

10-5-2004

Biological lubricant composition and method of applying lubricant composition

Julie-anne Mason Burdick

Martine Laberge

Gary Lickfield

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US006800298B1

(12) **United States Patent**
Burdick et al.

(10) **Patent No.:** **US 6,800,298 B1**
(45) **Date of Patent:** **Oct. 5, 2004**

(54) **BIOLOGICAL LUBRICANT COMPOSITION AND METHOD OF APPLYING LUBRICANT COMPOSITION**

(75) Inventors: **Julie-Anne Mason Burdick**, Gilbert, AZ (US); **Martine Laberge**, Seneca, SC (US); **Gary Lickfield**, Easley, SC (US)

(73) Assignee: **Clemson University**, Clemson, SC (US)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

(21) Appl. No.: **09/569,009**

(22) Filed: **May 11, 2000**

(51) **Int. Cl.**⁷ **A61K 9/16**; A61K 9/50; A01N 43/04

(52) **U.S. Cl.** **424/489**; 424/1; 424/450; 424/213.3; 424/402; 424/490; 514/54; 514/59; 536/112

(58) **Field of Search** 514/54, 59; 536/112; 264/4.32, 4.33; 424/450, 1, 489, 490, 213.3, 402.21, 24

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Primary Examiner—Jeffrey Fredman

(74) *Attorney, Agent, or Firm*—Dority & Manning, P.A.

(57) **ABSTRACT**

Fluid compositions and methods for lubrication of mammalian joints are disclosed, including both natural and artificial fluids. Synovial fluid acts to lubricate the bearing surfaces of bones and bone-like structures which are held in frictional contact within biological joints. Such fluids may be used to treat arthritic, injured, and diseased joints. Synovial fluid containing a dextran-based hydrogel with lipids provides enhanced rheological and tribological properties of such a fluid. Phospholipids are particularly useful in dextran-based compositions for synovial fluid. One phospholipid that can be used advantageously in synovial fluid is dipalmitoyl phosphatidylcholine (DPPC).

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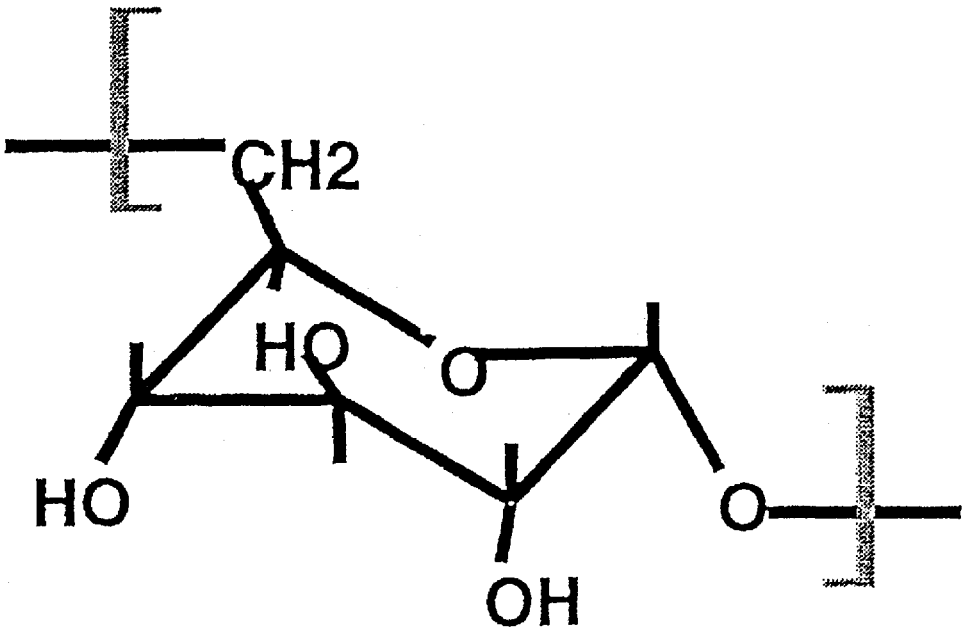


Figure 1 Chemical Structure of Dextran

BIOLOGICAL LUBRICANT COMPOSITION AND METHOD OF APPLYING LUBRICANT COMPOSITION

FIELD OF THE INVENTION

This invention relates to compositions, methods and apparatus for lubrication of mammalian joints, both natural and artificial.

BACKGROUND OF THE INVENTION

Synovial fluid acts to lubricate the bearing surfaces of bones and bone-like structures which are held in frictional contact within joints. Synovial fluid lubricates tendons, cartilage, bones, ligaments, and other biological structures that move within the body relative to each other. The human knee is an example of a joint that uses synovial fluid advantageously to provide for lubrication and for friction reduction. Synovial fluid is naturally excreted into the cavity of the joint in a normal healthy knee.

There are publications disclosing the use of propylene glycol and phospholipids in synovial fluid. For example, PCT publication WO 97/22345 to Hills et al. provides a discussion of a method of lubrication of synovial fluid by administering a composition comprising a mixture of phospholipids and propylene glycol. Another publication, PCT publication 89/01777 discloses using hyaluronic acid in saline solution as a lubricant for joints. Hyaluronic acid compositions may reduce the coefficient of kinetic friction between surfaces in contact with each other, and in particular, load bearing surfaces. Another publication, EP 0 767 212A1, is directed to a process for producing an aqueous solution of phosphorycholine group bearing polymer. This publication is directed to producing such compositions as starting materials for cosmetics having skin beautifying effects, and as contact lens cleaning agents.

U.S. Pat. No. 5,902,800 to Green et al. describes pharmaceutical compositions containing dextran, and a method for treatment of joint inflammation and pain brought about by arthritis, physical trauma, or infection using such dextran-containing formulations. The method comprises administering a bimodal molecular weight dextran formulation in conjunction with drugs or pharmaceuticals, such as corticosteroids, anti-inflammatory drugs, and antibiotics to enhance the effect of dextran in relieving pain and inflammation in an inflamed joint.

SUMMARY OF THE INVENTION

The present invention may be presented in many different embodiments, and representative embodiments are described herein. The invention is not limited to only those embodiments described, and a person of skill in the art may readily apply the invention in other ways that are apparent from this specification. Numerous examples are provided, but the invention is not intended to be limited to only those examples provided.

The invention generally comprises a biologically compatible lubricant composition useful for; injecting into damaged or diseased joints, filling cavities and spaces in artificial joints, applying to joints in connection with post-surgical procedures, and other applications in which a synovial fluid having good lubricity and biocompatibility is desirable. Treatment of osteo-arthritis joints is one application for compositions of this invention. In other applications, a composition may be injected following a joint injury, as a

visco-supplementation. The compositions may be used as lubricants in artificial joints following total joint replacements. Further, the compositions may be used for maintenance of an artificial joint to minimize wear of bearing surfaces in humans or mammals. In some applications, the compositions may be used to investigate or measure the wear performance of artificial joints in vitro in a joint simulator for research purposes.

The composition generally comprises an effective amount of dextran and a lipid. In one aspect of the invention, the lipid may be selected from the group of lipids comprising: lipopolysaccharides, sphingolipids, glycolipids, phosphatidylcholines, phosphatidyl ethanolamines, sphingomyelins, phosphatidyl inositols, phosphatidyl serines, phosphatidylethanolamine, phosphatidylserine, phosphatidylglycerol, phosphatidylinositol, sphingomyelin, dipalmitoyl phosphatidylcholine (DPPC), and phosphatidylcholines.

In one embodiment of the invention, the composition is presented which has a rheology of the fluid between about 1 and 20 Pa (sec) at a temperature range of about 25–45 C. The dextran typically comprises less than 40% by weight of the solution, and more preferably about 20% by weight, and still more preferably about 10% by weight or less.

In another aspect of the invention, a synthetic synovial fluid is disclosed comprising dextran and a phospholipid. In many instances the fluid comprises a crosslinked hydrogel. Many different phospholipids work well in this composition, and one desirable phospholipid is dipalmitoyl phosphatidylcholine (DPPC), which is further discussed in connection with the Example below.

A method of lubricating a joint or other physiological articulation is also presented by way of this invention. The method generally comprises administering to a joint or articulation in an effective amount of a composition comprising one or more phospholipids and dextran-based hydrogel which acts as a carrier. The method may be applied in instances for which the joint is a natural joint, or an artificial joint. In one application, the method may be applied in which the administration of the composition follows a total joint replacement operation. In one aspect of the invention, the method may include applying the lubricant compositions into an artificial joint simulator to simulate wear performance of the joint.

BRIEF DESCRIPTION OF THE DRAWING

The invention may be better understood by reference to the following drawing:

FIG. 1 shows a simplified schematic of dextran, which is used in the compositions of the invention.

DETAILED DESCRIPTION OF THE INVENTION

Reference now will be made to the embodiments of the invention, one or more examples of which are set forth below. Each example is provided by way of explanation of the invention, not as a limitation of the invention. In fact, it will be apparent to those skilled in the art that various modifications and variations can be made in this invention without departing from the scope or spirit of the invention. For instance, features illustrated or described as part of one embodiment can be used on another embodiment to yield a still further embodiment. Thus, it is intended that the present invention cover such modifications and variations as come within the scope of the appended claims and their equiva-

lents. Other objects, features and aspects of the present invention are disclosed in or are obvious from the following detailed description. It is to be understood by one of ordinary skill in the art that the present discussion is a description of exemplary embodiments only, and is not intended as limiting the broader aspects of the present invention, which broader aspects are embodied in the exemplary constructions.

In one aspect of this invention, a hydrogel made from polysaccharides is employed to serve as a carrier for phospholipids, which are organic molecules found naturally in synovial joints such as the shoulder and knee. Phospholipids contribute to the lubricating properties of articular cartilage provided by the synovial fluid in normal joints.

Hydrogels are polymers that swell when exposed to water. Some hydrogels are made from dextran, a polysaccharide that has been used in the prior art as a plasma expander and a drug carrier. To fabricate the gels of this invention, dextran may be coupled with glycidyl methacrylate. Gelation may occur using an initiator system of ammonium peroxydisulfate and N, N, N', N'-tetramethyl-ethylene diamine.

Natural joint lubrication is a complex process that allows the joint to operate in different conditions. Such conditions include: joint surface velocity and load applied on the joint. At high loads and low velocity, boundary lubrication is used as a means to protect the surfaces and minimize their contact (this is termed boundary lubrication). At higher velocities, a fluid film is generated between the surfaces because of pressure build-up, and completely separates the surfaces. This is termed fluid film lubrication. Since cartilage is highly deformable under pressure, this deformation may enhance the thickness of the fluid film. This process is sometimes termed an elastohydrodynamic lubrication mechanism. Articular cartilage is filled with "water" that is squeezed from the surface upon loading.

Synovial fluid in the joint is necessary for effective levels of fluid film lubrication which is the primary lubrication mechanism at high speeds. In conditions of low speed, high load and rest, this mechanism is assisted by boundary lubrication achieved in a layer of molecules attached to the surface of the cartilage, also known as surfactant. These molecules act as a protective layer for the cartilage surfaces and basically provide the final line of defense against destructive contact and possibly wear of the articular cartilage.

The different types of phospholipid adsorbed onto the surface of cartilage have been isolated by extraction and identified by chromatography on silica gel paper and mass spectroscopy. The primary phospholipid classes identified have been quantified by a phosphate assay. Gas chromatography and electrospray ionization mass spectrometry are sometimes used to further characterize the fatty acyl chains in each major phospholipid component and to identify the molecular species present. Phosphatidylcholine (41%), phosphatidylethanolamine (27%) and sphingomyelin (32%) comprise the major components of the lipid layer on a normal cartilage surface. When present in a carrier such as Dextran, the phospholipid molecules (single phospholipid or a mixture of phospholipids) are released and are present in the synovial cavity available for boundary lubrication (or surfactant).

Lipid-containing polysaccharide hydrogels made from dextran and phospholipids may be successfully deployed in joints. Hydrogel containing lipids with a lesser degree of cross-linking provides better lubrication properties than hydrogels with more cross-linking, or hydrogels with no lipids at all.

Polysaccharide hydrogels can be organic carriers for entrapped phospholipids. A potential use for the hydrogels containing lipids could be as a replacement lubricant in synovial joints, including degenerated and artificial joints.

People who suffer from the pain and loss of mobility due to diseased joints may benefit from implants designed to improve their situation. Orthopedic implants made from natural polymers and incorporating beneficial ingredients from synovial fluid may alleviate the decreased motion in these joints. Biocompatibility of a material is one of the primary concerns for a successful implant. Degradable polymeric implants have advantages over non-degradable implants provided the material functions in a predictable manner and matches the properties of the tissue which it was designed to replace. For example, degradable polymers do not require removal. They also can provide temporary functions until the native tissue repairs itself. The degradation of polymeric implants can be regulated to be faster or slower, depending on the material of construction and the required functional properties. Lastly, using naturally occurring materials minimizes the body's reaction to these implants.

Hydrogels

Hydrogels are water-swollen polymers made from natural or synthetic materials. They are made from monomers either by chemical reaction using a cross-linking agent, or by exposure to radiation such as electron beams, gamma radiation, X-rays, and ultraviolet light. The cross-linking forces that hold hydrogels together include: ionic interactions, hydrogen bonding, hydrophobic interactions, and van der Waals forces. The water content of the gel provides these materials their advantageous mechanical and surface properties. Further, it sometimes dictates their interaction with biological surfaces.

Generally, hydrogels degrade by two main mechanisms: physical (e.g., fracture) or chemical (e.g., hydrolysis, enzymatically). Several factors contribute to the rate of their degradation including the chemical composition, degree of swelling, the presence of enzymes, pH, and temperature. The degradation of hydrogels is mostly controlled by the degree of swelling which is determined by hydrophilicity and degree of cross-linking.

Degradation of Hydrogels

Hydrogels have been studied for their potential for controlled degradation. A synthetic synovial fluid must degrade at an acceptable rate to effectively serve as a carrier. Co-polymers, especially, have been formulated to control the rate of degradation. Some researchers have produced interpenetrating network polymers from polyethylene glycol (PEG) and dextran. These researchers have studied the in vitro degradation of the PEG/dextran hydrogel in the presence of papain and dextranase, two enzymes known to hydrolyze the respective polymers. The resulting degradation was due to the structure of the co-polymer, not just the presence of the enzymes.

PEG/alpha-hydroxy acids (i.e., polylactic acid [PLA] or polyglycolic acid [PGA]) have a degradation time by hydrolysis which varies from less than 1 day to up to 4 months.

Polysaccharide Hydrogels

Hydrogels made from polysaccharides, naturally hydrophilic substances, are attractive biomaterials because they

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are less likely to cause the adverse reactions observed with synthetic polymers. Several polysaccharides have been identified in the literature for their use in drug delivery.

Dextran-Based Hydrogels

Dextran is a D-glucose polysaccharide which is produced commercially by *Leuconostoc mesenteroides* bacteria. As shown in FIG. 1, the structure of dextran consists of a central ring containing hydroxyl functional groups which can be used for chemical derivatization. Synovial fluid is a dialysate derived from blood plasma. As a material, it has an egg-white consistency and has non-Newtonian characteristics: its viscosity decreases with increasing shear rate. Normal synovial joints contain about 0.13 to 3.5 ml of synovial fluid. Joint disease can cause the volume of synovial fluid to increase up to 200 ml.

Dipalmitoyl phosphatidylcholine (DPPC) is a phospholipid which has a polar head group and hydrophobic fatty acid tail. Phosphatidylcholine contains a glycerol backbone, two fatty acid chains, and a phosphorylated alcohol (choline). In the dipalmitoyl structure, the fatty acid portion consists of saturated C16 hydrocarbon chains. The concentration and content of synovial fluid changes in diseased joints. In particular, the volume and lipid concentration of synovial fluid in osteoarthritic (OA) and rheumatoid arthritic (RA) joints can increase significantly over normal joints.

Synovial Fluid

Synovial fluid performs several tasks in the synovial joint. For example, it is the source of nutrients for the articular cartilage. It carries metabolic substances to the chondrocytes and provides the waste removal from these cells. Because synovial fluid fills the joint space, it provides hydration to the tissues in the joint. Synovial fluid also functions in lubrication, load bearing, and shock absorption within the joint. The Theological properties of synovial fluid are responsible for optimum joint lubrication.

Synovial fluid may act as a shock absorber, particularly under high loads when the inherent molecules undergo conformational changes. The energy of conformation is stored and released later. In contrast, the molecules serve as lubricants at low loads because they are flexible enough to maintain their conformation.

Diseased Synovial Fluid

Diseased synovial fluid has decreased rheological properties and therefore does not fulfill its normal functions of lubrication and shock absorption. Normal synovial fluid behaves in a non-Newtonian manner: viscosity decreases as shear rate increases. In diseased joints, the synovial fluid's overall viscosity is lowered and it does not display the non-Newtonian behavior. Thus, in one aspect of this invention, an artificial synovial fluid composition is proposed which can provide a viscoelastic or visco-supplementation to a diseased synovial joint. This provides necessary lubrication and may relieve pain.

Synthetic Synovial Fluid

The degeneration or absence of synovial fluid for patients with joint diseases or artificial joints affects their mobility. These patients benefit from a synthetic material which can mimic synovial fluid properties. Particularly, the compositions of this invention do not cause an adverse tissue reaction, and yet contain components naturally found in synovial fluid. Also, the compositions of this invention have

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a viscosity compatible with natural synovial fluid, and provide similar frictional properties (i.e., lubrication) as the natural materials.

The body does not have a natural enzyme which degrades dextran. Therefore, it has been surprisingly discovered that by using dextran-based hydrogels, one may effectively increase the length of time a hydrogel made from dextran remains intact. In addition, the polysaccharide-based gel of this invention advantageously does not require additional surgeries to remove the material.

Phospholipids are responsible for the lubricating properties of synovial fluid. Phospholipids are the most abundant molecules used as surfactants by the body, they enhance boundary lubrication properties. Also, they are involved in the lubrication and protection of synovial articular cartilage. Further, DPPC phospholipids are particularly useful in the compositions of this invention for incorporation into the polysaccharide hydrogel.

Procedure to Make Dextran-Based Hydrogels

1. Synthesize the Dextran

Operating conditions:

Nitrogen atmosphere

Room temperature Stir for 48 hours

Ingredients:

25 grams dextran (dex) [40,000 m wt: Sigma #D-1662]
225 mL of dimethyl sulfoxide (DMSO) [Aldrich #27,685-5]
5 grams 4 (N, N¹-dimethylamino) pyridine (i.e. "DMAP") [Sigma #D5640]; amount of glycidyl methacrylate (GMA) [Sigma #M-1157] depends on desired degree of substitution.

For DS-14 (14 percent molar ratio GMA: dextran) add 3.1 mL glycidyl methacrylate; For DS-28 (28 percent molar ratio glycidyl methacrylate: dextran): add 6.1 mL glycidyl methacrylate.

Then, stop the reaction with 37% hydrochloric acid based on the molar ration of HCl to DMAP:

Operating Conditions:

Room temperature

Ambient atmosphere

Stir for 5 minutes

Ingredients:

Add 3.4 mL HCl to each flask.

Separation of the Dex-glycidyl Methacrylate from DMSO:

-Transfer the thickened solutions to 4-5 dialysis tubes (Sigma #250-7U); place the 2-3 dialysis tubes in 1L beakers filled with deionized water; keep the DS-14 and DS-28 dialysis tubes in separate beakers; cover the beakers with Parafilm® to minimize DMSO odors.

Operating Conditions:

Temperature=4 C

Ambient atmosphere.

Dialyze for 14 days; change the de-mineralized water at least 4 times; freeze-drying the dex-GMA: Transfer the 4-5 dialysis tube contents to nine 50-mL centrifuge tubes; place the capped centrifuge tubes in 20 C freezer for 24 hours; uncap the centrifuge tubes and put them in lyophilizer containers to freeze-dry for up to 72 hours; keep the DS-14 and DS-28 centrifuge tubes in separate containers. Then, re-cap the centrifuge tubes containing the freeze-dried fluffy product and store them in 20 C freezer until use.

2. Preparing the Hydrogels:

Make aqueous solutions:

500 mL of a 0.2M phosphate buffer solution (pH=8.5) from Na₂HPO₄ (m wt 141.96); 14.2 grams Na₂HPO₄ pow-

der; 500 mL deionized water; Adjust the pH with 1M HCl or NaOH; 50 mL of 0.1M ammonium persulfate (APS) solution:

1.255 grams APS [Aldrich #24,861-4]; 50 mL of phosphate buffer from above 50 mL of 0.067 M (N,N,N,N')-tetramethylethylenediamine (TEMED); 0.5055 mL TEMED [Sigma #T-8133]; 50 mL of phosphate buffer from above.

Prepare a paste of dipalmitoyl phosphatidylcholine lipid (DPPC): [Sigma #P-0763] and phosphate buffer (pH=8.5); put 1 gram DPPC in 20 mL vial; add phosphate buffer (pH=8.5) dropwise; stir with a spatula until the mixture has a toothpaste-like consistency.

Non-sterile Technique for Hydrogel Formation:

Without lipids—makes a 1.2 mL hydrogel (approximately); weigh 100 milligrams dextran-GMA; add 1 mL phosphate buffer; add 100 μ L APS solution; add 100 μ L TEMED solution; swirl container to mix contents then set container on level surface or draw solution into a syringe; hydrogel will form in approximately 30 minutes at room temperature.

With lipids—makes 1.5 mL hydrogel (approximately); weigh 100 milligrams dex-GMA.

Measure a 0.36 mg (rice grain-size) of dipalmitoyl phosphatidylcholine lipid (DPPC) [Sigma #P-0763]/phosphate buffer paste made in step 2b above; add 1 mL phosphate buffer; shake container to suspend lipids in phosphate buffer; add 200 μ L APS solution; add 200 μ L TEMED solution; swirl container to mix contents swirl container to mix contents then set container on level surface or draw solution into a syringe; hydrogel will form in approximately 30 minutes at room temperature.

Sterile technique for hydrogel formation: without lipids—makes a 1.2 mL hydrogel (approximately); weigh 100 milligrams dex-GMA Add 2 mL phosphate buffer; syringe filter this dex-GMA/phosphate buffer solution into one well of a 6-well culture plate using a 0.45 micron filter (Pall-Gelman Supor Acrodisc®); syringe filter the APS solution into one well of a 6-well culture plate using a 0.2 micron filter (Pall-Gelman Supor Acrodisc®); syringe filter the TEMED solution into one well of a 6-well culture plate using a 0.2 micron filter (Pall-Gelman Supor Acrodisc®); add 100 μ L of the filtered APS solution to the phosphate/dex-GMA mixture; add 100 μ L filtered TEMED solution to the phosphate/dex-GMA mixture; swirl container to mix contents then set container on level surface or draw solution into a syringe; hydrogel will form in approximately 30 minutes at room temperature; with lipids—makes a 1.5 mL hydrogel (approximately).

Weigh 100 milligrams dex-GMA; measure approximately 0.36 mg (rice grain-size) of dipalmitoyl phosphatidylcholine lipid (DPPC) [Sigma #P-0763]/phosphate buffer paste made in step 2b above Add 1 mL phosphate buffer; shake container to suspend lipids in phosphate buffer; syringe filter this dex-GMA/phosphate buffer solution into one well of a 6-well culture plate using a 0.45 micron filter (Pall-Gelman Supor Acrodisc®); syringe filter the APS solution into one well of a 6-well culture plate using a 0.2 micron filter (Pall-Gelman Supor Acrodisc®); syringe filter the TEMED solution into one well of a 6-well culture plate using a 0.2 micron filter (Pall-Gelman Supor Acrodisc®); add 200 μ L of the filter APS solution to the phosphate/dex-GMA mixture; swirl container to mix contents then set container on level surface or draw solution into a syringe; hydrogel will form in approximately 30 minutes at room temperature.

EXAMPLE

Synovial fluid can be reconstituted based on an adapted technique. Five solutions (pH=7) containing a fixed amount

of high purity hyaluronic acid (Genzyme Corporation, Cambridge, Mass.) (1.7×10^6 Daltons, 2.84 mg/ml or 0.287%) dissolved in aqueous sodium chloride solution (0.85% (w/v)) containing 0.05% sodium azide were made to contain physiologically significant amounts of DPPC (0.0, 0.025, 0.2 (normal), 0.4, (osteoarthritis (OA)), 0.8 (rheumatoid arthritis (RA) mg/ml). Phospholipid concentrations were verified using a phosphate assay against a set of standards in a UV/VIS spectrophotometer (Model 219 Cary, Varian Associates, Sunnyvale, Calif.). The viscosity of each solution was measured using a cup and bob rheometer (Epprecht-Contraves Rheomat 15T, Mettler Corp., Cincinnati, Ohio). Viscosity measurements were taken at various shear rates, while the temperature was held constant at 23 C.

It is possible to evaluate the ability of dipalmitoyl phosphatidylcholine (DPPC) to lower the coefficient of friction (μ) between rigid bearings when acting as a boundary lubricant at stresses in the range experienced by weight-bearing joints (3.5, 4.5, and 5.5 MPa). Friction tests were conducted in a fluid environment simulating different stage of synovial degeneration using the solutions previously described for the Theological analysis. A specially designed pin-on-plate friction table was used for friction testing. Two glass cylindrical pins (1 cm \times 2.5 cm) were fastened to a small steel plate upon which weights were placed to apply equal loading to each of the nominal line contacts on a flat glass plate. The arrangement of the pins allowed the upper surface to be self-supported and thus avoiding the interference of mechanical constraints on the friction force measurements.

Strain gages were mounted on the upper surface to provide a friction force transducer. The output from the strain gages were amplified, then collected and calibrated using an analog-to-digital converter (National Instruments) and a personal Macintosh IIsi computer with a data analysis software package (LabView II by National Instruments). The raw signal was filtered to remove vibrations not related to friction. The signals from the friction force transducers are compared before and after filtering. Borosilicate glass (Pyrex™) was used as the non-deformable bearing materials for friction studies. Since Pyrex™ has an elastic modulus of 62.7 GPa and poisson's ratio of 0.2, effects of hysteresis friction are negligible.

Phosphatidylcholine, which is the backbone of the phospholipid structure, has been shown to orient in organized bilayers on this material. Using a stroke of 75 mm and a frequency of 0.2 Hz, a maximum entraining velocity of 30 mm/sec which is the minimum speed range required for fluid film lubrication, the static and dynamic coefficient of friction were measured for each sinusoidal cycle for 5 minutes for 0, 100, 1000, 2000, and 3000 cycles. From the transient friction force measurements, the coefficient of friction at the point of maximum entrainment velocity was calculated for each experiment. Non-contact profilometry with a 20 \times Linnik magnification head was used to observe a roughness average of 2.27 0.58 nm (Peak-to-Valley of 19.65 7.09 nm) for the glass rods and plates (Topo-3D™ by Wyko, Corp. Tuscon, Ariz.).

Five experiments were conducted for each loading condition. After testing, the topography of the surfaces were examined with scanning electron microscopy and non-contact profilometry. A phosphate assay was also performed to evaluate the transfer of DPPC from the solution onto the glass surface. A statistical general linear model (GLM) was used to analyze the effect of DPPC concentration and loading on the coefficients of friction.

The results revealed that the viscosity of reconstituted synovial fluid is significantly dependent on the concentration of phospholipid. However, the depletion of lipid in the solution did not change the thixotropic behavior of the fluid and its non-newtonian character as a function of shear rate. Results from the friction study indicate that the presence of phospholipid in synthetic synovial fluid significantly decreases the coefficient of friction between rigid bearings. It appears that the conditions used did not provide for the formation of a fluid film between the bearings and that a transfer of DPPC molecules onto the glass bearings protective layer. The concentration, however, had no effect on the coefficient of friction; indicating that the amount of phospholipid does not influence the effectiveness of lubrication under conditions favorable to hydrodynamic and boundary lubrication. Boundary lubrication contributes significantly to the protection of bearing surfaces in adverse conditions which do not permit fluid film lubrication.

Thus, it has been shown that DPPC can effectively protect surfaces and reduce the coefficient of friction between glass surfaces. This study also shown that DPPC is effective in protecting the surface against wear. Boundary lubrication is an effective method to protect total joint replacement surfaces providing that they can attract a boundary surfactant.

Hydroxyl groups on the dextran chain are acryloylated (i.e., activated) using the glycidyl methacrylate ("GM"). In general, a rheometer is used to measure flow properties of fluids. One of these properties is viscosity. The units for viscosity are Pascal (seconds).

One advantage of using dextran in the compositions of the invention is that it will be slowly broken down. In arthritic human joints, there usually is a significant amount of hyaluronidase that will considerably speed up the degradation of hyaluronic acid. Therefore, lipid molecules can be released with time to replenish the surfaces of the joint.

It is understood by one of ordinary skill in the art that the present discussion is a description of exemplary embodiments only, and is not intended as limiting the broader aspects of the present invention, which broader aspects are embodied in the exemplary constructions. The invention is shown by example in the appended claims.

What is claimed is:

1. A biologically compatible injectable lubricant composition, comprising:

- (a) a dextran-based hydrogel component, said dextran-based hydrogel component being adapted for serving as a carrier wherein said dextran-based hydrogel comprises a dextran/glycidyl methacrylate copolymer hydrogel;
- (b) a suspension consisting of one or more phospholipids entrapped in the dextran-based hydrogel; and
- (c) wherein said dextran is less than about 40% of the injectable lubricant composition by weight.

2. The composition of claim **1** in which said suspension of phospholipids comprises a phosphatidylcholine-based compound.

3. The composition of claim **2** wherein said phosphatidylcholine-based compound comprises dipalmitoyl phosphatidylcholine (DPPC).

4. The composition of claim **1** in which the rheology of the injectable lubricant composition is between about 1 and about 20 Pa(sec) at a temperature range of about 25–45° C.

5. A synthetic synovial fluid comprising:

- (a) a dextran-based hydrogel carrier component comprising a dextran coupled with glycidyl methacrylate, and
- (b) a suspension consisting of one or more phospholipids entrapped in the dextran-based hydrogel, wherein said

one or more phospholipids are capable of contributing to the lubricating properties of articular cartilage.

6. The fluid of claim **5** wherein said one or more phospholipids is selected from the group of phospholipids consisting of:

phosphatidyl cholines, phosphatidyl ethanolamines, and mixtures thereof.

7. The fluid of claim **6** wherein the suspension of phospholipids comprises dipalmitoyl phosphatidylcholine (DPPC).

8. An injectable synovial fluid composition comprising:

(a) a dextran-based hydrogel component wherein said dextran-based hydrogel comprises a dextran/glycidyl methacrylate copolymer hydrogel, and

(b) a suspension consisting of one or more phospholipids entrapped in the dextran-based hydrogel, said one or more phospholipids being selected from the group of phospholipids consisting of: dipalmitoyl phosphatidylcholine (DPPC), phosphatidylethanolamine, phosphatidylserine, phosphatidylglycerol, phosphatidylinositol, sphingomyelin alpha-dipalmitoyl phosphatidylcholine, and mixtures thereof.

9. The composition of claim **8** wherein said suspension of phospholipids comprises dipalmitoyl phosphatidylcholine (DPPC).

10. The injectable synovial fluid composition of claim **8** wherein the dextran comprises from about 10 to about 40 percent by weight of the injectable synovial fluid composition.

11. The injectable synovial fluid composition of claim **8** wherein the dextran comprises between about 10 and about 20 percent by weight of said injectable synovial fluid composition.

12. An injectable liquid synovial fluid composition comprising:

(a) a first component comprising a hydrogel matrix comprising dextran coupled with glycidyl methacrylate; and

(b) a suspension consisting of dipalmitoyl phosphatidylcholine entrapped within the hydrogel matrix.

13. The composition of claim **12** wherein the rheology of the injectable synovial fluid is between 1 and 20 Pa(sec) at a temperature range of 25–45° C.

14. The composition of claim **12** additionally comprising a phosphate buffer.

15. A biologically compatible joint composition formed by combining:

(a) a dextran-based hydrogel comprising dextran coupled with glycidyl methacrylate; and

(b) one or more phospholipids, to form a suspension consisting of one or more phospholipids in the hydrogel, said one or more phospholipids being selected from the group of phospholipids consisting of: dipalmitoyl phosphatidylcholine (DPPC), phosphatidylethanolamine, phosphatidylserine, phosphatidylglycerol, phosphatidylinositol, sphingomyelin alpha-dipalmitoyl phosphatidylcholine, and mixtures thereof.

16. The composition of claim **1**, wherein the dextran is between about 10% and about 40% of the injectable lubricant composition by weight.

17. The composition of claim **1**, wherein the dextran is less than 10% of the injectable lubricant composition by weight.

18. The fluid of claim **5**, wherein the dextran is less than 40% of the synthetic synovial fluid by weight.

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19. The fluid of claim **5**, wherein the dextran is between about 10% and about 40% of the synthetic synovial fluid by weight.

20. The fluid of claim **5**, wherein the dextran is less than 10% of the synthetic synovial fluid by weight.

21. The fluid of claims **5**, wherein the dextran-based hydrogel is a degradable polymer.

22. The injectable synovial fluid composition of claim **8**, wherein the dextran is less than 10% by weight of the injectable synovial fluid composition.

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23. The composition of claim **12**, wherein the dextran is less than 40% of the composition by weight.

24. The composition of claim **12**, wherein the dextran is less than 10% of the composition by weight.

25. The composition of claim **15**, wherein the dextran is less than 40% of the composition by weight.

26. The composition of claim **15**, wherein the dextran is less than 10% of the composition by weight.

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