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Bacterial cellulose-based hydrogel for wound healing: characterization and in vitro evaluation

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ABSTRACT

Bacterial cellulose (BC) has been considered a promising biopolymer with applications in several areas of knowledge, including medicine, mainly due to its ability to assist in the treatment of dermal lesions. Many groups and companies have been making efforts to develop new BCbased materials in order to add new characteristics and therapeutic possibilities. Recently, Seven Indústria de Produtos Biotecnológicos Ltda company developed a BC-based hydrogel aiming to verify the interaction among the formulation components, its potential for wound healing and biocompatibility studies. BC-based hydrogel was characterized and compared with pristine BC film. Physicochemical characterization includes rheological measurements, thermal analyses, field emission gun - scanning electron microscopy (FE-SEM) and in vitro cell migration. BCbased hydrogel showed adequate interaction among the components of the formulation, which may positively influence its stability. In addition, the BC-based hydrogel accelerated the healing processes demonstrating its potential in dermal lesion treatment.

Introduction

Cellulose is the most abundant biopolymer on earth frequently obtained from plant sources. However, plant cellulose and BC show properties fairly different, which allow its applications in various fields such as physics, chemistry engineering and biological sciences. Additionally, BC production is an extremely pure process, which is entirely free of pectin, lignin and hemicelluloses, without components from animal origin and without causing any allergic reaction leading to simpler purification process related to plant cellulose (1,2).

Currently, several microorganisms have been reported with the ability to produce BC, however Gram-negative bacteria of Gluconacetobacter genus have received great prominence in recent years due to their capacity to producecellulose in commercial quantities. During the biosynthesis, thesebacteria are able to synthesize cellulose in the form of membranesat the air/liquid interface of the static culture medium. These membranes present highly porous structures constituted of a random microfibrillar 3D-network of cellulose chains aligned in parallel with high permeability to fluids been favorable for adhesion

and proliferation of cells (2-6).

BC membranes have shown to be a promising biomaterial for treatment of wounds healing, burns, tissue implants due to its unique properties such as high crystallinity, high mechanical strength, ultrafine fiber network structure and high water-uptake capability (water content >90 %). BC provided a humid environment to the affected region promoting the exudate absorption and the wounds healing acceleration without any toxicity (1,2,4,7,8). In addition, randomly arranged cellulose nanofibers mimic some components of the extracellular matrix, such as collagen fibers, since they have similar diameter (near to 100 nm), which promotes a faster healing process (9).

BC membranes have been commercialized as an ideal wound dressing device due to its high in vivo biocompatibility and great efficacy when applied in cutaneous lesions promoting healing more efficiently than other products available for this purpose. In addition, BC membranes consists on hysical barriers that reduce pain and bacterial infections (6,10).

The mechanical treatment (defibrillation process) of BC membranes originates a dispersion of nanofibers

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which may to be incorporated into hydrogels, giving rise to a new therapeutic possibility for the treatment of burns, The storage modulus (G'), loss modulus (G") and comchronic ulcers, skin lesions and other lesions, protecting plex viscosity (η^*) were performed as a function of angutissues formed around and over the wound (11). The possilar frequency range of 0.1-500 rad s⁻¹. bility of treating deeper wounds, in which CB membranes are not capable of shaping the injured area, has been the Thermal analysis subject of intense research by Seven Indústria de Produ-Lyophilized BC-based hydrogel (Nexfill[®] Hydrogel) tos Biotecnológicos Ltda. (Brazil), since this characteristic was evaluated by differential scanning calorimetry (DSC) can lead to successfully commercialization of BC-based technique using a DSC1 STARe System-Mettler Toledo. hydrogel (e.g. Nexfill[®]). The sample of \pm 5 mg were submitted to heating from 25to

Hydrogels are three-dimensional configurable polymers network with ability to absorb large amounts of water, saline and physiological solutions compared with general absorbent materials. They show excellent hydrophilic properties along with their high swelling ratio and biocompatibility, promoting their widely usage in biomedical, tissue engineering and drug delivery. Other characteristics of hydrogels are the long-term stability, facility of biochemical modification of the formed structures and the incorporation of several products inorder to combine the most important characteristics of each one (12-17).

To the best of our knowledge, few studies have in-The surface morphology of the lyophilized BC-based vestigated physicochemical characteristics and in vitro hydrogel (Nexfill® Hydrogel) was investigated by scanproperties of BC-based hydrogel. Herein, we report the ning electron microscopy FE-SEM on a JEOL microscope evaluation of the hydrogel containing BC as well as the (model JSM-7500F, Japan). The sample was frozen at -80 interaction between the formulation components keeping °C and lyophilized for 24 h. After that, lyophilized sample the wound healing properties of the BC without toxicity was attached to slab surface with double sided adhesive effects. tape and coated with carbon as conductive material. The sample was examined using an accelerating voltage of 2 Materials and methods kV. FE-SEM from pristine BC films were also obtained Materials as described by Machado et al. 2016 and compared with BC-based hydrogel (Nexfill[®] Hydrogel) was provided hydrogel results.

by Seven Indústria de Produtos Biotecnológicos Ltda. (Ibiporã, PR, Brazil) for further characterization and in vitro evaluation. The BC-based hydrogel (Nexfill[®] Hydrogel) composition was obtained according to the PI 0601330-9 A2 patent.

Fibroblast cultures internally isolated by Invitrocell, of city of Paulínia, São Paulo (Brazil) for donation of explant human cells. Cells were cultivated T-75 cm² flasks con-**Rheological properties** taining Dulbecco's modified Eagle's medium (DMEM), Rheological properties of the BC-based hydrogel (Nexsupplemented with 10 % fetal bovine serum (FBS), penicillin and streptomycin ((Sigma Aldrich®), USA), at 37 fill® Hydrogel) were evaluated using an Anton Paar rheometer (MCR302), equipped with two parallel-plates (PP 25) °C in humidified atmosphere containing 5 % CO₂ The sensor with a 25 mm, the gap between plates was 1.00 mm medium was changed every dayuntil cells reach 80-90 % and temperature of 32 °C. Rheo Compass[™] software was confluence, when fibroblasts were split with 0.05 % Trypsin/0.02 % EDTA. used to analyze the data.

The Flow curve was analyzed with shear rate range from 0 to 100 Pas⁻¹ for the ascent ramp for 120 s and from 100 to 0 Pas⁻¹ for the descent ramp for 120 s and it was applied "Power Law" model, according to Equation 1:

The evaluation of fibroblast migration allows the evaluation of the ability of cells to repair an opening in the $\tau = K \times \gamma^n \tau = K \times \gamma^n$ (Equation 1) culture caused by injury. The test substance, BC-based Where τ is shear stress, γ is shear rate, K is consistency hydrogel (Nexfill® Hydrogel) was evaluated at 3 different index and *n* is the flow rate. In this model, n > 1 represents concentrations as defined in the cell viability assay (10, a dilatant fluid, n < 1 represents a pseudoplastic fluid and n100 and 1000 μ g/mL). Cells were seeded at a density of = 1 represents a Newtonian fluid (18). 3 x 10⁵ cells/well on 6-well plates. After 24 h, the cells The range of frequencies used was 0.1 to 500 rad were washed with PBS without calcium and it was creat s^{-1} at 50 % strain, which proved to be in the linear ed a "scratch" with a pipet tip. Cells with test substance

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viscosity range.

200 °C at 10 °C/min under nitrogen atmosphere. Thermogravimetric analysis (TGA) and differential thermogravimetric analysis (DTG) of the lyophilized samplewas performed on TA Instruments (SDT-2960) (New Castle, DE, USA). Sample (5 mg) was accurately weighed in coated alumina pan and heated from 25 to 600 °C at 10 °C/min under nitrogen atmosphere. DSC and TGA from pristine BC films were similarly obtained and compared with hydrogel results.

Morphology of BC-based hydrogel

Fibroblast growing model Fibroblast culture

Cell Migration (Wound healing assay)

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were cultured in DMEM containing 10 % FBS and the evaluation was performed after 6 h of incubation with the treatment. The migration process was observed after 6 h of incubation and all images of the group were obtained under inverted microscope (200x) with camera coupled by photograph (increase 3x). The quantification of cell migration was done through image analysis by ImageJ (version 1.48v, National Institutes of Health, USA) and the quantification of wound extension was analyzed in relation the size obtained in the group of basal (untreated) cells. β-estradiol (0.1 mM) was used as inhibitory control of cell migration. The results are expressed as mean \pm standard error of the mean calculated in Microsoft Excel software using t student test. Significant differences between the control and treated groups are indicated by ***p<0.001, **p<0.01 and *p<0.05 (19).

Results and discussion Physicochemical studies Rheology properties

The study of flow properties is related to the deformation of the formulation when subjected to a shear stress, providing information on stability and consistency of the final product (20,21) BC-based hydrogel (Nexfill® Hydrogel) as depicted in Fig. 1.

According to Fig. 1, the hydrogel behaves as a non -Newtonian system, as it does not present a linear relationship between shear stress and shear rate. In agreement with the Equation 1 applied in flow curve (Fig. 1), it was observed that the value obtained by *n* (flow index) is lower than 1 (Table I) indicating that the hydrogel presented pseudoplastic behavior.



Figure 1. Tixotropic hysteresis loop of the BC-based hydrogel (Nexfill® Hydrogel)

Sample	Flow parameters		
	N	K	r ²
BC-based hydrogel (Nexfill®Hydrogel)	0.2579	83.0257	0.9987

Table I - Flow parameters of the BC-based hydrogel (Nexfill® Hydrogel) calculated by using the power law (Equation 1).

In the rheological behavior, the flow curve (Fig. 1) of strain the sample did not suffer deformation and was shows the pseudoplastic behavior that results from the used this value for test of frequency sweep. Frequency alignment of the disrupted a three-dimensional network in sweep was conducted to small amplitude oscillatory shear the system in the direction of flow, providing the protective (SAOS) in the LVE. The ratio of the storage modulus (G film formation characteristic that allows the skin surface to ') and loss (G ") plotted by frequency, which provides imbe covered, promoting a better protection (22). However, portant information about the structure of the gel (25). Imat flow curve (Fig. 1) there is hysteresis area and the hyportant aspects of BC-based hydrogel (Nexfill® Hydrogel) drogel present rheological characteristics thixotropic. structure, as well as, mechanical behavior was determinate Thixotropic products have the characteristic of deforthe frequency-dependence of dynamic moduli (G' and G") ming during application, becoming fluid, facilitating the and are present in Fig. 3.

scattering and recovering the initial viscosity at the time of Fig. 3 and it is observed that G' was higher than the application closure, avoiding the product to flow. Formucorresponding to the G" over the entire frequency sweep lations with thixotropic characteristics tend to have greater range, and the complex viscosity decreases with increaself-life, because during storage it has a constant viscosing frequency. This behavior indicates hydrogels possess sity, making it difficult to separate the constituents of the a solid-like gel structure (26). formulation (23,24). Strain sweep test allows determining The Frequency sweep (Fig. 3) provides information about the storage modulus (G') indicating the energy stored in the material and depends on the rearrangements that occur during the period of oscillation, which may characterize an elastic or solid character. On the other hand, the loss modulus (G") indicates the energy dissipated or lost The strain sweeps measurement was done to check for during the period of oscillation, which may characterize a viscous or liquid behavior. Thus, when there is a predominance of the elastic modulus (G') on the viscous modulus The hydrogel containing BC presented linear behavior (G") it is an indication that the analyzed system is more structured and there is a strong interaction between the components (27).

the amplitude in which the region of linear viscoelasticity is maintained for the sample and, through the identification of the strain values that the sample does not undergo deformation and thus other rheological tests, such as the frequency sweep. the linear-viscoelastic regime (LVE) limit and the curves are present in Fig. 2. until 10 %. So, a strain of 2 % was choose for the next steps, as frequency sweep.

BC-based hydrogel (Nexfill[®] Hydrogel) with 2 %



Figure 2 - Strain Sweep of the BC-based hydrogel (Nexfill® Hydrogel).

Similar results were observed (28) with gelatin hydro-

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Figure 3 - Frequency Sweep of the BC-based hydrogel (Nexfill® Hydrogel).

gels reinforced with chitin of which the mechanical spectra, predominance elastic modulus (G') on the viscous modulus (G'') and the G' values remained unchanged as the angular frequency (0.1–100 rad s⁻¹) indicating a strong and stiffness of the gelatin hydrogel. $450 \circ C (T_{onset} = 372 \circ C)$ was ascribed to the BC degradation process such as depolymerisation, dehydration and decomposition of glucose units (1,29). Four main mass loss events were observed for BC-based hydrogel (Fig. 3B). The first one, starting from low temperature to 110

Thermal behavior

Fig. 4 (A and B) shows TG/DTG results obtained from pristine BC films and BC-based hydrogel (Nexfill[®] Hydrogel), respectively.

For pristine BC films (Fig. 4A), two characteristic events were detected. First, the mass loss from 25 to 100 $^{\circ}$ C (3.51 %) was assigned to the water molecules. The second and main mass loss (75.46 %) starting from 250 to

450 °C ($T_{onset} = 372$ °C) was ascribed to the BC degradation process such as depolymerisation, dehydration and decomposition of glucose units (1,29). Four main mass loss events were observed for BC-based hydrogel (Fig. 3B). The first one, starting from low temperature to 110 °C ($T_{onset} = 55$ °C, 10.19 % of mass loss) corresponds to the solvents and water molecules (dehydration processes of the hydrogel) (1,29). The thermal degradation of the sample occurs in three subsequent steps ($T_{onset} = 192, 322$ and 377 °C). First step occurs from 110 to 250 °C (38.93 % of mass loss) attributed to the humectant compounds. The second ($T_{onset} = 322$ °C, 21.29 % of mass loss) and third ($T_{onset} = 377$ °C, 9.52 % of mass loss) steps were assigned to the degradation processes of BC and other polymers in



Figure 4 - Thermogravimetric (solid lines) and differential thermogravimetric (dashed lines) analysis of (A) pristine BC film and (B) BC-based hydrogel (Nexfill[®] Hydrogel).

agreement with pristine BC films (Fig. 4A) (1,29). Additionally, a residue of 19.70 % was detected for BC-based hydrogel (Nexfill[®] Hydrogel) and ascribed to inorganic salts and carbonaceous materials (carbon and carbon monoxide) (1,30).

The DSC curve of BC-based hydrogel (Fig. 5B) results showing an endothermic peak starting from room temperature to 110 °C as aforementioned in Fig. 4B, this event was assigned to solvents and water loss. It is worth



Figure 5 -. Differential scanning calorimetry curves of (A) pristine BC film and (B) BC-based hydrogel (Nexfill® Hydrogel).

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noting that the hydrogel showed an endothermic event more pronounced and at similar temperature relating to pristine BC films (Fig. 5A). Although it was expected water loss from BC-based hydrogel (Nexfill® Hydrogel) at lower temperatures than for pristine BC film, the hydrogel shows similar behaviour to pristine BC film. These results suggest a strong interaction of the components seen in the hydrogel through the rheological measures to oppose to water loss.

Morphology analysis

The morphology of dried pristine BC film and lyophilized BC-based hydrogel (Nexfill® Hydrogel) were investigated by FE-SEM as shown in Fig. 6.

Fig. 6A displays pristine BC film composed by threedimensional network porous structure containing randomly

arranged cellulose nanofibers (31). Fig. 6 (B-E) exhibit BCbased hydrogel (Nexfill® Hydrogel) with BC nanofibers clearly and well dispersed on its surface. These results suggest that the hydrogel could keep the characteristic properties of pristine BC films in its composition (8,32).



In vitro studies based hydrogel (Nexfill® Hydrogel) showed the highest significant when compared with basal control (p<0.001) The fibroblast migration ability was also evaluated after opening a "scratch" in the middle of the semi-confluent in 1000 mg/mL, demonstrating that in this concentration culture of fibroblasts after 6 h of treatment with BC-based the highest fibroblast migration toward the scratched area almost closing the wound while at 100 and 10 μ g/mL a hydrogel (Fig. 7). delay in fibroblast migration was observed relating to the Fig. 7 illustrates healing activity of different concentrabasal control (p<0.01 and p<0.05, respectively). tions (10, 100 and 1000mg/mL) of the BC-based hydrogel

(Nexfill[®] Hydrogel) related to the basal control (untreated cells). The reference substance β -estradiol promotes delay in wound closure presents a statistically significant difference when compared to baseline control (p<0.001). BC-



Figure 7 - Evaluation of the fibroblast migration capacity of the BC-based hydrogel (Nexfill® Hydrogel). The plot shows mean values \pm Standard error of the mean obtained for each treatment. The values differ of the basal control at *** for when p<0.001, ** for when p<0.01 and * for when p<0.05 in the student t statistical test.

Figure 6 - FE-SEM of the pristine BC film (A), BC-based hydrogel (Nexfill® Hydrogel) (B) 100x, (C) 200x, (D) 500x and (E) 1000x.

Similar results were also observed (33), which evaluated chemically modified BC membranes and demonstrated good in vitro compatibility with fibroblasts, once the membrane helped in the healing process.

Conclusions

BC-based hydrogel (Nexfill[®] Hydrogel) were developed as a potential strategy for the treatment of chronic wounds in which membrane occlusion is not adequate, or even for those cases where the depth of the lesion promoted by tissue loss hinders the adaptation of the membranes in the wound bed. As expected, the BC nanofibers present in the hydrogel were responsible for the building of a strong and structured network which should lead to a high interaction pattern with the biological interfaces but allowing its adequate and comfortable spreadability on the wounds. The set of data suggest that the BC-based hydrogel consists on a suitable formulation for wound repair since fibroblasts represent the first defense line against injuries and the increase of fibroblast proliferation in wound bed is fundamental for lesion repair.

Conflict of interest

There are no conflicts to declare.

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References

- Barud HS, de Araújo Júnior AM, Santos DB, de Assunção RM, Meireles CS, Cerqueira DA, et al. Thermal behavior of cellulose acetate produced from homogeneous acetylation of bacterial cellulose. Thermochim Acta. 2008;471:61-9.
- Ullah H, Wahid F, Santos HA, Khan T. Advances in biomedical and pharmaceutical applications of functional bacterial cellulose-based nanocomposites. Carbohydr polym. 2016;150:330-52.
- Brown RM. Cellulose structure and biosynthesis: what is in store for the 21st century. J Polym Sci A Polym Chem. 2004;42:487-95.
- Klemm D, Schumann D, Kramer F, Heßler N, Hornung M, Schmauder H-P, et al. Nanocelluloses as innovative polymers in research and application. In: Klemm D, editor. Polysaccharides II. Advances in Polymer Science, vol 205. Springer, Berlin, Heidelberg; 2006. p. 49-96.
- Jonas R, Farah LF. Production and application of microbial cellulose. Polym Degrad Stab. 1998;59:101-6.
- Picheth GF, Pirich CL, Sierakowski MR, Woehl MA, Sakakibara CN, de Souza CF, et al. Bacterial cellulose in biomedical applications: A review. Int J Biol Macromol. 2017;104:97-106.
- Barud HO, Barud HDS, Cavicchioli M, do Amaral TS, de Oliveira Junior OB, Santos DM, et al. Preparation and characterization of a bacterial cellulose/silk fibroin sponge scaffold for tissue regeneration. Carbohydr polym. 2015;128:41-51.
- Shao W, Wu J, Liu H, Ye S, Jiang L, Liu X. Novel bioactive surface functionalization of bacterial cellulose membrane. Carbohydr polym. 2017;178:270-6.
- Torres FG, Commeaux S, Troncoso OP. Biocompatibility of bacterial cellulose based biomaterials. J Funct Biomater. 2012;3:864-78.
- Helenius G, Bäckdahl H, Bodin A, Nannmark U, Gatenholm P, Risberg B. In vivo biocompatibility of bacterial cellulose. J Biomed Mater Res A. 2006;76:431-8.
- Gupta A, Low WL, Radecka I, Britland ST, Mohd Amin MCI, Martin C. Characterisation and in vitro antimicrobial activity of biosynthetic silver-loaded bacterial cellulose hydrogels. J microencapsul. 2016;33:725-34.

- 12. Matricardi P, Di Meo C, Coviello T, Hennink WE, Alhaique F. Interpenetrating polymer networks polysaccharide hydrogels for drug delivery and tissue engineering. Adv Drug Deliv Rev. 2013;65:1172-87.
- 13. Hamidi M, Azadi A, Rafiel P. Hydrogel nanoparticles in drug delivery. Adv Drug Deliv Rev. 2008;60:1638-49.
- Melo CS, Silva-Cunha A, Fialho SL. Formas farmacêuticas poliméricas para a administração de peptídeos e proteínas terapêuticos. Revista de Ciências Farmacêuticas Básica e Aplicada. 2013;33:469-77.
- 15. Klouda L, Mikos AG. Thermoresponsive hydrogels in biomedical applications. Eur J Pharm Biopharm. 2008;68:34-45.
- 16. Ischakov R, Adler-Abramovich L, Buzhansky L, Shekhter T, Gazit E. Peptide-based hydrogel nanoparticles as effective drug delivery agents. Bioorg Med Chem. 2013;21:3517-22.
- 17. Yadollahi M, Gholamali I, Namazi H, Aghazadeh M. Synthesis and characterization of antibacterial carboxymethyl cellulose/ZnO nanocomposite hydrogels. Int J Biol Macromol. 2015;74:136-41.
- Barnes HA, Hutton JF, Walters K. An introduction to rheology, volume 3. 1st ed. Amsterdam: Elsevier Science; 1989.
- Chun-Chi L, Park AY, Guan J-L. In vitro scratch assay: a convenient and inexpensive method for analysis of cell migration in vitro. Nat protoc. 2007;2:329-33.
- Schramm G. Reologia e reometria: fundamentos teóricos e práticos. São Paulo: Artliber; 2006.
- Tadros T. Application of rheology for assessment and prediction of the long-term physical stability of emulsion. Adv Colloid Interface Sci. 2004;108:227-58.
- Shawesh A, Kallioinen S, Hellen L, Antikainen O, Yliruusi J. Pluronic F-127 gels as a vehicle for topical formulations of indomethacin and rheological behaviour of these formulations. Pharmazie. 2002;57:186-90.
- 23. Martin AN, Bustamante P. Physical pharmacy: physical chemical principles in the pharmaceutical sciences. Philadelphia: Lea & Febiger; 1993.
- Corrêa NM, Júnior FBC, Ignácio RF, Leonardi GR. Avaliação do comportamento reológico de diferentes géis hidrofílicos. Rev Bras Cienc Farm. 2005;41:73-8.
- Clark AH, Ross-Murphy SB. Structural and mechanical properties of biopolymer gels. In: Biopolymers. Advances in Polymer Science, vol 83. Springer, Berlin, Heidelberg; 1987. p. 57-192.
- Tao Y, Zhang R, Xu W, Bai Z, Zhou Y, Zhao S, et al. Rheological behavior and microstructure of release-controlled hydrogels based on xanthan gum crosslinked with sodium trimetaphosphate. Food Hydrocoll. 2016;52:923-33.
- 27. Teng LY, Chin NL, Yusof YA. Rheological and textural studies of fresh and freeze-thawed native sago starch–sugar gels. I. Optimization using response surface methodology. Food Hydrocoll. 2011;25:1530-7.
- 28. Ge S, Liu Q, Li M, Liu J, Lu H, Li F, et al. Enhanced mechanical properties and gelling ability of gelatin hydrogels reinforced with chitin whiskers. Food Hydrocoll. 2018;75:1-12.
- Machado RT, Gutierrez J, Tercjak A, Trovatti E, Uahib FG, de Padua Moreno G, et al. *Komagataeibacter rhaeticus* as an alternative bacteria for cellulose production. Carbohydr polym. 2016;152:841-49.
- Barud HS, Souza JL, Santos DB, Crespi MS, Ribeiro CA, Messaddeq Y, et al. Bacterial cellulose/poly (3-hydroxybutyrate) composite membranes. Carbohydr Polym. 2011;83:1279-84.
- 31. Pacheco G, Nogueira CR, Meneguin AB, Trovatti E, Silva MC, Machado RT, et al. Development and characterization of bacterial cellulose produced by cashew tree residues as alternative carbon source. Ind Crops Prod. 2017;107:13-9.
- 32. de Lima Fontes M, Meneguin AB, Tercjak A, Gutierrez J, Cury BSF, dos Santos AM, et al. Effect of in situ modification of bacterial cellulose with carboxymethylcellulose on its nano/micro-structure and methotrexate release properties. Carbohydr polym.

2018;179:126-34.

 Birkheur S, de Sousa Faria-Tischer PC, Tischer CA, Pimentel EF, Fronza M, Endringer DC, et al. Enhancement of fibroblast growing on the mannosylated surface of cellulose membranes. Mater Sci Eng C. 2017;77:672 Carbinatto et al.