ENDOTHELIAL-SPECIFIC DYSFUNCTION

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#### **Abstract**

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We previously identified genomic instability as a causative factor for vascular aging. In the present study determined which vascular aging outcomes are due to local endothelial DNA damage, which was accomplished by genetic removal of ERCC1 DNA repair in mice (EC-KO mice). EC-KO showed a progressive decrease in microvascular dilation of the skin, increased microvascular leakage in the kidney, decreased lung perfusion, and increased aortic stiffness compared to WT. EC-KO showed expression of DNA damage and potential senescence marker p21 exclusively in the endothelium, as demonstrated in aorta. Also the kidney showed p21-positive cells. Vasodilator responses measured in organ baths were decreased in aorta, iliac and coronary artery EC-KO compared to WT, of which coronary artery was the earliest to be affected. Nitric oxide-mediated endothelium-dependent vasodilation was abolished in a rta and coronary artery, whereas endothelium-derived hyperpolarization and responses to exogenous nitric oxide were intact. EC-KO showed increased superoxide production compared to WT, as measured in lung tissue, rich in endothelial cells. Arterial systolic blood pressure was increased at 3 months, but normal at 5 months, at which age cardiac output was decreased. Since no further signs of cardiac dysfunction were detected this decrease might be an adaptation to prevent an increase of blood pressure. In summary, a selective DNA repair defect in the endothelium produces features of age-related endothelial dysfunction, largely attributed to loss of endotheliumderived nitric oxide. Increased superoxide generation might contribute to the observed changes affecting end organ perfusion, as demonstrated in kidney and lung.

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**Key words:** Aging, DNA damage, endothelium-dependent dilation, endothelial dysfunction,

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Despite the currently available prevention and treatment options, cardiovascular diseases (CVD) continue to be a main cause of morbidity and mortality worldwide. Even when traditional risk factors are absent or controlled, cardiovascular problems remain a major health issue as reflected by the independent risk factor, age [1]. Aging, which is not synonymous to age, is a natural but very complex process leading to the decline and ensuing loss of organ function. The accumulation of DNA damage is considered as one of the primary causes driving the process of aging, and involves various processes [2,3]. Firstly, cells with unrepaired DNA damage may enter into apoptosis or senescence; apoptosis can lead to atrophy and organ function decline due to the loss of cells or tissue, and senescence-related mechanisms trigger the acquisition of a senescence-associated secretory phenotype (SASP) that affects surrounding cells and triggers age-related traits [4]. In parallel, accumulating DNA damage also triggers a so-called 'survival response' that switches the organism's physiological status from one that promotes growth to one that suppresses growth and focuses on maintenance of cellular homeostasis and function [5]. In humans, the presence of individual genetic and environmental variations evoke differences in the rate of aging between individuals, but also between organs within an individual. This differential pace of aging is also observed in mouse models of accelerated aging as provoked by DNA repair defects [5].

Several mouse models have been generated that, by deficiency of specific repair pathways, show striking similarities to human aging [5]. One of these models is the  $Ercc1^{\Delta/-}$  mouse. The  $\Delta$  allele is a truncation of the ERCC1 (Excision Repair Cross Complementation group 1) protein by 7 amino acids of its C-terminus [6]. This results in a hypomorph mutation, that largely (but not completely) abolishes its interaction with the XPF protein. ERCC1-XPF forms a heterodimic structure-specific endonuclease that incises the damaged strand at some distance

5'of the lesion [7]. The  $\Delta$  allele has approximately 10% residual activity, causing impaired function of the protein, progressive accumulation of DNA damage and numerous features of accelerated ageing, which are strongly delayed by dietary restriction, the only universal antiaging intervention [8].

ERCC1 is an essential component in the pathway of DNA nucleotide excision repair (NER), which removes a wide class of helix-distorting DNA lesions induced by UV, chemicals and oxidative stress. Apart from that, ERCC1 is involved in other DNA repair systems such as double strand break and cross link repair [9]. Mutations in proteins of the NER pathway have shown severe effects on human health as evidenced in several human progeroid syndromes such as Cockayne syndrome, trichothiodystrophy and Xpf-Ercc1 syndrome [7,10].

 $Ercc1^{\Delta/-}$  mice are short-lived (24-28 weeks) and within 12 weeks from birth develop neurodegeneration, osteoporosis, many features of aging in liver, kidney, heart, muscle and the hematopoietic system. In 8-week old  $Ercc1^{\Delta/-}$  mice an increased blood pressure was observed, which appeared to become less apparent at 12 weeks of age [11,12]. Thus, the blood pressure increase might be biphasic. Also, increased vascular stiffness and loss of macro- and microvascular dilator function were observed [11]. The vasodilator dysfunction in  $Ercc1^{\Delta/-}$  mice is explained by reduced NO-cGMP signaling, partly due to decreased endothelial nitric oxide synthase (eNOS) expression [11]. Many of these features are very similar to what was previously found in normal rodent and human aging.

Segmental progeria observed in  $Ercc1^{\Delta/-}$  mice implies that affected organs might be influenced by the impact of local and/or systemic DNA damage, processes associated with oxidative stress. To address the question if a local endothelial DNA repair defect is critical for the specific changes in vascular function as observed in  $Ercc1^{\Delta/-}$  mice, we investigated cardiovascular function in a mouse model with specific loss of Ercc1 in vascular endothelial cells.

#### Methods

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#### Animals

We evaluated the effect of endothelial genomic instability on cardiovascular function in a mouse model with endothelium-specific deletion of Ercc1 (*Tie2Cre*<sup>+</sup> *Ercc1*<sup>fl/-</sup> mouse model). To target the endothelium, various Cre recombinase models are available. Tie2Cre models have been used most widely. VE-Cadherin- (CD144) Cre models have been suggested as being perhaps the models in which the endothelium is targeted most uniformly [13]. However, the only example known to us in which a direct comparison is made between the models does not reveal a difference, at least, when used for fate mapping purposes of EC in adult organs [14]. Both Tie2 and VE-Cadherin are not only expressed in endothelial cells, but also in hematopoietic (stem) cells (HSC), potentially affecting leucocyte populations of HSC-derived lineage [15-18]. Interestingly, Tie2 is known to be expressed in lineages forming monocytes that have a pro-angiogenic function [17]. Thus, leucocytes specifically devoted to endothelial maintenance would be undermined, possibly preventing also the recovery of the endothelium if Ercc1 deletion indeed leads to dysfunction of the mature endothelium. Therefore, we preferred the Tie2 promotor region as the sequence driving Cre-recombinase. To explore the consequences of Tie2Cre-driven Ercc1 deletion in HSC we have examined the blood of the relevant mouse strains (see below). The Cre-loxP system was used to generate a conditional mouse model expressing Crerecombinase under the control of the vascular endothelial cell receptor tyrosine kinase (*Tie2*) promoter (Tie2Cre). *Tie2Cre*<sup>+/-</sup> female mice were crossed with *Ercc1*<sup>+/-</sup> male mice to generate Tie2Cre+/- Ercc1+/- mice in a pure C57BL/6J background. The females were then crossed with Ercc1fl/fl male mice in a pure FVB/N background to produce Tie2Cre+ Ercc1fl/- mice in a C57BL6/FVB F1 hybrid background [19]. These *Tie2Cre*<sup>+</sup> *Ercc1*<sup>fl/-</sup> mice were homozygous

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for *Ercc1*, after deletion of the floxed allele in endothelial cells expressing Cre-recombinase. These mice are referred throughout this manuscript as endothelial cell-knock out mice (EC-KO). Littermates (genotypes: *Tie2Cre+ Ercc1*<sup>fl/+</sup>, *Tie2Cre- Ercc1*<sup>fl/+</sup>, *Tie2Cre- Ercc1*<sup>fl/-</sup>) were used as controls. All control mouse genotypes were combined and are referred to as WT mice in the paper. In order to test for potential differences between control genotypes, we performed some analyses separating the Cre+ Ercc1<sup>fl/+</sup> mice. For reactive hyperemia, *ex vivo* vascular function and mechanical properties of the carotid, we analyzed Cre+ Ercc1<sup>fl/+</sup> mice as a separate group. Mice were kept in individually ventilated cages, in a 12 h light/dark cycle and fed normal chow and water *ad libitum*.

EC-KO mice unexpectedly died at the age of 5.5 – 6 months (100% of the cases). Consequently, we decided to evaluate mice at 3 and 5 months of age. Mice under profound anaesthesia were euthanized by exsanguination from the vena porta. All animal procedures were performed at the Erasmus MC facility for animal experiments following the guidelines from Directive 2010/63/EU of the European Parliament on the protection of animals used for scientific purposes. All animal studies were approved by the Animal Care Committee of Erasmus University Medical Center Rotterdam (protocol number 118-13-03).

#### Pathological examination, tissue collection and blood analysis

All sudden deaths of EC-KO occurred at night, except for two cases. One of these two mice was submitted to whole body fixation in formalin for 48 hours and pathological examination. Tissues were processed by paraffin-embedding techniques, sectioned, and stained with Hematoxylin and Eosin. Slides were examined by a board-certified veterinary pathologist. For mice sacrificed at 3 and 5 months of age, blood was collected under anesthesia from the vena porta and analyzed for cell counts. Vascular, cardiac, renal and lung tissue were collected for further study. For scanning electron microscopy (EM) abdominal aorta was fixed in 4%

formaldehyde / 2% glutaraldehyde. The lumen was exposed after longitudinal opening of the aorta, and scanning EM recordings were made after platinum sputtering.

Blood vessel permeability

We performed Evans Blue dye method in mice, as described [20], to determine the presence of vascular leakage in kidneys. In brief, we injected 100 uL of 1% Evans Blue dye (0.133 gr of Evans Blue in 10 ml of PBS with Ca2+ and Mg2+, prepared under sterile conditions) through femoral cannulation. After 4 hours of incubation, blood was drawn (100-200ul). Blood sampling was followed by whole animal PBS perfusion through the femoral infusion cannula after opening of the right atrium. Perfusion was performed with a peristaltic rotation pump until no blood residue remained in the atrium. Kidneys were collected, weighted and transferred to sample tubes with 500 µl of formamide. The sample tubes were incubated in a heat block at 55°C for 24 hours to extract Evans Blue from the tissue. After incubation, the formamide/Evans Blue mixture was centrifuged to pellet any remaining tissue fragments. Absorbance of each sample was measured at 610 nm (VersaMax<sup>TM</sup> Microplate Reader). Absorbance values from a standard curve with known concentrations of Evans Blue in formamide, with pure formamide as a background blank, and the total weight of each sample, were used to calculate the amount of Evans Blue per mg of renal tissue.

#### **Cardiac function**

Cardiac geometry and function were measured by performing 2-D guided short axis M-mode transthoracic echocardiography (Vevo770 High-Resolution Imaging System, VisualSonics) equipped with a 35-MHz probe. Left ventricular (LV) external and internal diameters were traced, and heart rate, LV mass and fractional shortening were subsequently calculated using the VisualSonics Cardiac Measurements Package. Mice were anesthetized with 2,5% and

maintained with 2,0% isoflurane, the animals were breathing freely and intubation was not required, while body temperature was kept at 37°C.

#### **Blood pressure measurement**

Blood pressure (BP) was measured non-invasively in conscious mice using the tail cuff technique (CODA High-Throughput device, Kent Scientific). BP was measured on 5 consecutive days and each session consisted of 30 measurement cycles for each mouse. The first 4 days were taken as acclimatization sessions. BP values reported here correspond to the average of all valid measurements recorded at day 5.

#### In vivo aortic strain

Using the data on systolic and diastolic aortic diameters acquired by transthoracic echocardiography, we calculated aortic strain by subtracting the diastolic aortic diameter from the systolic aortic diameter.

## Microvascular vasodilator function and lung perfusion in vivo

We assessed *in vivo* vasodilator function using Laser Doppler perfusion imaging, after three to seven days of blood pressure measurement. Reactive hyperemia, defined as the increase of the hindleg perfusion after temporary occlusion of the blood flow, was calculated. Blood flow was measured in the left hindleg one day after removing the leg's hair using a hair removal cream. The hindleg was kept still with help of a fixation device. After recording baseline perfusion for 5 minutes, blood flow was occluded for 2 minutes with a tourniquet. To record hyperemia and the return of the blood flow to the post-occlusion baseline, blood flow was monitored for 10 minutes after releasing the tourniquet. During all measurements mice were under 2.8% isoflurane anesthesia, and temperature was constantly monitored and maintained between 36.4-37.0 °C. For each mouse we calculated the maximum response to occlusion and the area under

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the curve relative to the post-occlusion baseline. Only the area above the baseline was considered. Values below the baseline were set at 0.

In a separate set of 5 month-old WT vs. EC-KO (n= 4 vs 7), lung perfusion was measured by microCT imaging. µCT scans were performed and reconstructed at the Applied Molecular Imaging Erasmus MC facility (AMIEf) by using the Quantum FX (PerkinElmer). Mice were anesthetized with 2.5% isoflurane in O<sub>2</sub> and received an IV injection with eXIA160 (Binitio Biomedical Inc., Canada) contrast agent. The injected amount of agent followed the dose recommended by the manufacturers. First, a pre-contrast scan was made as a baseline. The animal was taped to the imaging bed with a catheter placed in the tail vein to ensure minimal displacement and prevent misalignment during post-processing. After acquisition of the precontrast scan, the contrast agent was slowly infused (150-200 uL in 1 minute), after which a second scan was made. Mice were scanned using intrinsic cardio-respiratory gating to reduce artifacts caused by breathing. CT acquisition parameters: 90kv, 160µA, field of view 20mm, 40 um resolution with an acquisition time of 4.5 min. Scans were quantified using Analyze 11.0 software (AnalyzeDirect). By using the image calculator option the pre-contrast image was subtracted from the post-contrast image. This resulted into an image of iodine only, which was subjected to further filtering with a median filter (kernel size 3 x 3 x 3). During semiautomatic segmentation of the lungs, the large and midsize blood vessels were excluded. On the resulting lung image segmentation, we calculated the average intensity value as a measure for average lung perfusion, with a minimum of 40% of total lung volume.

#### Ex vivo vascular functional assessment

Immediately after sacrifice thoracic aorta, iliac and left anterior descending coronary arteries were carefully dissected from mice and kept in cold Krebs-Henseleit buffer (in mmol/L: NaCl 118, KCl 4.7,CaCl<sub>2</sub> 2.5, MgSO<sub>4</sub> 1.2, KH<sub>2</sub>PO<sub>4</sub> 1.2, NaHCO<sub>3</sub> 25 and glucose 8.3 in distilled

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baths (Danish Myograph Technology, Aarhus, Denmark) containing 6 mL of Krebs-Henseleit buffer oxygenated with 95% O<sub>2</sub> and 5% CO<sub>2</sub>. After warming, the tension was normalized by stretching the vessels in steps until 90% of the estimated diameter at which the effective transmural pressure of 100 mmHg is reached. Thereafter, the viability of the vessels was tested by inducing contractions with 30 and 100 mmol/L KCl. After the maximum response to KCl had been reached vessels were washed. To evaluate vasodilatory responses, aortic and iliac segments were first pre-constricted with 30 nmol/L of the thromboxane A<sub>2</sub> analogue U46619, resulting in a preconstriction corresponding with 50-100% of the response to 100 mmol/L KCl. After this, concentration-response curves (CRCs) were constructed with the endotheliumdependent vasodilator acetylcholine (ACh) at cumulative doses (10<sup>-10</sup>-10<sup>-5</sup> mol/L). When the CRC to ACh was completed, we used the endothelium-independent vasodilator sodium nitroprusside (SNP, 10<sup>-4</sup> mol/L). Complete CRCs to SNP (10<sup>-10</sup>-10<sup>-4</sup> mol/L) were performed in parallel rings preconstricted with 30 nmol/L U46619. The contribution of nitric oxide (NO) and prostaglandins in the aortic ACh responses was explored by performing the experiments in the presence of the nitric oxide synthase inhibitor NG-nitro-L-arginine methyl ester salt (L-NAME, 10-4 mol/L) and the cyclo-oxygenase (COX) inhibitor indomethacin (INDO, 10-5 mol/L). Inhibitors were added to the organ bath 20 minutes prior to U46619. To assess the potential involvement of ROS in the blunted vasodilator response to ACh, we used N-acetyl-cysteine (NAC; 10<sup>-2</sup> mol/L), which is an aminothiol and synthetic precursor of intracellular cysteine and GSH and a non-specific ROS scavenger [21]. Moreover to determine whether altered vasodilation involves hydrogen peroxide, we used PEG-catalase

(PEG-CAT; 0.01 mg/ul), which catalyzes the decomposition of hydrogen peroxide to water

water; pH 7.4). Vessel rings of 1.5-2 mm length were mounted in small wire myograph organ

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and O<sub>2</sub>. Vessels were pre-treated with NAC or PEG-CAT for 1h prior to the ACh dose response curve.

In coronary arteries we investigated endothelium-dependent vasodilation by performing CRCs to ACh and to the Adenosine 5'-O-(2-thiodiphosphate) (ADPBS) and Uridine- 5'- O- (3thiotriphosphate) (UTPγS). The intracellular signalling activation caused by ADP and UTP, has not been studied in detail in the mouse heart. However, studies on blood pressure and cerebral arterioles in the eNOS-/- mice have shown that the two nucleotides do not cause vasodilation through the same mechanisms. It is thought that UTP-induced vasodilation exclusively involves endothelium-dependent hyperpolarization (EDH) [22], while ADP acts through both NO and EDH on a 50%/50% basis.[23] CRCs to ADPβS and UTPγS were performed in coronary arteries precontracted with U46619 and then in coronary segments precontracted with 30 mM KCl. The latter was done to elucidate the contribution of EDH in ADPβS- and UTPγS-induced vasodilation because when arteries are precontracted with 30 mmol/L KCl, EDH cannot occur because the artery is too strongly depolarized.[24-26] VSMC dilatory function was tested by constructing CRCs to the NO donor SNP.

In iliac rings, after washing out KCl 100 mmol/L, we investigated contractile responses to angiotensin II (Ang II, 10<sup>-10</sup>-10<sup>-7</sup> mol/L), endothelin-1 (ET-1 10<sup>-10</sup>-10<sup>-6</sup> mol/L) and phenylephrine (PE, 10<sup>-9</sup>-10<sup>-5</sup> mol/L). For detailed information see Supplementary Methods.

## Mechanical properties and dimensions of the vascular wall

Carotid arteries explanted from 5 months old mice were mounted in a pressure myograph (Danish Myograph Technology (DMT), Aarhus, Denmark) in calcium free buffer (in mmol/L: NaCl 120, KCl 5.9, EGTA 2, MgCl2 3.6, NaH2PO4 1.2, glucose 11.4, NaHCO3 26.3; pH 7.4). The intraluminal pressure of the carotid artery was increased stepwise by 10 mm Hg starting

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at 0 mm Hg and reaching 120 mm Hg. Lumen and vessel diameter were measured and used to calculate wall strain and stress [27].

Mechanical properties of the aortic wall were tested in a protocol that was earlier described by Fleenor and colleagues [28]. In short, aortic segments of 1.5 to 2.0 mm length were hung in small wire organ baths filled with Ca<sup>2+</sup>-free buffer with clamps just touching each other (zero position). After 1 hour of acclimatization the rings were pre-stretched 3 times for 3 minutes to 1 mm separation of the clamps from the zero position. After returning again to the zero position, the rings were set to a pretension of 1 mN by moving the clamps apart. The strain at this distance of the 2 clamps was set at "1". A series of 10% increasing strain values was created by stepwise increase of the clamp distance, with 3 minutes pauses between each step for equilibration. Thus, a series of 1, 1.1, 1.2, ..., 2.5 was constructed. The wires were not able to withstand more tension without bending. Burst point was not reached. Thus, applying this method we were able to measure mechanical properties of the aortic wall in the force range representing the plasticity observed in the physiological blood pressure range (80 - 120 mmHg); strain of 1.5 to 2.0, as determined with DMT normalization software), and beyond. For the force developed at each strain  $(\lambda)$  of unidirectional displacement, stress (S) was calculated applying the formula  $S = \lambda F/2HL$ , with F = developed force in mN, T = wall thickness, L =length of vessel segment. Wall thickness and other variables presented herein were measured by light microscopy, using calibrated Leica QWin software (Germany), at 50x magnification in 10 µm, eosin-stained cryo-sections made from separately isolated aortic tissue of the area adjacent to the segment tested in the organ bath. 6 EC-KO vs. 7 WT were tested of which 1 WT was a statistical outlier for stress at strain 2.4, 1 WT stiffness measurement failed due to technical problems with the organ bath set up. Only sections of segments that formed a complete vessel wall and that were, by approximation, circular were included for measurement

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of vessel diameter and circumference, explaining the lower n in EC-KO for these measurements.

#### **Quantitative real-time PCR**

Total RNA was isolated from aortic tissue and cDNA was prepared, which was amplified by real-time PCR on a StepOne thermocycler (Applied Biosystems). Each reaction was performed in duplicate with SYBR Green PCR Master Mix (Applied Biosystems).  $\beta$ -actin and HPRT-1 were used for normalization. The relative amount of genomic DNA in DNA samples was determined as follows: RQ =  $2^{(-\Delta\Delta Ct)}$ . Sequences of the primers used are provided in supplementary Table S1.

## Immunoblots and immune histology

Frozen tissues were homogenized in ice cold RIPA buffer (50 mmol/L HCl pH 7.4, 150 mmol/L NaCl, 1% NP-40, 0.25% Na-deoxycholate and 1 mmol/L EDTA) containing protease and phosphatase inhibitors (1 mmol/L PMSF, 1 mmol/L NaVO4, 1 mmol/L NaF, 1 µg/mL aprotinin, 1 µg/mL pepstatin and 1 µg/mL leupeptin) using a stainless-steel ultraturrax (Polytron). Homogenized tissues were centrifuged and protein concentration was measured in the supernatants using the BCA method (Thermo Scientific, USA). Membranes were blocked with 3 - 5% milk or 5 % BSA in TBS-T. After blocking, membranes were incubated overnight with the primary antibodies as follows: eNOS (Santa Cruz, SC-654 1:500 in 5% milk TBS-T), pSer1177- eNOS (Santa Cruz, SC-21871-R 1:500 in 5% BSA TBS-T), and Ercc1 (Abcam, Ab129267, 1:1000). We used an HRP (Horseradish peroxidase) - conjugated antibody (Bio-Rad 1:2000 in 1% milk-TBS-T) to detect the primary antibodies. For visualization we used an enhanced chemiluminiscent substrate for detection of HRP (Pierce ECL Immuno-Blotting Substrate, Thermo Scientific). Expression levels of eNOS and Ercc1were normalized to actin and cofilin. Lung protein of an Ercc1-full body knockout mouse was used as a negative control

for background subtraction.

For immunohistochemical stainings, aortic and kidney tissue were fixed in 4% buffered formaldehyde for 24 hrs, embedded in paraffin and sectioned at 5 μm. After deparaffinization and rehydration, all sections were incubated in antigen retrieval buffer (pH9) for 15 min at 100°C. Endogenous peroxidase was blocked by incubating the sections in 3% H<sub>2</sub>O<sub>2</sub> in methanol for 10 min. For immunohistochemical staining the slides were blocked for 1 hr and stained with P21 (1:100 ab107099) overnight at 4°C. Sections were incubated for 1hr at room temperature with the corresponding biotinylated secondary antibody (1:200 Vector BA-9400 and Dako E0432). After ABC (Vectastain PK-6100) incubation of 30 minutes, sections were subjected to DAB staining (Dako K3468). Images were acquired using Nanozoomer software and analyzed with NDP view 2.

## ROS, H<sub>2</sub>O<sub>2</sub>, and superoxide measurement

Various markers of oxidative stress were assessed as previously described [29,30]. Briefly, superoxide anion (O2<sup>-</sup>) production was measured in lung tissues (rich in endothelial cells) by lucigenin chemiluminescence assay. This assay uses NADPH as the substrate and accordingly the chemiluminescence signal reflects NADPH-dependent O2<sup>-</sup> generation and is a measure of NADPH oxidase (Nox) activity. Nox is a major source of ROS in vascular cells. Hydrogen peroxide (H2O2) levels were measured by Amplex Red assay. Global O2<sup>-</sup> levels in cell homogenate were measured by electron paramagnetic resonance (EPR) in samples containing 10 ug of protein and 1mM CMH (Enzo Life Sciences, UK) in a total volume of 100 ul of Krebs-HEPES buffer containing 25uM deferoximine and 5uM diethyldithiocarbamate (DETC). After homogenization, EPR samples were placed in 50µl glass capillaries and measurements were performed by Bruker BioSpin's e-scan EPR (Bruker® Biospin Corp.) equipped with a super-high Q microwave cavity at room

temperature. The EPR instrument settings for experiments were as follows: field sweep, 50 G; microwave frequency, 9.78 GHz; microwave power, 20 mW; modulation amplitude, 2 G; conversion time, 656 ms; time constant, 656 ms; 512 points resolution and receiver gain, 1×105. Results were normalized by protein content.

#### Statistical methods

Data are presented as mean and standard error of the mean, unless otherwise indicated. Statistical analysis between the groups of single values was performed by unpaired, two-tailed t-test. Differences in dose-response curves were tested by general linear model for repeated measures (sphericity assumed). Differences were considered significant at p <0.05.

#### Results

#### **General health features**

There were no general signs of developmental problems in EC-KO, and body weight was normal up until 5 months of age (Figure 1A). Blood cell analyses revealed no significant changes (supplementary Table S2). However, EC-KO had a strongly reduced lifespan, with a median of 24.6 weeks (supplementary Figure S1). Shortly before death, immobility and rapid breathing was observed in 2 of the EC-KO mice. Most deaths occurred at night. One of the two moribund mice, aged 22.6 weeks, was timely sacrificed to undergo full body pathological examination. Organs included were brain, heart, skeletal muscle, aorta, sciatic nerve, liver, spleen, lung and kidney. Again, no signs of developmental problems were observed. Except for necrosis observed in the medulla of the kidney, the examined organs did not show morphological or histological aberrations. In 3 out of 5 EC-KO vs. 1 out of 6 WT of 5 months of age the kidney revealed red blood cells in the tubules (Figure 1B-C), indicating microvascular leakage in EC-KO. These data suggest that endothelial DNA repair deficiency impairs the permeability of the renal medullary microvasculature.

#### Renal vascular permeability

To corroborate the increased permeability of the renal vasculature we used an *in vivo* Evans Blue tissue penetration assay, comparing the vessel leakage between EC-KO and WT mice (5 months old mice) in kidneys. The difference in vessel permeability was quantified spectrophotometrically by measuring the Evans Blue that was captured per gram of tissue. Our results show an increase in dye leakage from the kidney vessels of EC-KO mice when compared with WT mice (Figure 1D, p-value=0.05).

#### In vivo microvascular function

To further examine peripheral microvascular function we performed laser Doppler reactive hyperemia studies. At 3 months of age there was no difference in reactive hyperemia in the hindlimb skin between EC-KO and WT (Figure 2A, B, E, F). At 5 months EC-KO showed decreased reactive hyperemia (Figures 2C-F). When passing from the age of 3 to 5 months reactive hyperemia tended to increase in WT mice, whereas it tended to decrease in EC-KO mice. In addition, lung perfusion was measured in WT (n=4) and EC-KO mice (n=7) showing significantly decreased lung perfusion in EC-KO mice (Figure 3A-C). The evaluation of reactive hyperemia in the WT group showed no differences between Cre<sup>+</sup> Ercc1<sup>f/+</sup> and the other control genotypes.

#### Ex vivo vasodilator responses in aorta and iliac arteries

To examine vasodilation in large arteries and reveal the mechanism of vasodilator dysfunction *ex vivo* organ bath experiments were performed. Aorta and iliac artery of EC-KO showed decreased endothelium-dependent relaxations to acetylcholine compared to WT at the age of 5 months, which were still absent at 3 months of age (Figure 4A, B). Vascular smooth muscle dilatory function to the NO donor SNP was intact at both ages (Figure 4C-D). In WT mice, approximately half of the ACh response was mediated by NO (response to ACh was reduced by ~50% in the presence of the eNOS inhibitor L-NAME) (Figure 5A). No apparent contribution of prostaglandins was observed since the COX inhibitor indomethacin did not further reduce vasodilator responses (Figure 5A). Compared to WT mice, in EC-KO there was no contribution of the NO or prostaglandin pathways to the ACh responses (Figure 5B). In both WT and EC-KO a residual ACh response was observed that was similar in both groups of mice, suggesting that the contribution of endothelium-derived hyperpolarizing factors (EDHFs) is intact.

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We found no differences in the ex vivo vasodilatory responses between Cre<sup>+</sup> Ercc1<sup>f/+</sup> and the 419 rest of genotypes in the WT group (not shown). 420 The reduced NO availability and vasodilator dysfunction EC-KO mice could be explained by 421 422 oxidative stress. NAC resulted in a leftward shift (pEC50 control  $-6.996 \pm 0.1215$  (n=9) vs. 423 NAC  $-7.825 \pm 0.2451$  (n=10), p<0.05) of the ACh dose response in EC-KO mice (Figure 424 5C), but not in WT littermates. These findings suggest a role for ROS in impaired 425 vasodilation in EC-KO. PEG-CAT had no effect on ACh responses in EC-KO (Figure 5D) indicating that H<sub>2</sub>O<sub>2</sub> is likely not important in altered vasodilation in these mice. 426 427 To further examine the role of oxidative stress we measured NADPH-dependent ROS generation -by lucigenin chemiluminescence, O2 levels by EPR and H2O2 by Amplex Red. 428 429 This was done in lung tissue, which is relatively rich in endothelial cells, and which clearly 430 shows reduced perfusion (Fig. 3A-C). O2<sup>-</sup> and H2O2 levels were not different between EC-431 KO and WT (Supplementary Figure S2). However, NADPH-mediated O<sub>2</sub>- production, an 432 index of NADPH oxidase (Nox) activity, was significantly elevated in EC-KO compared to WT mice (Figure 5E). 433

#### 434 Ex vivo vasodilator responses in coronary arteries

As a representative for mid-sized arteries important for direct blood supply in vital organs relevant for cardiovascular disease we examined coronary artery function. In coronary arteries endothelium-dependent relaxation to ACh was significantly decreased in EC-KO both at 3 months and 5 months of age (Figure 6A, p-value=0.009 and 0.0007, respectively). Endothelium-independent relaxations to SNP were unchanged (Figure 6B). To study other endothelium-dependent agonists than ACh and the mechanism of vasodilator dysfunction ADPβS (NO and EDH-dependent) and UTPγS (EDH-dependent) were employed.

ADPβS relaxation curves were shifted rightward in EC-KO (Figure 6C, p-value=0.03) but responses to UTPγS unchanged (Figure 6D). Responses to ADPβS and UTPγS in arteries preconstricted with 30 mmol/L KCl were examined as to exclude EDH [24-26]. Maximal dilations to ADPβS were decreased in EC-KO vs. WT (Figure 6E), whereas dilations to UTPγS were cancelled in both mouse strains (Figure 6F). This result confirms that UTPγS is entirely dependent on EDH, and that NO-mediated responses are decreased in EC-KO.

#### Levels of eNOS, luminal endothelial coverage, and Ercc1 expression

Immunoblot analysis showed a tendency towards reduced baseline pulmonary eNOS protein level in EC-KO vs. WT, but this did not reach statistical significance (Figure 7A). Also, the ratio of eNOS-activating phosphorylation of the serine residue at position 1177 (pSer1177-eNOS) to total eNOS protein was not different at baseline (Figure 7A). The luminal surface of the abdominal aorta from 5 months-old animals was investigated for endothelial denudation (5 WT vs. 5 EC-KO). Scanning EM of the luminal surface also did not reveal a loss of endothelial cells (Figure 7B). ERCC1 protein expression of the conditional *Ercc1* KO allele was tested in homogenized lung tissue as a surrogate for endothelial knockout. ERCC1 protein was significantly lowered in 5 months old EC-KO (n=4) compared to WT (n=4) (Figure 7C).

#### Ex vivo vasoconstrictor responses

We tested contraction responses in iliac arteries to ET-1, Ang II and phenylephrine (supplementary Figure S3). Although at the age of 5 months phenylephrine responses were significantly lower in EC-KO, implying an effect of endothelial dysfunction on VSMC, we saw no consistent differences between WT and EC-KO of 3 and 5 months of age.

#### Mechanical properties and dimensions of the vascular wall

Since we previously found that arterial stiffness was increased in  $Ercc1^{\Delta/-}$  mice,[11] we measured aortic wall movement during cardiothoracic echography, and calculated

distensibility of the aorta. At 3 months no differences were found between EC-KO and WT but at 5 months distensibility was decreased in EC-KO despite normal pulse pressures (Table 1). Since echography was not accompanied by simultaneous blood pressure measurements, which are needed for indexation of aortic distensibility, we further evaluated the mechanical properties of aortic rings in organ baths. We confirmed that aorta of EC-KO was stiffer than that of WT (Figure 5F). Instead carotid arteries did not show significant differences in stiffness, lumen diameter or wall thickness under similar perfusion pressure increments between EC-KO and WT. Likewise, no differences in media strain or stress were observed (supplementary Figure S4).

To determine if the higher stiffness of aorta was associated with structural remodelling, the dimensions of transversally sectioned aortic segments were measured. This was done in sections taken from the part adjacent to the segment used for stiffness measurement. Wall thickness was not significantly increased (Figure 8A). Vascular diameter showed a trend to be increased in EC-KO, being statistically significant for external diameter (Figure 8B,C). Transversal surface area was higher in EC-KO than in WT aorta (Figure 8D). Vessel circumference also increased, showing a significant increase in external circumference (Figure 8 E,F). Hence, EC-KO showed a hypertrophic aorta wall featured by outward remodelling.

#### **Blood pressure**

Systolic blood pressure (SBP) was higher in EC-KO at 3 months (138 mm Hg in EC-KO vs 125 mm Hg in WT mice) whereas no differences were observed at 5 months (p-value SBP=0.72). No differences were observed in diastolic blood pressure (DBP) at 3 or 5 months (Table 1).

#### **Cardiac function**

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The change in SBP followed a biphasic course, being slightly elevated at 3 months and returned to normal at a time when endothelium-dependent vasodilation was markedly reduced (5 months). Therefore, we investigated cardiac function, measuring volume variables, as a possible explanation. Since male and female mice have a different heart volume and weight, both two-way ANOVA including genotype and sex, were used as statistical corrections for these variables. No differences between EC-KO and WT were observed at 3 months. However, stroke volume (SV) and cardiac output (CO) were significantly decreased in 5 month-old EC-KO compared to WT (Table 1). In agreement, SV and CO indexed for heart weight were also decreased. When indexed for body weight however, SV and CO were equal between EC-KO and WT (Table 1). To exclude a sex-specific effect of Ercc1 knockout we analysed males and females separately, and found that that CO and SV were lowered in EC-KO for both sexes (data not shown). Indexed CO and SV were unchanged per sex. Given that FS and HW were normal we conclude that there was no cardiac dysfunction. However, since non-indexed and heart weight-indexed CO and SV were significantly or borderline significantly (p=0.06) lowered, we cannot rule out that cardiac function adapted to decrease the blood pressure at 5 months of age.

## **Endothelial DNA damage response**

To study if Tie2Cre-driven *Ercc1* removal leads to an endothelial DNA damage response we performed immunohistochemistry on the damage response marker p21, a marker that is associated with cellular senescence, in aorta. We stained 4 randomly taken sections of thoracic aorta per mouse, using 5 mice per genotype (EC-KO or WT littermate). Controls incubated with secondary antibody alone were negative (not shown). When incubated with both primary and secondary antibody, we found that aortic sections in n=4 out of n=5 EC-KO contained scattered p21-positive endothelial cells (Figure 9A), whereas all WT mice (n=5) were devoid of positive cells (Figure 9B). There were no positive cells outside the endothelium,

demonstrating the specificity for vascular endothelial cells. Since leakage studies with Evans Blue revealed that the renal vasculature was also affected, we stained 4 randomly taken renal tissue section for p21 for each of n=5 mice. In 5 out of 5 EC-KO mice positive cells were detected, scattered over glomeruli and in vascular lumen (Figure 9C,D), whereas WT (n=5) kidneys were all negative (Figure 9E). The localization of the positive cells along vascular lumen indicates that renal endothelial cells were affected. Since glomeruli consist largely of endothelium, it seems likely that the p21-positive cells are endothelial cells as well.

It is generally believed that dysfunction of endothelial cells during aging contributes to a pro-

inflammatory lamina media of the vessel wall, and thus to hypertrophic vascular remodeling. We questioned if this occurs spontaneously in the absence of an exogenous pro-inflammatory stimulus, i.e. only by selective aging of endothelium. We tested expression of IL-1 $\alpha$ , IL-6, and TNF $\alpha$  mRNA. We chose these mediators because they are associated with the SASP, the secretory phenotype of senescent cells. We did not observe changes in aortic expression of IL-1 $\alpha$ , IL-6, and TNF $\alpha$  (Supplementary Figure S5).

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#### **Discussion**

We investigated the role of endothelial specific DNA repair defectiveness on cardiovascular function in a mouse model with specific loss of Ercc1 in vascular endothelial cells. We found that local endothelial genomic instability caused progressive macrovascular and microvascular vasodilator dysfunction at least in part due to specific loss of endothelium-derived NO. Smooth muscle responses to exogenously supplied NO were intact. Reduced eNOS expression does not seem to play a major role. The preserved endothelial cell layer, as confirmed by scanning EM as well as normal EDHF-mediated vasodilation, excludes the loss of NO through reduced EC numbers as a possible explanation. The most likely cause for the loss of vasodilation is reduced NO availability in EC-KO due to scavenging by ROS. The blunted endothelium-mediated NO responses are associated specifically with expression of the DNA damage response, cell stress and potential senescence marker p21. Thus, DNA damage results in a cell autonomous effect on NO signaling that might drive vascular aging. The change of endothelial function appears to affect VSMC as well, as evidenced by altered vasoconstriction, increased aortic stiffness and aortic hypertrophic remodeling, important features of vascular aging. This appears to be independent of a pro-inflammatory phenotype of medial cells, because in EC-KO aorta mRNA expression of inflammatory mediators IL-6 and TNFα, important in vascular inflammation, was not increased. Notably, the rate of development of vasodilator dysfunction is location-specific as at 3 months of age this dysfunction is observed in coronary arteries, but not in iliac artery, aorta, or the skin microvasculature. This suggests a non-developmental origin of the vasomotor dysfunction. Apart from location-specific effects with respect to the origin of the artery that was studied, we

also found location-specific effects within the arterial specimen itself. The presence of p21 only

in endothelial cells, and the absence of decreased VSMC responses to NO upon stimulation

with SNP suggests that a cell-autonomous effect is observed in EC-KO with regard to endothelium-derived NO. Previously, in the whole body *Ercc1* knockout strain, *Ercc1*<sup>Δ/-</sup> [11], lowering of eNOS was observed in lung tissue. In endothelial cells eNOS might mediate cell-autonomous effects. However, in EC-KO we only observed a statistically non-significant trend towards lowering of eNOS. It is known that eNOS reacts to aging in diverse ways, varying from increased expression to compensate for loss of vasodilator capacity due to NO scavenging by ROS in an early, compensated stage of endothelial aging, to decrease of eNOS and its activation in senescent cells [31-33]. The Cre-lox system does not remove the target gene with 100% efficiency, and indeed not all endothelial cells in EC-KO are p21-positive. Moreover, not all p21-positive cells might be senescent; the presence of several markers in combination is needed to confirm senescence. Therefore, it might be that there were senescent cells with lower eNOS, but not enough to statistically demonstrate eNOS lowering. Hence, the possibility that the observed lowering of ACh responses is the result of both NO quenching in the context of oxidative stress and eNOS lowering cannot be excluded.

Apart from vasodilator dysfunction EC-KO showed a severely compromised microvascular barrier function in the kidney. This was confirmed by histological examination and Evans Blue permeability tests, established methods for this purpose [34]. Therefore, the aging-mimicking effect of endothelial *Ercc1* deletion is not restricted to loss of vasodilator function, but at least affects barrier function in the kidney as well. Through this mechanism, the DNA damage response might contribute to progressive kidney damage, in addition to decreased NO signaling, an important determinant of renal deterioration [35]. Interestingly, cell cycle arrest in tubular cells induced by p21 plays a role in acute kidney injury (AKI), and plasma p21 levels have been proposed as a biomarker for AKI and renal aging [36,37]. It was suggested that this might take place independently from DNA damage because of the dissociation of DNA damage detection through ATM signaling [36,38]. However, this only excludes double strand break

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repair to be involved, although recently also transcription stress related R-loops were found to trigger ATM activation [39]. The question if DNA damage is involved therefore remains open. Our present finding prompts the question if endothelial aging, either caused by DNA damage or other mechanisms, might be implicated in p21-driven renal injury, and warrants further inspection of renal pathophysiology in endothelium-specific accelerated aging models.

In search of other features of vascular aging we tested vascular stiffness. At 5 months of age, aortic strain measured by echography was reduced in EC-KO, suggesting increased vascular stiffness. This was confirmed by ex vivo stress and strain measurements in aorta. The increased stiffness might be caused by the hypertrophic remodeling that we also observed in EC-KO. In contrast to aorta, carotid arteries did not show a change in vascular stiffness, again pointing to location-dependent difference. Increase of arterial stiffness with age, detected as increase of pulse wave velocity (PWV), is considered as a solid marker of vascular aging in humans [40]. PWV can be measured over different regions, such as from carotid to femoral, from brachial to carotid and from brachial to femoral artery. The different modes of PWV measurement show differential associations with age. Although this could involve technical aspects during measurements, it cannot excluded that differential rates of aging occur in diverse blood vessels. This is well-known for plaque development. Internal mammary arteries, for example, are relatively resistant to atherosclerotic burden, which has been attributed to endothelial features [41]. Coronary artery and aorta are generally known to be more vulnerable to plaque development. It is tempting to speculate that a differential susceptibility of the endothelium to DNA damage contributes to these differences.

Many of the features described in the EC-KO mice including vascular dysfunction, arterial remodeling, aortic stiffness and aging are typically associated with oxidative stress and increased activation of Noxs as demonstrated in various models of cardiovascular disease [42]. Our findings here of increased NADPH-mediated O<sub>2</sub>- production support this notion and

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suggest that EC Nox activity may be increased in EC-KO mice. Putative mechanisms whereby ERCC1 deficiency influences Noxs remain unclear and warrant further investigation. Reasons why there were no changes in global levels of O<sub>2</sub><sup>-</sup> and H<sub>2</sub>O<sub>2</sub> in EC-KO mice are unclear but may reflect efficient global antioxidant capacity.

As highlighted previously, vascular aging and DNA damage response are closely associated, as indicated by various research strategies from animal experiments to human (genetic) epidemiological studies and observations in progeroid syndromes [4,11,43]. In Mendelian randomization studies it was found that telomere length, an important marker of genomic instability, plays a causal role in CVD [44]. Epidemiologic research in large populations linking DNA damage response markers specifically obtained from circulating endothelial cells to various degrees of vascular dysfunction, eg. of vascular stiffness as measured by PWV, might provide important further evidence of the role of DNA damage in vascular aging. Epidemiological studies might also represent a future translational step of our findings as it could lead to development of markers that represent vascular age, which are potential tools for CVD risk prediction. Important in light of using endothelial cells for such marker studies is our observation that the effect of DNA damage on NO signaling is specifically evoked within the endothelium, possibly even cell-autonomously. Endothelium-specific markers might be an important addition to biomarker testing, such as inflammatory markers and telomere length, in white blood cells or in plasma, currently done in epidemiological studies that address vascular age and CVD risk [44]. Whether this concerns only endothelial DNA damage response markers or also inflammatory markers, is an important question. A limitation of our study is that we were unable to explore mRNA of inflammatory factors specifically in the endothelium (isolation of EC or their RNA was technically not feasible, data not shown). We cannot, however, exclude the possibility that due to cell-autonomous effects ECs may assume a pro-

inflammatory phenotype. Increased vascular leakage is suggestive of this and warrants further exploration.

Despite cell autonomous effects on NO signaling, changes in EC-KO were not restricted to endothelial function alone, as witnessed by hypertrophic vascular remodeling in aorta, changes in constrictions, but also the renal changes. EC-KO share some features with  $Ercc1^{\Delta/-}$  mice, including a worsened renal morphology and a shortened lifespan [45]. In an earlier publication rescuing the liver of Ercc1 null mutant mice from genetic Ercc1 inactivation, it was shown that next to the liver the renal tissue is exceptionally vulnerable to loss of Ercc1 function, and it was suggested that renal problems might be an important cause of death in the 'rescued' mice [46]. Our present results indicate that endothelial DNA damage might contribute to the renal problems.

Another important feature of aging is increased blood pressure. This appeared in EC-KO at 3 months of age, but was absent at 5 months. We observed clues that at 5 months stroke volume and cardiac output were adapted in EC-KO, possibly to normalize blood pressure in a phase state during which widespread overt vasodilator dysfunction can be found. This might not have happened at 3 months of age since vasodilator function is not as widespread at that age. In earlier studies we observed a small increase of blood pressure in  $Ercc1^{\Delta/-}$  mice. Apparently, the loss of endothelium-derived NO can be corrected, eg. by autonomic regulation.

In conclusion, we found that local endothelial genomic instability in mice reproduces important features of vascular aging that are also observed in humans. Increased vascular stiffness, vascular hypertrophic remodeling, loss of endothelium-dependent vasodilation, increased vascular leakage, and the differential vulnerability of various arteries are amongst the most important characteristics. Our present study adds to the growing evidence that the DNA damage response plays a central role in vascular aging, and that aging pathology can be driven

by genome instability and persistent DNA damage in a cell-autonomous manner in a variety of organs and tissues [47-51]. We propose epidemiological studies employing DNA damage response markers to further address the relevance in humans and provide a translational step towards CVD prediction markers. The loss of endothelium-derived NO and increased O2<sup>-</sup> bioavailability might play a major role in the observed phenotype. Further, we have shown that diet restriction is another potential treatment option, as this rescues loss of vasodilator function in *Ercc1*<sup>Δ/-</sup> mice as well as in humans [8,12,52]. Therefore, studies exploring the impact of dietary restriction on DNA damage-induced vascular aging and the involved rescue mechanisms can be of great value.

#### **Clinical Perspectives**

• Why was this study was undertaken?

We wanted to know if endothelial DNA damage causes features of vascular aging.

Brief summary of the results

We showed that endothelial DNA damage decreases endothelial-dependent vasodilations and end organ perfusion (lung and skin), increased vascular stiffness, vascular leakage (kidney) and wall thickness. The NO signaling pathway is specifically decreased. Superoxide formation, probably arising from NADPH oxidase, and possibly also cellular senescence might play a role in the observed aging features.

• What is the potential significance of the results to human health and disease?

The observation that the vascular changes are associated with p21 increase is clinically relevant considering the development of senolytic drugs. The decreased NO, and increased superoxides, is important for the clinical development of drugs acting on these pathways, eg. sGC activators and stimulators, PDE inhibitors, and Nox inhibitors.

Similar to human aging, arteries are differentially affected in mice lacking endothelial DNA repair. The coronary artery is the most rapidly affected vascular bed in our study and may have implications for coronary disease.

Renal vascular leakage and necrosis were observed, which might have implications for aging-related renal dysfunction. Our findings further support the use of p21 as a clinical biomarker for kidney injury.

Microvascular function is disturbed by the endothelial DNA repair defect and may
have impact on aging-associated end organ dysfunction.
Future clinical studies on DNA damage and repair in the human vascular system are
warranted. In particular, epidemiologic biomarker research specifically in endothelial
cells might provide further evidence of the role of DNA damage and repair in CVD,
and might be of additional value when optimizing CVD risk prediction

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## **Competing Interests**

The authors declare that there are no competing interests associated with the manuscript.

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**Author Contribution** 

The contributions of the authors are as follows: AJMR, AHD, IvdP, RMT, AM, DD, KAH and JH conceived the design of the study. PBN and EPF conducted and analyzed the ex-vivo

vascular experiments from aortas and illiacs arteries as well as immunoblots. PBN performed

blood pressure measurement and quantitative real-time PCR. EPF and RM assessed the blood

vessel permeability. ERB and KAH conducted and analyzed the ex-vivo vascular

experiments from coronary arteries. RB and RdV were in charge of mice breeding and

monitoring and evaluated the mechanical properties of the carotid vascular wall. RvV

performed cardiac function and blood pressure measurements. RdV and MdB performed

cardiac echography. MD performed detection of senescence markers. AdB, RT and RM

performed renal and further tissue histological analyses. YR, IvdP and JE assessed the

microvascular vasodilator function and lung perfusion in vivo. HvB performed electron

microscopy. RMT and ACM performed studies on ROS. MG and RS gave scientific advice

and contributed to the writing of the manuscript.

**Abbreviations** 

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736	ADPβS, Adenosine 5'-O-(2-thiodiphosphate); Ach, acetylcholine; ANG II, angiotensin II;
737	BP, blood pressure; cGMP, cyclic guanosine monophosphate; CVD, cardiovascular disease;
738	CO, cardiac output; CRCs, concentration-response curves; EC; endothelial cells; EC-KO,
739	endothelial-cell knockout; EDHFs, endothelium-derived hyperpolarizing factors; eNOS,
740	endothelial nitric oxide synthase; ERCC1, excision repair cross complementation group 1;
741	ET-1, endothelin 1; Il-6, interleuking-6; LNAME, $N(\omega)$ -nitro-L-arginine methyl ester; LV,
742	left ventricular; MMP13, matrix metalloproteinases 13; NAC, N-acetyl-cysteine; NER,
743	nucleotide excision repair; NO, nitric oxide; ROS, reactive oxygen species; SASP,
744	senescence-associated secretory phenotype; SBP, systolic blood pressure; SNP, sodium
745	nitroprusside; SV, stroke volume; TNF $\alpha$ , tumor necrosis factor $\alpha$ ; UTP $\gamma$ S, Uridine-5'-( $\gamma$ -thio)
746	triphosphate; VSMC, vascular smooth muscle cell; WT, wildtype.
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**Table 1**. Cardiac function, blood pressure and aorta distensibility at 3 and 5 months.

_	3 months			5 months		
Parameter	EC-KO (n=10-19)	<b>WT</b> (n=11-21)	p- value	EC-KO (n=11-17)	<b>WT</b> (n=12-31)	p-value
Stroke volume (uL)	33 (5.5)	36 (5.1)	0.21 <sup>a</sup>	32 (8.0)	36 (5.0)	0.01 <sup>a</sup>
Stroke volume index (uL/mg myocardium)*	30 (4.5)	31 (4.1)	0.56 <sup>b</sup>	25 (5.2)	30 (3.5)	0.03 <sup>b</sup>
Stroke volume index (uL/g) <sup>\$</sup>	1.4 (0.2)	1.4 (0.2)	0.81 <sup>b</sup>	1.2 (0.2)	1.3 (0.2)	0.49 <sup>b</sup>
Fractional shortening (%)	34 (5.1)	34 (5.7)	0.71 <sup>b</sup>	33 (6.5)	33 (6.0)	0.94 <sup>b</sup>
HR (bpm)	502 (37.4)	492 (37.0)	0.38 <sup>b</sup>	494 (40.1)	498 (49.2)	0.78 <sup>b</sup>
Cardiac output (ml/min)	17 (2.9)	18 (3.3)	0.24ª	16 (4.1)	18 (3.6)	0.01ª
Cardiac Index (ml/min/mg myocardium)*	15 (2.3)	15 (2.6)	0.92 <sup>b</sup>	13 (2.4)	14 (1.7)	0.06 <sup>b</sup>
Cardiac Index (ml/min/g) §	0.7 (0.1)	0.7 (0.1)	0.93 <sup>b</sup>	0.6 (0.1)	0.6 (0.1)	0.46 <sup>b</sup>
Heart weight (mg)	112 (12.8)	116 (17.1)	0.45 <sup>b</sup>	125 (25.3)	122 (20.2)	0.77 <sup>b</sup>
SBP (mmHg)	138 (14.6)	125 (11.9)	0.04 <sup>b</sup>	128 (22.8)	125 (20.6)	0.72 <sup>b</sup>
DBP (mmHg)	94 (15.2)	89 (15.6)	0.46 <sup>b</sup>	88 (19.3)	86 (20.7)	$0.86^{b}$
Aorta distensibility (mm)	0.3 (0.1)	0.3 (0.04)	0.69 <sup>b</sup>	0.2 (0.1)	0.3 (0.1)	0.05 <sup>b</sup>

Values are Mean (SD). HR, heart rate; bpm, beats per minute; SBP, systolic blood pressure; DBP, diastolic blood pressure. \* Values are corrected for heart weight, expressed as per 100 mg of heart weight. S Values are corrected for body weight, expressed as per gram of body weight. Two-way ANNOVA. The test.

## Figure legends

Figure 1. General health and pathology findings. Body weights at 5 months (n= 9 EC-KO,				
4 males and 5 females, and 37 WT, 19 males and 18 females) (A). Mason's trichrome staining				
of kidney sections from a control mouse (B) and a EC-KO mouse (C) The area encircled shows				
extravasation of red blood cells in the proximity of the tubules. Kidney sections from 5 EC-				
KO and 6 WT mice were examined. (D) Renal Evans Blue leakage (ug Evans Blue × mg of				
kidney tissue) 24 hours after intravenous injection, results are expressed as means $\pm$ SE, * p-				
value $\leq 0.05$ compared to WT group.				
Figure 2. In vivo vasodilator function was assessed using Laser Doppler perfusion				
imaging. Functional differences between skin reperfusion after 2 minutes of occlusion between				
WT (A) and EC-KO (B) at 3 months; and between WT (C) and EC-KO (D) at 5 months.				
Calculated area under the curve (E), and average maximum response (F) for the observed				
differences in skin reperfusion. $* = p < 0.05$ (t test EC-KO vs WT). At 3 months, 10 EC-KO				
and 20 WT mice were examined. At 5 months 13 EC-KO and 36 WT mice were examined.				
Figure 3. $\mu$ CT-based contrast-aided perfusion. $\mu$ CT-based contrast images of WT and EC-				
KO lungs (A). μCT-based contrast-aided perfusion images of WT and EC-KO lungs,				
showing average intensity of perfusion after subtraction of the contrast to non-contrast				
images as the color bar indicates (B). Scatter plots depicting average intensity as a measure				
for lung perfusion, which is significantly reduced in EC-KO compared to WT. * = $p < 0.05$ (t				
test EC-KO vs WT) (C). 7 EC-KO and 4 WT mice were included for these measurements.				
Figure 4. Endothelium-dependent and independent relaxations in isolated aortic and				
iliac rings measured ex vivo in organ bath set-ups. ACh-induced vasodilation of EC-KO				
and WT in aorta and iliac artery at 3 months (A), and at 5 months (B). Endothelial-				

independent relaxations induced by SNP in aortic and iliac rings at 3 months (C) and at 5

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months (D). \*\* = p<0.001; \*\*\* = p<0.0001 (general linear model for repeated measures, sphericity assumed; EC-KO- aorta vs WT-aorta and EC-KO- iliac vs WT-iliac). At 3 months arteries from 9-12 EC-KO and 12-15 WT were studied. At 5 months arteries from 7-11 EC-KO and 21-30 WT were studied. Figure 5. Contribution of NO, prostaglandins and oxidative stress to the endothelium**dependent vasodilations.** At 5 months we evaluated the contribution of NO and prostaglandins to ACh-induced vasodilation in WT (A) and EC-KO (B). Vasodilator response in the presence of the wide range free radical scavengers (NAC) (C) and the H<sub>2</sub>O<sub>2</sub> scavenger PEG-catalase in EC-KO mice (D). (E) Superoxide levels measured in lung tissue. (F) aortic stress-strain relationship measured ex vivo in small wire organ bath set up. The strain range corresponding to 80 - 120 mmHg pressure is indicated with the horizontal range bar. \*\*\* = p < 0.0001 (general linear model for repeated measures, sphericity assumed; the responses to ACh alone were compared to the responses to ACh after preincubation with L-NAME). Aorta arteries from 7-12 EC-KO and 21-28 WT were studied. Figure 6. Vasodilation in coronary arteries measured ex vivo in small wire organ bath set-ups. Relaxations to ACh (A), SNP induced vasodilatation (B), ADPβS (C) and UTPγS (D) in coronary rings preconstricted with U46619. Relaxations to ADPβS (E) and UTPγS (F) in coronary rings preconstricted with KCl 30mM. \*\*\* = p<0.0001 (GLM-RM, EC-KO-3) months vs WT- 3 months and EC-KO- 5 months vs WT- 5 months). At 3 months coronary arteries from 7 EC-KO and 8-9 WT were studied. At 5 months arteries from 7 EC-KO and 10 WT were studied. Figure 7. Levels of eNOS and scanning electron microscopy. Protein expression levels expressed as % of WT control in lung of (A) eNOS and p-eNOS over actin (n=5 EC-KO and

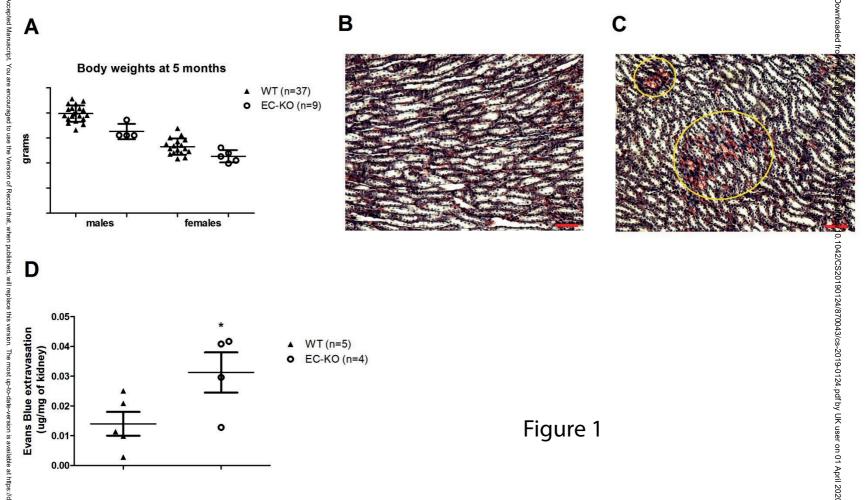
6 WT), (B) Representative scanning electron microscopy images of the endothelium (n=5 EC-

cells (panel E). Asterisks mark vascular lumen.

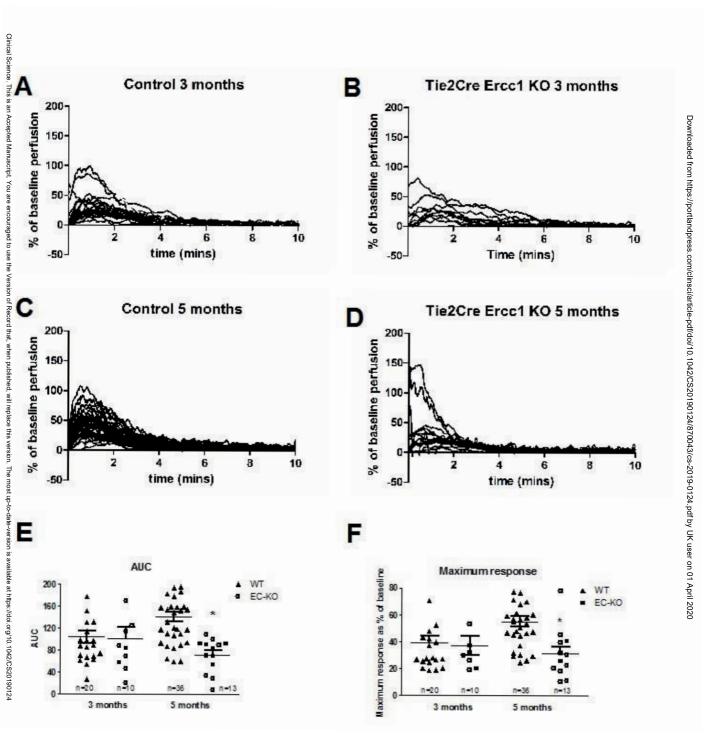
p<0.05, t-test. (D) Representative blot of ERCC1.					
Figure 8. Aortic wall dimensions. All measurements were performed on eosin-stained					
cryosections at 50x magnification using calibrated QWin software (Leica, Germany). Panel A					
- F depict the various dimension variables as indicated above the panels. 'Internal' and					
'External' refer to the use of respectively the internal and external border of the lamina media					
as reference points for the measurements. *; $p < 0.05$ , t-test.					
<b>Figure 9. P21 staining.</b> Photographs A through C show p21 staining in aortic tissue of EC-					
rigure 7. 121 stanning. I notographs 71 through C show p21 stanning in across disease of Ec					
KO (A) and WT (B). The endothelial localization is evident at 40 x magnification (closed					
arrowheads), and at larger magnification (80 x) the nuclear localization of p21 is visible					
(Panel A, open arrowhead). The p21-positive cell in panel A display the typical cobblestone					
appearance and localization on the lamina elastica interna (L.E.I), identifying the positive					
cells as endothelial cells. WT show p21-negative endothelial cell nuclei (B, grey arrowhead).					
Photographs C through E show p21 staining in the kidney in EC-KO (C,D) and WT (E). p21-					
positive cells are present along vascular lumen (closed arrowheads), along tubuli (grey					
arrowheads) and in glomeruli (gl; open arrowheads) (panel C). Panel D shows positive cells					
along the lumen of the vessel wall at higher magnification. WT mice did not present positive					

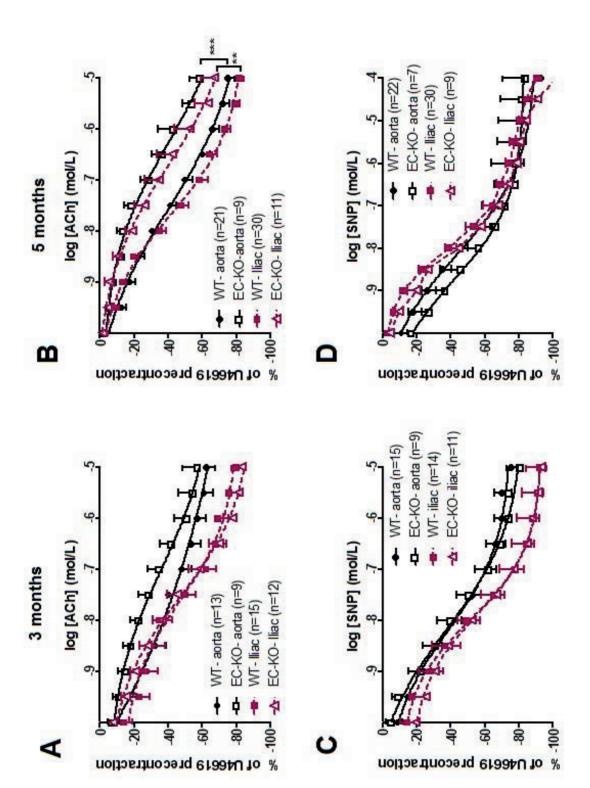
KO and 5 WT), and (C) expression of ERCC1 (arrowhead) (n=4 for both WT and EC-KO). \*:

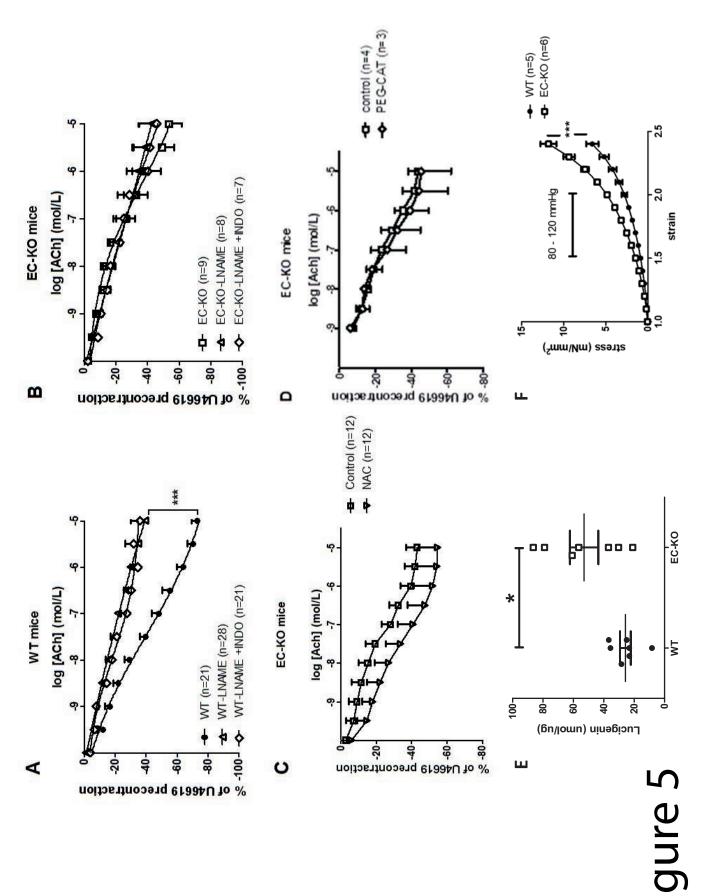
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## Figure 2

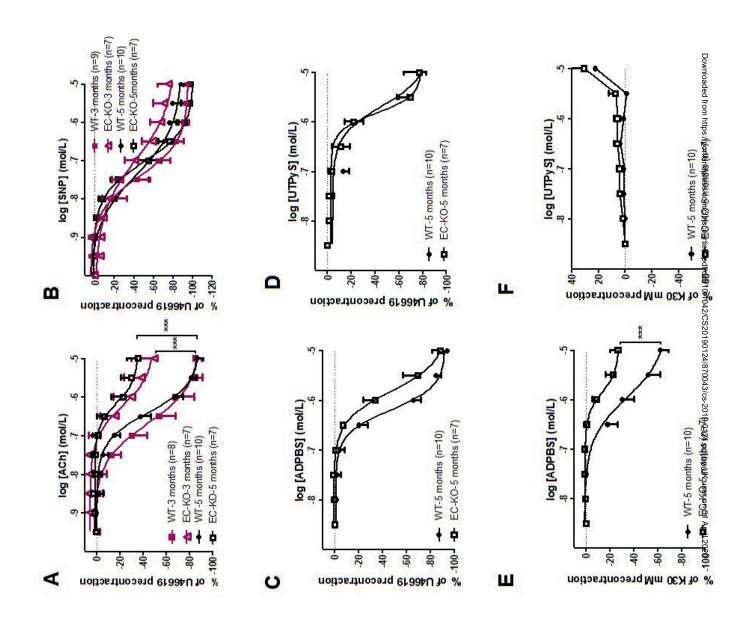


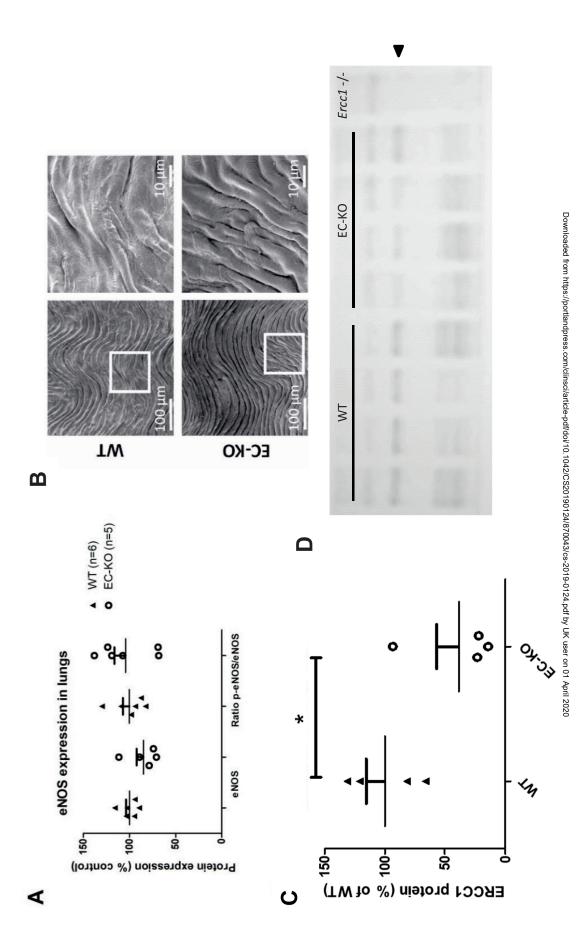




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## Figure 6





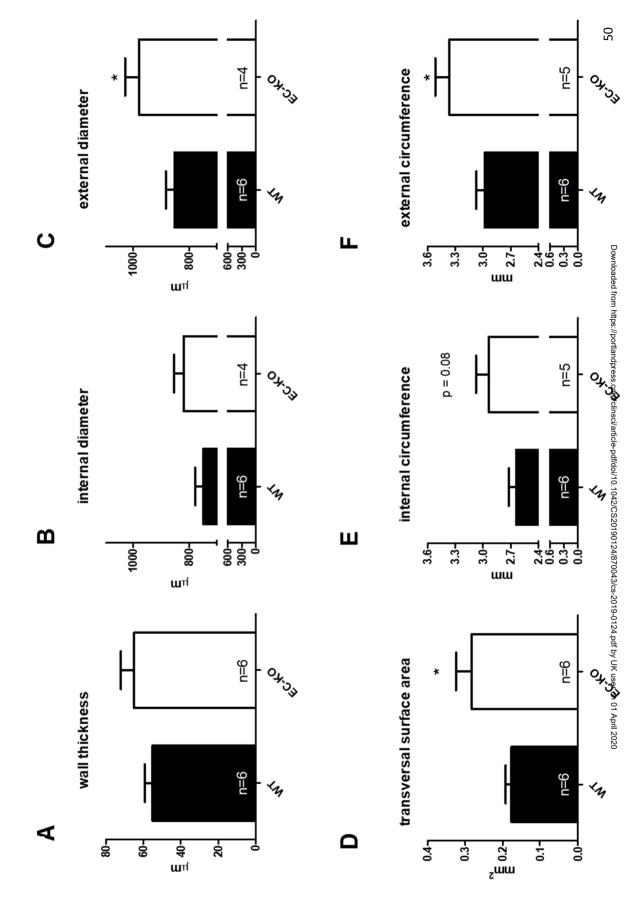


Figure 9 В . 240x 20 μm 80x 10 μm 10 μm 20 μm 80x L.E.I. L.E.I. 10 μm 40x 80x 20 μm 40x Ε D