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Standardization of an isolated pig heart preparation with parabiotic circulation: methodological considerations

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Abstract

In the present study we standardized an experimental model of parabiotic circulation of isolated pig heart. The isolated heart was perfused with arterial blood from a second animal as support and submitted to regional ischemia for 30 min, followed by total ischemia for 90 min and reperfusion for 90 min. Parameters for measurement of ventricular performance using different indices measured directly or indirectly from intraventricular pressure were defined as: maximum peak pressure, final diastolic pressure, pressure developed, first derivative of maximum pressure (dP/dt_{max}), first derivative of minimum pressure (dP/dt_{min}), systolic stress of the left ventricle (σ_s), and maximum elastance of the left ventricle. Isolated hearts subjected to regional and global ischemia presented significant worsening of all measured parameters. Less discriminative parameters were dP/dt_{max} and dP/dt_{min} . Elastance was the most sensitive parameter during the reperfusion period, demonstrating an early loss of ventricular function during reperfusion. The model proved to be stable and reproducible and permitted the study of several variables in the isolated heart, such as ischemia and reperfusion phenomena, the effects of different drugs, surgical interventions, etc. The model introduces an advantage over the classical models which use crystalloid solutions as perfusate, because parabiotic circulation mimics heart surgery with extracorporeal circulation.

Key words

- Isolated heart
- Ischemia
- Parabiotic circulation
- Reperfusion
- Model

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Introduction

Oscar Langendorff was the first to describe a method to investigate mechanical activity in isolated mammalian hearts (1). According to Döring (2), the method proposed by Langendorff at the end of the nineteenth century was widely accepted for the mechanical, coronary and metabolic study of

isolated mammalian hearts.

Heymans and Kochmann (3) replaced the original circuit with parabiotic circulation using an animal support. Various kinds of aqueous solutions were used for perfusion but certain specifications were followed for Langendorff type coronary blood flow preparations. In clinical practice, preparations utilizing blood for perfusion seem to have greater

applicability (4-7).

Although the Langendorff isolated heart preparation with parabolic circulation is substantially more complex than the classical preparation with the crystalloid solution, its scientific utility has greatly increased. A 10-year survey of the English scientific literature revealed that few references have been made to the standardization of blood-perfused isolated porcine heart models, the anesthesia of the support animal, maintenance of the model or the perfusion time achieved. Thus, the objective of the present study was to describe the standardization of an isolated porcine heart model with parabolic circulation.

Material and Methods

Animal model

Pigs aged on average 15 weeks were used because of their similarity to humans in terms of anatomy and ischemic response (8,9). Each experiment utilized two animals; the heavier animal weighing approximately 40 kg was the support animal and the lighter animal weighing approximately 20 kg supplied the isolated heart.

Support animal. Preanesthetic medication applied intramuscularly consisted of 1 mg atropine and 25 mg/kg ketamine. An intravenous injection containing 12.5 µg/kg fentanyl, 15 mg/kg pentobarbital and 8 mg pancuronium bromide was then performed. A 12.5-mg/kg dose of ketamine was applied hourly and a 1-mg dose of pancuronium bromide whenever needed (10). An orotracheal tube was inserted and the animal was placed on volume mechanical ventilation.

Animal donor. The preanesthetic medication applied intramuscularly contained 1 mg atropine and 25 mg/kg ketamine. A dose of 20 mg/kg pentobarbital was administered after establishing a venous access. An orotracheal tube was inserted and the animal was placed on pressurized mechanical ventilation.

Surgical technique

Support animal. Bilateral cervicotomy was performed to cannulate the left internal jugular vein (venous access), the left carotid (to monitor mean arterial pressure), the right internal jugular (perfusion system venous return), and the right carotid (perfusion system arterial blood). Heparin (500 IU/kg) was injected into the left internal jugular.

Animal donor. Median sternotomy. A dose of 500 IU/kg heparin was injected into the right atrium. The inferior and superior venae cavae were occluded and the heart was rapidly excised. The largest possible portion of the right atrium was removed, with preservation of the right coronary artery. The mitral valve was destroyed by sectioning the chordae tendineae and flaps and the mitral ring were closed with 2.0 polyester purse string sutures. A needle thermometer was inserted into the interventricular septum and a previously prepared latex balloon was inserted into the left ventricular cavity, which was then fixed to a plastic support and tied to the mitral ring. During this procedure, the apex of the left ventricle was perforated to permit drainage of blood from the Thebesian system of the left ventricle. A cannula was inserted into the ascending aorta and tied with a 3.0 polyester polyfilament to allow coronary perfusion via the aorta. The anterior interventricular coronary artery was dissected to permit placement of the minivascular clip at the appropriate time. A cannula was connected to the aorta with a previously prepared perfusion system and infusion of the aorta was started.

Perfusion system. The system was planned so that it would permit continuous retrograde perfusion of the isolated heart at a constant pressure, independent of the support animal's arterial pressure (Figure 1).

Experimental methodology

Perfusion of the isolated heart coronaries

was initiated and the myocardial septum temperature was expected to reach 36°C. In case of ventricular fibrillation, 5-joule shocks were applied to reestablish orderly electrical activity of the isolated heart. The model was stabilized for 20 min while the intraventricular pressure was measured. This was followed by the induction of myocardial regional ischemia, which was standardized by dissecting the anterior interventricular branch before the first diagonal branch and occluding it for 30 min.

After 30 min of regional ischemia, the microvascular clip was withdrawn, the heart was subjected to global ischemia for 90 min and reperfusion was initiated. The heart was defibrillated when the septal temperature reached 36°C and the pressure measured every 30 min for a period of 90 min.

Atrial pacemakers with a frequency of 160 bpm were used to stimulate all the isolated hearts. At the end of this procedure, the support animal was sacrificed. The isolated heart as well as the right ventricular wall, the atria and blood vessels were dissected according to the technique of Brooks et al. (11), and the left ventricle was weighed on an analytical scale to obtain its wet weight.

Method for the measurement of intraventricular pressure

The balloon introduced through the mitral ring after the destruction of the valve had a plastic support 1.5 cm in diameter. This plastic support permitted two catheters having an internal diameter of 2 mm to communicate with the balloon in such a way that during infusion of volume the pressure developed by the balloon in the left ventricle was also measured. The balloon was specifically designed to hold a volume of 60 ml without an increase in its internal pressure.

After stabilizing the isolated heart for 20 min, 5 ml saline was injected into the balloon at 1-min intervals to stabilize the intraventricular pressure. The largest possible vol-

ume of the balloon that maintained the diastolic pressure at 0 mmHg was determined. This volume was denoted V_0 and was then increased 2 ml at a time until the pressure developed by the left ventricle reached its maximum value. This volume was denoted V_{max} . This method, described by Strömer et al. (12), utilized the V_{max} to normalize the ventricular volume used for plotting and comparing data.

Two functional points of the volume pressure curve, 50 and 100% of V_{max} , were used to compare the results.

In addition, the following intraventricular pressure data were obtained: maximum peak pressure, final diastolic pressure, pressure developed, first derivative of maximum pressure (dP/dt_{max}), first derivative of minimum pressure (dP/dt_{min}), systolic stress of the left ventricle (σ_s), and maximum elastance of the left ventricle (E_{max}).

Systolic stress of the left ventricle was

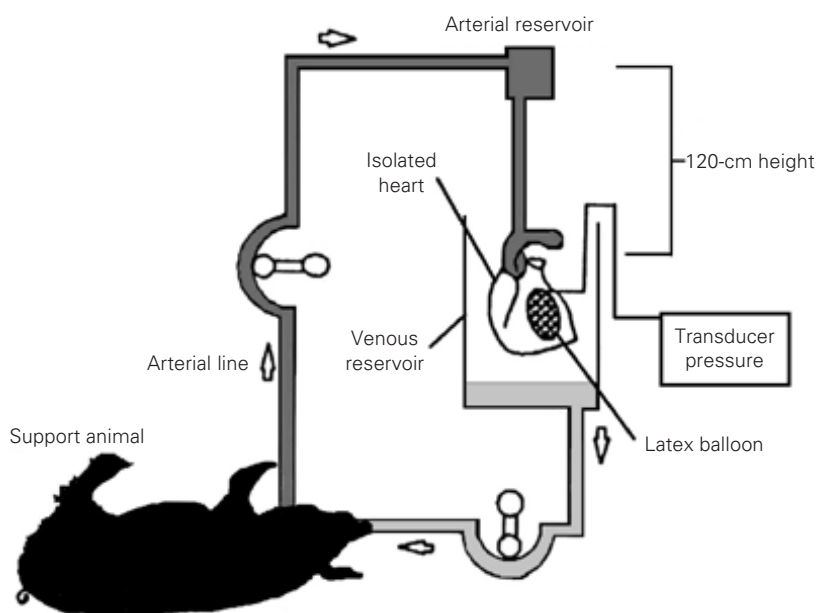


Figure 1. Diagram of the perfusion system in the isolated heart. Dark gray color is used to represent arterial blood. The arterial pump sends the blood to the conventional cardiotomy reservoir, which is located 120 cm above the isolated heart. The venous reservoir has a heat exchanger that warms the effluent blood from the isolated heart and returns it to the support animal through another pump that is represented in light gray. The intraventricular balloon is connected to a monitor to measure intraventricular pressure.

obtained using the measurements of ventricular pressure, balloon volume, and weight of left ventricle (11).

The radius of the left ventricle, R_1 , was calculated using the formula: $R_1^{1/3} = V_b/4/3 \pi$, where V_b = volume of the intraventricular balloon assuming that the shape of the left ventricle is spherical.

The volume of the left ventricle is the total volume of the balloon plus the volume of the left ventricle wall. The formula for determining the volume of the left ventricle is: volume of the left ventricle wall = weight of left ventricle/1.05, where 1.05 is the specific density of the myocardium. Volume of the ventricle (V_L) = $4/3 \pi (R_1 + h)^3$ and $h = (V_b/4/3 \pi)^{1/3} - R_1$, where h is the thickness of the left ventricle wall.

Systolic stress was calculated according to the Laplace Law as described by Mirsky (13): $\sigma_s = P_s[(R_1^2/h)/(2R_1 + h)]$, where P_s is the maximum systolic pressure, R_1 is the radius of the left ventricle with a determined volume in the balloon, and h is the thickness of the left ventricle wall.

E_{max} was calculated by linear regression of the maximum systolic curves obtained for intraventricular volume as described by Suga (14).

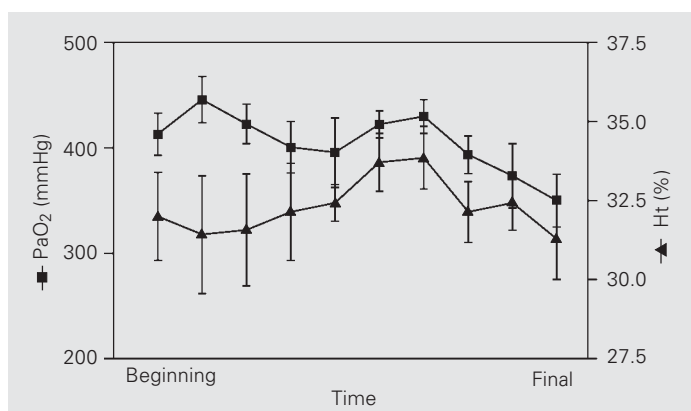


Figure 2. Perfusion parameters of the isolated heart. Hematocrit was constant without transfusions. The mean hematocrit (Ht, triangles) value of perfused blood was $31.30 \pm 3.40\%$ (95% CI, 28.14 to 34.43%). No significant differences were observed for any of the intervals studied. The oxygen supply to the isolated heart remained constant (PaO_2 , squares), never reaching values of less than 300 mmHg. Data are reported as means \pm 2 SEM.

Statistical analysis

Data are reported as means \pm 2 SEM. The Student *t*-test was used to compare data obtained before and after global ischemia in the samples studied. Analysis of variance (ANOVA) was used to assess variations in the gasometric parameters and the Dunnett test to identify the differences between groups.

ANOVA was also used to evaluate elastance and compliance and the Dunnett test to identify the differences between groups.

The statistical package Graph Pad Prism 3.0 version for Windows (Graph Pad Software, San Diego, CA, USA, www.graphpad.com) was used for all statistical calculations, with the level of significance set at $P < 0.05$.

Results

Perfusion parameters

The initial hematocrit of perfused blood was $32.00 \pm 3.70\%$ (95% CI, 28.58 to 35.42%), with variations during the experiment as demonstrated in Figure 2. The mean hematocrit value of perfused blood was $31.30 \pm 3.40\%$ (95% CI, 28.14 to 34.43%). No significant differences were observed for any of the intervals studied. The oxygen supply to the isolated heart remained constant, never reaching values of less than 300 mmHg (Figure 2).

Isolated heart after regional and global ischemia

Reperfusion of the hearts was performed after 30 min of regional ischemia and 90 min of global ischemia, and intraventricular pressure and its derivatives were observed every 30 min.

Figure 3 illustrates the values obtained with 90 min of reperfusion for systolic and

diastolic pressure in comparison with values obtained during the control period. Diastolic pressure did not differ significantly from control at the 30- and 60-min reperfusion periods, but at the 90-min period a significant difference was observed compared to control.

Table 1, which shows 100% V_{max} values, demonstrated that systolic pressure was a differentiating factor that indicated deterioration for all the periods studied that was significantly different from the control group.

The pressure developed during all periods showed a significant reduction compared to control (Figure 4).

There was a significant reduction in dP/dt_{max} compared to control for all periods studied and a significant reduction in dP/dt_{min} compared to control for only two periods of study (Figure 5).

There was a significant reduction in systolic stress (σ_s) compared to control for all periods studied (Figure 6). The elastance values decreased significantly in comparison with the control at 30, 60 and 90 min of reperfusion (Figure 7).

Discussion

Support animal

A smaller animal donor was a better option because a large heart was not needed to obtain the parameters required for this study and the costs of the experiment were reduced.

The mean time required for the removal of the heart and for initiating perfusion of the isolated heart was 815.7 ± 109 s, similar to literature data regarding similar experiments conducted on cats and rats (15-17).

The mean weight of the donor animals was 22.00 kg, which was an adequate size for manipulating the heart, especially when the maximum volume of the latex balloon installed within the left ventricle was standardized. Therefore, the utilization of smaller

animals does not seem to be a limiting factor. The use of smaller hearts in the preparation of the “working heart” type may be more

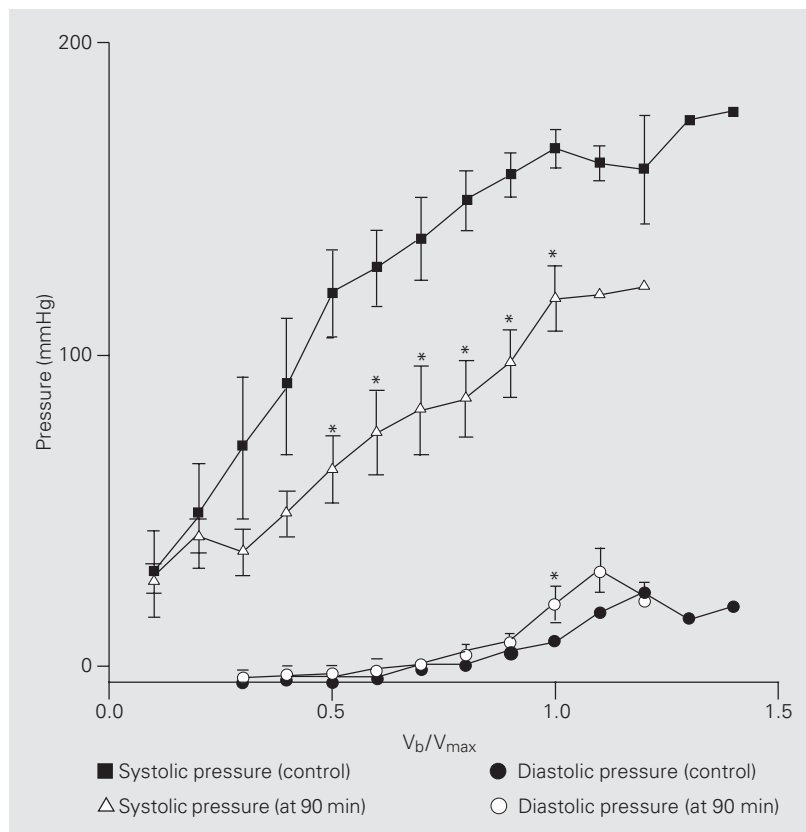


Figure 3. Systolic and diastolic pressure during the control period and after 90-min reperfusion. Data are reported as means \pm 2 SEM. * $P < 0.05$ compared to respective control (Student *t*-test).

Table 1. Values with 100% V_{max} .

Parameters	Control (N = 7)	Reperfusion		
		30 min (N = 7)	60 min (N = 7)	90 min (N = 6)
P_s	163.30 \pm 6.21	131.70 \pm 4.60*	131.70 \pm 8.24*	100.70 \pm 9.62*
P_d	7.43 \pm 1.56	11.14 \pm 4.73	14.00 \pm 5.95	19.50 \pm 4.73*
$P_{dev.}$	156.30 \pm 5.71	121.90 \pm 8.79*	116.60 \pm 0.85*	100.00 \pm 9.67*
dP/dt_{max}	1418.00 \pm 71.15	1188.00 \pm 93.70*	1159.00 \pm 93.30*	1027.00 \pm 31.40*
dP/dt_{min}	-889.00 \pm 73.45	-858.10 \pm 86.21	-768.90 \pm 63.04	-710.80 \pm 60.79
σ_s	161.60 \pm 4.45	102.70 \pm 14.02*	110.70 \pm 6.90*	101.00 \pm 0.18*

Observe that with 30, 60 and 90 min reperfusion, all parameters, except dP/dt_{min} , were significantly different compared to 100% V_{max} . V_{max} : maximum value; P_s : maximum peak pressure; P_d : final diastolic pressure; $P_{dev.}$: pressure developed; dP/dt_{max} and dP/dt_{min} : first derivative of maximum and minimum pressures, respectively; σ_s : systolic stress of the left ventricle.

* $P < 0.05$ compared to control values (Student *t*-test)

interesting because the cardiac output developed will be proportional. This means less blood circulating in the system and less damage to blood components.

Porcine models were chosen because the coronary anatomy and circulatory system of these animals are similar to those of man (8,9). The collateral coronary system is also similar because both species have few pre-existing collateral coronary arteries, although they have the capacity to develop a collateral circulatory system after myocardial infarction (18). Although the myocardial collateral circulation in humans is heterogeneous, the porcine heart can be used as a highly sensitive model for the study of therapeutic interventions (19). A big difference in the porcine and human vascular anatomy is the hemiazygous vein that drains directly into the coronary sinus, but this did not interfere

with any phase of the experiment. Since none of the cases required therapeutic transfusion, there was no need for blood typing. The use of a large support animal and a small volume of crystalloid solution were initially effective in maintaining almost normal hematocrit levels. Vasoactive drugs were not needed to maintain the support animal, which was an important factor since these drugs could cause secondary problems in the isolated heart, involving the inclusion of another variable in the protocol or the use of another vasoactive group of drugs.

Perfusion circuit

The perfusion circuit of the isolated heart with a conventional cardiotomy reservoir placed at a height of 120 cm was very practical. The perfused heart model at constant pressure excluded the variations in the performance of an isolated heart dependent on the perfusion pressure.

Perfusion of the heart with different pressures produces a varied performance of ventricular function. Hence, when the perfusion pressure is approximately 50 mmHg, the performance is inferior to that at 90-mmHg pressure (20). Another reason for using constant pressure was to avoid conflicting results when using a constant perfusion flow model. The models that use a constant flow in coronary perfusion present perfusion pressure variations due to their high or low resis-

Figure 4. Pressure developed during the control period and after 90-min reperfusion. Data are reported as means \pm 2 SEM. * $P < 0.05$ compared to control (Student *t*-test).

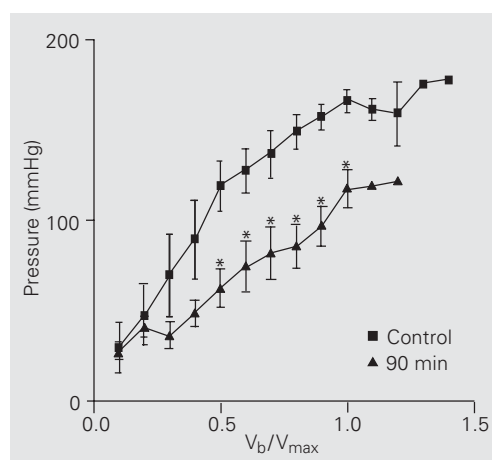
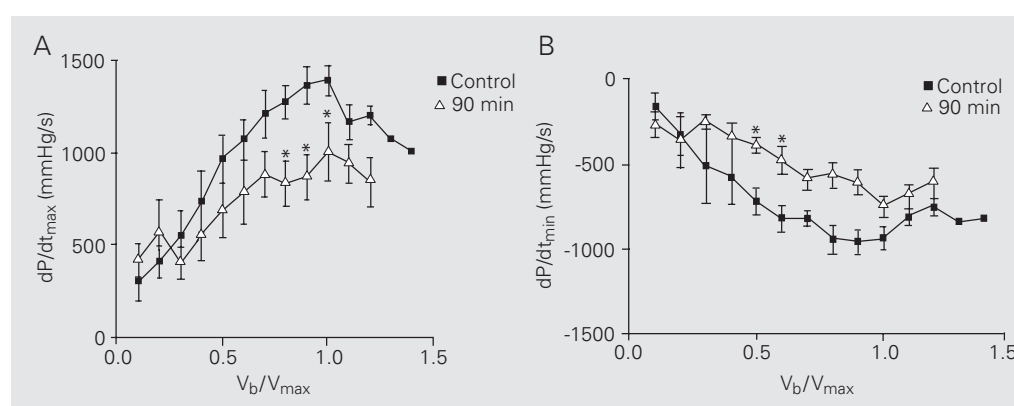


Figure 5. First derivative of maximum (dP/dt_{max} , A) and minimum (dP/dt_{min} , B) pressures during the control period and after 90-min reperfusion. Data are reported as means \pm 2 SEM. * $P < 0.05$ compared to control (Student *t*-test).



tance. This could result in a better or poorer ventricular performance and also in changes in myocardial oxygen consumption secondary to the Gregg phenomenon (21). This phenomenon has been discussed in the literature and some points are cited below:

1) Hypoperfusion: the best performance is secondary to an increase in coronary perfusion pressure resulting from an initial hypoperfusion of the myocardium. This is a pathological explanation of the Gregg phenomenon as a nonphysiological fact (22).

2) It has been suggested in the literature that the Gregg phenomenon only occurs in a "nonworking heart" (23). However, this suggestion is not often supported in the literature. Other investigators have observed this phenomenon in the "working heart" (24), which contradicts the findings by Ross Jr. et al. (23).

3) Distention of the coronary arteries as proposed by Lochner et al. (25): an increase in coronary perfusion pressure produces distention, which causes distention of the surrounding myocardial fibers resulting in improved cardiac performance secondary to the Frank-Starling mechanism.

4) Oxygen flow and supply: according to Abel and Reis (26), in the absence of previous ischemia, an increased cardiac performance in the Gregg phenomenon is secondary to an increase in the flow and supply of oxygen. In this case, the Gregg phenomenon would only be a physiological response.

Hence, it seems reasonable to conclude that the Gregg phenomenon occurs and can be observed in working and nonworking heart preparations as long as they are not grossly hypoperfused and the coronary circulation remains intact. Another finding related to the Gregg phenomenon is the Anrep effect.

Knowlton and Starling (27), in 1912, observed that a rapid increase in aortic pressure increased resistance to the flow in isolated heart-lung preparations, causing a positive inotropic effect on the isolated heart,

which results in a gradual reduction of the diastolic volume of the left ventricle after a transitory dilation. In 1912, Anrep (28) also described this phenomenon. This slow improvement in cardiac function, a few seconds after an increase in aortic pressure, was called the Anrep phenomenon (29).

According to Monroe et al. (30), this is due to momentary subendocardial ischemia and redistribution of the secondary flow. Although the Anrep effect on working or nonworking hearts with constant flow or constant pressure as proposed by Monroe et al. (30) is debatable, no study has been conducted to test this hypothesis (29). Based on the data cited above, we opted for a model with constant pressure in order to avoid variable performance related to the Gregg phenomenon and the Anrep effect and not to interventions in the isolated heart.

The chamber prepared to receive the effluent blood proved to be adequate as it accommodated the isolated heart well and

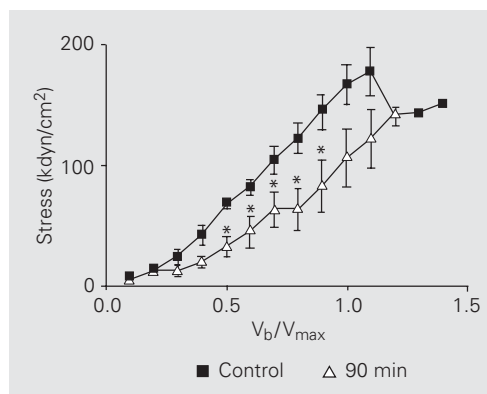


Figure 6. Systolic stress of the left ventricle. Data are reported as means \pm 2 SEM. *P<0.05 compared to control (Student *t*-test).

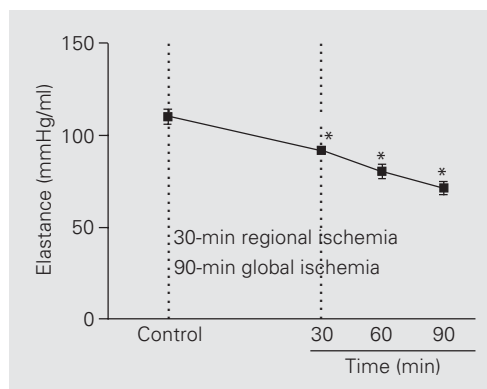


Figure 7. Values of elastance of the left ventricle for the different periods of reperfusion and control. Data are reported as means \pm 2 SEM. *P<0.05 compared to control (ANOVA).

had an efficient heat exchanger that warmed the blood returning to the support animal.

Polyvinyl tubes measuring 1/4 inch in internal diameter were used so that the initial filling volume was small, as shown by the minimum hematocrit variation of the support animal.

The same system but with smaller reservoirs and tubes with small internal diameters may be used for smaller animals.

Perfusion parameters to the isolated heart

Characterization of the perfusion of the isolated heart is important as it guarantees the control of variables such pH, electrolytes and hematocrit.

Although Heymans and Kochmann (3) described parabolic circulation in 1904, it was only recently that the procedure started to be used more frequently. Pasini et al. (5) recently described the characterization of this model with regard to the response of the support animal to anesthesia, heparinization and parabolic circulation. Anesthetic induction and maintenance did not interfere with the arterial pressure of the support animal. Hemodynamic stability was good and in accordance with the findings of Pasini et al. (5).

There was no need for transfusion since the hematocrit level of the support animal remained stable, also in agreement with Pasini et al. (5) and Budrikis et al. (31). This is mainly because only a small volume was needed to fill the perfusion system and to return all the blood to the support animal. Saline (0.9%) was chosen to fill the system because it was easily available and did not contain potassium, with consequent reduced costs.

The partial pressure of oxygen supplied to the isolated heart was always above 300 mmHg, without a statistically significant variation. These data agree with those obtained by Budrikis et al. (31) who used parabolic circulation in pigs with the PaO₂ always above 300 mmHg. Li et al. (20) utilized

parabolic circulation during 6 h of perfusion with the PaO₂ always higher than 200 mmHg and obtained results very similar to those obtained in the present study.

In our study, we did not measure the circulating catecholamines but Pasini et al. (5) showed that they increased after anesthesia and surgical manipulation, an event closely similar to the situation to which a patient is submitted during extracorporeal circulation.

Monroe et al. (15) demonstrated the role of the support animal in relation to the supply of catecholamines and its possible action in clearance produced by the isolated heart in dogs with parabolic circulation. In their experiment, they excluded the support animal after stabilization and perfused the isolated heart with an isolated lung. There was a reduction in the effluent catecholamines in parallel to a fall in cardiac performance. On returning perfusion to the support animal, the catecholamines again increased and the performance also improved, regaining original values.

After the introduction of heparin and perfusion of the isolated heart, another similarity observed between this parabolic circulatory model and the clinical situation was the increase in the level of fatty acids circulating as a result of the action of heparin on the endothelial lipase and the liberation of catecholamines (5). Without any doubt, this increase in fatty acids influences the cardiac metabolism, which makes this model especially interesting because the metabolic changes and the myocardial perfusion conditions are similar to those that occur in human hearts submitted to extracorporeal circulatory surgery. The isolated heart predominantly uses fatty acids in its metabolism and this is very close to clinical reality (32).

Masuda et al. (4) demonstrated that the performance of crystalloid-perfused hearts depended on the perfusion pressure. Blood perfused hearts presented fewer variations in performance when there were great varia-

tions in perfusion pressure. This indicated that preparations using blood had greater applicability in therapeutic interventions.

Isolated hearts respond differently to therapeutic intervention depending on whether the perfusion is done with blood or crystalloid solutions. When blood preparations are utilized, the responses of the heart are more similar to those observed in clinical practice than in the case of crystalloid-perfused hearts (6).

This demonstrates the utility of the model used in this study, which is ideal for the study of cardiac performance under different perfusion conditions using different substrates, drugs and surgical interventions, etc.

Methodology for the measurement of ventricular parameters

Langendorff type preparations have often been used to measure contractile function (12). Nevertheless, a common problem is comparing different hearts in different situations. The hearts may vary in size, degree of hypertrophy or dilation.

Heart rate, temperature and perfusion parameters can be normalized but the intraventricular volume cannot be fixed.

Various strategies have been described. Brooks et al. (11) studied hypertrophied hearts and set a reference volume of 0.025 ml/kg for the donor animal, which is used for comparing different hearts. Eberli et al. (33), Feldman et al. (34), and Lorell et al. (35) studied hearts with concentric ventricular hypertrophy and fixed the ventricular volume for a diastolic pressure of 10 mmHg. Glass et al. (36) used the necessary intraventricular volume (V_{\max}) to compare maximum peak pressure developed. This strategy is very similar to the methods used to study papillary muscles, whereby the investigator measures the length of the longest papillary muscle (L_{\max}) to determine the highest developed tension. As L_{\max} standardizes the other values, it is possible to compare vary-

ing lengths of papillary muscles (12).

In the present study, the ventricular volume was incremented and standardized by V_{\max} and the curves obtained for each reading were compared with 50 and 100% V_{\max} situations.

According to Strömer et al. (12), 50% V_{\max} was sufficient to determine the differences when conducting any kind of study on hearts. The authors emphasized the standardization of intraventricular volume followed by a comparison of the hearts in terms of the same physiological factor.

In the present study, the physiological factors were assessed with 50 and 100% V_{\max} , and it was observed that 100% V_{\max} had a greater capacity to demonstrate differences and therefore was the most discerning factor.

The hemodynamic parameters studied were parameters commonly used (2). The physiological aspect at 100% V_{\max} demonstrated significant differences throughout the reperfusion periods in terms of systolic pressure, developed pressure and dP/dt_{\max} .

Diastolic pressure presented a gradual increase during the reperfusion process with a significant difference only at 90 min of reperfusion. This occurrence may have been due to very similar values or a greater difficulty in demonstrating alterations in the diastolic function of damaged hearts. As the dP/dt_{\min} did not demonstrate statistically significant alterations, it was not a sensitive parameter for diastolic function in this study.

Systolic stress was the only variable that showed statistically significant differences in all the reperfusion periods at 50 and 100% V_{\max} . According to Brooks et al. (11), it is a highly sensitive measure of the cardiac contractile condition.

Elastance demonstrates its capacity to create pressure when the intraventricular volume increases. Ventricles that function well produce an increase in pressure when they undergo distention in comparison with poorly functioning ventricles. Maximum

elastance is a highly sensitive indicator for demonstrating deterioration of the myocardial contractile condition. There was a reduction in E_{\max} 30 min after the beginning of perfusion, which deteriorated during its course and reached its maximum fall at 90 min of perfusion. During the reperfusion of the hearts, it was observed that maximum elastance permitted early detection of the ventricular function alterations that occurred during reperfusion of the hearts. This index, which is independent of the preload and afterload, has proved to be highly sensitive to changes in the contractile condition and is in accordance with the findings of Suga (14), Sagawa et al. (37), Burkhoff and Sagawa (38) and Ko et al. (39).

Blood-perfused hearts present smaller

variations in coronary blood flow because of viscosity and oncotic properties (12). Although blood flow was not measured in this experiment, we believe that it was very close to clinical reality.

In summary, the model presented is easily executable, provides a heart with controllable variables that help develop different methods of study, but the team involved in the study should undergo a period of training. Further studies using this preparation will achieve greater proximity to clinical reality because of the above cited peculiarities and will provide a powerful tool for the clinical investigation of new drugs and surgical interventions, as well as for studies on ischemia and myocardial reperfusion.

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