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A consensus research agenda for optimising nasal drug delivery

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10 ABSTRACT

Nasal drug delivery has specific challenges which are distinct from oral inhalation, alongside which it is often considered. The next generation of nasal products will be required to deliver new classes of molecule, e.g. vaccines, biologics and drugs with action in the brain or sinuses, to local and systemic therapeutic targets. Innovations and new tools/knowledge are required to design products to deliver these therapeutic agents to the right target at the right time in the right patients. We report the outcomes of an expert meeting convened to consider gaps in knowledge and unmet research needs in terms of (i) formulation and devices, (ii) meaningful product characterization and modeling, (iii) opportunities to modify absorption and clearance. Important research questions were identified in the areas of device and formulation innovation, critical quality attributes for different nasal products, development of nasal casts for drug deposition studies, improved experimental models, the use of simulations and nasal delivery in special populations. We offer these questions as a stimulus to research and suggest that they might be addressed most effectively by collaborative research endeavors,

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Biopharmaceutics; nose-tobrain; vaccine; sinus; biologics; formulation; device; deposition; nasal cast

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1. Introduction

Nasal drug delivery has several specific challenges which are 25 distinct from oral inhalation, alongside which it is often considered. An expert meeting was convened on 15 May 2019 to scope the future needs of nasal delivery. The meeting, jointly designed by Professors Sonvico, Scherließ and Forbes, was held at the Department of Pharmaceutics and Biopharmaceutics of Kiel

30 University in Germany and attended by expert academic and industrial associates who included drug delivery scientists, device designers and product developers (listed as coauthors). Deliberations focused on (i) formulation and device needs, (ii) meaningful product characterization and modeling, (iii) influen-35 cing absorption and clearance.

Nasal administration is often associated with prescribed and over-the-counter medicinal products for the management of ailments such as nasal congestion, common cold symptoms, seasonal allergies or more persistent conditions such

40 as chronic sinusitis. These are treated with drug solutions or suspensions, typically using a hand-operated metered dose pump that delivers a conical spray upon actuation into the nasal cavities. This simple approach and the ease of administration lends itself to regulatory approaches focused on device 45 and formulation.

The nose offers easy access to a highly vascularized and relatively permeable mucosa, making it attractive not only for topical treatment of local diseases but also for systemic drug delivery. The presence of immunocompetent cells and the direct access to the brain via the olfactory region are auspi-50 cious as special target sites for needle-free vaccination or central nervous system targeting. However, factors related to the physiological function of the nose and special needs of new drug candidates are hurdles on the way to optimized nasal drug delivery. Nasal delivery notably provides successful 55 noninvasive, systemic delivery for a variety of peptide drugs. Desmopressin was the first nasal peptide product in 1978, guickly followed by calcitonin, buserelin, naferelin and oxytocin [1]. After a period of latency, new applications are now gathering momentum, including (i) vaccination [2], e.g. 60 FluMist® the nasal influenza vaccine, and (ii) drug delivery to the brain [3], e.g. naloxone for emergency reversal of opioid overdose (Narcan®) and the recently approved potential blockbuster product esketamine nasal spray (Spravato®) for treatment resistant depression. Illustrative examples of nasal 65 delivery systems in clinical trials include low-dose oxytocin for effects on social-cognitive behavior [4] and insulin for effects on cognition and Alzheimer's disease [5]. There are too many molecules and therapies currently in the pre-clinical and clinical development pipeline to summarize, fully in this article; the 70 interested readers are referred to dedicated databases, such as Pharmacircle. There are also multiple patents in the nasal drug

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delivery area, but this too is a complex and specialist area beyond the scope of this article.

75 More challenging drug candidates like water insoluble compounds and degradation-sensitive proteins require more sophisticated formulation and delivery approaches. Furthermore, it is desirable to control deposition, absorptive and non-absorptive clearance by tailored adaption of formulation and/or device,

80 while considering the variability in the entire patient population from infant to geriatric. Meaningful and biorelevant prediction models for deposition, clearance and absorption are needed in which to assess the efficacy of new nasal drug delivery approaches. The purpose of the meeting was to establish a focus group

- 85 to pave the way for future development of nasal products by identifying and addressing technical and regulatory hurdles hampering the development of innovative nasal products. This is easier in the precompetitive space where open innovation is possible [6]. If a consensus can be agreed regarding the most
- 90 important research questions, then expertise can be combined in collaborative efforts to understand better how to optimize nasal products.

2. Formulations and delivery devices

A variety of devices and formulations are well established for nasal delivery (reviewed elsewhere; see [7–10]). Liquid formulations dominate the market and are delivered as drops, pump or propellant-driven sprays, or by nebulization. Powders are generally delivered by devices that spray the powder or require insufflation by the patient. Spray characteristics, 100 deposition, mucociliary clearance, dissolution and absorption

- strongly affect the performance of nasal drug delivery systems. All of these steps can be influenced by formulation and device design. While the formulation is often key to performance, the device supports an optimized formulation and these components should not be considered in isolation. In principle, pro-
- ducts for nasal drug delivery should be as simple as possible to reduce failure modes, but there are scenarios where high technology concepts may offer advantages, e.g. absorption enhancement in systemic delivery, targeted deposition in
- 110 nose-to-brain delivery and adjuvants for nasal vaccination. The ideal attributes of a nasal spray are efficient deposition in the nasal cavity, reproducibility, robustness, tolerability and low respirable fraction [11–13]. The dependence of nasal deposition on aspects of the spray plume is poorly defined

115 as it is technically difficult to vary properties such as droplet size distribution, droplet velocity and spray cone angle systematically and human factors are also a big influence.

Formulation is a critical determinant of product performance and may be the dominant factor for therapeutic effi-

- 120 ciency [11]. The critical quality attributes for nasal formulations are not well established, but different pharmacokinetics or clinical outcomes can be influenced by the use of powders versus solutions, different excipients and delivered volume/ mass. A possible strategy to protect the drug from enzymatic
- 125 degradation may be the forming of protective shells, such as liposomes or micelles, or the addition of enzyme inhibitors and the addition of mucoadhesive agents may enhance absorption by prolonging the residence time of the formulation in the nose [13,14]. For powders, changing the particle

size distribution or applying particle engineering can influence 130 deposition and dissolution [12]. For wet nasal sprays changing droplet size distribution is more difficult due to limitations of typical swirl spray nozzles.

A better understanding of the local effects of excipients and formulation strategies in the nasal environment is 135 required to precisely control the outcomes. In this regard, marketing applications often include quality-by-design and design-of-experiments analyses, but these are not public data and the effective extent and focus of these investigations has not been standardized. Wide ranges of variables may be 140 tested to evaluate their impact on product performance in vitro - but it is unclear how and to what extent this relates to in vivo performance. Some critical product attributes are likely to be product-specific, whereas others may be more generalizable. Defining these attributes is pivotal to guiding 145 formulation and device optimization in product development and developing 'best practice' for product characterization. An aspect often overlooked is the sensory impact of formulations including taste, odor, and somatosensory perception (in particular for powders). While liquids may drip down the 150 esophagus and lead to bad tastes, powders may cause greater sensory irritations [15]. The evaluation of sensory effects of nasal formulations is underestimated until now and masking of unpleasant tastes, odors and sensation in nasal formulations is an unworked field for research. Sensory properties can 155 sometimes be harnessed for positive effects, although blinding in clinical studies can be compromised.

As supportive and inseparable parts of nasal drug delivery systems, the device design and functionality are essential. The impact of different devices on delivered dose and site of deposi-160 tion (e.g. reservoir vs single dose) and their use by the patient (angle, actuation force, inhalation maneuver,) compared to formulation variables (powder or solution) is not understood fully. Devices may be designed to target a specific site within the nasal cavity with the aim of optimizing pharmacokinetics. Device, for-165 mulation and patient-related variables influence regional deposition and several attempts have been made to model this in view of understanding and predicting drug deposition in the nasal cavity [16]. There are instances when special product designs may be required for particular delivery needs, e.g. mucosal, sinus, systemic 170 or nose-to-brain delivery, or delivered substance, e.g. small molecule, biologic or vaccine.

The compliance of patients may be encouraged with robust and easy to use devices and minimal device-related sensory effects. High-speed impaction, low temperature or direct contact of the device tip with the particularly sensitive anterior part of nasal mucosa cause unpleasant sensations which need to be avoided [8]. The development and evaluation of gentle devices, especially for children, is therefore desirable.

3. Product characterization

Comprehensive *in vitro* quality and performance requirements for nasal products include physico-chemical properties of the formulation such as pH, osmolarity and viscosity, device extractables and leachables, delivered dose uniformity through container life, device robustness, spray pattern and Q6

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plume geometry [7,17,18]. Human factors guidelines [19] attempt to account for usability and variation introduced by patient-device interaction. Variables include penetration depth, angle, head orientation, actuation force, sniffing/inha-

- 190 lation maneuver, counter and nostril closure. Taking these into account early avoids problems in the clinic and allows a product development 'story' to be developed, although it is unclear whether there are nasal-specific human factors and what these might be.
- 195 Formulations are characterized according to product type [12,20]. Liquid formulations require a focus on API solubility, viscosity, surface tension and density. For particle/droplet size produced by nasal sprays, the emphasis is on the containment of inhalable aerosols, with a requirement to determine the percen-
- 200 tage of droplets below 10 μm. In contrast, aerodynamic particle size distribution is required for orally inhaled products and several non-compendial tests are available, often aimed at more biorelevant characterization of product performance. In contrast to nasal sprays, nasal nebulizers produce particle of much lower
- size, predominately less than 5 µm, however, there is no standard or regulation about nasal nebulizers. When the API is delivered as a solid, e.g. in powders or suspensions, the physical and chemical properties of the particles should be determined and drug dissolution in physiological conditions may become an important
- 210 consideration. Some tests for nasal products such as spray pattern and plume geometry may be of limited biological relevance, although they may be useful for regulatory or quality control purposes. Some locally-acting formulations are sufficiently straightforward that BE studies can be waived, e.g. mometasone
- 215 furoate nasal suspension spray [21]. Excipients and physicochemical properties (volume, osmolarity, viscosity) can effect dissolution rate, which may vary according to the environment of the local deposition site in the nasal cavity. Dissolution is not generally considered to be clinically significant for nasal products 220 and is little researched – there are no sustained release nasal
- 220 and is little researched there are no sustained release nasal spray products. However, despite similar conclusions being reached for orally inhaled drug products in 2012 [22], there is

currently a high level of interest in the dissolution of aerosol medicines for oral inhalation.

225 Computational fluid dynamics (CFD) provides a useful research tool, although predictions of in vivo deposition patterns require experimental verification. Nor is the relationship between spray velocity and in vivo deposition fully elucidated. The US FDA directs nasal medicinal product developers toward deposition studies using casts and dissolution. It is 230 still unclear what the impact of dissolution is for current suspension/powder products. A variety of casts have been developed for predicting regional deposition, analogous to the more advanced casts of the throat/lungs that are being used for pulmonary drug delivery [13] and similar guestions 235 arise regarding the need for idealized casts, or casts that reflect sub-populations of patient anatomy or disease. There is little validation of nasal cast models [23], and it has been proposed that biorelevance could be improved by using materials being able to better mimic physiological conditions, such 240 as softer, expandable materials with a flexible nasal valve, or by introducing cells or mucus to reflect the surface characteristics of the nasal mucosa.

4. Drug retention and absorption in the nasal cavity

245 To optimize nasal drug delivery, the device and formulation must be designed to overcome the physiological constraints on drug delivery (Figure 1). It is difficult to model the interplay of deposition, clearance and absorption that determines local exposure and systemic pharmacokinetics in vitro. The nasal epithelium is generally considered to be less restrictive compared to the gas-250 trointestinal tract, but drug permeability may vary in different regions of the nasal cavity (olfactory, vestibule, turbinates, septum), between species and/or individuals and in pathological conditions, but it is unknown to what extent such variations may impact the pharmacokinetics and clinical effects compared 255 to device and formulation factors. For example, the presence and impact of transporters is unclear. Biorelevant models to evaluate

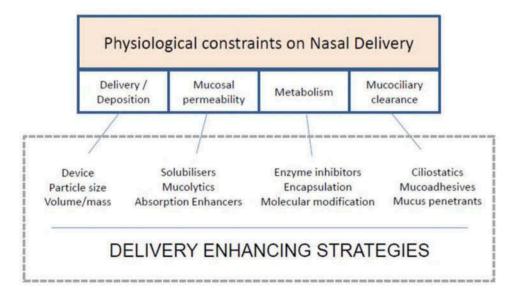


Figure 1. To optimize nasal drug delivery, the device and formulation must be designed to overcome the physiological constraints on drug delivery [adapted from Ref 24].

permeability or dissolution in simulated nasal environments have been developed that can guide the development of bioe-

- 260 guivalent products and tackle challenges related to novel products such as poor water solubility, high dose, controlled release formulation, biotechnological products and systemic delivery of actives. Experimental systems for studying drug transport in the airways include cell lines, e.g. Calu-3 [24] or RPMI 2650 [26],
- 265 primary cells [27] and reconstructed epithelia [28]. Neuronepithelial cocultures are under development to simulate the nose-to-brain route [29] as an alternative to ex vivo olfactory tissue which is difficult to use. Although there is limited IVIVC for nasal permeability models, these models can be used at an air 270 interface to study particle deposition and formulation effects
- including the functionality and safety of excipients, e.g. by measuring changes in transepithelial electrical resistance induced by absorption enhancers. However, tolerability may vary in vitro vs in vivo as well as in some populations, e.g. pediatrics or older 275 people.
- Mucociliary clearance varies within and between people but is a hindrance to drug retention in the nose [30]. In humans, material deposited in the nasal cavity is normally cleared in 12–15 min, although this may rise to >30 min if mucociliary 280 clearance is impaired [31]. If a formulation affects drug dissolution or mucus biochemistry and structure, it may modify clearance rate. Experimental models to study mucociliary clearance include ciliated cells for measuring ciliary beat frequency and airway tissue models such as chick and sheep trachea, frog
- 285 palate. Although the nose is generally regarded as a single compartment in pharmacokinetic modeling, clearance rates may vary from different deposition sites. Mechanistic models are increasingly being used in drug delivery science and can pull together deposition, dissolution, clearance and permeability data in
- 290 a combinatorial approach which utilize a mix of experimental data and simulations [16,32]. Such an approach could be used to determine the interplay and biological relevance of dissolution and mucociliary clearance.

Device and formulation can be used to target sites in the nasal 295 cavity, e.g. sinuses and NALT which are difficult to reach. Exclusive targeting of such regions seems not possible, but it is possible to influence regional deposition as demonstrated with nasal nebulizers using air vibration to improve deposition in maxillary sinuses [33,34]. Furthermore, it must be remembered that dose

- 300 will redistribute (smear) across the nasal cavity by mucociliary clearance, thus deposition in the turbinates may be adequate to target the nasal mucosal surface for local effects or drug absorption. Validation of targeting specific sites could be achieved by studying regio-temporal drug disposition after applying radiola-
- 305 belled API to specific nasal sites using a catheter to provide proof of concept for targeting particular absorption sites/mechanisms. Pharmacokinetic-modifying formulation options include polymers, which can modulate absorption and target dendritic cells. Mucus penetrating and mucoadhesive formulations have been
- 310 studied; some excipients are able to combine both properties, e.g. chitosan [35]. Pharmaceutical acceptability is an important issue for absorption enhancers, although some such as chitosan, alkylsaccharides and pectin are already utilized in products. Many 'advanced' formulations are under investigation for nose-to-brain
- 315 delivery, although simple formulations also seem to be effective [36]. However, it remains unclear (i) how much drug reaches the

brain via this route, (ii) the nature and capacity of the pathway(s) of the nose-to-brain shunts and their relative contributions to drug transport, and (iii) whether or how nanoparticle formulations enhance drug delivery to the brain via this route. Delivery 320 drugs to the brain may be a benefit or safety concern depending on the drug target.

5. Conclusions and expert opinion

The global nasal drug delivery technology market size was valued at USD 41.01 billion in 2017 and is projected to expand 6.5% by 325 2025 [37] including novel drugs and targets. New technology and tools will be required to develop these products and key challenges for nasal delivery are how to achieve prolonged nasal retention or target drugs to the systemic circulation or brain selectively (Figure 2). Current research questions include: 330

- Device innovation Can devices be designed with regard to human factors, including simplicity and robustness? Are such devices able to target specific sites in the nasal cavity?
- 335 • Formulation innovation Can the use of functional excipients be extended (e.g. permeation enhancers; dissolution modifiers) and what are their sensory effects? What new opportunities do nanomedicines offer? 340
- Critical quality attributes Can critical attributes be defined for different nasal products, e.g. solution sprays, suspensions, powders or locally versus systemically targeted products? These could be investigated systematically using quality by design approaches.
- Experimental models and simulation ٠ How useful are nasal casts? How can they be 'validated'? How would their usefulness be demonstrated experimentally? Can the nasal vibrissae and mucosal surface be represented in models? Are a range of nasal casts 350 needed (small, medium, large, male/female, children of different ages) to reflect the large variability in anatomy in human subjects?
- Nasal casts for drug deposition Are current experimental models for dissolution, perme-355 ability and clearance fit for testing drug delivery strategies or are new models needed? Can experimental data be used as inputs for mechanistic modelling to predict the pharmacokinetics?
- 360 Nasal delivery in special populations Are there specific requirements for products for paediatric (infant and child) or elderly patients? How and why should these differ from products for the adult population? Are different devices or formulations needed in patients with 365 nasal pathology?

We offer these questions as a stimulus to research and suggest that they might be addressed most effectively by collaborative research endeavors, Better understanding will enable development of innovative optimized products for nasal drug delivery and will allow development of evidence-based best practice

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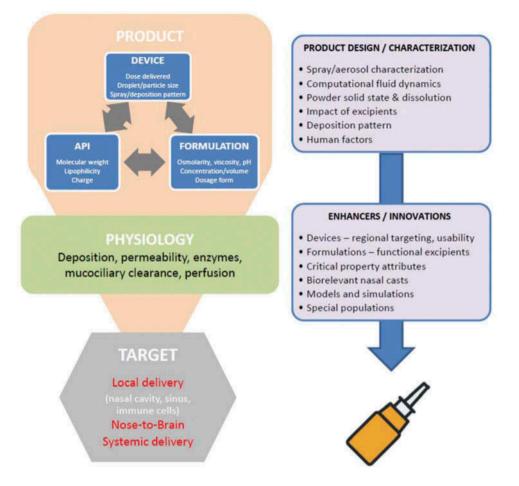


Figure 2. The next generation of nasal products will be required to deliver new classes of molecule, e.g. vaccines, biologics and drugs with action in the brain, to local and systemic therapeutic targets. Innovations and new tools/knowledge are required to design products to deliver these drugs to the right target at the right time in the right patients [38].

370 and appropriate regulations to assure their quality and fitness for purpose.

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Author Contributions

This article codifies the gist of the discussions and key issues identified, based on contemporaneous notes made at the meeting; post-hoc referencing benchmarks the subject matter to the pharmaceutical literature.

- 380 The final expert opinion section of the article reports a consensus on the key research questions for the development of the next generation of nasal drug products. The meeting was designed by B Forbes, R Scherließ and F Sonvico, who created the first draft of the manuscript. All authors attended and contributed to discussion at the workshop. All authors contributed to manuscript review and editing. All authors concur that
- this report accurately describes the consensus research agenda for optimising nasal drug delivery developed at the workshop.

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Declaration of Interest

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