

Materials 3D Printed via fused deposition modelling elicit myofibrillar alignment and enhanced differentiation of skeletal muscle cells *in-vitro*

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INTRODUCTION: 3D printing allows the generation of physical devices within short time-periods from bespoke CAD designs. 3D printing technologies such as selective laser sintering (LS) and stereolithography (SL) are now being utilised within biomedical engineering for the fabrication of microfluidic devices¹ and scaffolds for living cells², using what is hoped are biodegradable and biocompatible 3D printed materials. If these technologies are going to form the platforms within which complex cellular physiological processes are to be re-created then understanding and defining the compatibility between various mammalian cell types and the printed materials is of paramount importance. This investigation sought to examine the biocompatibility of C₂C₁₂ muscle cells on commercially available polymers; poly-lactic acid (PLA), acrylonitrile butadiene styrene (ABS), polyethylene terephthalate (PET) and polycarbonate (PC) when 3D printed via FDM.

METHODS: Biocompatibility experiments were designed to simultaneously assess both the direct (cells cultured directly on the material) and indirect (cells cultured in chemically leached medium) effects of each polymer on cellular viability, morphology and differentiation after 3 days in GM (GM72hrs) and 5 days in DM (DM120hrs). C₂C₁₂ muscle precursor cells (MPCs) were seeded into eight six-well plates at a density of 6x10⁵ cells for each repeat (n=3). Each well/six-well plate was considered n=1 per condition (Control & Material), per analysis at each time-point totaling n=18 per analyses. This protocol was completed separately for each polymer (PLA, ABS, PET and PC). After alamarBlue® cellular viability analysis was conducted, cells were stained for the actin cytoskeleton and nucleic DNA in addition to being harvested for PCR assays.

RESULTS: Polymer dependent reductions in cell viability were observed when cultured directly on 3D printed materials (GM72hrs: PLA; P≤0.05, PC; P≥0.05, DM120hrs: PLA; P≤0.05, PC; P≤0.05). Cells cultured on PET also showed reduced viability (P≤0.05); however this was not evident in cells cultured on ABS (P≥0.05). In-direct observations outlined increases in cell viability when cultured in leached constituents of PLA after DM120 (P≤0.05) and ABS after GM72

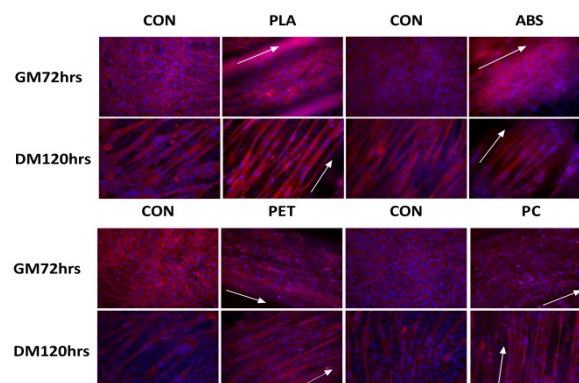


Fig.1: Morphological staining of the actin cytoskeleton (red) & nucleic DNA (blue) for PLA, ABS, PET, PC and respective controls at GM72 & DM120 time-points.

(P≤0.05), however this was not evident in PET (P≥0.05) or PC (P≥0.05).

Morphological observations (Fig.1) outlined reduced myotube widths in cells cultured on PLA (P≤0.0001), PC (P≤0.05) and PET (P≤0.0001) however this was not apparent in ABS (P≥0.05). Thinner myotubes were observed in cells cultured in chemical leachate of ABS (P≤0.05), however no difference was observed between other in-direct conditions. C₂C₁₂ cultured on 3D printed materials also exhibited significant nucleic (PLA; P≤0.0001, ABS; P≤0.05, PET; P≤0.05, PC; P≤0.0001) and myofibrillar alignment (PLA; P≤0.0001, ABS; P≤0.05, PET; P≤0.05, PC; P≤0.0001).

Augmented myogenin ΔC_T expression was documented at early time-points; GM72 in PLA (P≤0.0001), ABS (P≤0.05) and PC (P≤0.0001), however this was not observed in PET (P≥0.05). Myogenin remained potentiated after DM120 in PLA (P≤0.05), however this response was reduced in ABS (P≥0.05), PET (P≥0.05) and PC (P≥0.05). No difference was observed in cells cultured in the leached medium of materials.

DISCUSSION & CONCLUSIONS: This investigation observed biocompatible polymers 3D printed via FDM which exhibit morphological alignment and enhanced differentiation of C₂C₁₂ cells, providing rationale for use when re-creating platforms for cellular physiological processes.

REFERENCES: ¹Kitson, P.J. et al., 2012. *Lab on a Chip*, 12(18), p.3267. ²Lantada, A.D. et al., 2012. *Plasma Processes and Polymers*, 9(1), pp.98–107.