

Concept Paper

Neural wave interference in inhibition-stabilized networks

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Abstract: We study how excitation propagates in chains of inhibition-stabilized neural networks with nearest-neighbor coupling. The excitation generated by local stimuli in such networks propagates across space and time, forming spatiotemporal waves that affect the dynamics of excitation generated by stimuli separated spatially and temporally. These interactions form characteristic interference patterns, manifested as network preferences: for spatial and temporal frequencies of stimulus intensity, for stimulus velocities, and as contextual ("lateral") interactions between stimuli. Such preferences have been previously attributed to distinct specialized mechanisms.

Keywords: vision, sensing, neural networks, lateral interactions, contextual modulation

1. Introduction

Waves propagating through a medium from difference sources may form patterns. When the wave equations are linear, the waves interfere constructively or destructively, yielding local nodes and antinodes that may retain their spatial positions (as in standing waves) or evolve in space and time (producing dynamic patterns). Such effects were originally studied for acoustic and light waves [1–4] followed by observations of interference for quantum particles [5,6].

More recently, propagation of activity in the neural tissue was studied in terms of the waves of neural excitation [7,8]. One may expect that a wave generated in a sensory network at one stimulus location

would interfere with the waves generated at other locations. Such "lateral" interactions between stimuli are commonly observed in psychophysical and physiological studies of biological sensory systems, where spatially separated stimuli produce patterns of facilitation and suppression in the intervening space [9–11]. But these interactions have not been attributed to neural wave interference. Instead, they have been commonly described in terms of filter characteristics of sensory systems and in terms of long-range neuronal mechanisms [12].

On the description of sensory mechanisms as filters, the response of a biological sensory system to a stimulus is predicted by convolving the stimulus with a kernel whose parameters are estimated in psychophysical [13,14] or physiological [15] studies, or are selected for computational reasons in view of the goals of the visual system (e.g., [16]). Mathematically, this approach is equivalent to describing the system by a set of spatiotemporal differential equations, for which the solutions are found by convolving the simulated inputs with the Green's function of the neural network [17,18].

Here we propose that the commonly observed phenomena of suppression and facilitation of spatially and temporally separated stimuli in biological sensory systems can be understood in terms of interference of neural waves propagating through the network, and described by the spatiotemporal differential equations supporting damped-wave solutions. We investigate the interference patterns created by the waves of excitation in one-dimensional neural chains. We find that such patterns resemble several salient properties of the sensory phenomena that have been attributed to distinct specialized mechanisms [9–11,19,20]. We show that these phenomena can be controlled by a small number of parameters in the interest of making the sensory system selectively tuned to useful properties of the optical environment.

2. Inhibition-stabilized networks with nearest-neighbor coupling

Neural networks underlying sensory processes have been modeled at different levels of abstraction, including the models for local circuitry and for interactions between the local circuits [8,21]. Yet the consequences of interference tend to depend more significantly on network geometry and topology (i.e.,

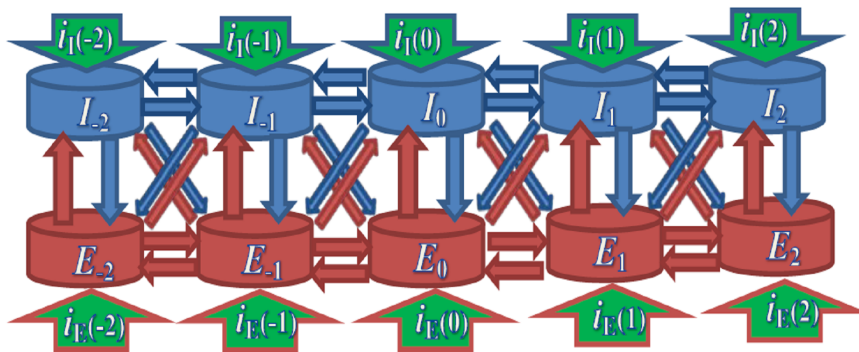


Figure 1. Generic circuit. An inhibitory-excitatory neuronal chain with nearest-neighbor coupling [21,22]. The arrows indicate excitatory (red) and inhibitory (blue) interactions between neurons, while currents $i_E(l)$ and $i_I(l)$ correspond to the inputs into each node generated by the stimulus.

whether the network is one- or two-dimensional or whether it is fractal) than on the finer detail of local circuitry: the "node" of the network. To illustrate basic principles of neural-wave interference, here we consider a simple model: a chain of inhibition-excitation nodes with nearest-neighbor interactions (Fig. 1). We use the Wilson-Cowan model [22] because even a single-node version of it (which consists of one excitatory cell and one inhibitory cell) has proven useful for understanding behavior of small cortical circuits [23], and its rich dynamical properties [24] have been helpful in studies of large-scale neural phenomena [25,26].

Consider a nearest-neighbor chain of Wilson-Cowan nodes [22]:

$$\begin{aligned}\tau_E \frac{dr_E(l)}{dt} &= -r_E(l) + g(\mathcal{W}_E) \\ \frac{dr_I(l)}{dt} &= -r_I(l) + g(\mathcal{W}_I),\end{aligned}\tag{1}$$

where

$$\begin{aligned}\mathcal{W}_E &= w_{EE}r_E(l) + \tilde{w}_{EE}r_E(l+1) + \tilde{w}_{EE}r_E(l-1) \\ &- w_{EI}r_I(l) - \tilde{w}_{EI}r_I(l+1) - \tilde{w}_{EI}r_I(l-1) + i_E(l),\end{aligned}\tag{2}$$

$$\begin{aligned}\mathcal{W}_I &= w_{IE}r_E(l) + \tilde{w}_{IE}r_E(l+1) + \tilde{w}_{IE}r_E(l-1) \\ &- w_{II}r_I(l) - \tilde{w}_{II}r_I(l+1) - \tilde{w}_{II}r_I(l-1) + i_I(l),\end{aligned}\tag{3}$$

and where l is the number (or, equivalently, the discrete spatial coordinate) of an excitatory-inhibitory node in the chain (Fig. 1). Variables $r_E(l)$ and $r_I(l)$ are the firing rates of the excitatory and inhibitory cells at node l , respectively, and τ_E is the characteristic time of excitatory cells (while time is normalized on the characteristic time of the inhibitory cells). Coefficients w_{EE} , w_{EI} , w_{IE} and w_{II} describe the interactions of the excitatory and inhibitory cells within every node (as in [23]), and \tilde{w}_{EE} , \tilde{w}_{EI} , \tilde{w}_{IE} , \tilde{w}_{II} represent the strength of coupling between the nearest nodes. Inputs $i_E(l)$ and $i_I(l)$ of the excitatory and inhibitory cells are provided by the optical stimulation, while input ratio $i_E(l)/i_I(l) = \alpha$ is the same for all the nodes (although it could be modeled as an additional parameter). Below we focus on the linear regime of this system, where sigmoid function g is approximated by $g(x) \approx x$. In other words, we consider the following equations:

$$\begin{aligned}\tau_E \frac{dr_E(l)}{dt} &= -r_E(l) + \mathcal{W}_E \\ \frac{dr_I(l)}{dt} &= -r_I(l) + \mathcal{W}_I.\end{aligned}\tag{4}$$

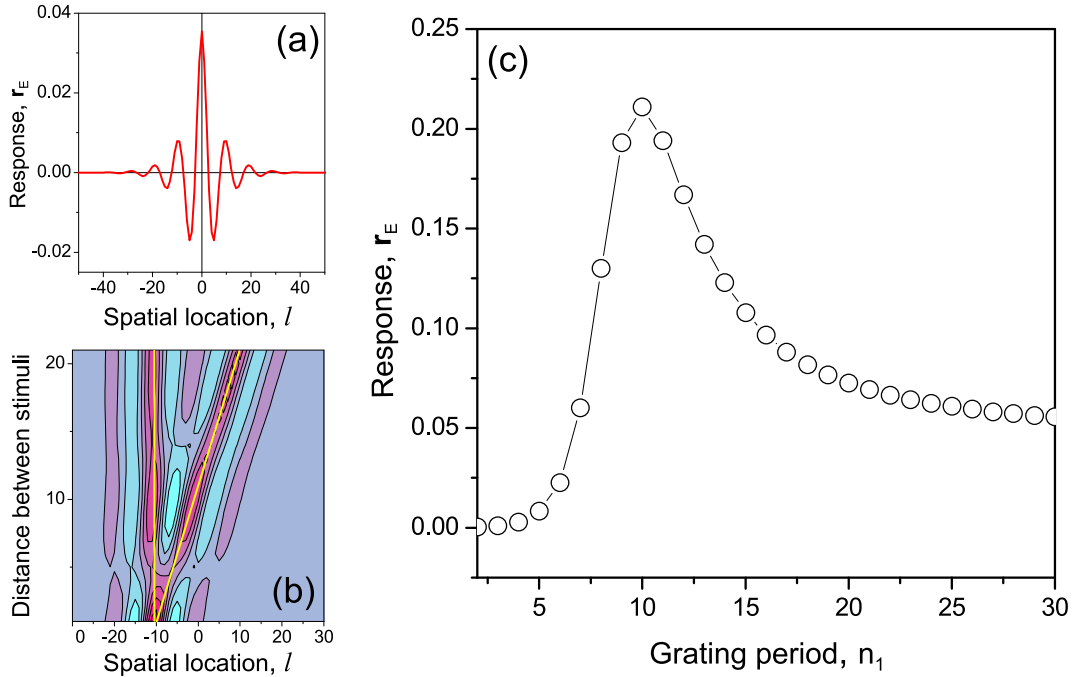


Figure 2. Spatial interference. **(a)** Stationary response $r_E(l)$ to a static point stimulus, where $i_E(0) = \alpha j$ and $i_I(0) = (1 - \alpha)j$ with $\alpha = 0.8, j = 0.01$ and chain parameters $\tau_E = 4, w_{EE} = 2, w_{IE} = 1.5, \tilde{w}_{EE} = \tilde{w}_{IE} = \tilde{w}_{EI} = 1, \tilde{w}_{II} = 0.7$ (i.e., $\mathcal{K} = -1.2$), $\mathcal{T} = -0.8, \mathcal{M} = 0.01$. Chain length was 200 nodes. The simulation time required to reach a stationary regime was 10,000 with time step $dt = 0.0001$. **(b)** Map of responses $r_E(l)$ across location l for different distances l_1 and l_2 between two static point stimuli $i_E(l_1) = i_E(l_2) = \alpha j$ and $i_I(l_1) = i_I(l_2) = (1 - \alpha)j$, with all other currents set to zero. All the other parameters were as in (a). Different rows of the map represent different simulations. The two yellow lines mark stimulus locations across the simulations. Because of the neural wave interference, the middle point between the stimuli is either facilitated (warm colors) or suppressed (cool colors), depending on the inter-stimulus distance and the spatial period of the excitation wave. **(c)** Response $r_E(0)$ at the center of a "Gabor patch" stimulus plotted as a function of stimulus spatial period n_1 , with all chain parameters as in (a) and stimulus parameters in (14) set to $n_0 = 25$ and $j_0 = 0.0005$.

3. Analysis of stability

We begin by analyzing the stability of the linearized equations, since a similar analysis of two coupled equations for a single node has been helpful for understanding the dynamical regimes observed in local circuits: pairs of coupled excitatory and inhibitory cells [24]. Consider a perturbation around the solution $r_E(t, l) = r_I(t, l) = 0$ at zero inputs $i_E = i_I = 0$. In contrast to the single-node configuration [24], we must take into account the spatial dependence of the perturbations, namely

$$\begin{aligned} r_E &= \Delta_E e^{\lambda t + ikl} \\ r_I &= \Delta_I e^{\lambda t + ikl} \end{aligned} \quad (5)$$

with constant amplitudes Δ_E and Δ_I , wave number k , and temporal rate λ . By substituting (5) in the linearized equations (1) we observe:

$$\begin{aligned}(w_{EE} + 2\tilde{w}_{EE} \cos k - 1 - \tau_E \lambda)\Delta_E - (w_{EI} + 2\tilde{w}_{EI} \cos k)\Delta_I &= 0, \\ (w_{IE} + 2\tilde{w}_{IE} \cos k)\Delta_E - (w_{II} + 2\tilde{w}_{II} \cos k + 1 + \lambda)\Delta_I &= 0.\end{aligned}\quad (6)$$

This algebraic set has a solution if

$$\lambda_{\pm} = \frac{\bar{W}_{EE} - 1 - \tau_E \bar{W}_{II} - \tau_E \pm \sqrt{\mathcal{A}}}{2\tau_E}, \quad (7)$$

where

$$\mathcal{A} = (\bar{W}_{EE} - 1 - \tau_E \bar{W}_{II} - \tau_E)^2 - 4\tau_E [(\bar{W}_{II} + 1)(1 - \bar{W}_{EE}) + \bar{W}_{EI}\bar{W}_{IE}], \quad (8)$$

with

$$\bar{W}_s = w_s + 2\tilde{w}_s \cos k,$$

and index s is EE, EI, IE, II . Note that results of [24] follow when all values of \tilde{w}_s are zero.

Stability of the neural chain requires that $\text{Re}\lambda_{\pm}(k) < 0$ for all k , resulting in conditions

$$\begin{aligned}w_{EE} - 1 - \tau_E w_{II} - \tau_E + 2\mathcal{R} \cos k &< 0 \quad \text{and} \\ (w_{II} + 1)(1 - w_{EE}) + w_{EI}w_{IE} - \mathcal{K} \cos^2 k - 2\mathcal{K}\mathcal{T} \cos k &> 0,\end{aligned}\quad (9)$$

where

$$\mathcal{K} = 4(\tilde{w}_{II}\tilde{w}_{EE} - \tilde{w}_{EI}\tilde{w}_{IE}), \quad \mathcal{R} = \tilde{w}_{EE} - \tau_E \tilde{w}_{II}, \quad (10)$$

and

$$\mathcal{T} = (\tilde{w}_{EE}(w_{II} + 1) + \tilde{w}_{II}(w_{EE} - 1) - \tilde{w}_{EI}w_{IE} - \tilde{w}_{IE}w_{EI})/\mathcal{K}. \quad (11)$$

Since $|\cos k| < 1$, the first stability equation in (9) can be rewritten as

$$\mathcal{Q} = w_{EE} - 1 - \tau_E w_{II} - \tau_E + 2|\tilde{w}_{EE} - \tau_E \tilde{w}_{II}| < 0, \quad (12)$$

where the slowest decaying perturbation has $k \approx 0$ if $\mathcal{R} = \tilde{w}_{EE} - \tau_E \tilde{w}_{II} > 0$ or $k \approx \pi$ if $\mathcal{R} = \tilde{w}_{EE} - \tau_E \tilde{w}_{II} < 0$ for $\mathcal{A} < 0$.

In effect, if the chain is stimulated by a short pulse of current (a short-lived stimulus), the excitation with either $k \approx 0$ (all nodes oscillate "in-phase") or $k \approx \pi$ (all nodes oscillate "out of phase") can persist for some time, when $\mathcal{R} > 0$ or $\mathcal{R} < 0$, respectively, for $\mathcal{A} < 0$. This result is consistent with the numerical simulations illustrated in Fig. 3.

Analyzing the second stability condition in (9), we obtain parameter regions where the set of linearized equations (1) is stable. Namely, in addition to the constraint (4), the following conditions should be satisfied:

$$\begin{aligned}(w_{II} + 1)(1 - w_{EE}) + w_{EI}w_{IE} - \mathcal{K} + 2\mathcal{K}\mathcal{T} &> 0 \quad \text{if } \mathcal{K} > 0, \mathcal{T} < 0, \\ (w_{II} + 1)(1 - w_{EE}) + w_{EI}w_{IE} - \mathcal{K} - 2\mathcal{K}\mathcal{T} &> 0 \quad \text{if } \mathcal{K} > 0, \mathcal{T} > 0, \\ (w_{II} + 1)(1 - w_{EE}) + w_{EI}w_{IE} - \mathcal{K} + 2\mathcal{K}\mathcal{T} &> 0 \quad \text{if } \mathcal{K} < 0, \mathcal{T} > 1, \\ (w_{II} + 1)(1 - w_{EE}) + w_{EI}w_{IE} - \mathcal{K} - 2\mathcal{K}\mathcal{T} &> 0 \quad \text{if } \mathcal{K} < 0, \mathcal{T} < -1, \\ (w_{II} + 1)(1 - w_{EE}) + w_{EI}w_{IE} + \mathcal{K}\mathcal{T}^2 &> 0 \quad \text{if } \mathcal{K} < 0, -1 < \mathcal{T} < 1.\end{aligned}\quad (13)$$

Eq. (13) defines the regime of stabilization by inhibition, including the terms responsible for stabilization of individual nodes (the first additive terms in every row of (13)) and the terms responsible for stabilization of the chain. As mentioned, under null interactions between the nodes (i.e., under $\mathcal{K} = 0$, $\mathcal{KT} = 0$) we reproduce the results derived in [24].

In contrast to the single-node model, now the instability can occur over time by virtue of an exponential increase of spatial amplitudes $\Delta_E \exp(-\lambda(k)t)$ and $\Delta_I \exp(-\lambda(k)t)$ of waves $r_E(t, l)$ and $r_I(t, l)$ with different wave numbers k (i.e., spatial periods $2\pi/k$). This so-called *corrugation instability* is well known in physics, in particular in acoustics and hydrodynamics [1]. It arises because of mutual excitation of the nodes in the chain. If neither (4) nor (13) is satisfied, the solution $r_E(t, l) = r_I(t, l) = 0$ at $i_E(l) = i_I(l) = 0$ becomes unstable. In this case, the system can be attracted to another fixed point, or it can develop periodic, quasi-periodic, or chaotic oscillations. This behavior is different from the behavior of the single-node model [24]. Now the oscillations occur both in space and time, and they can be chaotic because of the mixing of oscillations with different wave numbers k (and thus different time scales $\lambda_{\pm}(k)$). In what follows, we focus on the interference of neural waves in stable regimes (4)–(13).

4. Parameters responsible for network behavior

To summarize, the preceding analysis of linearized equations (4), and the analysis of static responses of the network to point stimuli, helped to reveal the parameters that underlie qualitatively different classes of network behavior. These parameters are captured by the following coefficients:

$$\begin{aligned}\mathcal{K} &= 4(\tilde{w}_{II}\tilde{w}_{EE} - \tilde{w}_{EI}\tilde{w}_{IE}), \mathcal{R} = \tilde{w}_{EE} - \tau_E\tilde{w}_{II}, \\ \mathcal{T} &= (\tilde{w}_{EE}(w_{II} + 1) + \tilde{w}_{II}(w_{EE} - 1) - \tilde{w}_{EI}w_{IE} - \tilde{w}_{IE}w_{EI})/\mathcal{K}. \\ \mathcal{Q} &= w_{EE} - 1 - \tau_E w_{II} - \tau_E + 2|\tilde{w}_{EE} - \tau_E\tilde{w}_{II}| < 0, \\ \mathcal{M} &= (w_{II} + 1)(1 - w_{EE}) + w_{EI}w_{IE} + \mathcal{K}\mathcal{T}^2, \\ \tilde{k} &= \pm \arccos(-\mathcal{T}), \quad \kappa = \pm \sqrt{-\mathcal{M}/[\mathcal{K}(1 - \mathcal{T}^2)]}.\end{aligned}$$

Although this modeling framework employs a large overall number of parameters, all stationary solutions (the spatial distribution of network activity) are controlled by two quantities, \mathcal{T} and \mathcal{M}/\mathcal{K} , and the dynamical behavior of the network is additionally controlled by \mathcal{Q} and \mathcal{R} . In particular, \mathcal{T} determines whether the system has a purely decaying spatial response (for $|\mathcal{T}| > 1$) or it shows decaying oscillations (for $|\mathcal{T}| < 1$) with wave number \tilde{k} (e.g., Fig. 2). Ratio \mathcal{M}/\mathcal{K} defines the exponent of spatial decay (i.e., how fast the response decreases along the chain) away from the stimulus. Remarkably, when we choose different sets of parameters that correspond to the same magnitudes of \mathcal{T} and \mathcal{M}/\mathcal{K} , but different magnitudes of \mathcal{R} , the network produces nearly the same responses for lasting stimuli, and very different responses for short-lived stimuli (Fig. 3).

5. Spatial interference and intrinsic tuning

First, we consider the steady-state response $r_E(l)$ to a spatially localized static stimulus ("point stimulus")

$$i_E(l \neq 0) = i_I(l \neq 0) = 0, \quad i_E(0) = \alpha j, \quad i_I(0) = (1 - \alpha)j$$

with total current j applied to the zeroth node. Depending on parameters \mathcal{T} and \mathcal{M}/\mathcal{K} , the response will have the form of either spatial damped oscillations (Fig. 2a) or purely exponential spatial decay (not shown). For the regime of damped oscillations, the number of significant oscillations (i.e., oscillations whose amplitudes are comparable to those at the locus of stimulation) is controlled by ratio \tilde{k}/κ and it can be readily estimated using parameters \mathcal{T} , \mathcal{M} and \mathcal{K} .

Applying two point stimuli, for which $i_E(l) = i_I(l) = 0$ for any l except l_1 and l_2 , with

$$i_E(l_1) = i_E(l_2) = \alpha j, \quad i_I(l_1) = i_I(l_2) = (1 - \alpha)j,$$

we obtain an interference of two "static waves" generated by the two stimuli. Depending on distance $l_1 - l_2$ between the stimuli, we obtain different interference responses $r_E(l)$, displayed in Fig. 2b as a map in which the rows correspond to the simulations with different distances $l_1 - l_2$.

Fig. 2b reveals that the response at the middle position $l = (l_1 + l_2)/2$ between the point stimuli could be either facilitated (warm colors) or suppressed (cool colors). These results suggest a new interpretative framework for the experimental studies of visual sensitivity with different spatial arrangements of local stimuli, such as strings [9] or rings [10] of Gabor patches, which had revealed strong modulations of sensitivity between stimulus locations.

Next, consider the pattern of neuronal interference created by a spatially extended stimulus, such as the commonly used "Gabor patch"

$$j(l) = j_0 \cos(2\pi l/n_1) \exp(-l^2/n_0^2) \quad (14)$$

with spatial period n_1 , Gaussian width n_0 , and amplitude j_0 . As we show in Fig. 2c, spatial period n_1 affects the response at the location of the strongest excitation $r_E(l = 0)$. As spatial period n_1 increases, the response first increases, reaches a maximum, and then decreases. This effect can be interpreted as a constructive interference of neural waves. The maximal response $r_E(l = 0, n_1)$ is reached when the periodicity of the stimulus matches the periodicity of the neural wave. In other words, the maximal response of the network is attained when a stimulus evokes oscillations whose period coincides with the period of the stimulus. (This period of oscillation may be called "intrinsic" or "natural" period of the network.)

Notably, the effect of inter-stimulus distance on the pattern of facilitation and suppression arises here from the nearest-neighbor interactions alone, requiring no long-range interactions between neurons

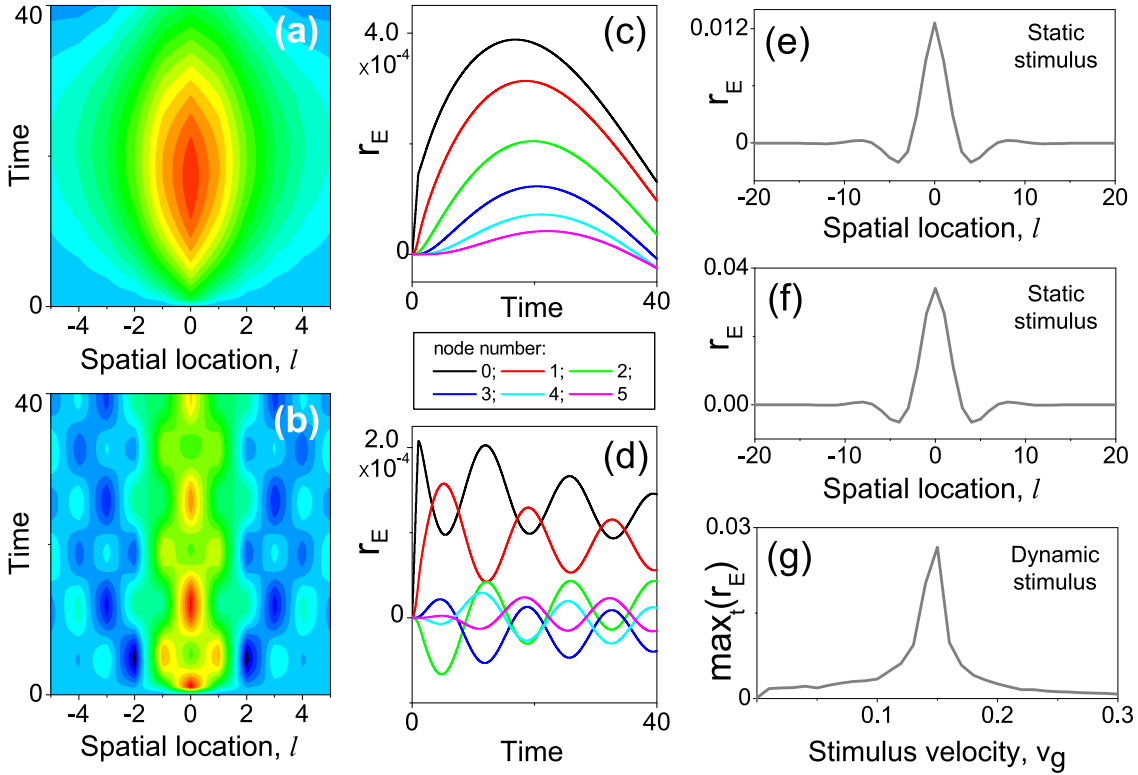


Figure 3. Spatiotemporal interference. **(a-b)** A map of spatiotemporal response $r_E(t, l)$ to short-lived point stimulus. The abscissa is spatial coordinate l and the ordinate is time t after stimulus onset, $r_E(0, i) = r_I(0, i) = 0$. The red, cyan, and blue regions represent highly positive, near zero, and highly negative values of r_E respectively. [Chain length was 200 nodes. Other chain parameters were $i_E(t, l) = i_I(t, l) = 0$ for all $l \neq 0$; $i_E(t < t_{\text{stim}}, 0) = \alpha j$, $i_I(t < t_{\text{stim}}, 0) = (1 - \alpha)j$ and $i_E(t > t_{\text{stim}}, 0) = 0$, $i_I(t > t_{\text{stim}}, 0) = 0$, and $w_{EE} = 2$, $w_{IE} = 1.5$, $\mathcal{M} = 0.01$, $\mathcal{Q} = -0.01$, $\mathcal{T} = -0.8$, $\mathcal{K} = -0.1$, $\alpha = 0.8$ for both (a) and (b), where $\mathcal{R} = 1$ (a), $\tilde{w}_{EE} = 1.3$ (a), $\tilde{w}_{IE} = 1.7$ (a) and $\mathcal{R} = -1$ (b) $\tilde{w}_{EE} = 1.5$ (b), $\tilde{w}_{IE} = 1.6$ (b). Simulation time was 40, and the time step was $dt = 10^{-6}$. Stimulus duration was 1 and stimulus intensity was $j = 4 \times 10^{-4}$.] **(c-d)** Results of the simulations as in (a) and (b), respectively, now displaying functions $r_E(t, 0), r_E(t, 1) \dots r_E(t, 5)$. The nodes oscillate in phase when $\mathcal{R} > 0$ and out of phase when $\mathcal{R} < 0$. **(e-f)** Steady-state responses for a static point stimulus $i_E(t, l) = i_I(t, l) = 0$ and $i_E(t, 0) = \alpha j$, $i_I(t, 0) = (1 - \alpha)j$ for the same chain parameters as in (a) and (b), respectively. (Stimulus intensity was $j = 4 \times 10^{-4}$.) Although chain responses to short-lived and lasting stimuli differ (because of the different signs of \mathcal{R}), the steady-state responses are nearly identical, except for a slightly different amplitude $r_E(l = 0)$ (since the steady-state response is controlled only by $\mathcal{T}, \mathcal{M}, \mathcal{K}$). **(g)** Maximal response $\max_t[r_E(t, l = 0)]$ over the entire observation period on the central node for a drifting Gabor patch (15) with parameters $n_1 = 2$, $n_0 = 20$, $j_0 = 0.0005$. The response is stronger than for static stimuli ($v_g = 0$).

6. Spatiotemporal interference

Next, we briefly consider the spatiotemporal interference that arises in the network when the stimuli appear at different locations and at different temporal instants. These conditions commonly occur in

the studies that use short-lived and moving stimuli, where the latter may be equivalently described as sequential presentation of a short-lived stimulus at spatially adjacent locations.

The time course of chain response $r(l)$ after extinguishing the stimulus has the form of either a purely exponential temporal decay or a damped temporal oscillation. Here we focus on the response regime of temporal oscillation, which is similar to the response regime found in biological vision [13,14].

We simulated a short-lived point excitation with $i_E(t, l) = i_I(t, l) = 0$ for all t and l except $l = 0, t < t_{\text{stim}}$ when

$$i_E(t < t_{\text{stim}}, l = 0) = \alpha j, i_I(t < t_{\text{stim}}, l = 0) = (1 - \alpha)j.$$

For $\mathcal{R} > 0$, the slowest decaying response under $t > t_{\text{stim}}$ corresponds to the case, where all the nodes respond in phase (Fig. 3a,c) and the wave of neural excitation propagates with a very high velocity.

Interestingly, the maximum excitation at $r_E(t, l = 0)$ is reached long after extinguishing the stimulus. (In Fig. 3, the stimulus was turned off at $t = 1$ whereas r_E reached its maximum at $t = 20$.) Such response delays must be taken into account in the studies that use rapidly alternating or short-lived stimuli [27].

In case of $\mathcal{R} < 0$, a long decay occurs for a fast spatial oscillating mode, resulting in out-of-phase oscillations in the neighboring neurons (Fig. 3b,d) and yielding a well-defined velocity of the neural wave. This makes the shape of the neural wave more complicated than in the case of $\mathcal{R} > 0$, forming multiple regions of facilitation and suppression in the $l - t$ map (Fig. 3b) even for a single short pulse of stimulation. We therefore expect that different stimuli (not shown) will generate non-trivial interference patterns. For example, consider network response to a dynamic stimulus, a drifting Gabor patch:

$$j(l) = j_0 \cos(2\pi(l - v_g t/n_1)) \exp(-l^2/n_0^2). \quad (15)$$

The well-defined velocity of the wave for $\mathcal{R} < 0$ suggests that the interference pattern will generate clear maxima of $r_E(l)$ when the stimulus moves with the same velocity as the intrinsic ("natural") velocity of the neural wave. This result agrees with the numerical stimulations illustrated in Fig. 3g, and it suggests a simple neural mechanism for tuning the sensory system to stimulus velocity, as a special case of spatiotemporal neural-wave interference, making unnecessary the assumption of specialized neural circuits for sensing velocity (*cf.* [19,20]). Notably, and in spite of the very different spatiotemporal responses of the system to short-lived stimuli (Fig. 3a,b), responses to static stimuli for $\mathcal{R} > 0$ and $\mathcal{R} < 0$ are similar to one another (Fig. 3e,f). This is because the steady-state response of the network is fully determined by terms \mathcal{K} , \mathcal{T} and \mathcal{M} .

7. Conclusions

We have analyzed interference of the neural waves propagating through an inhibitory-excitatory neural chain with nearest-neighbor coupling. First, we defined the region of stability of the corresponding linearized coupled equations with respect to corrugation perturbations, and then derived the combinations of parameters responsible for the shape of neural waves generated by static and short-lived stimuli. We found that the interference patterns generated in this network have three properties commonly

observed in biological vision: (1) selectivity for to spatial and temporal frequencies of stimulus intensity modulation, (2) selectivity for stimulus velocity, and (3) "lateral interactions" between spatially separate stimuli. It is plausible that neural wave interference is responsible for some of the basic visual phenomena that had been attributed to specialized neural circuits [9–11,19,20].

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