



Ramírez-Torres, A., Penta, R., Rodríguez-Ramos, R. and Grillo, A. (2019) Effective properties of hierarchical fiber-reinforced composites via a three-scale asymptotic homogenization approach. *Mathematics and Mechanics of Solids*, 24(11), pp. 3554-3574. (doi: [10.1177/1081286519847687](https://doi.org/10.1177/1081286519847687))

There may be differences between this version and the published version. You are advised to consult the publisher's version if you wish to cite from it.

<http://eprints.gla.ac.uk/195989/>

Deposited on: 31 March 2020

Enlighten – Research publications by members of the University of Glasgow
<http://eprints.gla.ac.uk>

Effective properties of hierarchical fiber-reinforced composites via a three-scale asymptotic homogenization approach

Mathematics and Mechanics of Solids
XX(X):1–26
© The Author(s) 2018
Reprints and permission:
sagepub.co.uk/journalsPermissions.nav
DOI: 10.1177/ToBeAssigned
www.sagepub.com/

SAGE

Ariel Ramírez-Torres¹, Raimondo Penta², Reinaldo Rodríguez-Ramos³ and Alfio Grillo¹

Abstract

The study of the properties of multiscale composites is of great interest in engineering and biology. Particularly, hierarchical composite structures can be found in nature and in engineering. During the past decades, the multiscale asymptotic homogenization technique has shown its potential in the description of such composites by taking advantage of their characteristics at the smaller scales, ciphered in the so-called *effective coefficients*. Here, we extend previous works by studying the in-plane and out-of-plane effective properties of hierarchical linear elastic solid composites via a three-scale asymptotic homogenization technique. In particular, the approach is adjusted for a multiscale composite with a square-symmetric arrangement of uniaxially aligned cylindrical fibers, and the formulae for computing its effective properties are provided. Finally, we show the potential of the proposed asymptotic homogenization procedure by modeling the effective properties of musculoskeletal mineralized tissues, and compare the results with theoretical and experimental data for bone and tendon tissues.

Keywords

Hierarchical composites, Three-scale asymptotic homogenization, Fiber-reinforced composites, Musculoskeletal mineralized tissues, Effective coefficients

¹ Dipartimento di Scienze Matematiche "G. L. Lagrange", Politecnico di Torino, 10129. Torino, Italia

² School of Mathematics and Statistics, Mathematics and Statistics Building, University of Glasgow, University Place, Glasgow G128QQ, UK

³ Departamento de Matemáticas, Facultad de Matemática y Computación, Universidad de La Habana, CP 10400, La Habana, Cuba

Corresponding author:

Ariel Ramírez-Torres, Dipartimento di Scienze Matematiche "G. L. Lagrange", Politecnico di Torino, 10129. Torino, Italia.
Email: ariel.ramirez@polito.it

Introduction

Hierarchical solids are multiscale materials made of different phases which themselves exhibit a finer scale structure. Several examples of the existence of hierarchical composite structures can be found in nature such as musculoskeletal mineralized tissues (MMTs), lotus leaves, among many others. Nowadays, the study of the physical properties of multiscale composite materials is of great interest due to its utility, for instance, in the modeling and design of bioinspired and biomimetic hierarchical materials¹⁻³. In particular, MMTs constitute a widely studied class of hierarchical composite materials. For instance, we refer to the compilation of articles edited by Cowin⁴ on structural and mechanical properties of bone.

The different homogenization techniques used in the modeling of multiscale composites have the important advantage of decoupling the structural characteristic lengths. In the case of linear elastic composite materials, the scientific literature develops in two main approaches, the asymptotic homogenization and the average field theory (see, e.g., the review paper⁵ and references therein). On one hand, average field techniques^{6,7} aim to find the effective elastic properties which relate the fine scale strain and stress averages over a representative volume, characterizing, in an ideal form, the material heterogeneity. On the other hand, the asymptotic homogenization technique⁸⁻¹² exploits the scales separation among the characteristic lengths of the local structures and the one of the whole material by employing multiple scale expansions of the fields.

Multiscale asymptotic homogenization techniques take advantage of the information available at the smaller scales to obtain an effective description of the medium or phenomenon at its larger scales. In the scientific literature, there exist several works focusing on modeling and simulation of the macroscopic properties of hierarchical composite materials using average field techniques¹³⁻¹⁶, reiterated asymptotic homogenization^{9,17-25} and hybrid models²⁶. For instance, starting from the basic equations of the phases of a composite featuring a heterogeneous structure over several separated scales,¹⁷ achieved to deduce the phenomenological equations of a porous medium and, in the process, the authors also obtained the governing equations for the intermediate scales of the mixture. Afterwards, a rigorous foundation of the technique was given in¹⁸ focused on the heat equation for composites and in²⁷, a further generalization of reiterated homogenization was introduced via a three-scale convergence approach providing a groundwork where the asymptotic parameters independently approach zero. Moreover, in²², the authors adopted an asymptotic homogenization technique to obtain a homogenized model for a fluid saturated porous medium containing double porous substructures by considering a hierarchical porous arrangement. In²³, recurrent sequences of local and averaged elasticity problems for a fiber reinforced composite were written through the introduction of a power series expansion for each level. Furthermore, in²⁴, the authors considered a hierarchical laminated composite with the particularity that the microstructure presented a combination of linear and non-linear generalized periodicity. Therein, the solution of the problem was sought via a multi-step homogenization approach. In addition, a step-by-step approach to study the properties of bone using models of micromechanics and composite laminate theory was followed in¹⁵ and¹⁶. Finally, the approach in²⁶ presents a combination of Eshelby based techniques with the asymptotic homogenization to analyze in a bottom-up process the stiffening of old bone tissues. From a computational point of view, the work by²⁸ proposes a methodology for the development of adaptive methods for hierarchical modeling of elastic heterogeneous bodies.

In this work, we exploit the three-scale asymptotic homogenization approach developed in^{29,30} to investigate the effective properties of linear elastic, hierarchical, fiber-reinforced composites. The three-scale homogenization approach permits to individualize each hierarchical level and to investigate how the

49 properties at the lower scales influence the effective ones in a single scheme. In a previous work²⁹, the
 50 three-scale asymptotic technique has been applied to compute the effective shear modulus for hierarchical
 51 fiber-reinforced composites. Here, we go further and propose a procedure to compute the effective in-
 52 plane elastic coefficients, which involve the solution of coupled elastic problems. Furthermore, we show
 53 the potential of the multiscale asymptotic homogenization process by applying it to a biological scenario
 54 of interest. Specifically, we are interested in modeling the effective properties of MMTs by performing
 55 a parametric analysis of the mineral crystals' volume fraction. Since the goal is to offer a modeling tool
 56 for studying hierarchical composites, we conveniently adopt the modeling assumptions made in^{31,26}.
 57 In³¹, the authors studied the elastic stiffness tensor of a mineralized turkey leg tendon tissue using a
 58 multiscale model based on average fields Eshelby techniques, such as the Mori-Tanaka and the self-
 59 consistent schemes. In²⁶, the approach in³¹ was extended to the asymptotic homogenization technique
 60 by means of a hybrid hierarchical modeling framework applicable to MMTs, and capable to account for
 61 fused mineral structures in the composite tissue. The results of the present framework are consistent with
 62 the experimental and theoretical data reported in^{26,31}.

63 The manuscript is organized as follows. First, the physical and mathematical framework of the problem
 64 is introduced. Next, we present the principal results of the three-scale asymptotic homogenization
 65 technique and we address the general local problems associated with each hierarchical level. The in-plane
 66 and out-of-plane local problems for uniaxially fiber-reinforced hierarchical composites with isotropic
 67 constituents are also specified. In addition, the form of the effective coefficients is provided. Furthermore,
 68 we compute the effective properties of MMTs and compare the results with experimental and numerical
 69 data provided in the scientific literature. Finally, we discuss the current approach and give directions for
 70 future developments of the study.

71 Formulation of the problem

72 Geometrical description

73 Let us denote by $\Omega \subset \mathbb{R}^3$ a multiscale composite characterized by three well-separated characteristics
 74 lengths (see Fig. 1), namely ℓ_1 , ℓ_2 and L , and introduce the scaling parameters ε_1 and ε_2 as follows,

$$\varepsilon_1 = \frac{\ell_1}{L} \ll 1 \quad \text{and} \quad \varepsilon_2 = \frac{\ell_2}{L} \ll \varepsilon_1. \quad (1)$$

75 We note that in (1), we have amended a typo on the definition of ε_2 in previous works^{29,30}. From relation
 76 (1), two formally independent variables are introduced, i.e.

$$\eta = \frac{x}{\varepsilon_1} \quad \text{and} \quad \varsigma = \frac{x}{\varepsilon_2}. \quad (2)$$

77 In what follows, we consider each field and material property Φ^ε to be η - and ς - periodic and we introduce
 78 the notation $\Phi^\varepsilon(x) = \Phi(x, \eta, \varsigma)$.

79 At the first hierarchical level, the composite Ω comprises two solid constituents and is partitioned into
 80 two sub-domains $\Omega_m^{\varepsilon_1}$ and $\Omega_f^{\varepsilon_1}$. The former denotes the host phase (or matrix) and the latter represents
 81 a finite collection of disjoint subphases (e.g. inclusions or fibers). Specifically, $\bar{\Omega} = \bar{\Omega}_m^{\varepsilon_1} \cup \bar{\Omega}_f^{\varepsilon_1}$ with
 82 $\bar{\Omega}_m^{\varepsilon_1} \cap \bar{\Omega}_f^{\varepsilon_1} = \Omega_m^{\varepsilon_1} \cap \bar{\Omega}_f^{\varepsilon_1} = \emptyset$ and we denote with Γ^{ε_1} the interface between both constituents $\Omega_m^{\varepsilon_1}$ and
 83 $\Omega_f^{\varepsilon_1}$. Furthermore, we denote by \mathcal{Y} the unitary periodic cell containing a portion of the host phase \mathcal{Y}_m and

one subphase (or a finite collection of subphases) \mathcal{Y}_f . We enforce that the constituents of each periodic cell satisfy that $\overline{\mathcal{Y}} = \overline{\mathcal{Y}}_m \cup \overline{\mathcal{Y}}_f$ with $\overline{\mathcal{Y}}_m \cap \overline{\mathcal{Y}}_f = \mathcal{Y}_m \cap \overline{\mathcal{Y}}_f = \emptyset$, and we indicate with $\Gamma_{\mathcal{Y}}$ the interface between \mathcal{Y}_m and \mathcal{Y}_f .

At the second hierarchical level, we consider that each subphase $i\Omega_f^{\varepsilon_1}$ ($i = 1, \dots, N$) is also a composite material with periodic microstructure. We suppose that each subphase $i\Omega_f^{\varepsilon_1}$ is composed of a host phase $\Omega_m^{\varepsilon_2}$ with a finite number of subphases denoted by $\Omega_f^{\varepsilon_2}$. In particular, we assume that for each i , $i\overline{\Omega}_f^{\varepsilon_1} = \overline{\Omega}_m^{\varepsilon_2} \cup \overline{\Omega}_f^{\varepsilon_2}$ with $\overline{\Omega}_m^{\varepsilon_2} \cap \overline{\Omega}_f^{\varepsilon_2} = \Omega_m^{\varepsilon_2} \cap \overline{\Omega}_f^{\varepsilon_2} = \emptyset$ and the interface between $\Omega_m^{\varepsilon_2}$ and $\Omega_f^{\varepsilon_2}$ is denoted with Γ^{ε_2} . At this hierarchical level, \mathcal{Z} stands for the unitary periodic cell containing a portion of the host phase indicated with \mathcal{Z}_m and one subphase (or a finite collection of subphases) \mathcal{Z}_f . Analogously to the upper hierarchical level, we set $\overline{\mathcal{Z}} = \overline{\mathcal{Z}}_m \cup \overline{\mathcal{Z}}_f$, with $\overline{\mathcal{Z}}_m \cap \overline{\mathcal{Z}}_f = \mathcal{Z}_m \cap \overline{\mathcal{Z}}_f = \emptyset$ and we indicate with $\Gamma_{\mathcal{Z}}$ the interface between \mathcal{Z}_m and \mathcal{Z}_f .

In Table 1, we resume the symbols introduced above.

Table 1. Symbols and their description.

Symbol	Description
Ω	Multiscale composite body
$\Omega_m^{\varepsilon_1}$ ($\Omega_m^{\varepsilon_2}$)	Host (or matrix) phase at the ε_1 (ε_2)-hierarchical level
$\Omega_f^{\varepsilon_1}$ ($\Omega_f^{\varepsilon_2}$)	Finite collection of disjoint subphases at the ε_1 (ε_2)-hierarchical level
Γ^{ε_1} (Γ^{ε_2})	Interface between constituents $\Omega_m^{\varepsilon_1}$ and $\Omega_f^{\varepsilon_1}$ ($\Omega_m^{\varepsilon_2}$ and $\Omega_f^{\varepsilon_2}$)
\mathcal{Y} (\mathcal{Z})	Unitary periodic cell at the ε_1 (ε_2)-hierarchical
\mathcal{Y}_m (\mathcal{Z}_m)	level portion of $\Omega_m^{\varepsilon_1}$ ($\Omega_m^{\varepsilon_2}$) contained in the unitary cell \mathcal{Y} (\mathcal{Z})
\mathcal{Y}_f (\mathcal{Z}_f)	Finite collection of subphases $\Omega_f^{\varepsilon_1}$ ($\Omega_f^{\varepsilon_2}$) contained in the unitary cell \mathcal{Y} (\mathcal{Z})
$\Gamma_{\mathcal{Y}}$ ($\Gamma_{\mathcal{Z}}$)	Interface between \mathcal{Y}_m and \mathcal{Y}_f (\mathcal{Z}_m and \mathcal{Z}_f)

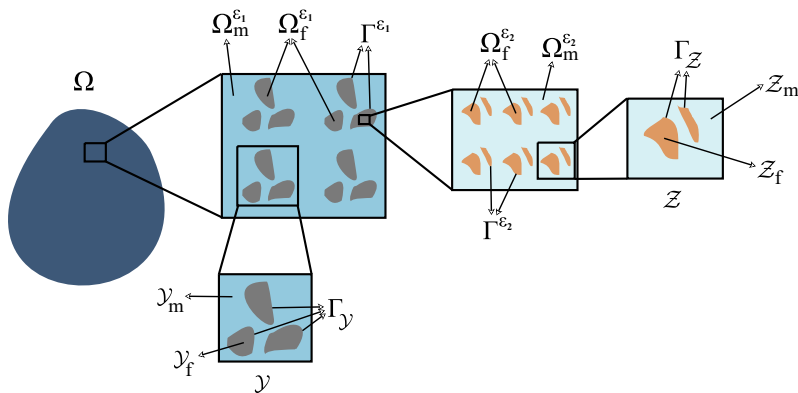


Figure 1. Schematic of the cross-section of a hierarchical periodic composite with three structural levels.

Formulation of the problem

We consider that the constitutive response of all the constituents of the hierarchical composite body Ω is linear elastic. This assumption implies that the constituents' constitutive relationships are all given by the formula,

$$\boldsymbol{\sigma}^\varepsilon = \mathcal{C}^\varepsilon : \mathbf{E}(\mathbf{u}^\varepsilon), \quad (3)$$

where $\mathbf{E}(\mathbf{u}^\varepsilon) := \text{Sym}(\text{Grad}\mathbf{u}^\varepsilon)$ represents the strain tensor under the hypothesis of small displacements \mathbf{u}^ε , and \mathcal{C}^ε is the fourth-order, positive definite elasticity tensor with both major and minor symmetries, i.e., component-wise, $\mathcal{C}_{ijkl}^\varepsilon = \mathcal{C}_{jikl}^\varepsilon = \mathcal{C}_{ijlk}^\varepsilon = \mathcal{C}_{klij}^\varepsilon$ ($i, j, k, l = 1, 2, 3$), and is supposed to be phase-wise smooth.

Then, ignoring inertia and volume forces, the differential problem arising from the (local) balance of linear momentum when equipped, for example, with Dirichlet-Neumann external boundary conditions reads

$$(\mathcal{P}^\varepsilon) \begin{cases} \text{Div}[\mathcal{C}^\varepsilon : \mathbf{E}(\mathbf{u}^\varepsilon)] = \mathbf{0}, & \text{in } \Omega \setminus (\Gamma^{\varepsilon_1} \cup \Gamma^{\varepsilon_2}), \\ \mathbf{u}^\varepsilon = \mathbf{u}^*, & \text{on } \partial\Omega_D, \\ [\mathcal{C}^\varepsilon : \mathbf{E}(\mathbf{u}^\varepsilon)] \cdot \mathbf{N} = \mathbf{S}^*, & \text{on } \partial\Omega_N, \end{cases} \quad (4)$$

where \mathbf{N} is the outward unit vector field normal to the boundary $\partial\Omega$ of Ω , \mathbf{u}^* is the displacement field prescribed on the Dirichlet portion of $\partial\Omega$, i.e., $\partial\Omega_D$, and \mathbf{S}^* is the field of tractions imposed on the Neumann boundary $\partial\Omega_N$. It holds that $\partial\Omega = \partial\Omega_D \cup \partial\Omega_N$, with $\partial\Omega_D \cap \partial\Omega_N = \emptyset$. Furthermore, continuity conditions for displacements and traction are imposed on both Γ^{ε_1} and Γ^{ε_2} , i.e.

$$[[\mathbf{u}^\varepsilon]] = \mathbf{0}, \quad \text{on } \Gamma^{\varepsilon_1} \cup \Gamma^{\varepsilon_2}, \quad (5a)$$

$$[[\mathcal{C}^\varepsilon : \mathbf{E}(\mathbf{u}^\varepsilon)] \cdot \mathbf{N}_Y] = \mathbf{0}, \quad \text{on } \Gamma^{\varepsilon_1}, \quad (5b)$$

$$[[\mathcal{C}^\varepsilon : \mathbf{E}(\mathbf{u}^\varepsilon)] \cdot \mathbf{N}_Z] = \mathbf{0}, \quad \text{on } \Gamma^{\varepsilon_2}, \quad (5c)$$

where \mathbf{N}_Y and \mathbf{N}_Z represent the outward unit vectors normal to the surfaces Γ^{ε_1} and Γ^{ε_2} , respectively. The operator $[[\cdot]]$ denotes the jump across the interface between two constituents in the same hierarchical level.

Three-scale asymptotic homogenization procedure

The property of separation of scales together with definition (2), imply that,

$$\text{Grad}\Phi^\varepsilon(x) = \text{Grad}_x\Phi(x, \eta, \varsigma) + \varepsilon_1^{-1}\text{Grad}_\eta\Phi(x, \eta, \varsigma) + \varepsilon_2^{-1}\text{Grad}_\varsigma\Phi(x, \eta, \varsigma), \quad (6)$$

where the chain rule has been used, and the sub-indices of the gradient operators on the right-hand-side indicate that the derivative is performed with respect to x , η , and ς . In addition, the following average operators over the periodic cells \mathcal{Y} and \mathcal{Z} are introduced,

$$\langle \Phi^\varepsilon(x) \rangle_\eta = \frac{1}{|\mathcal{Y}|} \int_{\mathcal{Y}} \Phi(x, \eta, \varsigma) d\eta, \quad (7a)$$

$$\langle \Phi^\varepsilon(x) \rangle_\zeta = \frac{1}{|\mathcal{Z}|} \int_{\mathcal{Z}} \Phi(x, \eta, \varsigma) d\varsigma, \quad (7b)$$

119 where $|\mathcal{Y}|$ and $|\mathcal{Z}|$ denote the volume fractions of the periodic cells \mathcal{Y} and \mathcal{Z} , respectively.

120 At this stage, we perform a three-scale asymptotic expansion for the displacement \mathbf{u}^ε in powers of the
121 scaling parameters ε_1 and ε_2 . Specifically, we impose that

$$\mathbf{u}^\varepsilon(x) = \tilde{\mathbf{u}}^{(0)}(x, \eta, \varsigma) + \sum_{i=1}^{+\infty} \tilde{\mathbf{u}}^{(i)}(x, \eta, \varsigma) \varepsilon_2^i, \quad (8)$$

122 where

$$\tilde{\mathbf{u}}^{(0)}(x, \eta, \varsigma) = \mathbf{u}^{(0)}(x, \eta, \varsigma) + \sum_{j=1}^{+\infty} \mathbf{u}^{(j)}(x, \eta, \varsigma) \varepsilon_1^j. \quad (9)$$

123 Now, we embrace the homogenization process illustrated in^{29,30}. That is, we first substitute the expansion
124 (8) into the original problem constituted by equations (4) and (5a)-(5c), and then, we equate the resulting
125 expressions in powers of ε_2 , and subsequently, using (9), in powers of ε_1 .

126 Following this procedure, it can be shown that the term $\mathbf{u}^{(0)}$ is a function of the ‘‘slow’’ variable only,
127 i.e., $\mathbf{u}^{(0)}(x, \eta, \varsigma) \equiv \mathbf{u}^{(0)}(x)$, and solution of the *homogenized problem*

$$(\mathcal{P}) \begin{cases} \text{Div}_x[\hat{\mathcal{C}} : \mathbf{E}_x(\mathbf{u}^{(0)})] = \mathbf{0}, & \text{in } \Omega_h, \\ \mathbf{u}^{(0)} = \mathbf{u}^*, & \text{on } \partial\Omega_D^h, \\ [\hat{\mathcal{C}} : \mathbf{E}_x(\mathbf{u}^{(0)})] \cdot \mathbf{N} = \mathbf{S}^*, & \text{on } \partial\Omega_N^h, \end{cases} \quad (10)$$

128 where Ω_h represents the homogeneous macro-scale domain in which the homogenized equations are
129 defined. In (10), $\hat{\mathcal{C}}$ represents the *effective fourth-order elasticity tensor* of the hierarchical composite
130 material, which is given by the formula

$$\hat{\mathcal{C}} = \langle \mathcal{C}^{\varepsilon_1} + \mathcal{C}^{\varepsilon_1} : \mathbf{T}\mathbf{E}_\eta(\boldsymbol{\omega}) \rangle_\eta, \quad (11)$$

131 where the fourth-order tensor $\mathcal{C}^{\varepsilon_1}$ is given by

$$\mathcal{C}^{\varepsilon_1}(x) = \begin{cases} \mathcal{C}^{\text{m},\eta}(x, \eta), & \eta \in \Omega_{\text{m}}^{\varepsilon_1}, \\ \mathcal{C}^{\text{f},\eta}(x, \eta), & \eta \in \Omega_{\text{f}}^{\varepsilon_1}. \end{cases} \quad (12)$$

132 In (12), $\mathcal{C}^{\text{m},\eta}$ and $\mathcal{C}^{\text{f},\eta}$ represent the elasticity tensors corresponding to the constituents $\Omega_{\text{m}}^{\varepsilon_1}$ and $\Omega_{\text{f}}^{\varepsilon_1}$,
133 respectively. Furthermore, $\boldsymbol{\omega}$ is a third-order, η -periodic tensor field such that

$$\mathbf{u}^{(1)}(x, \eta, \varsigma) \equiv \mathbf{u}^{(1)}(x, \eta) = \boldsymbol{\omega}(x, \eta) : \mathbf{E}_x[\mathbf{u}^{(0)}(x)], \quad (13)$$

134 with $\mathbf{E}_x(\mathbf{u}^{(0)}(x)) := \text{Sym}[\text{Grad}_x \mathbf{u}^{(0)}(x)]$. Moreover, $\mathbf{T}\mathbf{E}_\beta(\boldsymbol{\omega}) = \frac{1}{2}[\text{TGrad}_\beta \boldsymbol{\omega} + {}^t(\text{TGrad}_\beta \boldsymbol{\omega})]$, with
135 $\beta = x, \eta, \varsigma$ (see³²). The operation ${}^t(\mathcal{A})$ transposes the fourth-order tensor \mathcal{A} by exchanging the order of

its first pair of indices only, and $\text{TGrad}_\beta \boldsymbol{\omega}$ is the fourth-order tensor defined as

$$\text{TGrad}_\beta \boldsymbol{\omega} = \frac{\partial \omega_{ikl}}{\partial \beta_j} \mathbf{e}_i \otimes \mathbf{e}_j \otimes \mathbf{e}_k \otimes \mathbf{e}_l. \quad (14)$$

Note that we are not using the covariant formalism in this work, otherwise the partial differentiation on the right-hand-side of (14) should be substituted with a covariant derivative.

Particularly, the third-order tensor field $\boldsymbol{\omega}$ is determined by solving the following auxiliary cell problem

$$(\mathcal{P}_Y) \begin{cases} \text{Div}_\eta[\mathcal{C}^{\varepsilon_1} + \mathcal{C}^{\varepsilon_1} : \text{T}\mathbf{E}_\eta(\boldsymbol{\omega})] = \mathbf{0}, & \text{in } \mathcal{Y} \setminus \Gamma_Y, \\ [(\mathcal{C}^{\varepsilon_1} + \mathcal{C}^{\varepsilon_1} : \text{T}\mathbf{E}_\eta(\boldsymbol{\omega})) \cdot \mathbf{N}_Y] = \mathbf{0}, & \text{on } \Gamma_Y, \\ [\boldsymbol{\omega}] = \mathbf{0}, & \text{on } \Gamma_Y, \end{cases} \quad (15)$$

where the condition $\langle \boldsymbol{\omega} \rangle_\eta = \mathbf{0}$ is imposed to guarantee uniqueness in the local problem (15). We remark that the condition of zero average of the third-order tensor $\boldsymbol{\omega}$ is just one particular way, without losing generality, to close the problem (15).

At this point we note that in this formulation (see^{29,30} for more details), the homogenization process accomplishes to relate the length scales in a cascade mode from the lower to the higher one, so that, the fourth-order elasticity tensor $\mathcal{C}^{\text{f},\eta}$ in (12), corresponding to the constituent $\Omega_{\text{f}}^{\varepsilon_1}$, is in fact, an effective one, and is given through the formula

$$\mathcal{C}^{\text{f},\eta} \equiv \tilde{\mathcal{C}} = \langle \mathcal{C}^{\varepsilon_2} + \mathcal{C}^{\varepsilon_2} : \text{T}\mathbf{E}_\varsigma(\tilde{\boldsymbol{\omega}}) \rangle_\varsigma. \quad (16)$$

We denote with $\tilde{\mathcal{C}}$ the *effective fourth-order elasticity tensor at the ε_1 -hierarchical level* of the composite material. In particular, for $\eta \in \Omega_{\text{f}}^{\varepsilon_1}$,

$$\mathcal{C}^{\varepsilon_2}(x) = \begin{cases} \mathcal{C}^{\text{m},\varsigma}(x, \eta, \varsigma), & \varsigma \in \Omega_{\text{m}}^{\varepsilon_2}, \\ \mathcal{C}^{\text{f},\varsigma}(x, \eta, \varsigma), & \varsigma \in \Omega_{\text{f}}^{\varepsilon_2}, \end{cases} \quad (17)$$

where $\mathcal{C}^{\text{m},\varsigma}$ and $\mathcal{C}^{\text{f},\varsigma}$ denote the elasticity tensors corresponding to the constituents $\Omega_{\text{m}}^{\varepsilon_2}$ and $\Omega_{\text{f}}^{\varepsilon_2}$, respectively. In (16), $\tilde{\boldsymbol{\omega}}$ is a third-order, ς - and η -periodic tensor field such that

$$\begin{aligned} \tilde{\mathbf{u}}^{(1)}(x, \eta, \varsigma) &= \tilde{\boldsymbol{\omega}}(x, \eta, \varsigma) : (\mathcal{I} + \text{T}\mathbf{E}_\eta[\boldsymbol{\omega}(x, \eta)]) : \mathbf{E}_x[\mathbf{u}^{(0)}(x)] \\ &\quad + \tilde{\boldsymbol{\omega}}(x, \eta, \varsigma) : \text{T}\mathbf{E}_x[\boldsymbol{\omega}(x, \eta)] : \mathbf{E}_x[\mathbf{u}^{(0)}(x)]_{\varepsilon_1}, \end{aligned} \quad (18)$$

where \mathcal{I} is the fourth-order identity tensor, i.e., for every symmetric tensor \mathbf{A} , it holds that $\mathcal{I} : \mathbf{A} = \mathbf{A}$. Furthermore, the tensor $\tilde{\boldsymbol{\omega}}$ is solution of the cell problem

$$(\mathcal{P}_Z) \begin{cases} \text{Div}_\varsigma[\mathcal{C}^{\varepsilon_2} + \mathcal{C}^{\varepsilon_2} : \text{T}\mathbf{E}_\varsigma(\tilde{\boldsymbol{\omega}})] = \mathbf{0}, & \text{in } Z \setminus \Gamma_Z, \\ [(\mathcal{C}^{\varepsilon_2} + \mathcal{C}^{\varepsilon_2} : \text{T}\mathbf{E}_\varsigma(\tilde{\boldsymbol{\omega}})) \cdot \mathbf{N}_Z] = \mathbf{0}, & \text{on } \Gamma_Z, \\ [\tilde{\boldsymbol{\omega}}] = \mathbf{0}, & \text{on } \Gamma_Z, \end{cases} \quad (19)$$

where the condition $\langle \tilde{\boldsymbol{\omega}} \rangle_\varsigma = \mathbf{0}$ is imposed to guarantee uniqueness in the local problem (19).

154 Effective properties of hierarchical fiber-reinforced composites

155 In this section, we particularize the results given in the previous section by focusing on a three-scale
 156 composite material with a square-symmetric arrangement of uniaxially aligned cylindrical fibers (see Fig.
 2). For this particular case, the three-dimensional cell problems (15) and (19) can be re-formulated as two-

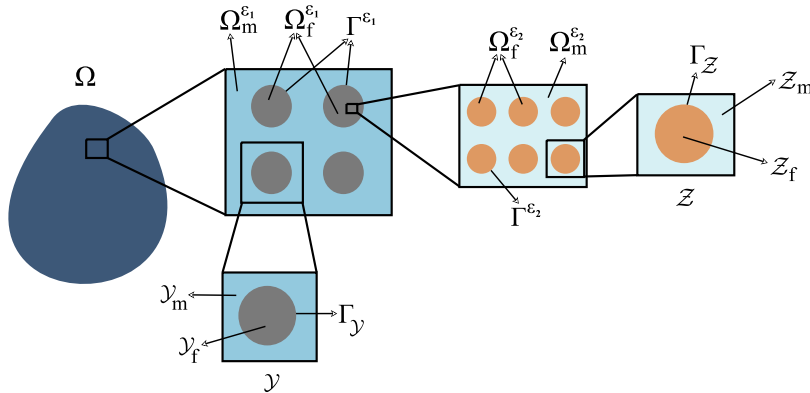


Figure 2. Schematic of the cross-section of a hierarchical fiber-reinforced periodic composite with three structural levels.

157 dimensional local problems defined over the cells' cross-sections corresponding to a square embedding
 158 a single circle.
 159

160 Specifically, we assume that at the ε_2 -hierarchical level, both $\mathcal{C}^{m,\varsigma}$ and $\mathcal{C}^{f,\varsigma}$ are piece-wise constant.
 161 This consideration indicates that the dependence of the cell problem \mathcal{P}_Z on η and x is lost, and
 162 consequently, that the auxiliary third-order tensor $\tilde{\omega}$ depends only on ς . Therefore, the effective elasticity
 163 tensor at the ε_1 -hierarchical level, $\tilde{\mathcal{C}}$, is likewise piece-wise constant. Additionally, considering that $\mathcal{C}^{m,\eta}$
 164 is piece-wise constant, it can be deduced, in a similar way, that ω will only depend on η and that the
 165 effective elasticity tensor, $\hat{\mathcal{C}}$, will be piece-wise constant.

166 In like manner, we suppose that all the constituents in Ω are isotropic. This assumption together
 167 with the specified geometrical microstructure at the ε_2 -hierarchical level implies that \mathcal{C} is tetragonal
 168 symmetric. This means that the effective elasticity tensor $\tilde{\mathcal{C}}$ has six independent elastic coefficients.
 169 Moreover, the assumption of isotropy of the constituent $\Omega_m^{\varepsilon_1}$ induces that the effective coefficient $\hat{\mathcal{C}}$ is
 170 at most monoclinic. Therefore, the cell problems \mathcal{P}_Z and \mathcal{P}_Y uncouple in sets of equations for the
 171 in-plane and out-of-plane stresses. That is, the local problems (15) and (19) rewrite, each one, as four

172 in-plane problems \mathcal{P}_α^{qq} ($q = 1, 2, 3$) and \mathcal{P}_α^{12} , with $\alpha = \eta, \varsigma$

$$(\mathcal{P}_\alpha^{qq}) \begin{cases} \frac{\partial \sigma_{11}^{qq\gamma, \alpha}}{\partial \alpha_1} + \frac{\partial \sigma_{12}^{qq\gamma, \alpha}}{\partial \alpha_2} = 0, & \text{in } \tilde{K}_\alpha^\gamma, \\ \frac{\partial \sigma_{21}^{qq\gamma, \alpha}}{\partial \alpha_1} + \frac{\partial \sigma_{22}^{qq\gamma, \alpha}}{\partial \alpha_2} = 0, & \text{in } \tilde{K}_\alpha^\gamma, \\ [\omega_{1qq}^\alpha] = 0, \quad [\omega_{2qq}^\alpha] = 0, & \text{on } \tilde{\Gamma}_\alpha, \\ [\sigma_{11}^{qq, \alpha} N_1^\alpha + \sigma_{12}^{qq, \alpha} N_2^\alpha] = -[\mathcal{C}_{11qq}^\alpha N_1^\alpha], & \text{on } \tilde{\Gamma}_\alpha, \\ [\sigma_{21}^{qq, \alpha} N_1^\alpha + \sigma_{22}^{qq, \alpha} N_2^\alpha] = -[\mathcal{C}_{22qq}^\alpha N_2^\alpha], & \text{on } \tilde{\Gamma}_\alpha, \end{cases} \quad (20a)$$

$$(\mathcal{P}_\alpha^{12}) \begin{cases} \frac{\partial \sigma_{11}^{12\gamma, \alpha}}{\partial \alpha_1} + \frac{\partial \sigma_{12}^{12\gamma, \alpha}}{\partial \alpha_2} = 0, & \text{in } \tilde{K}_\alpha^\gamma, \\ \frac{\partial \sigma_{21}^{12\gamma, \alpha}}{\partial \alpha_1} + \frac{\partial \sigma_{22}^{12\gamma, \alpha}}{\partial \alpha_2} = 0, & \text{in } \tilde{K}_\alpha^\gamma, \\ [\omega_{1qq}^\alpha] = 0, \quad [\omega_{2qq}^\alpha] = 0, & \text{on } \tilde{\Gamma}_\alpha, \\ [\sigma_{11}^{12\alpha} N_1^\alpha + \sigma_{12}^{12\alpha} N_2^\alpha] = -[\mathcal{C}_{1212}^\alpha N_2^\alpha], & \text{on } \tilde{\Gamma}_\alpha, \\ [\sigma_{21}^{12\alpha} N_1^\alpha + \sigma_{22}^{12\alpha} N_2^\alpha] = -[\mathcal{C}_{1212}^\alpha N_1^\alpha], & \text{on } \tilde{\Gamma}_\alpha, \end{cases} \quad (20b)$$

173 and two anti-plane problems \mathcal{P}_α^{3q} ($q = 1, 2$)

$$(\mathcal{P}_\alpha^{3q}) \begin{cases} \frac{\partial \sigma_{31}^{3q\gamma, \alpha}}{\partial \alpha_1} + \frac{\partial \sigma_{32}^{3q\gamma, \alpha}}{\partial \alpha_2} = 0, & \text{in } \tilde{K}_\alpha^\gamma, \\ [\omega_{33q}^\alpha] = 0, & \text{on } \tilde{\Gamma}_\alpha, \\ [\sigma_{31}^{3q, \alpha} N_1^\alpha + \sigma_{32}^{3q, \alpha} N_2^\alpha] = -[\mathcal{C}_{3131}^\alpha N_q^\alpha], & \text{on } \tilde{\Gamma}_\alpha, \end{cases} \quad (21)$$

174 where $\gamma = m, f$, and $\tilde{K}_\zeta^\gamma := \tilde{Z}_\gamma$ and $\tilde{K}_\eta^\gamma := \tilde{Y}_\gamma$ denote, respectively, the two-dimensional cross-sections
175 of \mathcal{Z}_γ and \mathcal{Y}_γ . The interface between the constituents \tilde{Z}_m and \tilde{Z}_f (\tilde{Y}_m and \tilde{Y}_f) is denoted by $\tilde{\Gamma}_Z$ ($\tilde{\Gamma}_Y$).

176 Additionally, in (20a)–(21)

$$\omega_{kpq}^\alpha := \begin{cases} \tilde{\omega}_{kpq}, & \text{for } \alpha = \varsigma, \\ \omega_{kpq}, & \text{for } \alpha = \eta, \end{cases} \quad (22)$$

177 and

$$\sigma_{ij}^{pq\gamma, \alpha} := \begin{cases} \mathcal{C}_{ijkl}^{\gamma, \varsigma} \frac{\partial \tilde{\omega}_{kpq}}{\partial \varsigma_l}, & \text{for } \alpha = \varsigma, \\ \mathcal{C}_{ijkl}^{\gamma, \eta} \frac{\partial \omega_{kpq}}{\partial \eta_l}, & \text{for } \alpha = \eta. \end{cases} \quad (23)$$

178 In (23), $\mathcal{C}_{ijkl}^{\gamma, \varsigma}$ and $\mathcal{C}_{ijkl}^{\gamma, \eta}$ are the components of the elasticity tensor of the constituent $\gamma = m, f$ at the ε_2 -
179 and ε_1 -hierarchical levels, respectively.

180 Furthermore, component-wise, the fourth-order effective elasticity tensor at the ε_1 -hierarchical level
 181 $\hat{\mathcal{C}}$, and the fourth-order effective elasticity tensor of the hierarchical composite material $\check{\mathcal{C}}$, are

$$\check{\mathcal{C}}_{ijpq} = \langle \mathcal{C}_{ijpq}^{\varepsilon_2} + \mathcal{C}_{ijkl}^{\varepsilon_2} \frac{\partial \tilde{\omega}_{kpq}}{\partial \zeta_l} \rangle_{\zeta}, \quad (24a)$$

$$\hat{\mathcal{C}}_{ijpq} = \langle \mathcal{C}_{ijpq}^{\varepsilon_1} + \mathcal{C}_{ijkl}^{\varepsilon_1} \frac{\partial \omega_{kpq}}{\partial \eta_l} \rangle_{\eta}, \quad (24b)$$

182 respectively.

183 The theory of analytical functions in³³ applied to the cell problems (20a)-(21) allow us to find the
 184 effective coefficients $\check{\mathcal{C}}_{ijpq}$ and $\hat{\mathcal{C}}_{ijpq}$ given in (24a) and (24b), respectively. In the present study we
 185 follow the procedure adopted in³⁴⁻³⁷ and we adapt it to the obtained scale-coupled cell problems (see
 186 Appendix). We note that in the previous work²⁹ we dealt with the solution of the coupled-anti-plane cell
 187 problems, and therefore only the procedure for the coupled-in-plane cell problems is shown. In particular,
 188 the choice of the microstructure and material symmetry, and the generality of the analytical approach
 189 permit us to focus on the solution of the cell problems in only one hierarchical level. We note that due
 190 to the algebraic complexity of the analytical formulae for the effective coefficients given by relations
 191 (53a)–(53d) and (55), we use Matlab in order to solve the infinite linear systems (49) and (51), truncated
 192 to a fixed order, and, subsequently, to evaluate the results in the corresponding formulae for the effective
 193 coefficients.

194 Modeling MMTs' effective properties

195 In the present section we show the potential of the three-scale asymptotic homogenization approach
 196 to compute the effective properties of MMTs. Bones and tendons are examples of MMTs, which
 197 are hierarchically structured materials, and whose principal constituents, organized spanning several
 198 length scales, are mineral crystals, collagen, and water. The principal elements of MMTs are cylindrical
 199 mineralized collagen fibrils consisting in self-assembled collagen molecules that are aligned in staggered
 200 arrays³¹. The hydroxyapatite crystals are distributed in both the intrafibrillar space, reinforcing the
 201 collagen fibrils, and in the extrafibrillar space, which primarily consists of mineral and water (see^{31,38}
 202 and references therein).

203 Geometrical model for MMTs

204 In the present work, we consider an approximated model for MMTs. Specifically, at the ε_2 -hierarchical
 205 level we suppose that \mathcal{Z}_m represents the minerals surrounding a single collagen fiber denoted by \mathcal{Z}_f .
 206 The collection of all collagen fibers at the ε_2 -hierarchical level $\Omega_f^{\varepsilon_2}$, together with the host phase $\Omega_m^{\varepsilon_2}$
 207 (representing the minerals) will constitute the mineralized collagen fiber \mathcal{Y}_f at the ε_1 -hierarchical level.
 208 The finite collection of mineralized collagen fibers $\Omega_f^{\varepsilon_1}$ are supposed to be periodically distributed in the
 209 extrafibrillar space $\Omega_m^{\varepsilon_1}$. The union of the disjoint sets $\Omega_f^{\varepsilon_1}$ with $\Omega_m^{\varepsilon_1}$ will form each one of the mineralized
 210 collagen fibril bundles. Finally, the extrafibrillar space is supposed to be a mixture of water and minerals
 211 (see Fig. 3). The situation just described, where mineralized collagen fibers are unidirectionally aligned,
 212 can be, for example, the case of a mineralized turkey leg tendon, and it can be considered as a simplified
 213 model for bones³¹.

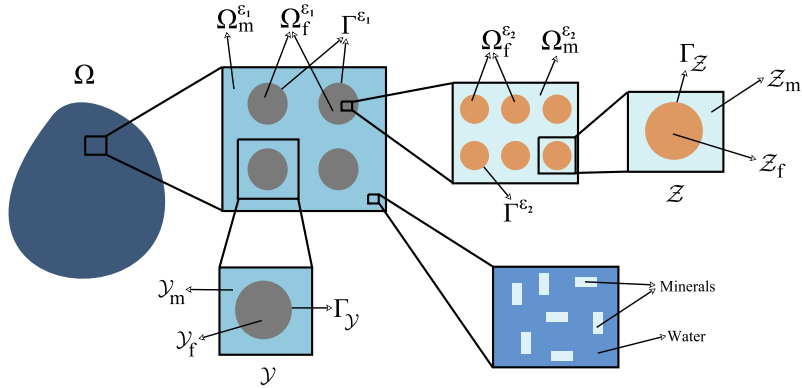


Figure 3. Schematic of the cross-section of MMTs.

214 In order to find the effective properties of the extrafibrillar space we take advantage of Reuss' lower
 215 bound formula³⁹ to compute the effective properties of the mixture $\Omega_m^{\varepsilon_1}$ as follows

$$\mathcal{C}^{m,\eta} = \langle (\mathcal{C}_{ES})^{-1} \rangle^{-1}, \quad (25)$$

216 where

$$\mathcal{C}_{ES}(x) = \begin{cases} \mathcal{C}^{w,\varsigma}(x, \eta, \varsigma), & \text{if } \varsigma \text{ is in the water phase,} \\ \mathcal{C}^{m,\varsigma}(x, \eta, \varsigma), & \text{if } \varsigma \text{ is in the mineral phase.} \end{cases} \quad (26)$$

217 In (26), $\mathcal{C}^{w,\varsigma}$ and $\mathcal{C}^{m,\varsigma}$ are the elasticity tensors related to the water and mineral phases,
 218 respectively. In particular, and following³¹, we replace the material properties of water by those of
 219 polymethylmethacrylate (PMMA).

220 We remark that the present three-scale asymptotic approach can be improved to compute the effective
 221 properties of the composite extrafibrillar space. However, a realistic geometrical description of the
 222 structure of the extrafibrillar space requires numerical simulations in three dimensions for elastic
 223 composites (see e.g.^{26,40,41}) which are beyond the scope of this work. Here we estimate the effective
 224 elastic constants of the extrafibrillar space by means of the Reuss bounds, thus obtaining a fully semi-
 225 analytic computational framework at each hierarchical level of organization. Reuss's formula (25) permits
 226 to obtain a lower bound for the current model. When we say that we obtain a lower bound for the model,
 227 it means that indeed, by considering the asymptotic homogenization approach instead, effective values
 228 above those computed using Reuss' scheme are expected⁴¹.

229 *Effective properties of MMTs*

230 To model the effective properties of MMTs, we conveniently take advantage of some of the modeling
 231 assumptions in^{31,26}. Specifically, we consider all constituents of the hierarchical composite material are
 232 isotropic and that correspond to those of a bone tissue³¹. That is, Young's modulus (E) and Poisson's
 233 ratio (ν) of the mineral crystals, collagen fibers and water constituents (individuated by the subscripts m,
 234 c and p, respectively) are given as reported in Table 2.

Table 2. Young's modulus and Poisson's ratio of the mineral crystals, collagen fibers and water constituents.

Parameter	Unit	Value
E_M	[GPa]	110
E_c	[GPa]	5.00
E_p	[GPa]	4.96
ν_M	[-]	0.28
ν_c	[-]	0.30
ν_p	[-]	0.37

Moreover, we perform a parametric analysis of the MMTs' effective properties by increasing the volume fraction of the mineral crystals, denoted by V , in the mineralized collagen fibril bundle from 0.2 to 0.5³¹. Following³¹, we also take into account the mineral distribution parameter ϕ , defined as the ratio of the mineral volume in the mineralized collagen fibril to the total mineral volume in the mineralized collagen fibril bundle. In⁴², the mineral distribution parameter was estimated to be less than or equal to 0.7, here we chose $\phi = 0.5$. Specifically, the parameter ϕ is related to the phase volume fractions using the following empirical formula^{31,43}

$$V^{f,\eta} = \phi V + h(V), \quad (27)$$

where $h(V) := \frac{\varpi}{1+\varpi}(1-V)$ and $\varpi := 0.36 + 0.084 e^{6.7V}$. In (27), the symbol $V^{f,\eta}$ represents the volume fraction of the mineralized collagen fibrils in the mineralized collagen fibril bundle. Therefore, the volume fraction of the extrafibrillar space in the mineralized collagen fibril bundle is given by $V^{m,\eta} = 1 - V^{f,\eta}$. Additionally, the volume fractions of the mineral crystals ($V^{m,\zeta}$) and of collagen ($V^{f,\zeta}$) in the mineralized collagen fibril are given by³¹

$$V^{m,\zeta} = \phi \frac{V}{V^{f,\eta}} \quad \text{and} \quad V^{f,\zeta} = 1 - V^{m,\zeta}. \quad (28)$$

Finally, the volume fractions of the mineral crystals and water phases in the extrafibrillar space are

$$V^{f,ES} = (1 - \phi) \frac{V}{1 - V^{f,\eta}} \quad \text{and} \quad V^{m,ES} = 1 - V^{f,ES}, \quad (29)$$

respectively.

Figure 4 shows the effective coefficients $[\hat{\mathcal{C}}]_{11}$ (left panel) and $[\hat{\mathcal{C}}]_{33}$ (right panel), obtained by applying the three-scale homogenization approach, plotted with respect to the degree of mineralization of the tissue. In Fig. 4, we also show a comparison with the theoretical results obtained in³¹. Qualitatively, the results are in agreement with the ones obtained by³¹, that is, the effective axial and transverse stiffness coefficients increase with respect to the minerals volume fraction. It is known that the results obtained by the asymptotic homogenization method are closer to those obtained by Reuss formula. Therefore, even in this case, we are positive that using an asymptotic approach for the characterization of the composite extrafibrillar space, the effective elastic coefficients will remain close to those in³¹.

It is also known that the asymptotic homogenization technique gives effective properties lying between those computed using Reuss and Voigt formulae (see e.g.⁴¹), which is the case shown in Fig. 4 (right panel), i.e. the results are below those obtained by³¹ for $\hat{\mathcal{C}}_{33}$. However, for $\hat{\mathcal{C}}_{11}$, the results lie above

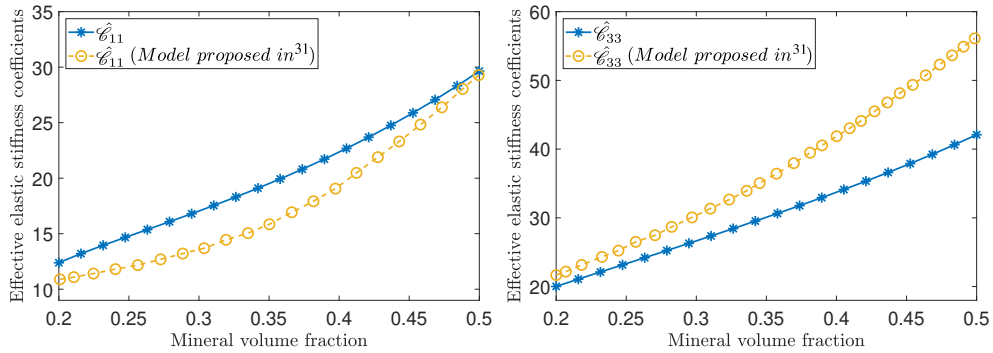


Figure 4. Elastic stiffness coefficients $\hat{\mathcal{C}}_{11}$ (left) and $\hat{\mathcal{C}}_{33}$ (right) with respect to the mineral volume fraction V . A comparison with the theoretical results in³¹ are also shown.

260 those in³¹. Even though we were not quite expecting this, the curve found with the present approach
 261 remains closer to that predicted by³¹. Furthermore, we obtain a **satisfactory agreement** with experimental
 262 data, and actually the obtained bounds are tighter than those in³¹, as shown by Fig 5. In Fig. 5, we
 263 compare the effective axial and transverse stiffness coefficients with the experimental data showed in³¹
 264 corresponding to mineralized turkey leg tendon, human femur and mice bone. As commented before,
 265 the results fit very well the experimental data. We note that a Voigt formulation for computing the
 266 extrafibrillar space's effective properties is also plausible. Indeed, we also considered Voigt upper bounds
 267 to model the properties of the extrafibrillar space. However, we preferred not to show them since the
 268 results did not match well the experimental and theoretical data.

269 The results shown in Fig. 5 could be of special interest for clinical applications including, for instance,
 270 tissue reconstruction. Indeed, following the methodology presented in this work, and considering other
 271 internal structures and properties, we could assess, in principle, how well fabricated a composite is by
 272 matching our analytical/computational results with the real properties of a target tissue (see e.g.⁴⁴). Since
 273 the present homogenization approach takes into consideration three spatial scales, with respect to two-
 274 scale methods, it provides a better “microscope” to resolve the internal structure of a composite and to
 275 capture its material properties.

276 For completeness in the analysis we show in Fig. 6 the shear effective elastic coefficients $\hat{\mathcal{C}}_{44}$, $\hat{\mathcal{C}}_{55}$
 277 and $\hat{\mathcal{C}}_{66}$ with respect to the mineral volume fraction. As shown in Fig. 6, the shear coefficients $\hat{\mathcal{C}}_{44}$,
 278 $\hat{\mathcal{C}}_{55}$ and $\hat{\mathcal{C}}_{66}$ increase with increasing tissue's mineralization. Furthermore, the coefficients $\hat{\mathcal{C}}_{44}$ and $\hat{\mathcal{C}}_{55}$
 279 coincide. We remark that the homogenized elasticity tensor has tetragonal symmetry (6 independent
 280 elastic coefficients), i.e. the matrix representation of $\hat{\mathcal{C}}$ (in Voigt notation) is

$$[\hat{\mathcal{C}}] = \begin{pmatrix} \hat{\mathcal{C}}_{11} & \hat{\mathcal{C}}_{12} & \hat{\mathcal{C}}_{13} & 0 & 0 & 0 \\ \hat{\mathcal{C}}_{12} & \hat{\mathcal{C}}_{11} & \hat{\mathcal{C}}_{13} & 0 & 0 & 0 \\ \hat{\mathcal{C}}_{13} & \hat{\mathcal{C}}_{13} & \hat{\mathcal{C}}_{33} & 0 & 0 & 0 \\ 0 & 0 & 0 & \hat{\mathcal{C}}_{44} & 0 & 0 \\ 0 & 0 & 0 & 0 & \hat{\mathcal{C}}_{44} & 0 \\ 0 & 0 & 0 & 0 & 0 & \hat{\mathcal{C}}_{66} \end{pmatrix}. \quad (30)$$

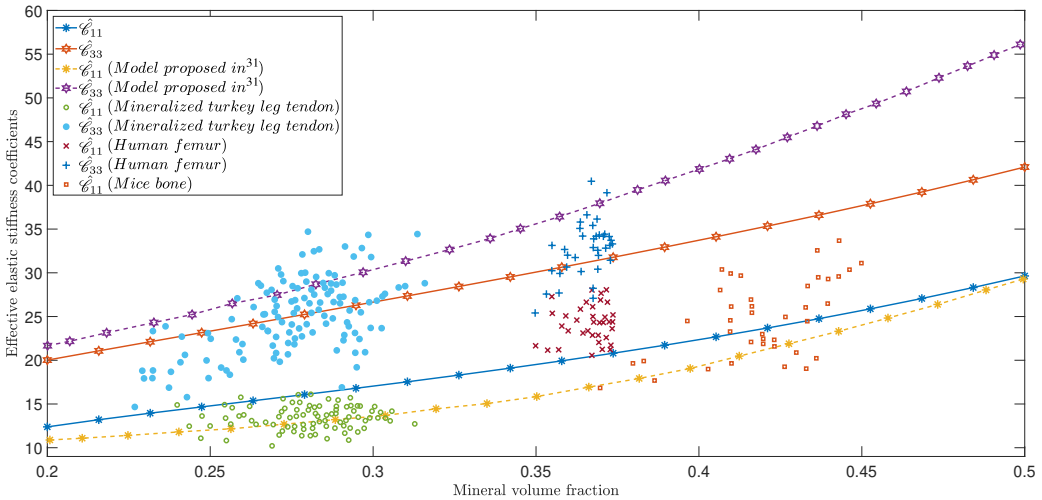


Figure 5. Comparison of the predicted and measured elastic stiffness coefficients \hat{C}_{11} (transverse) and \hat{C}_{33} (axial) with the experimental and theoretical data reported in³¹ (and references therein) corresponding to mineralized turkey tendon leg, human femur and mice bone.

281

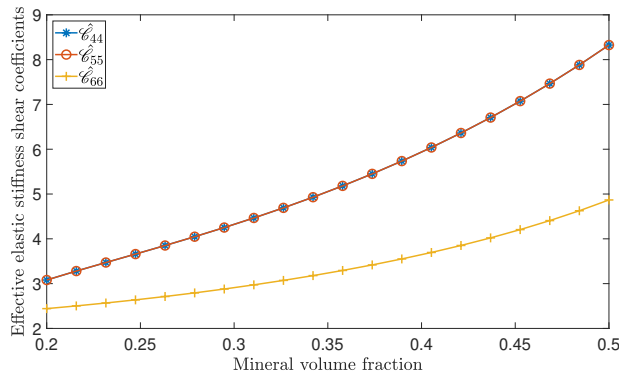


Figure 6. Shear effective elastic stiffness coefficients plotted with respect to the mineral volume fraction.

282 We now turn the attention to the computation of the effective Young’s modulus (\hat{E}), shear modulus
 283 ($\hat{\mu}$) and Poisson’s ratio ($\hat{\nu}$) of the hierarchical composite tissue. In particular, the effective shear modulus
 284 for hierarchical fiber-reinforced composites has been recently studied in the previous work²⁹. Here, we
 285 adapt the computational scheme developed therein to the present framework. In the present study, via
 286 the homogenization process, the resulting homogenized mineralized tissue shows characteristics of a

287 tetragonal material. Therefore, using Voigt notation, we have that

$$\hat{E}_1 = \frac{\Delta}{(\hat{\mathcal{C}}_{23})^2 - \hat{\mathcal{C}}_{22}\hat{\mathcal{C}}_{33}}, \quad \hat{\nu}_{12} = \hat{\nu}_{21} = \frac{\hat{\mathcal{C}}_{13}\hat{\mathcal{C}}_{23} - \hat{\mathcal{C}}_{12}\hat{\mathcal{C}}_{33}}{(\hat{\mathcal{C}}_{23})^2 - \hat{\mathcal{C}}_{22}\hat{\mathcal{C}}_{33}}, \quad (31a)$$

$$\hat{E}_2 = \frac{\Delta}{(\hat{\mathcal{C}}_{13})^2 - \hat{\mathcal{C}}_{11}\hat{\mathcal{C}}_{33}}, \quad \hat{\nu}_{13} = \hat{\nu}_{31} = \frac{\hat{\mathcal{C}}_{12}\hat{\mathcal{C}}_{23} - \hat{\mathcal{C}}_{13}\hat{\mathcal{C}}_{22}}{(\hat{\mathcal{C}}_{23})^2 - \hat{\mathcal{C}}_{22}\hat{\mathcal{C}}_{33}}, \quad (31b)$$

$$\hat{E}_3 = \frac{\Delta}{(\hat{\mathcal{C}}_{12})^2 - \hat{\mathcal{C}}_{11}\hat{\mathcal{C}}_{22}}, \quad \hat{\nu}_{23} = \hat{\nu}_{32} = \frac{\hat{\mathcal{C}}_{12}\hat{\mathcal{C}}_{13} - \hat{\mathcal{C}}_{11}\hat{\mathcal{C}}_{23}}{(\hat{\mathcal{C}}_{13})^2 - \hat{\mathcal{C}}_{11}\hat{\mathcal{C}}_{33}}, \quad (31c)$$

288 where

$$\Delta = (\hat{\mathcal{C}}_{13})^2\hat{\mathcal{C}}_{22} - 2\hat{\mathcal{C}}_{12}\hat{\mathcal{C}}_{13}\hat{\mathcal{C}}_{23} + \hat{\mathcal{C}}_{11}(\hat{\mathcal{C}}_{23})^2 + (\hat{\mathcal{C}}_{12})^2\hat{\mathcal{C}}_{33} - \hat{\mathcal{C}}_{11}\hat{\mathcal{C}}_{22}\hat{\mathcal{C}}_{33}. \quad (32)$$

289 Figure 7 shows the predicted effective Young's moduli (top left), shear moduli (top right) and Poisson's
 290 ratio (bottom). We remark that it has been difficult to find experimental data measuring the anisotropic
 291 properties of MMTs and validating the computations reported in Fig. 7. Additionally, as details regarding
 292 the mineral content in the tissue are often not available in experimental studies, we cannot establish
 293 a logical correspondence with the numerical results shown in Fig. 7, as we did previously in Fig. 5.
 294 However, in what follows, we make a qualitative comparison with the data available in the scientific
 295 literature. In this respect, bone has been an extensively discussed hierarchical tissue, and several
 296 experimental techniques, such as micromechanical tests or nanoindentation⁴⁵, have been used in the
 297 measurement of its mechanical properties. For instance, the experimental studies conducted in⁴⁶ for bone
 298 tissues show that the magnitude of Young's and shear moduli increase with the degree of mineralization.
 299 This trend is captured by our computations as shown in Fig. 7 (top left and top right panels). In addition,
 300 Young's moduli and Poisson's ratio of single trabeculae in three orthogonal material directions were
 301 measured in⁴⁷ using compression tests. Therein, it was reported Young's modulus values in the trabeculae
 302 longitudinal direction significantly higher than those on the transverse directions. This experimental
 303 findings are in agreement with the predicted results from the present theoretical approach as shown in Fig.
 304 7 (top left panel). Moreover, the data collected in the review paper⁴⁵ shows Young's modulus of trabecular
 305 bone varying between 0 Gpa and 25 Gpa (see Fig. 5 of⁴⁵), which is in the range of the results obtained
 306 for low mineral concentrations. Finally, we observe that $\hat{\nu}_{12}$ decreases, and that $\hat{\nu}_{13} = \hat{\nu}_{23}$ increases, with
 307 the augment of tissue's mineralization.

308 Conclusions

309 In the present work we have depicted a three-scale asymptotic homogenization procedure to investigate
 310 the effective properties of multiscale, linear elastic composite materials. Using this approach we compute
 311 the effective properties of a linear elastic, fiber reinforced hierarchical material using an analytical
 312 resolution process, allowing us to reduce the computational cost necessary to calculate the homogenized
 313 properties. Furthermore, the three-scale scheme was employed in a biological scenario of interest, that is,
 314 the modeling of the macroscopic behavior of MMTs. Specifically, we conducted a parametric study by
 315 varying the mineralization of the heterogeneous tissue, and we compared the effective axial and transverse
 316 elastic stiffness constants with theoretical and experimental values. In the study, we take advantage of

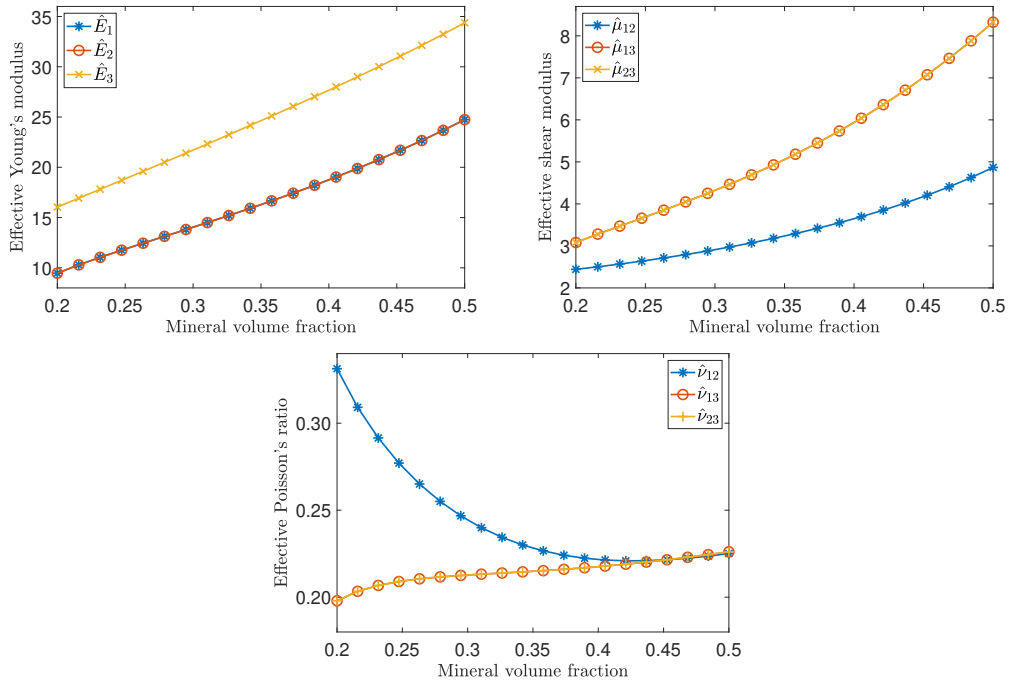


Figure 7. Comparison of the predicted effective Young's modulus, shear modulus and Poisson's ratio of the musculoskeletal mineralized tissue with respect to the mineral volume fraction. (Top) \hat{E}_1 , \hat{E}_2 and \hat{E}_3 , (middle) $\hat{\mu}_{12}$, $\hat{\mu}_{13}$ and $\hat{\mu}_{23}$, (bottom) $\hat{\nu}_{12}$, $\hat{\nu}_{13}$ and $\hat{\nu}_{23}$.

317 Reuss' lower formula to model the properties of the extrafibrillar space. In this sense, we hypothesize
 318 that performing an asymptotic homogenization approach to describe the extrafibrillar space will produce
 319 more accurate outcomes for the description of MMTs. Finally, we computed the effective Young's and
 320 shear moduli, and Poisson's ratio, and we showed that the predictions are consistent with experimental
 321 findings concerning bone tissues.

322 Minerals content can substantially affect the macroscopic tissue behavior^{15,26,48}. Given the complexity
 323 that represents to take into account the shape of the mineral crystals embedded in the water solution, one
 324 limitation of this work is related to the fact that we model the effective behavior of the extrafibrillar space
 325 using Reuss lower formula. In this direction, we aim to account for another scale in the homogenization
 326 process, and to solve the related local problem by means of the finite elements method²⁶. Further
 327 developments of this work include: (i) the generalization to a nonlinear framework (e.g. considering
 328 hyperelasticity)^{32,49,50} and (ii) the consideration of growth of the tissue and remodelling of its internal
 329 structure^{32,50-54}. Another issue that could arise in our formulation is that of a non-macroscopically
 330 uniform medium. In other words, a medium in which the periodic cells are not independent of the
 331 macroscale and thus, the geometry can be varying over the multiple scales, not only the elastic constants.
 332 In this particular case, the generalized Reynold's transport theorem (see e.g.⁵⁵) has to be enforced as

done, for instance in⁵⁶ and in⁵⁷ in the context of poro-mechanics. Alternative approaches that are rapidly emerging in the literature also involve a more explicit definition of the normal vector⁵⁸, which has been used to investigate the role of porosity gradients to optimize filter efficiency⁵⁹. Also, the macroscopic uniformity assumption may also not be suitable for modelling peculiar situations, such as, for example, localized deformations and damage phenomena that can violate the periodicity constraint. In this context, hierarchical computational schemes have been developed for overcoming this issue^{28,60,61}. In an idealized setting, one may think of reinterpreting the small parameter ε_2 as e.g. the damage length-scale and perform an analytical three-scale homogenization approach.

Finally, we remark that the technique has the advantage of reducing the intrinsic geometrical complexities when studying heterogeneous materials, and it ciphers the constituent's properties at the several scales in the effective coefficients,.

Acknowledgements

ART gratefully acknowledges the research project “Mathematical multi-scale modeling of biological tissues” (N. 64) financed by the Politecnico di Torino (Scientific Advisor: Alfio Grillo). ART and AG acknowledge the Dipartimento di Scienze Matematiche (DISMA) “G.L. Lagrange” of the Politecnico di Torino, “Dipartimento di Eccellenza 2018–2022” (“Department of Excellence 2018–2022”). RRR acknowledges the funding of Proyecto Nacional de Ciencias Básicas 2016–2018 (Project No. 7515) and to Departamento de Matemáticas y Mecánica, IIMAS and PREI-DGAPA at UNAM.

References

1. Bae WG, Kim HN, Kim D et al. 25th anniversary article: Scalable multiscale patterned structures inspired by nature: the role of hierarchy. *Advanced Materials* 2013; 26(5): 675–700. DOI:10.1002/adma.201303412.
2. Kim CS, Radow C and Sano T (eds.) *Hybrid and Hierarchical Composite Materials*. Springer International Publishing, 2015. DOI:10.1007/978-3-319-12868-9.
3. Yang W, Chen IH, Gludovatz B et al. Natural flexible dermal armor. *Advanced Materials* 2012; 25(1): 31–48. DOI:10.1002/adma.201202713.
4. Cowin SC (ed.) *Bone Mechanics Handbook*. Second edition ed. CRC Press, 2001. ISBN 0-8493-9117-2.
5. Hori M and Nemat-Nasser S. On two micromechanics theories for determining micro–macro relations in heterogeneous solids. *Mechanics of Materials* 1999; 31(10): 667–682. DOI:10.1016/s0167-6636(99)00020-4.
6. Hill R. Elastic properties of reinforced solids: Some theoretical principles. *Journal of the Mechanics and Physics of Solids* 1963; 11(5): 357–372. DOI:10.1016/0022-5096(63)90036-x.
7. Mura T. *Micromechanics of defects in solids*. Springer Netherlands, 1987. DOI:10.1007/978-94-009-3489-4.
8. Bakhvalov N and Panasenko G. *Homogenisation: Averaging Processes in Periodic Media*. Springer Netherlands, 1989. DOI:10.1007/978-94-009-2247-1.
9. Bensoussan A, Lions JL and Papanicolau G. *Asymptotic Analysis for Periodic Structures*. Elsevier Science, 1978.
10. Cioranescu D and Donato P. *An Introduction to Homogenization*. Oxford University Press, 1999. ISBN 0198565542.
11. Sanchez-Palencia E. *Non-Homogeneous Media and Vibration Theory*. Springer Berlin Heidelberg, 1980. DOI: 10.1007/3-540-10000-8.

- 372 12. Auriault JL, Boutin C and Geindreau C (eds.) *Homogenization of Coupled Phenomena in Heterogenous Media*.
373 ISTE, 2009. DOI:10.1002/9780470612033.
- 374 13. Milton GW. *The Theory of Composites*. Cambridge University Press, 2002. DOI:10.1017/cbo9780511613357.
- 375 14. Bader TK, Hofstetter K, Hellmich C et al. The poroelastic role of water in cell walls of the hierarchical composite
376 “softwood”. *Acta Mechanica* 2011; 217(1-2): 75–100. DOI:10.1007/s00707-010-0368-8.
- 377 15. Nikolov S and Raabe D. Hierarchical modeling of the elastic properties of bone at submicron scales: The role of
378 extrafibrillar mineralization. *Biophysical Journal* 2008; 94(11): 4220–4232. DOI:10.1529/biophysj.107.125567.
- 379 16. Hamed E, Lee Y and Jasiuk I. Multiscale modeling of elastic properties of cortical bone. *Acta Mechanica* 2010;
380 213(1-2): 131–154. DOI:10.1007/s00707-010-0326-5.
- 381 17. Mei CC and Auriault JL. Mechanics of heterogeneous porous media with several spatial scales. *Proceedings*
382 *of the Royal Society A: Mathematical, Physical and Engineering Sciences* 1989; 426(1871): 391–423. DOI:
383 10.1098/rspa.1989.0132.
- 384 18. Allaire G and Briane M. Multiscale convergence and reiterated homogenisation. *Proceedings of the Royal*
385 *Society of Edinburgh: Section A Mathematics* 1996; 126(02): 297–342. DOI:10.1017/s0308210500022757.
- 386 19. Crolet J, Aoubiza B and Meunier A. Compact bone: Numerical simulation of mechanical characteristics. *Journal*
387 *of Biomechanics* 1993; 26(6): 677–687. DOI:10.1016/0021-9290(93)90031-9.
- 388 20. Telega JJ, Galka A and Tokarzewski S. Application of the reiterated homogenization to determination of
389 effective noduli of a compact bone. *Journal of Theoretical and Applied Mechanics* 1999; 37: 687–706.
- 390 21. Lukkassen D and Milton GW. On hierarchical structures and reiterated homogenization. In Cwikel M, Englis
391 M, Kufner A et al. (eds.) *Function Spaces, Interpolation Theory and Related Topics*. De Gruyter, pp. 355–368.
- 392 22. Rohan E, Naili S, Cimmman R et al. Multiscale modeling of a fluid saturated medium with double porosity:
393 Relevance to the compact bone. *Journal of the Mechanics and Physics of Solids* 2012; 60(5): 857–881. DOI:
394 10.1016/j.jmps.2012.01.013.
- 395 23. Dimitrienko Y, Dimitrienko I and Sborschikov S. Multiscale hierarchical modeling of fiber reinforced
396 composites by asymptotic homogenization method. *Applied Mathematical Sciences* 2015; 9: 7211–7220. DOI:
397 10.12988/ams.2015.510641.
- 398 24. Tsalis D, Charalambakis N, Bonnay K et al. Effective properties of multiphase composites made of elastic
399 materials with hierarchical structure. *Mathematics and Mechanics of Solids* 2015; 22(4): 751–770. DOI:
400 10.1177/1081286515612142.
- 401 25. Nascimento ES, Cruz ME and Bravo-Castillero J. Calculation of the effective thermal conductivity of multiscale
402 ordered arrays based on reiterated homogenization theory and analytical formulae. *International Journal of*
403 *Engineering Science* 2017; 119: 205–216. DOI:10.1016/j.jjengsci.2017.06.023.
- 404 26. Penta R, Raum K, Grimal Q et al. Can a continuous mineral foam explain the stiffening of aged bone tissue?
405 a micromechanical approach to mineral fusion in musculoskeletal tissues. *Bioinspiration & Biomimetics* 2016;
406 11(3): 035004. DOI:10.1088/1748-3190/11/3/035004.
- 407 27. Trucu D, Chaplain M and Marciniak-Czochra A. Three-scale convergence for processes in heterogeneous media.
408 *Applicable Analysis* 2012; 91(7): 1351–1373. DOI:10.1080/00036811.2011.569498.
- 409 28. Zohdi TI, Oden J and Rodin GJ. Hierarchical modeling of heterogeneous bodies. *Computer Methods in Applied*
410 *Mechanics and Engineering* 1996; 138(1-4): 273–298. DOI:10.1016/s0045-7825(96)01106-1.
- 411 29. Ramírez-Torres A, Penta R, Rodríguez-Ramos R et al. Homogenized out-of-plane shear response of three-scale
412 fiber-reinforced composites. *Computing and Visualization in Science* 2018; DOI:10.1007/s00791-018-0301-6.
- 413 30. Ramírez-Torres A, Penta R, Rodríguez-Ramos R et al. Three scales asymptotic homogenization and its
414 application to layered hierarchical hard tissues. *International Journal of Solids and Structures* 2018; 130-131:

- 415 190–198. DOI:10.1016/j.ijisolstr.2017.09.035.
- 416 31. Tiburtius S, Schrof S, Molnár F et al. On the elastic properties of mineralized turkey leg tendon tissue:
417 multiscale model and experiment. *Biomechanics and Modeling in Mechanobiology* 2014; 13(5): 1003–1023.
418 DOI:10.1007/s10237-013-0550-8.
- 419 32. Ramírez-Torres A, Stefano SD, Grillo A et al. An asymptotic homogenization approach to the microstructural
420 evolution of heterogeneous media. *International Journal of Non-Linear Mechanics* 2018; DOI:10.1016/j.
421 ijnonlinmec.2018.06.012.
- 422 33. Muskhelishvili NI. *Some Basic Problems of the Mathematical Theory of Elasticity*. Springer Netherlands, 1977.
423 DOI:10.1007/978-94-017-3034-1.
- 424 34. Pobodrya BE. *Mechanics of composite materials*. Moscow State University Press, Moscow, in Russian, 1984.
- 425 35. Rodríguez-Ramos R, Sabina FJ, Guinovart-Díaz R et al. Closed-form expressions for the effective coefficients of
426 a fiber-reinforced composite with transversely isotropic constituents – i. elastic and square symmetry. *Mechanics
427 of Materials* 2001; 33(4): 223–235. DOI:10.1016/s0167-6636(00)00059-4.
- 428 36. Sabina FJ, Rodríguez-Ramos R, Bravo-Castillero J et al. Closed-form expressions for the effective coefficients of
429 a fibre-reinforced composite with transversely isotropic constituents. II: Piezoelectric and hexagonal symmetry.
430 *Journal of the Mechanics and Physics of Solids* 2001; 49(7): 1463–1479. DOI:10.1016/s0022-5096(01)00006-0.
- 431 37. Bravo-Castillero J, Guinovart-Díaz R, Sabina FJ et al. Closed-form expressions for the effective coefficients
432 of a fiber-reinforced composite with transversely isotropic constituents – II. piezoelectric and square symmetry.
433 *Mechanics of Materials* 2001; 33(4): 237–248. DOI:10.1016/s0167-6636(00)00060-0.
- 434 38. Weiner S and Wagner HD. THE MATERIAL BONE: Structure-mechanical function relations. *Annual Review
435 of Materials Science* 1998; 28(1): 271–298. DOI:10.1146/annurev.matsci.28.1.271.
- 436 39. Reuss A. Berechnung der Fließgrenze von Mischkristallen auf Grund der Plastizitätsbedingung für Einkristalle
437 . *ZAMM - Zeitschrift für Angewandte Mathematik und Mechanik* 1929; 9(1): 49–58. DOI:10.1002/zamm.
438 19290090104.
- 439 40. Penta R and Gerisch A. Investigation of the potential of asymptotic homogenization for elastic composites
440 via a three-dimensional computational study. *Computing and Visualization in Science* 2015; 17(4): 185–201.
441 DOI:10.1007/s00791-015-0257-8.
- 442 41. Penta R and Gerisch A. The asymptotic homogenization elasticity tensor properties for composites with
443 material discontinuities. *Continuum Mechanics and Thermodynamics* 2017; 29(1): 187–206. DOI:10.1007/
444 s00161-016-0526-x.
- 445 42. Alexander B, Daulton TL, Genin GM et al. The nanometre-scale physiology of bone: steric modelling and
446 scanning transmission electron microscopy of collagen-mineral structure. *Journal of The Royal Society Interface*
447 2012; 9(73): 1774–1786. DOI:10.1098/rsif.2011.0880.
- 448 43. Raum K, Cleveland RO, Peyrin F et al. Derivation of elastic stiffness from site-matched mineral density and
449 acoustic impedance maps. *Physics in Medicine and Biology* 2006; 51(3): 747–758. DOI:10.1088/0031-9155/
450 51/3/018.
- 451 44. Hollister SJ and Lin CY. Computational design of tissue engineering scaffolds. *Computer Methods in Applied
452 Mechanics and Engineering* 2007; 196(31-32): 2991–2998. DOI:10.1016/j.cma.2006.09.023.
- 453 45. Wu D, Isaksson P, Ferguson SJ et al. Young’s modulus of trabecular bone at the tissue level: A review. *Acta
454 Biomaterialia* 2018; DOI:10.1016/j.actbio.2018.08.001.
- 455 46. Mulder L, Koolstra JH, den Toonder JM et al. Relationship between tissue stiffness and degree of mineralization
456 of developing trabecular bone. *Journal of Biomedical Materials Research Part A* 2008; 84A(2): 508–515. DOI:
457 10.1002/jbm.a.31474.

- 458 47. Hong J, Cha H, Park Y et al. Elastic moduli and poisson's ratios of microscopic human femoral trabeculae. In
459 Jarm T, Kramar P and A AZ (eds.) *11th Mediterranean Conference on Medical and Biomedical Engineering*
460 *and Computing 2007, IFMBE Proceedings*, volume 16. Springer Berlin Heidelberg, 2007. pp. 274–277. DOI:
461 10.1007/978-3-540-73044-6_68.
- 462 48. García-Rodríguez J and Martínez-Reina J. Elastic properties of woven bone: effect of mineral content and
463 collagen fibrils orientation. *Biomechanics and Modeling in Mechanobiology* 2016; 16(1): 159–172. DOI:
464 10.1007/s10237-016-0808-z.
- 465 49. Pruchnicki E. Hyperelastic homogenized law for reinforced elastomer at finite strain with edge effects. *Acta*
466 *Mechanica* 1998; 129(3-4): 139–162. DOI:10.1007/bf01176742.
- 467 50. Collis J, Brown DL, Hubbard ME et al. Effective equations governing an active poroelastic medium.
468 *Proceedings of the Royal Society A: Mathematical, Physical and Engineering Science* 2017; 473(2198):
469 20160755. DOI:10.1098/rspa.2016.0755.
- 470 51. Sanz-Herrera J, García-Aznar J and Doblaré M. Micro-macro numerical modelling of bone regeneration in
471 tissue engineering. *Computer Methods in Applied Mechanics and Engineering* 2008; 197(33-40): 3092–3107.
472 DOI:10.1016/j.cma.2008.02.010.
- 473 52. Peter MA. Coupled reaction–diffusion processes inducing an evolution of the microstructure: Analysis
474 and homogenization. *Nonlinear Analysis: Theory, Methods & Applications* 2009; 70(2): 806–821. DOI:
475 10.1016/j.na.2008.01.011.
- 476 53. O’Dea RD, Nelson MR, Haj AJE et al. A multiscale analysis of nutrient transport and biological tissue growth
477 *in vitro*. *Mathematical Medicine and Biology* 2014; 32(3): 345–366. DOI:10.1093/imammb/dqu015.
- 478 54. Collis J, Hubbard M and O’Dea R. Computational modelling of multiscale, multiphase fluid mixtures with
479 application to tumour growth. *Computer Methods in Applied Mechanics and Engineering* 2016; 309: 554–578.
480 DOI:10.1016/j.cma.2016.06.015.
- 481 55. Holmes MH. *Introduction to Perturbation Methods*. Springer New York, 2013. DOI:10.1007/
482 978-1-4614-5477-9.
- 483 56. Penta R, Ambrosi D and Shipley RJ. Effective governing equations for poroelastic growing media. *The*
484 *Quarterly Journal of Mechanics and Applied Mathematics* 2014; 67(1): 69–91. DOI:10.1093/qjmam/hbt024.
- 485 57. Penta R, Ambrosi D and Quarteroni A. Multiscale homogenization for fluid and drug transport in vascularized
486 malignant tissues. *Mathematical Models and Methods in Applied Sciences* 2015; 25(01): 79–108. DOI:
487 10.1142/s0218202515500037.
- 488 58. Bruna M and Chapman SJ. Diffusion in spatially varying porous media. *SIAM Journal on Applied Mathematics*
489 2015; 75(4): 1648–1674.
- 490 59. Dalwadi MP, Griffiths IM and Bruna M. Understanding how porosity gradients can make a better filter using
491 homogenization theory. *Proceedings of the Royal Society A: Mathematical, Physical and Engineering Sciences*
492 2015; 471(2182): 20150464.
- 493 60. Fish J. Multiscale analysis of composite materials and structures. *Composites Science and Technology* 2000;
494 60(12-13): 2547–2556. DOI:10.1016/s0266-3538(00)00048-8.
- 495 61. Ghosh S, Lee K and Raghavan P. A multi-level computational model for multi-scale damage analysis in
496 composite and porous materials. *International Journal of Solids and Structures* 2001; 38(14): 2335–2385.
497 DOI:10.1016/s0020-7683(00)00167-0.
- 498 62. Grigolyuk EI and Fil’shtinskii LA. Perforated plates and shells. *Nauka, Moscow, in Russian* 1970; .
- 499 63. Sokolnikoff IS. *Mathematical theory of elasticity*. McGraw–Hill, New York, 1956.

500 64. Kantorovich LV and Krylov VI. *Approximate methods of higher analysis*. Interscience Publishers, Inc., The
501 Netherlands, 1964.

502 Solution of the cell problems

503 Following the procedure given in^{34–37}, we present an analytical approach to find the solution of the
504 cell problems \mathcal{P}_α^{qq} ($q = 1, 2, 3$) and \mathcal{P}_α^{12} . In particular, the choice of the microstructure and material
505 symmetry allow us to focus on only one hierarchical level.

506 Theoretical background

507 In the present section we list some theoretical results that will be useful in the remainder of the text.

508 **Definition 1.** Let w_1 and w_2 two linearly independent complex numbers on \mathbb{R} . That is, there not exist
509 two real numbers a and b , with $a, b \neq 0$ such that $aw_1 + bw_2 = 0$. We define a lattice, the set of all
510 complex numbers of the form

$$w = mw_1 + nw_2, \quad m, n \in \mathbb{Z}, \quad (33)$$

511 which is denoted by $L = [w_1, w_2]$.

512 **Proposition 1.** The Laurent series expansion of the $(k - 1)$ -th ($k = 2, 3, \dots$) derivative of the function
513 Z of Weierstrass (ζ) and Natanzon's function (Q) in zero are, respectively,

$$\zeta^{(k-1)} = \frac{(k-1)!}{z^k} - (k-1)! \sum_{l=1}^{\infty o} \Lambda_{kl} z^l \quad \text{and} \quad Q^{(k-1)} = (k-1)! \sum_{l=1}^{\infty o} \mathring{\Lambda}_{kl} z^l, \quad (34a)$$

514 where

$$\Lambda_{kl} = -\binom{k+l-1}{l} R^{k+l} S_{k+l} \quad \text{and} \quad \mathring{\Lambda}_{kl} = k \binom{k+l}{l} R^{k+l} T_{k+l}. \quad (35)$$

515 The superscript “o” over the sum operator indicates that the sum is carried out only over odd natural
516 numbers. The reticulate sums (which contains the geometrical information of the problem) are defined
517 by $S_{k+l} = \sum_{w \in L^*} \frac{1}{w^{k+l}}$ ($k+l \geq 2$) and $T_{k+l} = \sum_{w \in L^*} \frac{\bar{w}}{w^{k+l+1}}$ ($k+l \geq 3$). The series S_{k+l} vanishes
518 when $k+l$ is not a multiple of 4. Furthermore, the series T_{k+l} vanishes when $k+l$ is not of the form
519 $4t - 1$ for $t \in \mathbb{N}$ ⁶². Moreover, L^* represents the lattice excluding the number $w = 0$ and \bar{w} denotes the
520 conjugate of the complex number w .

521 **Proposition 2.** The function Z of Weierstrass and Natanzon's function possess the following properties
522 of quasi-periodicity

$$\zeta(z + w_p) - \zeta(z) = \delta_p, \quad \zeta^{(k)}(z + w_p) - \zeta^{(k)}(z) = 0, \quad \forall k \geq 1 \quad (36a)$$

$$Q(z + w_p) - Q(z) = \bar{w}_p P(z) + \xi_p, \quad Q^{(k)}(z + w_p) - Q^{(k)}(z) = \bar{w}_p P^{(k)}(z), \quad \forall k \geq 1, \quad (36b)$$

523 where $P(z) = -\zeta'(z)$, $\delta_p = 2\zeta(w_p/2)$ and $\xi_p = 2Q(w_p/2) - \bar{w}_p P(w_p/2)$. Moreover, Legendre's
524 relations are fulfilled, i.e.,

$$\delta_1 w_2 - \delta_2 w_1 = 2\pi i, \quad (37a)$$

$$\delta_1 \bar{w}_2 - \delta_2 \bar{w}_1 = \xi_2 w_1 - \xi_1 w_2. \quad (37b)$$

525 **Remark 1.** In the case of a square array of periodic cells, that is, for $w_1 = 1$ and $w_2 = i$, we have that
526 $\delta_1 = \pi$, $\delta_2 = -i\pi$, $\xi_1 = -\frac{5S_4}{\pi}$ and $\xi_2 = i\frac{5S_4}{\pi}$.

527 Solution of the in-plane cell problems \mathcal{P}^{qq}

528 The structure of the in-plane cell problems \mathcal{P}^{qq} ($q = 1, 2, 3$) given in (20a) is of plane-strain and
529 therefore, the theory of harmonic functions and the Kolosov-Muskhelishvili complex potentials⁶³ are
530 applicable³⁴⁻³⁷. The Kolosov-Muskhelishvili complex potentials are related to ω_{1qq} and ω_{2qq} , and to the
531 stress components by means of the formulae,

$$2\mathcal{C}_{1212}^\gamma(\omega_{1qq}^\gamma + i\omega_{2qq}^\gamma) = \chi^\gamma \varphi^{qq\gamma} - z(\overline{\varphi^{qq\gamma}})' - \overline{\psi^\gamma}, \quad (38a)$$

$$\sigma_{11}^{qq\gamma} + \sigma_{22}^{qq\gamma} = 2((\varphi^{qq\gamma})' + (\overline{\varphi^{qq\gamma, \alpha}})'), \quad (38b)$$

$$\sigma_{22}^{qq\gamma} - \sigma_{11}^{qq\gamma} = 2(\bar{z}(\varphi^{qq\gamma})'' + (\psi^{qq\gamma})'), \quad (38c)$$

532 where $\chi^\gamma = 3 - 4\nu^\gamma$ and $\nu^\gamma = \mathcal{C}_{1122}^\gamma / (\mathcal{C}_{1111}^\gamma + \mathcal{C}_{1122}^\gamma)$. The notation φ' indicates the derivative of φ
533 with respect to the complex variable z . Following³⁴⁻³⁷, the complex potentials $\varphi^{qq\gamma}$ and $\psi^{qq\gamma}$ can be
534 written as

$$\varphi^{qqm}(z) = \frac{a_0^{qq}}{R} z + \sum_{k=1}^{\infty} a_k^{qq} R^k \frac{\zeta^{(k-1)}(z)}{(k-1)!}, \quad \varphi^{qqf}(z) = \sum_{k=1}^{\infty} \frac{z^k}{R^k} c_k^{qq}, \quad (39a)$$

$$\psi^{qqm}(z) = \frac{b_0^{qq}}{R} z + \sum_{k=1}^{\infty} b_k^{qq} R^k \frac{\zeta^{(k-1)}(z)}{(k-1)!} + \sum_{k=1}^{\infty} a_k^{qq} R^k \frac{Q^{(k-1)}(z)}{(k-1)!}, \quad \psi^{qqf}(z) = \sum_{k=1}^{\infty} \frac{z^k}{R^k} d_k^{qq}, \quad (39b)$$

535 where a_k^{qq} , b_k^{qq} ($k = 0, 1, 2, \dots$), and c_k^{qq} , d_k^{qq} ($k = 1, 2, \dots$) are complex coefficients to be determined. The
536 radius of the fiber's circular cross section is denoted with R .

537 Using Proposition 1 the complex potentials φ^{qqm} and ψ^{qqm} can be rewritten as follows

$$\varphi^{qqm}(z) = \frac{a_0^{qq}}{R} z + \sum_{l=1}^{\infty} \left(a_l^{qq} \frac{R^l}{z^l} + A_l^{qq} \frac{z^l}{R^l} \right), \quad (40a)$$

$$\psi^{qqm}(z) = \frac{b_0^{qq}}{R} z + \sum_{l=1}^{\infty} \left(b_l^{qq} \frac{R^l}{z^l} + B_l^{qq} \frac{z^l}{R^l} + \hat{A}_l^{qq} \frac{z^l}{R^l} \right), \quad (40b)$$

538 where $A_l^{qq} = \sum_{k=1}^{\infty} \Lambda_{kl} a_k^{qq}$, $B_l^{qq} = \sum_{k=1}^{\infty} \Lambda_{kl} b_k^{qq}$ and $\hat{A}_l^{qq} = \sum_{k=1}^{\infty} \hat{\Lambda}_{kl} a_k^{qq}$.

539 Then, find the solution of problem (20a) is equivalent to determine the unknowns a_k^{qq} , b_k^{qq} , c_k^{qq} and
540 d_k^{qq} . In particular, we show that for computing the effective coefficients, it is sufficient to find a_1^{qq} . In the
541 following, we outline in three steps, the procedure in³⁴⁻³⁷.

542 **Step 1:** By taking into account the continuity conditions on ω_{1qq} and ω_{2qq} and the two expressions in
 543 (38a) for $\gamma = m$ and $\gamma = f$, we can deduce that

$$\chi^* (\chi^m \varphi^{qqm} - z \overline{(\varphi^{qqm})'} - \overline{\psi^{qqm}}) = \chi^f \varphi^{qqf} - z \overline{(\varphi^{qqf})'} - \overline{\psi^{qqf}}, \quad (41)$$

544 where $\chi^* = \mathcal{C}_{1212}^f / \mathcal{C}_{1212}^m$. Furthermore, the continuity conditions for traction on the interface $\tilde{\Gamma} = R e^{i\theta}$,
 545 $\theta \in [0, 2\pi]$, lead us to the following relation

$$\begin{aligned} & (\sigma_{11}^{qqm} + 2i\sigma_{12}^{qqm} - \sigma_{11}^{qqm})e^{i\theta} - (\sigma_{11}^{qqm} + \sigma_{22}^{qqm})e^{-i\theta} + 2\beta_1^{qq}e^{i\theta} - 2\beta_2^{qq}e^{-i\theta} \\ & = (\sigma_{22}^{qqf} + 2i\sigma_{12}^{qqf} - \sigma_{11}^{qqf})e^{i\theta} - (\sigma_{11}^{qqf} + \sigma_{22}^{qqf})e^{-i\theta}, \end{aligned} \quad (42)$$

546 where

$$\beta_j^{qq} = \begin{cases} \frac{[\mathcal{C}_{1122}] + (-1)^j [\mathcal{C}_{1111}]}{2}, & q = 1, \\ (-1)^j \beta_j^{11}, & q = 2, \\ \frac{1 + (-1)^j}{2} [\mathcal{C}_{1133}], & q = 3, \end{cases} \quad (43)$$

547 with $j = 1, 2$.

548 **Step 2:** Subsequently, let us evaluate (38a) (for $\gamma = m$) in z and $z + w_p$ and subtract the results of
 549 these evaluations. Using the expansions (40a) and (40b), the properties of quasiperiodicity (36a)–(36b),
 550 the periodic properties of the functions involved and Legendre's relations, we obtain that

$$a_0^{qq} + \overline{a_0^{qq}} = [(\tau_2 - \chi^m \tau_1) a_1^{qq} + (\overline{\tau_2} - \chi^m \overline{\tau_1}) \overline{a_1^{qq}} + (\tau_3 + \overline{\tau_3}) b_1^{qq}] \frac{R^2}{\chi^m - 1}, \quad (44a)$$

$$a_0^{qq} - \overline{a_0^{qq}} = [-(\tau_2 + \chi^m \tau_1) a_1^{qq} + (\overline{\tau_2} + \chi^m \overline{\tau_1}) \overline{a_1^{qq}} - (\tau_3 - \overline{\tau_3}) b_1^{qq}] \frac{R^2}{\chi^m - 1}, \quad (44b)$$

$$\overline{b_0^{qq}} = (\tau_4 \chi^m a_1^{qq} + \overline{\tau_5 a_1^{qq}} - \overline{\tau_6 b_1^{qq}}) R^2, \quad (44c)$$

551 where

$$\tau_1 = (\overline{w_1} \delta_2 - \overline{w_2} \delta_1) / W, \quad \tau_4 = -(w_1 \delta_2 - w_2 \delta_1) / W, \quad (45a)$$

$$\overline{\tau_2} = (\overline{w_1} \xi_2 - \overline{w_2} \xi_1) / W, \quad \overline{\tau_5} = (w_1 \xi_2 - w_2 \xi_1) / W, \quad (45b)$$

$$\overline{\tau_3} = (\overline{w_1} \delta_2 - \overline{w_2} \delta_1) / W, \quad \overline{\tau_6} = -(w_1 \delta_2 - w_2 \delta_1) / W, \quad (45c)$$

552 where $W = \overline{w_1} w_2 - w_1 \overline{w_2}$. Furthermore, substituting the Kolosov-Muskhelishvili relationships (38b)
 553 and (38c) in equation (42), we obtain

$$z \overline{(\varphi^{qqm})'} + \overline{\psi^{qqm}} + \varphi^{qqm} + \overline{z \beta_1^{qq}} + z \beta_2^{qq} = z \overline{(\varphi^{qqf})'} + \overline{\psi^{qqf}} + \varphi^{qqf}. \quad (46)$$

554 **Step 3:** Now, substituting the Laurent expansions (40a) and (40b) in (41) and in (46), we obtain the
 555 following infinite linear system in the unknowns $\tilde{a}_l^{qq} = a_l^{qq} / (R \beta_2^{qq})$ ($q = 1, 2, 3$ and $l = 1, 3, 5, \dots$)

$$\tilde{a}_l^{qq} + \mathcal{H}_l^1 \tilde{a}_1^{qq} + \mathcal{H}_l^2 \overline{\tilde{a}_1^{qq}} + \sum_{k=1}^{\infty} \mathcal{W}_{kl} \tilde{a}_k^{qq} + \sum_{k=1}^{\infty} \mathcal{M}_{kl} \overline{\tilde{a}_k^{qq}} = \mathcal{H}_l^{qq}, \quad (47)$$

556 where

$$\mathcal{H}_l^1 = [2\tau_4\chi^m(\chi^m - 1)\beta R^2\delta_{1l} + (\overline{\Lambda_{1l}} - \overline{\tau_6 R^2\delta_{1l}})(\tau_2 - \chi^m\tau_1)\mu R^2]/[2(\chi^m - 1)], \quad (48a)$$

$$\mathcal{H}_l^2 = [2\overline{\tau_5}(\chi^m - 1)\beta R^2\delta_{1l} + (\overline{\Lambda_{1l}} - \overline{\tau_6 R^2\delta_{1l}})(\overline{\tau_2} - \chi^m\overline{\tau_1})\mu R^2]/[2(\chi^m - 1)], \quad (48b)$$

$$\mathcal{W}_{kl} = \chi^{mf*}\mathcal{V}_{kl} + \tau_l\Upsilon\Lambda_{k1}, \quad (48c)$$

$$\mathcal{M}_{kl} = \chi^{m*}\mathcal{N}_{kl} + \tau_l\Upsilon\overline{\Lambda_{k1}}, \quad (48d)$$

$$\mathcal{N}_{kl} = (l+2)\overline{\Lambda_{k(l+2)}} + k\overline{\Lambda_{(k+2)l}} + \overline{\Lambda_{kl}}, \quad (48e)$$

$$\mathcal{V}_{kl} = \sum_{j=1}^{\infty} \Lambda_{k(j+2)}\overline{\Lambda_{(j+2)l}}, \quad (48f)$$

$$\mathcal{H}_i^{qq} = (\theta\beta_1^{qq}/\beta_2^{qq} - \overline{\tau_6}R^2\Upsilon^*)\delta_{1l} + \overline{\Lambda_{1l}}\Upsilon^*, \quad (48g)$$

$$\mu = \beta\alpha_0^{-1}(1 + \chi^*\chi^m - \chi^* - \chi^f), \quad (48h)$$

$$\beta = (1 - \chi^*)(\chi^*\chi^m + 1)^{-1}, \quad (48i)$$

$$\alpha_0 = \chi^*[1 - Re(\tau_3)R^2] + (\chi^f - 1)\left[\frac{Re(\tau_3)R^2}{\chi^m - 1} + \frac{1}{2}\right], \quad (48j)$$

$$\theta = -(\chi^*\chi^m + 1)^{-1}, \quad (48k)$$

$$\chi^{m*} = (1 - \chi^*)(\chi^*\chi^m + 1)^{-1}, \quad (48l)$$

$$\chi^{mf*} = (\chi^{m*}(\chi^*\chi^m - \chi^f))(\chi^* + \chi^f)^{-1}, \quad (48m)$$

$$\Upsilon = (\chi^{m*}(1 + \chi^*\chi^m - \chi^* - \chi^f))\alpha_0^{-1}, \quad (48n)$$

$$\Upsilon^* = (\chi^{m*}(\chi^f - 1))(2\alpha_0)^{-1}. \quad (48o)$$

557 In particular, the linear system (47) can be equivalently rewritten as

$$\begin{pmatrix} \tilde{\mathcal{A}}_r^{qq} \\ \tilde{\mathcal{A}}_i^{qq} \end{pmatrix} = \begin{pmatrix} \mathcal{I} + \check{\mathcal{M}}_r + \check{\mathcal{W}}_r & \check{\mathcal{M}}_i - \check{\mathcal{W}}_i \\ \check{\mathcal{M}}_i + \check{\mathcal{W}}_i & \mathcal{I} + \check{\mathcal{M}}_r - \check{\mathcal{W}}_r \end{pmatrix}^{-1} \begin{pmatrix} \mathcal{H}_r^{qq} \\ \mathcal{H}_i^{qq} \end{pmatrix}, \quad (49)$$

558 where $\tilde{\mathcal{A}}_r^{qq} = (Re(\tilde{a}_1^{qq}), Re(\tilde{a}_3^{qq}), \dots)^T$, $\tilde{\mathcal{A}}_i^{qq} = (Im(\tilde{a}_1^{qq}), Im(\tilde{a}_3^{qq}), \dots)^T$, with \mathbf{a}^T denoting the
559 operation of transposition of the vector \mathbf{a} . Moreover, \mathcal{I} is the infinite identity matrix, $\check{\mathcal{M}}_r = Re(\check{\mathcal{M}})$,
560 $\check{\mathcal{W}}_r = Re(\check{\mathcal{W}})$, $\check{\mathcal{M}}_i = Im(\check{\mathcal{M}})$, $\check{\mathcal{W}}_i = Im(\check{\mathcal{W}})$, $\mathcal{H}_r^{qq} = Re(\mathcal{H}^{qq})$ and $\mathcal{H}_i^{qq} = Im(\mathcal{H}^{qq})$, where $Re(\Phi)$
561 and $Im(\Phi)$ denote the operators that extract the real and imaginary parts of Φ , respectively. The
562 matrices $\check{\mathcal{M}}$ and $\check{\mathcal{W}}$ are decomposed additively as follows, $\check{\mathcal{M}} = \mathcal{U} + \mathcal{M}$ and $\check{\mathcal{W}} = \mathcal{Q} + \mathcal{W}$, where the
563 components of \mathcal{U} and \mathcal{Q} , are given by the following expressions,

$$\mathcal{U}_{kl} = \begin{cases} [2\tau_4\chi^m(\chi^m - 1)\chi^{m*}R^2\delta_{1l} + (\overline{\Lambda_{11}} - \overline{\tau_6 R^2\delta_{11}})(\tau_2 - \chi^m\tau_1)\Upsilon R^2][2(\chi^m - 1)]^{-1}, & k = 1, \\ 0, & k > 1, \end{cases} \quad (50a)$$

$$\mathcal{Q}_{kl} = \begin{cases} [2\overline{\tau_5}(\chi^m - 1)\chi^{m*}R^2\delta_{1l} + (\overline{\Lambda_{11}} - \overline{\tau_6 R^2\delta_{11}})(\overline{\tau_2} - \chi^m\overline{\tau_1})\Upsilon R^2][2(\chi^m - 1)]^{-1}, & k = 1, \\ 0, & k > 1. \end{cases} \quad (50b)$$

564 Equation (49) is an infinite linear system with an infinite number of unknowns for which is possible to
 565 obtain a solution by truncation through a convergent sequence of solutions^{35–37,64}.

566 *Solution of the problem \mathcal{P}^{12}*

567 The solution of the in-plane problem \mathcal{P}^{12} (20b) can be found following a similar procedure to the one
 568 outlined above. In such a case, the following infinite linear system in the unknowns \tilde{a}_l^{12} ($l = 1, 3, 5, \dots$)
 569 is obtained

$$\begin{pmatrix} \mathcal{A}_r^{12} \\ \mathcal{A}_i^{12} \end{pmatrix} = \begin{pmatrix} \mathcal{I} + \check{\mathcal{M}}_r + \check{\mathcal{W}}_r & \check{\mathcal{M}}_i - \check{\mathcal{W}}_i \\ \check{\mathcal{M}}_i + \check{\mathcal{W}}_i & \mathcal{I} + \check{\mathcal{M}}_r - \check{\mathcal{W}}_r \end{pmatrix}^{-1} \begin{pmatrix} \mathcal{H}_r^{12} \\ \mathcal{H}_i^{12} \end{pmatrix}, \quad (51)$$

570 where $\check{\mathcal{A}}_r^{12} = (Re(\tilde{a}_1^{12}), Re(\tilde{a}_3^{12}), \dots)^T$, $\check{\mathcal{A}}_i^{12} = (Im(\tilde{a}_1^{12}), Im(\tilde{a}_3^{12}), \dots)^T$, $\mathcal{H}_l^{12} = \theta \beta_1^{12} R \delta_{1l}$ and $\beta_1^{12} =$
 571 $-i(\mathcal{C}_{1212}^m - \mathcal{C}_{1212}^f)$.

572 **Effective coefficients**

573 The fact that $\mathcal{C}^{\varepsilon_2}$ is isotropic, together with the assumption that the cell's cross section corresponds to a
 574 square embedding a single circle, induce that the tensor \mathcal{C} has tetragonal symmetric structure. This result
 575 together with the isotropy assumption of the constituent $\Omega_{m1}^{\varepsilon_1}$ imply that the effective tensor $\hat{\mathcal{C}}$ is at most
 576 monoclinic. That is, $\hat{\mathcal{C}}$ has at most 13 independent effective elastic coefficients. In the following, we will
 577 consider two elasticity tensors \mathcal{C}^m and \mathcal{C}^f having tetragonal symmetric structure. In this way, the results
 578 will apply to both hierarchical levels.

579 *The in-plane effective coefficients*

580 Taking into account the major and minor symmetries of the elasticity tensor, the non-zero effective
 581 coefficients corresponding to the in-plane problems \mathcal{P}^{qq} are

$$\hat{\mathcal{C}}_{11qq} = \langle \mathcal{C}_{1111}^{\varepsilon} \frac{\partial \omega_{1qq}}{\partial y_1} + \mathcal{C}_{1122}^{\varepsilon} \frac{\partial \omega_{2qq}}{\partial y_2} + \mathcal{C}_{11qq}^{\varepsilon} \rangle, \quad (52a)$$

$$\hat{\mathcal{C}}_{12qq} = \langle \mathcal{C}_{1221}^{\varepsilon} \frac{\partial \omega_{2qq}}{\partial y_1} + \mathcal{C}_{1212}^{\varepsilon} \frac{\partial \omega_{1qq}}{\partial y_2} \rangle, \quad (52b)$$

$$\hat{\mathcal{C}}_{21qq} = \langle \mathcal{C}_{2121}^{\varepsilon} \frac{\partial \omega_{2qq}}{\partial y_1} + \mathcal{C}_{2112}^{\varepsilon} \frac{\partial \omega_{1qq}}{\partial y_2} \rangle, \quad (52c)$$

$$\hat{\mathcal{C}}_{22qq} = \langle \mathcal{C}_{2211}^{\varepsilon} \frac{\partial \omega_{1qq}}{\partial y_1} + \mathcal{C}_{2222}^{\varepsilon} \frac{\partial \omega_{2qq}}{\partial y_2} + \mathcal{C}_{22qq}^{\varepsilon} \rangle, \quad (52d)$$

$$\hat{\mathcal{C}}_{33qq} = \langle \mathcal{C}_{3311}^{\varepsilon} \frac{\partial \omega_{1qq}}{\partial y_1} + \mathcal{C}_{3322}^{\varepsilon} \frac{\partial \omega_{2qq}}{\partial y_2} + \mathcal{C}_{33qq}^{\varepsilon} \rangle. \quad (52e)$$

582 We observe that the variable y plays the role of η and ς since the procedure to obtain the effective
 583 coefficients, for this particular case, is the same.

584 Working with the expressions (52a)–(52e), applying Green's theorem to find the integrals involved,
 585 taking into account the periodicity properties of the involved functions, the continuity conditions on the

586 interface $\tilde{\Gamma}$, the Kolosov-Muskhelishvili formula (38a), the Laurent expansions of φ^{qqm} and ψ^{qqm} , the
587 orthogonality property of the system of functions $\{e^{im\theta}\}_{n=-\infty}^{+\infty}$ in the interval $[-\pi, \pi]$, we can write

$$\begin{aligned} \hat{\mathcal{C}}_{11qq} &= \langle \mathcal{C}_{11qq} \rangle - V_f \beta_2^{11} [\beta_2^{11} [2\chi^* \beta(\chi^f + 1) \mathcal{C}_{1212}^m]^{-1} Re(\chi^f \Xi^{qq} - \overline{\Xi^{qq}}) \\ &\quad + Re((\chi^m + 1) \overline{\tilde{a}_1^{qq}} + \beta_1^{qq} (\beta_2^{qq})^{-1})], \end{aligned} \quad (53a)$$

$$\begin{aligned} \hat{\mathcal{C}}_{22qq} &= \langle \mathcal{C}_{22qq} \rangle - V_f \beta_2^{11} [\beta_2^{11} [2\chi^* \beta(\chi^f + 1) \mathcal{C}_{1212}^m]^{-1} Re(\chi^f \Xi^{qq} - \overline{\Xi^{qq}}) \\ &\quad - Re((\chi^m + 1) \overline{\tilde{a}_1^{qq}} + \beta_1^{qq} (\beta_2^{qq})^{-1})], \end{aligned} \quad (53b)$$

$$\hat{\mathcal{C}}_{33qq} = \langle \mathcal{C}_{33qq} \rangle - V_f \beta_2^{33} \beta_2^{qq} [2\chi^* \beta(\chi^f + 1) [\mathcal{C}_{1212}^m]^{-1} Re(\chi^f \Xi^{qq} - \overline{\Xi^{qq}})], \quad (53c)$$

$$\hat{\mathcal{C}}_{12qq} = V_f \beta_2^{qq} Im((\chi^m + 1) \overline{\tilde{a}_1^{qq}} + \beta_1^{qq} (\beta_2^{qq})^{-1}), \quad (53d)$$

588 where $V_f = \pi R^2$ represents the volume fraction of the circular inclusion and

$$\begin{aligned} \Xi^{qq} &= \{[(\beta\chi_-^m + \mu\beta_0)\tau_2 - (\beta\chi_-^* + \mu\beta_0)\tau_1\chi^m]R^2\}(\chi^m - 1)^{-1} \tilde{a}_1^{qq} + \{[(\beta\chi_-^* + \mu\beta_0)\overline{\tau_2} \\ &\quad - (\beta\chi_-^m + \mu\beta_0)\overline{\tau_1}\chi^m]R^2\}(\chi^m - 1)^{-1} \overline{\tilde{a}_1^{qq}} + (\beta\chi_+ + \mu\beta_0) \tilde{A}_1^{qq} + (\beta\chi_- + \mu\beta_0) \overline{\tilde{A}_1^{qq}} \\ &\quad + \beta(\chi^f + 1) - 2\beta_0\vartheta, \end{aligned} \quad (54a)$$

$$\beta_0 = (\chi^f + 1) \left[\frac{Re(\tau_3)R^2}{\chi^m - 1} + \frac{1}{2} \right] - i\chi^* Im(\tau_3)R^2, \quad (54b)$$

$$\chi_-^m = \chi^f + 1 - \chi^* \chi^m + \chi^*, \quad (54c)$$

$$\chi_-^* = \chi^f + 1 + \chi^* \chi^m - \chi^*. \quad (54d)$$

589 In (54a), we denote by $\tilde{A}_l^{qq} = \sum_{k=1}^{\infty} \Lambda_{kl} \tilde{a}_l^{qq} / (R\beta_2^{qq})$.

590 Resuming, formulae (53a), (53b), (53c) and (53d) give the effective coefficients $\hat{\mathcal{C}}_{11qq}$, $\hat{\mathcal{C}}_{22qq}$, $\hat{\mathcal{C}}_{33qq}$
591 and $\hat{\mathcal{C}}_{12qq}$, respectively. As anticipated, the effective coefficients depend solely on the unknowns a_1^{qq} .

592 Finally, proceeding in an analogous way, the only one non-zero effective coefficient corresponding to
593 the in-plane problem \mathcal{P}^{12} is

$$\hat{\mathcal{C}}_{1212} = \mathcal{C}_{1212}^m - \llbracket \mathcal{C}_{1212} \rrbracket V_f Im((\chi^m + 1) \tilde{a}_1^{12}). \quad (55)$$