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Semi-automatic segmentation and surface reconstruction of CT images by using rotoscoping and warping techniques

Segmentation and surface reconstruction of CT

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Abstract

Background: Quick and large-scale segmentation along with three-dimensional (3D) reconstruction is necessary to make precise 3D musculoskeletal models for surface anatomy education, palpation training, medical communication, morphology research, and virtual surgery simulation. However, automatic segmentation of the skin and muscles remain undeveloped.

Materials and methods: Therefore, in this study, we developed workflows for semi-automatic segmentation and surface reconstruction, using rotoscoping and warping techniques.

Results: The techniques were applied to multi detector computed tomography images, which were optimized to quickly generate surface models of the skin and the anatomical structures underlying the fat tissue.

Conclusions: The workflows developed in this study are expected to enable researchers to create segmented images and optimized surface models from any set of serially sectioned images quickly and conveniently. Moreover, these optimized surface models can easily be

modified for further application or educational use.

Key words: cross-sectional anatomy, segmentation, surface reconstruction, three-dimensional imaging, landmark, surface anatomy, rotoscopy

INTRODUCTION

Segmentation and surface reconstruction of anatomical structures from medical images form an essential step for designing a surgical plan or conducting a morphological research.

Several methods and softwares have been developed for segmentation and surface reconstruction [8,9,5,17,31]. However, automatic segmentation of the skin and the muscles remain undeveloped owing to the ambiguous boundaries between them and the neighbouring structures.

Superficial anatomy is based on projections of the major organs of human body, with the help of surface landmarks. It deals with anatomical features that can be observed by sight, without dissection. In addition, it includes the theories and systems pertaining to the proportions of the human body and location of surface landmarks that may relate to the deeper anatomical structures. [15,19,29,30,1,2,4,7,20,10,18,16].

In this study, we developed workflows for semi-automatic segmentation and surface reconstruction with the help of rotoscopy and warping techniques, derived from the field of graphic design and animation. By using the workflows developed in this study, optimized and small-sized surface models with respect to superficial anatomy can be made. These surface models can be 3-dimensionally displayed in a portable document format (PDF) file. Additionally, the surface models and stereoscopic structures can be related with the displayed landmarks in real time [25,26,24,28,27].

The workflows developed in this study are expected to enable researchers to create segmented images and optimized surface models from any set of serially sectioned images quickly and conveniently. Moreover, they can be translated into different formats, and easily modified for further application or educational use owing to their small file size and optimized surface structure.

MATERIALS AND METHODS

(1) Semi-automatic segmentation

Multi detector computed tomography (MDCT) scans (Siemens, SOMATOM definition AS+128; resolution: 512 X 512, interval: 1 mm) were obtained from a 41-year-old male (stature: 1.75 m, weight: 71 kg) using; Fig. 1). The acquired MDCT images (1,332) were opened using After Effects version CC 2015 (Adobe, San Jose, California, United States). Subsequently, the skin and the anatomical structures underlying the fat tissue were outlined.

Firstly, outline of skin was drawn semi-automatically only in one of the images using 'Roto Brush tool', which was followed by automatic outlining in the next 30 to 50 images (Fig. 2).

Secondly, incorrectly generated outlines owing to the unclear skin boundaries were refined semi-automatically. They were also partially refined using the 'Roto Brush tool'. In case of the anatomical structures underlying the fat tissue, boundary between the fat, bones, and muscles were not clear than that of the skin. Therefore, the outlines in 10 to 20 images were automatically generated after manual intervention. During automatic outline generation, the unnecessary outline of inner structure, such as that of intestine, was also drawn. However, the inner outline can be removed easily in the next step of 3D reconstruction. Therefore they were ignored in this step. Consequently, 2 sets of segmented images of the skin and the structures underlying the fat tissue were constructed.

(2) 3D reconstruction

All the 1,332 segmented images of the skin and the anatomical structures underlying the fat tissue were opened using Mimics version 16.1, which has several options for surface reconstruction (Materialise, Leuven, Belgium; [25,26,24,28,27]). The segmented images were surface-reconstructed (Fig. 3a, 3b) using both the highest-quality and low-quality options of the Mimics. The highest-quality surface models have a large file size, which is difficult to display. Therefore, low-quality surface models were wrapped using the highest-quality model in the next step. As a result, two sets (highest quality and low quality) of images for the skin

and the structures underlying the fat tissue were obtained. During surface reconstruction procedure, the unnecessary inner structures that were outlined in the segmentation procedure were easily removed by means of clicking. Hence, two surface models were saved as stereolithography (STL) files, which were subsequently accessed using Maya software.

(3) Optimization and morphing

The surface models were subsequently optimized and labeled using Maya version 2018 (Autodesk, Inc., San Rafael, California, United States) and ZBrush 4 (Pixologic Inc, Los Angeles, California, United States) [26]. The imported highest-quality surface models had a more realistic shape than the low-quality surface models; however, they consisted of triangular polygonal structures with large numbers of polygons. Triangular polygonal structures are difficult to refine and label. Moreover, large files are difficult to display on multiple devices. Therefore, we used warping technique to make optimized surface models [26].

Firstly, triangular structure of the low-quality surface model was quadrangulated automatically by using 'zRemesher' function of the ZBrush software.

Secondly, the number of quadrangulated surfaces was decreased as much as possible without compromising the original shape of the anatomical structures, using the 'zRemesher' function of the ZBrush software (Fig. 3c) [26]. During this procedure, the detailed shape of the anatomical features was simplified, which was recovered in the next step.

Thirdly, the simplified regions were recovered by '3D morphing' technique using 'ShrinkWarp' function of the Maya software. The low-quality surface model was overlapped with the highest-quality surface model to recover the simplified regions (Fig. 3d) [26]. As a result, the shape obtained by the low-quality surface model changed to that of the highest-quality models. This process resulted in creation of the optimized surface models.

(4) Labeling and converting Into a PDF File

The body landmarks in the optimized surface models were annotated by anatomists. 3D spheres were made, and moved to the region of body landmarks, and named as the

landmarks [28,27]. As a result, 36 3D spheres corresponding to the body landmarks were made on the surface model, that depicted the anatomical structures underlying the fat tissue (Table 1). All the 3D spheres and the surface models were saved as STL files, which were subsequently sent to the next software package.

Surface models were arranged using Deep Exploration Standard (Right Hemisphere, San Ramon, California, United States). The arranged STL files were saved as WRL (file extension for a Virtual Reality Modeling Language (VRML) file format) files. The surface models saved in the WRL format were transported to a PDF file. We used the previously formulated and detailed transfer methods [21,30,27].

Previously, the procedure was conducted using the 3D Reviewer, a software that accompanies the Acrobat 9.0 Pro Extended (Adobe Systems, San Jose, CA) [21,23,27]. However, the use of this software is now discontinued. Thus, we used another software, Tetra4D Converter (Tech Soft 3D, Inc., Ashby Avenue Berkeley, CA) to transfer the surface models to a PDF file. The name of the surface model was displayed in the left window (model tree), while the surface model was exhibited in the right window of the PDF file (Fig.4)

RESULTS

The use of After effects, Mimics, Maya, ZBrush, and Deep Exploration Standard enabled generation of surface models for superficial anatomy of human body using MDCT images.

The surface models can be 3-dimensionally displayed in a PDF file. They can be translated into different formats and easily modified according to the purpose owing to their small size and optimized surface structure. When a user clicks a landmark point, its anatomic name is highlighted in the left tree window. Reverse highlighting is also possible, wherein clicking on text in the left tree window displays the corresponding landmarks. Additionally, the surface models and stereoscopic structures related with the landmarks can be displayed in real time.

Because of the small file size, the surface models can be used in three-dimensional

applications on mobile devices. As an example of an on-line use, we tested the real-time display performance. Unlike surface models in the PDF file, the on-line uploaded surface models can be displayed on smart phones and internet browsers [26].

The PDF file (size: 1.3 MB) is available in the form of a supplement file of this paper (supplementary). Moreover, the source files, including the original MDCT images, segmented images, surface models, and optimized surface models are available through a direct email request to the corresponding author. Our data sharing policy allows free downloading and does not require registration.

DISCUSSION

Semi-automatic outlining methods have been previously discussed using visible human dataset [23,22,11,12,14,24]. In this study, we suggested more advanced and quicker methods based on techniques of graphic design and animation. We used several software packages, namely, After Effects, Mimics, ZBrush, Maya, Deep Exploration, and Tetra4D.

Every software package has its own set of useful functions; however, no single software can contain all the necessary functions. Thus, we used multiple softwares in this study. In the segmentation step, some inner structure were automatically outlined, and some regions were incorrectly selected between the skin and the outside surface. These misselected structures, especially the unintended regions, such as the lungs, were easily deleted after surface reconstruction, using the surface-reconstruction software. Maya software aids in optimization of the images; however, the quality is not good, and the process is semi-automatic. Conversely, ZBrush software has a strong optimization function. Thus, we only used this function of the ZBrush. Deep Exploration software was used as a bridge between Maya and Tetra4D. Both these softwares has an arrange function, but the function is hard to handle. Therefore, we used the software only for arrangement.

In this study, we developed innovative and quick methods for segmentation and surface reconstruction of CT images using new techniques of graphic design and animation.

Rotoscoping is an animation technique used in motion graphics. Designers use it to trace over movie footage, frame by frame, to separate a specific region. Shape of structures in

the CT images also change smoothly like a movie. Therefore, we assumed that the image slices of body can be used as a movie sequence. Additionally, we assumed that the skin and the structures underlying the fat tissue can be the objects to be separated from the movie. Among the various rotoscoping softwares, After Effects has an automatic rotoscoping function. It automatically changes the shape of the subsequent images after drawing the shape of one image. Therefore, we used this function of the software for segmentation.

The rotoscoping technique was applied to the skin and anatomical structures underlying the fat tissue. Automatic segmentation of the fat tissue and the muscles in CT images is difficult. Many segmentation methods have been developed to segment skin, bone, heart, and air passage, as they have different Hounsfield units (HU) than the neighbouring structures. However, the HU of the muscles is almost same as that of the neighbouring structures, making their segmentation difficult [3,31,6,5,9,13,8,17].

Warping is another 3D animation technique for character motion. We used this function to optimize the surface models. Detailed surface models obtained from CT, magnetic resonance imaging, or 3D scanning, have large file sizes that cannot be displayed or handled in real time. Therefore, the surface models were reduced, however, after reduction the detailed regions disappeared. Therefore, by using the warping function in Maya software, reduced surface model was warped to detailed surface model, and the disappeared regions were recovered with reduced surfaces.

The animation techniques used in this study can segment the target structures from the neighbouring structures with similar HUs, such as all the muscles, digestive system, respiratory system. Moreover, these techniques are commonly used in the design field. Therefore, segmentation can be easily done even by a medical trainee or a student, in addition to a technician or a medical expert.

Quick and large-scale segmentation along with 3D reconstruction is necessary for designing a surgical plan or conducting a morphological research. The workflows developed in this study are expected to enable researchers to create segmented image and optimized surface models from any set of serially sectioned images quickly and conveniently. Moreover, the optimized surface models can be easily modified for further application or educational use.

Generally, CT machines are limited in terms of scan length. In this study, we used the

128-channel MDCT scanner (Siemens, SOMATOM Definition AS+128). Maximum scan length of this machine is 1.7 m, however, the height of our volunteer (corresponding author) was 1.76 m. Therefore, the image was cut at the thigh. We intend to create landmarks for the whole body in our future studies, using another scanning machine with a suitable volunteer.

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FIGURE LEGENDS

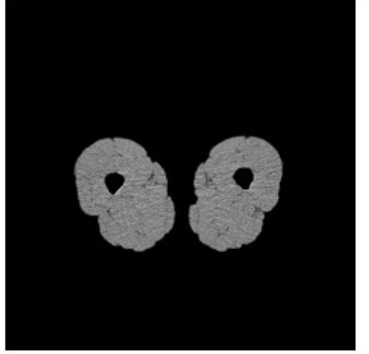
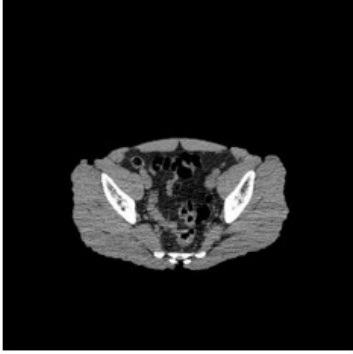
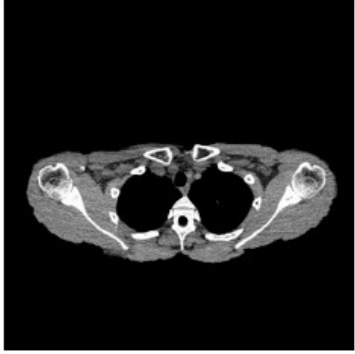
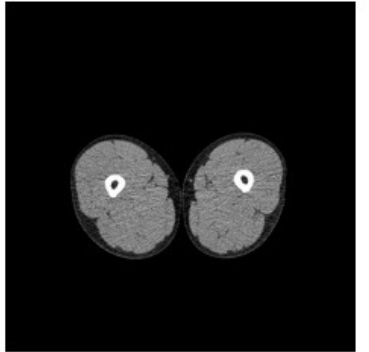
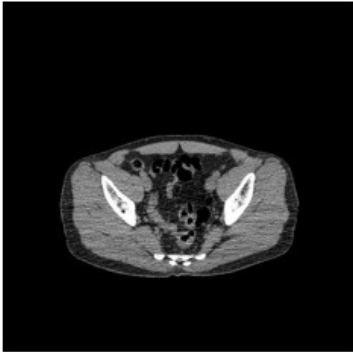
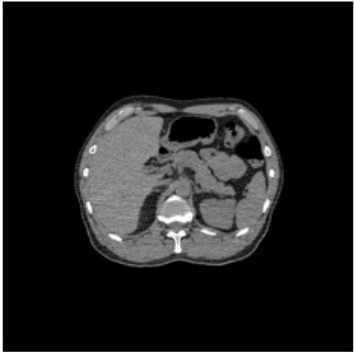
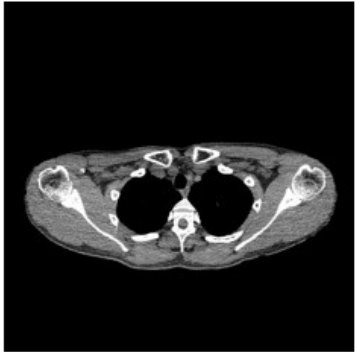
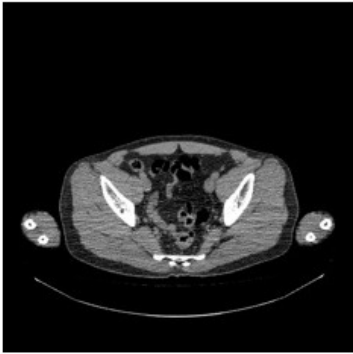
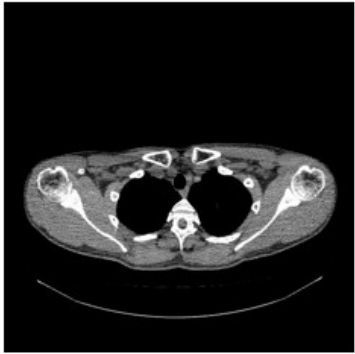
Figure 1. MDCT images: Original images (top line), segmented images of skin (middle line), and segmented images of structures underlying the fat tissue (bottom line)

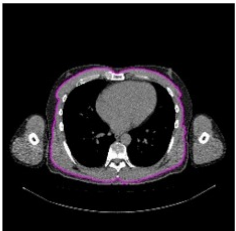
Figure 2. Outline of structures underlying the fat tissue is semi-automatically drawn in 576th and 626th images, wherein the outline of the intervening 48 images are drawn automatically using the roto-scoping technique.

Figure 3. Surface models of the anatomical structures underlying the fat tissue, front view (top line) and back view (bottom line). Highest-quality surface model (a), low-quality surface model (b), reduced surface model (c), and warped surface model (d).

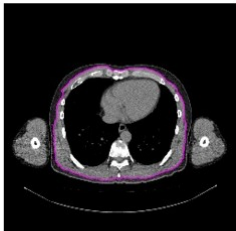
Figure 4. The name of the surface model is displayed in the left window (model tree), while the surface model is exhibited in the right window of the PDF file.

Supplementary of Fig. 4. PDF file with surface models and landmarks





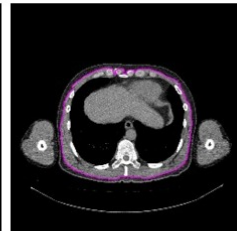
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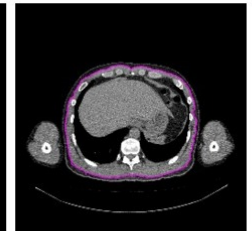
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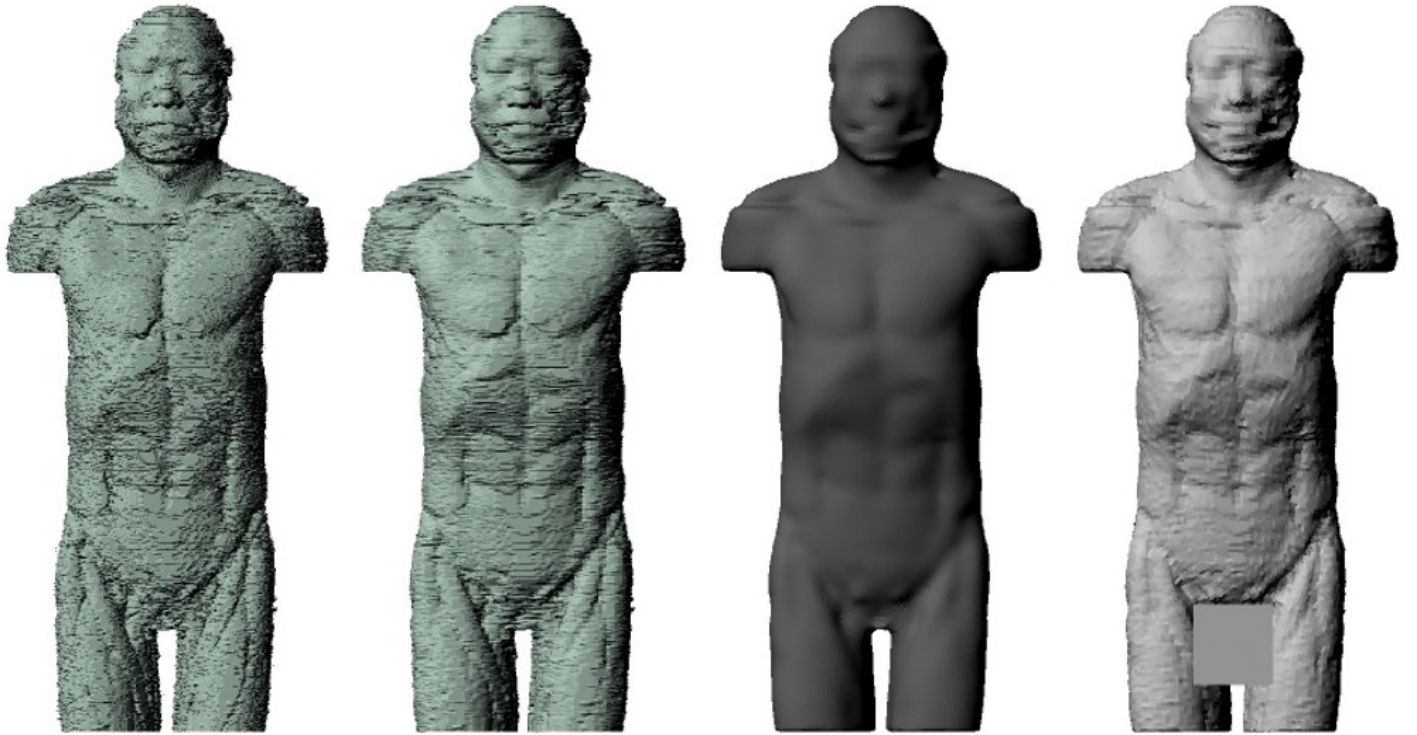
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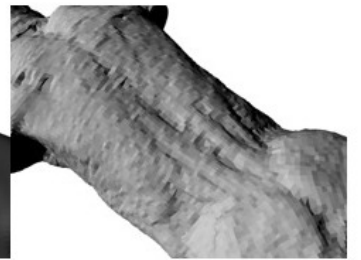
a



b



c



d

