

Functionalization and characterization of magnetic nanoparticles for the detection of ferritin accumulation in Alzheimer's disease

Tamara Fernández, Alberto Martínez-Serrano, Lorena Cussó, Manuel Desco, and Milagros Ramos-Gómez

ACS Chem. Neurosci., **Just Accepted Manuscript** • DOI: 10.1021/acschemneuro.7b00260 • Publication Date (Web): 03 Jan 2018

Downloaded from <http://pubs.acs.org> on January 17, 2018

Just Accepted

“Just Accepted” manuscripts have been peer-reviewed and accepted for publication. They are posted online prior to technical editing, formatting for publication and author proofing. The American Chemical Society provides “Just Accepted” as a free service to the research community to expedite the dissemination of scientific material as soon as possible after acceptance. “Just Accepted” manuscripts appear in full in PDF format accompanied by an HTML abstract. “Just Accepted” manuscripts have been fully peer reviewed, but should not be considered the official version of record. They are accessible to all readers and citable by the Digital Object Identifier (DOI®). “Just Accepted” is an optional service offered to authors. Therefore, the “Just Accepted” Web site may not include all articles that will be published in the journal. After a manuscript is technically edited and formatted, it will be removed from the “Just Accepted” Web site and published as an ASAP article. Note that technical editing may introduce minor changes to the manuscript text and/or graphics which could affect content, and all legal disclaimers and ethical guidelines that apply to the journal pertain. ACS cannot be held responsible for errors or consequences arising from the use of information contained in these “Just Accepted” manuscripts.

1
2
3 **1 Functionalization and characterization of magnetic nanoparticles for**
4
5 **2 the detection of ferritin accumulation in Alzheimer's disease**
6
7

8
9 **3**
10
11 **4 Tamara Fernández¹, Alberto Martínez-Serrano², Lorena Cussó^{3,4,5}, Manuel**
12
13 **5 Desco^{3,4,5} and Milagros Ramos-Gómez^{1,6,*}**
14
15

16
17 6 1 Centre for Biomedical Technology (CTB), Universidad Politécnica de Madrid, Spain
18

19
20 7 2 Department of Molecular Biology and Centre for Molecular Biology “Severo Ochoa”
21
22 8 (CBMSO), Universidad Autónoma de Madrid and Consejo Superior de Investigaciones
23
24 9 Científicas, Madrid, Spain.
25

26
27 10 3 Departamento de Ingeniería Biomédica e Ingeniería Aeroespacial, Universidad Carlos
28
29 11 III de Madrid, 28911 Leganés, Spain.
30

31
32 12 4 Instituto de Investigación Sanitaria Gregorio Marañón, 28007 Madrid, Spain.
33

34
35 13 5 Centro de Investigación Biomédica en Red de Salud Mental (CIBERSAM), 28029
36
37 14 Madrid, Spain
38

39
40 15 6 CIBER de Bioingeniería, Biomateriales y Nanomedicina (CIBER-BBN), Madrid,
41
42 16 Spain.
43

44
45 17 *Corresponding author
46

47
48 18
49

50
51 19
52

53
54 20
55

56
57 21
58

1
2
3 1 **Abstract**
4

5 2 Early diagnosis in Alzheimer's disease (AD), prior to the appearance of marked clinical
6 3 symptoms, is critical to prevent irreversible neuronal damage and neural malfunction that leads
7 4 to dementia and death. Therefore, there is an urgent need to generate new contrast agents which
8 5 reveal by a non-invasive method the presence of some of the pathological signs of AD.
9
10
11
12

13
14 6 In the present study we demonstrate for the first time a new nanoconjugate composed of
15 7 magnetic nanoparticles bound to an anti-ferritin antibody, which has been developed based on
16 8 the existence of iron deposits and high levels of the ferritin protein present in areas with a high
17 9 accumulation of amyloid plaques (particularly the subiculum in the hippocampal area) in the
18 10 brain of a transgenic mouse model with five familial AD mutations.
19
20
21
22

23
24 11 Both in vitro and after intravenous injection, functionalized magnetic nanoparticles were able to
25 12 recognize and bind specifically to the ferritin protein accumulated in the subiculum area of the
26 13 AD transgenic mice.
27
28
29
30

31 14 **Keywords**
32
33

34 15 Iron oxide nanoparticles, nanoconjugates, ferritin, iron deposits, microglia, Alzheimer's disease.
35

36 16 **Introduction**
37
38

39 17 Alzheimer's disease (AD) is a progressive neurodegenerative disorder, with no known
40 18 prevention or cure, which affects approximately 47 million patients worldwide¹. At present, a
41 19 definitive diagnosis of AD is only possible after the patient's death, when the presence of
42 20 amyloid plaques and tangles in the brain parenchyma can be revealed by histological
43 21 examination². Current diagnostic practices, including assessments of clinical history to detect
44 22 changes in behavior, physical examination, neuropsychiatric testing (Mini-Mental State
45 23 Examination, MMSE), diagnostic laboratory tests and neuroimaging, can only make a
46 24 "probable" diagnosis of AD³.
47
48
49
50
51
52
53
54
55
56
57
58
59
60

1
2
3 1 To date, the best-established biomarkers for the detection and monitoring of AD include
4
5 2 measures of β amyloid peptide and tau in cerebrospinal fluid, hippocampal atrophy as assessed
6
7 3 by magnetic resonance imaging (MRI), reduction in the rate of glucose metabolism in the brain,
8
9 4 assessed by positron emission tomography (PET) with fluorodeoxyglucose, and brain
10
11 5 accumulation of β amyloid peptide visualized by PET using Pittsburgh Compound B^{3,4}. None of
12
13 6 these methods, alone or in combination, provide high accuracy in the early diagnosis of
14
15 7 pathology. Therefore, great emphasis has been placed on the search for biomarkers indicative of
16
17 8 AD, but most attempts to date have had limited success⁵.

18
19 9 With the improvements in imaging technologies in recent years, there has been a growing
20
21 10 interest in developing methods to visualize amyloid plaques in AD, especially in transgenic
22
23 11 mice, using methods that could eventually be applied to humans^{6,7}. The therapeutic approaches
24
25 12 currently developed show that the available therapies are more effective when applied at very
26
27 13 early stages, when a low burden of amyloid plaques can be detected^{8,9}. Therefore, early
28
29 14 diagnosis of the disease is a critical issue.

30
31 15 MRI has a higher spatial resolution than PET in the study of whole brain. MRI is a widely
32
33 16 available technique that can produce images in both experimental animals and in patients
34
35 17 without the need for a radiotracer¹⁰. Several groups have been able to visualize amyloid plaques
36
37 18 in vivo utilizing both the endogenous contrast induced by the plaques attributed to their iron
38
39 19 content and by selectively enhancing the signal from amyloid plaques using molecular-targeting
40
41 20 vectors labeled with MRI contrast agents^{11,12}. These data were corroborated using both
42
43 21 postmortem brain tissue from AD patients¹³, and brain tissue from transgenic AD mice^{14,15,16}.

44
45
46 22 Histological findings associated with AD show the presence of iron deposits in the vicinity of
47
48 23 plaques in the brains of patients with the disease^{17,18}. The intrinsic MRI contrast arising from the
49
50 24 iron associated with plaques creates an unexpected opportunity for the noninvasive investigation
51
52 25 of the temporal course of development of the plaques in the animal brain, thus reducing
53
54 26 intersubject variability¹⁶. However, the limiting factor of this methodological approach, in
55
56 27 which no contrast agent is used, is that only amyloid plaques with a diameter of more than 50

1
2
3 1 μm can be detected, using acquisition times that generally exceed 2h. These very long times
4
5 2 complicate the acquisition of in vivo images, not only in research animals, but also in the
6
7 3 clinical setting.

8
9 4 In order to detect amyloid plaques at early stages of the disease, and to diminish the acquisition
10
11 5 times of in vivo imaging, several studies have proposed the use of magnetic iron oxide
12
13 6 nanoparticles as specific contrast agents for MRI^{19, 20}. The hypointense effect exhibited by these
14
15 7 particles in T2 and T2* image sequences provides greater contrast in MR images. Therefore, the
16
17 8 use of magnetic iron oxide nanoparticles (MNPs) may be a good method for the early diagnosis
18
19 9 of AD.

20
21
22 10 Different types of functionalized MNPs have been evaluated in AD models including those
23
24 11 coupled to amyloid B peptide 1–40²¹, amyloid B peptide 1–30²², amyloid B peptide 1–42¹¹ and
25
26 12 to peptides highly specific for A β amyloid fibrils^{23, 24}; also by coupling the MNPs to antibodies
27
28 13 which specifically recognize amyloid B peptide 1–42 as a component of amyloid
29
30 14 plaques^{25, 26, 27, 19}. MNPs functionalized with different markers of amyloid plaques, such as
31
32 15 Thioflavin S²⁸, Congo Red²⁹, 1,1-dicyano-2-[6-(dimethylamino)naphthalene-2-yl] propene
33
34 16 (DDNP)³⁰ and curcumin³¹, have also been used to target and detect amyloid plaques in AD
35
36 17 transgenic mice using ex vivo MRI with long acquisition times.

37
38
39 18 The localized iron accumulation and formation of iron deposits in the brain, together with
40
41 19 changes in the regulation of iron-storage and the association of iron with several proteins is
42
43 20 evident in several neurodegenerative diseases, including AD^{32, 33}. Proteomic analysis has also
44
45 21 shown higher levels of ferritin, the main protein that stores and transports iron in vertebrates, in
46
47 22 the hippocampal region of AD patients compared to healthy individuals³⁴. Moreover, iron and
48
49 23 ferritin are deposited in close proximity to amyloid plaques in the cerebral cortex of AD
50
51 24 patients, as determined in post-mortem specimens^{35, 36}.

52
53 25 The present manuscript presents a novel nanoconjugate based on MNPs bound to an anti-ferritin
54
55 26 antibody, which could be a useful tool to detect increases in the expression of ferritin in the

1 brain parenchyma of transgenic mice with five familial Alzheimer's disease mutations
2 (5XFAD) by MRI³⁷. This nanoconjugate showed a high specific binding to the ferritin protein
3 present in the subiculum of 5XFAD mice after being injected intravenously, while non-
4 functionalized MNPs could not be detected in the same brain region after injection. The results
5 demonstrated that the functionalization of MNPs with the anti-ferritin antibody generated a
6 specific contrast agent useful for detecting the presence of ferritin in the brain parenchyma of
7 the 5XFAD mice, and consequently the presence of iron deposits in the vicinity of amyloid
8 plaques, one of the hallmarks of AD.

9 ***Results and Discussion***

10 We report here a novel method for the selective marking of the protein ferritin, present in areas
11 with a high accumulation of amyloid plaques, with functionalized magnetic nanoparticles. This
12 novel nanoconjugate, which selectively marked ferritin, might be used in the near future as a
13 contrast agent for MRI enabling the noninvasive early detection of AD.

14 The development of biofunctionalized devices could become a useful tool in diagnosis and
15 therapy of several neuropathologies and become a strategy to deepen knowledge in cell biology
16 and histopathology in neuroscience.

17 **Iron and ferritin accumulation in 5XFAD mice**

18 There is some evidence for altered iron metabolism in AD, including alterations in iron
19 accumulation and changes in transferrin and ferritin levels¹⁷. Striking iron accumulation has
20 been closely associated with amyloid plaques, neurofibrillary tangles, and neuropil threads in
21 clinical cases of AD³⁸. Increased levels of ferritin have also been observed by proteomic
22 analysis within the hippocampal region in AD patients compared to healthy individuals³⁴. To
23 determine whether these highly relevant histological findings were also present in 5XFAD mice,
24 the presence of iron was evaluated in 9-month-old 5XFAD transgenic and nontransgenic mice
25 by Prussian blue staining. Brain sections from nontransgenic mice showed no obvious Prussian
26 blue staining, indicating a lack of iron accumulation in the brain (Figure 1A). However, iron

1
2
3 1 burden was obvious in the subiculum of 5XFAD mice (Figure 1B), an area usually containing a
4 high number of amyloid plaques³⁷. In fact, when brain sections were stained with Thioflavin S,
5 a marker of amyloid plaques, a strong signal could be detected in the subiculum area only in the
6 5XFAD mice (Figure 1D), indicating a high density of amyloid plaques coinciding with the
7 strong accumulation of iron in this hippocampal region. As expected, amyloid protein was not
8 detected in nontransgenic mice (Figure 1C).

9
10 Since high iron content was observed in 5XFAD mice in the hippocampal area, we stained
11 similar brain sections with an anti-ferritin antibody to determine the levels of this iron-binding
12 protein in this region. While the presence of this protein in control mice was almost negligible
13 (Figure 1E), in 5XFAD brain sections, strong labeling for ferritin protein was evident in the
14 subiculum (Figure 1F).

15 This high expression of ferritin in the subiculum of the 5XFAD transgenic mice coincided
16 perfectly with the presence of a high number of amyloid plaques in the same area (arrows in
17 Figure 1D and 1F).

18 The regional accumulation of iron deposits in the brain, together with changes in the regulation
19 of iron storing proteins and the association of iron with neuropathology is evident in several
20 neurodegenerative diseases, including AD, Parkinson's disease, multiple sclerosis and
21 Huntington's disease, where the accumulation of iron in the brain corresponds to the regions of
22 greatest neuronal degeneration³⁹⁻⁴⁴. Iron accumulation in these neurodegenerative diseases
23 occurs in different brain regions. In AD, iron accumulation occurs in the hippocampus⁴⁰. In
24 Huntington's disease, an increased iron burden in the cortex and striatum has been shown in
25 both patients and transgenic mouse models for the disease⁴¹. In patients with Parkinson's
26 disease, accumulation of iron occurs in the substantia nigra⁴². In the case of multiple sclerosis,
27 an increase in iron in the spinal cord white matter has also been described⁴³. Therefore, a
specific contrast agent able to detect iron deposits by MRI could be useful for the diagnosis of
several neurodegenerative diseases. Furthermore, each neurodegenerative disorder could then be
distinguished by determining the brain area(s) where such iron accumulations occur. In this

1 way, the developed nanoconjugate would be a useful tool to detect AD, depending on the
2 location of the iron accumulations in the brain.

3 Iron deposits and a strong immunoreactivity for ferritin have been observed near the amyloid
4 plaques in the cortex and in the hippocampus of AD patients^{35, 36}. Ferritin accumulation was
5 almost exclusively associated with reactive microglial cells, which appeared to have greatly
6 proliferated³⁶. To determine if iron and ferritin accumulations in 5XFAD mice were deposited
7 close to the amyloid plaques, a double staining was performed using an antibody specific for the
8 ferritin protein and a specific marker for amyloid plaques (Thioflavin S). Cells labeled with the
9 anti-ferritin antibody were found near the amyloid plaques, with their processes in close contact
10 with and surrounding the plaques in 5XFAD brains (Figure 2). In brain slices obtained from AD
11 patients, astrocytes and microglia have been shown to be associated with the amyloid plaques,
12 where they show an activated, amoeboid state surrounding the plaques with their processes^{44,45}.
13 In the case of 5XFAD mice, staining with the astrocytic marker for glial fibrillary acidic protein
14 (GFAP) showed a high number of GFAP-positive cells throughout the subiculum with no
15 colocalization with ferritin positive cells (Figure 3C). However, the selective labeling of
16 microglial cells using tomato lectin, a protein with specific affinity for poly-N-acetyl
17 lactosamine sugar residues that are found on the plasma membrane and in the cytoplasm of
18 microglia, established a high colocalization of this marker with ferritin (Figure 3D). These
19 results indicate that microglial cells colocalized with ferritin and were abundant in areas
20 showing a high density of ferritin and amyloid plaques (Figures 3A and 3B, respectively).

21 Previous studies suggested that in the brain of patients with AD, the enhanced ferritin
22 expression indicated microglia degeneration instead of reflecting an activated state^{45, 46}. The
23 enhanced expression of ferritin protein has been described to increase the susceptibility of
24 microglia to degeneration, particularly in the aging brain⁴⁵. Senescent microglia may be less
25 efficient in maintaining iron homeostasis, and free iron could promote oxidative damage in
26 neurodegenerative diseases. Therefore, in brains affected by AD, increased expression of ferritin
27 could constitute a marker of microglial degeneration.

1
2
3 1 These results indicate that the increased presence of ferritin in AD brains could serve as an
4
5 2 interesting biomarker to reveal the presence and localization of amyloid plaques. Therefore,
6
7 3 conjugation of an anti-ferritin antibody with magnetic nanoparticles could produce a specific
8
9 4 contrast agent useful for noninvasively detecting the presence of amyloid plaques in the brain
10
11 5 using MRI.

6 **Coupling of the anti-ferritin antibody to MNPs**

7 An anti-ferritin polyclonal antibody was immobilized onto 50nm dextran-coated MNPs as
8
9 described in the methods section. A polyclonal antibody that recognizes multiple epitopes on
10
11 the same antigen was chosen due to its high affinity and tolerance to possible changes in the
12
13 antigen⁴⁷. The preparation of the nanoconjugates was based on the carbodiimide method⁴⁸,
14
15 leading to the formation of a very stable complex. The efficiency of the antibody binding to the
16
17 MNPs was determined by a dot-blot assay (Figure 4). Dot-blot analysis confirmed a high level
18
19 of anti-ferritin antibody binding to MNPs, since only small traces of free anti-ferritin antibody
20
21 were detected in the unbound fraction (Figure 4C); a high amount of anti-ferritin antibody
22
23 present at the beginning of the coupling reaction (Figure 4A) could be detected conjugated to
24
25 the MNPs in the MNPs-anti-ferritin fraction (Figure 4B) after the coupling reaction. Therefore,
26
27 the binding of the anti-ferritin antibody to the MNPs to form the MNP-anti-ferritin conjugate
28
29 was highly effective.

30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60
19 These previous results were also confirmed by protein quantification using an improved
20
21 Bradford protein assay permitting quantification of low protein concentrations⁴⁹. The binding
22
23 efficiency was estimated to be about 30 ± 14 molecules of anti-ferritin bound per nanoparticle.
24
25 Binding of the antibody to the MNPs may increase the final hydrodynamic diameter of the
26
27 MNPs as previously described for similar MNPs⁵⁰ in which the antibody bound to the MNPs
28
29 increased twofold their final hydrodynamic diameter.

25 **Cell viability after incubation with MNPs**

1
2
3 1 To discard a potential neurotoxicity of the MNPs, we determined that the incubation of human
4
5 2 neuroblastoma SH-SY5Y cells with MNPs and MNPs-anti-ferritin was feasible and did not
6
7 3 impair cell viability in vitro. SH-SY5Y cells were incubated with both types of MNPs and
8
9 4 tested for viability using doses up to 200 $\mu\text{g}/\text{mL}$ and incubation times of 72 hours, which did not
10
11 5 significantly affect neuroblastoma cells survival, as evaluated by the lactate dehydrogenase
12
13 6 (LDH) activity assay (Figure 5A). Once determined that MNPs did not induce a loss of cell
14
15 7 viability on SHSY5Y cell line, we analyzed the effect of MNP and MNPs-anti-ferritin on
16
17 8 primary cell cultures obtained from mouse brains, in order to discard an effect of the MNPs on
18
19 9 some specific type of brain cells (i.e.,neurons, astrocytes, or microglial cells). The results
20
21 10 showed that cell viability rates were similar in control and MNPs-treated cell cultures (Figure
22
23 11 5B) and that the number of neurons and astrocytes did not decrease in the presence of MNPs or
24
25 12 MNPs-anti-ferritin with respect to untreated control cells (Figure 5C). The number of microglia
26
27 13 cells stained with the anti-Iba1 antibody were higher in MNPs-treated cells compared to
28
29 14 untreated control cells (in which no microglial cells were detected), indicating that MNPs were
30
31 15 preferentially taken up by the microglial cells (Figure 5D), although the viability of the cells
32
33 16 during the periods of time analyzed was not affected.

34
35 17 These results suggested that although iron oxide nanoparticles could induce oxidative stress⁵¹,
36
37 18 the levels of intracellular iron accumulation resulting from the incubation with MNPs and the
38
39 19 presence of the antibody in the case of the nanoconjugate MNP-anti-ferritin, did not induce
40
41 20 acute cell toxicity at the times and concentrations analyzed. In addition, Mahmoudi and
42
43 21 coworkers⁵² have shown that the interaction of nanoparticles with serum proteins forming the
44
45 22 nanomaterial's protein corona inhibits the formation of A β fibril upon their entrance to the
46
47 23 biological medium.

24 **In vitro specificity of the MNP-anti-ferritin conjugate**

51
52 25 To verify the in vitro specificity of the MNP-anti-ferritin conjugate, fixed brain sections from 9-
53
54 26 month-old 5XFAD and nontransgenic mice, with a high (Figure 6A) and low (Figure 6E)
55
56 27 expression of ferritin, respectively, were incubated with the MNP-anti-ferritin conjugate. The

1
2
3 1 presence of the MNP-anti-ferritin conjugate bound to the subiculum in brain slices was detected
4
5 2 using an anti-rabbit-Cy3 antibody which recognized only the polyclonal ferritin antibody bound
6
7 3 to the MNPs. The results indicated a strong binding in the case of 5XFAD mice (Figure 6B and
8
9 4 6C) and a nearly absent, undistinguishable from background, binding in nontransgenic mice
10
11 5 (Figure 6F and 6G). The accumulation of MNPs in the slices could even be observed by
12
13 6 transmission light microscopy as highly localized and crowded black dots in 5XFAD (Figure
14
15 7 6D). This type of signal was undetectable in nontransgenic mice (Figure 6H).

16
17 8 As evidenced in Figure 6, the accumulation of the MNP-anti-ferritin conjugate in the subiculum
18
19 9 is higher in 5XFAD than in nontransgenic brain sections (compare Figure 6 B–D with panels F–
20
21 10 H). The binding of MNP-anti-ferritin conjugate colocalized with cells showing clear-cut, high
22
23 11 expression of ferritin in 5XFAD (Figure 6A) in comparison with nontransgenic (Figure 6E)
24
25 12 mice.

26
27
28 13 Also, the accumulation of bound MNP-anti-ferritin conjugate in the subiculum of 5XFAD mice
29
30 14 regionally correlates with the presence of amyloid plaques and ferritin in the subiculum,
31
32 15 previously shown in Figure 1D and 1F, respectively. As expected, in brain sections from
33
34 16 nontransgenic mice (Figure 6F–H), very few MNP-anti-ferritin nanoconjugate could be detected
35
36 17 (Figure 6G), and the black stain observed by transmission light microscopy was absent (Figure
37
38 18 6H), consistent with the very weak expression of ferritin in the subiculum of nontransgenic mice
39
40 19 (Figure 6E).

41
42 20 Consequently, these results indicated that the MNP-anti-ferritin conjugate specifically binds and
43
44 21 detects the enhanced expression of the ferritin protein that occurs in the subiculum of 9-month-
45
46 22 old 5XFAD mice *in vitro*.

47 48 49 23 **In vivo specificity of the MNP-anti-ferritin conjugate**

50
51 24 Once the *in vitro* specificity of the MNP-anti-ferritin nanoconjugate was confirmed in fixed
52
53 25 5XFAD brain sections, its efficiency was tested *in vivo* after intravenous injection in 5XFAD
54
55 26 mice. Since the previous *in vitro* results indicated the absence of detectable signal in control
56
57

1 animals, wild type mice were not used in these experiments to reduce the number of animals
2 used in adherence to the 3Rs principles. Plain non-functionalized MNPs and MNP-anti-ferritin
3 conjugates were intravenously injected into the retro-orbital sinus of 5XFAD mice. Six hours
4 after intravenous administration of the MNPs, 5XFAD brains were fixed and subsequently
5 analyzed by histological analyses to localize the final distribution of the MNPs. The
6 accumulation of ferritin protein and amyloid plaques in the subiculum of transgenic mice was
7 again confirmed using an anti-ferritin antibody and Thioflavin-S staining, respectively (Figure
8 7A). Serial sections were stained with the secondary polyclonal Cy3-antibody alone to detect
9 the presence of the MNP-anti-ferritin conjugates in the subiculum of 5XFAD mice previously
10 injected with the nanoconjugate (Figure 7B). Moreover, the MNPs were fluorescently labeled
11 using an antibody against their coating (antidextran-FITC; Figure 7D and 7G). The results
12 shown in Figure 7 demonstrate that the MNP-antiferritin nanoconjugates injected intravenously
13 accumulate in the subiculum area of the transgenic 5XFAD brains, where a high number of
14 amyloid plaques and an enhanced expression of ferritin exist (Figure 7A–E). In contrast, when
15 non-functionalized MNPs were injected intravenously in 5XFAD mice, only very few,
16 occasional, MNPs could be detected in the subiculum area (Figure 7 F–H), demonstrating a high
17 specificity of the MNP-anti-ferritin conjugates to reveal the accumulation of ferritin in the brain
18 of living 5XFAD mice. These results also indicated that non-functionalized MNPs did not bind
19 to 5XFAD brain parenchyma in a non-specific manner after intravenous injection,
20 demonstrating a lack of nonspecific binding of the non-functionalized MNPs to the iron deposits
21 found in the subiculum of 5XFAD mice. Moreover, the robust colocalization (Figure 7E) of the
22 ferritin antibody signal (Figure 7C) and the MNPs (Figure 7D) indicated that the MNP-anti-
23 ferritin nanoconjugate was highly stable under physiological in vivo conditions, avoiding
24 potential opsonization when circulating through the bloodstream and eluding clearance by the
25 reticuloendothelial system before reaching its target.

26 The ferritin protein also circulates in the plasma, where it transports iron. Ferritin in plasma has
27 been shown to enter the brain parenchyma through the blood brain barrier (BBB) using the

1 ferritin H receptor present on the plasma membrane of endothelial cells that form the BBB^{53,54}.
2 Therefore, a theoretical drawback of the present method would be that it might be possible that
3 plasmatic ferritin could saturate all the antibody recognition sites available on the MNPs, thus
4 preventing the binding of the nanoconjugate to the ferritin present in the brain parenchyma. This
5 would seriously limit the efficacy of the iron-ferritin detection method, and its potential use as a
6 diagnostic tool. Although we cannot exclude some binding to plasma ferritin, our results
7 indicate that the MNP-anti ferritin conjugate has enough free binding sites to recognize the
8 ferritin accumulated in the subiculum of 5XFAD mice.

9 Based on our results, we propose that the MNPs conjugated to anti-ferritin antibody could be a
10 useful tool for the imaging and detection of iron accumulations in the brain parenchyma of AD
11 patients. Future work will be needed to increase the binding capacity and affinity of the
12 nanoconjugate. A limitation of our method is the need to open the BBB with the use of
13 mannitol.

14 Although intravenous mannitol injection has been used safely in patients under a variety of
15 clinical settings⁵⁵, a potential future clinical use of this contrast agent would require further
16 modifications including the coupling of MNPs with specific proteins actively transported into
17 the brain²² or their PEGylation¹¹ in order to increase the ability of the MNPs to cross the BBB
18 and avoid the use of mannitol.

19 **Ex vivo brain MRI**

20 After confirming that MNP-anti-ferritin nanoconjugate injected intravenously specifically
21 bound to the subiculum region in transgenic 5XFAD brains, MR images from the same area
22 were acquired from a different set of experimental animals after the injection of non-
23 functionalized and functionalized MNPs as a preliminary study. Nontransgenic mice injected
24 with MNP-anti-ferritin and 5XFAD mice without MNPs did not show any non-specific marks in
25 MR images (data not shown). Although there were no evident marks on MR images of the
26 injected MNPs (Figure 8 A and 8B), a significant decrease in T2* value in both the right and

1 left hippocampus was found in 5XFAD animals injected with functionalized MNPs as
2 compared to 5XFAD mice injected with non-functionalized MNPs (Figure 8 C). Therefore,
3 changes in T2* value in MNP-anti-ferritin injected 5XFAD mice could be attributed to ferritin
4 accumulation and consequently to amyloid plaque deposition in the transgenic mice, as
5 previously demonstrated by histological analysis (Figure 7). Therefore, our results are consistent
6 with the literature. Yang et al⁵⁶ also reported a decrease of T2* value in the hippocampus after
7 nanoparticle administration in both in vivo and ex vivo MRI studies.

8 In order to increase the binding of the nanoconjugate MNPs-anti-ferritin to the transgenic mouse
9 brains, higher amounts of anti-ferritin antibody could be used for the coupling reaction.
10 Moreover, the dosage we used of MNP-anti-ferritin at 20 $\mu\text{mol Fe}_3\text{O}_4/\text{kg}$ body weight is far
11 from the range of preclinical MRI applications for which contrast agents are typically injected
12 intravenously by femoral or tail vein, at 200 $\mu\text{mol Fe}_3\text{O}_4/\text{kg}$ body weight for diagnostic
13 purposes^{11,29} and similar to the doses of commercial MNPs (i.e., Endorem[®], Resovist[®], or
14 Feridex[®]) used in clinical trials (15 $\mu\text{mol Fe}_3\text{O}_4/\text{kg}$ body weight). Therefore, since no
15 cytotoxicity of the MNPs used to synthesize the nanoconjugate was observed even at the highest
16 concentration used (Figure 5), a higher dose of MNPs could be injected in vivo to induce
17 qualitative changes on brain MRI allowing visual ferritin accumulation in the future.

18 The specificity of this nanoconjugate is important because, to date, the detection of iron deposits
19 associated with AD by MRI is only possible when a high concentration of iron is deposited
20 around the amyloid plaques¹², preventing early diagnosis of the disease. The use of contrast
21 agents like the one described here, based on MNPs functionalized with antibodies directed
22 against the protein that stores iron, would allow an earlier detection of the accumulation of
23 ferritin and, hence, of iron, as we have shown in the present work. This would allow an early
24 diagnosis of the disease, since the presence of iron deposits in the brains of patients with AD is
25 one of the most common histopathological features associated with the disease¹⁷. Iron is known
26 to promote aggregation of β -amyloid peptide and therefore a large number of therapeutic trials
27 are currently aimed at reducing elevated levels of iron in the brains of AD patients⁵⁷. Thus, an

1
2
3 1 effective method for early and sensitive detection of iron levels in the brains of AD patients is
4
5 2 necessary.

6
7 3 These preliminary results of detecting ferritin accumulation in 5XFAD mice show a potential
8
9 4 future high-specificity tool for diagnosis of Alzheimer's disease.

10 11 12 5 **Methods**

13 14 15 6 **Animals**

16
17 7 Hemizygous 5xFAD mice obtained from the Jackson Laboratory were used as a model of
18
19 8 Alzheimer's disease³⁷. These 5xFAD mice carry five mutations associated with familial AD
20
21 9 (Swedish (K670N, M671L), Florida (I716V) and London (V717I) mutations in amyloid
22
23 10 precursor protein (APP) and M146L and L286V mutations in presenilin 1 (PS1)) and develop
24
25 11 several features of AD described in humans, such as the presence of amyloid plaques, which
26
27 12 appear as early as 2 months of age in these mice³⁷. N=3 Nine month old male 5XFAD
28
29 13 transgenic mice and n= 3 their wild-type (nontransgenic) littermates were used for all
30
31 14 experiments as proof of concept to determine the specificity of the nanoconjugate. All
32
33 15 procedures involving the use of animals were reviewed and approved by the local Animal Care
34
35 16 Committee (Universidad Politécnica de Madrid) according to the guidelines of the European
36
37 17 Community (ECC/566/2015).

38 39 40 18 **Histological analysis**

41
42 19 5XFAD and nontransgenic mice (9-month old) were anesthetized with an overdose of chloral
43
44 20 hydrate and intracardially perfused with freshly prepared 4% paraformaldehyde (in 0.1 M
45
46 21 phosphate buffer, pH 7.4). Brains were removed, postfixed for 12 h in the same fixative at 4 °C,
47
48 22 and dehydrated in 30% sucrose solution at 4 °C until sunk. Thirty- μ m thick coronal sections
49
50 23 were collected using a freezing microtome (Leica SM 2400).

51
52
53 24 Prussian blue iron staining was used to visualize the iron deposits in the brain sections of
54
55 25 5XFAD and nontransgenic mice⁵⁸. A previous inactivation of endogenous peroxidase activity in

1 the tissue was performed by incubating the sections in 3% H₂O₂ and 10% methanol in
2 phosphate buffered saline (PBS); samples were maintained at room temperature in the dark with
3 shaking for 30 minutes. After rinsing with PBS, sections were incubated in the Prussian blue
4 solution (2% potassium ferrocyanide trihydrate (Sigma # P-3289), 2% HCl, 1% Triton X-100 in
5 distilled H₂O) for 30 minutes. Samples were then washed twice in distilled H₂O and treated with
6 a solution of Ni-DAB (5mg of 3, 3'-diaminobenzidine (Sigma), 35 μ L of 8% NiCl₂ and 4 μ L of
7 30% H₂O₂ in 10 mL of PBS) for 15 minutes. Sections were rinsed in PBS and mounted onto
8 gelatinized glass slides (Menzel-Glaser). The slides were dried overnight, successively
9 dehydrated with ethanol, delipidated with xylene and coverslipped with DPX mounting
10 medium.

11 Thioflavin S was used for the specific staining of amyloid plaques in brain sections from
12 5XFAD mice^{49, 59}. Brain sections from 5XFAD and nontransgenic mice were mounted onto
13 polylysine- treated slides (Thermo Scientific) and allowed to dry for 48h. Sections were then
14 incubated in 0.05% Thioflavin-S (Sigma) diluted in 50% ethanol for 30 minutes, protected from
15 light. After the incubation, sections were rinsed twice in 50% ethanol and once in distilled H₂O.
16 The slides were dried overnight and coverslipped with Mowiol mounting medium.

17 **Immunohistochemistry**

18 Thirty- μ m serial sections obtained from 5XFAD and nontransgenic mice were also assessed by
19 immunohistochemistry using a polyclonal antibody against ferritin (1:1000; Sigma) and a
20 monoclonal antibody against GFAP (1:1000; Sternberger). Briefly, free-floating sections were
21 incubated overnight at 4 °C with the primary antibodies diluted in PBS with 2% nonspecific
22 serum. Sections were rinsed four times in PBS for a total time of 1 h and then incubated for 2 h
23 with the secondary antibodies diluted in PBS (anti-mouse or anti-rabbit Cy3- conjugated
24 antibodies, 1:200, all from Jackson Immunoresearch). Streptavidin-FITC (1:300; Vector Labs)
25 was used to detect biotinylated Lectin (1:500; Sigma) for microglial cell staining. Brain sections
26 were mounted onto gelatinized glass slides (Menzel-Glaser). The slides were dried overnight
27 and coverslipped with Mowiol.

1 **Preparation of MNP-anti-ferritin nanoconjugate**

2 MNP-anti-ferritin conjugates were prepared according to the carbodiimide method⁴⁸. Briefly, 1
3 mg of 50nm in diameter Fe₃O₄-dextran coated MNPs with a magnetite content of 35% (w/w)
4 and functionalized with -COOH groups (Kisker # PMC-50) were washed with 0.1 M 2-(*N*-
5 morpholino)ethanesulfonic acid (MES) buffer at pH 5.5 and diluted to a final volume of 500 μ L
6 in MES buffer containing 20 mg of freshly prepared 1-ethyl-3-(3-dimethylaminopropyl)
7 carbodiimide (EDC) and 40 mg of sulfo-*N*-hydroxysuccinimide (NHS). The particles were
8 mixed on a shaker for 2 h at room temperature. After incubation, the particles were washed
9 twice with 1 mL MES buffer at pH 5.5 and the activated particles were resuspended in 0.5 mL
10 MES buffer at pH 5.5. Amine group-containing ligands (150 μ g of a polyclonal anti-ferritin
11 human antibody, Sigma-Aldrich Cat. No. F5012) were added to the activated particles and the
12 suspension was mixed on a shaker overnight at room temperature. The conjugate was washed
13 three times with 1 mL PBS, centrifuged each time at 5000 rpm for 5 minutes, resuspended in
14 0.5 mL of PBS, and kept at 4 °C until use.

15 **Dot-blot assay**

16 To test the efficiency of the coupling reaction of the anti-ferritin antibody to the MNPs, 1 μ L
17 drops of each solution used in the preparation of the MNP-anti-ferritin conjugate (anti-ferritin
18 antibody, MNPs alone, medium containing unbound anti-ferritin antibody, and MNP-anti-
19 ferritin conjugate) were deposited onto a nitrocellulose membrane strip (Bio-Rad). After drying
20 at room temperature, dot-blot was blocked for 1 hour at room temperature with 5% skim milk
21 in Tris-buffered saline (500 mM NaCl in 20 mM Tris, pH 7.4) containing 0.05% Tween 20
22 (TTBS) and then incubated with a goat anti-rabbit peroxidase-conjugated antibody (1:5000; Life
23 Technologies) for 1 hour at room temperature. Immunoreactivity was detected using the ECL
24 Western blotting detection system (Amersham Biosciences). In addition, protein concentrations
25 in the coupling reaction (total and unbound antibody) were determined by an improved
26 Bradford protein assay permitting quantification of low protein concentrations⁶⁰, in order to
27 confirm dot-blot results. The number of anti-ferritin molecules was calculated as previously

1
2
3 1 described⁶¹. In both assays, a control was performed to discard the precipitation of the antibody
4
5 2 during the coupling reaction.

6 7 3 **Cell viability assays**

8
9
10 4 Human neuroblastoma cells (SH-SY5Y; ECACC No. 94030304) were maintained in DMEM
11
12 5 medium supplemented with 10% heat-inactivated fetal bovine serum, 2mM L-glutamine,
13
14 6 0.1mM nonessential amino acids, 100U/mL penicillin and 100 mg/mL streptomycin (Life
15
16 7 Technologies). The cell line was maintained at 37°C in a humidified incubator of 5% CO₂: 95%
17
18 8 air and passaged twice per week. For the cell viability assay, cells were plated on 96 well plates
19
20 9 (15x10³ cells/well, in triplicate for each condition). Twenty four hours after plating, the cells
21
22 10 underwent treatment with MNPs and MNPs-anti-ferritin. Cell viability was evaluated 72 hours
23
24 11 after the incubation with the MNPs by the LDH assay, using the Cytotoxicity Detection kit
25
26 12 (Roche) and following the manufacturer's instructions. Briefly, after the incubation time with
27
28 13 the MNPs, cells were rinsed in PBS and lysed with 1% Triton X-100. Lysate was then collected
29
30 14 after centrifugation at 1500 rpm for 5 minutes to remove cell debris. Cell-free supernatants were
31
32 15 incubated with the kit's substrate mixture. LDH activity was determined in a coupled enzymatic
33
34 16 reaction; during this reaction, the tetrazolium salt is reduced to formazan. The formazan dye was
35
36 17 quantified spectrophotometrically at 490 nm. LDH activity present in the medium was
37
38 18 expressed as a percentage of the maximum activity, considering 100% of LDH activity released
39
40 19 to the medium as the absorbance obtained when control cells (cells without MNPs) were lysed
41
42 20 with 1% Triton X-100.

43
44 21 Cortical mixed neuronal and glial cell cultures were prepared from 18-day-old BCL56 embryos
45
46 22 as previously described⁶². Cerebral cortices were enzymatically dissociated in PBS containing
47
48 23 1% bovine serum albumin, 0.4 mg/ml papain, and 6 mM glucose. Dissociated cells were
49
50 24 collected by centrifugation (800 x g, 5 minutes) and resuspended in medium supplemented with
51
52 25 20% horse serum. Culture medium consisted of Neurobasal with 1% glutamax-I and B27
53
54 26 supplements (all from Gibco). The cells were then plated at 1x10⁵ cells/cm² on plastic plates
55
56 27 pretreated for 1 day with 10 mM poly-L-lysine and for 2 hours with laminin (1 mg/ml). The

1 medium was replaced after 1 day by Neurobasal with 1% glutamax-I and B27 supplements.
2
3
4 Two-thirds of the medium were replaced every second day. Cell cultures were maintained for 7
5
6 days and then MNPs and MNPs-anti-ferritin were added at 200 μ g/mL for 3 days. To visualize
7
8 the final location of MNPs in cortical cell cultures, red fluorescent MNPs (Chemicell nano-
9
10 screenMAG/R) were used (Figure 5D). Cells were then fixed in 4% paraformaldehyde and
11
12 immunofluorescence was performed using the following primary antibodies: anti- β -III-tubulin
13
14 (Sigma) to stain neurons, anti-GFAP (Sigma) to stain astrocytes, and anti-Iba-1 (Sigma) to label
15
16 microglial cells. Cell nuclei were counterstained with Hoechst 33258 (Molecular Probes). For
17
18 the cell viability assay, cells were plated on 96-well plates (15 x 10³ cells/well, in triplicate for
19
20 each condition). Twenty-four hours after plating, the cells underwent treatment with MNPs and
21
22 MNPs-anti-ferritin. Cell viability was evaluated 72 hours after the incubation with the MNPs by
23
24 using the Cell Proliferation Assay kit (AppliChem) following manufacturer instructions. This
25
26 employs 2,3-bis-(2-methoxy-4-nitro-5-sulfophenyl)-2H-tetrazolium-5-carboxanilide salt (XTT).
27
28 In living cells, mitochondria have the capability to reduce XTT to form an orange-colored,
29
30 water-soluble dye⁶³. Therefore, the concentration of this dye is proportional to the number of
31
32 metabolically active cells. The absorbance of each well was measured spectrophotometrically at
33
34 450 nm by using an ELX808 microplate reader (BioTeK).
35
36

37 **In vitro specificity of the MNP-anti-ferritin conjugate**

38
39 To test the specificity of MNP-anti-ferritin conjugates, 5XFAD and nontransgenic brain
40
41 sections were incubated with the MNP-anti-ferritin nanoconjugate (2 mg/mL). Sections were
42
43 then washed three times in PBS and incubated for 1 hour at room temperature with a goat anti
44
45 rabbit Cy3 antibody (1:200; Jackson Immunoresearch). Sections were then washed in PBS and
46
47 distilled water and mounted onto polylysine coated slides (Menzel-Glaser). The slides were
48
49 dried overnight and coverslipped with Mowiol.
50
51

52 **In vivo specificity of the MNP-anti-ferritin conjugate**

1
2
3 1 Mice were anesthetized with a mixture of isoflurane and oxygen (1.5% isoflurane per 1 L
4 oxygen) and homeothermy was maintained through a heated water blanket (TP 500 model,
5 Gaymar Industries, Inc, NY, USA) set at 37 °C. To facilitate the penetration of the MNPs
6 through the BBB, 100 μ L of a solution of mannitol (15% in PBS; Sigma) was injected into the
7 retro-orbital sinus. Then, 15 minutes later, 150 μ L (2 mg/mL) of plain MNPs or MNP anti-
8 ferritin conjugate were intravenously injected (approximately 200 μ g MNPs/mL blood) in the
9 same location⁶⁴. Six hours after injection of the MNPs, mice were intracardially perfused and
10 the brains were fixed as described in the histological analysis section. To identify the presence
11 of the MNP-anti-ferritin nanoconjugate, brain sections were incubated with a secondary anti-
12 rabbit Cy3 antibody (1:200; Jackson Immunoresearch). A monoclonal anti-dextran antibody
13 (1:500; Stem Cell Technologies) and a secondary anti-mouse FITC antibody (1:200; Jackson
14 Immunoresearch) were used to identify the magnetic nanoparticles.

15 **Ex vivo brain MRI**

16 Transgenic 5XFAD mice were injected with MNPs and MNP-anti-ferritin as described in the
17 previous section. Six hours after the injection, mice were transcardially perfused with PBS
18 followed by 4% PFA. After this process, brains were extracted and immersed in Fomblin
19 (Solvay Solexis Inc., Thorofare, NJ) in order to provide a completely dark background around
20 the brains being imaged. A Bruker 7T scanner Biospec 70/20 was used to perform
21 Multiplegradient echo 3D images with the following parameters: 98 μ m isotropic spatial
22 resolution, TR = 200 ms, matrix = 128 \times 128 \times 128, 10 echoes times (TE), first = 2.7 ms with
23 echo spacing (ES) = 3.57 ms, FA = 15°, imaging time = 5hours and 7minutes.

24 The apparent transverse relaxation time T2* was measured using the ten-echo train image sets
25 described above in several brain regions defined by region of interest (ROI). Right and left
26 dorsal hippocampus were manually drawn and T2* values were obtained using the
27 quantification tool of ParaVision 5.0 (Bruker, Germany).

28 **Optical microscopy**

1
2
3 1 Analyses and photography of Prussian blue or fluorescence stained samples were carried out
4
5 2 using an inverted Leica DMIRB microscope equipped with a digital camera (Leica DC100,
6
7 3 Nussloch, Germany). The confocal microscopy analysis was performed using a LSM 510
8
9 4 META confocal microscope coupled to an inverted microscope Axiovert200 (Zeiss) with image
10
11 5 capture software Zeiss ZEN 2008 sp2.

12 13 6 **Statistical analysis**

14
15
16 7 Results are presented as mean \pm S.E.M. of at least 3 independent experiments. The data were
17
18 8 analyzed by single factor analysis of variance followed by the post hoc Tukey's honestly
19
20 9 significant difference test. A significance level of $p < 0.05$ was chosen. STATISTICA software
21
22 10 (StatSoft, Tulsa, OK) was utilized for all statistical tests.

23 24 11 ***Safety***

25
26
27 12 Not applicable

28 29 13 ***Abbreviations***

30
31
32 14 AD: Alzheimer's disease

33
34
35 15 PET: positron emission tomography

36
37
38 16 MNPs: magnetic iron oxide nanoparticles

39
40
41 17 MRI: magnetic resonance imaging

42
43 18 5XFAD: transgenic mice model with five familial Alzheimer's disease mutations

44
45
46 19 PBS: phosphate buffered saline

47
48 20 GFAP: glial fibrillary acidic protein

49
50
51 21 LDH: lactate dehydrogenase

52
53 22 MES: 2-(N-morpholino) ethanesulfonic acid

54
55
56 23 BBB: blood brain barrier

1
2
3 1 DDNP: 1,1-dicyano-2-[6-(dimethylamino)naphthalene-2-yl] propene
4

5 2 ***Author Information***
6

7
8 3 *Corresponding autor
9

10 4 Milagros Ramos-Gómez*
11

12
13 5 Centre for Biomedical Technology (CTB), Universidad Politécnica de Madrid. Campus de
14

15 6 Montegancedo, Pozuelo de Alarcón, 28223 Madrid, Spain
16

17
18 7 *E-mail: milagros.ramos@ctb.upm.es
19

20
21 8 ***Author Contributions***
22

23 9 MRG and AMS conceived the study, participated in its design and coordination and drafted the
24
25 10 manuscript. TFC, LC and MD carried out all experimental studies and helped to draft the
26
27 11 manuscript.
28
29

30 12 ***Funding Sources***
31

32 13 This work was supported by Reina Sofia Foundation (to MRG). This study was also funded by
33
34 14 the Comunidad de Madrid (Neurotec-S2010/BMD-2460). Work at AMS laboratory was funded
35
36 15 by MINECO (SAF2010-17167 and SAF2014-56101-R), Comunidad de Madrid (Neurostem-
37
38 16 CM S2010-BMD-2336) and Instituto de Salud Carlos III (RETIC TerCel, RD12/0019/0013).
39
40 17 Work at MD laboratory was cofunded by FEDER "Una manera de hacer Europa" and the
41
42 18 Comunidad de Madrid (BRADE S2013/ICE-2958).
43
44

45 19 ***Conflict of Interest***
46

47
48 20 The authors declare that they have no competing interests.
49

50 21 ***Acknowledgment***
51
52
53
54
55
56
57
58
59
60

1 We would like to thank Beatriz Moreno and Soledad Martinez for the excellent technical
2 assistance. We thank Dr. R. Martínez (Cajal Institute, Madrid, Spain) for providing the Iba1
3 antibody.

4 **References**

5 (1) (2016) World Alzheimer Report 2016 Improving healthcare for people living with dementia
6 coverage, Quality and costs now and in the future.

7 (2) Apostolova, L. G., Hwang, K. S., Andrawis, J. P., Green, A. E., Babakchianian, S., Morra, J.
8 H., Cummings, J. L., Toga, A. W., Trojanowski, J. Q., Shaw, L. M., Jack, C. R., Petersen, R. C.,
9 Aisen, P. S., Jagust, W. J., Koeppe, R. A., Mathis, C. A., Weiner, M. W., and Thompson, P. M.
10 (2010) 3D PIB and CSF biomarker associations with hippocampal atrophy in ADNI subjects.

11 *Neurobiol. Aging* 31, 1284–1303.

12 (3) Smailagic, N., M, R. F., Ciapponi, A., Giannakou, A., Ol, P., X, B. C., and Cullum, S.

13 (2015) Mini-Mental State Examination (MMSE) for the detection of Alzheimer ' s disease and
14 other dementias in people with mild cognitive impairment (MCI) (Review). *Cochrane*
15 *Database Syst Rev* CD010783.

16 (4) Reiman, E. M., Quiroz, Y. T., Fleisher, A. S., Chen, K., Velez-Pardo, C., Jimenez-Del-Rio,
17 M., Fagan, A. M., Shah, A. R., Alvarez, S., Arbelaez, A., Giraldo, M., Acosta-Baena, N.,
18 Sperling, R. A., Dickerson, B., Stern, C. E., Tirado, V., Munoz, C., Reiman, R. A., Huentelman,
19 M. J., Alexander, G. E., Langbaum, J. B. S., Kosik, K. S., Tariot, P. N., and Lopera, F. (2012)
20 Brain imaging and fluid biomarker analysis in young adults at genetic risk for autosomal
21 dominant Alzheimer's disease in the presenilin 1 E280A kindred: A case-control study. *Lancet*
22 *Neurol.* 11, 1048–1056.

23 (5) Koffie, R. M., Farrar, C. T., Saidi, L.-J., William, C. M., Hyman, B. T., and Spires-Jones, T.
24 L. (2011) Nanoparticles enhance brain delivery of blood-brain barrier-impermeable probes for
25 in vivo optical and magnetic resonance imaging. *Proc. Natl. Acad. Sci.* 108, 18837–18842.

- 1
2
3 1 (6) Chamberlain, R., Wengenack, T. M., Poduslo, J. F., Garwood, M., and Jack, C. R. (2011)
4
5 2 Magnetic resonance imaging of amyloid plaques in transgenic mouse models of Alzheimer's
6
7 3 disease. *Curr. Med. Imaging Rev.* 7, 3–7.
8
9 4 (7) Baltes, C., Princz-Kranz, F., Rudin, M., and Mueggler, T. (2011) Detecting amyloid- β
10
11 5 plaques in Alzheimer's disease. *Methods Mol. Biol.* 711, 511–533.
12
13
14 6 (8) Wisniewski T, B. A. (2010) Vaccination as a therapeutic approach to Alzheimer's disease.
15
16 7 *Mt Sinai J Med* 77, 17–31.
17
18 8 (9) Thomas Wisniewskia, A. E. M. S. (2010) Murine models of Alzheimer's disease and their
19
20 9 use in developing immunotherapies. *Biochim Biophys Acta.* 1802, 847–859.
21
22
23 10 (10) Wadghiri, Y. Z., Sigurdsson, E. M., Sadowski, M., Elliott, J. I., Li, Y., Scholtzova, H.,
24
25 11 Tang, C. Y., Aguinaldo, G., Pappolla, M., Duff, K., Wisniewski, T., and Turnbull, D. H. (2003)
26
27 12 Detection of Alzheimer's amyloid in transgenic mice using magnetic resonance microimaging.
28
29 13 *Magn. Reson. Med.* 50, 293–302.
30
31
32 14 (11) Wadghiri, Y. Z., Li, J., Wang, J., Hoang, D. M., Sun, Y., Xu, H., Tsui, W., Li, Y.,
33
34 15 Boutajangout, A., Wang, A., de Leon, M., and Wisniewski, T. (2013) Detection of Amyloid
35
36 16 Plaques Targeted by Bifunctional USPIO in Alzheimer's Disease Transgenic Mice Using
37
38 17 Magnetic Resonance Microimaging. *PLoS One* 8, 1–10.
39
40 18 (12) Wadghiri YZ, Hoang DM, Wisniewski T, S. E. (2012) In vivo magnetic resonance imaging
41
42 19 of amyloid- β plaques in mice. *Methods Mol Biol* 849, 435–451.
43
44
45 20 (13) Benveniste, H., Einstein, G., Kim, K. R., Hulette, C., and Johnson, G. A. (1999) Detection
46
47 21 of neuritic plaques in Alzheimer's disease by magnetic resonance microscopy. *Proc. Natl. Acad.*
48
49 22 *Sci.* 96, 14079–14084.
50
51
52 23 (14) Braakman, N., Matysik, J., Van Duinen, S. G., Verbeek, F., Schliebs, R., de Groot, H. J.
53
54 24 M., and Alia, A. (2006) Longitudinal assessment of Alzheimer's beta-amyloid plaque
55
56 25 development in transgenic mice monitored by in vivo magnetic resonance microimaging. *J.*

- 1
2
3 1 *Magn. Reson. Imaging* 24, 530–536.
4
5
6 2 (15) Jack, C. R. (2005) In Vivo Magnetic Resonance Microimaging of Individual Amyloid
7
8 3 Plaques in Alzheimer’s Transgenic Mice. *J. Neurosci.* 25, 10041–10048.
9
10
11 4 (16) Vanhoutte, G., Dewachter, I., Borghgraef, P., Van Leuven, F., and Van Der Linden, A.
12
13 5 (2005) Noninvasive in vivo MRI detection of neuritic plaques associated with iron in
14
15 6 APP[V717I] transgenic mice, a model for Alzheimer’s disease. *Magn. Reson. Med.* 53, 607–
16
17 7 613.
18
19 8 (17) Connor, J. R., Menzies, S. L., Martin, S. M. S., and Mufson, E. J. (1992) A Histochemical
20
21 9 Study of Iron , Transferrin , and Ferritin in Alzheimer ’ s Diseased Brains. *J. Neurosci. Res.* 83,
22
23 10 75–83.
24
25 11 (18) Meadowcort, M. D., Connor, J. R., Smith, M. B., and Yang, Q. X. (2009) Magnetic
26
27 12 Resonance Imaging and Histological Analysis of Beta- Amyloid Plaques in Both Human
28
29 13 Alzheimer’s Disease and APP/ PS1 Transgenic Mice. *J Magn Reson Imaging* 29, 997–1007.
30
31
32 14 (19) Yang, C. C., Yang, S. Y., Chieh, J. J., Horng, H. E., Hong, C. Y., Yang, H. C., Chen, K. H.,
33
34 15 Shih, B. Y., Chen, T. F., and Chiu, M. J. (2011) Biofunctionalized magnetic nanoparticles for
35
36 16 specifically detecting biomarkers of Alzheimer’s disease in vitro. *ACS Chem. Neurosci.* 2, 500–
37
38 17 505.
39
40
41 18 (20) McLachlan, S. J., Morris, M. R., Lucas, M. A., Fisco, R. A., Eakins, M. N., Fowler, D. R.,
42
43 19 Scheetz, R. B., and Olukotun, A. Y. (1994) Phase I clinical evaluation of a new iron oxide MR
44
45 20 contrast agent. *J. Magn. Reson. Imaging* 4, 301–307.
46
47 21 (21) Wadghiri YZ, Sigurdsson EM, Wisniewski T, T. D. (2005) MR Imaging of amyloid
48
49 22 plaques in transgenic mice, in *Amyloid proteins: Methods and Protocols* (EM, S., Ed.), pp 365–
50
51 23 379. Humana Press Inc, Totowa, New Jersey.
52
53
54 24 (22) Sigurdsson, E. M., Wadghiri, Y. Z., Mosconi, L., Blind, J. A., Knudsen, E., Asuni, A.,
55
56 25 Scholtzova, H., Tsui, W. H., Li, Y., Sadowski, M., Turnbull, D. H., de Leon, M. J., and

- 1
2
3 1 Wisniewski, T. (2008) A non-toxic ligand for voxel-based MRI analysis of plaques in AD
4 transgenic mice. *Neurobiol. Aging* 29, 836–847.
5
6
7 3 (23) Plissonneau, M., Pansieri, J., Heinrich-Balard, L., Morfin, J.-F., Stransky-Heilkron, N.,
8 Rivory, P., Mowat, P., Dumoulin, M., Cohen, R., Allémann, É., Tóth, É., Saraiva, M. J., Louis,
9 C., Tillement, O., Forge, V., Lux, F., and Marquette, C. (2016) Gd-nanoparticles
10 functionalization with specific peptides for β -amyloid plaques targeting. *J. Nanobiotechnology*
11 14, 60.
12
13
14
15
16
17
18 8 (24) Ansciaux, E., Burtea, C., Laurent, S., Crombez, D., Nonclercq, D., Vander Elst, L., and
19 Muller, R. N. (2015) In vitro and in vivo characterization of several functionalized ultrasmall
20 particles of iron oxide, vectorized against amyloid plaques and potentially able to cross the
21 blood-brain barrier: Toward earlier diagnosis of Alzheimer's disease by molecular imag.
22 *Contrast Media Mol. Imaging* 10, 211–224.
23
24
25
26
27
28 13 (25) Poduslo JF, Hultman KL, Curran GL, Preboske GM, Chamberlain R, Marjańska M, et al.
29 (2011) Targeting vascular amyloid in arterioles of Alzheimer disease transgenic mice with
30 amyloid β protein antibody-coated nanoparticles. *J Neuropathol Exp Neurol* 70, 653–661.
31
32
33
34
35 16 (26) Jaruszewski, K. M., Curran, G. L., Swaminathan, S. K., Rosenberg, J. T., Grant, S. C.,
36 Ramakrishnan, S., Lowe, V. J., Poduslo, J. F., and Kandimalla, K. K. (2014) Multimodal
37 Nanoprobes to target cerebrovascular amyloid in Alzheimer's disease brain. *Biomaterials* 35,
38 1967–1976.
39
40
41
42
43 20 (27) Yin, Z., Yu, T., and Xu, Y. (2015) Preparation of Amyloid Immuno-Nanoparticles as
44 Potential MRI Contrast Agents for Alzheimer's Disease Diagnosis. *J. Nanosci. Nanotechnol.*
45 15, 6429–6434.
46
47
48
49
50 23 (28) Siegemund, T., Paulke, B. R., Schmiedel, H., Bordag, N., Hoffmann, A., Harkany, T.,
51 Tanila, H., Kacza, J., and Härtig, W. (2006) Thioflavins released from nanoparticles target
52 fibrillar amyloid β in the hippocampus of APP/PS1 transgenic mice. *Int. J. Dev. Neurosci.* 24,
53 195–201.
54
55
56
57
58
59
60

- 1
2
3 1 (29) Hu, B., Dai, F., Fan, Z., Ma, G., Tang, Q., and Zhang, X. (2015) Nanotheranostics: Congo
4 Red/Rutin-MNPs with Enhanced Magnetic Resonance Imaging and H₂O₂-Responsive
5 Therapy of Alzheimer's Disease in APP^{swe}/PS1^{dE9} Transgenic Mice. *Adv. Mater.* 27
6 (37):5499-5505.
7
8
9
10
11 5 (30) Zhang, D., Fa, H.-B., Zhou, J.-T., Li, S., Diao, X.-W., and Yin, W. (2015) The detection of
12 β -amyloid plaques in an Alzheimer's disease rat model with DDNP-SPIO. *Clin. Radiol.* 70, 74–
13 80.
14
15
16
17
18 8 (31) Cheng, K. K., Chan, P. S., Fan, S., Kwan, S. M., Yeung, K. L., Wang, Y. X. J., Chow, A.
19 H. L., Wu, E. X., and Baum, L. (2015) Curcumin-conjugated magnetic nanoparticles for
20 detecting amyloid plaques in Alzheimer's disease mice using magnetic resonance imaging
21 (MRI). *Biomaterials* 44, 155–172.
22
23
24
25
26 12 (32) Altamura, S., and Muckenthaler, M. U. (2009) Iron toxicity in diseases of aging:
27 Alzheimer's disease, Parkinson's disease and atherosclerosis. *J. Alzheimer's Dis.* 16, 879–895.
28
29
30
31 14 (33) Bartzokis G, T. T. (2000) MRI evaluation of basal ganglia ferritin iron and neurotoxicity in
32 Alzheimer's and Huntington's disease. *Cell Mol Biol* 46, 821–833.
33
34
35
36 16 (34) Sultana, R., Boyd-Kimball, D., Cai, J., Pierce, W. M., Klein, J. B., Merchant, M., and
37 Butterfield, D. A. (2007) Proteomics analysis of the Alzheimer's disease hippocampal
38 proteome. *J. Alzheimers. Dis.* 11, 153–164.
39
40
41
42 19 (35) Rogers JT, Bush AI, Cho HH, Smith DH, Thomson AM, Friedlich AL, Lahiri DK,
43 Leedman PJ, Huang X, C. C. (2008) Iron and the translation of the amyloid precursor protein
44 (APP) and ferritin mRNAs: riboregulation against neural oxidative damage in Alzheimer's
45 disease. *Biochem Soc Trans* 36, 1282–1287.
46
47
48
49
50
51 23 (36) Grundke-Iqbal, I., Fleming, J., Tung, Y. C., Lassmann, H., Iqbal, K., and Joshi, J. G.
52 (1990) Ferritin is a component of the neuritic (senile) plaque in Alzheimer dementia. *Acta*
53 *Neuropathol.* 81, 105–110.
54
55
56
57
58
59
60

- 1
2
3 1 (37) Oakley, H., Cole, S. L., Logan, S., Maus, E., Shao, P., Craft, J., Guillozet-Bongaarts, A.,
4
5 2 Ohno, M., Disterhoft, J., Van Eldik, L., Berry, R., and Vassar, R. (2006) Intraneuronal β -
6
7 3 Amyloid Aggregates, Neurodegeneration, and Neuron Loss in Transgenic Mice with Five
8
9 4 Familial Alzheimer's Disease Mutations: Potential Factors in Amyloid Plaque Formation. *J.*
10
11 5 *Neurosci.* 26, 10129–10140.
12
13 6 (38) Smith, M. A., Harris, P. L., Sayre, L. M., and Perry, G. (1997) Iron accumulation in
14
15 7 Alzheimer disease is a source of redox-generated free radicals. *Proc. Natl. Acad. Sci. U. S. A.*
16
17 8 94, 9866–9868.
18
19
20 9 (39) Abo-Krysha, N., and Rashed, L. (2008) The role of iron dysregulation in the pathogenesis
21
22 10 of multiple sclerosis: an Egyptian study. *Mult. Scler.* 14, 602–608.
23
24 11 (40) Raven, E. P., Lu, P. H., Tishler, T. A., Heydari, P., and Bartzokis, G. (2013) Increased iron
25
26 12 levels and decreased tissue integrity in hippocampus of Alzheimer's disease detected in vivo
27
28 13 with magnetic resonance imaging. *J. Alzheimer's Dis.* 37, 127–136.
29
30
31 14 (41) Chen, J., Marks, E., Lai, B., Zhang, Z., Duce, J. A., Lam, L. Q., Volitakis, I., Bush, A. I.,
32
33 15 Hersch, S., and Fox, J. H. (2013) Iron Accumulates in Huntington's Disease Neurons:
34
35 16 Protection by Deferoxamine. *PLoS One* 8, 1–12.
36
37
38 17 (42) Mochizuki, H., and Yasuda, T. (2012) Iron accumulation in Parkinson's disease. *J. Neural*
39
40 18 *Transm.* 119, 1511–1514.
41
42 19 (43) Hametner, S., Wimmer, I., Haider, L., Pfeifenbring, S., Brück, W., and Lassmann, H.
43
44 20 (2013) Iron and neurodegeneration in the multiple sclerosis brain. *Ann. Neurol.* 74, 848–861.
45
46
47 21 (44) Meadowcroft, M. D., Connor, J. R., and Yang, Q. X. (2015) Cortical iron regulation and
48
49 22 inflammatory response in Alzheimer's disease and APP SWE/PS1 Δ E9 mice: A histological
50
51 23 perspective. *Front. Neurosci.* 9, 1–16.
52
53 24 (45) Lopes, K. O., Sparks, D. L., and Streit, W. J. (2008) Microglial dystrophy in the aged and
54
55 25 Alzheimer's disease brain is associated with ferritin immunoreactivity. *Glia* 56, 1048–1060.
56
57
58
59
60

- 1
2
3 1 (46) Mrak, R.E. (2012) Microglia in Alzheimer brain: a neuropathological perspective. *Int J*
4
5 2 *Alzheimers Dis* 2012, 165021.
6
7 3 (47) Lipman, N. S., Jackson, L. R., Weis-Garcia, F., and Trudel, L. J. (2005) Monoclonal versus
8
9 4 polyclonal antibodies: distinguishing characteristics, applications, and information resources.
10
11 5 *ILAR J.* 46, 258–268.
12
13 6 (48) Monagle, J. J. (1962) Carbodiimides. III. Conversion of isocyanates to carbodiimides-
14
15 7 catalyst studies. *J. Org. Chem.* 27, 3851–3855.
16
17
18 8 (49) Schmidt, M. L., Robinson, K. A., Lee, V. M., and Trojanowski, J. Q. (1995) Chemical and
19
20 9 immunological heterogeneity of fibrillar amyloid in plaques of Alzheimer’s disease and Down’s
21
22 10 syndrome brains revealed by confocal microscopy. *Am. J. Pathol.* 147, 503–515.
23
24
25 11 (50) Mu, K., Zhang, S., Ai, T., Jiang, J., Yao, Y., Jiang, L., Zhou, Q., Xiang, H., Zhu, Y., Yang,
26
27 12 X., and Zhu, W. (2015) Monoclonal antibody-conjugated superparamagnetic iron oxide
28
29 13 nanoparticles for imaging of epidermal growth factor receptor-targeted cells and gliomas. *Mol.*
30
31 14 *Imaging* 14.
32
33
34 15 (51) Novotna, B., Jendelova, P., Kapcalova, M., Rossner, P., Turnovcova, K., Bagryantseva, Y.,
35
36 16 Babic, M., Horak, D., and Sykova, E. (2012) Oxidative damage to biological macromolecules in
37
38 17 human bone marrow mesenchymal stromal cells labeled with various types of iron oxide
39
40 18 nanoparticles. *Toxicol. Lett.* 210, 53–63.
41
42
43 19 (52) Mahmoudi, M., Monopoli, M. P., Rezaei, M., Lynch, I., Bertoli, F., Mcmanus, J. J., and
44
45 20 Dawson, K. A. (2013) The Protein Corona Mediates the Impact of Nanomaterials and Slows
46
47 21 Amyloid Beta Fibrillation. *ChemBioChem* 14, 568–572.
48
49 22 (53) Li, L., Fang, C. J., Ryan, J. C., Niemi, E. C., Lebrón, J. a, Björkman, P. J., Arase, H., Torti,
50
51 23 F. M., Torti, S. V, Nakamura, M. C., and Seaman, W. E. (2010) Binding and uptake of H-
52
53 24 ferritin are mediated by human transferrin receptor-1. *Proc. Natl. Acad. Sci. U. S. A.* 107, 3505–
54
55 25 3510.
56
57
58
59
60

- 1
2
3 1 (54) Wallace, D. F., McDonald, C., and Subramaniam, V. N. (2010) Transferrin receptor 1: A
4 ferritin receptor as well? *Gastroenterology* 139, 1052–1053.
5
6
7 3 (55) Brown, R. C., Egleton, R. D., and Davis, T. P. (2004) Mannitol opening of the blood-brain
8 barrier: Regional variation in the permeability of sucrose, but not $^{86}\text{Rb}^+$ or albumin. *Brain Res.*
9 1014, 221–227.
10
11
12
13 6 (56) Jing Yang, Youssef Zaim Wadghiri, Dung Minh Hoang, Wai Tsui, Yanjie Sun, E., and
14 Chung, Yongsheng Li, Andrew Wang, M. de L. and T. W. (2011) Detection of Amyloid
15 Plaques Targeted by USPIO-A β 1-42 in Alzheimer's Disease Transgenic Mice using Magnetic
16 Resonance Microimaging. *Neuroimage* 55, 1600–1609.
17
18
19
20 10 (57) Bush, A. I., and Tanzi, R. E. (2008) Therapeutics for Alzheimer's disease based on the
21 metal hypothesis. *Neurotherapeutics* 5, 421–432.
22
23
24
25 12 (58) Hall, a P., Davies, W., Stamp, K., Clamp, I., and Bigley, A. (2013) Comparison of
26 Computerized Image Analysis with Traditional Semiquantitative Scoring of Perls' Prussian
27 Blue Stained Hepatic Iron Deposition. *Toxicol. Pathol.* 992–1000.
28
29
30
31 15 (59) Bussière, T., Bard, F., Barbour, R., Grajeda, H., Guido, T., Khan, K., Schenk, D., Games,
32 D., Seubert, P., and Buttini, M. (2004) Morphological characterization of Thioflavin-S-positive
33 amyloid plaques in transgenic Alzheimer mice and effect of passive Abeta immunotherapy on
34 their clearance. *Am. J. Pathol.* 165, 987–995.
35
36
37
38
39 19 (60) Ernst, O., and Zor, T. (2010) Linearization of the Bradford Protein Assay. *J. Vis. Exp.* 1–6.
40
41
42
43 20 (61) Fernández-Cabada, T., Pablo, C. S.-L. de, Pisarchyk, L., Serrano-Olmedo, J. J., and
44 Ramos-Gómez, M. (2016) Optical Hyperthermia Using Anti-Epidermal Growth Factor
45 Receptor-Conjugated Gold Nanorods to Induce Cell Death in Glioblastoma Cell Lines. *J.*
46 *Nanosci. Nanotechnol.* 16, 7689–7695.
47
48
49
50 24 (62) Alvarez, G., Muñoz-Montaña, J. R., Satrústegui, J., Avila, J., Bogónez, E., Díaz-Nido, J.,
51 and Díaz-Nido, J. (1999) Lithium protects cultured neurons against beta-amyloid-induced
52
53
54
55
56
57
58
59
60

1 neurodegeneration. *FEBS Lett.* 453, 260–264.

2 (63) Berridge, M. V., Herst, P. M., and Tan, A. S. (2005) Tetrazolium dyes as tools in cell
3 biology: New insights into their cellular reduction. *Biotechnol. Annu. Rev.* 11, 127-152.

4 (64) Yardeni, T., Eckhaus, M., Morris, H. D., Huizing, M., and Hoogstraten-Miller, S. (2011)
5 Retro-orbital injections in mice. *Lab Anim. (NY).* 40, 155–160.

6 ***Figure captions***

7 **Figure 1: Iron, amyloid, and ferritin accumulation in 5XFAD mice.** Coronal brain sections
8 of nontransgenic (**A**, **C**, and **E**) and 5XFAD transgenic (**B**, **D**, and **F**) mice stained with: **A** and
9 **B**) Prussian blue to detect iron accumulation; **C** and **D**) Thioflavin S to label amyloid plaques;
10 and **E** and **F**) an anti-ferritin antibody to detect the protein ferritin. No obvious label of any
11 markers can be detected in nontransgenic mice, while the subiculum in 5XFAD mice showed a
12 strong labeling for iron (arrow in **B**), amyloid plaques (arrow in **D**), and ferritin (arrow in **F**).
13 Scale bars in **A** and **B**: 200 μm and in **C-F**: 500 μm .

14 **Figure 2: Spatial relationship between ferritin and amyloid plaques in 5XFAD mice.** Serial
15 confocal microscopy images obtained every 5 μm from the top of the section to the bottom (**A**
16 **through D**) in the Z axis from the subiculum of a 5XFAD mouse. Coronal brain sections were
17 labeled with an antibody anti-ferritin (red) and Thioflavin S (green) to detect the presence of
18 ferritin and amyloid plaques, respectively. Scale bar: 25 μm .

19 **Figure 3: Cell types that accumulate ferritin in 5XFAD mice.** **A**) Coronal brain section of a
20 5XFAD mouse stained with an anti-ferritin antibody showing the accumulation of ferritin in the
21 subiculum area (arrow). **B**) Higher magnification of the same anatomical region showing a high
22 regional colocalization of amyloid plaques stained with Thioflavin S (green) and the anti-ferritin
23 antibody (red). **C**) Sections stained with the astrocytic marker GFAP (green) showed a high
24 number of GFAP-positive cells throughout the subiculum area with no colocalization with the
25 ferritin-positive cells (red). **D**) Microglial cells in the subiculum area labeled with tomato lectin

1
2
3 1 (green) showing a high degree of colocalization (yellow) with the ferritin stain (anti-ferritin
4
5 2 antibody in red). Scale bars in **A**: 500 μm ; in **B-D**: 100 μm .

6
7
8 3 **Figure 4: Dot-blot assay to determine the effectiveness of the anti-ferritin antibody**

9
10 4 **coupling to MNPs.** One μl of **A**) anti-ferritin antibody used for the coupling reaction, **B**) MNPs
11
12 5 functionalized with the anti-ferritin antibody, **C**) supernatant after the coupling reaction (anti-
13
14 6 ferritin antibody not bound to MNPs), and **D**) MNPs used as a negative control. Note that a very
15
16 7 high fraction of the initial antibody present in the coupling reaction did bind to the MNPs.

17
18 8 **Figure 5: Cell viability after incubation with magnetic nanoparticles.** Analysis of the

19
20 9 viability of human neuroblastoma SH-SY5Y cells (**A**) and neuronal-glia mixed primary cell
21
22 10 cultures obtained from mouse brains (**B**) exposed to increasing concentrations of MNPs and
23
24 11 MNP-anti-ferritin for 72 hours, assessed by the LDH and XTT assays, respectively. No
25
26 12 remarkable changes in cell viability were observed when cells were exposed to increasing
27
28 13 concentrations of both types of MNPs for 72 hours. Cell viability in LDH and XTT assays was
29
30 14 considered maximum (100%) when cells were incubated without MNPs. The number of
31
32 15 neurons, astrocytes and microglial cells did not show any changes when primary cell cultures
33
34 16 obtained from mouse brains were incubated with either MNPs or MNPs-anti-ferritin (**C**).

35
36 17 Microfluorescence images of red fluorescent MNPs-treated cell cultures stained with anti- β -III-
37
38 18 tubulin (neurons), anti-GFAP (astrocytes) and anti-Iba1 (microglia) in green show that the
39
40 19 nanoparticles are uptaken preferentially by microglial cells (**D**). Inserts in **D** show single
41
42 20 staining for fluorescent MNPs (red) and microglial cells stained with anti-Iba-1 (green). Nuclei
43
44 21 were counterstained with Hoechst (blue). Each value in the graph bars represents the mean \pm
45
46 22 SEM of $n = 3$ independent experiments. ANOVA followed by the post-hoc Tukey's test
47
48 23 revealed the absence of significant differences ($p > 0.05$) for each group compared to untreated
49
50 24 cells with MNPs. Scale bar in **D**: 50 μm .

51
52
53 25 **Figure 6: *In vitro* specificity of the MNP-anti-ferritin conjugate.** Coronal brain sections of

54
55 26 5XFAD (**A**) and nontransgenic (**E**) mice were stained with an antibody anti-ferritin to determine

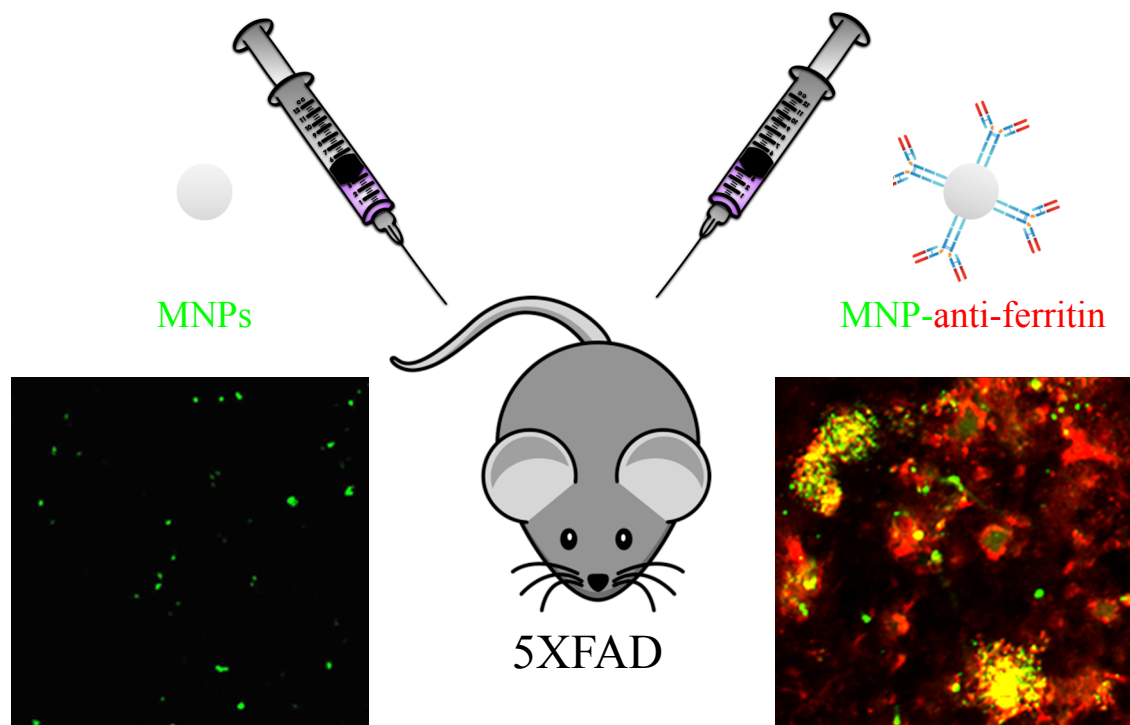
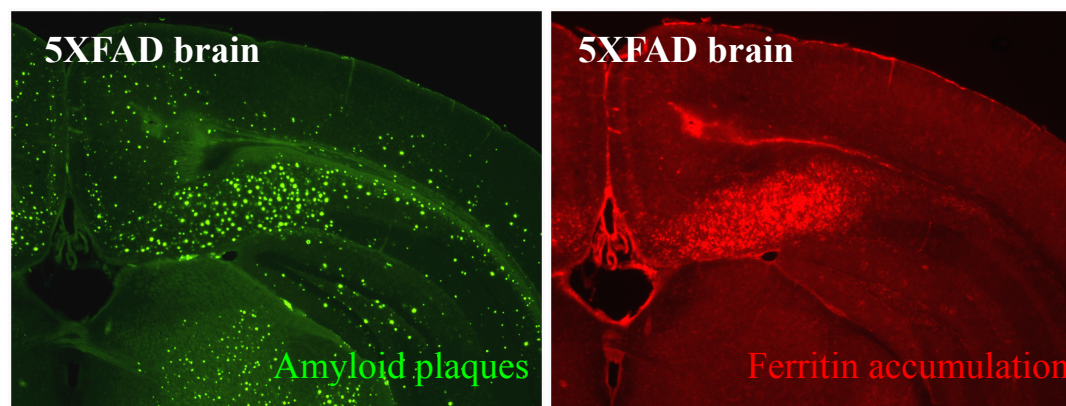
1 the accumulation of this protein in the subiculum region (boxes in **A** and **E**). Note the high
2 accumulation of ferritin in 5XFAD brain compared to nontransgenic mice. Coronal brain
3 sections of 5XFAD (**B-D**) and nontransgenic (**F-H**) mice, adjacent to those shown in **A** and **E**
4 respectively, were incubated first with the nanoconjugate MNP-anti-ferritin and then with a
5 secondary antibody-Cy3 to detect the presence of the nanoconjugate MNP-anti-ferritin stained
6 in red (**C, G**). MNPs were also detected by transmitted light microscopy as black dots in
7 5XFAD (**D**) and nontransgenic (**H**) mice. **B** and **F** show merged images of **C** and **D**, and **G** and
8 **H**, respectively. Note the high rate of colocalization of ferritin and MNPs (**B**) demonstrating an
9 optimal biofunctionalization of the particles and the absence of binding of the nanoconjugate to
10 the nontransgenic brain sections (**F-H**) where no ferritin accumulation can be detected (**E**).
11 Scale bars: **A** and **E**: 500 μm ; **B-D** and **F-H**: 50 μm .

12 **Figure 7: *In vivo* specificity of the MNP-anti-ferritin conjugate in 5XFAD mice.** Coronal
13 brain section of a 5XFAD mouse showing **A**) the accumulation of ferritin (red) and amyloid
14 plaques stained with Thioflavin S (green); **B**) the subiculum region of a 5XFAD mouse
15 previously injected intravenously with the MNP-anti-ferritin conjugate, showing the presence of
16 the MNP-anti-ferritin nanoconjugate (red) closely bound to amyloid plaques stained with
17 Thioflavin S (green). Coronal sections of the subiculum of 5XFAD mice injected with the
18 functionalized MNP-anti-ferritin nanoconjugate (**C-E**) and with the non-functionalized MNPs
19 (**F-H**). The anti-ferritin antibody of the nanoconjugate was detected using a secondary antibody-
20 Cy3 (red) (**C, F**). All MNPs were detected using an anti-dextran-FITC antibody (green) (**D, G**).
21 Merged images of **C** and **D**, and **F** and **G** are shown in **E** and **H**, respectively. Note the high
22 accumulation of MNPs in the subiculum of animals injected with the nanoconjugate MNP-anti-
23 ferritin (**C-E**) and the absence of MNPs in the same area when non-functionalized MNPs were
24 used (**F-H**). Scale bars: **A** and **B**: 100 μm ; **C-H**: 50 μm .

25 **Figure 8: *Ex vivo* MRI in 5XFAD mice.** Ex vivo MR images used to determine absolute T2*
26 values (msec) in regions of interest (ROIs), which were the left and right hippocampus of
27 5XFAD mice injected with MNPs (A) and MNPs-anti-ferritin (B). Graphic shows the data

1
2
3 1 corresponding to the T2* value obtained in the analyzed ROIs of the left and right hippocampus
4
5 2 in 5XFAD mice injected with MNPs versus MNP-anti-ferritin (*p < 0.05; ANOVA followed by
6
7 3 the post-hoc Tukey's test).
8
9
10 4
11
12 5
13
14
15 6
16
17
18 7
19
20
21 8
22
23
24 9
25
26
27 10
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

Potential use of the MNP-anti-ferritin nanoconjugate as an effective MRI contrast agent for the diagnosis of Alzheimer's disease



Non-functionalized MNPs
do not bind to 5XFAD brains

MNP-anti-ferritin conjugates
specifically bind to 5XFAD brains

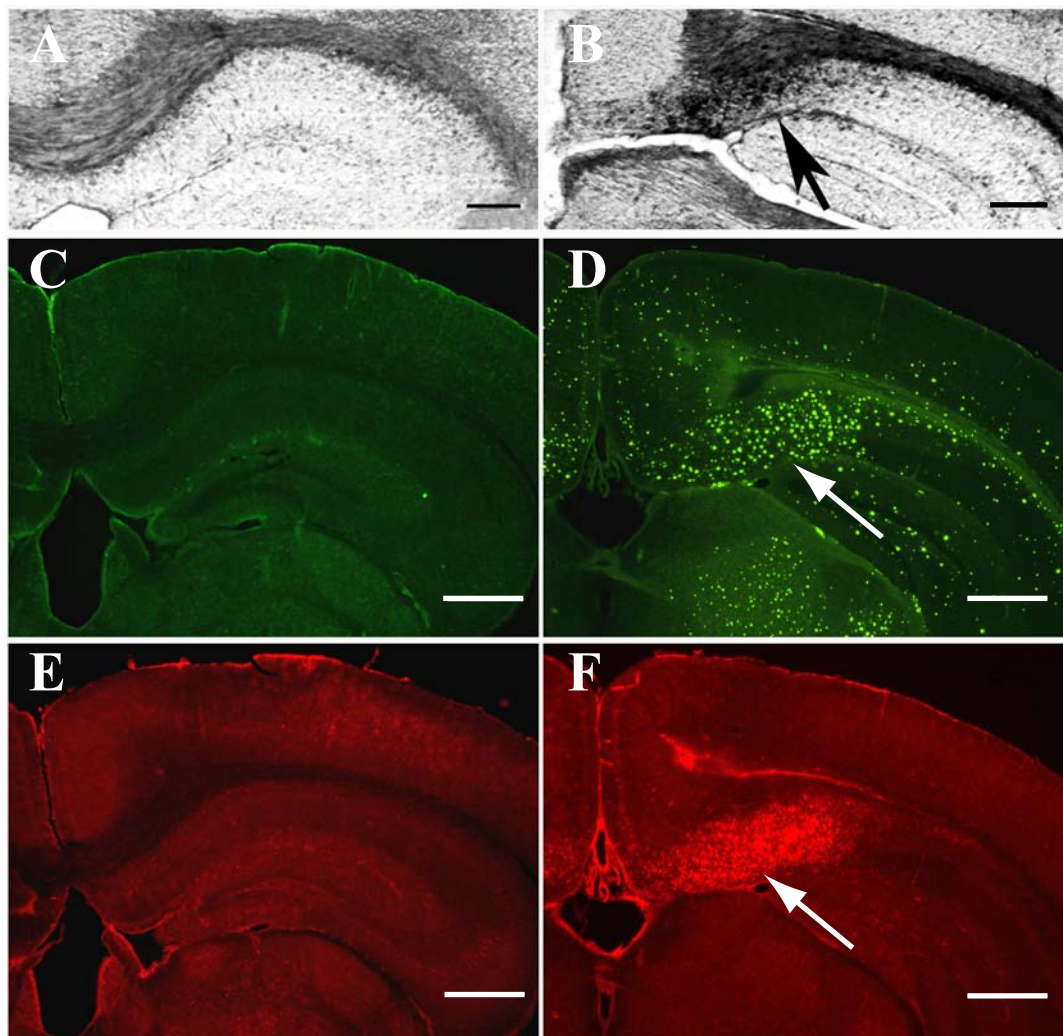


Figure 1

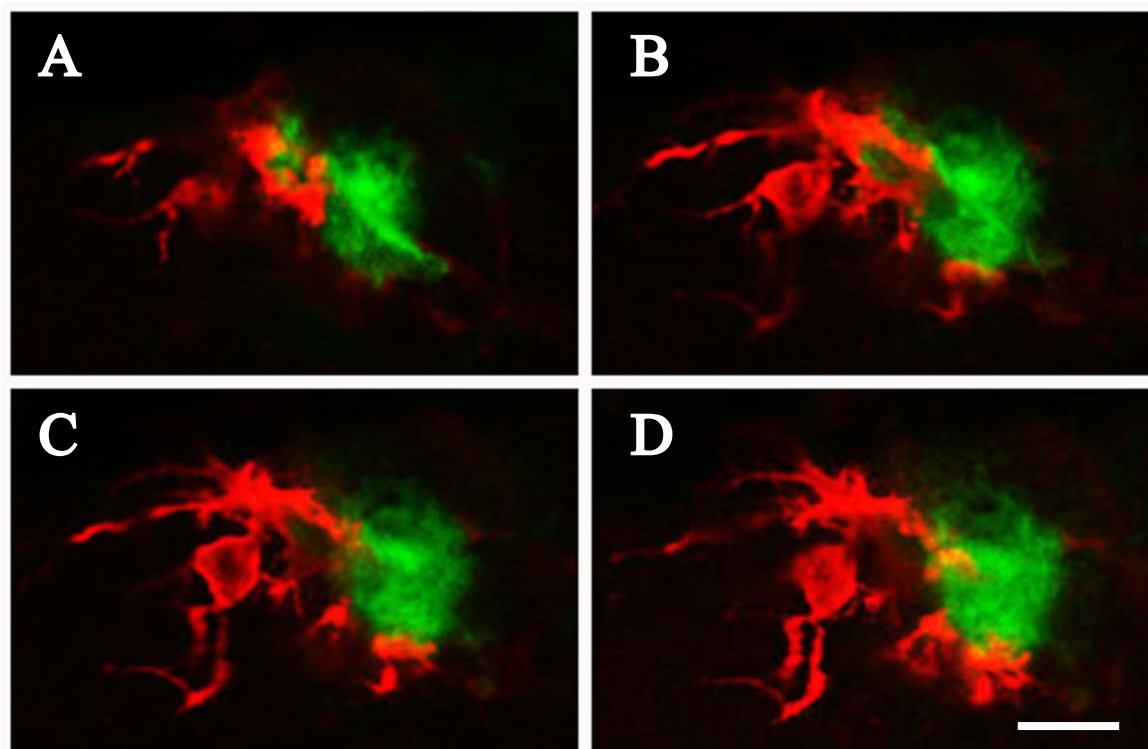


Figure 2

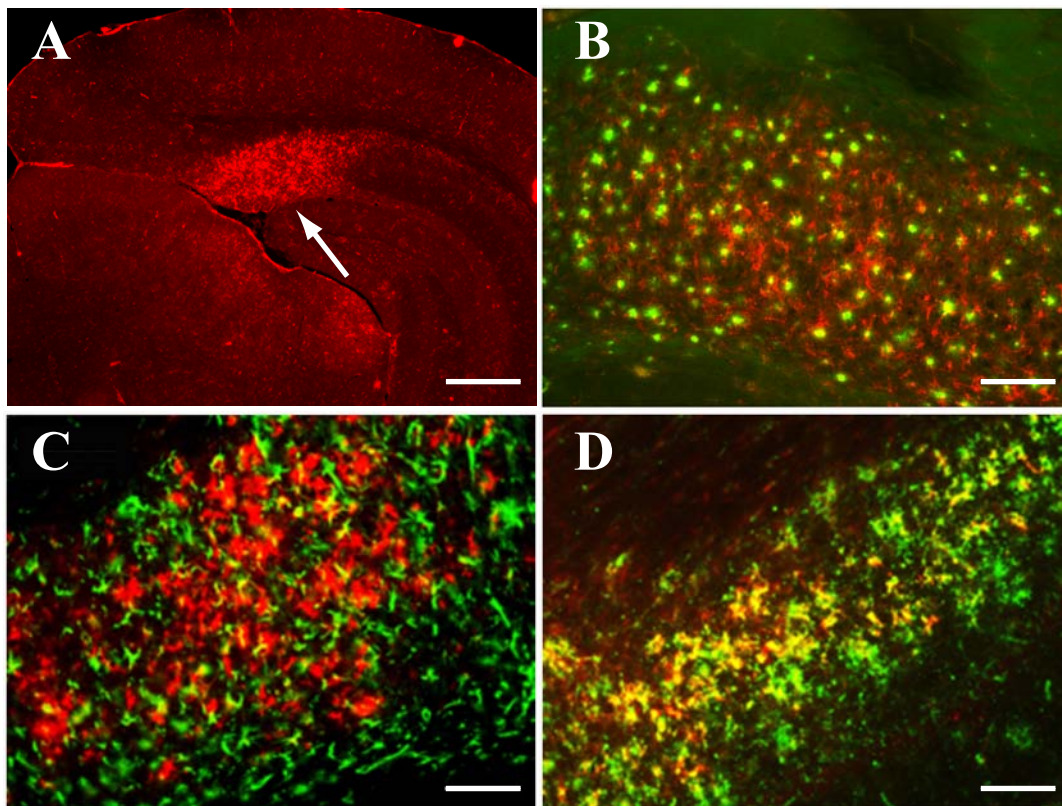


Figure 3

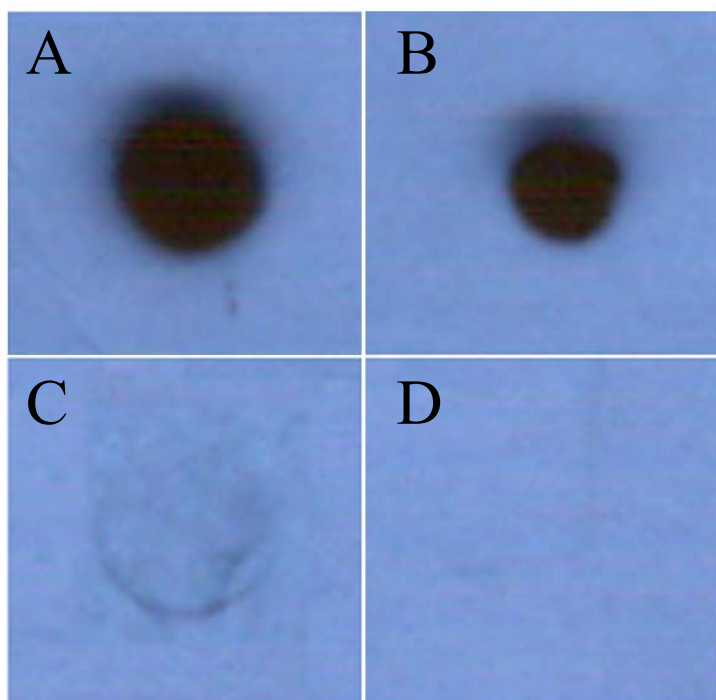


Figure 4

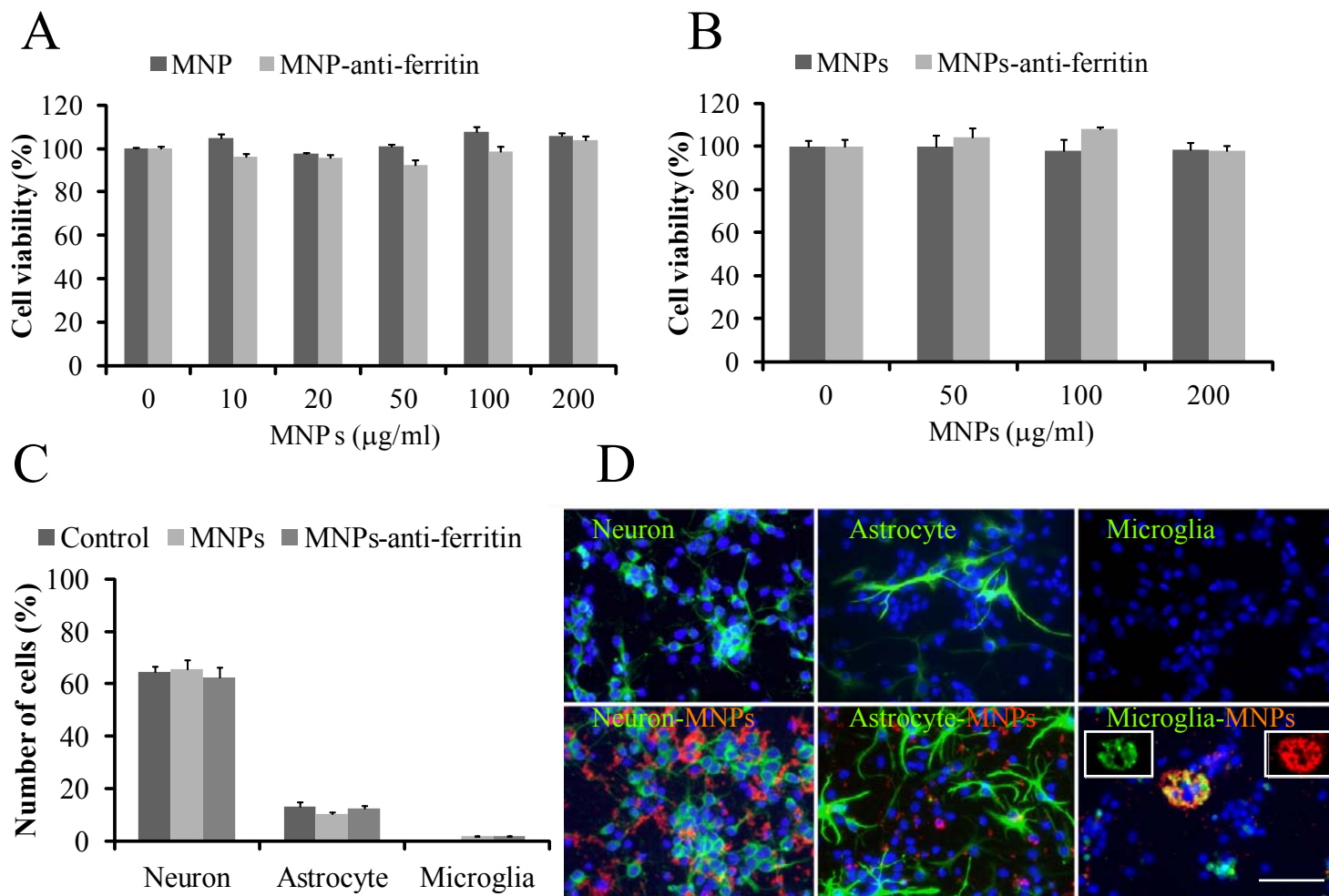


Figure 5

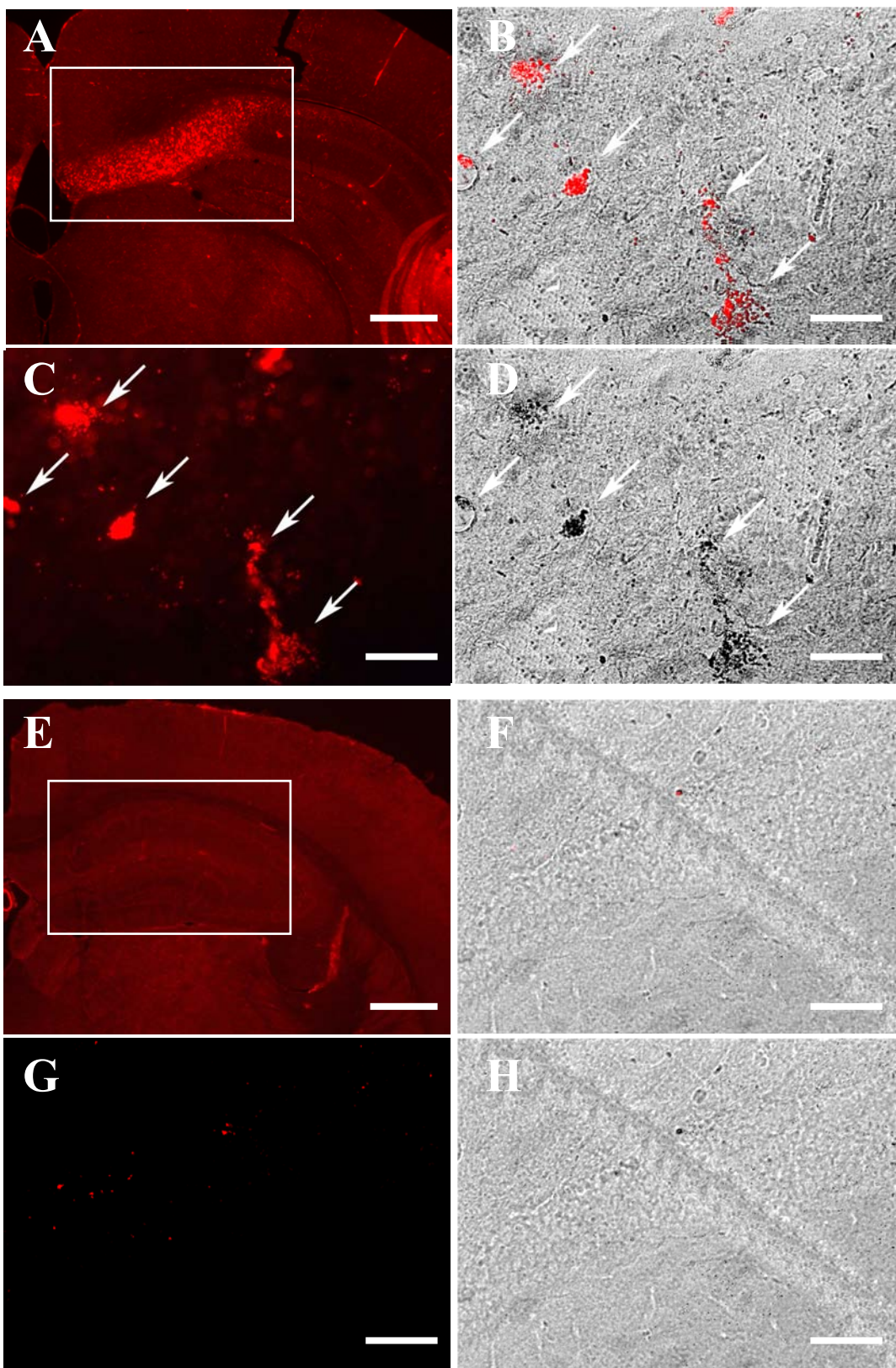


Figure 6

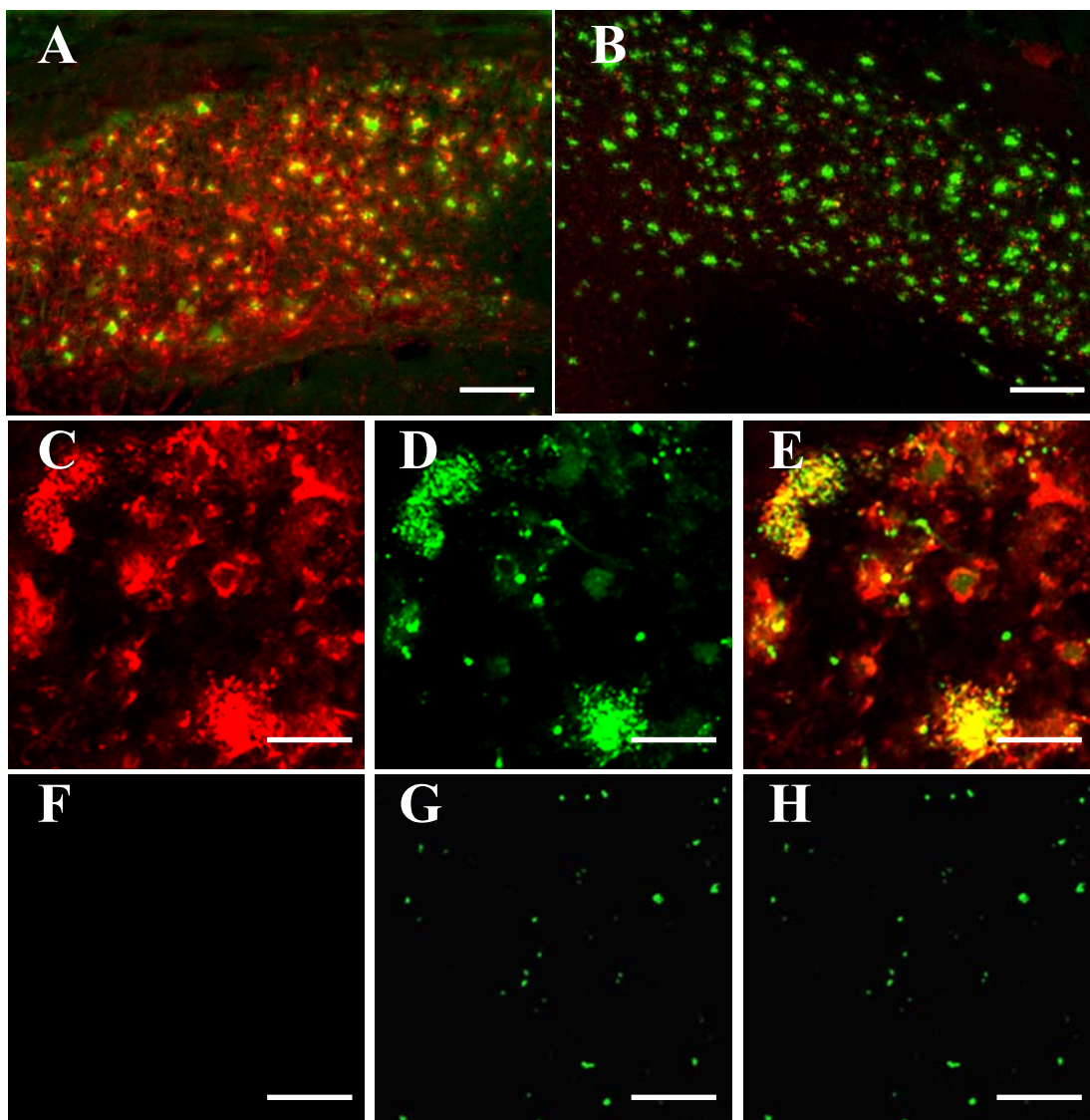


Figure 7

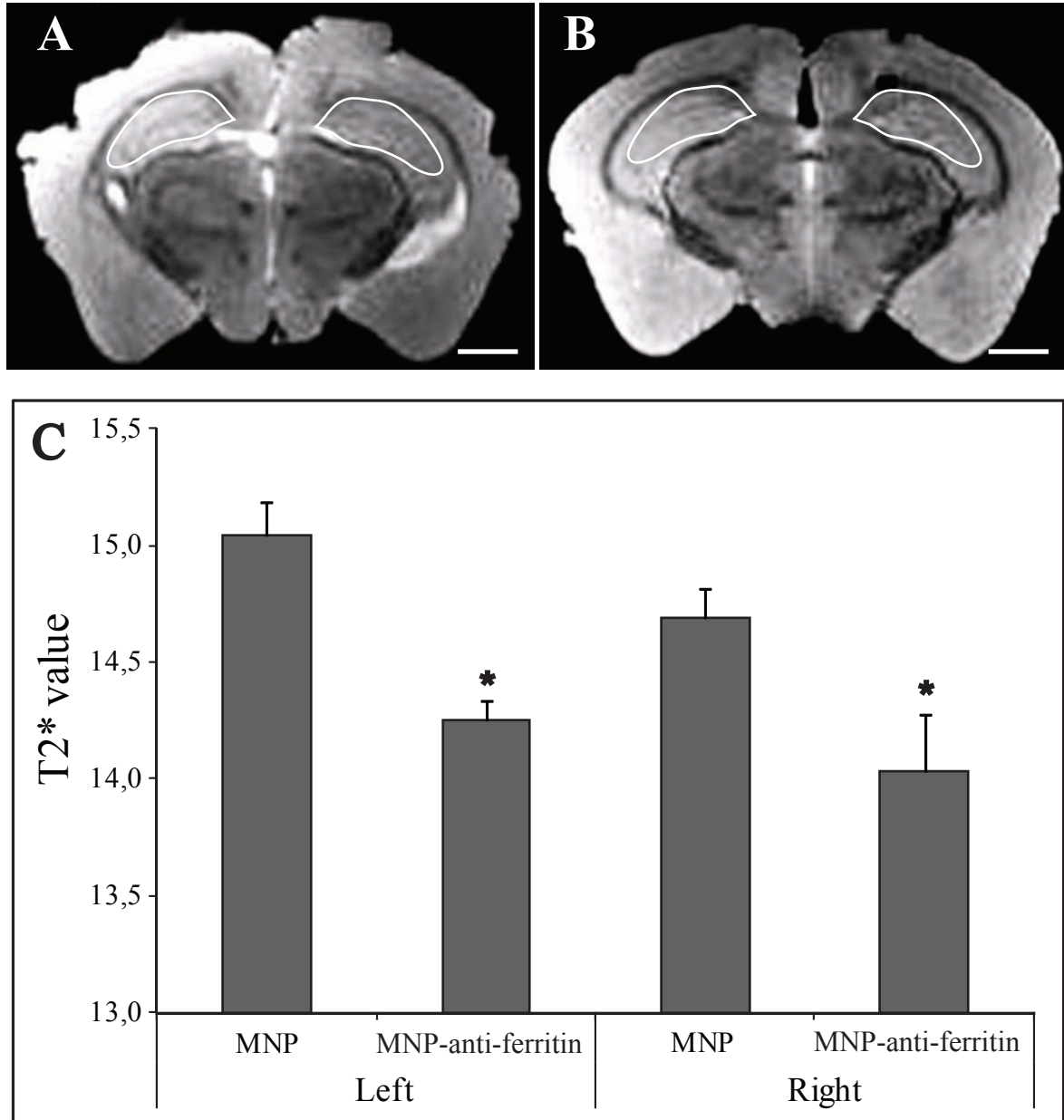


Figure 8