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Measurement of Daily Energy Expenditure in Individuals with Chronic Heart Failure

 $\mathbf{B}\mathbf{y}$

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A THESIS

Presented to the Faculty of

The Graduate College in the University of Nebraska

In Partial Fulfillment of Requirements

For the Degree of Master of Science

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Under the Supervision of Professor Joseph F. Norman

University of Nebraska Medical Center Omaha, Nebraska

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Advisory Committee:

Dr. Bunny Pozehl Dr. Ka-Chun Siu

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Measurement of Daily Energy Expenditure in Individuals with Chronic Heart Failure Yanlong Li, M.S.

University of Nebraska Medical Center, 2016

Advisor: Joseph F. Norman, PT, PhD, CCS, FAACVPR

Being able to accurately monitor and quantify the amount of physical activity an individual with chronic heart failure (CHF) performs can be of assistance in developing appropriate interventions. This thesis attempted to evaluate the validity of the RT3 accelerometer (RT3) and 7-day Physical Activity Recall Questionnaire (7 day PAR) in measuring the daily activity levels of community dwelling individuals with CHF. Fifty-four individuals with CHF participated in a 7 day session to estimate their daily physical activity by using the RT3 accelerometer and 7-day PAR questionnaire. In addition, 15 of the 54 individuals participated in a second study in with the validity of RT3was compared to oxygen consumption (VO2) measured by a MedGraphics VO2000 gas analyzer during typical daily activities. Although there was no significant difference between the RT3 and VO2 on mean caloric (Kcal) expenditure (p=0.67), the accelerometer tended to underestimate the energy expenditure (EE) and its validity was affected by activity intensity, movement patterns, placement location and soft tissue adhesion. The 7-day PAR overestimated EE by 22%, when compared to the RT3. There was no significant difference in the outcomes if the 7-day PAR only focused on day time activity versus 24-hour activity which included sleep. The second study revealed that the resting metabolic rate in individuals with CHF is significantly lower than 3.5 ml/kg/min, which indicates this metabolic constant for the general population is probably not appropriate for estimating daily energy expenditure in individuals with CHF.

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Introduction:

Chronic disease is now seen as one of as the primary factors causing death or disability in both developing and developed countries. In addition, chronic diseases greatly affect individuals' living situations and daily activity levels. For those who have been diagnosed with a chronic disease or a functional limitation the most common problem is decreased physical activity tolerance. For those with multiple illnesses or various stages of symptoms, activity tolerance becomes an even greater problem. A decrease in activity can have a negative impact on an individual's cognitive abilities and moods as well.

In the past these individuals were typically treated with bedrest, activity restrictions, and medication with the goals of preventing the progression of the disease and maintaining function. However, individuals who followed this regimen demonstrated rapid decrease in their functional abilities along with further disease progression. Therefore, their caregiver started to wonder if decreasing their activity level might be the reason for the additional decline in these individuals' physical condition and the exacerbation of their symptoms.

A great deal of research has investigated whether there is a relationship between an individual's activity level and the prevalence of disability. Dianna Carroll and Elizabeth Courtney-Long³ compared adults with a disability to adults without disabilities. They found that inactivity was more prevalent among adults with a disability (47.1% versus 26.1%). In addition, inactive adults with disabilities were 50% more likely to report one or more chronic diseases than were those who were physically active. Today more and more healthcare providers and researchers are coming to believe that maintaining an individual's activity level

helps him/her maintain an independent level of function and decreases mortality.

Therefore, it is vital for physical therapists to encourage individuals to exercise to maintain their level of function, and to monitor and increase levels of activity during treatment sessions. To achieve these goals, it is critical for physical therapists to evaluate an individual's physical activity capacity and to estimate daily energy expenditures based on an individual's ability under varied environmental conditions. When making such assessments physical therapists must utilize accurate measurement methods. By doing this, physical therapists can help prevent/delay the onset of chronic disease, delay the progression of functional impairments, and improve an individual's functional abilities.

According to the World Health Organization's definition, physical activity is any bodily movement produced by skeletal muscles that requires energy expenditure. Based on this definition there are currently many methods that can be used to measure or evaluate physical activity from different perspectives. For example, individuals can complete subjective questionnaires, diaries, and surveys regarding their daily activity. Pedometers, doubly-labeled water tests, indirect calorimetry measurements and accelerometer data can also provide objective results. The validity and reliability of most of these measurement methods have been widely tested and validated. Some have limited practical application in the clinic due to the time and/or expense required to administer them. This paper reviews the most common methods that have been used to estimate physical activity capacity and then analyzes the characteristics of these measurement methods based on former research

Background of measurement methods

Measurement is the assignment of a number to a characteristic of an object or an event in order to describe its details or to make it comparable to other objects or events. Measurement can be completed via two different approaches: objective quantification and subjective assessment. Measurement systems utilize both of these approaches to varying degrees therefore all measurement methods may be classified into two main categories: objective measurement and subjective measurement.

Subjective measurement

Subjective measurement methods that address physical activity include: questionnaires, diaries, logs, and surveys. They estimate physical activity based on an individual's perception of the intensity and duration of the activity; his/her ability to use the measurement tool; and interaction with a researcher or therapist while completing the tool. Because using subjective measurement tools is relatively inexpensive and they are easier to use in large-scale studies⁴, they have been widely employed for measuring physical activity and for energy expenditure estimation. Although test results come primarily from an individual's subjective recall researchers can still treat them as reliable data and use them for comparisons among different studies. To that end, many subjective measurement methods include a standardized administration procedure⁵. Such standardized processes decrease the variability caused by an individual's personal feelings or researcher bias, thus increasing the reliability of the data/results

Based on former studies, 4,6,7 there are five factors predominantly responsible for the

validity of a subjective measurement: (1) the level of accuracy with which an individual can recall a particular memory,(2) the degree of clarity with which an individual can classify an activity by intensity, (3) an individual's confidence level when reporting an activity during an interview,(4) the appropriate interpretation based on an individual's report, and (5)the formula used for the energy expenditure calculation. These factors may affect test results to varying degrees depending on the protocol used during the subjective testing.

Therapists and researchers have made extensive use of subjective measurement techniques to gauge physical activity levels. Questionnaire-based evaluation methods and diaries have the advantage of being time efficient and easy to use. They do not require specialized knowledge on the part of the individual or the examiner regarding the proper use of a device (e.g., how to adjust the device or how to properly wear it). By simply reviewing an individual's diaries or examining a completed survey or questionnaire, evaluators can calculate an individual's activity level based on the formula associated with the measurement tool in question. Furthermore, such methods do not require an extended evaluation time on the part of either the evaluator or the individual; all that is needed is for the individual to regularly record his or her activities and report to the evaluator.

The validity and reliability of these measurement methods has been tested and the findings indicate a strong correlation between the results gathered from subjective reporting and the "gold standard" of doubly labeled water. For example, Herv &Besson and SørenBrage used doubly labeled water as a benchmark by which to gauge the validity and reliability of the Recent Physical Activity Questionnaire in terms of its ability to accurately measure energy expenditure. They found that the questionnaire had a significant association with this

benchmark method⁸. However other studies have noted limitations that may affect the validity of questionnaires, diaries, and surveys. Rajna Golubic and Anne M. May⁹ conducted a study often European countries and found that the questionnaire underestimated physical activity energy expenditures. That said, the researchers suggested that questionnaires and surveys could be a good fit for large-scale epidemiological studies. Other studies such as the one conducted by David Donaire-Gonzalez¹⁰ have indicated that surveys can be a valid tool to classify but not to quantify activity level.

Such results may be due to many factors. For example, questionnaires might not have the ability to identify those in special populations because their questions and scoring systems are based on the entire population being studied including those without disabilities or chronic diseases. Moreover, the use of these methods is highly limited by region, culture, language, and target population. As of yet, no study has shown that evaluation methods can be universally applied. Furthermore, such measurement methods require patients to use their memories to recall what activities they performed, and thus validity may be affected by incorrect recall or even by fabricated memories. In summary, such restrictions may have an impact on measurement results therefore affecting the validity of these methods

Objective Measurement

Segen's Medical Dictionary defines objective measure as, "the quantification of a physiologic or medical variable by instrumentation rather than by subjective human assessment." Compared to subjective assessment, objective measurement methods can provide more consistent and unchanging estimates that can reflect real-time performance.

Because an objective measurement directly quantifies and records biomechanical or physiological consequences it should not be affected by characteristics of either the subject or the examiner, or by the type of the instrument that is used in measuring.

Methods for objectively measuring human physical activity capacity and energy expenditure (EE) can be categorized into two major groups: direct physical measurement and direct/indirect physiological measurement. Direct physical measurement of a subject's biomechanical performance utilizes tools such as accelerometers, pedometers, or Actiheart (an accelerometer combined with a heart rate monitor). Such instruments allow researchers and therapists to estimate an individual's physical activity level based on the motion data generated from body movement over a given period of time. Generally speaking, high-intensity activity isreflected by high-motion data (activity count/step count). By using the relevant estimation equation developed throughlaboratory research therapists can transfer the activity count into energy expenditure (EE),therebymonitoring an individual's activity level and establishing a treatment plan.

The second technique for assessing the physiological results of performing physical activity is direct/indirect physiological measurement. Common methods include doubly-labeled water tests and direct/indirect calorimetry. These approaches follow varying protocols but primarily focus on measuring the human body's metabolic rate in order to estimate an individual's energy expenditure (EE) during a certain period of time. For example, the doubly-labeled water method uses isotope-labeled water to calculate amount of oxygen lost. By monitoring deuterium losses, the researcher can calculate the total amount of oxygen lost.

from the body's water pool via conversion to carbon dioxide, and thus estimate energy production. In contrast, calorimetry measures the heat eliminated or stored in the body system. Researchers can estimate the subject's energy expenditure (EE) either by directly measuring the amount of heat production in an enclosed space or by an indirect method that uses a gas analyzer to calculate oxygen consumption and carbon dioxide elimination.

Since doubly-labeled water and direct/indirect calorimetry are based on physiological changesthey provide highly reliable and valid data. Due to their high accuracy, many researchers utilize these methods and consider them to be the "gold standard" by which to compare other measurement techniques. However, since these methods necessitate that special criteria be met in order to achieve valid results, they are more commonly applied in laboratory settings rather than in clinics.

The goal of this project is to identify a method that is both highly practical for use in clinics and that can provide valid measurement results that are as accurate as direct/indirect physiological measurement. After comparing various measurement methods, the accelerometer appears to be the best choice. It appears to be able to cover both the practicability and validity aspects in clinical physical activity measurement since this method does not require special training, and its validity has already been tested on a healthy population.

The accelerometer is the primary topic of this section. Its basic principles of operation are discussed along with its validity, reliability, and influence factors. The accelerometer is also compared with other measurement methods in order to identify the practicability and validity in physical activity measurement. (For references, please see Appendix A)

Accele rometer

An accelerometer is a device that can record acceleration generated by motion along a reference axis. It was first used to investigate gait velocity and acceleration in 1950¹¹. Since then and especially following technological advances in the 1970's and going forward many studies have been conducted with the clinical utilization of the accelerometer. Research topics have included energy estimations, fall assessment/monitoring, gait assessment and posture control^{11,12,13} and the monitoring of respiration rates.^{14,15}

In spite of all of these applications, the most common usage of accelerometers is to estimate daily activity levels and energy expenditure (EE). Compared to other procedures accelerometry has shown promising possibilities when used to objectively estimate physical activity behavior¹⁶. Colbert et al. using the doubly-labeled water method as a benchmark compared it with the outcomes from 7 different energy expenditure (EE) measurement methods. They found that with an appropriate estimation equation, accelerometers provided data that was more accurate than that provided by other measurement approaches¹⁷. Moreover, the accelerometer is more economical and easier to operate than either doubly-labeled water(DLW) or direct/indirect calorimetry since it does not require an expensive or complicated device and does not requirespecific training. Because of these advantages, many European countries have incorporated accelerometers into their physical activity monitoring systems.¹⁸

In addition, due to the amount of progress that has been made regarding measurement protocols for healthy populations, current research is able to target more specific populations such as those with physical limitations or specific diseases. This field of research – which has

seen considerable activity – seeks to test the accelerometer's validity and practicability in these populations. It also aims to develop a standard measurement protocol for clinical evaluation and to identify the possible influence factors and limitations of the accelerometer with community dwelling populations.

1. Basic Principle of Accelerometer

1.1 Structure

TThe accelerometer can monitor body motion from various angles and directions by measuring acceleration along reference axes in different planes. It can provide a real-time assessment of magnitude and the total volume of movement. In addition, the accelerometer can filter out "noise" – the vibrational forces irrelevant to normal body movement via apreset cutoff frequency. Piezoresistive, piezoelectric, and differential capacitive accelerometers are the most common types of accelerometers found on the market. The piezoresistive accelerometer responds to constant acceleration and is simpler and less expensive than other types of accelerometers. Its drawbacks are temperature-sensitive drift and alower output level. The piezoelectric accelerometer is unmatched in terms of its upper frequency range, low packaged weight, and high temperature range but it is unable to detect the constant component of acceleration. Finally, the differential capacitive accelerometer is commonly used in mobile and portable systems and in consumer electronics. This is due to its low power consumption, large output level and fast response to motion.¹¹

Although many types of accelerometers are available on the market, they all operate on the same principle. An accelerometer's basic structure includes a horizontal cantilevered mass

and a seismic mass. When there is an applied acceleration, the inertial force generated from acceleration or gravity causes the seismic mass to bend or compress which causes a voltage to be sent that is proportional to the acceleration change. By calculating, transcoding, and calibrating this signal therapists and researchers can arrive at a clear picture of a patient's activity ability.¹¹

2. Guidelines for Accelerometer Selection and Placement

2.1 Accelerometer Selection

When utilizing a device as a measurement tool in research or clinical settings the most important concern is its validity and reliability. Various research studies have been conducted to confirm the accelerometer's validity and reliability. Some researchers have argued that the accelerometer and its estimation equation cannot provide a very accurate measurement estimate. ^{21, 22, 23} As evidence, they point out that some measurement processes only deliver reliable outcomes either under certain laboratory conditions ²⁴ or in a preset community environment. According to such researchers, the accelerometer tends to underestimate activity levels ^{21, 22} when used to approximate daily energy expenditures (EE's) in community dwelling living situations. They also hold that its validity is highly dependent on the type of activity that has been measured ²⁵. Even so the accelerometer is still able to demonstrate a good correlation with the "gold standard." Guy Plasquiet.al. ²⁶ has reviewed 25 articles that confirmed the accelerometer's validity via the use of DLW as a reference. They found that correlation results varied based on age group, demographic, location of accelerometer placement and research environment. Many of the studies that were reviewed (17/25) showed

that the accelerometer had a moderate to good correlation (R>60%) with the DLW test in measuring physical activity or energy expenditure (EE). Furthermore, the accelerometer displayed a high level of validity and reliability in measuring an activity's intensity over time. Therefore, by using calibrated estimation equations the accelerometer should be able to provide more specific measurement results by adapting to specific characteristics of a sample based on a particular age group or disease.

Besides validity, other factors also need to be taken into account before selecting the accelerometer. One such factor is the varying level of practicability offered by different types of accelerometers. Today three kinds of accelerometers are commonly used for research and clinical applications: uniaxial, biaxial, and triaxial. All three have the same basic structure. The only difference between them is the number of dimensions that they can measure. Generally speaking, the more axes/dimensions that the accelerometer can track, the more complex activities the accelerometer can record. However, this does not mean that the triaxial accelerometer is always the best choice. Since the triaxial accelerometer is more complicated than the uniaxial accelerometer, there is a huge price difference between these devices. In order to maximize the cost/effect ratio, many studies have been conducted to determine whether the different types of accelerometers are able to provide similar results. Since these studies have had dissimilar objectives and have used different measurement parameters the results have varied.

For example, Jérémy Vanhelst and Laurent Béghin²⁷compared uniaxial accelerometers and triaxial accelerometers for measuring the percentage of time that adolescent in

the uniaxial accelerometer and the triaxial accelerometer at the right hip simultaneously for seven days. These researchers found that the two accelerometers demonstrated a very good reliability in measuring the percentage of time spent engaged in assorted activity levels (sedentary, light, moderate, and vigorous). The Intra Class Correlation was higher than 95%. The difference between the data obtained from the two accelerometers never exceeded 2.1%, and the difference decreased as physical activity levels increased. Based on their findings, they claimed that there is no significant difference between the uniaxial accelerometer and triaxial accelerometer when measuring physical activities in community dwelling situations.

In contrast, Ott et.al²⁸ compared the validity of the uniaxial accelerometer (CSA) and the triaxial accelerometer (Tritrac-R3D) among 28 children aged 9-11 as they performed eight different free-play activities. These were playing a video game, throwing and catching, walking, bench stepping, hopscotch, basketball, aerobic dance, and running. Subjects spent five minutes at each activity station. Heart rate and activity count were recorded for the last three minutes of each activity in order to minimize the effect of prior activities. They found that both kinds of accelerometers demonstrated a significant correlation between activity counts, heart rate, and predicted MET level. However, when the uniaxial accelerometer (r=0.43 with MET, r=0.64 with heart rate) was compared to the triaxial accelerometer, the triaxial accelerometer had a stronger correlation (r=0.69 with MET, r=0.73 with heart rate).

In another study, Leenders et al.²⁹ focused on adults and compared the DLW with CSA (uniaxial) and TriTrac-R3D (triaxial) in order to evaluate the correlation between these two measuring methods. Thirteen subjects participated in a seven-day experiment. The

accelerometers were secured at the waist and attached to a belt. The triaxial accelerometer demonstrated a stronger correlation with DLW's results (r =0.54) than did the uniaxial accelerometer (r =0.45). This study suggested that the triaxial accelerometer is the better choice for measuring activities in a community dwelling situation and for focusing on complex activity patterns. However, if the goal is to focus solely on simple activity patterns like walking or if the research will take place in a controlled laboratory environment, both uniaxial and triaxial accelerometers can provide a strong correlation with DLW.

Hendelmanet al.³⁰ tested the validity of uniaxial and triaxial accelerometers against indirect calorimetry for walking and a range of household and recreational activities. They found that when focusing solely on walking, the correlation of energy expenditure results between the uniaxial accelerometer and indirect calorimetry was 0.77. For the same activities, the correlation between the triaxial accelerometer and indirect calorimetry was 0.89. Welket al.³¹ conducted a similar study that investigated the validity of three different accelerometers; the ActiGraph (uniaxial), TriTrac-R3D (triaxial) and the BioTrainer (biaxial) compared to indirect calorimetry in measuring laboratory treadmill exercise and non-laboratory activities of daily living. During treadmill walking and running, all accelerometers demonstrated a strong correlation with VO2 (ActiGraph: r=0.85, TriTrac-R3D: r=0.93, BioTrainer: r=0.87). However, when the focus was on activities of daily living, the correlation for all three accelerometers decreased (0.59 for TriTrac-R3D and BioTrainer and to 0.48 for ActiGraph). These figures are similar to Leenders' correlation results.

Accelerometer selection can be influenced by multiple factors. Although many studies have found that the validity coefficients for multiple-axis accelerometers are higher than those

for uniaxial models³², many other factors need to be considered when choosing an accelerometer. These include cost effectiveness, appropriateness for the design if the study and compatibility with the research goals.

2.2Guidelines for Placement

Generally speaking, the sternum, lower back, and waist are the most common locations for placingaccelerometers. ¹¹ Guy Plasqui and Klaas R. Westerterp²⁴ reviewed 28 articles that sought to test the validity of accelerometers as compared to the DLW method in the estimation of daily energy expenditures. Among these papers, nearly half of them (10) selected the lower back as their fitting location for the accelerometer. Other placement locations included the waist (6), hip (5), ankle/shoes (3), and a combination of chest and thigh (2). The correlation between each placement location and DLW can be seen in Table 1. Since researchers like to track the whole body's movement as much as possible during the measurement process, they select a location close to the body's center of gravity in order to track the total acceleration generated by the movement of the whole body. Because it is impractical to place the accelerometer inside the human body, the low back seems the optimum choice for placement because it is at the same level as the center of gravity and it is relatively easy to place the accelerometer there. This placement does not affect an individual's activities of daily living during the monitoring process.

The accelerometer placement will vary depending on the research goal or design. To get the best results a researcher may place the accelerometer in a location other than the lowback even though the low back is considered the "gold standard" for accelerometer placement^{33,34}.

It is also important to take into account the limitations/characteristics of the accelerometer being used when deciding the placement.

Type	Brand	Correlation coefficient (Placement location)	
Uniaxial	Life Corder	0.72-0.83 (Waist)	
	Actigraph/CSA/MTI	0.58-0.96 (Lower back); 0.33-0.62 (Hip);	
	Caltrac	0.26 ^{NS} (Waist)	
Biaxial	Actiwatch	0.27 ^{NS} (Ankle)	
Triaxial	Tritrac-R3D	0.31 (Waist)* 0.54 ^{NS} (Hip)	
	Tracmor	0.63-0.91 (Lower back)	
Combined	ActiReg	Did not provide; (mean ± 2 SD)= 0.41 ± 2.69	
system			
Pedometer	Foot-ground contact	0.17-0.23 ^{NS} (Shoes)	
	pedometer		

Table 1 Correlation between the outcome of accelerometer at each placement location and DLW

NS= not significant;

*There is a difference between the days on which the accelerometer was worn (4 days) and the DLW monitoring period (10 days).

3. Limitations

3.1 Placement issue

An inappropriate placement location may result in a strong impact on the validity and reliability of the data. When testing the validity of accelerometer data for estimating daily energy expenditures via comparison with the doubly-labeled water method, Guy Plasqui and Klaas R. Westerterp²⁴ found a strong correlation (R>80%) between accelerometer results and

DLW results when the researcher fit the accelerometer on subjects' lower back or waist. The correlation between these two methods fell to less than 25% when the accelerometer was placed on the ankle or shoes. These findings indicate that measurement errors can result if the placement location is not carefully considered. Such miscalculations are especially likely to happen when placements are not appropriate for the research goal and design.

A second concern regarding accelerometer placement is loosening of the accelerometer. Individuals may report that their accelerometers loosened on their bodies during the monitoring period or throughout the course of the day. A loose placement may cause inaccurate measurement due to increased signal-to-noise ratios or cause inconsistencies between data collection and activities for some other reason.³⁵

The final concern about placement is convenience. Many individuals report that they feel uncomfortable when performing daily activities with an accelerometer on their body. In addition, individuals need to remove the accelerometer during bathing and sleeping for both safety and comfort issues. Removal of the device can lead to data loss and also increase the possibility that individuals will either replace the device incorrectly or not at all. However, with the development of technology many accelerometers (Like the newly developed Actigraph GTG9X) have been able to provide a smaller wireless sensor that greatly improves the comfort of the device while it is being worn. Besides that, many accelerometers are now waterproofed which may help in preventing the loss of data due to removal of the device while showering or performing some other water activity.

Even if an optimal placement location has been selected, sometimes accelerometers are still not able to provide accurate measurement. For example, underestimation of activity level

is a common issue in many studies, especially those that focus on measuring sedentary activity. One of the most reasonable explanations is that an accelerometer fastened at a certain position on the body (for example, the waist), might not be able to cover movement from other body parts. Some studies try to correct the problem by making use of multiple accelerometer systems during assessment. However, this technique has not been shown to improve results.

3.2 Movement Pattern

Another limitation of accelerometers is that they can only accurately assess limited types of movement patterns. For the population that uses ambulation as its major habitual activity, the accelerometer can provide relatively valid measurement results. However, for individuals who prefer non-ambulatory activities — such as cycling or performing isometric movement—measurement results may not be accurate.³⁶ For example, crouch walking costs more energy than walking with a normal gait due to the continuous contraction of the quadriceps. However, an accelerometer placed at the waist might result in a lower activity count for crouch walking, because this activity does not cause the body's center of gravity to shift as much. For that reason, we need to select the devices based on the characteristics of the movement pattern in order to decrease the chance for measurement error.

3.3 Estimation Equation

Many accelerometers can convert activity counts into energy cost by using a preset energy estimation equation. Kate Lyden and Sarah L. Kozey²¹ analyzed nine published and two proprietary energy expenditure (EE) prediction equations on 277 patients for six treadmill

activities(1.34, 1.56,2.23 ms⁻¹, each at a 0 and a 3% grade) and five self-paced activities of daily living (ADLs). During those activities, all subjects ascended stairs, descended stairs, and moved a 6 kg box. The remaining two activities were randomly selected from a catalog of 14 possible options (cleaning a room, dusting, gardening, laundry, mopping, mowing, painting, raking, sweeping, trimming, vacuuming, washing dishes, basketball, and tennis). The results indicated that all of the equations underestimated the energy expenditure (bias -0.1 to -1.4 METs and -0.5 to -1.3 kcal, respectively). Misclassification rates ranged from 21.7 (95% CI 20.4-24.2%) to 34.3% (95% CI 32.3, 36.3%), with vigorous intensity activities misclassified the most frequently. These findings suggest that the relationship between activity counts and energy expenditure (EE) is specific to the activity being performed. This could be a limitation for measuring activities of daily living in community dwelling situations and could lead to substantial misclassification of activity levels.

3.4Frequency-based Filtering

Since accelerometers measure acceleration with a certain recording frequency and summarize this as a count over a period of time, they might not be able to specifically describe an activity's intensity level. Take, for example, an accelerometer with a 20-second recording period. Such a device would not differentiate between an activity with 1 count per second for 20 seconds and an activity with 20 activity counts in first 5 seconds and 0 activity counts for remaining 15 seconds. This weakness of the accelerometer greatly affects its ability to categorize activities' intensities. As a consequence, data analysis might underestimate the true intensity level, resulting in incorrect information reported to individuals/subjects.

4. Comparison with other Measurement Methods.

Although the accelerometer has many limitations, when it is compared with other measurement methods – like the doubly-labeled water approach or the pedometer – it still shows itself to be a more practical and simple measurement technique. For example, in the past, when researchers attempted to determine the energy cost for certain activities, they usually used doubly-labeled water under laboratory conditions³⁷ or portable calorimeters in the field.³⁰ Although these two measurement techniques were considered the "gold standard" for estimating energy expenditure, neither of them have a wide practicability in clinical settings. This is because many factors impede the use of these two methods. For example, doubly-labeled water is very expensive, and its output is highly limited. Portable calorimeters need highly trained specialists to collect and measure data. These properties restrict the use of these methods, rendering them limited to laboratory research.

The pedometer is a frequently seen device for monitoring physical activity, and it has a long history of use among different types of individuals. The pedometer's advantage is that it is easy to utilize. Individuals do not need specific training regarding its appropriate use. All they need to do is wear the device during movement. Regarding the pedometer's validity and reliability, Lara Allet and Ruud H. Knols³⁸ reviewed 25 articles on pedometer and accelerometer usage by individuals with osteoarthritis, cardiovascular diseases (CVD), Type-2diabetes mellitus, and chronic obstructive pulmonary disease (COPD). Their study found that pedometers can be good and reliable measurement instruments. Additionally, Lorraine S. Evangelista and Kathleen Dracup³⁹ observed that the pedometer was a valid indicator of exercise adherence in heart failure patients who participated in a home-based

walking program. However, this latter study also pointed out a limitation of the pedometer, which is that it can only show a high correlation with the number of steps in walking activity. Moreover, research conducted by Thais Sant'Anna and Victoria C. Escobar⁴⁰ indicated the validity of pedometer data is more limited for energy expenditure during slow walking. This study also found that pedometers significantly underestimated activity time. Therefore, this device may not appropriate for at-home monitoring of individuals' daily activity levels and energy expenditure. Table 2 provides a summary of the advantages and disadvantages of various measurement methods of physical activity. (For references, please see Appendix B)

Background Information on Chronic Heart Failure(CHF)

1.1 Definition

Heart failure, as the final stage of many cardiopulmonary diseases, occurs when the heart is unable to pump in a manner that is sufficient for maintaining blood flow to meet the body's needs. According to the American Heart Association, heart failure is a complex clinical syndrome that results from any structural or functional impairment of ventricular filling or ejection of blood⁴². It has a high mortality rate and it greatly decreases an individual's functional level. The most characteristic symptom of heart failure is exercise intolerance which involves increased shortness of breath, excessive tiredness, and excessive fluid retention. Exercise intolerance greatly limits an individual's exercise capacity and daily living activities. In addition, it decreases the individual's quality of life and increases his or her mortality risk. At first, individuals may only present symptoms with strenuous activities or exercise. As the disease progresses they may complain of shortness of breath and fatigue even

Method	Advantages	Disadvantages
Doubly-labeled	Gold standard; high	Very expensive; requires specialized
water test	accuracy and reliability	instrumentation, such as isotope ratio
		Mass Spectrometry to measure stable
		isotopes ⁴¹
Indirect	Classic measurement	Needs a specialist to adjust the device;
calorimetry	method for estimating	gas leaks may lead to error; primarily for
	resting energy expenditures	assessing resting energy expenditures
Questionnaires,	Easy to apply; proven	Mainly based on patient's memory; may
diaries, and	consistency with DLW	have subjective affect; especially hard to
surveys		apply to children and seniors
Pedometer	Easy to use; does not require	Only measure the count of step; cannot
	a specialist to adjust	distinguish the intensity of an activity;
		only applicable to walking and running;
		not usable for sedentary activities
Accelerometer	Easy to use; can estimate	Results can be affected by fitting
	energy expenditure by using	location; activity pattern, validity
	an equation; can be applied	varying in the field environment activity
	to all types of activity, based	measurement; tends to underestimate
	on fitting location; shows a	energy expenditure; equations are highly
	good reliability	specific for different subjects

Table 2 Advantages and disadvantages of each measurement method

at rest. In severe situations, individuals may not be able to lie flat at night and during sleep due to increased fluid retention in the pulmonary system and a decrease in the supply of oxygen to the body. Since heart failure is an irreversible process the prognosis is usually poor. Because of this individual with heart failure have to live with the disease and manage its symptoms for the rest of their lives.

1.2 Types of Heart Failure

Today most cardiologists and researchers use the ejection fraction as their primary measurement to categorize heart failure. ⁴³ Patients with CHF might have reduced or preserved ejection fractions based on their condition. The ejection fraction is the percentage of blood pumped out of a filled ventricle as a result of a heartbeat. To be considered normal it should be between 55% and 75%. ⁴⁴

Based on different ejection fractions individuals with heart failure can be categorized into two main groups. The first group contains individuals with preserved ejection fraction (HFpEF), and the second group contains individuals with reduced ejection fraction (HFrEF). In the first group the individuals' systolic functions are preserved. Their hearts are able to pump out blood within the normal ejection fraction range which means the heart muscle contracts normally. However, in these individuals the left ventricle does not relax as it should during the refilling process. This decreases the volume of blood that returns to left ventricle thus limiting heart function in these individuals. The second type of heart failure, HFrEF, is also known as systolic heart failure. Here the ejection fraction is usually lower than 40%, which means the left ventricle does not contract effectively. This decreases the circulation of

oxygen-rich blood in the body which restricts the individual's ability to physically function in their daily lives.

Despite the fact that HFpEF and HFrEF differ based on the level of ejection fraction the clinical symptoms can be the same. According to Michael R. Zile, 45 there was a similar impairment in the ability to increase cardiac output and maintain low-LV diastolic pressure sufficiently in individuals with or without reduced ejection fraction. Both groups demonstrated decreased physical activity levels and functional levels in their normal daily lives.

2. Pathophysiology

Any conditions that reduce the efficiency of the heart muscle may cause heart failure.

Due do direct damage to the heart muscle or prolonged overloading, the heart's workload surpasses its normal functional capacity. This forces the heart to initiate a remodeling process to adapt to the overloading and to maintain function. The first pathological change is always related to vascular endothelium remodeling. There modeling process can be initiated in two ways. The first is via a change in local hemodynamic or in response to circulating chemical signals. After the endothelial cells sense the change from the environment they release the mediator to the vascular smooth muscle. This causes immune system cells to accumulate in response to the inflammatory process. This may change the blood flow dynamic and increase the resistance of the circulation system, thus intensifying the load on the heart. This can prompt pathophysiological changes to the ventricle and activate many endocrine processes meant to compensate for the dysfunction. If the circulatory resistance exceeds the normal

systolic pressure the heart will respond by thickening the myocardial wall to increase the ventricle's force of contraction. In the initial stages these compensatory strategies will maintain cardiac output. However, these adaptations cannot sustain cardiac output for long. This is because the thickening of the myocardial wall decreases the ventricle's volume and the heart's compliance (the heart becomes stiffer) which also limits cardiac output. At this point the body needs to escalate its heart rate to compensate for the low stroke volume in order to maintain the heart's output. However, a rapid heart rate greatly reduces the myocardial cells' resting time and impedes the coronary perfusion time which damages the heart muscle. A prolonged perfusion deficit increases the risk of further damage to the heart, and finally leads to the decompensation stage — heart failure.

3. Physical Activity Changes in Patients with Heart Failure

Exercise intolerance is a cardinal sign of individuals with CHF. These individuals show fatigue and shortness of breath while performing physical activity until in end stage they have these symptoms at rest. This changing pathology greatly affects an individual's ability to participate in daily activities and decreases their quality of life. There are other factors that can contribute to a low exercise capacity⁴⁷. In this paper we will mainly focus on hypoxia and muscle disuse.

3.1 Hypoxia and Muscle Response

Hypoxia means a decreased oxygen level or inadequate oxygen delivery at the tissue level. It can be created by the environment or a change in the pathology. Usually the human body is able to compensate to some extent for a decreased oxygen level by using alternate

metabolic methods such as anaerobic metabolism and glycolysis or by increasing the total number of erythrocytes in order to improve the oxygen transfer through the blood. However, for the individual with CHF who cannot maintain their cardiac output due to irreversible changes in their heart muscle and compromised physiology a prolonged low cardiac output will decrease the peripheral vascular blood flow and decrease the oxygen delivery to the peripheral skeletal muscular system.

The blood flow through the renal system is also been decreased which triggers the renal system to enter a hypovolemic state in order to retain blood volume. The renal system then increases the production of rennin, which can be converted to angiotens in. Angiotens in can intensify peripheral vascular resistance, thereby elevating blood pressure. However, rennin can also stimulate the release of aldosterone, the hormone that increases sodium re-absorption in the proximal tubule. This causes excessive water retention and leads to peripheral edema, which may compress the arteries and cause further reduction of blood flow

The diminished left ventricular output leads to hypertension in the pulmonary capillary wedge which results in an accumulation of fluid in the alveoli and small airways. The fluid in the lungs' interstitium impedes ventilation and perfusion, thus decreases the oxygen level in the blood. All these pathology changes will severely decrease the oxygen level in the body and produce hypoxia in multiple body systems, especially the skeletal muscle system.

The traditional theories related to muscle wasting and atrophy that present in individuals with CHF suggested they were due to a deceased appetite and reduced physical activity.

However, more and more evidence is accumulating that shows hypoxia itself contributes to the loss of muscle mass during chronic hypoxia 48. Many studies have been conducted in order

to find out the relationship between hypoxia and skeletal muscle dysfunction^{49,50}. Based on the outcomes, the findings are that chronic hypoxia leads to a negative regulation of protein balance in the skeletal muscle system which significantly changes the fiber proportions of muscle, thus impacting the individual's exercise capacity.

3.1.1 Chronic Hypoxia and Regulation of Protein Balance

The effect of hypoxia on protein balance regulation is based on its duration. Research⁴⁸ has found that hypoxia may increase the speed of protein turnover, but depending on the length of time the hypoxia lasts, the outcome is totally different. Acute hypoxia causes the increase of protein synthesis, a general increase in growth hormone, activation of satellite cells and an increase in the recruitment of type II muscle fibers. In fact it can be said that short term hypoxia improves muscle strength and endurance.

In contrast, chronic hypoxia usually triggers muscle wasting. Although chronic hypoxia also increases both protein synthesis and degradation, the increased rate of protein degradation is higher than the rate of protein synthesis which results in skeletal muscle loss⁴⁸. Individuals with CHF who have significantly decreased cardiac output due to pathologic changes in their cardiovascular system will have widespread chronic hypoxia that affects the entire muscle system of the body. This will cause general skeletal muscle weakness and exercise intolerance.

3.1.2 Chronic Hypoxia and Muscle Alternation

We know that human muscle contains 3 different types of myosin heavy chain fibers depending on their metabolic pathway and function: Type I, Type IIa and Type IIb. Type 1

fibers have been called "slow twitching" fibers because they depend primarily on aerobic metabolism and are able to provide long term fatigue resistant contractions. In contrast, Type IIb fibers depend primarily on anaerobic metabolism (glycolytic) and are able to quickly generate large amounts of force. Type IIa fibers have intermediate properties compared to type I and type IIb fibers. The percentage of each type of muscle fiber in a particular muscle group may be different from other muscle groups depending on the specific function of that group. Research shows that chronic hypoxia affects muscle fiber distribution⁴⁹. Interestingly, muscle fiber composition will be totally different in the peripheral muscles and the respiratory muscles. Individuals with CHF will demonstrate a decrease in type I fibers and an increase in type IIb fibers when compared to normal individuals. In contrast, the respiratory muscles such as the diaphragm will show an increase in type I fibers and a decrease in type IIb fibers in individuals with CHF compared to normal individuals. One possible explanation is that the peripheral muscles develop anaerobic instead of aerobic metabolism to try to maintain normal functioning during prolonged hypoxemia. The respiratory muscles, on the other hand, adjusting to a constantly increasing demand for oxygen from the periphery develop more type I fibers to try to meet the demand with a more fatigue resistant aerobic system to manage the increased workload as effectively as possible. This shifting of fiber types helps the muscle groups temporarily maintain their primary function. However, due to the characteristics of the different fiber types, these changes will negatively alter the muscle performance in each area and greatly limit the individual's level of function. For example, the individual with CHF will demonstrate decreased activity tolerance with an early onset of fatigue in the peripheral muscles due to the decreased percentage of type I fibers. Moreover, the individual will report

increased dyspnea during activity as the respiratory muscles will be unable to provide enough muscle strength to increase the inhalation of oxygen due to the decreased number of type IIb fibers in the diaphragm.

3.1.3 Muscle Disuse

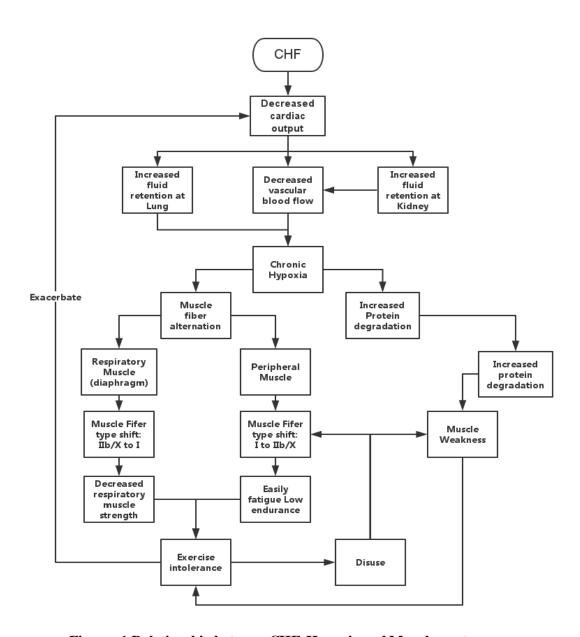
Besides hypoxia, muscle disuse is another factor that will exacerbate activity intolerance. The fact that muscle disuse is a consequence of activity intolerance makes it a major factor in the downward spiral of an individual with CHF. Because activity intolerance limits as individual's ability to perform daily activities, they tend to be more sedentary and do less activity compared to healthy individuals. Without proper stimulation from physical activity the peripheral muscles lose muscle mass and demonstrate increased weakness thus increasing activity intolerance which becomes a vicious cycle. Muscle weakness in the lower legs decreases the normal "muscle pump" effect on the peripheral vascular system. This increases fluid retention in the peripheral tissues and causes further hypoxia. This creates another vicious cycle as well as a risk for non-healing wounds that further debilitates the individual with CHF. The figure 1 has depicted the possible progression of exercise intolerance in patient with CHF. (For references, please see Appendix C)

4 Conclusions

An appropriate level of activity can help prevent exacerbations of CHF. It can also allow individuals with CHF to maintain their ability to perform their ADL's without difficulty.

Therefore, it is helpful for physical therapists to find a valid measurement method that can be used to guide the treatment plans and home programs of individuals with CHF. Consistent

follow through with a home exercise/activity program is crucial to the success of preventing a decline in the functional status of an individual with CHF. Objective measurement methods, like the accelerometer, have the potential to be very effective in monitoring daily activity levels and energy expenditures in clinical settings and at home.



Figures 1 Relationship between CHF, Hypoxia and Muscle waste

In light of that the validity of the Stay-healthy RT3 accelerometer (RT3) was tested under various measurement conditions. By comparing the RT3 accelerometer with indirect

calorimetry (the "gold standard' for measuring physical activity levels and energy expenditure), we looked at the validity of the RT3 accelerometer data for measuring special daily tasks (Aim 1). The RT3 accelerometer was also compared with the 7-day Physical Activity Recall Scale (7-dayPAR) by looking at a sample of individuals with CHF over seven days. This showed that the accelerometer is superior to the 7-day Physical Activity Recall Scale (7-day PAR) in accurately recording an individual's activity level and energy expenditure(Aim 2). And finally, a re-evaluation of the baseline metabolic level for individuals with CHF was performed to determine whether resting metabolic rates vary between a healthy population and individuals with CHF. This showed that it is necessary to readjust the value of 1 MET for individuals with CHF because the traditional MET intensity scale is not accurate for them (Aim 3).

Methods

Research Design: A descriptive correlational design was used in this study.

Sample: A total sample of 54 subjects was recruited from the Heart Failure Clinic at BryanLGH Heart Institute in Lincoln, Nebraska. The mean age of the 54 subjects was 73.5 ± 7.6 years. There were 38 males and 16 females. The mean left ventricular ejection fraction was $31 \pm 7.6\%$. Subjects had a mean Body Mass Index (BMI) of 29.8 ± 5.8 . This study was approved by the University of Nebraska Medical Center Institutional Review Board All subjects were required to complete the consent form that was approved by the IRB prior to the study.

Procedure:

Stage 1: Subjects who met inclusion criteria were approached for participation in the study and were given the consent form. They read the form while in the clinic or took it home to read if they so desired. The RT3 accelerometers were placed on subjects at waist level in the BryanLGH Heart Institute clinic. Instructions were given regarding the 7 day wearing period of the accelerometers. Detailed written instructions for the use of the RT3 were also given to the subjects to reference during the 7 day wearing period. The RT3 accelerometer was returned by the subject to the clinic at the end of the 7 day wearing period and the 7- Day PAR questionnaire was administered via interview.(Please see Appendix D& E)

Stage 2: Fifteen subjects were recruited from the subjects who had completed Phase I to participate in Phase II of the study. A separate time was scheduled at the subject's convenience to complete the data collection. Each subject was fitted with a face mask and pneumotach from which the volume of gas exhaled was calculated and proportional samples of expired gas were taken into the MedGraphics VO2000 (Medical Graphics Corp., St. Paul, MN) for analysis of O2 and CO2 levels. The measured absolute VO2 (L•min-1)was converted to kilocalories (Kcal) and relative VO2 (ml•kg-1•min-1) for assessing the energy expenditure(EE) of subjects. At the same time the subjects also wore the RT3 at their waist to monitor the activity count during the whole test session. The subjects were randomly assigned to perform a sequence of light and moderate physical activity tasks, which included reading the paper, watching TV, dusting, vacuuming, wash dishes and stair climbing. The ratio between the light and moderate activities was 4:1 (80% light activity, 20% moderate activity).

sequences. The detail of the protocol can be found in the table 3..

	Order of Activities									
	First6MW		#1	#2	#3	#4	#5	#6		Second
Sequen	TTrial									6MWTTri
ce										al
1	6-MWT	R	Read6	Wash6	Vac3	TV6	Dust6	Stairs	R	6-MWT
			min.	min.	min	min.	min.	3 min		
2	6-MWT	E	Wash6	Vac3	TV6	Dust6	Stair3	Read	E	6-MWT
			min.	min	min.	min.	min	6		
								min.		
3	6-MWT	S	Vac3	TV6	Dust6	Stairs	Read6	Wash	S	6-MWT
			min.	min.	min.	3 min	min.	6		
								min.		
4	6-MWT	Т	TV6	Dust6	Stairs	Read6	Wash6	Vac3	Т	6-MWT
			min.	min.	3 min	min.	min.	min		
5	6-MWT		Dust6	Stairs3	Read6	Wash	Vac3 min	TV6		6-MWT
			min.	min	min.	6 min.		min.		
6	6-MWT		Stairs3	Read6	Wash	Vac3	TV6 min.	Dust		6-MWT
			min	min.	6 min.	min		6		
								min.		

Table 3 Testing Protocol

Data Analysis

The SPSS 20.0 software was used to analyze the data. The level of significance was set at <0.05. To look at the validity of the energy expenditure (EE) data from the RT3 accelerometer, it was compared with the energy expenditure (EE) data from the MedGraphics VO-2000 (includes Total EE and Active EE) to find out if there was a significant difference between them. The activity recorded by the RT3 and the activity recorded by the MedGraphics VO-2000 were also compared to see if there was a correlation between them.

The active energy expenditure (EE) as estimated by both the 7-day PAR and RT3 were averaged in order to find the activity level for the individuals with CHF. Then, the energy as estimated both by the 7-PAR and the RT3 accelerometer were paired to determine the reliability of the 7-day PAR and see if there was a significant difference between the two methods.

For the subjects who participated in the Phase II study, the O2 and CO2 levels were recorded during the seated rest periods by MedGraphics VO-2000 (Medical Graphics Corp., St. Paul, MN). The data was analyzed by SPSS 20.0 and compared to standard data from a healthy population (3.5 ml/kg/min = 1 Metabolic Equivalent (MET)) to see if there was a difference in the metabolic rate between the healthy population and individuals with CHF.

Results

1. Validity of RT3 Accelerometer

There were 14 valid records for RT3 and MedGraphics VO-2000 which included total energy expenditure and active energy expenditure for each individual. These were all

transferred into Kcal in order to make the data comparable. The summary of the energy expenditure for each activity can be seen in table 4.

Next the correlation between the recorded Activity levels of the RT3 and the MedGraphics VO-2000 for each of the activities was calculated. The result of the Spearman rank order correlation test is shown in table 5.

(Kcal/min)		Total EE*	Active EE**		
	RT3	MedGraphics VO-2000	RT3	MedGraphics VO-2000	
resting EE	1.0793	1.0297	NA	NA	
1st 6 mwt	21.4667	21.6876	14.8223	15.5094	
read paper	7.1313	7.3005	0.7122	1.3801	
wash dishes	8.471	10.8482	1.6934	4.7521	
vacuum	5.4225	8.1495	2.1433	5.1278	
watch TV	6.9271	6.4274	0.355	1.3798	
dust	8.6031	12.0936	2.1406	7.1507	
stairs	7.8027	12.8097	4.5518	9.7203	
2nd 6 mwt	19.3203	15.0897	13.4484	11.8894	

Table 4 Summary of energy expenditure for each activity

The results demonstrate that the total energy expenditure (EE)as recorded by the RT3 accelerometer shows a moderate to strong correlation (0.67<r<0.91) to the total EE recorded by the MedGraphics VO-2000 and the only activity that demonstrated a weak correlation was

^{*}Total energy expenditure (EE) includes both resting energy expenditure and the energy used to perform the activities of the study protocol.

^{**}Active EE is only the energy used to perform the activities of the study protocol. It was calculated by using the total energy expenditure minus the resting energy expenditure.

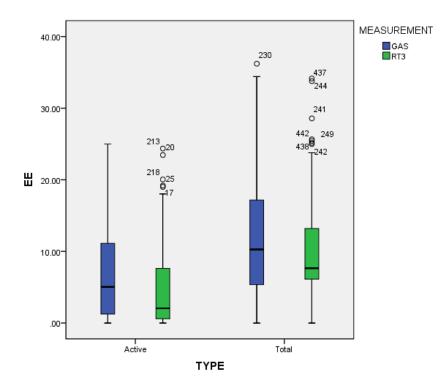
reading the paper (r=0.31).On other hand, when testing the correlation between the active energy expenditure results from the MedGraphics VO-2000 and activity level recorded by the RT3 there was little or no correlation between MedGraphics VO-2000 and RT3 in reading the paper, washing the dishes and watching TV. All of the other activities show a moderate to strong correlation (0.6<r<0.9) between the two methods

	1st	read	wash	stairs	watch	dust	vacuum	2nd
	6MWT	paper	dishes		TV			6MWT
TOT Gas	0.807	0.318	0.782	0.811	0.674	0.689	0.911	0.737
vs. RT-3								
P value	<0.001	0.248	0.001	<0.001	0.006	0.005	< 0.001	0.002
ACT Gas	0.732	0.051	0.168	0.657	0.422	0.662	0.908	0.705
vs. RT-3								
P value	0.002	0.856	0.549	0.008	0.117	0.01	<0.001	0.003

Table 5 Spearman rank order correlation test

Since the RT3 is able to covert activity levels into kilo calories by using a preset equation the outcomes between the RT3 and MedGraphics VO-2000 could be compared directly to each other. In order to find out the general validity of the RT3,the results of all 8 activities had to be combined and the Wilcoxon signed ranks test must be used to compare the mean outcome level from all 8 activities. The statistical results showed that there was no significant difference between the two methods for both total energy expenditure and active energy expenditure measurements. (total_{all}: p=0.674, p>0.06; active_{all}: p=0.161, p>0.05). Figure 2 has

demonstrated the outcome of Wilcoxon test.



Figures 2 Wilcoxon test results of total energy expenditure and active energy expenditure measurements

Since the two methods showed no significant difference in the measurement of general energy expenditure, it was felt that it would be helpful to determine if different intensity levels of activity or movement patterns would affect the validity of the RT3. In order to test those influences, each activity had to be compared separately to see if there was a significant difference between the two methods. The results are shown in table 6.

The results showed that the RT3 showed good validity when measuring activities which have low intensity and a simple activity pattern. When increasing the intensity or performing more complex movement patterns the results demonstrated significant differences between the RT3 and the MedGraphics VO-2000.

	P value _{TOT}	P value ACT
resting	0.594	NA
1st 6mwt	0.73	0.638
2nd 6mwt	0.06	0.084
read paper	0.975	0.198
watch TV	0.917	0.308
wash dishes	0.221	0.03
dust	0.023	0.03
vacuum	0.005	0.003
stair	0.003	0.002

Table 6Wilcoxon signed ranks test

2. Average daily active energy expenditure baseline for people who have CHF

Both the RT3 accelerometer and the 7-day PAR questionnaire were used during the 7 days of daily activity energy expenditure estimation in Phase 1. All the results were recorded or calculated in Kcal. The statistical results for active energy expenditure are included in table 7.

3. Comparison between the seven-day PAR and RT3 accelerometer

When the 7-dayPAR was compared with the RT3 accelerometer there was a significant different between the total energy expenditure estimated by the 7-day PAR (7-days PAR TOT) and the energy expenditure level recorded by the RT3 (RT3 TOT) (p<0.05). Because the RT3

was only able to record the daily activity, and the 7-day PAR TOT included the energy expenditure measurement for time asleep. The difference may be due to the missing sleep data. In order to eliminate bias, the data was adjusted from the 7-day PAR TOT to 7-day PAR daytime by subtracting the night energy expenditure from the total energy expenditure.

Comparing the two measurements again with only daytime activity the results showed that there was no significant difference between the results of the RT3 and the 7-day PAR for the measurement of daily activity estimation (p=0.387>0.05).

	Mean (Kcal)	SD.	95% Confidence Interval for Mean		
RT3 AEE	309.8351	192.6193	256.2095	363.4606	
RT3 TOT	1956.79	460.0294	1836.9396	2091.0204	
7 days PAR	2040.2774	814.7396	1827.6217	2293.1596	
(day time)					
7 days PAR	2517.1504	870.5340	2292.2928	2787.8313	
(Total)					

Table 7 Statistical results for 7 days energy expenditure estimation

The correlation between the two measurement methods demonstrates a moderated correlation between the RT3 and seven-day PAR in estimating energy expenditure (r=0.58, p<0.05). There is a weak (r=0.35), but significant correlation (p=0.014<0.05) between the 7-day PAR (estimated energy expenditure) and the RT3 (activity level) measurement methods.

4. Resting energy expenditure

The results of the MedGraphics VO-2000data were used to estimate the mean resting energy expenditure level of individuals with CHF and compare it to the value for MET resting levels in a healthy population (3.5ml/kg/min). The results are shown in table 8.

The results show that the mean resting energy expenditure for individuals with CHF is 2.72 ml/kg/min vs. 3.5 ml/kg/min in healthy individuals. This is a significant difference as shown by the p- value of 0.006<0.05.

	Test Value = 3.5							
	Mean	t	df	Sig. (2-tailed)	Mean	95% Confidence Interva		
	value				Difference	of the Difference		
						Lower	Upper	
Resting	2.72	-3.213	14	.006	77933	-1.2995	2591	

One-Sample Test

Table 8 Statistical result of resting energy expenditure for CHF patient

Discussion:

Compared to other measurement methods, the accelerometer provides a promising approach in measurement of energy expenditure in healthy populations due to its high validity. Although there have been many studies conducted to test its measurement validity and reliability, only a few of them have focused on the heart failure population. Moreover, since most of the studies have been in a controlled environment, the results of these studies do not show the true validity of the accelerometer particularly while measuring an individual's daily

energy expenditure in a community dwelling situation. This project has shown that the accelerometer (RT3) has good potential to be used as a valid measurement tool to estimate daily energy expenditure for individuals with CHF in a community dwelling environment.

1. The validity of RT3

The RT3 accelerometer has demonstrated reasonable reliability and validity in estimating daily activities of individuals with CHF based on the results of this research project. TheRT3 has shown a moderate to good correlation (r =0.67-0.91) with the MedGraphics VO-2000 when estimating the energy expenditure for most daily activities (Table 5). However, if we only focus on active energy expenditure, we find that the 6 minute walk test demonstrates a stronger correlation than most of the daily activities. This finding is similar to previous research conducted by Hendelman et.ah³⁰. They studied the correlation between a portable metabolic system and an accelerometer in evaluating the metabolic cost of four overground walking activities at self-selected speeds and a series of indoor and outdoor household activities. They found that the accelerometer demonstrated a better correlation with the portable metabolic system while measuring walking (r=0.89) than with all of the activities combined (r=0.62). Welk et.al³¹ has also found that compared to daily activities, walking on the treadmill generated a better correlation with the VO2 measurement than the daily activities did. A possible explanation may be related to the design of the device and/or the selection of the calibrated parameter. Since most of the accelerometers were designed and calibrated for use during lab based activities those activities which are similar to lab activities may have better results than those that are more similar to activities in community dwelling environments. And although the accelerometer used in that study includes multiple calibration options and preset estimation equations that cover many different activities, none of them were able to provide an option that could be used universally.

The only daily activity that showed an insignificant correlation in total energy expenditure between the results of the RT3 accelerometer and the VO-2000 is "reading the paper". The probable reasons for this are the location of the accelerometer placement and the lack of motion that occurs at the site during this activity. It is difficult for an accelerometer placed at the waist to register upper extremity activities. A similar result occurred when measuring active energy expenditure. The results show that the active energy expenditure outcomes of the RT3 and the VO-2000 measurements related to "reading the paper", "watching TV" and "washing the dishes" (Reading the paper: p=0.856, Watching TV: p=0.117, Washing the dishes p= 0.549) showed insignificant correlations with P>0.05.Because those activities require more upper extremity movement than whole body movement, an accelerometer that has been placed at the waist will not be able to measure the energy expenditure as accurately as the VO-2000.

Another possible reason affecting the accelerometer measurements may be the movement "pattern" during measurement. Reading the paper is a relatively low intensity activity when compared to the other selected activities. It requires the subject to maintain the upper extremities in a stable position so that the eyes are able to read the content of the paper. This means that the arms do not generate much movement. Most of the muscles in the upper arm perform isometric contractions to "hold" the paper in place. Since the accelerometer measures energy by calculating the acceleration that is generated by movement, it is difficult for the accelerometer to measure the energy that generated by isometric contractions.

Besides looking at the correlation of the RT3 to the VO-2000, the actual energy expenditure measured by these two methods was compared. The results showed that there is no significant difference between the outcomes of the two methods when they measure total energy expenditure for all 8 activities. However, when comparing each activity separately there was a pattern of increasing disparity between the measurements of the RT3 and VO-2000 shown with the increasing of activity intensity and complexity. This finding is similar to the findings of Lyden's research²¹. They found that with increasing intensity, the accelerometer demonstrates more misclassifications when compared to indirect calorimetry. One possible reason is the equation being used to calculate the energy expenditures measured by the accelerometer. As mentioned before, most of the energy estimation equations were created from test results generated in a laboratory setting. The accelerometer will generate a better outcome if the measured activity is similar to the activity that was used to create the equation. However, compared to community dwelling environments, the lab environment is highly controlled. Because of this it is unlikely the accelerometer will be able to cover all of the possible daily activity movements with one of its preset equations.

We have also found that the RT3 tends to underestimate the actual energy expenditure when compared to the VO-2000. This finding is similar to prior research^{30,31,40}. This is in addition to the location of the accelerometer placement and the effect movement patterns may have on the accuracy of the measurement. One other possible reason for the underestimation of energy expenditure is that the accelerometer cannot be 100 % attached to the skin so there will always some minimal movement between the accelerometer and the individual's skin. The amount of movement will increase as the intensity of the activity goes up, and it may

cause inaccurate acceleration input to the accelerometer.

2. The difference between seven-day PAR and RT3 in measurement of free-living activities

Many research studies have been conducted to compare the validity of the 7-day PAR with objective measurement protocols. In Leenders' research⁴, the author compared the 7-day PAR with an accelerometer (Tritrac-R3D) and found that the 7-day PAR overestimated energy expenditure by 25% when compared to the accelerometer. In this study the total energy expenditure estimated by the 7-day PARwas 22% higher than the accelerometer which is similar to Leenders' findings. However, since the formula that was used to calculate total energy expenditure also included sleeping time and our participants did not wear the accelerometer while sleeping, which may have caused the discrepancy in the results. Because of this only the daytime activity energy expenditure was used (7-day PARday) instead of the total energy expenditure for a 24 hour period (7-day PARtot). With that modification no significant difference was shown between the two measurements. This means that the 7-dayPAR was able to measure the daily energy expenditure accurately when it was used to describe the physical activity characteristics of a special population. Moreover, there was a strong correlation between the 7-dayPARdayand the accelerometer, which means the 7-day PAR was also able to measure each individual's physical activity information within a discreet group of people. Although the 7-day PAR did not show intensity changes during daily activities (poor correlation with VM), it still showed a relatively accurate estimate when comparedto data from an objective measurementtool.

3. The Resting Metabolic Rate in patient with CHF

The metabolic rate has been defined as a physiological measure expressing the energy cost of a physical activity. It has been widely used to evaluate an individual's functional level, categorize different activities into light, moderate and high intensity groups and to monitor the level of a workload. Many researchers and therapists have applied the classic MET level scale in their treatments to guide an individual's treatment progression, especially for individuals with CHF. Because the activity capacity of individuals with heart failure is lower than that of healthy individuals, the normal MET scale may not be appropriate for those individuals with CHF due to the difference in their metabolic rate. Savage et al. 51 found that compared to healthy individuals, the individual with coronary heart disease demonstrated a lower resting metabolic rate (23% to 36% lower) than the widely accepted 3.5 ml/kg/min based on a healthy individual's BMI. This study showed that individuals with CHF show significantly lower resting energy expenditure than the criteria for a healthy individual (2.7 ml/kg/min vs. 3.5ml/kg/min, decreased 22.9%). This may be due to the decreased metabolic rate of these patients. If individuals with CHF have a lower metabolic rate, it maybe inappropriate to use 3.5 ml/kg/min as their default measurement criteria. Their MET level criteria may not be the same as that of healthy individuals which means the normal MET level categorization of activities might actually be harder for individuals with CHF than was thought. For example, based on the compendium, walking on a firm level surface at the speed of 2.0 MPH is considered to be a light activity (2.5MET). However, walking at that same speed on a firm level surface, based on this study appears to be too difficult for an individual with CHF and possibly increases the risk of secondary injury. The MET level of this activity should be

recalibrated to 3.2 MET for this type of individual, which would make it a moderate intensity activity (3-6 METs). Further research is needed to study the possibility of modifying the MET classification for specific populations, especially those with CHF, to get a more accurate measurement of their abilities and to set up more appropriate treatment programs for these individuals.

Conclusion

Overall, this study reveals that the accelerometer has demonstrated a good capacity for estimating daily activities. The measurement results that measured by accelerometer have shown a moderate to good correlation with the outcome of indirect calorimetry when measuring total daily energy expenditure. However, the validity of accelerometer may be influenced by activity intensity, movement patterns, placement location and adhesion. For the 7 days PAR questionnaire, the results of this study agree with previous studies that indicate PAR overestimated the energy expenditure by 22%. However, if we only focus on daily activities energy expenditure, there is no significant difference between the outcome of 7 days PAR and accelerometer. Although there are considerable errors in some of the estimations, both of the accelerometer and 7 days PAR questionnaire are still able to provide valid measurement outcome record of physical activity for evaluation patient's behavior and epidemiologic research.

In our research, we also found that the rest energy expenditures of CHF patients is significant lower than normal criteria, which indicate the assumed metabolic constant may not appropriate to be used to estimate daily energy expenditure in patient with CHF. However,

due to the small sample size, further research is needed to better understand how the CHF will affect the resting metabolic rate, and find out if it is necessary to re-adjust the MET criterion in treating the patient with CHF.

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Appendix A

Article Name	Author	Purpose	Methods	Result	Common	Citation
Quantitating	Steele,	To determine the	47 outpatients with stable	For the reliability, The	Subjects were	Chest
physical activity	B.G; Holt,	reliability, validity, and	COPD and dyspnea were	intraclass correlation	mainly male. There	2000,
in COPD using	R.N.L.;	stability of a triaxial	recruited. The	coefficient of 3 6mwt is 0.84.	are only test 3 days	117,
a triaxia1	Belza, B.;	accelerometer for walking	accelerometer was placed	For Concurrent validity,	of the Home daily	1359-13
accelerometer.	Ferris, S.;	and daily activity	on patients' waist. There	Significant correlations were	activities. Author	67
	Lakshminar	measurement in a COPD	were 3 6mwt been tested	evident between	also uses Modified	
	yan S.;	sample.	for the reliability of	accelerometer activity at	Activity Recall	
	Buchner,		accelerometer. The	home, level of obstructive	Questionnaire as	
	D.M.		authors also measured	pulmonary disease ($r = 0.62$;	one of the factor to	
			daily activity over 3 full	p < 0.001), exercise capacity	test validity but the	
			days at home to test	(r = 0.74; p < 0.001),	result was not	
			validity.	dyspnea over the past 30	significant.	
				days ($r = -0.29$; $p < 0.05$),		
				and self-efficacy for activity		
				(r = 0.43; p < 0.01)		
Executive	Foster ER,	To investigated	27 People with severe	Possible depression (64%)	CHF patient	Am J
dysfunction and	Cunnane	participation levels and	CHF (New York Heart	and cognitive impairment	demonstrated	OccupT
depressive	KB,	relationships among	Association Class III or	(15%–59%) were prevalent.	significant	her.
symptoms	Edwards	cognition, depression, and	IV) completed	Participants reported	reduction in activity	2011
associated with	DF,	participation for people	standardized tests of	significant reductions in	participation; this	May-Ju

reduced	Morrison	with severe congestive	cognition and self-report	participation across all	could be due to	n;65(3):
participation of	MT, et.al.	heart failure (CHF).	measures of executive	activity domains since CHF	impaired executive	306-13
people with			dysfunction, depressive	diagnosis (ps < .001). Worse	function or	
severe			symptoms, and	executive dysfunction and	cognitive level. In	
congestive heart			participation	depressive symptoms were	the other hand, a	
failure.				associated with reduced	prolonged disabled	
				participation and together	condition will	
				accounted for 35%-46% of	continue worsen the	
				the variance in participation	cognition and	
				(ps<.01).	participation, this	
					will lead patient fall	
					in vicious circle.	
Vital signs:	Carroll DD,	Using 2009-2012	Data from the 2009-2012	Overall, 11.6% of U.S. adults	Background for	MMWR
disability and	Courtney-L	National Health Interview	National Health Interview	aged 18-64 years reported a	chronic disease and	Morb
physical activity	ong EA,	Survey to estimate the	Survey (NHIS) were used	disability. Compared with	physical inactivity.	Mortal
- United States,	Stevens	prevalence of disability	to estimate the prevalence	adults without disabilities,		Wkly
2009-2012.	AC, Sloan	and its relationship with	of, and association	inactivity was more prevalent		Rep.
MMWR Morb	ML	Physical inactivity	between, aerobic physical	among adults with any		2014
Mortal Wkly			activity (inactive,	disability (47.1% versus		May
			insufficiently active, or	26.1%) and for adults with		9;63(18)
			active) and chronic	each type of disability.		:407-13.
			diseases (heart disease,	Inactive adults with		
			stroke, diabetes, and	disabilities were 50% more		
			cancer) among adults	likely to report one or more		
			aged 18-64 years by	chronic diseases than those		
			disability status and type	who were physically active.		

			(hearing, vision,	Approximately 44% of adults		
			cognitive, and mobility).	with disabilities received a		
			The prevalence of, and	recommendation from a		
			association between,	health professional for		
			receiving a health	physical activity in the past		
			professional	12 months		
			recommendation for			
			physical activity and level			
			of aerobic physical			
			activity was assessed			
			using 2010 data.			
Comparisons of	Leenders	Determine the relative	Twelve healthy	EE determined by PAR was	It would be good if	Med Sci
four methods of	NYJM,	validity among estimates	college-aged women	significant higher than PAEE	there is a	Sports
estimating	Sherman	of physical activity using	participate the research,	estimated from either the	measurement be a	Exerc.
physical activity	WM,	the 7-d Physical Activity	Subjects wore at the waist	Tritrac, CSA, or the Yamax	"golden standard"	2000
in adult women.	Nagaraja	Recall questionnaire and	a Tritrac-R3D	data. Time spent in light,		Jul;32(7
	HN	three activity monitors	accelerometer, a	moderate, and hard physical):1320-6
		(CSA and Tritrac	Computer Science	activity was not significantly		
		accelerometers, Yamax	Application Inc. activity	different between PAR, CSA,		
		pedometer).	monitor (CSA), both of	and Tritrac.		
		,	which measure bodily			
			accelerations in various			
			planes, and a Yamax			
			Digi-Walker-500 that			
			records steps. After the			
			7-d period subjects			
	1	1	, , , , , , , , , , , , , , , , , , ,	1	l	1

			responded to a 7-d			
			Physical Activity Recall			
			interview (PAR)			
Seven-Day	SALLIS, J.	Clinical Guideline for 7			Background	
Physical	F	days PAR			information	
Activity Recall.						
Overestimation	Watkinson	To investigate the	Exploratory	45.9% of inactivity	This article shown	Internati
of physical	C, van	discrepancy between	cross-sectional analysis of	population (according to	the reason why we	onal
activity level is	Sluijs EM,	objective and self-rated	PA awareness using	objective measurement) are	need a objective	Journal
associated with	Sutton S,	physical activity in	baseline data collected	overestimate their activity	measurement	of
lower BMI: a	Hardeman	different population	from 365 ProActive	level, multiple logistic	method during	Behavio
cross-sectional	W, Corder		participants between 2001	regression model adjusted for	clinical treatment,	ral
analysis.	K, Griffin		and 2003 in East Anglia,	age and smoking, males (OR	people tend to	Nutritio
	SJ		England. Self-rated PA	= 2.11,95% CI $= 1.12,3.98$),	overestimate their	n and
			was defined as 'active' or	those with lower BMI (OR =	activity level when	Physical
			'inactive' (assessed via	0.89, 95% CI = $0.84, 0.95$),	they using	Activity
			questionnaire). Objective	younger age at completion of	subjective	2010,
			PA was defined according	full-time education (OR =	measurement.	7:68
			to achievement of	0.83, 95% CI = 0.74, 0.93)		
			guide line activity levels	and higher general health		
			(≥30 minutes or <30	perception (OR = 1.02 CI =		
			minutes spent at least	1.00, 1.04) were more likely		
			moderate intensity PA,	to overestimate their PA		
			assessed by heart rate			
			monitoring)			
Self-reported	Cust AE,	To identify the	97 men and 80 women	Participants in the	This article show	Epidemi

Confidence in	Armstrong	applicability of	completed European	high-confidence group had	another possible	ology
Recall as a	BK, Smith	Self-reported confidence	Prospective Investigation	higher validity and	affect factor for	2009;20
Predictor of	BJ, Chau J,	ratings in epidemiologic	into Cancer and Nutrition	repeatability coefficients than	subjective	:
Validity and	van der	studies	(EPIC) past-year	those in the low-confidence	measurement, the	433–441
Repeatability of	Ploeg HP,		questionnaire and the	group for most comparisons.	most interesting	
Physical	Bauman A.		International Physical	For IPAQ: rho = 0.34 (95%	thing in the results	
Activity			Activity Questionnaire	confidence interval [CI] =	id that Women were	
Questionnaire			(IPAQ) last-7-day	0.08 to 0.55) and 0.01 (-0.17	less likely than men	
Data			questionnaire. at baseline	to 0.20) for high- and	to report high recall	
			and at 10 months and	low-confidence groups,	confidence of	
			wore an accelerometer as	respectively. For Epic: rho =	past-year activity,	
			an objective comparison	0.81 (0.72 to 0.87) and 0.63	which means they	
			measure for three 7-day	(0.48 to 0.74), respectively	result may have	
			periods during the same		lower validity	
			timeframe. Participants		compare to male.	
			rated their confidence in			
			recalling physical activity			
			for each question using a			
			5-point scale and were			
			dichotomized at the			
			median confidence value.			
Estimating	Besson H,	assess the validity and	Total energy expenditure	Estimated TEE and PAEE	Back ground info	Am J
physical activity	Brage S,	reliability of the Recent	(TEE) was measured for	were significantly associated		ClinNutr
energy	Jakes RW,	Physical Activity	14 d by using the doubly	with criterion measures		. 2010
expenditure,	Ekelund U,	Questionnaire (RPAQ),	labeled water technique	(TEE: $r = 0.67$; PAEE: $r =$		Jan;91(1
sedentary time,	Wareham	which assesses usual	combined with a measure	0.39) The correlation):106-14

and physical	NJ	physical activity (PA) in 4	of resting metabolic rate	between self-reported and		
activity		domains (work, travel,	to yield PA energy	measured time spent was		
intensity by		recreation, and domestic	expenditure (PAEE) in 25	significant for vigorous PA (r		
self-report in		life)	men and 25 women.	= 0.70) and marginally		
adults			Simultaneously, intensity	insignificant for sedentary		
			of activity was measured	time $(r = 0.27, P = 0.06)$. The		
			by using combined heart	intraclass correlation		
			rate and movement	coefficient for repeatability		
			sensing for 11 d.	of total PAEE (kJ/d) was 0.76		
			Repeatability of the	(P < 0.0001).		
			RPAQ was assessed in an			
			independent sample of 71			
			women and 60 men aged			
			31-57 y.			
Validity of	Golubic R,	To examine the validity of	580 men and 1343 women	RPAQ significantly	Background info,	PLoS
Electronically	May AM,	the Recent Physical	from 10 European	underestimated PAEE and	individualized	One.
Administered	Benjaminse	Activity Questionnaire	countries attended 2 visits	MVPA in women and men.	definition of 1MET	2014
Recent Physical	nBorch K,	(RPAQ) which assesses	at which PA energy	(using individualized	and	Mar
Activity	Overvad K,	physical activity (PA) in 4	expenditure (PAEE), time	definition of 1MET for	non-individualized	25;9(3):
Questionnaire	Charles	domains (leisure, work,	at moderate-to-vigorous	MVPA) Correlations	definition of	e92829.
(RPAQ) in Ten	MA, Diaz	commuting, home) during	PA (MVPA) and	(95% CI) between subjective	1METmay bring in	
European	MJ,	past month	sedentary time were	and objective estimates were	different for the test	
Countries.	Amiano P,		measured using	statistically. When using	result.	
	Palli D,		individually-calibrated	non-individualized definition		
	Valanou E,		combined heart-rate and	of 1MET (3.5 mlO2/kg/min),		
	Vigl M,		movement sensing. At the	MVPA was substantially		

	Franks PW,		second visit, RPAQ was	overestimated		
	Wareham		administered			
	N, Ekelund		electronically. Validity			
	U, Brage S		was assessed using			
			agreement analysis			
Validation of the	Donaire-Go	Validate the Yale Physical	172 COPD patients	Spearman correlations were	Background info	Arch
Yale Physical	nzalez D,	Activity Survey in COPD	(Mean age was 70 (8)	low to moderate (from 0.29		Broncon
Activity Survey	Gimeno-Sa	patients in order to	years) from 8 university	to 0.52, all P<.001). ICCs		eumol.
in chronic	ntos E,	quantify and classify their	hospitals in Spain wore an	showed weak agreement		2011
obstructive	Serra I,	levels of physical activity.	accelerometer	(from 0.34 to 0.40, all		Nov;47(
pulmonary	Roca J,		(SenseWear(®)Pro(2)Arm	P<.001). Significant		11):552-
disease patients.	Balcells E,		band) for 8 days and	differences in accelerometer		60
	et al.		answered the	measurements were found		
			questionnaire 15 days	according to questionnaire		
			later.	tertiles (all P<.001). The area		
				under the ROC for		
				identifying sedentarism was		
				0.71 (95% CI: 0.63-0.79).		

Appendix B

Article Name	Author	Purpose	Methods	Result	Common	Citation
A Review of	Yang CC,	This paper reviews the	The	PA monitoring using	Background Inof	Sensors
Accelerometry-	Hsu YL	development of wearable	authors searched for	accelerometry techniques		(Basel).
Based Wearable		accelerometry-based	published literature after	enables automatic,		2010;10
Motion		motion detectors. Various	year 2000 using a range	continuous and long-term		(8):7772
Detectors for		research using	of related keywords such	activity measurement of		-88
Physical		accelerometry-based	as	subjects in a free-living		
Activity		wearable motion detectors	accelerometry,	environment		
Monitoring		for physical activity	accelerometer, wearable,			
		monitoring and	physical activity, human			
		assessment are also	motion, human			
		reviewed	movement, activity			
			classification, energy			
			expenditure, fall			
			detection, balance			
			stability and			
			gait. Selected literatures			
			before year 2000 are also			
			inc luded			
Fall Detection	Hung CY,	This is a pilot study that	The experiment designed	The BPA can be calculated	Background Info	Journal
and Precaution	Tuan PC	aim to prevent fall by	will integrate body model,	through MEMS		of Nan
through MEMS		integrate accelerometer	accelerometer and Lab	accelerometer. In terms of the		Kai,
Accelerometer.		into a fall detection	View software to	time of fall down will spend		Vol. 6,
		system	measurement the	2.5 second; the 40 degree is		No. 2

			accelerometer output	dangerous postures angular,		(Special
			during the body model	which have 0.5 seconds		Issue on
			fall down. Then calculate	precaution time available.		Geronte
			the Body posture angle			chnolog
			through the accelerometer			y),
			output			pp.81-8
						8 (2009)
A description of	Lyons GM,	To examine the accuracy	2 accelerometer were	'Best estimate' thresholding	Different posture	Med
an	Culhane	of accelerometer in	placed on one CVA	improved sitting detection	threshold setting	Eng
accelerometer-b	KM, Hilton	detecting different	patient for 4days (avg 7	accuracy by 18%, to 93%	have a impact on	Phys.
ased mobility	D, Grace	activities by using 2	hours/day). The	and lying detection accuracy	the accuracy of	2005
monitoring	PA, Lyons	different posture threshold	placement locations	by 5%, to 84%. Compare to	mobility monitor	Jul;27(6
technique	D	methods, mid-point and	include trunk and upper	mip point threshold methods	systems.):497-50
		best estimation	thigh. The patient stays in			4
			an uncontrolled			
			environment			
Respiratory rate	Lapi S,	Identify the applicability	22 normal subjects,	spirometric and	Another possible	RespirP
assessments	Lavorini F,	of accelerometer in	without any respiratory	accelerometric RR values did	application of	hysiolN
using a	Borgioli G,	measuring respiratory rate	issue, 5 obesity patient	not differ in any of the cases.	accelerometer in	eurobiol
dual-accelerom	Calzolai M,	for the patient who has	and 4 patient with	RR assessment was	practical daily	. 2014
eter device	Masotti L	eupnoea and stressed	idiopathic scoliosis. RR	unaffected by recumbence.	treatment.	Jan
	et al.	breathing	was measured by visual	During handgrip, spirometric		15;191:
			inspection, spirometry	(16.43±3.10bpm) and		60-6
			and a pair of	accelerometeric		
			accelerometers positioned	(16.22±2.76bpm) control RR		
			on the torso(T10).	values did not differ and		

			Subjects were asked to	increased to comparable		
			perform spontaneous	levels (24.22±7.30 and		
			breathing, voluntarily	24.82±5.45bpm,		
			modified breathing, and	respectively) by the end of		
			exercise hyperpnoea in	exercise. At rest, visual		
			order to test the validity	(18.94±3.45bpm) and		
			and sensitivity of	accelerometric		
			accelerometer.	(19.27±3.83bpm) RR values		
				were compliant in normal		
				subjects as well as in		
				scoliotic and obese patients		
Estimation of	Liu GZ,	Present an adaptive	Twelve healthy subjects	Experiment results indicated	Background info	Telemed
Respiration	Guo YW,	band-pass filtering	using BSN platform with	the method was capable of		JE
Rate from	Zhu QS,	method combined with	3d accelerometer to	offering pervasive respiration		Health.
Three-Dimensio	Huang BY,	principal component	monitor the RR during	rate monitoring during		2011
nal Acceleration	Wang L,	analysis to derive the	various body activities	various body activities.		Nov;
Data Based on		respiratory rate from	such as sitting, walking,	Furthermore, the result		17(9):
Body Sensor		three-dimensional	running, and sleeping.	demonstrated that this		705–711
Network		acceleration data,		method was more robust,		
				resilient to motion artifact,		
Reliable	Westerterp	Review the evidence that		Accelerometry is the most	Although	CurrOpi
assessment of	KR	presented on the validity		promising method to	accelerometer is	nClinNu
physical activity		of methods to assess		objectively assess physical	able to deliver a	trMetab
in disease: an		physical activity as		activity behavior as a	good objective	Care.
update on		applied in health and		reflection of metabolic health	measurement, there	2014Sep
activity		disease.		or determinant of metabolic	is still 30% of	;17(5):4

monitors				risk. The validity of	variance unable to	01-6.
				accelerometer-based activity	explain. Further	
				monitors is judged with	improvement	
				doubly labelled	should focus on the	
				water-assessed activity	activity other than	
				energy expenditure or PAI as	running, walking,	
				a reference, where the	and light intensity	
				optimal observation time is 1	activities	
				or 2 weeks. Amount all 11		
				accelerometers, Actigraph		
				GT3X, Dynaport, and		
				TracmorD, came out better		
				validity.		
Comparative	Colbert	To compare the validity of	56 adults aged ≥65 yr	All three monitors were	Based on statistical	Med Sci
Validity of	LH,	various physical activity	wore three activity	significantly correlated with	result, although all	Sports
Physical	Matthews	measures with doubly	monitors during a 10-d	PAEE (r=0.48-0.60,	of the methods	Exerc.
Activity	CE,	labeled water	free-living period and	P<0.001). For survey, only	demonstrated	2011
Measures in	Havighurst	(DLW)-measured	completed three different	CHAMPS was significantly	difference when	May;43(
OlderAdults	TC, Kim K,	physical activity energy	surveys. Total energy	correlated with PAEE	compare to DLW, it	5):867-7
	Schoeller	expenditure (PAEE) in	expenditure was measured	(r=0.28, P=0.04). Mean SE	seems that the	6
	DA	free-living older adults	using DLW, resting	for all correlations were high,	monitor was able to	
			metabolic rate was	and different tools was	provide a superior	
			measured with indirect	significantly different from	result than survey.	
			calorimetry	DLW for all but the YPAS		
				and regression-estimated		
				PAEE from the ActiGraph		

WHO Europe,					Background info	http://w
Review of						ww.euro
physical activity						.who.int
surveillance						/data/
data sources in						assets/p
European Union						df_file/0
Member States						005/148
						784/e95
						584.pdf
						Access
						time:
						2015/11/
						27
Methodological	Cliff DP,	The purpose of the review			Background Info	Journal
considerations	Reilly JJ,	is to outline an				of
in using	Okely AD,	evidence-guided protocol				Science
accelerometers		for using accelerometry in				and
toassess		young children and to				Medic in
habitual		identify gaps in the				e in
physical activity		evidence base where				Sport 12
in children aged		further investigation is				(2009)
0–5 years		required				557-567
Physical	Jacobi D,	To evaluate two	Experiment 1, 13	Experiment 1, there was no	Although	Obesity
activity-related	Perrin AE,	accelerometers, the RT3	overweight/obese subjects	significant difference	accelerometer did	(Silver
energy	Grosman	and the TriTrac-R3D for	(BMI 34.2+/-6.4 kg/m2)	between methods in mean	not provide accurate	Spring).

expenditure	N, Dor éMF	their ability to produce	were monitored over 2	PAEE (DLW: 704+/-223	estimates of PAEE	2007
with the RT3		estimates of physical	weeks in everyday life,	kcal/d, RT3: 656+/-140	at individual levels,	Apr;15(
and TriTrac		activity-related energy	PAEE being	kcal/d, TriTrac-R3D	the data suggest that	4):950-6
accelerometers		expenditure (PAEE) in	simultaneously measured	624+/-419	RT3 has the	
in overweight		overweight/obese adults.	by the doubly labeled	kcal/d).Correlation for PAEE	potential to assess	
adults			water method	between RT3 and DLW was	PAEE at group	
			(DLW).Experiment 2, 8	higher than between	levels in	
			overweight/obese subjects	TriTrac-R3D and DLW	overweight/obese	
			(BMI 34.3+/-5.0 kg/m2)	(r=0.67, p<0.05 and r=0.36,	subjects	
			and 10 normal-weight	p=0.25, respectively.		
			subjects (BMI 20.8+/-2.1	Experiment 2, both		
			kg/m2) were monitored	accelerometers were		
			during a treadmill	sensitive to the changes in		
			walking protocol, PAEE	treadmill speed, with no		
			being simultaneously	significant difference in		
			measured by indirect	mean PAEE between		
			calorimetry.	methods in overweight/obese		
				subjects		
A	Lyden K,	The purpose of this study	Two hundred and	Across all activities, each	The estimation	Eur J
comprehensive	Kozey SL,	was to evaluate the	seventy-seven participants	equation underestimated EE	equation is one of	Appl
evaluation of	Staudenme	validity of nine published	completed an average of	(bias -0.1 to -1.4 METs and	the most important	Physiol.
commonly used	yer JW,	and two proprietary EE	six treadmill (TRD) (1.34,	-0.5 to -1.3 kcal,	part during physical	2011
accelerometer	Freedson	prediction equations for	1.56, 2.23 ms(-1) each at	respectively). For ADLs EE	activity	Feb;111
energy	PS	three different	0 and 3% grade) and five	was underestimated by all	measurement. For	(2):187-
expenditure and		accelerometers.	self-paced activities of	prediction models (bias -0.2	now, most of	201.
MET prediction			daily living (ADLs). EE	to -2.0 and -0.2 to -2.8,	equation were	

equations			estimates were compared	respectively), while TRD	generate from Lab	
			with indirect calorimetry	activities were	result, which may	
				underestimated by seven	demonstrate limit	
				equations, and overestimated	applicability when	
				by four equations (bias -0.8	been used in	
				to 0.2 METs and -0.4 to 0.5	practical clinic	
				kcal, respectively).vigorous	field.	
				intensity activities being		
				most often misclassified		
Estimating	Crouter SE,	The purpose of this study	Forty-eight participants	The Actigraph and Actical	Another research	Eur J
energy	Churilla	was to examine the	(age: 35 +/- 11.4 years)	regressions tended to	focus on estimation	Appl
expenditure	JR, Bassett	validity of published	performed various	overestimate walking and	equation, it has the	Physiol.
using	DR Jr.	regression equations	activities that ranged from	sedentary activities and	same result like	2006
accelerometers		designed to predict energy	sedentary behaviors	underestimate most other	Lyden's research,	Dec;98(
		expenditure (EE) from	(lying, sitting) to vigorous	activities. The AMP-331	the equation tend to	6):601-1
		accelerometers	exercise. The activities	gave a close estimate of EE	underestimate the	2
		(Actigraph, Actical, and	were split into three	during walking, but	PA, especially in	
		AMP-331) compared to	routines of six activities,	overestimated sedentary/light	vigorous activity	
		indirect calorimetry, over	and each participant	activities and underestimated	level,	
		a wide range of activities	performed at least one	all other activities. The only		
			routine. The participants	equation not significantly		
			wore three devices	different from actual time		
			(Actigraph, Actical, and	spent in both light and		
			AMP-331) and	moderate physical activity		
			simultaneously, EE was	was the Actigraph Freedson		
			measured with a portable	kcal equation. All equations		

			metabolic system	significantly underestimated		
				time spent in vigorous		
				physical activity ($P < 0.05$).		
Accelerometry	Gorman E,	To investigate the	59 articles were reviewed	The cut-points ranging	For physical	Eur Rev
analysis of	Hanson	appropriate cut point for		between 574 and 3,250	activity level	Aging
physical activity	HM, Yang	mod-vigorous physical		counts/min for MVPA and 50	estimation, one of	Phys
and sedentary	PH, Khan	activity by review former		and 500 counts/min for	the most important	Act.
behavior in	KM,	research. And use the		sedentary time, Based on this	parts is how to	2014;11:
older adults: a		selected cut point to		cut point, the median MVPA	differentiate the	35-49
systematic		analyze accelerometry		minutes per day for	intensity of the	
review and data		data from a sample of		community-dwelling older	activity. So it is	
analysis		community-dwelling		women ranged between 4	important for us to	
		older women		and 80 min while percentage	know the proper cut	
				of sedentary time per day	point to category	
				ranged between 62 % and	the different activity	
				86 %	level, However, due	
					to the difference	
					between the	
					monitor devices,	
					there is no standard	
					cut point	
					recommendation for	
					us to use as	
					reference.	
Physical	Plasqui G,	This review focuses on	The PubMed Central	Many studies showed poor	Interesting article, it	Obesity
activity	Westerterp	the ability of different	database was searched	results. Only a few	point out that	(Silver

assessment with	KR	accelerometers to assess	using the following key	mentioned partial	accelerometer did	Spring).
accelerometers:		daily physical activity as	words: doubly or double	correlations for	not shown a good	2007
an evaluation		compared with the doubly	labeled or labeled water in	accelerometer counts or the	correlation with the	Oct;15(
against doubly		labeled water (DLW)	combination with	increase in R(2) caused by	DLW, I think it may	10):237
labeled water.		technique	accelerometer,	the accelerometer. In	due to many factors,	1-9
			accelerometry, motion	addition, standard errors or	like different	
			sensor, or activity	limits of agreement were	placement location	
			monitor 41 articles were	often large or not presented.	in different	
			identified. 28 article have	The CSA/MTI/Actigraph and	research, moreover,	
			contained sufficient and	the Tracmor were the two	since nearly half of	
			new data. 8 accelerometer	most extensively validated	the selected article	
			were included	accelerometers.	are using CSA and	
					Tracmor, I think	
					there may be	
					individual bias	
					during the article	
					selection process.	
Comparison of	Vanhelst J,	to compare physical	Sixty-two participants,	The concordance correlation	ANOVA shown a	BMC
uniaxial and	B éghin L,	activity (PA) levels and	aged 13-16 years, were	coefficient between two	significant	Med
triaxia laccelero	Duhamel	patterns obtained	recruited in this ancillary	accelerometers at each	difference in lower	Res
metry in the	Α,	simultaneously by triaxial	study, All participants	intensity level was superior	intensity activities,	Method
assessment of	Bergman P,	accelerometry and	wore a uniaxial	to 0.95.The ANOVA test	but the different	ol. 2012
physical activity	et.al	uniaxial accelerometry in	accelerometer (ActiGraph	showedno significant	never exceed 2.1%.	Mar
among		adolescents in free-living	GT1M®, Pensacola, FL)	difference for vigorous		12;12:2
adolescents		conditions	and a triaxial	intensity, Bland & Altman		6
under			accelerometer (RT3®,	method showed good		

free-living			Stayhealthy, Monrovia,	agreement between both		
conditions: the			CA) simultaneously for 7	accelerometers ($p < 0.05$).		
HELENA study.			days			
The use of	Ott AE,	compared the validity of	28 9-11 years children	both kinds of accelerometer	If only focus on	Pediatr.
uniaxial and	Pate RR,	uniaxial accelerometer	when they performed	were able to demonstrate a	simple activity, like	Exerc.
triaxial	TrostSG,Wa	(ActiGraph) with triaxial	eight different free-play	significant correlation	walking or running,	Sci.
accelerometers	rd DS, et al	accelerometer	activities. (Playing a	between the activity counts,	the uniaxial	12:360-
to measure		(Tritrac-R3D)	video game, throwing and	heart rate and predicted MET	accelerometer was	370,
children"free			catching, walking, bench	level. However, compare to	able to provide the	2000
play" physical			stepping, hopscotch,	the uniaxial accelerometer	activity count as	
activity			basketball, aerobic dance,	(r=0.43 with MET, r=0.64	good as triaxial	
			and running)	with heart rate), triaxial	accelerometer,	
				accelerometer was able to	however, triaxial	
				provide a stronger correlation	accelerometer is	
				(r=0.69 with MET, r=0.73	able to monitor	
				with heart rate).	more complicated	
					activities. So we	
					should select the	
					proper device based	
					on our research	
					design and goals.	
Evaluation of	Leenders	Compare different	13 subjects have	The triaxial accelerometer	For the adult, the	Med.
methods to	NY,	methods of measuring	participated in a 7 days	has demonstrated a strong	triaxial	Sci.
assess physical	Sherman	physical activity (PA) in	experimental protocol.	correlation with the results	accelerometer	Sports
activity in	WM,	women by the doubly	The accelerometer was	that measured by DLW ((r	demonstrated a	Exerc.
free-living	Nagaraja	labeled water method	secured at the waist and	=0.54) than uniaxial	superior validity	33:1233

conditions	HN, Kien	(DLW)	attached to a belt.	accelerometer ((r =0.45)	compare to uniaxial	-1240,
	CL				accelerometer,	2001.
					especially at free	
					living environment.	
Validity of	Hendelman	To examine the validity of	25 subjects completed	Observed MET levels	The accelerometer	Med Sci
accelerometry	D, Miller	accelerometry in	four bouts of overground	differed from values reported	is tend to	Sports
for the	K, Baggett	assessing moderate	walking at a range of	in the Compendium of	underestimate	Exerc.
assessment of	C, Debold	intensity physical activity	self-selected speeds,	Physical Activities.	activity level, this is	2000;32
moderate	E, Freedson	in the field and to	played two holes of golf,	Relationships between counts	same with other	(Suppl
intensity	P.	evaluate the metabolic	and performed indoor	and METs were stronger for	research, moreover,	9):442–
physical activity		cost of various	(window washing,	walking (CSA, $r = 0.77$;	accelerometer was	9.
in the field.		recreational and	dusting, vacuuming) and	Tritrac, $r = 0.89$) than for all	able to provide a	
		household activities	outdoor (lawn mowing,	activities combined (CSA, r	stronger correlation	
			planting shrubs)	= 0.59; Tritrac, $r = 0.62$).	only under	
			household tasks, Energy	Metabolic costs of golf and	controlled	
			expenditure was measured	the household activities were	environment or Lab	
			using a portable metabolic	underestimated by 30-60%		
			system and accelerometer.	based on the equations		
				derived from level walking.		
A comparative	Welk GJ,	The purpose of this study	52 participants completed	The correlations between the	Same with	Med.
evaluation of	Blair SN,	was to evaluate the	two 30-min	monitors and measured VO2	Hendelman's	Sci.
three	Wood K,	absolute and relative	choreographed routines,	were higher for treadmill	research, this study	Sports
accelerometry-b	Jones S,	validity of three	Three different treadmill	activity (mean $r = 0.86$)	demonstrated that	Exerc.
ased	Thompson	contemporary activity	paces were completed in	compared with lifestyle	the accelerometer	32:S489
physicalactivity	RW;	monitors (Computer	both routines to evaluate	activity (mean r =	still has limitation	-S497,
monitors		Science and Applications,	reliability and validity	0.55).Correlations among the	when monitor	2000

		Inc. [CSA], Tritrac, and	under laboratory	different monitors were high	activity level in free	
		Biotrainer) under both	conditions. Six different	for both treadmill $(r = 0.86)$	environment.	
		laboratory and field	lifestyle activities were	and lifestyle activities (r =		
		conditions.	also examined to evaluate	0.70), Under field conditions,		
			the validity of the	all of the monitors		
			monitors under field	underestimated EE (range:		
			conditions	42-67% of measured value)		
Conducting	Trost SG,	The purpose of this	Systemic review focus on	No definitive evidence exists	Although there is no	Med.
Accelerometer-	McIver KL,	review is to address	accelerometer selection,	currently to indicate that one	definitive evidence,	Sci.
Based Activity	Pate RR	important methodological	number of accelerometers	make and model of	the validity	Sports
Assessments in		issues related to	needed, placement of	accelerometer is more valid	coefficients for	Exerc.,
Field-Based		conducting	accelerometers, epoch	and reliable than another	multiple axis	Vol. 37,
Research.		accelerometer-based	length, and days of		accelerometers have	No.
		assessments of physical	monitoring required to		been found higher	11(Supp
		activity in free-living	estimate habitual physical		than uniaxial	l), pp.
		individuals	activity.		models. But this	S531–S
					does not mean the	543,
					multiple axis one	2005
					will always superior	
					to uniaxial one, the	
					selection is highly	
					based on research	
					design and goal.	
An	Morillo,	This paper presents a	A trial involving 15	Results demonstrated the	Background info	IEEE.
Accelerometer-	D.S.;	body-fixed-sensor-based	patients at a sleep unit	feasibility of implementing		Trans.
based device for	Ojeda,	approach to assess	was undertaken. Vibration	an accelerometry-based		Inf.

sleep apnea	J.L.R.;	potential sleep apnea	sounds were acquired	portable device as a simple		Technol.
screening.	Foix,	patients.	from an accelerometer	and cost-effective solution		Biomed.
	L.F.C.;		sensor fixed with a	for contributing to the		2010,
	Jim énez,		noninvasive mounting in	screening of sleep		14,
	A.L.		supine position	apnea-hypopnea syndrome		491-499
				and other breathing		
				disorders.		
Measuring	Kuo YL,	To investigate	Twenty typically	The Minimod gave more	Just like the	Gait
distance walked	Culhane	measurement of the	developing children and	accurate measurement of	researcher's	Posture
and step count	KM,	distance walked and step	twenty children with CP,	continuous walking over	suggestion:"Researc	2009,
in children with	Thomason	count in children with CP	aged 4-16 years, were	level ground. On the other	hers and clinic ians	29,
cerebral palsy:	P, Tirosh O,	who have atypical gait by	recruited to study, three	hand, the AMP performed	need to consider	304-310
An evaluation	Baker R.	using portable monitors	walking conditions were	better in detecting the walks	different	
of two portable			performed (continuous	in a structured activity lap	characteristics of	
activity			walking, structured	and during stair ascent and	the monitoring	
monitors.			activity lap walking and	descent	devices and walking	
			stair climbing).		conditions, and	
			Measurements of the		choose an	
			activity monitors were		appropriate device	
			compared to known		that is most	
			walking distances and		reflective of what	
			video recordings for step		they want to	
			count		measure"	
A Randomized	Steele BG,	To evaluate the	One hundred six subjects	There are less decline at 20	intervention	Arch
Clinical Trial of	Belza B,	effectiveness of an	were randomly arrange	weeks in exercise adherence	enhanced exercise	Phys
an Activity and	Cain KC,	exercise adherence	into intervention and	(intervention mean, +3 min;	adherence and	Med

Exercise	Coppersmit	intervention to maintain	usual care groups.	control mean, -13 min;	exercise capacity in	Rehabil.
Adherence	h J	daily activity, adherence	Intervention group	P=.015) and exercise	the short term but	2008
Intervention in		to exercise, and exercise	include Twelve-week	capacity (intervention mean,	produced no	Mar;89(
Chronic		capacity over 1 year after	adherence intervention	-10.7 m; control mean, -35.4	long-term benefit.	3):404-1
Pulmonary		completion of an	(weekly phone calls and	m; P=.023). There were no	The primary	2.
Disease.		outpatient pulmonary	home visit) including	differences in daily activity	endpoint of daily	
		rehabilitation program	counseling on	at 20 weeks or any	activity measures	
			establishing, monitoring,	differences in any primary	by accelerometer	
			and problem-solving in	variable at 1 year.	did increase more	
			maintaining a home		during the exercise	
			exercise program.		adherence	
			Primary outcomes		intervention in the	
			included daily activity		intervention group	
			(accelerometer), exercise		than in the control	
			adherence (exercise		group, but after	
			diary), and exercise		controlling for	
			capacity (six-minute walk		baseline differences	
			test). All measures were		this was not	
			performed at baseline,		statistically	
			after the pulmonary		significant	
			rehabilitation program (8			
			wk), after the adherence			
			intervention (20 wk), and			
			at 1 year.			
Accelerometers	Corder K,	This review examines		Accelerometry is able to	Background for	Current
and pedometers:	Brage S,	recent literature on the		adequately assess physical	accelerometer	Opinion

methodology	Ekelund U	validation of movement		activity but currently	selection	in
and clinical		sensors to assess habitual		methods have limited		Clinical
application		physical activity.		accuracy for the estimation		Nutritio
				of free-living energy		n and
				expenditure. Pedometers		Metabol
				provide an inexpensive		ic Care.
				overall measure of physical		ssue:
				activity but are unable to		Volume
				assess intensity, frequency		10(5),
				and duration of activity or to		Septemb
				estimate energy expenditure		er 2007,
						p
						597–603
Assessment of	Nichols JF,	compare the validity of	Validity was determined	The relationship between	This article shown	Res Q
physical activity	Morgan	the Computer Science and	in 60 adults during	CSA counts and VO2 was	that the preset	Exerc
with the	CG, Chabot	Applications, (CSA) Inc.,	treadmill exercise, using	linear ($R2 = .89 \text{ SEE} = 3.72$	equation that based	Sport.
Computer	LE, Sallis	accelerometer in	oxygen consumption	ml.kg-1.min-1), as was the	on lab finding may	2000;71
Science and	JF, Calfas	laboratory and field	(VO2) as the criterion	relationship between velocity	not appropriate for	:36–43.
Applications,	KJ	settings and establish	measure, while 30 adults	and counts in the field (R2	use in the field	
Inc.,		CSA count ranges for	walked and jogged	= .89, SEE $= 0.89$ mi.hr-1).	settings.	
accelerometer:		light, moderate, and	outdoors on a 400-m	There is a significant		
laboratory		vigorous physical activity	track.	different between lab and		
versus field				field for light and vigorous		
validation				intensity.		
Wearable	Allet L,	This review aims to	In March 2009 a librarian	25 articles were included,	feasible methods for	Sensors
systems for	Knols RH,	identify the actual state of	performed an electronic	two RCTs focusing on	monitoring human	(Basel).

monitoring	Shirato K,	applying wearable	search on PubMed and the	arthritis,	mobility are	2010;10
mobility-related	de Bruin	systems for monitoring	Physiotherapy Evidence	four focusing on COPD, six	available,	(10):902
activities in	ED,	mobility-related activity	Database (PEDro). The	focusing on CVD, and 13	evidence-based	6-52
chronic disease:		in individuals with	keywords include:	focusing on Diabetes	clinical applications	
a systematic		chronic disease	(chronic diseases OR		of these methods in	
review		conditions. Focus on	cardiovascular disease OR		individuals with	
		technologies and	CVK OR diabetes OR		chronic diseases are	
		applications, feasibility	diabetic OR COPD OR		in need of further	
		and adherence aspects,	osteoarthritis) AND (gait		development	
		and clinical relevance of	disorder OR walking OR			
		wearable motion sensing	kinematic OR gait			
		technology	analysis system OR gait			
			analysis device) AND			
			(accelerometer* OR			
			pedometer* OR			
			gyroscope* OR wearable			
			system OR activity			
			monitor OR motion			
			sensing OR			
			instrumentation OR			
			equipment) AND			
			(physical activity OR			
			motor activity OR			
			activity).			
Validity of	Evangelista	Determine if pedometers	Exercise adherence was	Patients who showed	Subject age	J Card
pedometers for	LS, Dracup	offered a practical,	measured using	improvements in their	between 18 and 80	Fail.

measuring	K, Erickson	cost-effective, and	pedometers in 38 patients	pedometer scores (>10%)	years with advanced	2005
exercise	V,	acceptable assessment	(74% men) age 54.1 ±	over 6 months had better	HF defined as left	Jun;11(5
adherence in	McCarthy	strategy that could be	11.7 years who	functional status at 6 months	ventricular systolic):366-71
heart failure	WJ	used with confidence to	participated in a 12-month	(6-minute walk distance 1718	dysfunction with a	
patients		measure exercise	home-based walking	± 46 versus 1012 ± 25	left ventricular	
		adherence to a	program. They will have a	meters, $F = 5.699$, $P = .022$;	ejection fraction	
		home-based walking	baseline test at the	VO2 max 17 ± 0.7 versus 10	≤40% and New	
		program among HF	beginning of research	$\pm 0.5 \text{ units}, F = 7.162, P$	York Heart	
		patients	session and a comparison	= .011) when compared with	Association class	
			of functional status as	patients whose pedometers	II-IV. Pedometers	
			measured by the 6-minute	reflected minimal change in	were given to	
			walk distance and peak	distance walked	patients and they	
			oxygen uptake (VO2		were also asked to	
			max) at 6 months		complete daily	
					activity diaries for	
					the first 6 months of	
					the trial.	
Evaluation of a	Sant'Anna	To assess the criterion	Patients with COPD	Correlations between the	video and the	Arch
new motion	T, Escobar	validity and	(N=30; 17 men; forced	pedometer and the criterion	multi-sensor is	Phys
sensor in	VC,	reproducibility of a new	expiratory volume in the	method were high for SC	criterion methods.	Med
patients with	Fontana	pedometer in patients	first second, 44±17%	during slow and fast walking		Rehabil.
chronic	AD,	with chronic obstructive	predicted) were	(r=.79 and r=.95) and for EE		2012
obstructive	Camillo CA	pulmonary disease	videotaped while	during fast walking		Dec;93(
pulmonary		(COPD).	performing 2 protocols:	(r=.83).During the ADLs		12):231
disease			one including 2 slow and	circuit, the pedometer		9-25.
			2 fast 5-minute walks, and	underestimated AT by an		

			I			
			another including a circuit	average of 55% but provided		
			of activities of daily living	an acceptable EE estimation		
			(ADLs). Concomitantly,	in a group basis		
			patients wore 2 motion			
			sensors: the new			
			pedometer and a			
			multi-sensor			
			accelerometer			
The doubly	Wong WW,	This study was designed			Background info for	J Nutr.
labeled water	Roberts	to evaluate the			DLW test	2014
method	SB, Racette	longitudinal				May;14
produces highly	SB, Das	reproducibility of the				4(5):777
reproducible	SK, et.al.	DLW method using 2				-83.
longitudinal		protocols developed and				
results in		implemented in a				
nutrition studies		multicenter clinical				
		trial-the Comprehensive				
		Assessment of Long-term				
		Effects of Reducing				
		Intake of Energy				
		(CALERIE)				

Appendix C

Article Name	Author	Purpose	Methods	Result	Common	Citation
2013 ACCF/AHA	Yancy CW, Jessup M,				CHF background	Circulatio
Guide line for the	Bozkurt B, Butler J,				info	n.
Management of Heart	Casey DE Jr, et.al.					2013;128:
Failure: Executive						1810-185
Summary: A Report of the						2;
American College of						
Cardiology						
Foundation/American						
Heart Association Task						
Force on Practice						
Guidelines						
Guide lines for the	Karl Swedberg,				Background info	European
diagnosis and treatment of	Go teborg					Heart
chronic heart failure:						Journal
executive summary						(2005) 26,
(update 2005) The Task						1115–114
Force for the Diagnosis						0
and Treatment of Chronic						
Heart Failure of the						
European Society of						
Cardiology						
Heart Rhythm Society,					Background info	http://ww
Ejection Fraction						w.hrsonli

					ne.org/Pat
					ient-Reso
					urces/The
					-Normal-
					Heart/Eje
					ction-Frac
					tion#axzz
					35ZUt3Qr
					E, assess
					time,
					06/22/201
					4
Effects of exercise on left	Zile MR, Kjellstrom	The purpose of the	Subjects with HF and	Although	Circ
ventricular systolic and	B, Bennett T, Cho Y,	current study was to	a preserved EF (n=8)	exercise	Heart
diastolic properties in		define	and subjects with HF	limitations	Fail. 2013
patients with heart failure		exercise-induced	and a reduced EF	were similar	May;6(3):
and a preserved ejection		changes in indices of	(n=5) underwent	between HF	508-16.
fraction versus heart		left ventricular (LV)	symptom-limited	and a reduced	
failure and a reduced		systolic and diastolic	Naughton protocol	EF and HF and	
ejection fraction		properties in patients	treadmill exercise	a preserved	
		with chronic heart	tests. Implantable	EF, there were	
		failure (HF), compare	hemodynamic monitor	significant	
		these changes in	data and	differences in	
		patients with HF and	echocardiographic data	exercise-induc	
		a reduced ejection	were obtained before	ed changes in	
		fraction (EF) versus	exercise and at peak	LV systolic	

		HF and a preserved	exercise. Implantable	and diastolic	
		EF, and compare the	hemodynamic monitor	properties	
		hemodynamic	data were obtained		
		responses to activities	during activities of		
		of daily living with	daily living during a		
		symptom-limited	24-hour time period.		
		upright exercise.			
Cardiovascular	Heusch G, Libby P,				Lancet.
remodelling in coronary	Gersh B, Yellon D				2014 May
artery disease and heart					31;383(99
failure					32):1933-
					43.
Effects of different	Feiereisen P, Vaillant	analyze the effects of	Patients with CHF (N	Exercise	J
training modalities on	M, Gilson G,	3 different training	= 45), NYHA class	training has no	Cardiopul
circulating	Delagardelle C	modalities (endurance	II-III, left ventricular	effects on	mRehabil
anabolic/catabolic		training, strength	ejection fraction <	circulating	Prev.
markers in chronic heart		training, and	35%, were randomly	IGF-1 and GH.	2013
failure		combined strength	assigned to 1 of 3	The decreases	Sep-Oct;
		and endurance	training modalities.	in cytokines	33(5):303
		training [CT]) on	They trained for 40	are evident	-8
		circulating cytokines,	sessions, 3 times	only when all	
		IGF-1, and GH levels.	weekly. Fifteen CHF	trained	
			patients served as a	patients are	
			control group. Blood	compared with	
			samples were collected	the control	
			at baseline and 48	group,	

		hours after the last training session	independently of the modality of		
			training		
A cuto va chucuic hymovicu	Daldia ava I		intervention.	Based on the	Cell
· -	Deldicque L,				
1	Francaux M			literature review,	MolExerc
for skeletal muscle mass?				hypoxia itself	Physiol.
				contributes to the	2013;2(1)
				loss of muscle mass	:1–23.
				during chronic	
				hypoxia	
Skeletal muscle	Gosker H.R.,			chronic hypoxia	Am J
dysfunction in chronic	Wouters E.F., van			will cause the	ClinNutr.
obstructive pulmonary	der Vusse GJ.,			muscle fiber	71
disease and chronic heart	Schols A.M			alternation and	2000:103
failure: underlying				changing the	3-1047
mechanisms and therapy				muscle function	
perspectives.				based on the type	
				of muscle	
The response of human	Lundby C, Calbet JA,			The same to	Cell
-	Robach P			Gosker's research.	MolLife
hypoxia				chronic hypoxia	Sci 2009,
				will cause the	66:3615-3
				muscle fiber	623
				alternation and	

					changing the muscle function	
					based on the type	
					of muscle	
A re-examination of the	Savage PD, Toth MJ,	Compare the	109 (60 men and 49	Mean resting	The patient with	J
metabolic equivalent	Ades PA	traditionally accepted	women) subjects with	value for 1	CAD may present	Cardiopul
concept in individuals		value for 1 MET to	documented coronary	MET was a	decreased MET	mRehabil
with coronary heart		direct measurements	heart disease and a	VO2 value of	level when	Prev.
disease		of resting metabolic	body mass	2.58 +/- 0.4	compare to the	2007
		rates in a group of	index >or=25 kg/m2.	mL	healthy population.	May-Jun;
		stable individual with	Measurements	O2.kg(-1).min	Future studied are	27
		coronary heart disease	included indirect	(-1) for	required.	(3):143-8
			calorimetry, body	overweight		
			composition, and	subjects		
			exercise capacity	measured in		
			(peak oxygen uptake	the supine		
			[VO2]). In a sub study	position and		
			of 17 (10 men, 7	2.84 +/- 0.59		
			women) normal	mL.O2.kg(-1).		
			weight subjects (body	min(-1) for		
			mass index <25	normal weight		
			kg/m2), metabolic rate	individuals		
			in the seated position	measured in		
			was also measured.	the seated		
				position.		
				Caloric		

	expendit	ure
	value wa	as 0.74
	+/- 0.12	
	kcal.kg(-	1).h(-
	1) rather	than
	the expe	cted
	value of	1
	kcal.kg(-	1).h(-
	1).	

Appendix D



COLLEGE OF NURSING

Lincoln Division

ADULT INFORMED CONSENT FORM IRB # 394-07-FB

Title of this Research Study

PSYCHOMETRIC TESTING OF MEASURES TO ESTIMATE ENERGY EXPENDITURE IN ELDERLY HEART FAILURE PATIENTS

Invitation

You are invited to take part in this research study. The information in this form is meant to help you decide whether or not to take part. If you have any questions, please ask.

Why are you being asked to be in this research study?

You being asked to be in this study because you are 60 years or older and you are currently receiving treatment for heart failure from the BryanLGH Heart Institute. You must be able to speak and read English in order to complete questionnaires about your daily physical activity.

What is the reason for doing this research study?

The purpose of this study is to evaluate ways to measure daily physical activity levels in heart failure patients.

What will be done during this research study?

If you decide to participate, you will be asked to complete two questionnaires that ask you about your activity levels for the past 7 days. You will also be asked to complete two questionnaires that ask you about your sleep and one questionnaire that asks you about your mood. If you respond that you are feeling down, depressed or hopeless nearly every day we will refer you to your primary care provider for evaluation.

You will wear three activity monitors for 7 days. One of the monitors is the size of a pager or small cell phone and fastens on to the waistband of your slacks. The second monitor snaps on to two electrodes (similar to those used for an EKG) that are placed on your upper chest. The third monitor is similar to a watch and is worn on your wrist. These activity monitors are commercially available.

It will take approximately 60 minutes for you to complete the questionnaires and get the activity monitors put on. You will not need to do anything with the activity monitors other than wear them.

IRB RE-APPROVED 7/16/09
VALID UNTIL 7/16/10

Subject's Initials

Commerce Court / P.O. Box 880220 / Lincoln, NE 68588-0220 / (402) 472-3657 / FAX (402) 472-7345

IRB # 394-07-FB Page 2 of 5

You will return to the clinic at the end of 7 days to turn in the activity monitors and complete two questionnaires about your activity over the past 7 days. This visit will take no more than 45 minutes.

What are the possible risks of being in this study?

The electrodes that are used to place one of the activity monitors on your chest could irritate your skin. Additional electrodes will be sent home with you to change where it is located on your chest so it does not irritate your skin.

It is possible that other rare side effects could occur which are not described in this consent form. It is also possible that you could have a side effect that has not occurred before.

What are the possible benefits to you?

You are not expected to get any benefit from being in this research study.

What are the possible benefits to other people?

The information obtained from this study may help other patients by providing information about ways to evaluate or measure daily physical activity in patients with heart failure.

What are the alternatives to being in this research study?

Instead of being in this research study you can choose not to participate. If you decide not to participate you would continue to receive usual care from the BryanLGH Heart Institute.

What will being in this research study cost you?

There is no cost to you to be in this research study. Travel to BryanLGH Heart Institute for testing (at the beginning and one week later) is necessary and these costs are your responsibility.

Will you be paid for being in this research study?

You will not be paid to be in this research study.

Who is paying for this research?

This research is being paid for by grant funds from the American Nurses Foundation. The University of Nebraska Medical Center receives money from the American Nurses Foundation to conduct this study.

IRB RE-APPROVED 7/16/09 VALID UNTIL 7/16/16	Subject's Initials	_

IRB # 394-07-FB Page 3 of 5

What should you do if you are injured or have a medical problem during this research study?

If you are injured or have a medical problem as a result of being in this study, you should immediately contact one of the people listed at the end of this consent form.

How will information about you be protected?

You have rights regarding the privacy of your medical information collected before and during this research. This medical information, called "protected health information" (PHI), includes demographic information (like your address and birth date), the results obtained from the questionnaire and the activity monitors, as well as your medical history. You have the right to limit the use and sharing of your PHI, and you have the right to see your medical records and know who else is seeing them.

By signing this consent form, you are allowing the research team to have access to your PHI. The research team includes the investigators listed on this consent form and other personnel involved in this specific study at UNMC and the Nebraska Medical Center.

Your PHI will be used only for the purpose(s) described in the section "What is the reason for doing this research study?" Your PHI will be shared, as necessary, with the Institutional Review Board (IRB) and with any person or agency required by law. You are also allowing the research team to share your PHI with other people or groups listed below. All of these persons or groups listed below are obligated to protect your PHI.

Your health insurance company.

Your PHI may also be shared with the American Nurses Foundation, which sponsors this research and provides funds to the UNMC/THE NEBRASKA MEDICAL CENTER to conduct this research. However, this organization does not have the same obligation to protect your PHI.

You are authorizing us to use and disclose your PHI for as long as the research study is being conducted.

You may cancel this authorization to use and share your PHI at any time by contacting the principal investigator in writing. If you cancel this authorization, you may no longer participate in this research. If you cancel this authorization, use or sharing of future PHI will be stopped. The PHI which has already been collected may still be used.

The information from this study may be published in scientific journals or presented at scientific meetings but your identity will be kept strictly confidential.

IRB RE-APPROVED 7/16/04
VALID UNTIL 7/16/15

<u>IRB # 394-07-FB</u> Page 4 of 5

What are your rights as a research subject?

You have rights as a research subject. These rights are explained in this consent form and in *The Rights of Research Subjects* that you have been given. If you have any questions concerning your rights or complaints about the research, talk to the investigator or contact the Institutional Review Board (IRB) by telephone (402) 559-6463, e-mail: IRBORA@unmc.edu, or mail: UNMC Institutional Review Board, 987830 Nebraska Medical Center, Omaha, NE 68198-7830.

What will happen if you decide not to be in this research study?

You can decide not to be in this research study at any time. Deciding not to be in this research study will not affect your medical care or your relationship with the investigators, the University of Nebraska Medical Center or BryanLGH Heart Institute. Your doctor will still take care of you and you will not lose any benefits to which you are entitled.

What will happen if you decide to stop participating once you start?

You can stop being in this research study ("withdraw") at any time. Deciding to withdraw will otherwise not affect your care or your relationship with the investigator, the University of Nebraska Medical Center or BryanLGH Heart Institute. You will not lose any benefits to which you are entitled.

You may be taken off the study if you don't follow instructions of the investigator or the research team. You may also be taken off the study if your medical condition changes.

If the research team gets any new information during this research study that may affect whether you would want to continue being in the study you will be informed promptly.

Documentation of informed consent

You are freely making a decision whether to be in this research study. Signing this form means that (1) you have read and understood this consent form, (2) you have had the consent form explained to you, (3) you have had your questions answered and (4) you have decided to be in the research study.

If you have any questions during the listed below. You will be given a co			investigators			
Signature of Subject:		Date:	_ Time:			
My signature certifies that all the elements of informed consent described on this consent form have been explained fully to the subject. In my judgment, the participant possesses the legal capacity to give informed consent to participate in this research and is voluntarily and knowingly giving informed consent to participate.						
Person obtaining consent:			Time: Initials			
IRB RE-APPROVI	116/10	•				

IRB # 394-07-FB

Page 5 of 5

Authorized Study Personnel

Principal Investigator:

Bunny Pozehl, PhD, APRN 402-472-7352 (w) 402-429-5289 (h)

Secondary Investigators:

Kathleen Duncan, PhD, RN 402-472-7338(w) 402-488-8395 (h)

Joe Norman, PhD 402-559-5715 (w) 402-339-3708 (h)

Melody Hertzog, PhD 402-472-3260 (w)

Participating Personnel:

Ann Ziemann Walker, BSN, RN 402-525-3880 (h)

Participating Personnel Lisa Bauer, MSN, RN 402-932-1849 (h)

Participating Personnel Lindsey Adam, BSN, RN 402-314-1359

IRB RE-APPROVED 7/16/09
VALID UNTIL 7/16/10



COLLEGE OF NURSING Lincoln Division

IRB #394-07-FB – Addendum Consent Form

Page 1 of 3

Title of this Research Study

PSYCHOMETRIC TESTING OF MEASURES TO ESTIMATE ENERGY EXPENDITURE IN ELDERLY HEART FAILURE PATIENTS

You are invited to take part in an additional 36 minutes of physical activity monitoring. The monitoring will involve wearing the activity monitors (like you wore previously) for 36 minutes of activity. You will breathe into a face mask that will monitor your oxygen levels as you participate in 24 minutes of light activity (e.g., reading the newspaper, watching television, washing dishes, dusting), 6 minutes of moderate activity (e.g., vacuuming, stair climbing), and a 6 minute walk test.

The monitoring itself will take 36 minutes to complete. Fifteen minutes will be needed to get the monitoring equipment on and you will be required to rest for 15 minutes after completion of the activity.

The 6 minutes of moderate intensity activity and the 6 minute walk test have potential associated risks of heart rate and blood pressure changes, fatigue, shortness of breath, muscle and joint discomfort. Your blood pressure, heart rate and oxygen level will be checked before and after each activity. The mouthpiece may be uncomfortable during the test and may cause some soreness in the mouth. You should be aware that these tests involve the possible risk of falls and/or muscle-joint injuries. You will be closely monitored throughout the test procedures by a nurse practitioner and an American College of Sports Medicine certified exercise physiologist. The activities and tests will be performed at the BryanLGH Heart Institute where a cardiologist is available if needed. You will be closely monitored throughout the test procedures and you will regularly be asked to rate your level of distress to help determine your response to the activity. If you need to stop because you are feeling distress your blood pressure, heart rate and oxygen level would be checked immediately. Following the 30 minutes of activity, you will be required to rest to help establish you are not experiencing any activity related changes. Your blood pressure, heart rate and oxygen level would be checked at the end of this rest period.

It is possible that other rare side effects could occur that are not described in this consent form. It is also possible that you could have a side effect that has not occurred before.

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IRB RE-APPROVED 7	6	09	
VALID UNTIL 7/167			
and the same of th			

IRB #394-07-FB – Addendum Consent Form

Page 2 of 3

If you are injured or have a medical problem as a direct result of being in this study, you should immediately contact one of the people listed at the end of this consent form. Immediate emergency medical treatment for this injury will be available at BryanLGH Medical Center. You or your insurance company will need to pay for any costs. The costs for any other medical problems unrelated to this research study are also your responsibility. There are no plans to provide payment for things like lost wages, disability or discomfort. Agreeing to this does not mean you have given up any legal rights.

Your willingness to complete this activity monitoring will provide you with information about your tolerance of light to moderate activity. You are not expected to get any benefit from completing this activity.

Instead of completing this activity you can choose not to participate. There is no cost to you to complete this activity. You will not be paid to do this.

You can decide not to do this activity at any time. Deciding not to do this test will not affect your medical care or your relationship with the investigators, the University of Nebraska Medical Center, or BryanLGH Heart Institute. Your doctor will still take care of you and you will not lose any benefits to which you are entitled.

Documentation of informed consent

You are freely making a decision whether to complete this 36 minutes of activity monitoring. Signing this form means that (1) you have read and understood this consent form addendum, (2) you have had the addendum form explained to you, (3) you have had your questions answered and (4) you have decided to do the test.

If you have any questions, you should talk to one of the investigators listed below. You

will be given a copy of this consent form to keep.		
Signature of Subject:	Date:	Time:
My signature certifies that all the elements of informed consent form have been explained fully to the subject. I possesses the legal capacity to give informed consent to soluntarily and knowingly giving informed consent to present the soluntarily and knowingly giving informed consent to present the soluntarily and knowingly giving informed consent to present the solution.	In my judgment, o participate in tl	the participant
Person obtaining consent:	Date:	Time:
1	Subject'	s Initials
7/1/6		

IRB #394-07-FB – Addendum Consent Form

Page 3 of 3

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Participating Personnel Lindsey Adam, BSN, RN 402-314-1359

IRB RE-APPROVED 7/// 04
VALID UNTIL 7////

Appendix E

		Subject C	Dateode Number
Modified 7 Da	ny Physical Activ	ity Record	
I would like to know about your physical acti the last weekend, Saturday and Sunday. This week, not a history of what you usually do.			
A. Your Sleeping Habits:			
First let me ask you about your sleeping habit	ts.		
How many hours did you sleep on average ea quarter-hour, that is 0, 15, 30 or 45 minutes).		e last 7 nights? (Reco	rd to the nearest
hours minutes/night X 7	night/week		
Did you nap during the day?yes	no		
If yes, how much time did you spend	napping?		
hours minutes/day X	day/week		
B. Your Physical Activity:			
Now I am going to ask about your physical a how much time you spent doing various activity to include it. Do not include rest periods.	rities. You must ha	ave spent at least 5 mi	
Light A	Activities <	2.0 METS	
First, let's consider light activities or activities much time did you spend:	s that involve sitting	ng or standing with litt	tle movement. How
Watching TV	hours	minutes/day X	days/week
Reading	hours	minutes/day X	days/week
Playing Cards	hours	minutes/day X	days/week
Ironing	hours	minutes/day X	
Knitting	hours	minutes/day X	days/week
Cooking	hours	minutes/day X	days/week
Can you think of any other activities that you	did this nest week	that are of similar in	tancity?
Can you think of any other activities that you		minutes/day X	
(list activity)	nours	illilidics/day A	days/ week
(iist abtivity)	hours	minutes/day X	days/week
(list activity)			
(list activity)	hours	minutes/day X	days/week
(

Moderate Activities 2-3.9 METS

Now let's look at moderate activities. How	much time did you	spend:	
Cleaning	hours	minutes/day X	davs/week
Shopping		minutes/day X	
Raking the lawn	hours	minutes/day X	days/week
Fishing	hours	minutes/day X	days/week
Painting (not ceilings)	hours	minutes/day X	
Walking less than 3 miles per hour	hours	minutes/day X	days/week
Home repair	hours	minutes/day X	days/week
Riding or pushing a power lawn mower	hours	minutes/day X	days/week
Golfing with a cart	hours	minutes/day X	days/week
(list activity) (list activity)		minutes/day X minutes/day X	
Haro	Hard Activities		
Now let's look at hard activities. How muc	h time did you sper	nd doing hard activities	Ε
Golfing, walking and pulling			
or carrying clubs	hours	minutes/day X	days/week
Walking on a level surface			-
at least 3 miles per hour	hours	minutes/day X	days/week
Scrubbing floors	houre	minutes/day X	days/week
Painting ceilings			
	hours	minutes/day X	days/week
Mowing a lawn with a power mower	hours		days/week
Mowing a lawn with a power mower Can you think of any other activities that you at a brisk pace (1 miles in 20 minutes or less	hours hours ou did this past weeks)?	minutes/day X minutes/day X ek that are of similar in	days/week days/week tensity to walking
Can you think of any other activities that you	hours hours ou did this past weeks)?	minutes/day X minutes/day X ek that are of similar in minutes/day X	days/week days/week tensity to walking days/week
Can you think of any other activities that year a brisk pace (1 miles in 20 minutes or les	hours hours ou did this past weeks)?	minutes/day X minutes/day X ek that are of similar in	days/week days/week tensity to walking days/week

Very Hard Activities >6.0 METS

Now let's look at very hard activities. How	much time did you s	pend:		
Digging Swimming (breast stroke) Walking on a hilly terrain at least 3 mph	hours hours hours	minutes/day X minutes/day X minutes/day X	- 1	
Can you think of any other activities that you did this past week that are of similar intensity to walking on a hilly terrain at a brisk pace (1 mile in 20 minutes or less)?				
(list activity)	hours	minutes/day X	=	
(list activity)	hours	minutes/day X	_ days/week	
Hellman, Williams, and Thalken, 1996				