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Biofabrication and Evaluation, *in vitro* and *in vivo*, of a Dual Responsive Glucose and Lactate Implantable Biosensor in a Piglet Trauma Model

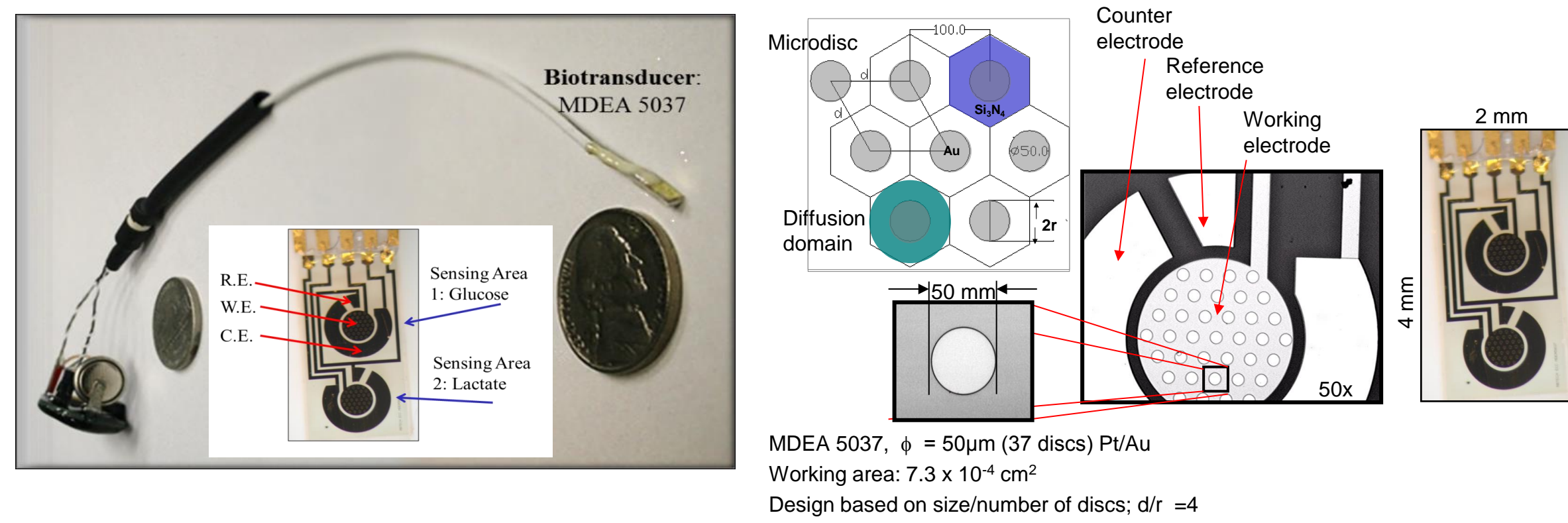
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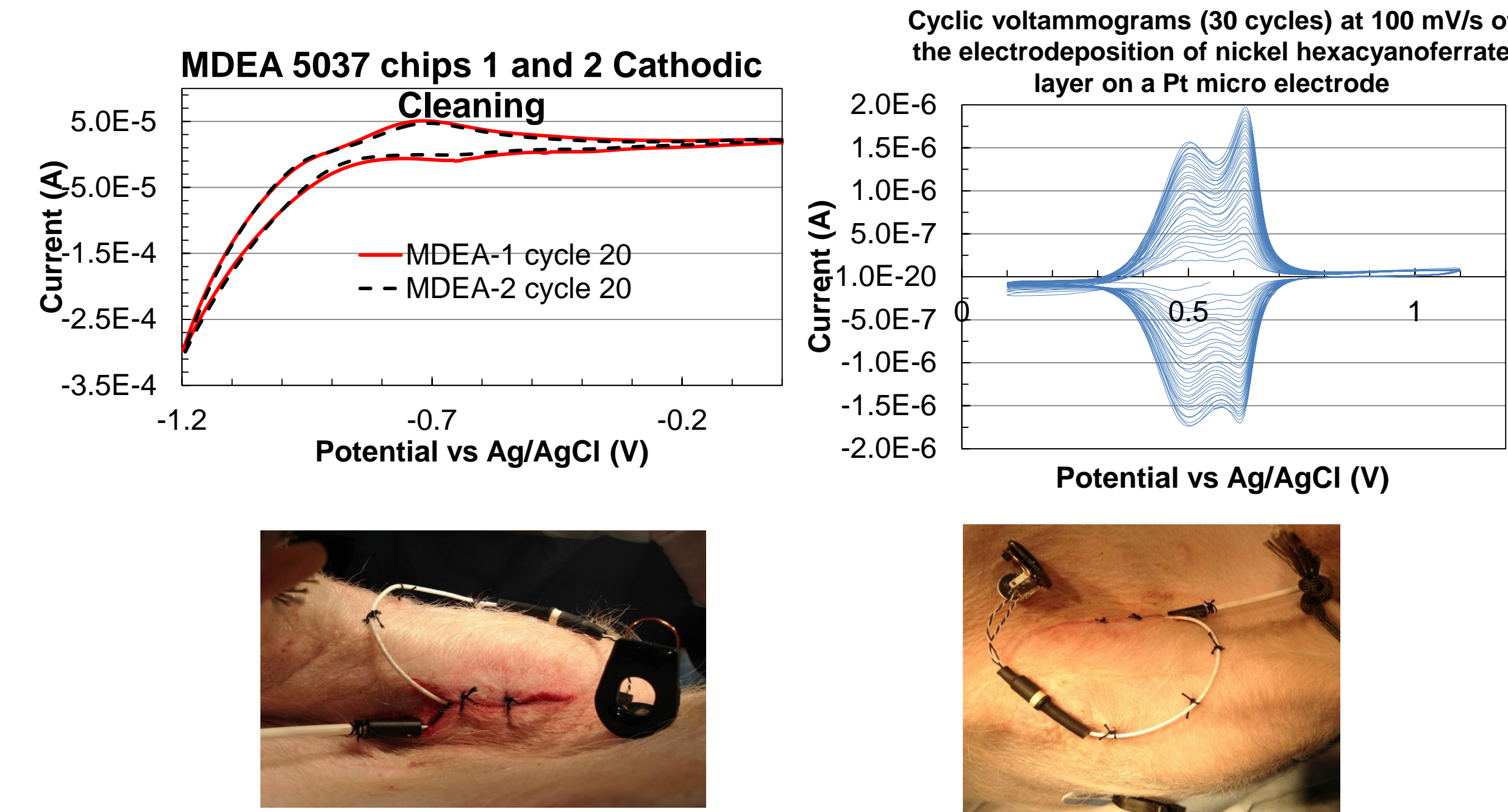
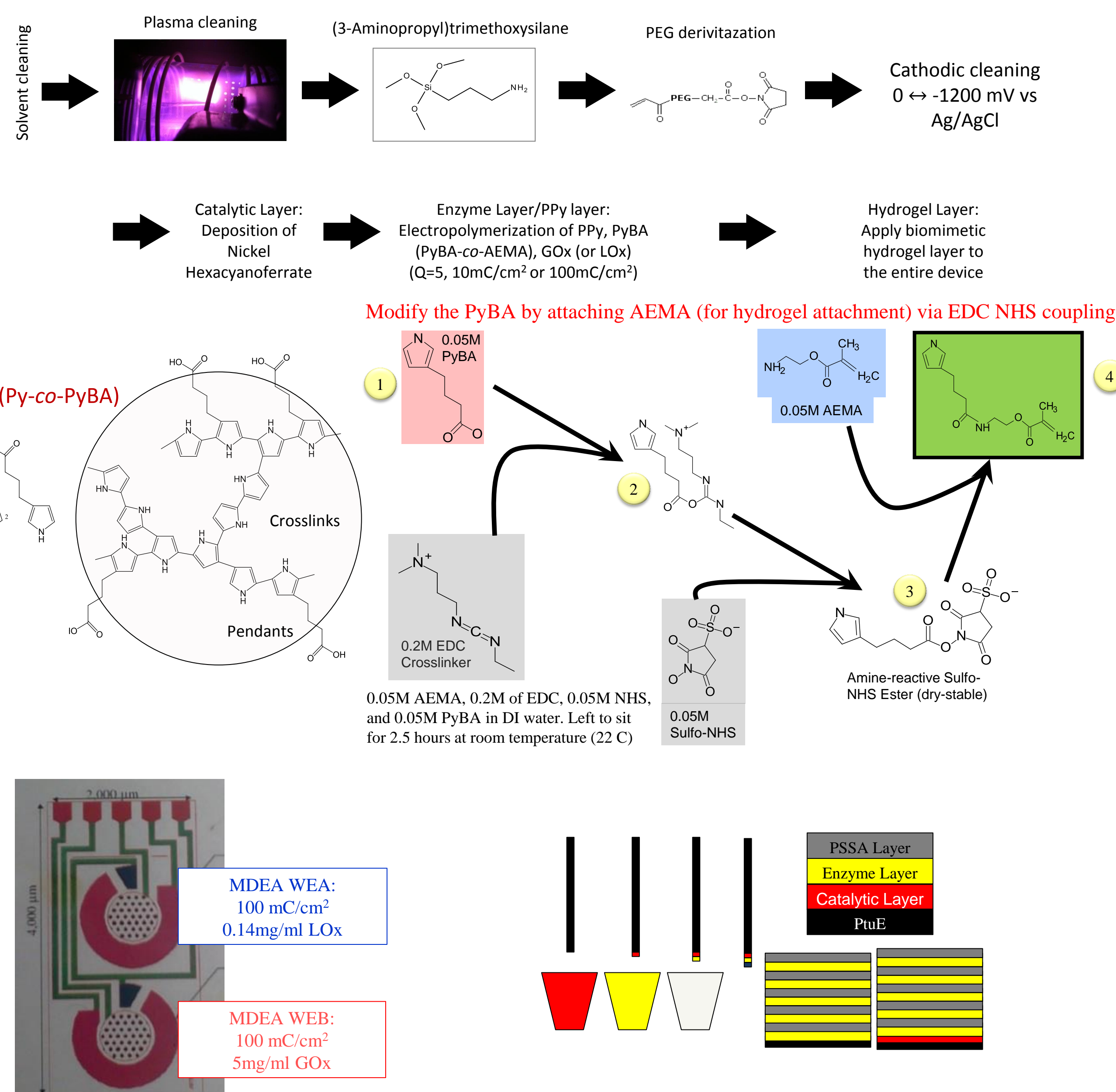
1. Introduction

- Pressing need for the design and development of a device for **simultaneous** measurement of interstitial levels of glucose and lactate levels during **hemorrhage**
- Minimally invasive, dual responsive Electrochemical Cell-on-a-Chip Microdisc Electrode Array (ECC MDEA 5037) has been developed for use with a wireless biosensor system.
- Fabrication of the biorecognition membrane via pyrrole electropolymerization, ***in vitro*** and ***in vivo*** characterization of the resulting biotransducer (as well as the intermediate steps in fabrication) are described.



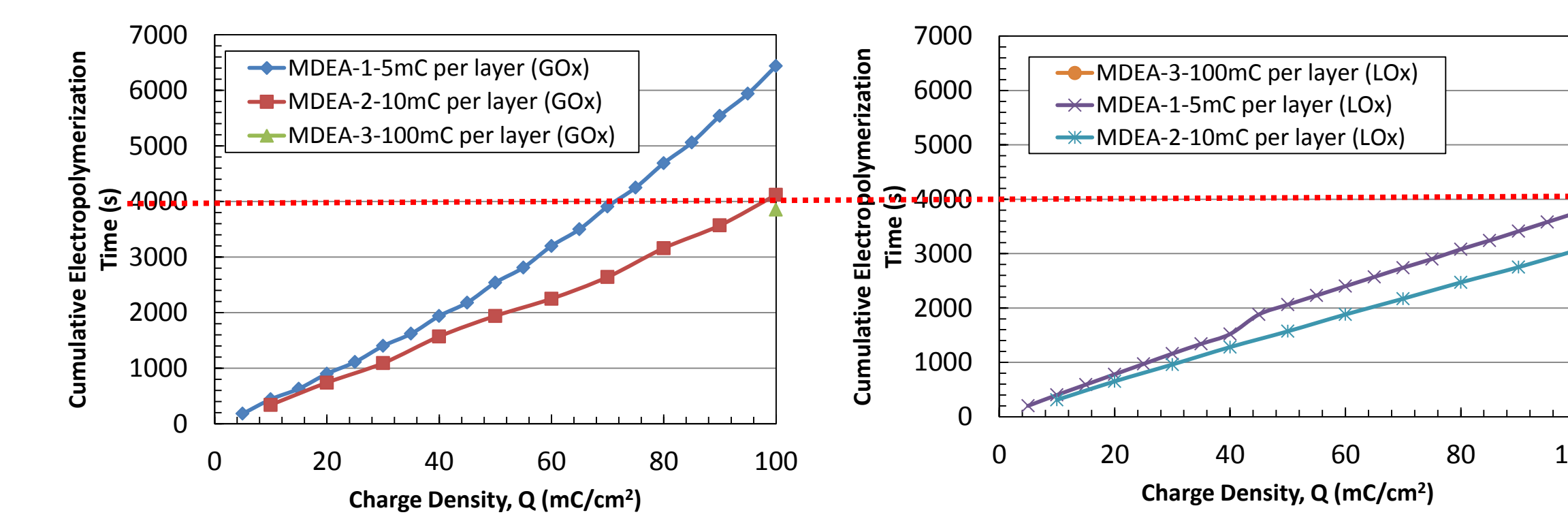
- A dual responsive Electrochemical Cell-on-a-Chip Microdisc Electrode Array (ECC MDEA 5037) powered by a wireless potentiostat and developed for use in a wireless implantable biosensor system. Insert shows the reference electrode (R.E.), working electrode (W.E.) and counter electrode (C.E.) for each electrochemical cell area
- Front-end details of the MDEA5037 device

2. Materials and Methods

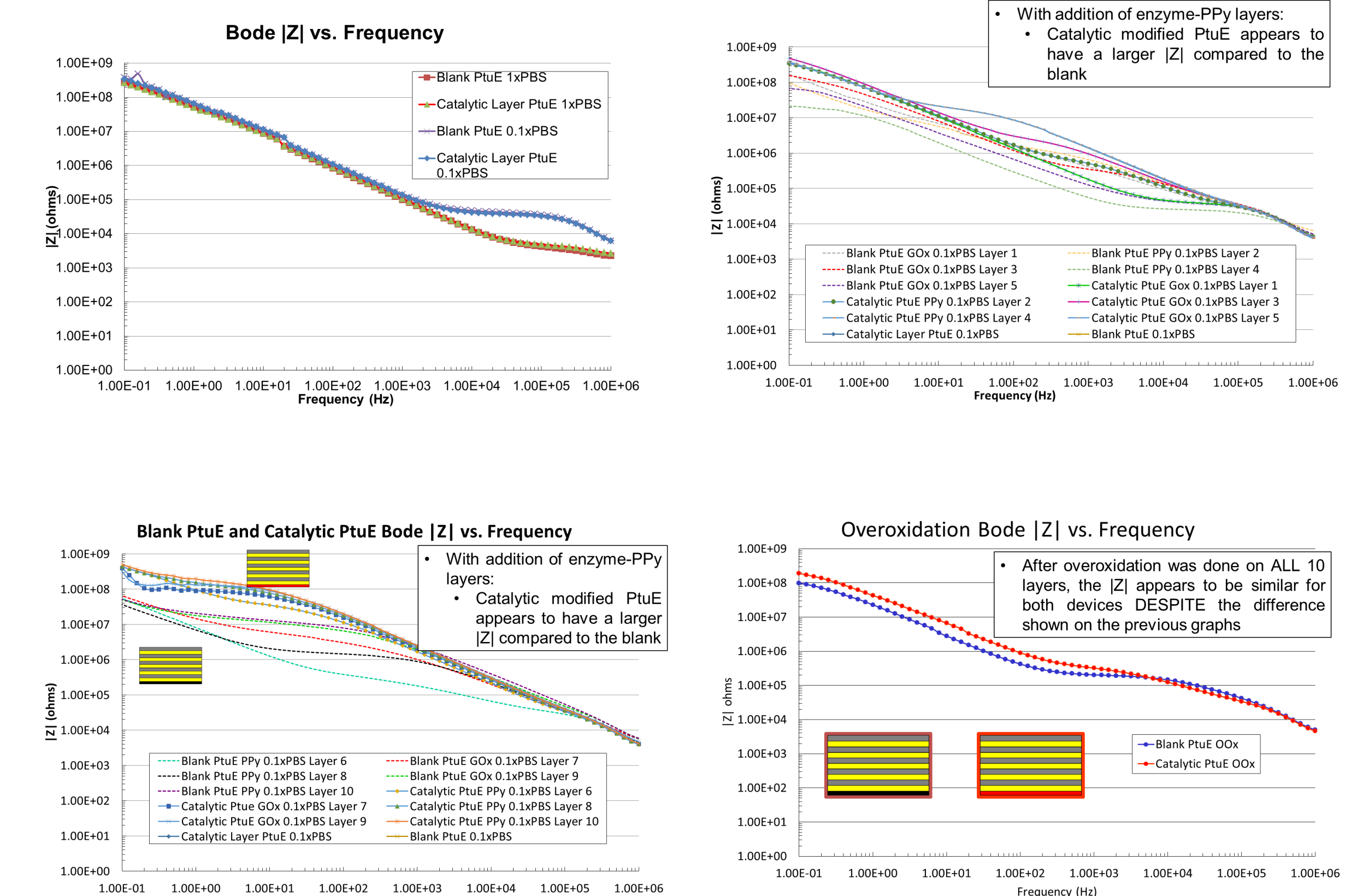


- Sample data from cathodic cleaning after 20 cycles on 2 different MDEA devices. Demonstrates consistency and reproducibility of electrode areas
- Cyclic voltammograms (30 cycles) at 100 mV/s of the electrodeposition of nickel hexacyanoferrate layer on a Pt micro electrode
- Implantation of dual (glucose and lactate) sensing device in shoulder muscle of piglet

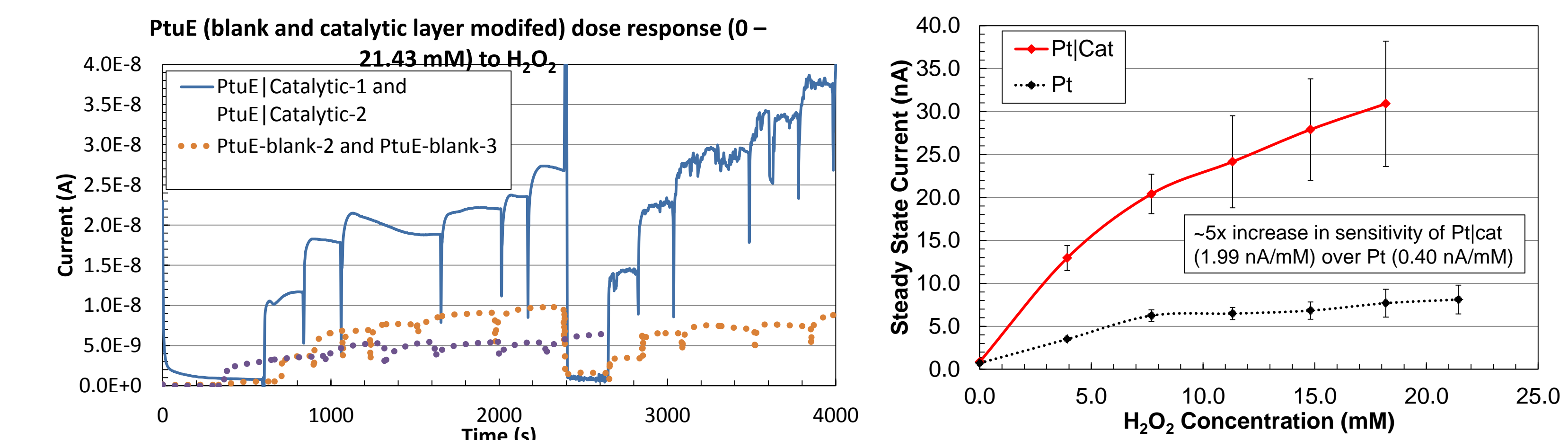
3. Results and Discussion



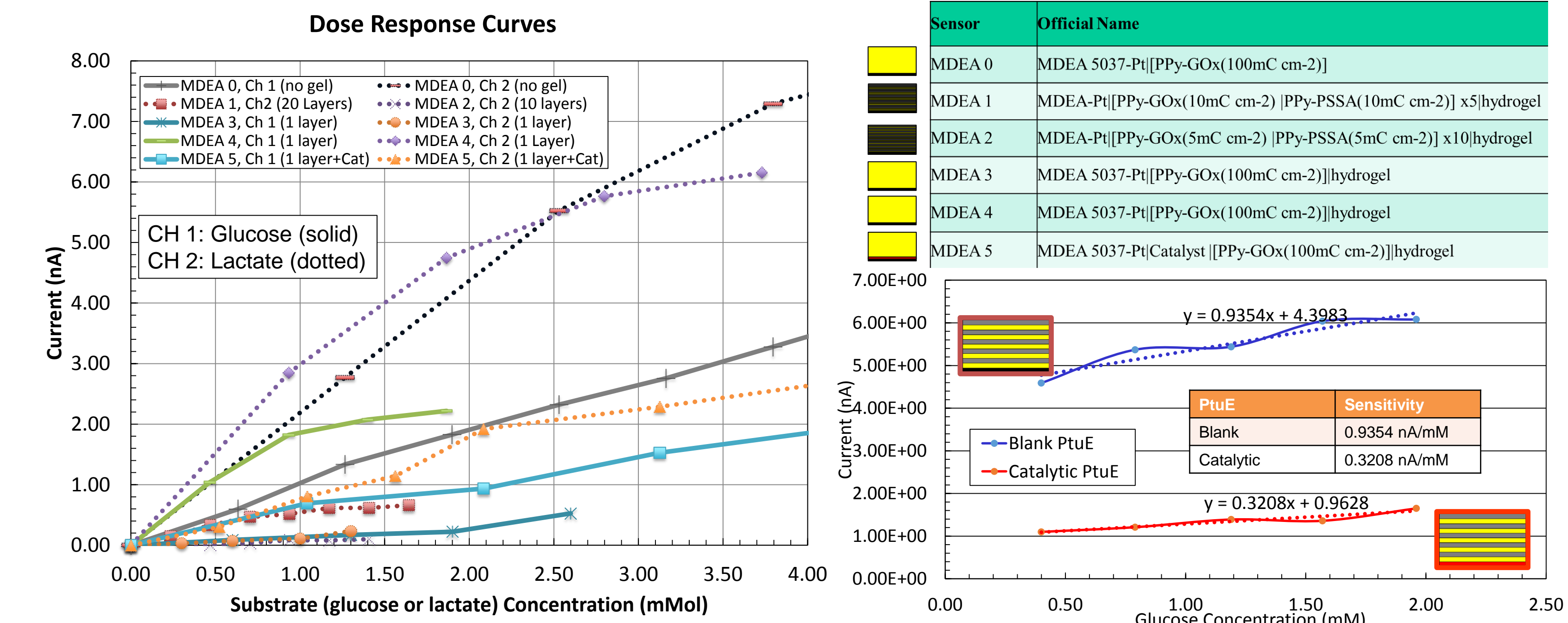
- Cumulative electropolymerization time vs. cumulative charge density for glucose oxidase (GOx) and lactate oxidase (LOx) systems at different charge densities



- The variation in the sets of curves is due to the difference in buffer conditions
- Both** the blank and catalytic layer modified devices appear **similar** and do not show any variation in |Z|



Role of catalytic layer: Blank sensor vs. catalytic sensor response to varying H₂O₂ concentration



Device	Sensitivity (nA/mM) - Glucose	Sensitivity (nA/mM) - Lactate	Response Time
MDEA 5037-Pt[PPy-GOx(100mC cm ⁻²)]	2.19	1.05	12 minutes (no hydrogel layer)
MDEA-Pt[PPy-GOx(10mC cm ⁻²) PPy-PSSA(10mC cm ⁻²)x5]gel	N/A	0.70	18-20 minutes
MDEA-Pt[PPy-GOx(5mC cm ⁻²) PPy-PSSA(5mC cm ⁻²)x10]gel	N/A	0.07	18-20 minutes
MDEA 5037-Pt[PPy-GOx(100mC cm ⁻²)]gel	3.05	1.95	10-14 minutes (thinner hydrogel layer)
MDEA 5037-Pt[Catalyst][PPy-GOx(100mC cm ⁻²)]gel	0.67	0.57	10-14 minutes (thinner hydrogel layer)

- Response to glucose and lactate concentrations in the tissue of the piglets and device details
- In vitro* characterization: Comparing role of catalytic layer
- In vivo* characterization: Summary of sensitivities and response times for various implanted devices.

4. Conclusions and Summary

- Demonstrated dual glucose and lactate responsive biotransducer
- Increasing the charge density does not appear to change the biotransduction characteristics significantly
- The catalytic modified devices showed consistency in electrodeposition
- Electrochemical Impedance Spectroscopy (EIS)
 - The catalytic layer did not change the impedance of the Pt electrode
 - The EIS data showed that each successive layer reduced the impedance of the blank device compare to the catalytic layer modified device
 - The overoxidation data showed that the impedance of both devices are similar regardless of catalytic layer
- In vitro* dose response to glucose, showed that the blank device has a higher sensitivity (0.94 nA/mM) than the catalytic modified device (0.32 nA/mM)
- In vivo* response to glucose and lactate showed that the device with **no catalytic** layer had ~5x (3.05 nA/mM vs. 0.67 nA/mM) the sensitivity to glucose and ~4x (1.95 nA/mM vs. 0.57 nA/mM) the sensitivity to lactate
- The hydrogel coated device showed a greater sensitivity to glucose and lactate over the non hydrogel coated device

5. Key References

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