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Dislocation of large-diameter head metal-on-metal total hip arthroplasty and hip resurfacing arthroplasty

Short title: Dislocation of large-diameter head total hip arthroplasty

Simo S.A. Miettinen¹, MD, Tatu J. Mäkinen^{2,3}, PhD, Inari Laaksonen⁴, PhD, Keijo Mäkelä⁴, PhD, Heini Huhtala⁵, MSc, Jukka S. Kettunen¹, PhD, Ville Remes^{2,3}, PhD

¹ Department of Orthopaedics, Traumatology and Hand Surgery, Kuopio University Hospital, P.O. Box 1777, 70211 Kuopio, Finland

² Department of Orthopaedics and Traumatology, Helsinki University Hospital, P.O. Box 900, 00029 HUS, Finland

³ Pihlajalinna Oy, Tietokuja 4, 00330 Helsinki, Finland

⁴ Department of Orthopaedics and Traumatology, Turku University Hospital, P.O. Box 28, 20701 Turku, Finland

⁵ Faculty of Social Sciences, 33014 University of Tampere, Finland

Corresponding author:

Simo Miettinen

Department of Orthopaedics, Traumatology and Hand Surgery,

Kuopio University Hospital

P.O. Box 1777

70211 Kuopio

Finland

E-mail: simo.miettinen@kuh.fi

Tel: +358 500 673 858

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ABSTRACT

Introduction

Dislocation of large-diameter head (LDH) metal-on-metal (MOM) total hip arthroplasty (THA) or hip resurfacing arthroplasty (HRA) is a rare complication. This study aimed to determine the incidence and risk factors for dislocation of LDH MOM THAs and HRAs.

Methods

This retrospective analysis considered 4,038 cementless LDH MOM THAs and HRAs, 3,207 THAs in 2,912 patients and 831 HRAs in 757 patients. The end of follow-up was revision due to dislocation. Incidence of dislocation was evaluated from this study population of 4,038, and study groups were formed. The study was designed as a case-control study, and a threefold stratified randomized control group was formed. Demographic data was collected and radiological analyses were performed in the study groups.

Results

There were 26/3,207 (0.8%) early dislocations in the THA group, and 6/831 (0.7%) in the HRA group ($p = 0.9$). Most LDH THA dislocations occurred in a group with head size ≤ 38 mm (18/26) ($p < 0.001$). In dislocated hips, there were more dysplastic acetabula and post-traumatic hips than in the control group ($p = 0.036$). In the dislocation group, the mean acetabulum component anteversion angle was 19.6° (SD 13.4°) and in the control group it was 23.2° (SD 10.4°) ($p = 0.006$); 7/32 (21.8%) of dislocated THAs needed revision surgery, and mean time to revision from the index surgery was 1.2 (SD 2.6) years.

Discussion

Dislocations occurred more often in THAs of head size ≤ 38 mm and with a smaller anteversion angle of the acetabulum component. Hip dysplasia and post-traumatic osteoarthritis were more common in patients with dislocation.

Keywords: Complication total hip, Dislocation, Large-diameter head, Primary total hip arthroplasty

Introduction

Second-generation metal-on-metal (MOM) total hip arthroplasties (THA) were introduced in the early 1990s, and they became common in the early 2000s (1, 2). Large-diameter head (LDH) MOM THA was believed to be an answer to hip instability associated with smaller diameter head metal-on-polyethylene (MOP) bearing THAs (1, 3). Hip dislocation remains the most frequent complication after THA, with a reported incidence ranging from 1% to 11% with polyethylene-on-metal THAs (4–8). In LDH MOM THAs, hip dislocation rates have been found to be very low (< 1%) or even nonexistent (1, 9).

The main risk factors for dislocations have are female gender, advanced age, neuromuscular or cognitive disorders, substance abuse, previous hip surgery and soft-tissue or bone deficits of the hip (10). Hip dysplasia or technical errors in surgery (e.g. acetabulum component malposition or failure to restore the centre of hip rotation) are risk factors for dislocation (11, 12). High-risk patients might benefit from LDH MOM THAs in the future to avoid dislocation, even though the issues caused by adverse reaction to metal debris (ARMD) in MOM THAs have discontinued the use of MOM bearings (13).

The aims of this study were to find out the incidence of dislocation in LDH MOM THA and hip resurfacing arthroplasty (HRA), and to evaluate patients according to demographic and radiographic risk factors predisposing to hip instability. We also studied if there were any differences in the rate of dislocations between the THA and HRA components.

Methods

A multicentre retrospective study was performed in three participating university hospitals – Helsinki University Hospital, Kuopio University Hospital and Turku University Hospital. A total of 4,038 THAs were performed between January 2004 and December 2009, 3,207 THAs in 2,912 patients and 831 HRAs in 757 patients. The median follow-up time in the dislocation group was 6.1 (SD 1.5, range 2.0–7.9) years, and in the control group 4.4 (SD 1.8, range 1.7–7.8) years ($p = 1.0$), respectively.

The primary outcome of this study was to find out the dislocation rate for LDH MOM hip devices, and the secondary outcome was to evaluate the possible risk factors for dislocations. Patient demographic data in terms of age, gender, preoperative diagnosis (primary osteoarthritis, developmental dysplasia of the hip, fracture, rheumatoid arthritis, avascular necrosis and other arthritis) and underlying systemic diseases affecting risk of dislocation (rheumatoid arthritis, alcohol abuse, neurological disease) were collected from the patient medical records (Table 1). Head size ≥ 38 mm were considered as LDH hip device. There were 4,038 hips including 831 HRAs and 3,207 THAs. In the THA group there were 122 THAs with head size < 38 mm.

There was a total of 32/4,038 (0.8%) dislocations. For these patients, a control group of threefold the number of patients was formed by selecting THAs and HRAs from the study population of 4,006 THAs and HRAs without dislocation. Patients in the control group were stratified by age, gender, hospital and by type of arthroplasty (THA or HRA). Selection was performed by assigning a different number to each THA and HRA. A random number generator was used to randomly assign THAs and HRAs to the control group. Similarity of

randomized groups was controlled by comparing age, gender, THA components and follow-up time of the randomized group (96 patients) to the study population without THA dislocation (n = 3,900). There were no statistically significant differences in these factors between the control group and study group.

There were four different THAs and four HRAs in the dislocation group. THAs and HRAs were performed according to the manufacturers' instructions.

Radiological analysis

Radiological analyses were performed on plain radiographs taken before surgery and at the 3-month follow-up visit or at the time dislocation first occurred (Tables 2 and 3). Numerous different radiographic measurements have been used in assessing hip dysplasia at skeletal maturity (14, 15). For this study, we selected some of the most commonly used and repeatable measurements, assessed from the preoperative radiographs (Figures 1 and 2).

Crowe classification was used to define developmental hip dysplasia (DDH) (16). Crowe type I has < 50% subluxation, type II has between 50% and 74% subluxation, type III has between 75% and 99% subluxation and type IV has complete dislocation (16). The Wiberg centre–edge (CE) angle was measured (16). A CE angle < 20° has been postulated as indicating hip dysplasia, and one > 25° as indicating a normal hip (17, 18). The acetabular depth–width ratio (ADR) was measured along a line running perpendicularly from the width line to the deepest point of the medial arch (19) (Figure 2). For ADR, mean cut-off values are 0.235 for males and 0.233 for females (19). The femoral head extrusion index (FHEI) was measured to assess the degree of femoral head lateralization over the acetabular edge

(20) (Figure 2). The normal range of FHEI was originally 70–100% but subsequently a cut-off value of 75% was proposed (19, 20).

The functional structure of the acetabulum changes due to osteoarthritis. It has been stated that fixation of the cementless acetabular component is related to the bone structure of the acetabulum (21). We classified acetabula into three types (Type A, Type B and Type C) based on their acetabulum roof morphology on plain preoperative radiographs according to Dorr (21). A Type A acetabulum has an isosceles triangle with equal medial and lateral walls or beams and a shorter base. Type B has an extended triangle which has a pseudopod that extends into the teardrop and creates a thick medial wall. Type C is found only in dysplastic hips, and has a right-angled triangle with a straight lateral wall; the femoral head may or may not be located under the triangle (21).

Restoration of leg length and femoral offset are important factors for the success of THA (22, 23). The radiographic teardrop in AP view was a landmark for many of the measurements used in our study (14, 15, 24). The inter-teardrop line was used as the transverse axis of the pelvis (Figure 1). Leg length discrepancy (LLD) was evaluated from the preoperative and postoperative radiographs, where LLD was the perpendicular distance between a line passing through the lower edge of the inter-teardrop line to a line passing through the tip of the lesser trochanter (Figure 1) (25, 26). Hip offset was measured with a standard method, where the offset is the perpendicular distance between the centre of rotation of the femoral head and the femoral shaft midline (Figure 1) (27). The anatomic hip centre was located from the pre- and postoperative radiographs by a method described by Fessy (28), which has been shown to be the most precise method for determination of the

anatomic hip centre (15). Neck–femoral shaft angle was also measured from the preoperative radiographs.

Acetabular component inclination and anteversion angles were measured from the postoperative radiographs. The inclination angle of the acetabulum component was measured according to the method described by Widmer (29). Anteversion was measured according to the method described by Murray (30). The number of acetabular components which were positioned within the safe zone (5–25° anteversion and 30–50° inclination) described by Lewinnek was analysed (31).

Acetabulum components were divided into four groups based on the amount of containment of the cup, as described by Sarmiento (32). Containment was measured from the postoperative radiographs. Containment by bone was recorded as 100%, 90–99%, 75–99% and < 75%. Radiolucent gaps on the initial postoperative radiograph, and radiolucent lines or osteolysis at the acetabular bone–acetabular component interface on subsequent radiographs were recorded according to the assessment described by DeLee (33).

Picture archiving and communication systems (PACS) were used in every participating hospital. At Helsinki University Central Hospital, there was an Agfa IMPAX (ver. 6.5.2.657) PACS, and Sectra Workstation IDS7 (ver. 15.1.8.5) PACS were used at Kuopio University hospital and Turku University Central Hospital.

Intra- and interobserver error

Measurements were re-analysed after 2 months by the same observer (S.M.) to determine intraobserver error, and by the other observer (J.K.) to determine interobserver error. Bland–

Altman analysis was used to determine whether intra- and interobserver agreement was acceptable. Mean values and variances were tested with paired t-test and Pitman's test for differences in variance.

Statistical analysis

Comparisons between the groups were performed with Pearson's chi-square test. Comparison of continuous data was carried out using a Mann–Whitney U-test. Two-tailed p values are reported, and $p < 0.05$ was considered statistically significant. All the data was analysed statistically using SPSS (IBM Corp. Released 2012. IBM SPSS Statistics for Windows, Version 21.0. Armonk, NY: IBM Corp).

Ethics

The ethical review committee of the University of Turku gave permission (ETMK: 78/1801/2013) for this study.

Results

There were 26/3,207 (0.8%) dislocations in the LDH MOM THA group and 6/831 (0.7%) in the HRA group ($p = 0.9$). In the group of 3,207 THAs with head size < 38 mm, 5/122 (4.1%) dislocations occurred, and 21/3,085 (0.7%) with head size ≥ 38 mm, respectively. There was a total of 7/4,038 (0.2%) THA dislocations which needed revision surgery, and of these, 6/3,207 (0.2%) occurred in the THA group and 1/831 (0.1%) in the HRA group ($p = 0.680$). Median time to revision for any reason in the dislocation group was 42 (SD 2.2, min 1 day, max 7.0 years) days, and in the control group was 114 (SD 0.5, min 22 days, max 1.5 years) days ($p = 0.635$). The mean age of the patients in the dislocation group was 59.5 (SD 8.5,

37.0–80.0) years, and in the control group was 59.1 (SD 9.0, 37.0–79.0) years ($p = 0.956$). Demographic data and surgical details are given in Table 1.

In Crowe DDH classification, there were no statistically significant differences between the groups (Table 3). Radiographic measurements showed that CE angle, neck–femoral shaft angle, FHEI and ADR were similar in both groups (Table 2). The rotation centre of the hip was measured with the X-Y-coordinate model described by Fessy (28), and there were no differences between the groups (Table 3). The change in hip offset was not statistically significant between the groups (Table 3). Acetabulum bone structure had a statistically significant difference between the groups, and there were more Type A patients in the dislocation group (Table 2). There were no statistically significant differences between the groups for LLD or LLD change in pre- and postoperative radiographs.

For postoperative radiographic measurements, the only statistically significant difference was the acetabulum component anteversion angle, which was smaller in the dislocation group (19.6° ; SD 13.4, range -12.0 – 40.0°) than in the control group (23.2° ; SD 10.4, range 3.0 – 58.0°) ($p = 0.006$) (Table 3). Acetabulum components were positioned in Lewinnek's safe zone only in 13/32 (40.6%) of THAs in the dislocation group and in 40/96 (41.7%) of THAs in the control group ($p = 0.917$) (Table 3). However, only one acetabulum component of a dislocated and revised THA was in Lewinnek's safe zone (Table 5).

Of the dislocated THAs, 7/32 (21.8%) needed revision surgery, and mean time to revision from the index surgery was 1.2 (SD 2.6, min 3 days, max 7.0 years) years (Table 4). 5/7 (71%) of the revisions due to dislocation were done within 2 months after the index surgery (Table 5), and 6/7 (86%) of these patients had a posterolateral approach. Only one of the

dislocated and revised HRAs and only one revised LDH THA had a head size over 38 mm (Table 5).

Intra- and interobserver error

Intra- and interobserver measurements were at an acceptable level. Pitman's test revealed that there were no significant differences in intraobserver measurements ($p > 0.05$).

Discussion

Dislocation is an unfortunately frequent and serious complication following conventional THA, but is extremely rare with LDH MOM THAs or HRAs (1, 4). Prevalence of dislocation has been reported as being between 0.3% and 10% in primary THAs (34). In a large registry-based study, revision rate due to dislocation of different head size THA was $\leq 2.5\%$ at 12 years follow-up (35). Understanding the mechanisms and causes of dislocation are essential in clinical decision-making before and during THA. Known risk factors for THA dislocation are surgical approach and technique, operative diagnosis, arthroplasty type, hip anatomy and patient compliance and diseases (36). Dislocation causes significant costs, and it has been calculated that post-THA instability represents 10% of all revision surgeries (37).

Patient-related risk factors must be evaluated and considered preoperatively, intra-operatively and post-operatively (9). There is evidence that age is an independent risk factor for dislocation but evidence of this is still controversial (38). Advanced age (> 75 years) is related to decline in muscular tone, inability to follow postoperative protocols and higher incidence of cognitive problems which have been linked to increased dislocation rates (39–41). In our study, mean patient age in the dislocation group was quite low; because of that,

age was stratified while the control group was selected. Patients with neuromuscular and cognitive disorders as well as alcoholism have been found to be at higher risk for dislocation (36, 42). In our study, only two of the dislocations occurred in alcohol abusers.

Surgical factors affecting risk of dislocation are surgical approach, implant-related factors, soft-tissue repair and surgeon experience. Higher dislocation rates have been reported for the posterior approach (2.03–5.8%) compared to the anterolateral approach (2.18–2.3%) and to the direct lateral approach (0.55%) (43). In our study, we did not find any statistically significant difference between surgical approaches; however, in dislocated and revised THAs there were more cases of posterolateral approach than of direct lateral approach.

Implant-related risk factors are implant type, design and head size. Larger head sizes have been found to decrease the rate of dislocation for all surgical approaches (44). A prospective study assessing three different head size THAs (< 36 mm, 36 mm and > 36 mm) showed that dislocation rates were significantly lower in the group of head size > 36 mm (0%) compared to the group of head size < 36 mm (1.25%) (45). Our results are comparable to those of Allen et al., as in our study 18/26 (69.2%) of the dislocations occurred in LDH THA of head size \leq 38 mm, and only one revised THA due to dislocation had a head size over 38 mm. In a recent large sample size register study, where different bearings (ceramic-on-ceramic, metal-on-metal and metal-on-polyethylene) were compared, Shah et al. showed that between head sizes of 28 mm and 32 mm there was no difference in the risk of revision due to dislocation (46). Our study findings support this finding, as the highest percentage of dislocations were in THAs with head size < 38 mm. LDH MoM bearings give excellent stability but can entail some serious problems such as ARMD, and the use of these implants is no longer recommended (13). Alternatives to LDH MoM THAs are dual mobility implants

and constrained acetabulum liners. Dual mobility THAs have been challenging LDH MoM THAs and have been gaining popularity in recent years, mainly due to the low rate of dislocation (1.1%) and good overall survivorship, especially in patients with a fracture of the femoral neck (47).

Forces affecting a reconstructed hip joint have been noted to alter if the rotation centre of the hip changes, and this may predispose THA to dislocation (11, 48). In our study, neither preoperative nor postoperative radiological measurements showed any statistically significant difference between the groups; in addition, dislocation group measurements were within normal limits given in the literature (17, 19, 20). Changes in hip rotation centre and hip offset between preoperative and postoperative measurements were not statistically significant. LLD change was also at an acceptable level, and there were no statistically significant differences between preoperative and postoperative measurements in either group in our study. It is more demanding to perform THA on a dysplastic hip joint than on normal hip anatomy, and further on, DDH raises the risk of dislocation (12, 16). In our study, we did not find any statistically significant differences between the groups for DDH measurements. However, when comparing operative diagnosis, there were more dysplastic hip joints in the dislocation group.

Component malposition is the most common cause of instability following THA. Acetabular component placement has been deemed suboptimal if outside Lewinnek's safe zone (31). Excessive anteversion may result in anterior dislocation, and excessive retroversion may result in posterior dislocation. The most common surgical error is acetabular component placement in excessive anteversion and abduction (48). In our study, dislocation occurred more often in THAs where the anteversion angle was smaller than in the control group.

However, in both groups anteversion and inclination angle were within Lewinnek's safe zone. In addition, the mean difference of anteversion angles in between-group comparison was small (3.6°), which makes the clinical relevance of the difference non-significant. Acetabulum components were out of Lewinnek's safe zone in 6/7 of the revised and dislocated THAs. It can be assumed that technical error in acetabulum component positioning in the index surgery is the main reason for revision in cases where dislocation has occurred soon after the index surgery. There was more acetabulum roof morphology variation and more dysplastic hips in the dislocation group, which might contribute to technical error and acetabulum component malpositioning.

Most single-episode dislocations of THA can be treated successfully conservatively, as our study showed. Most dislocations occur early (0–6 months) after the index surgery, and lead more often to revision surgery (34, 49). Our study finding supports these previous study findings, as 5/7 of these revisions were done within 2 months after the index operation.

The retrospective study design has some inherent limitations, which might be minimized by a prospective study design. Typical flaws of retrospective studies also concern our study. The influence of postoperative activity and range of motion restrictions on hip dislocation after THA are controversial, and that is why we did not include those factors in our study (40, 41). Surgeon experience affects the risk of dislocation. Surgeons who do fewer than 30 THAs yearly have the highest dislocation rates (50). We did not study surgeons' experience because there was a total of 46 surgeons in three participating hospitals. These surgeons performed 4,038 THAs, and it was not possible to determine the yearly amount of THAs for each surgeon from the hospitals' medical records. Also, surgical technique between orthopaedic surgeons may not be reproducible, and this causes differences between

surgeons' personal results. In our study there were no revisions due to ARMD and one reason for this might be the short follow-up as, typically, ARMD reactions appear during a longer follow-up. A history of spinal fusion has been found to be an independent risk factor for dislocation (51). However, in this study we did not explore this as a risk factor because our assumption was that there are only a few spinal fusion patients in this small sample size of a dislocation group (n = 32), rendering the statistical and clinical significance inconclusive.

We showed that dislocation of LDH THA is a very rare complication. Hip dysplasia was associated with dislocation even with larger head sizes. Placing the acetabulum component at the correct inclination and anteversion angles, and restoring the hip anatomical rotation centre reduces the risk of dislocation. In our study, dislocations occurred more often in THAs where acetabulum component anteversion angles were smaller. In the past, LDH MoM bearings were thought to be an answer for hip instability related to smaller head size THAs. However, due to ARMD issues, these implants are banned. Nevertheless, some small minority of patients with a high risk of dislocation (e.g. an alcohol abuser with an acute femoral neck fracture) and who have contraindication to dual mobility implant or constrained acetabular liner, might be considered to have LDH MOM THA to reduce the risk of dislocation, even though it is not generally advisable.

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Declaration of conflicting interests

Each author certifies that he or she has no commercial associations that might pose a conflict of interest in connection with the submitted article.

Authors contributions

S.M. participated in planning the study protocol, collecting data for this study at Kuopio University Hospital, analyzing radiographs and statistics, and preparing the manuscript.

T.M. participated in planning the study protocol, collecting data for this study at Helsinki University Hospital, and preparing the manuscript.

I.K. participated in planning the study protocol, collecting data for this study at Turku University Central Hospital, and preparing the manuscript.

K.M. participated in planning the study protocol, collecting data for this study at Turku University Central Hospital, and preparing the manuscript.

H.H. participated in planning the study protocol, performing statistical analyses, and preparing the manuscript.

J.K. participated in planning the study protocol, collecting data for this study at Kuopio University Hospital, and preparing the manuscript.

V.R. participated in planning the study protocol, collecting data for this study at Helsinki University Hospital, and preparing the manuscript.

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Tables

Table 1. Demographic data of the patients.

| | Dislocation group n (%) | Control group n (%) | <i>p</i> - value |
|--|-------------------------------|---------------------------|---------------------|
| Gender | | | 0.757 |
| Male | 19 (59.4) | 54 (56.3) | |
| Female | 13 (40.6) | 42 (43.8) | |
| Surgical approach | | | 0.707 |
| Posterior | 26 (81.3) | 75 (78.1) | |
| Direct lateral (Hardinge) | 6 (18.8) | 21 (21.9) | |
| Operation side | | | 0.759 |
| Left | 17 (53.1) | 48 (50.0) | |
| Right | 15 (46.9) | 48 (50.0) | |
| Operation diagnosis | | | 0.046 |
| Primary osteoarthritis | 16 (50.0) | 70 (72.9) | |
| Developmental dysplasia of the hip | 3 (9.4) | 10 (10.4) | |
| Fracture (acute or sequelae of the hip) | 5 (15.6) | 4 (4.2) | |
| Rheumatoid arthritis | 3 (9.4) | 2 (2.1) | |

| | | | |
|--|------------|-----------|--------|
| Avascular necrosis | 4 (12.5) | 8 (8.3) | |
| Other arthritis | 1 (3.1) | 2 (2.1) | |
| Diseases affecting risk of dislocation | | | 0.147 |
| None | 27 (84.4) | 87 (90.6) | |
| Rheumatoides arthritis | 2 (6.3) | 2 (2.1) | |
| Other arthritis | 1 (3.1) | 0 (0.0) | |
| Long term cortisone medication use | 0 (0.0) | 2 (2.1) | |
| Osteoporosis | 0 (0.0) | 1 (1.0) | |
| Alcohol abuse | 2 (6.3) | 1 (1.0) | |
| Neurological disease | 0 (0.0) | 3 (3.1) | |
| THA type | | | 1.000 |
| HRA | 6 (18.8.6) | 18 (18.8) | |
| Conventional THA | 26 (81.3) | 78 (81.3) | |
| Conventional THA subtypes | | | <0.001 |
| Head diameter >38mm | 8 (25.0) | 61 (63.5) | |
| Head diameter 38mm | 13 (40.6) | 15 (15.6) | |
| Head diameter <38mm | 5 (15.6) | 2 (2.1) | |
| Femoral implant type | | | 0.900 |
| Tapered | 1 (3.1) | 5 (5.2) | |
| Fit and fill | 25 (78.1) | 72 (75.0) | |
| Other | 0 (0.0) | 1 (1.0) | |
| HRA | 6 (18.8) | 18 (18.8) | |
| Intraoperative complication | | | 0.390 |
| None | 27 (84.4) | 90 (93.8) | |

| | | |
|-------------------------|---------|---------|
| Periprosthetic fracture | 3 (9.4) | 3 (3.1) |
| Nerve injury | 1 (3.1) | 2 (2.1) |
| Other | 1 (3.1) | 1 (1.0) |

Table 2. Radiographic assessments.

| | Dislocation group | Control group | p- |
|---|-------------------------------------|-------------------------------------|-------------|
| | n = 32 | n = 96 | valu |
| | | | e |
| Preoperative radiographic measurements | | | |
| Center-Edge angle (CE) | 41.9 (SD 13.195, range 3.0-74.0) | 41.3 (SD 12.885, range 14.0-76.0) | 0.164 |
| Neck-femoral shaft angle | 136.0 (SD 5.734, range 124.0-149.0) | 135.5 (SD 5.058, range 126.0-150.0) | 0.169 |
| Acetabulum depth ratio | 0.255 (SD 0.069, range 0.13-0.48) | 0.254 (SD 0.056, range 0.11-0.42) | 0.676 |
| Femoral head extrusion index (FHEI) | 81.3 (SD 13.881, range 49.0-100.0) | 81.3 (SD 12.373, range 54.2-100.0) | 0.644 |
| Fessy x, mm | 31.9 (SD 6.552, range 16.2-43.2) | 33.6 (SD 5.856, range 22.5-51.3) | 0.642 |
| Fessy y, mm | 23.8 (SD 7.618, range 10.0-41.4.0) | 22.9 (SD 6.782, range 11.7-50.4) | 0.052 |
| Hip offset, mm | 40.4 (SD 6.273, range 30-50) | 40.2 (SD 8.670, range 15-57) | 0.450 |

| | | | |
|--|------------------------------------|----------------------------------|-------------|
| LLD, mm | 37.3 (SD 9.149, range 7-49) | 38.2 (SD 9.086, range 17-59) | 0.20 2 |
| Postoperative radiographic measurements | | | |
| Fessy x, mm | 29.6 (SD 5.477, range 21.6-45.0) | 28.2 (SD 4.390, range 18.9-39.6) | 0.22 9 |
| Fessy y, mm | 22.8 (SD 6.143, range 13.0-46.8) | 22.3 (SD 5.102, range 13.5-49.5) | 0.60 6 |
| Change of the hip rotation center, mm | 3.33 (SD 10.429, range -22.7-15.3) | 6.0 (SD 8.638, range 21.0-27.0) | - 0.50 2 |
| Change of the hip rotation center | | | 0.74 6 |
| <10mm | 22 (68.8) | 63 (65.6) | |
| ≥10mm | 10 (31.3) | 33 (34.4) | |
| Unable to measure | | 0 | |
| Hip offset, mm | 48.0 (SD 8.533, range 21-64) | 49.1 (SD 7.375, range 32-65) | 0.16 7 |
| Hip offset change postoperatively, mm | 7.5 (SD 7.331, range 1179-18.0) | 8.8 (SD 6.843, range 5.5-24.3) | - 0.65 4 |
| LLD, mm | 45.8 (SD 9.189, range 34.2-62.1) | 46.4 (SD 8.513 range 27.0-62.1) | 0.15 2 |
| LLD change postoperatively | | | 0.15 2 |
| ≤20 mm lengthing | 22 (68.8) | 81 (84.4) | |

| | | | |
|--|------------------------------------|-----------------------------------|------|
| >20 mm lengthening | 4 (12.5) | 5 (5.2) | |
| Shortening of the leg | 4 (12.5) | 6 (6.3) | |
| Unable to measure | 2 (6.3) | 4 (4.2) | |
| Acetabular component inclination angle | 47.4 (SD 6.031, range 38.0-60.0) | 45.6 (SD 7.805, range 25.0-64.0) | 0.95 |
| Acetabular component anteversio angle | 19.6 (SD 13.421, range -12.0-40.0) | 23.2 (SD 10.443, range -3.0-58.0) | 0.00 |
| Cup position at Lewinnek safe zone | | | 0.91 |
| No | 19 (59.4) | 56 (58.3) | 7 |
| Yes | 13 (40.6) | 4 (41.7) | |

Table 3. Radiographic classifications.

| | Dislocation | Control | <i>p</i> -value |
|--|-------------|---------|-----------------|
| | group | group | |
| | n = 32 | n = 96 | |
| Preoperative radiographic classifications | | | |
| Acetabulum bone structure | | | 0.011 |
| Type A | 6 (18.8) | 3 (3.1) | |

| | | | |
|--------------------------|-----------|-----------|-------|
| Type B | 20 (62.5) | 72 (75.0) | |
| Type C | 6 (18.8) | 21 (21.9) | |
| Crowe DDH classification | | | 0.084 |
| None | 26 (81.3) | 83 (86.5) | |
| Type I | 2 (6.3) | 7 (7.3) | |
| Type II | 3 (9.4) | 6 (6.3) | |
| Type III | 1 (3.1) | 0 | |
| Type IV | 0 | 0 | |

Postoperative radiographic measurements

| | | | |
|--------------------------|-----------|-----------|-------|
| Cup containment | | | 0.439 |
| Complete 100% | 19 (59.4) | 46 (47.9) | |
| 90-99% | 11 (34.4) | 38 (39.6) | |
| 75-90% | 2 (6.3) | 12 (12.5) | |
| <75% | 0 | 0 | |
| Radiolucent lines (>2mm) | | | 0.469 |
| None | 29 (90.6) | 92 (95.8) | |
| Yes | 3 (9.4) | 4 (4.2) | |

Table 4. Revised patients.

| | Dislocation group | Control group | |
|--------------------------------|--------------------------|----------------------|-----------------------|
| | n (%) | n (%) | |
| | | | <i>p</i>-value |
| Revision | | | <0.001 |
| Yes | 10 (31.3) | 6 (6.3) | |
| No | 22 (68.7) | 90 (93.7) | |
| Reason for revision | | | 0.028 |
| Dislocation | 7 | 0 | |
| Infection | 1 | 0 | |
| Acetabulum component loosening | 1 | 1 | |
| Periprosthetic fracture | 1 | 4 | |
| Component malposition | 0 | 1 | |

Table 5. Dislocation and revised patients.

| Surgical approach | Follow-up (years) | THA type | THA model | Head size | Time to revision | Inclination angle | Anteversion angle | Lewinnek's safe zone |
|---------------------------|-------------------|------------------|------------------------|-----------|------------------|-------------------|-------------------|----------------------|
| Posterolateral | 3.9 | Conventional THA | Synergy/BHR | 46 | 1.3 years | 39 | -2 | No |
| Posterolateral | 4.4 | HRA | Biomet Recap | 48 | 36 days | 55 | N/A | No |
| Posterolateral | 6.1 | Conventional THA | Biomet BiMetric/M2a38 | 38 | 3 days | 60 | 35 | No |
| Posterolateral | 6.6 | Conventional THA | Biomet BiMetric/M2a38 | 38 | 44 days | 42 | 22 | Yes |
| Posterolateral | 6.1 | Conventional THA | Biomet BiMetric/M2a38 | 38 | 7 days | 50 | 14 | No |
| Posterolateral | 2.0 | Conventional THA | Corail/Summit Pinnacle | 36 | 39 days | 40 | -3 | No |
| Direct lateral (Hardinge) | 7.9 | Conventional THA | Biomet BiMetric/M2a38 | 38 | 7.0 years | 48 | 34 | No |

Figure legends

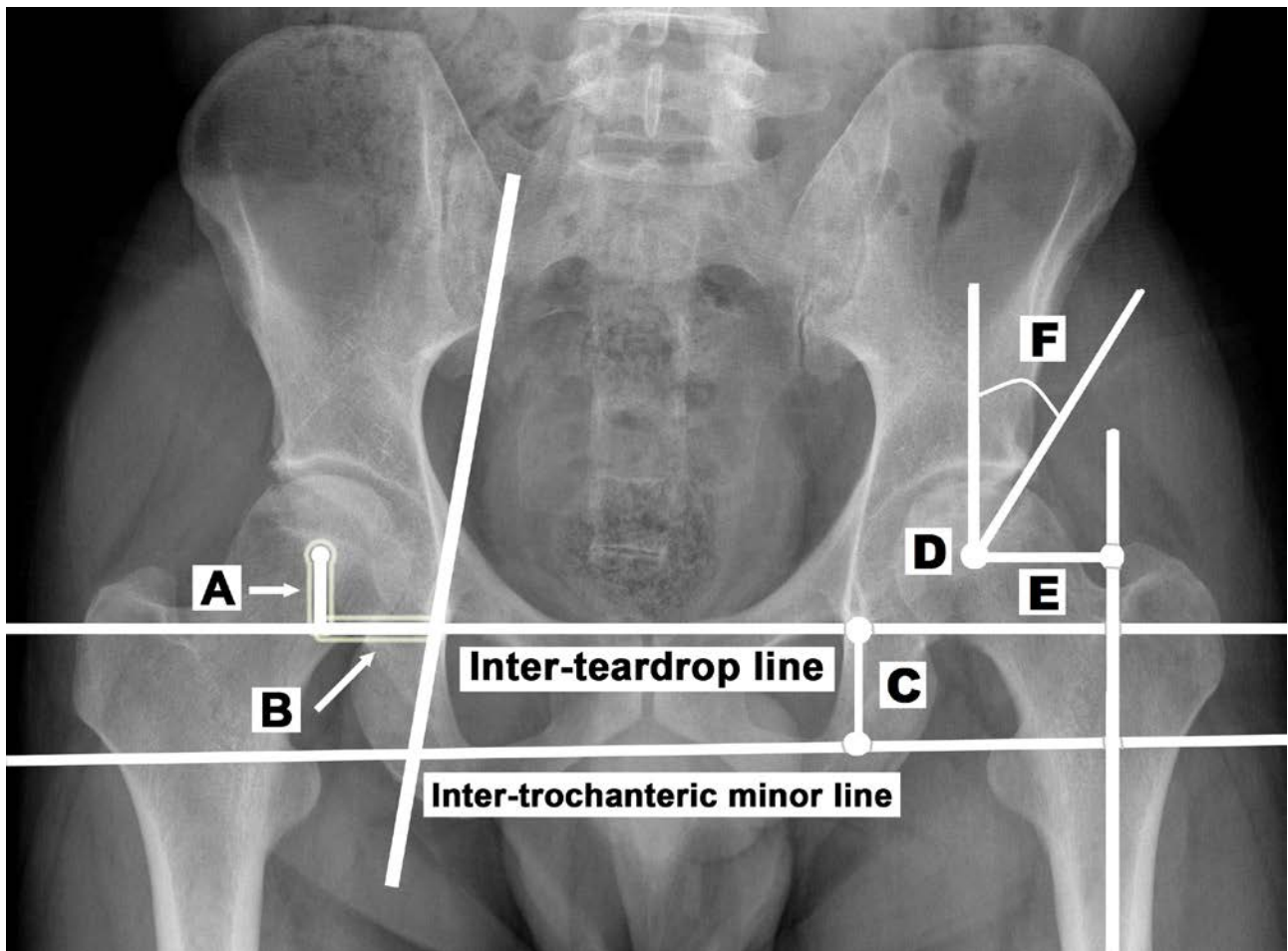


Figure 1. Vertical (A) distance of the hip joint center is measured between center of the femoral head and perpendicular to inter-teardrop line. Horizontal (B) distance of the hip joint center is measured from intersection of the distal end of the inter-teardrop line and from the line between inferior edge of the sacroiliac joint and teardrop. Leg length discrepancy (LLD) measurement (C) described by Kjellberg (24). D is rotation center of the hip. A standard hip offset measurement (E) described by Woolson (26). Center-edge angle (F) is formed by vertical line through the center of the femoral head and perpendicular to the transverse axis of the pelvis.

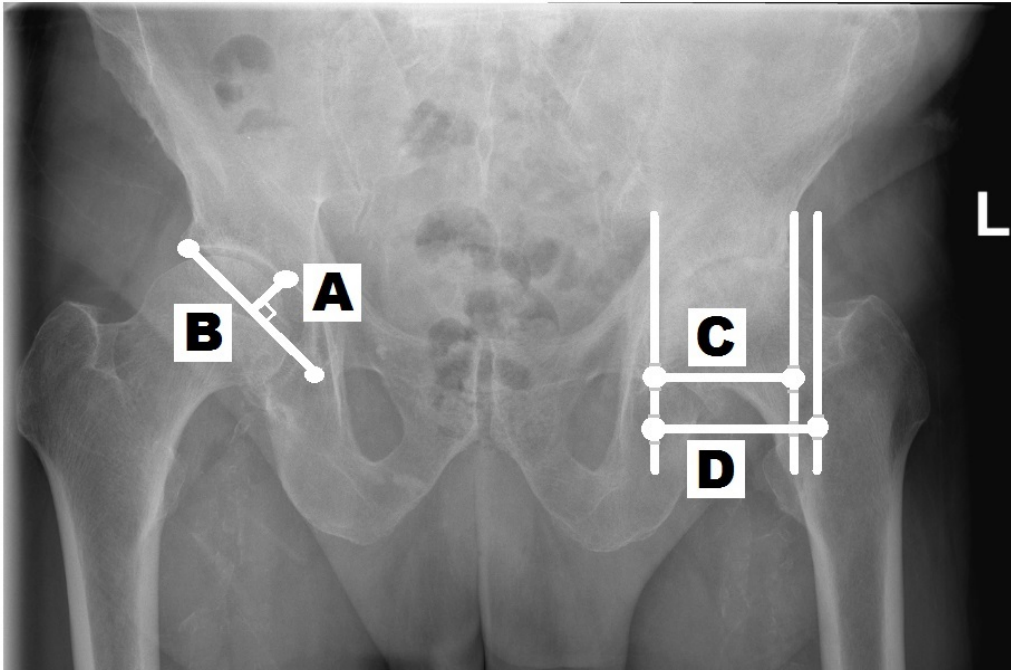


Figure 2. The acetabular depth-width ratio (ADR) is the depth of the acetabulum (A) divided by the width of the acetabulum (B). The femoral head index (FHEI) quantifies how much of the femoral head is covered by the acetabulum ($C/D \times 100$).