

European Heart Journal - Cardiovascular Imaging

European Association of Cardiovascular Imaging (EACVI) Expert Consensus Paper: Comprehensive Review of Cardiovascular Magnetic Resonance (CMR) Normal Values of Cardiac Chamber Size and Aortic Root in Adults and Recommendations for Grading Severity

--Manuscript Draft--

Manuscript Number:	
Full Title:	European Association of Cardiovascular Imaging (EACVI) Expert Consensus Paper: Comprehensive Review of Cardiovascular Magnetic Resonance (CMR) Normal Values of Cardiac Chamber Size and Aortic Root in Adults and Recommendations for Grading Severity
Article Type:	Original Paper
Keywords:	Grading, severity, cardiovascular magnetic resonance, position statement, cardiac chambers
Corresponding Author:	Steffen E Petersen, M.D. NIHR Cardiovascular Biomedical Research Unit at Barts London, UNITED KINGDOM
Corresponding Author Secondary Information:	
Corresponding Author's Institution:	NIHR Cardiovascular Biomedical Research Unit at Barts
Corresponding Author's Secondary Institution:	
First Author:	Steffen E Petersen, MSC MPH M.D. DPHIL
First Author Secondary Information:	
Order of Authors:	Steffen E Petersen, MSC MPH M.D. DPHIL Mohammed Y Khanji, PhD Sven Plein, PhD Patrizio Lancellotti, PhD Chiara Bucciarelli-Ducci, PhD
Order of Authors Secondary Information:	
Abstract:	<p>This consensus paper provides a framework for grading of severity of cardiovascular magnetic resonance (CMR) imaging-based assessment of chamber size, function and aortic measurements. This does not currently exist for CMR measures. Differences exist in the normal reference values between echocardiography and CMR along with differences in methods used to derive these. We feel that this document will significantly complement the current literature and provide a practical guide for clinicians in daily reporting and interpretation of CMR scans.</p> <p>This manuscript aims to complement a recent comprehensive review of CMR normal value publications to recommend cut-off values required for severity grading. Standardization of severity grading for clinically useful CMR parameters is encouraged to lead to clearer and easier communication with referring clinicians and may contribute to better patient care. To this end, the European Association of Cardiovascular Imaging (EACVI) has formed this expert panel that has critically reviewed the literature and has come to a consensus on approaches to severity grading for commonly quantified CMR parameters.</p>

Preamble

This consensus paper provides a framework for grading of severity of cardiovascular magnetic resonance (CMR) imaging-based assessment of chamber size, function and aortic measurements. This does not currently exist for CMR measures. Differences exist in the normal reference values between echocardiography and CMR along with differences in methods used to derive these. We feel that this document will significantly complement the current literature and provide a practical guide for clinicians in daily reporting and interpretation of CMR scans.

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**European Association of Cardiovascular Imaging (EACVI) Expert Consensus Paper:
Comprehensive Review of Cardiovascular Magnetic Resonance (CMR) Normal Values of
Cardiac Chamber Size and Aortic Root in Adults and Recommendations for Grading Severity**

*Steffen E Petersen^{1,2}, *Mohammed Y Khanji^{1,2}, Sven Plein³, Patrizio Lancellotti^{4,5}, Chiara
Bucciarelli-Ducci⁶

*Joint first authors, contributed equally to this work.

¹NIHR Barts Biomedical Research Centre, William Harvey Research Institute, Queen Mary
University of London, London, UK;

² Barts Heart Centre, St Bartholomew's, Barts Health NHS Trust, London, UK

³Multidisciplinary Cardiovascular Research Center & Leeds Institute of Cardiovascular and
Metabolic Medicine, University of Leeds, Leeds, UK;

⁴Department of Cardiology, University of Liege Hospital, GIGA Cardiovascular Sciences, Heart
Valve Clinic, CHU Sart Tilman, Liege, Belgium

⁵Gruppo Villa Maria Care and Research, Anthea Hospital, Bari, Italy

⁶ Bristol NIHR Biomedical Research Unit, Bristol Heart Institute Division of Biomedical Imaging,
University of Bristol, Bristol, UK.

Corresponding author

Professor Steffen E Petersen

NIHR Barts Biomedical Research Centre, William Harvey Research Institute, Queen Mary

University of London, London, UK

London, Charterhouse Square

London, EC1M 6BQ

United Kingdom

Tel: 0044 207 8826902

s.e.petersen@qmul.ac.uk

Key words

Grading, severity, cardiovascular magnetic resonance, position statement, cardiac chambers

Funding

None

Potential conflicts of interest

SEP and CBD - Consultancy for Circle Cardiovascular Imaging Inc., Calgary, Canada

1 **European Association of Cardiovascular Imaging (EACVI) Expert Consensus Paper:**
2 **Comprehensive Review of Cardiovascular Magnetic Resonance (CMR) Normal Values of Cardiac**
3 **Chamber Size and Aortic Root in Adults and Recommendations for Grading Severity**

4
5 *Steffen E Petersen^{1,2}, *Mohammed Y Khanji^{1,2}, Sven Plein³, Patrizio Lancellotti^{4,5}, Chiara
6 Bucciarelli-Ducci⁶

7 *Joint first authors, contributed equally to this work.

8
9 ¹NIHR Barts Biomedical Research Centre, William Harvey Research Institute, Queen Mary
10 University of London, London, UK;

11 ² Barts Heart Centre, St Bartholomew's, Barts Health NHS Trust, London, UK

12 ³Multidisciplinary Cardiovascular Research Center & Leeds Institute of Cardiovascular and
13 Metabolic Medicine, University of Leeds, Leeds, UK;

14 ⁴Department of Cardiology, University of Liege Hospital, GIGA Cardiovascular Sciences, Heart Valve
15 Clinic, CHU Sart Tilman, Liege, Belgium

16 ⁵Gruppo Villa Maria Care and Research, Anthea Hospital, Bari, Italy

17 ⁶ Bristol NIHR Biomedical Research Unit, Bristol Heart Institute Division of Biomedical Imaging,
18 University of Bristol, Bristol, UK.

19
20 **Corresponding author**

21 Professor Steffen E Petersen

22 NIHR Barts Biomedical Research Centre, William Harvey Research Institute, Queen Mary University
23 of London, London, UK

24 London, Charterhouse Square

25 London, EC1M 6BQ

26 United Kingdom

27 Tel: 0044 207 8826902

28 s.e.petersen@qmul.ac.uk

29 **Key words**

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32 **Funding**

33 **None**

34

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36 SEP and CBD - Consultancy for Circle Cardiovascular Imaging Inc., Calgary, Canada

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This manuscript aims to complement a recent comprehensive review of CMR normal value publications to recommend cut-off values required for severity grading. Standardization of severity grading for clinically useful CMR parameters is encouraged to lead to clearer and easier communication with referring clinicians and may contribute to better patient care. To this end, the European Association of Cardiovascular Imaging (EACVI) has formed this expert panel that has critically reviewed the literature and has come to a consensus on approaches to severity grading for commonly quantified CMR parameters.

76 **Introduction**

77 Cardiovascular Magnetic Resonance (CMR) imaging is now firmly established in clinical practice as
78 a cardiac imaging modality, which complements other non-invasive techniques, such as
79 echocardiography, nuclear cardiac imaging and cardiac computed tomography. CMR has an
80 important role in a wide range of clinical indications and scenarios.¹⁻³

81

82 Patient impact is dependent on the quality of the clinical CMR service provision. Efforts to
83 standardize CMR image acquisition,^{4,5} CMR image analysis and CMR image reporting contribute to
84 raising overall CMR service quality.⁶ Certification of individuals in CMR sets minimum standards of
85 expertise and provides evidence to those that can demonstrate it.⁷

86

87 Communication of CMR and other imaging modality findings is a key component to ensure that
88 they positively impact patient management.⁸ Complementing a description of a parameter as
89 being normal or abnormal (reference values), clinical imaging physicians most often qualify the
90 extent of abnormalities using terms such as 'mild', 'moderate' or 'severe'. Such descriptions allow
91 the clinician not only to understand that the parameter is abnormal but also the extent to which
92 their patient's measurements deviate from normal. As well as providing normative data it would
93 be beneficial to standardize cut-offs for severity of abnormality across centres, such that
94 moderately abnormal has the same implication in all. The association of continuous information
95 with prognosis may be stronger than between the categories of normal, mildly, moderately and
96 severely abnormal and prognosis.⁹ However, communication of the degree of abnormality in
97 categories may be clearer to the referring physician and thus may lead to more rapid and
98 consistent clinical decisions.

99

100 For CMR measurements there is no consensus on how to categorize the severity of abnormality.
101 The echocardiography community has published consensus statements to this end.^{10,11} Here, we
102 attempt to suggest approaches to grade the severity of abnormality for common and clinically
103 useful CMR parameters. Recommendations on image analysis, including chamber quantification,
104 have been published and are not the scope of this paper.⁶ Readers of this expert consensus article
105 should ensure they are aware of the analysis methods used for the original data from which the
106 normal reference ranges are derived, as different analysis approaches can have a clinically
107 relevant impact on results. Between CMR and other imaging modalities that can measure the
108 same phenotype systemic biases may exist. Using the same cut-off values based on different
109 modalities may thus not always be appropriate and even using the same cut-off values for
110 different CMR techniques needs to be interpreted with caution given documented differences
111 (e.g. between fast gradient echo and steady state free precession for myocardial mass and
112 volumes).¹²

113 The authors acknowledge explicitly that the same value on a continuous scale or the same
114 category may not reflect the same degree of abnormality depending on the context. Despite a
115 normal left ventricular ejection fraction value in the context of severe mitral regurgitation this may
116 still suggest an abnormal systolic function. Similarly, a patient with severe concentric hypertrophy
117 and a 'normal' left ventricular ejection fraction may still have abnormal systolic function. Thus, any
118 attempt to categorize the severity of abnormality should not be seen as providing optimal cut-off
119 values in every case. Physicians reporting CMR scans should provide an interpretation that
120 considers the clinical context.

121

122

123 **Methodology for severity grading**

124

125 The writing group considered several different approaches to define the cut-off values for mild,
126 moderate and severely abnormal measurements. Multiple statistical techniques exist for
127 determining threshold values, all of which have limitations.¹³ The first approach would be to
128 define these cut-offs for abnormalities based on standard deviations below and above the normal
129 reference limit derived from a group of healthy subjects. These data exist for most CMR
130 parameters. However, not all cardiac parameters are normally distributed, such as aortic valve
131 regurgitant fraction, making the use of standard deviation as a measure of spread potentially
132 problematic.

133 The second approach would be to define abnormalities based on percentile values (95th, 99th,
134 etc.) of measurements. These are derived from a population that would include normal subjects
135 along with individuals with disease states.¹⁴ They would consider asymmetric distribution and
136 range of abnormality present within the general population. A limiting factor for this approach is
137 that large enough population data sets do not exist for most CMR variables. Ideally, an approach
138 could classify outcomes directly. A moderately abnormal variable would imply a moderate risk of a
139 particular adverse outcome for that patient. Risk data are still sparse for some CMR measures and
140 a moderate degree of deviation from normal may have differential effects on different important
141 outcomes (e.g. morbidity and mortality). The third approach defines cut-off values based on
142 expert opinion. Although scientifically least rigorous, this method considers the collective
143 experience of a panel of experienced CMR experts. We used expert consensus mainly when the
144 statistical methods would not provide equally distributed value ranges between the severity
145 categories and to provide some consistency if well-established cut-offs exist for other imaging
146 modalities (e.g. LVEF grading). Despite the limitations, this categorization of CMR parameters in
147 the abnormal range represents another step towards the standardization of clinical CMR

148 complementing the consensus documents on CMR image acquisition, interpretation and analysis
149 and reporting.^{4,6,15} Derived parameter values could be automatically categorized in clinical
150 reporting software or in clinical trials for improved interpretation of CMR results.

151

152 In the following sections we present consensus suggestions on the grading severity of abnormality
153 based on the anatomical structure assessed. We do not attempt to provide values for each normal
154 reference paper that exists at the time of publication. Specifically, this consensus paper
155 complements a comprehensive recent systematic review of normal ranges using CMR.¹⁶ Much of
156 what is presented in this paper is derived from published normal ranges with relatively small
157 samples but can be updated in the future, using the same principles, with larger datasets. For
158 example, it would also be ideal to have reference ranges categorized by age as well as gender.
159 However, because of the small number of individuals included in the current studies, the
160 consensus was to delay providing age categorised grading until larger reference ranges are
161 published. This will hopefully provide more accurate ranges. We did not include the recent UK
162 Biobank reference ranges in this consensus document given that the LV ejection fractions were
163 significantly lower than currently accepted normal ranges.¹⁷ Further analysis of the data was
164 considered to be required by the writing group before recommending its use in routine clinical
165 practice. It should also be noted that recent European Society of Cardiology heart failure
166 guidelines now categorise heart failure patients as those having reduced (<40%), mid-range (40-
167 49%) and preserved (>50%) ejection fraction based on transthoracic echocardiographic
168 measures.¹⁸

169

170 Most of the normal range publications did not specify the ethnicity but were derived from a
171 Western population and would largely if not all have been Caucasians and predominantly from the
172 United Kingdom.¹⁹⁻²⁵ The approaches here are mostly defining cut-off values based on standard

173 deviations reported in the normal population apart from ejection fraction measurement that are
174 derived from a combination of standard deviation and expert consensus. Using the statistical
175 method, the normal range is defined as +/- 2 standard deviations from the mean, mildly abnormal
176 from this cut-off to 3 SD, moderately abnormal from the mild cut-off to 4 SD and severe being
177 more than 4 SD from the population mean. The term "Opposite" refers to values that are outside
178 the normal range but in the opposite direction of typical thought of as pathology, e.g. smaller LV
179 end-diastolic volumes or supra-normal LV ejection fraction. This consensus agreement was to
180 allow commonly used cut-offs that are used for different imaging modalities and avoid confusion.
181 It should be emphasized that these cut-offs are to allow clearer and easier communication of
182 grading. As such, any new or omitted reference range can easily be categorized using the same
183 principles.

184

185 ***Measurements and methods***

186

187 The summary of measurements and techniques used in deriving the normal values from the
188 published papers that are included in this consensus paper are included in Table 1 with description
189 of the methodology used in the relevant subsections. Table 2 provided additional details of the
190 individual studies used to derive the grading parameters. Grading suggestions for left ventricular
191 (Table 3), right ventricular (Table 4), left atrial (Table 5), right atrial (Table 6) and aortic parameters
192 (Table 7), based mainly on a recent review containing normal ranges, are provided.¹⁶

193

194 **Left and right ventricular ejection fraction**

195 Ejection fraction of the left ventricle is one of the most commonly used cardiac imaging
196 parameters in clinical practice. Left and right ventricular ejection fraction grades were decided on
197 using a combination of statistical method and consensus consistent with the method used by the

198 EACVI echocardiography recommendations.¹¹ Normal range was based on statistical method
199 (published mean +/- 2 standard deviation). Mildly reduced systolic function was based on a
200 combination of statistical method (for upper range, mean - 2 standard deviations) and consensus
201 (for lower range). Grading for moderate and severely reduced left ventricular systolic function was
202 based on consensus between the group and in line with the cut offs published in the EACVI
203 echocardiography document.¹¹

204 Normalizing or indexing the reference values according to body habitus can be done in many
205 different ways, most commonly values are indexed to body surface area. The principles of
206 categorizing abnormal values to mildly, moderately or severely abnormal are independent of the
207 indexing approach.

208

237 **Left and right atria**

238

239 We would ideally recommend using volume assessment rather than the areas for the atria for
240 increased accuracy. However, there are some discrepancies in the normal reference values for LA
241 volume between some studies and this should be considered when interpreting the results.^{19,21} As
242 3-dimensional analysis tools are not readily available and may be more time consuming, our
243 current recommendation would be to use the biplane method of disks/ area analysis based on 2-
244 dimensional images from 4 and 2 chamber views. There is need for a future update of the grading
245 cut-offs for LA and RA volumes with larger reference range studies. In the meantime, we have still
246 included the LA area measurements. Similar caution in interpretation should be used when
247 assessing RA volume measurements as discrepancies also exist for normal reference range values
248 for the RA. This is likely in part due to the assumptions made when using the equations to derive
249 volume measurements from a single 4 chamber view.

250

251 It should be noted that echo assessment predominantly uses the area-length method or the
252 modified Simpson' rule (Figure 2). Differences in volumes from 3D CMR measures and from echo
253 will exist due to different techniques, spatial resolution and from the inclusion of the appendages
254 in the volumes measured by CMR. For these reasons care should be taken to avoid direct
255 comparison of measurements and cut-offs obtained from CMR and echo.

256

257 ***Aortic root indices***

258 Although the proposed acquisition method is relatively simple, correct alignment of the oblique
259 sagittal and coronal imaging planes may be difficult and ensuring reliable measurements can be
260 challenging, as applied in the study of Burman et al.²⁵ A 3-dimensional SSFP or a contrast enhanced
261 magnetic resonance angiography may be the more appropriate method for ensuring precise
262 measurements. However, further studies are needed to validate the most accurate and
263 reproducible method of measuring the aorta using CMR and other imaging modalities. Previous
264 guidelines recommended that maximum aneurysm diameter be ideally measured perpendicular to
265 the centre line of the vessel with 3-dimensional reconstruction of CT scan images whenever
266 possible. This approach appears to offer more accurate and reproducible measurements of true
267 aortic dimensions compared with axial cross-section diameters. Using sagittal and coronal views in
268 CMR can provide a good estimation of aortic measurements but may be inaccurate in measuring
269 the true maximum diameters in cases where asymmetry exists.

270

271 **Limitations**

272

273

274 The measures for grading are based on currently available normal ranges. These are based on
275 relatively small cohorts of healthy volunteers and there may be some variations between
276 published reference ranges. Utilizing the methodology outlined in this consensus paper we plan to
277 update this consensus paper using normal ranges of larger cohorts, such as from the UK Biobank

278 study, once further validation work has been completed in order to provide more robust reference
279 ranges. Reference values for LV volumes and mass are influenced by gender and age and thus
280 were presented separately in reference range paper, however, given the small sample sizes in the
281 age categorized tables we considered it would be more accurate to provide age categorized
282 grading parameters derived from larger data sets in the future.

283 Indexed measurements may present limitations when considering obese patients, as the increase
284 in chambers volumes/dimensions is not necessarily proportional to the increase in body surface
285 area and may thus lead to inconsistencies. Unfortunately, this is a common problem for a number
286 of imaging modalities and is not unique to CMR. Ideally the cut-offs for severity categorization
287 using CMR and other imaging modalities should be linked with their impact on the outcomes.
288 However, data regarding this are currently limited. Direct comparison in large cohorts with
289 echocardiography should be done in the future since CMR and echo measures are not directly
290 comparable (different techniques, different measurements' methods) and cut-offs may not be the
291 same when considering severity categorization. This will have obvious clinical impact such as when
292 deciding on suitability for advanced cardiac device therapy e.g. cardiac resynchronization therapy
293 or implantable cardioverter defibrillators.

294
295 Aortic measurements may be more accurately determined using more advanced CMR techniques
296 (e.g. 3D high resolution non-contrast native MRA with high isotropic resolution); also, the studies
297 quoted were published before the SCMR 2013 Standardized image interpretation and post
298 processing in CMR paper,⁶ so could introduce some variability in measurements reported between
299 the studies quoted, and contemporary practices.

300
301 The normal ranges for right ventricular end-diastolic volumes indexed to body surface area using
302 the contemporary steady state free precession cine imaging approach contain the cut-off values

303 for major or minor criteria as part of the ARVC task force criteria.²⁶ The ARVC task force criteria
304 were developed largely based on gradient echo cine CMR which is known to underestimate
305 volumes due to lower/incomplete endocardial border definition.^{12,27} Arguably, the ARVC Task
306 Force criteria may need updating based on contemporary SSFP cine normal ranges provided in this
307 expert consensus document to avoid being too sensitive or lacking specificity.

308

309

310 **Acknowledgements**

311 Dr Bucciarelli-Ducci is supported by the Bristol NIHR Cardiovascular Biomedical Research Unit at
312 the Bristol Heart Institute, Bristol, UK. Professor Steffen Petersen is supported by the NIHR Barts
313 Biomedical Research Centre. The views expressed are those of the authors and not necessarily
314 those of the National Health Service, National Institute for Health Research, or Department of
315 Health. Prof Plein is supported by a British Heart Foundation Personal Chair (CH/16/2/32089).

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427 *Eur Heart J* 2014; 35:2873–926.

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430

431 **Table 1: Summary of measurements and techniques used in the normal values published papers included in this**
 432 **consensus paper.**

Parameter/Method	Technique	Advantages	Limitations
LV mass and volumes^{19,20} (Figure 1)	Papillary muscles included in the mass and excluded from the volumes (Figure 1)	More accurate assessment of mass	More time consuming. Often not followed in clinical practice
RV mass and volumes^{19,20} (Figure 1)	Papillary muscles included in the mass and excluded from the volumes (Figure 1)	More accurate assessment of mass	More time consuming
LA volumes¹⁹ (Figure 2)	Biplane area-length method in HLA and VLA. LA appendage included in LA area but not PVs (Figure 2)	Available from standard imaging SSFP	Not as accurate as SAX contours or 3D analysis
LA volumes²¹	3D modelling, including tracking of AV ring. At phase in which LA size maximal. LA appendage included in LA area but not PVs	More accurate than biplane area length method	Requires 3D modelling software for SSFP image analysis
RA volumes²² (Figure 3)	3D modelling, including tracking of AV ring and time volume curves. At phase in which RA size maximal.	More accurate than area length method (Figure 3)	Requires 3D modelling software for SSFP image analysis
Aortic root dimensions²⁵ (Figure 4)	SSFP images endo-endo from oblique coronal and oblique sagittal views in late diastole (Figure 4)	Accurate assessment of aortic dimensions in 2D	Requires ECG gating. Not as accurate as 3D assessment

433

434 Abbreviations: AV= Atrioventricular; HLA= Horizontal long axis; LA= Left atrium; LV= Left ventricle;
 435 PV= Pulmonary vein; RA= Right atrium; RV= Right ventricle; SAX= Short axis; SSFP= Steady state
 436 free precession; VLA= Vertical long axis; 2D= 2-dimensional; 3D= 3- dimensional

Table 2. Details of individual studies used to derive the grading parameters in this consensus document.

Study author	Subjects (M:F)	Age range, years	Subjects details	Country	Field strength	Chamber	Measurement methods
Maceira et al ²⁰	120 (60:60) 10 M and 10 F in 6 age deciles from 20 to 80 years	20-80	Healthy volunteers. Asymptomatic, no known cardiovascular risk factors or history of cardiac disease. Normal physical examination and ECG. Normal BNP levels.	UK	1.5 Tesla	Left Ventricle	SSFP cine imaging. Left ventricular short axis stack. Papillary muscles included in mass and excluded from volumes. Slice thickness of 7mm. Basal slices for end-diastole and end-systole had at least 50% of blood volume surrounded by myocardium. The apical slice defined as last slice showing intracavity blood pool (Figure 1)
Maceira et al ²³						Right Ventricle	Included papillary muscles in mass and excluded them from volumes. Slice thickness of 7mm.
Maceira et al ²¹						Left atrium	3-D modelling, including tracking of AV ring. Atrial volumes analysed in 2 steps. Endocardial borders included atrial appendage included in the volume. Systolic descent and twist of the mitral valve was calculated from the tracking of the valve motion on the long axis cine to allow for correction for increase in LA volume due to AV ring descent. LA diameters and areas were measured at end systole. Left atrial appendage included in the atrial volume, but pulmonary veins were not. Slice thickness of 5mm with no inter-slice gap.
Maceira et al ²²						Right atrium	3-D modelling, including tracking of AV ring and time-volume curve analysis. RA maximum volume and maximum diameter measured in the 4-chamber and right 2-chamber views. Volume analysis in 2 steps. 1) Delineation of atrial endocardial border in all cardiac phases. 2) Systolic descent and twist of the tricuspid valve calculated from tracking valve motion in long axis cines, to correct for the increase in atrial volumes due to AV ring descent. Atrial appendage included in volumes, vena cava excluded. Diameters and areas from 2D images measured in the phase and corresponding cines where atrial size and volumes were at a maximum. Longitudinal diameter measured from the midpoint of a line between the septal and lateral (superior and inferior pertaining to the 2-chamber view) insertion of the tricuspid valve to the roof of the right atrium. Transverse diameter measured perpendicular to the midpoint of the longitudinal diameter. Slice thickness of 5mm with no inter-slice gap.

Hudsmith et al¹⁹	108 (63:45)	21-68	Healthy volunteers. No history of cardiac disease, hypertension or cardiac risk factors and had a normal baseline electrocardiogram	UK	1.5 Tesla	Left Ventricle	SSFP cine imaging. Papillary muscles were included in the mass and excluded from the volumes. Slice thickness of 7mm was used for scanning (Figure 1).
						Right Ventricle	RV volumes below the pulmonary valve. RV volumes were excluded if the surrounding muscle was thin and not trabeculated, suggestive of right atrium. Papillary muscles were included in the mass and excluded from the volume calculation.
						Left atrium	Left atrial volumes, ejection fraction and stroke volumes using the biplane area-length method in the horizontal and vertical long axis. Left atrial appendage included in the atrial volume, but the pulmonary veins were excluded
Alfakih et al²⁴	60 (30:30)	20-65	Healthy volunteers. with no history of cardiovascular disease or hypertension, with a normal blood pressure, normal cardiovascular examination and normal resting electrocardiogram. Subjects with arrhythmia, who were pregnant or elite athletes were excluded.	UK	1.5 Tesla	Left Ventricle	SSFP cine imaging. Papillary muscles included in the mass and excluded from the volumes (Figure 1). Slice thickness of 7mm.
						Right ventricle	Included papillary muscles in the RV volume and excluded them from the mass (Figure 1).
Sievers et al²⁸	70 (38:32)	25-73	Healthy volunteers. No cardiac or pulmonary disease and no cardiovascular risk factors.	Germany	1.5 Tesla	Right atrium	SSFP cine images. Atrial parameters from both short axis (atrial appendage was included in the volume, vena cava excluded, not included in this paper) and area length method (right atrial volumes and EF were then calculated using the area length method for ellipsoid bodies using formula: $8 \times (\text{Area1})^2 / 3\pi \text{Length}$, included in this paper) from the 4-chamber view (Figure 3).
Burman et al²⁵	120 (60:60)	20-80	Healthy volunteers. Asymptomatic, had no known cardiovascular risk factors or history of cardiac disease. Physical examination was normal and the ECG was unremarkable. All brain natriuretic peptides (BNP) levels were in the normal range.	UK	1.5 Tesla	Aorta	SSFP cines images. Maximum systolic and end diastolic measurements at 3 levels in sagittal and coronal LVOT planes: at level of the aortic annulus, at level of the maximum diameter across the sinuses, and at sinotubular junction (Figure 4). Slice thickness of 7mm.

438 Abbreviations: BNP = brain natriuretic peptide; ECG = electrocardiogram; EF = ejection fraction; LV = left ventricle; RV = right ventricle; SSFP = steady state free precession; UK =
439 United Kingdom;

440

441 **Table 3 – Left ventricle ranges for adults aged 20-80 years* based on Kawel-Boehm meta-analysis.**¹⁶

	Women					Men					Methods and Reference
	“Opposite”	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	“Opposite”	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	
20-80 years											
EDV [ml]	<86	86 - 178	179 - 201	202 - 224	>224	<106	106 - 214	215 - 241	242 - 268	>268	SM
EDV /BSA [ml/m ²]	<56	56 - 96	97 - 106	107 - 116	>116	<57	57 - 105	106 - 117	118 - 129	>129	SM
ESV [ml]	<22	22 - 66	67 - 77	78 - 88	>88	<26	26 - 82	83 - 96	97 - 110	>110	SM
ESV/BSA [ml/m ²] [#]	<14	14 - 34	35 - 39	40 - 44	>44	<14	14 - 38	39 - 44	45 - 50	>50	SM
EF [%]	>78	57 - 77	41 - 56	30 - 40	<30	>78	57 - 77	41 - 56	30 - 40	<30	SM, EC
Mass [g]	<56	56 - 140	141 - 161	162 - 182	>182	<92	92 - 176	177 - 197	198 - 218	>218	SM
Mass/BSA [g/m ²]	<41	41 - 81	82 - 91	92 - 101	>101	<49	49 - 85	86 - 94	95 - 103	>103	SM

442 Abbreviations: BSA = Body surface area; EC = Expert consensus; EDV = End-diastolic volume; EF = Ejection fraction; ESV = End-systolic volume; LV=
 443 Left ventricular; “Opposite” refers to values that outside the normal range but in the opposite direction of typical pathology, e.g. smaller LV end-
 444 diastolic volumes or supra-normal LV ejection fraction; SM = Statistical method.

445 *Combined values from references Alfakih²⁴ (30 Males:30 Females), Hudsmith¹⁹ (63 Males:45 Females), Maceira²⁰ (60 Males:60 Females), unless stated
 446 otherwise.

447 [#]From references Hudsmith¹⁹ (63 Males:45 Females) and Maceira²⁰ (60 Males:60 Females) only.

448

449

450

451 **Table 4 – Right Ventricle ranges for adults aged 20-68 years* based on Kawel-Boehm meta-analysis.**¹⁶

	Women					Men					Methods and Reference
	“Opposite”	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	“Opposite”	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	
20-68 years											
EDV [ml]	<77	77-201	202-232	233-263	>263	<118	118-250	251-283	284-316	>316	SM
EDV /BSA [ml/m ²]	<48	48-112	113-128	129-144	>144	<61	61-121	122-136	137-151	>151	SM
ESV [ml]	<24	24-84	85-99	100-114	>114	<41	41-117	118-136	137-155	>155	SM
ESV/BSA [ml/m ²] [#]	<12	12-52	53-62	63-72	>72	<19	19-59	60-69	70-79	>79	SM
EF [%]	>71	51-71	41-51	30-40	<30	>72	52-72	41-52	30-40	<30	SM, EC
Mass [g] [#]	<21	21-49	50-56	57-63	>63	<25	25-57	58-65	66-73	>73	SM
Mass/BSA [g/m ²] [#]	<12	12-28	29-32	33-36	>36	<13	13-29	30-33	34-37	>37	SM

452 Abbreviations: BSA = Body surface area; EC = Expert consensus; EDV = End-diastolic volume; EF = Ejection fraction; ESV = End-systolic volume; RV=
 453 right ventricular; “Opposite” refers to values that outside the normal range but in the opposite direction of typical pathology, e.g. smaller LV end-
 454 diastolic volumes or supra-normal LV ejection fraction; SM = Statistical method.

455 *Combined values from references Alfakih²⁴ (30 Males:30 Females), Hudsmith¹⁹ (63 Males:45 Females).

456 [#]From references Hudsmith (63 Males:45 Females) only.

457

458

459 **Table 5 – Left atrial maximal volume in the adult based on 3D modeling method and left atrial maximal area in the adult for the SSFP technique*.**²¹

	Women					Men					Methods and Reference
	“Opposite”	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	“Opposite”	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	
20-80 years											
Max. LA volume (ml)	<38	38-98	99-113	114-128	>128	<47	47-107	108-122	123-137	>137	SM
Max. LA volume/ BSA (ml/m ²)	<27	27-53	54-60	61-67	>67	<26	26-52	53-59	60-66	>66	SM
Adults											
Area (cm ²) 4Ch	<13	13-27	28-31	32-35	>35	<15	15-29	30-33	34-37	>37	SM
Area/BSA (cm ² / m ²) 4Ch	<8.4	8.4-15.6	15.7-17.4	17.5-19.2	>19.2	<7.4	7.4-14.6	14.7-16.4	16.5-18.2	>18.2	SM
Area (cm ²) 2Ch	<10	10-28	29-33	34-38	>38	<12	12-30	31-35	36-40	>40	SM
Area/BSA (cm ² / m ²) 2Ch	<6.2	6.2-15.8	15.9-18.2	18.3-20.6	>20.6	<6.2	6.2-15.8	15.9-18.2	18.3-20.6	>20.6	SM
Area (cm ²) 3Ch	<10	10-24	25-28	29-31	>31	<12	12-26	27-30	31-33	>33	SM
Area/BSA (cm ² / m ²) 3Ch	<6.4	6.4-13.6	13.7-15.4	15.5-17.2	>17.2	<6.4	6.4-13.6	13.7-15.4	15.5-17.2	>17.2	SM

460 Abbreviations: BSA – Body surface area; LA – Left atrium; Max – Maximum; “Opposite” refers to values that outside the normal range but in the
 461 opposite direction of typical pathology; SM = Statistical method; 2Ch = 2 chamber view; 3Ch = 3 chamber view; 4Ch = 4 Chamber view; SSFP= Steady
 462 state free precession.

463 *From reference according to reference Maceira, 2010 (60 Males:60 Females) only.²¹

464

465 **Table 6 – Right atrial maximal volume and right atrial maximal area in the adult for the SSFP technique based on Sievers²⁸ and Maceira**

466 publications*.²²

	Adults					Methods and Reference
	“Opposite”	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	
25-73 years						
Max. RA volume (ml)*	<37	37-169	170-202	203-235	>235	SM
Max. RA volume/BSA (ml/m2)*	<18	18-90	91-108	109-126	>126	SM
20-80 years						
Area (cm2) 4Ch#	<14	14-30	31-34	35-38	>38	SM
Area/BSA (cm2/m2) 4Ch#	<8	8-16	17-18	19-20	>20	SM
Area (cm2) 2Ch#	<14	14-30	31-34	35-38	>38	SM
Area/BSA (cm2/m2) 2Ch#	<8	8-16	17-18	19-20	>20	SM

467 Abbreviations: BSA = Body surface area; Max = Maximum; Min = Minimum; “Opposite” refers to values that outside the normal range but in the
 468 opposite direction of typical pathology; RA = Right atrium; SM = Statistical method; 2Ch = 2 chamber view; 4Ch = 4 Chamber view; SSFP= Steady state
 469 free precession.

470 *From reference a Sievers 2007 (38 Males:32 Females) only.²⁸

471 #From reference Maceira 2013 (60 Males:60 Females) only.²²

472

473

474

475 **Table 7: Aortic root dimensions reference ranges for based on Burman publication*.²⁵**

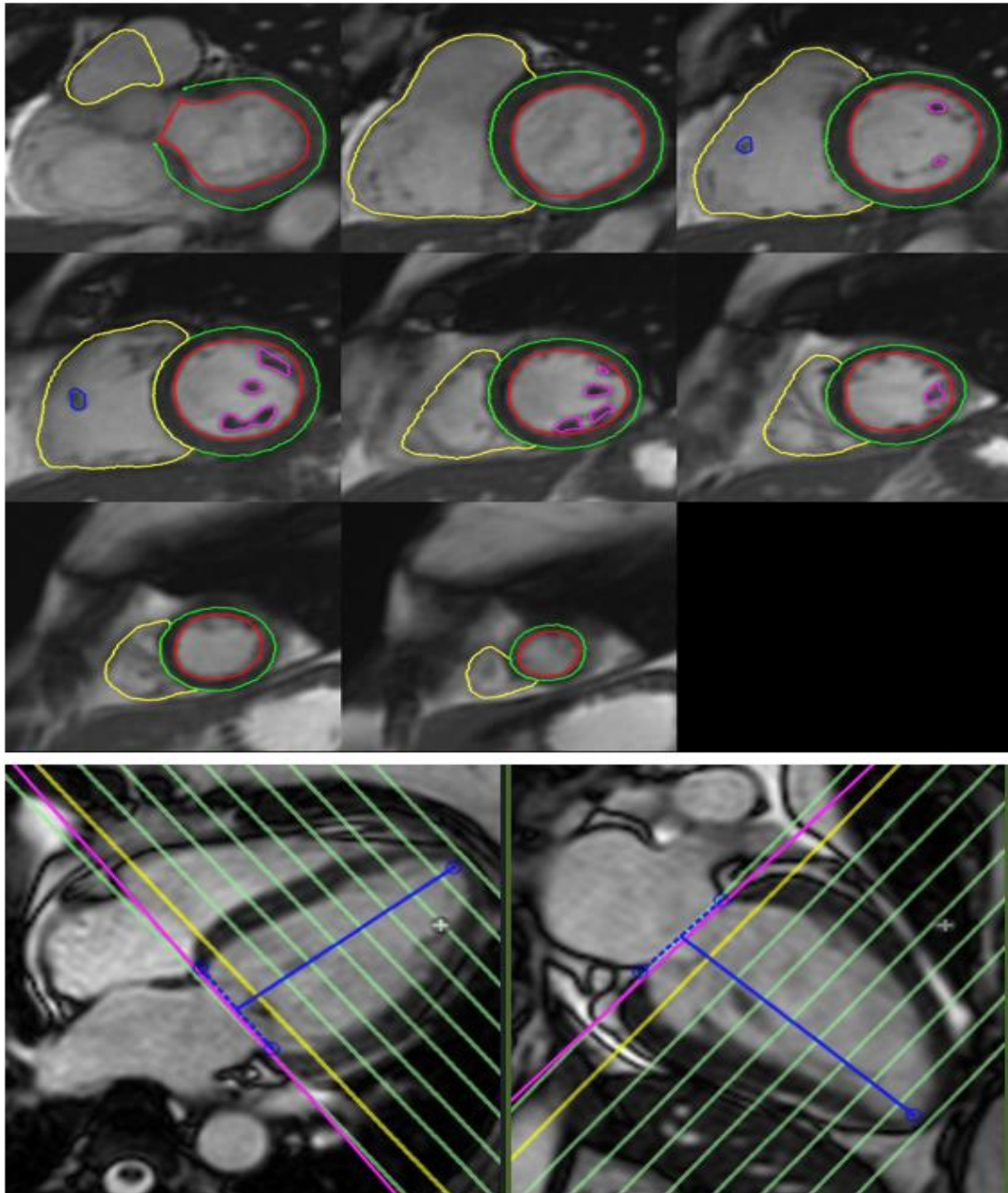
	Women					Men					Methods and Reference
	"Opposite"	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	"Opposite"	Reference range	Mildly abnormal	Moderately abnormal	Severely abnormal	
20 – 80 years											
Annulus (s) (mm)	<16.	16 - 23	24 - 25	26 - 28	>28	<17	17 - 27	28 - 29	30 - 32	>32	SM
Annulus (c) (mm)	<19	19 - 27	28 - 29	30 - 32	>32	<21	21 - 30	31 - 33	34 - 36	>36	SM
Aortic sinus(s) (mm)	<22	22 - 35	36 - 39	40 - 42	>42	<24	24 - 40	41 - 45	46 - 50	>50	SM
Aortic sinus(c) (mm)	<24	24 - 36	37 - 40	41 - 43	>43	<25	25 - 42	43 - 47	48 - 52	>52	SM
STJ (s) (mm)	<18	18 - 30	31 - 33	34 - 36	>36	<17	17 - 33	34 - 37	38 - 42	>42	SM
STJ (c) (mm)	<18	18 - 28	29 - 31	32 - 34	>34	<18	18 - 32	33 - 36	37 - 40	>40	SM

476 Abbreviations: c = Coronal left ventricular outflow plane; F = Female; M = Male; STJ = Sino tubular junction; s = Sagittal left ventricular outflow plane;

477 SM = Statistical method

478 *From reference Burman 2008 (60 Males:60 Females) only.²⁵

479

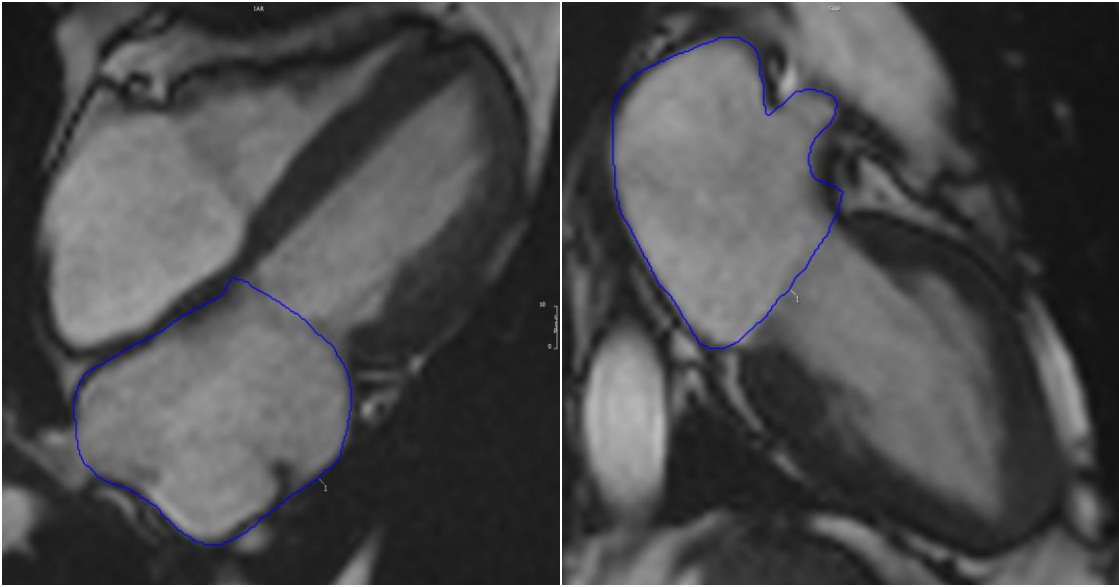


LV epicardium —
 RV endocardium —
 LV endocardium —

480

481 **Figure 1: Short axis slices including left ventricular endocardial and epicardial contours and right**
 482 **ventricular endocardial contours. The 4 and 2 chamber views show the full coverage of the left**
 483 **and right ventricles required for analysis.**
 484

485



486

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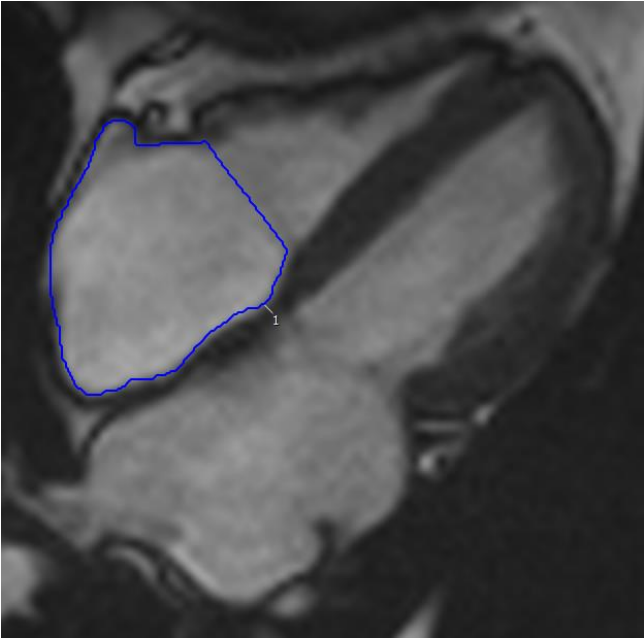
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Figure 2: Left atrial contours for area assessment in 4 and 2 chambers during atrial end diastole, measures just before the mitral valve opening for maximum LA volume.

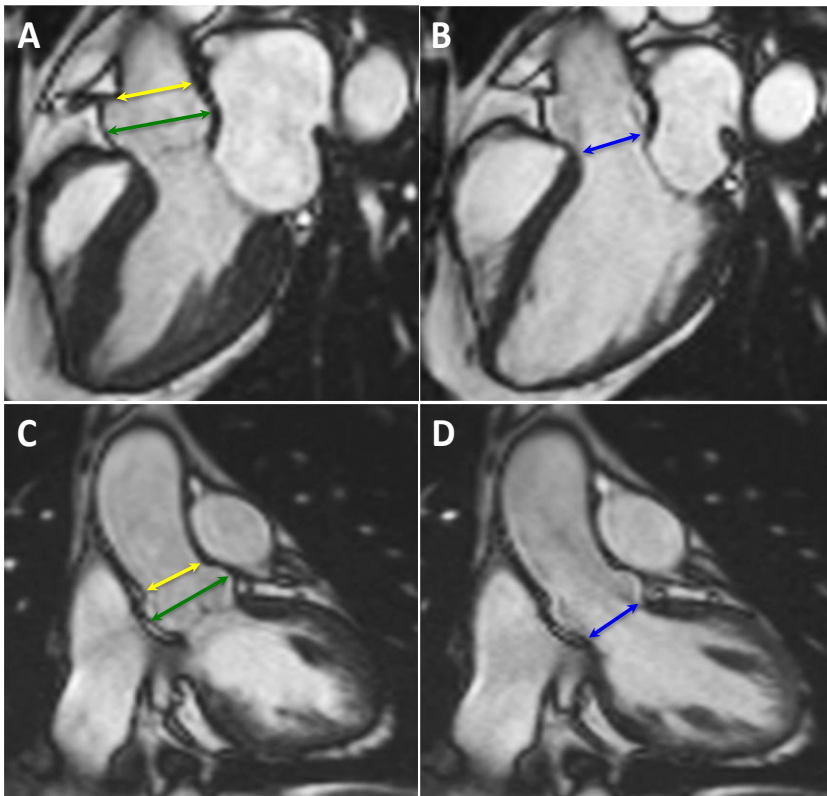


492

493 **Figure 3: Right atrial contour for area length measurement during atrial end diastole for**
494 **maximal RA volume.**

495

496



Annulus ↔
 Sinus ↔
 Sino-tubular junction ↔

497

498 **Figure 4: Oblique sagittal[#] (A, B) and oblique coronal^{*} (C, D) left ventricular outflow views**
 499 **showing the common aortic root measurements. Typically, annulus measured during systole and**
 500 **sinuses of Valsalva and sino-tubular junction measured in diastole.** ^{11,29}
 501

502 ^{*}Oblique sagittal images were obtained by aligning orthogonal to the coronal scouts in the axis of
 503 the left ventricular outflow tract and proximal ascending aorta.

504 [#]Oblique coronal acquisitions were then located orthogonal to the oblique sagittal cine, aligned
 505 with the axis of the left ventricular outflow tract.²⁵
 506

Word count including references, tables, figure legends

6793