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(54) **NANOPARTICLES OF CERIUM OXIDE TARGETED TO AN AMYLOID-BETA ANTIGEN OF ALZHEIMER'S DISEASE AND ASSOCIATED METHODS**

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USPC **424/194.1**; 424/489; 424/9.32; 424/193.1; 514/17.7; 514/17.8

(58) **Field of Classification Search**

CPC A61K 47/48907; A61K 47/48538;
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See application file for complete search history.

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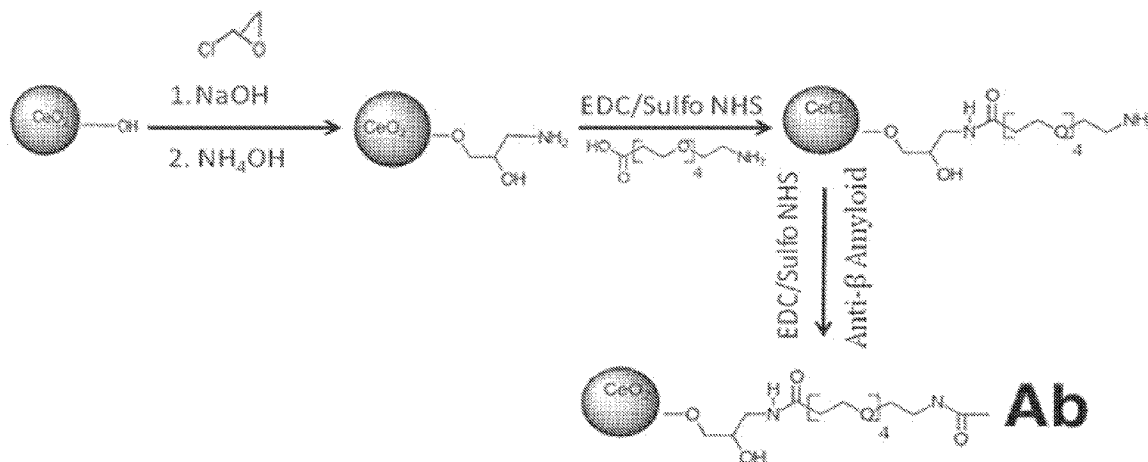
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(57) **ABSTRACT**

Disclosed is a composition immunologically targeted to Alzheimer's disease (AD), the composition containing amine functionalized nanoparticles of Cerium oxide coated with polyethylene glycol and bearing an antibody specific for an amyloid-beta antigen associated with AD. The invention also includes a medication manufactured with the targeted nanoceria particles and methods of treatment by administering the targeted nanoceria particles to patients in need thereof.

11 Claims, 12 Drawing Sheets



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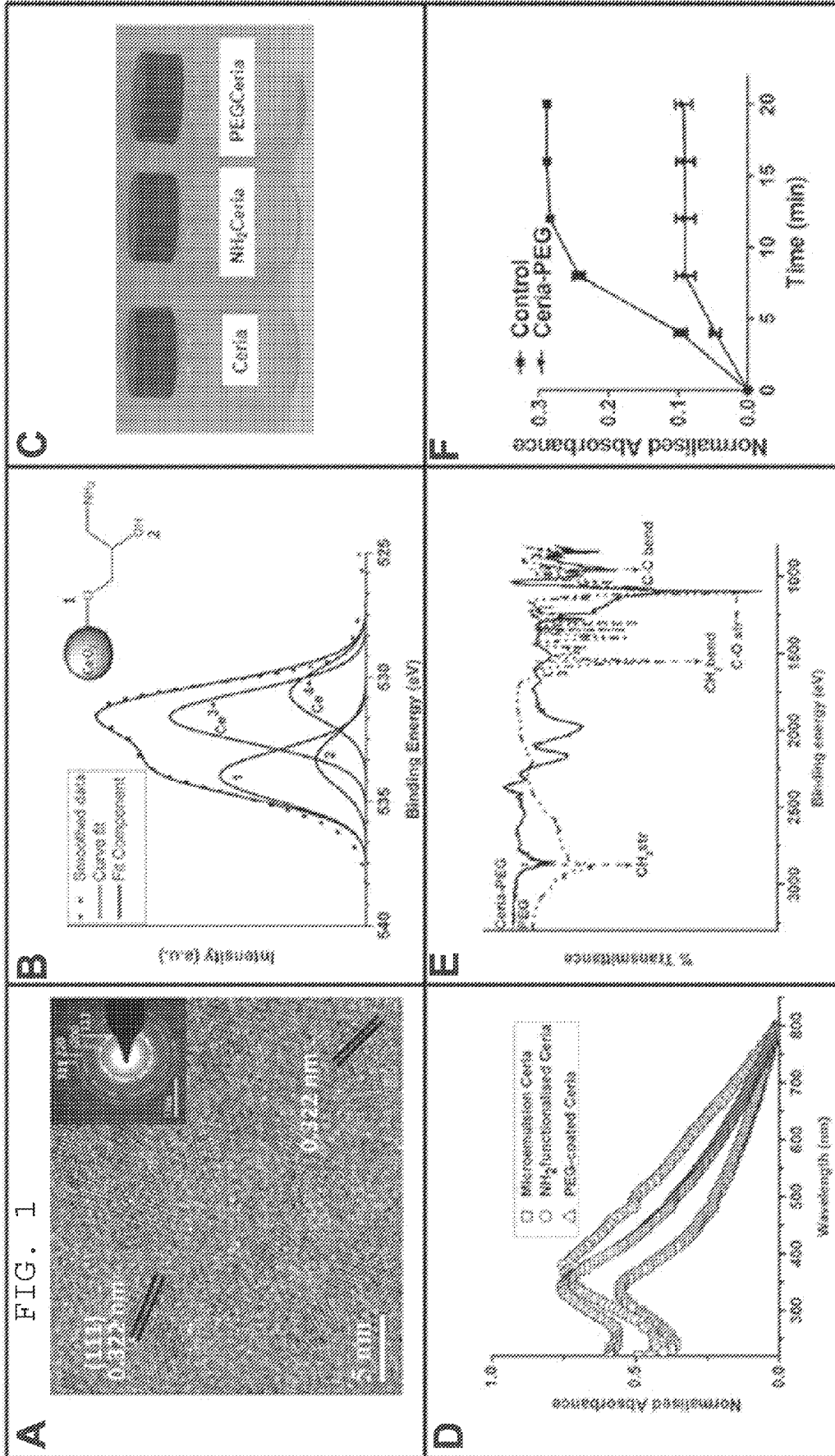
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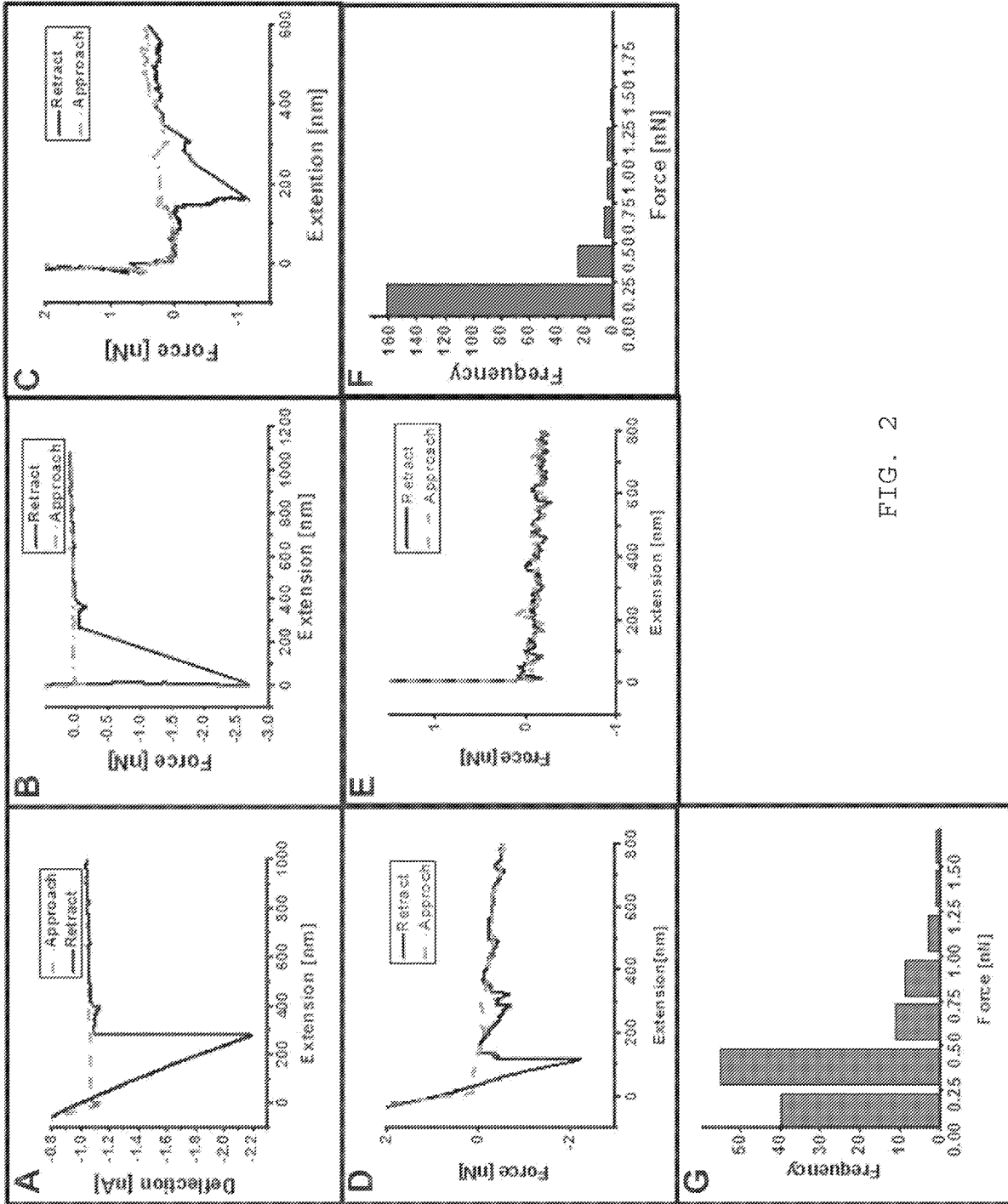


FIG. 2

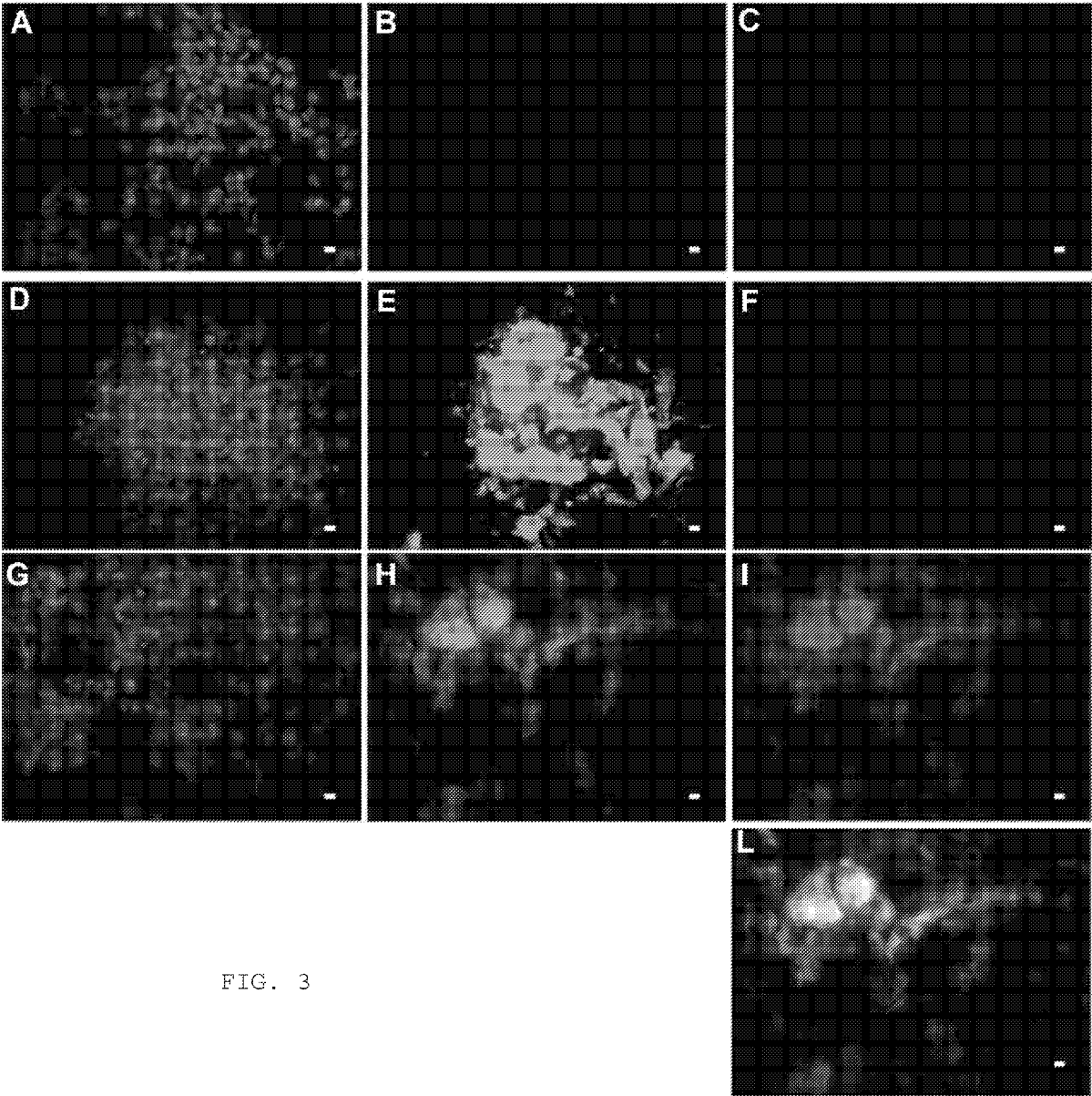


FIG. 3

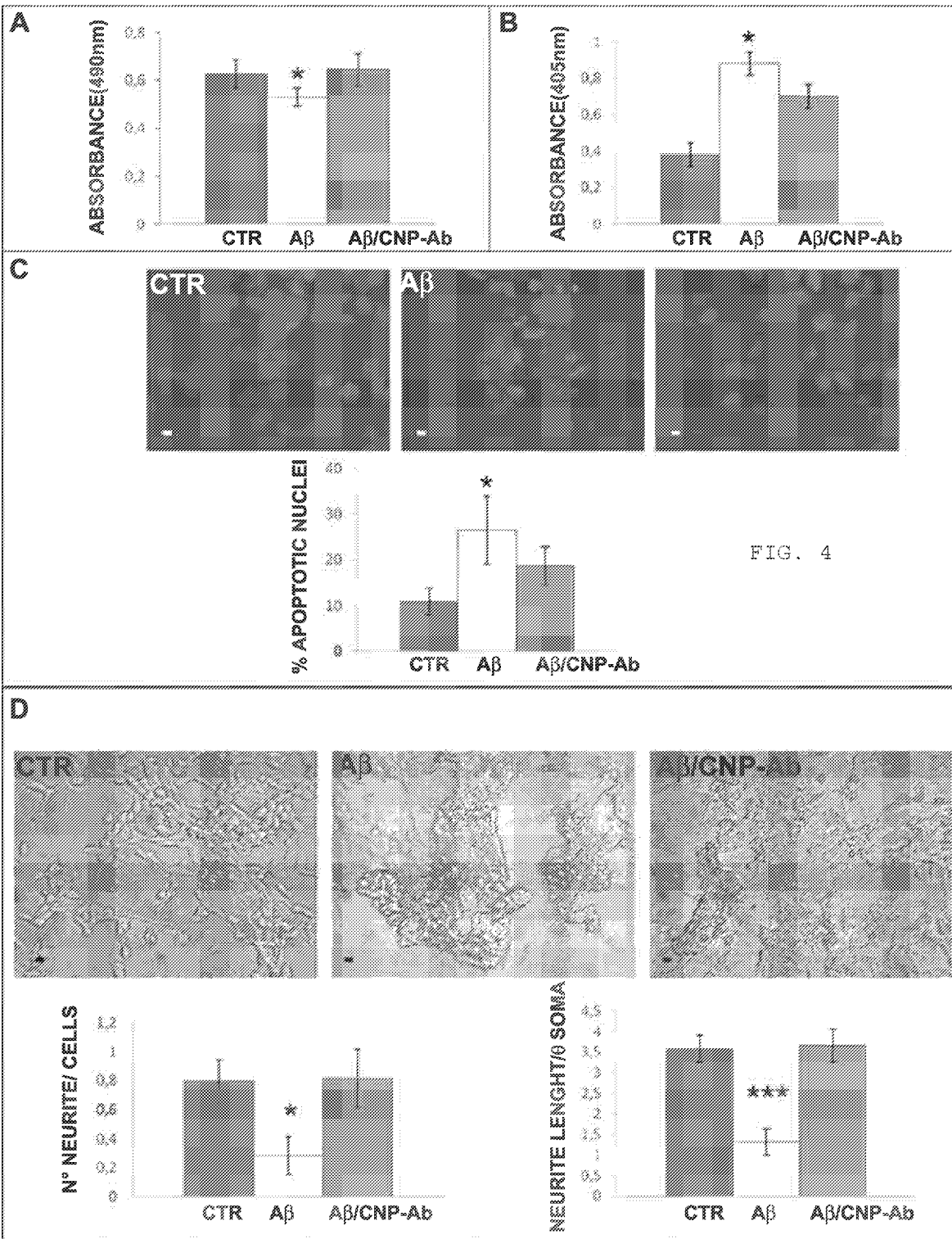


FIG. 4

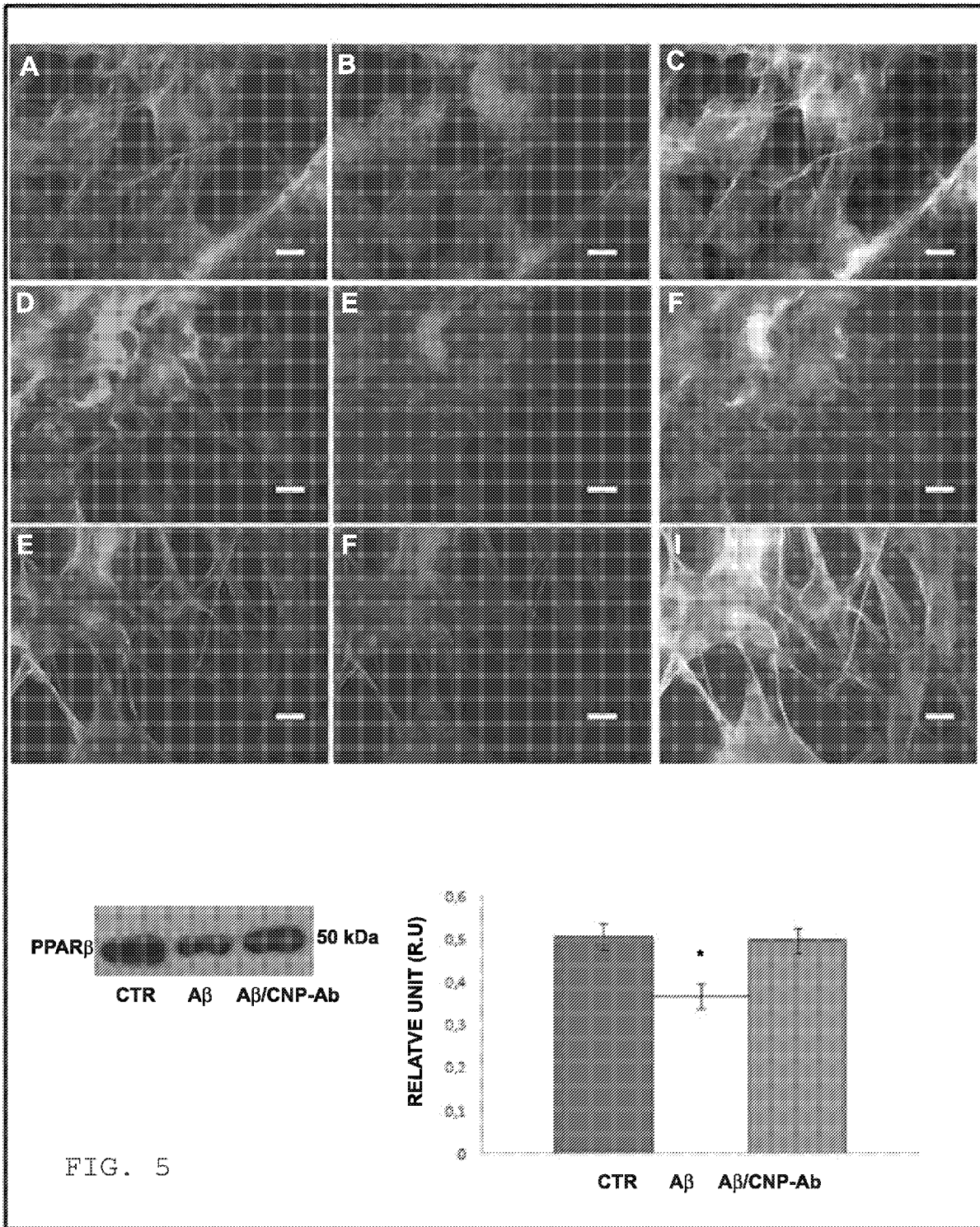


FIG. 5

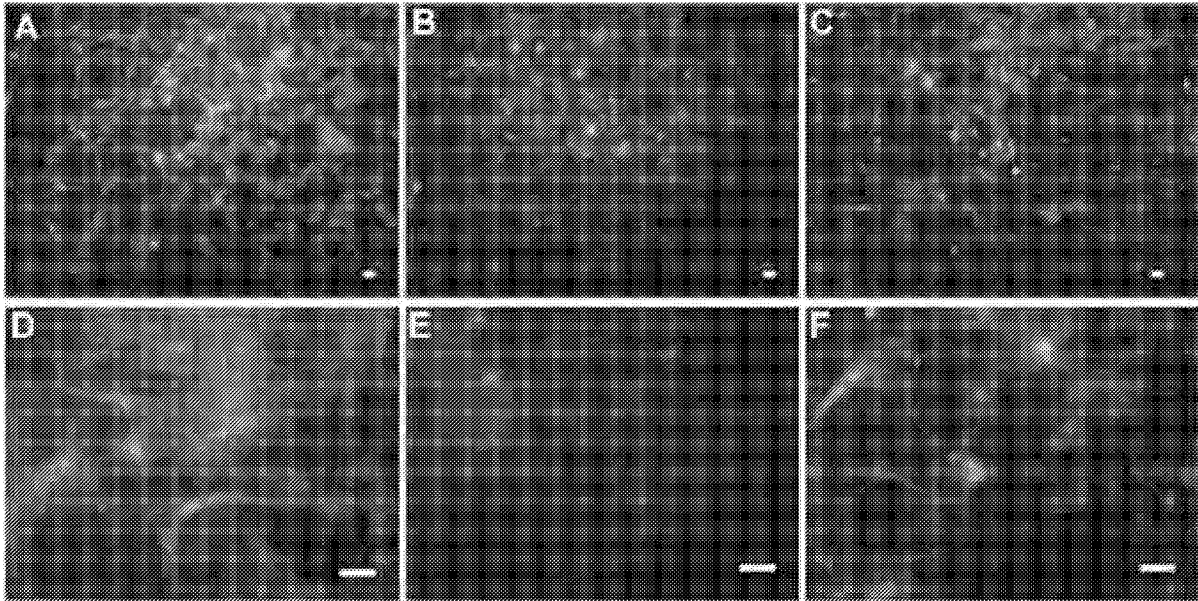
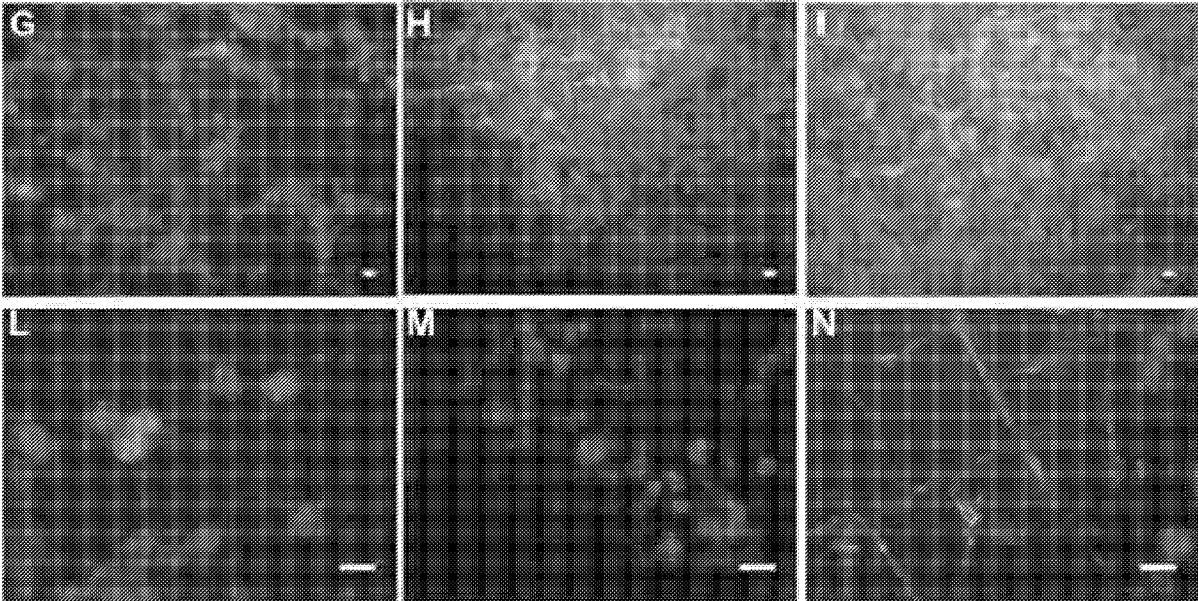
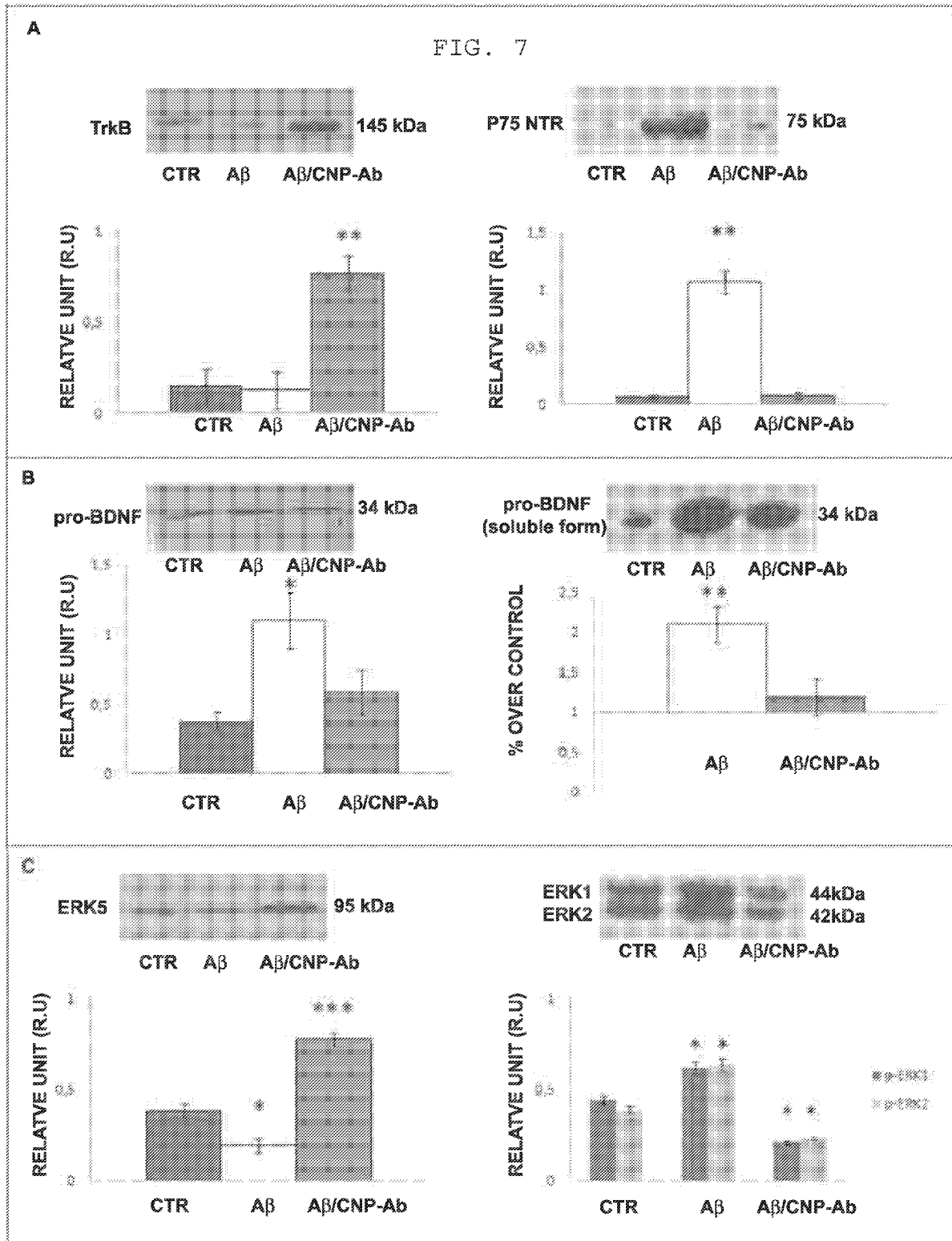


FIG. 6





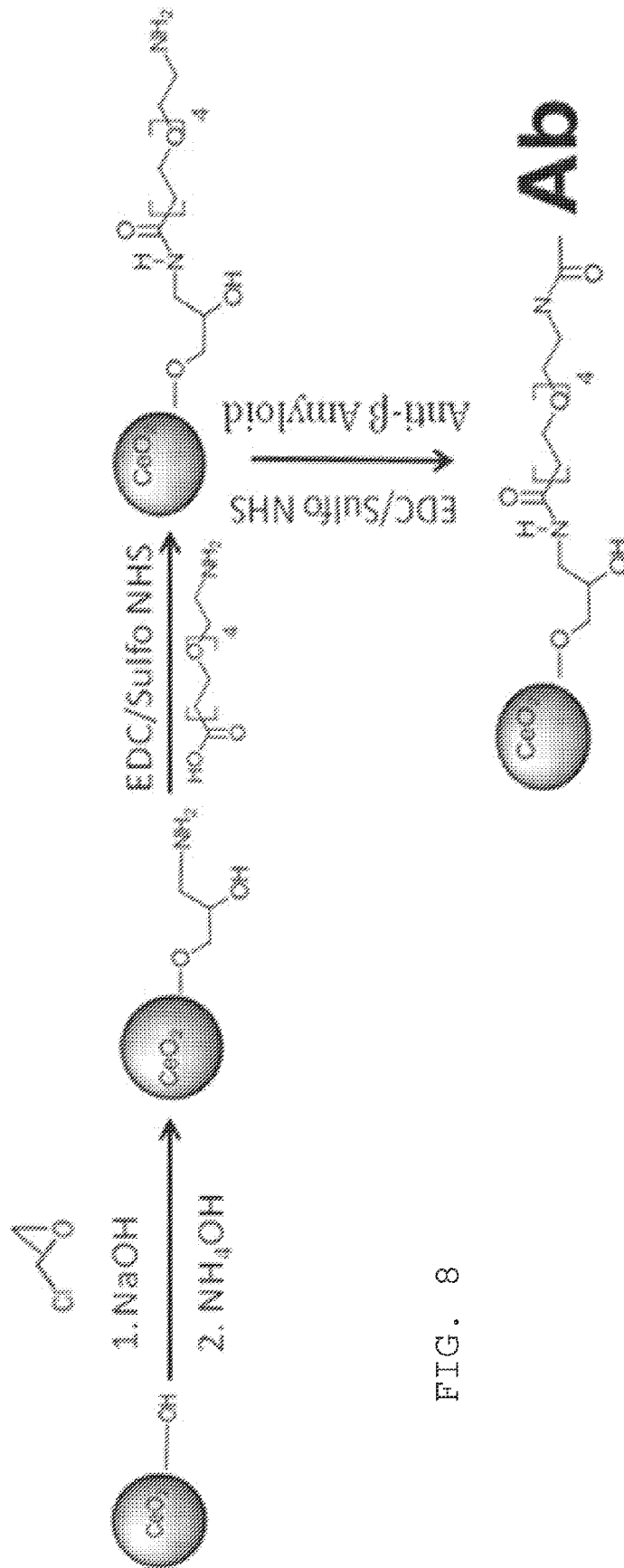


FIG. 8

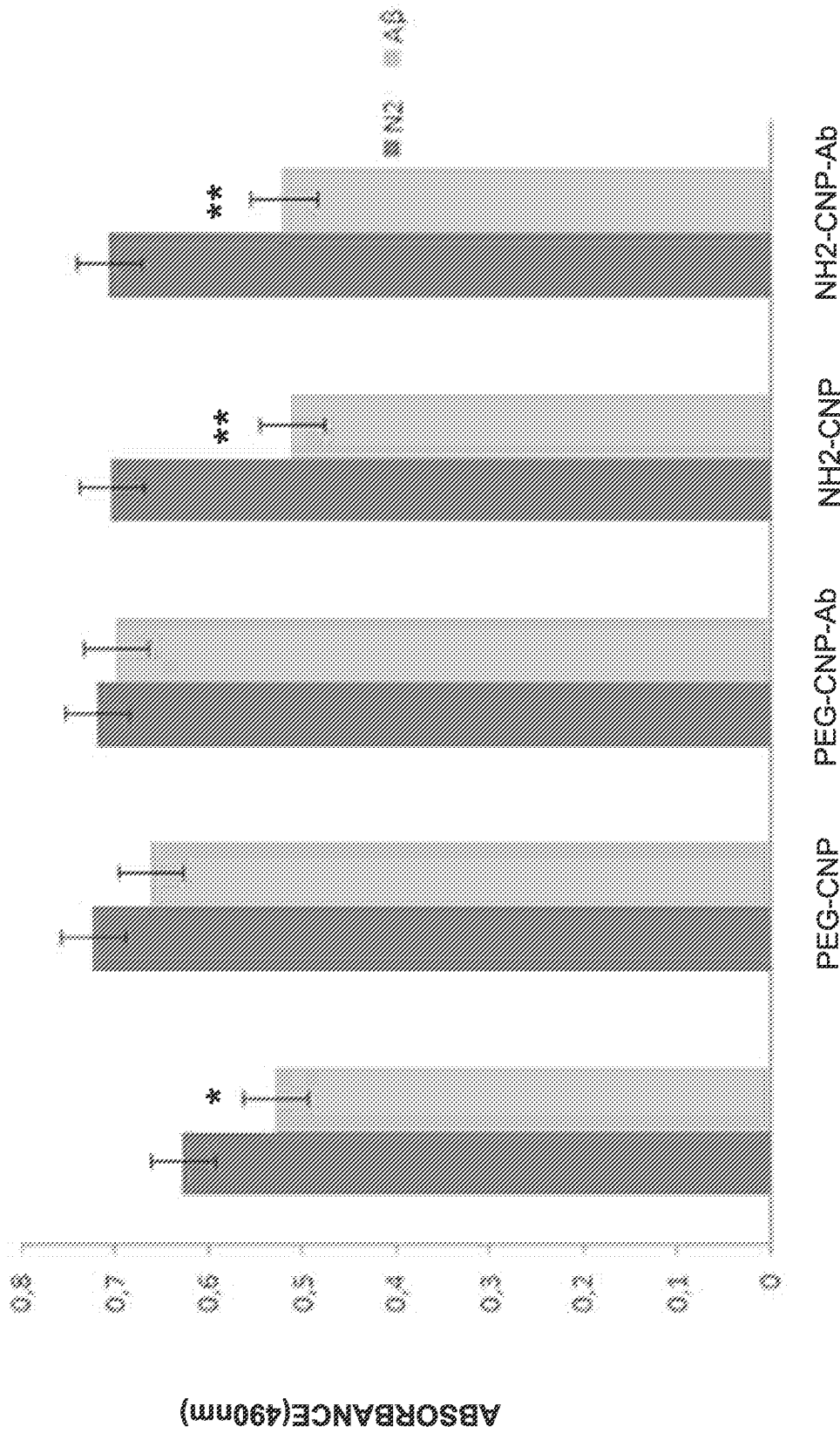


FIG. 9

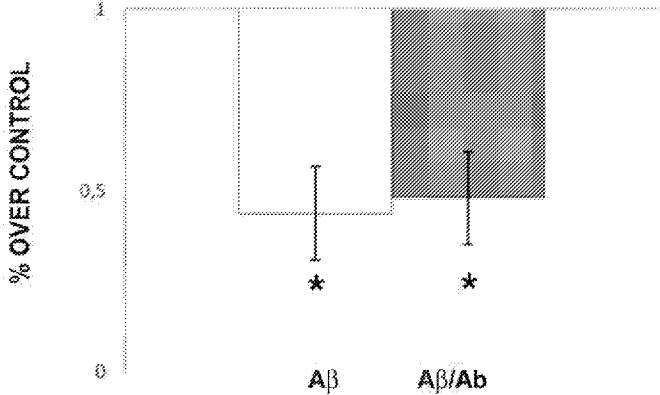
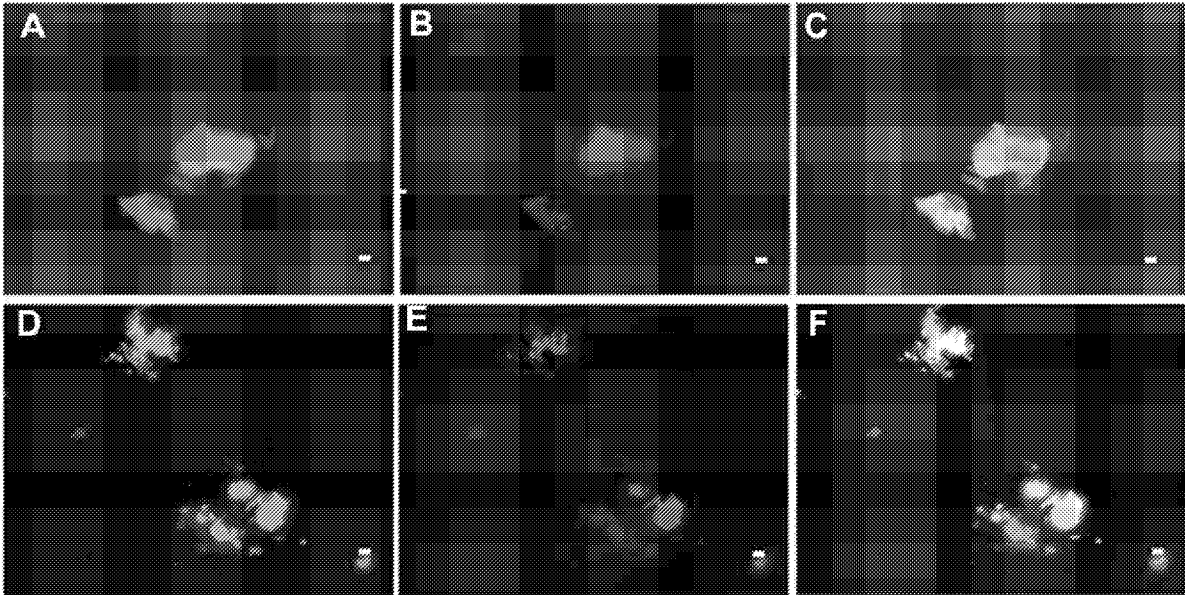
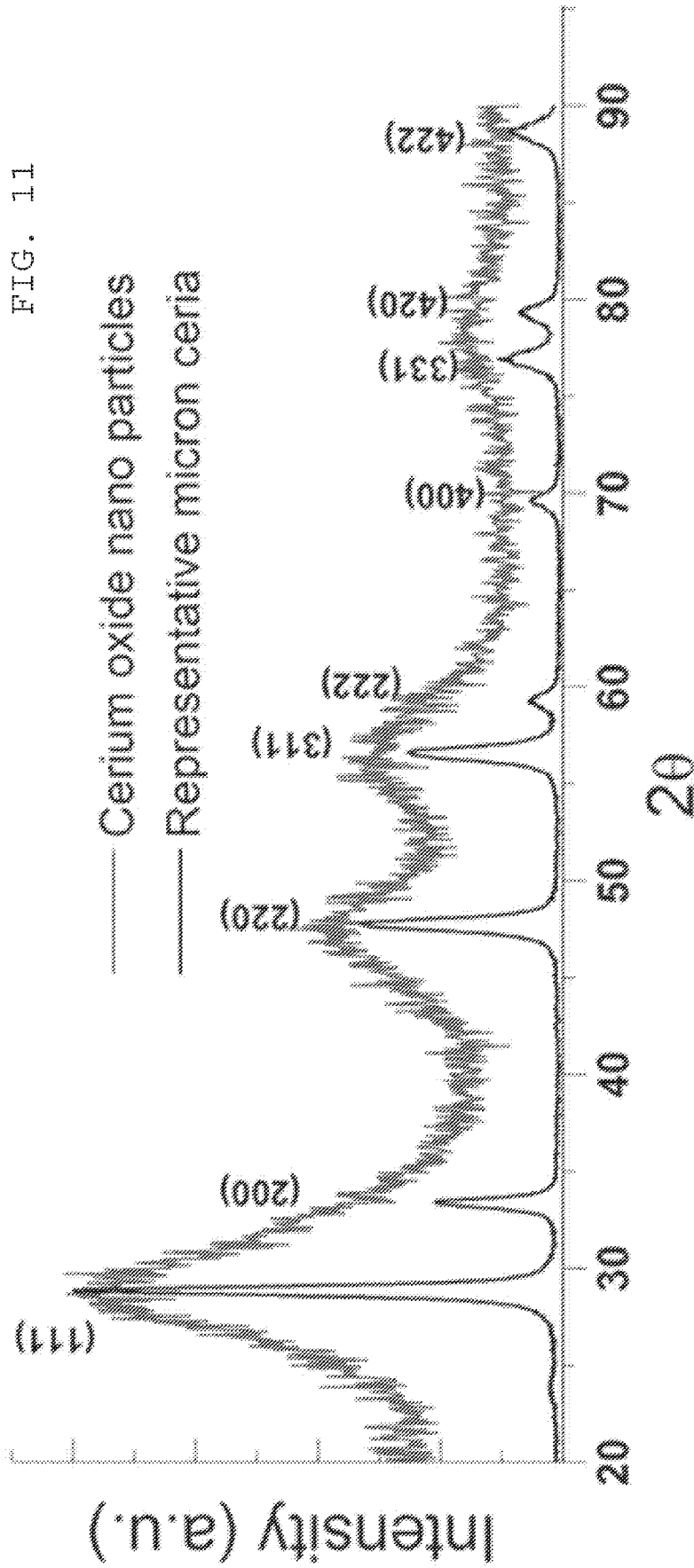
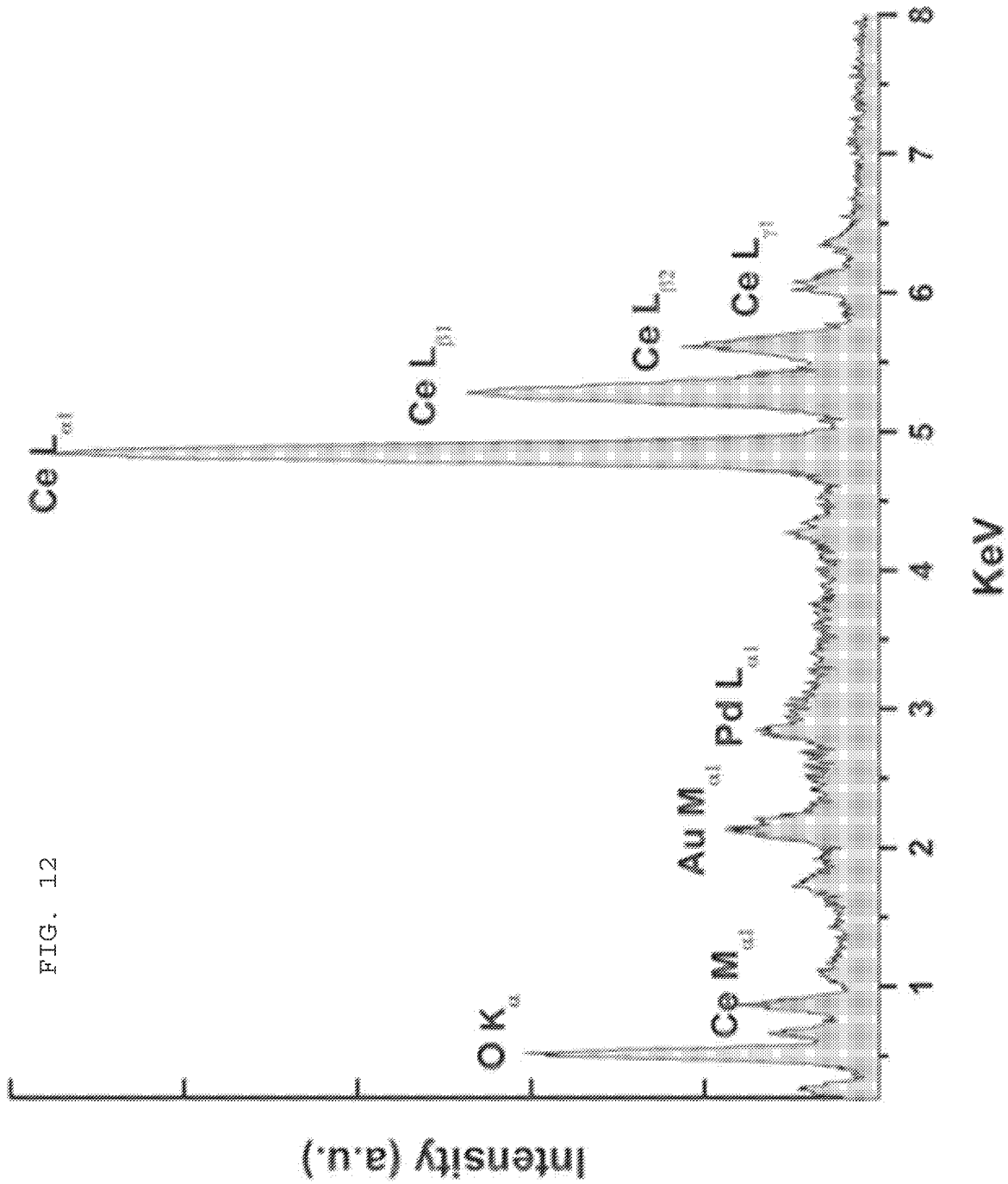


FIG. 10





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**NANOPARTICLES OF CERIUM OXIDE
TARGETED TO AN AMYLOID-BETA
ANTIGEN OF ALZHEIMER'S DISEASE AND
ASSOCIATED METHODS**

RELATED APPLICATION

This application claims priority from copending provisional application Ser. No. 61/383,773, which was filed on 17 Sep. 2010, and which is incorporated herein by reference in its entirety.

STATEMENT OF GOVERNMENT RIGHTS

The invention claimed herein was made with at least partial support from the U.S. Government. Accordingly, the government may have certain rights in the invention, as specified by law.

FIELD OF THE INVENTION

The present invention relates to the field of neurological diseases and, more particularly, to a cerium oxide nanoparticulate composition useful in treatment of Alzheimer's disease.

BACKGROUND OF THE INVENTION

Current therapies for Alzheimer disease (AD) provide moderate symptomatic delay at various stages of the disease, but do not arrest the disease progression, and hence, new approaches to the disease management are urgently needed.

In recent years, cerium oxide nanoparticles have been studied as possible potent antioxidant agents that might be able to exert neuroprotective effects. We herein disclose the specific design of a targeted nanoceria-based formulation suitable for AD therapy. The test results obtained indicate the present composition is useful for selective delivery of immunonanoparticles to A β (amyloid-beta) plaques with concomitant rescue of neuronal survival and neurite dystrophy. The formulation appears to work by regulating the expression of the BDNF signal transduction pathway.

Oxidative stress and amyloid-beta (A β) are considered major etiological and pathological factors initiating and promoting neurodegeneration in Alzheimer's disease (AD) due to the production of free radicals (1-6). To date, use of multiple doses of antioxidants has met with only limited success in abolishing these pathological conditions (7).

Recently, we have discovered that cerium oxide nanoparticles (CNPs) are redox active and biocompatible with both superoxide dismutase (8) and catalase mimetic activity (9). Among the lanthanide series of elements, cerium is distinctive in that it has two partially filled subshells of electrons, 4f and 5d, with many excited substates, resulting in a valence structure that undergoes significant alterations depending on the chemical environment (10-13). A predominant +3 oxidation state on the surface of CNPs is responsible for the nanoparticles' unique antioxidant properties (14, 15). We have shown that a single dose of CNPs prevents retinal degeneration induced by peroxides (16). In vitro, one low dose maintained radical scavenging and protective effects for long durations and multiple insults, suggesting the possibility of its regenerative activity. Therefore, CNPs have been investigated as possible nanopharmacological composition for use against diseases associated with oxidative stress (17-22).

Previously, on an AD human in vitro model, we have confirmed the anti-oxidant properties of CNPs. We have also

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demonstrated that CNPs do not act as mere anti-oxidant agents, but that they seem regulate signal transduction pathways involved in neuroprotection (23). To date, no early biomarkers for AD have been identified, therefore the appearance of symptoms is indicative of the full-blown disease.

The present disclosure concerns a novel approach wherein a CNP formulation comprises specifically targeted nanoparticles able to direct only to such targets as the brain areas of neurodegeneration and to exert specific effects counteracting neurite dystrophy and inhibiting disease progression. The presently disclosed composition is active at significantly lower dosages and in a single administration as opposed to free nanoparticles. This improvement was achieved by the synthesis of CNPs through the development of an improved method for the conjugation of anti-amyloid β antibodies to the nanoparticles with selective delivery to A β plaques and a concomitant increase of neuronal survival.

SUMMARY OF THE INVENTION

With the foregoing in mind, the present invention advantageously provides a composition of polyethylene glycol (PEG) coated nanoparticles of Cerium oxide having an antibody bound thereto, the antibody being specific for an antigen associated with a predetermined disease condition. Preferably, the nanoparticles are amine functionalized prior to coating, so as to promote coating by the PEG. In a preferred embodiment of the invention, the antibody is specifically targeted against an amyloid-beta antigen associated with a neurodegenerative disease. The nanoparticles are approximately from 3-5 nm in size prior to coating with PEG. The composition may be contained in a manufactured medication biologically acceptable for administration to a patient exhibiting symptoms of the predetermined disease. Accordingly, a method of treatment for the predetermined disease condition includes administration of the composition to a patient in need thereof.

More specifically, the present invention provides for a composition specifically targeted to a neurodegenerative disease, said composition comprising amine functionalized nanoparticles of Cerium oxide coated with polyethylene glycol and bearing an antibody specific for an antigen associated with the neurodegenerative disease. As noted above, this composition may also be contained in a manufactured medication biologically acceptable for administration to a patient exhibiting symptoms of the neurodegenerative disease. Included in this preferred embodiment of the invention is a method of treatment for a neurodegenerative disease, the method comprising administering this variation of the composition to a patient in need thereof.

A more specific yet embodiment of the present invention includes a composition immunologically targeted to Alzheimer's disease (AD), the composition comprising amine functionalized nanoparticles of Cerium oxide coated with polyethylene glycol and bearing an antibody specific for an amyloid-beta antigen associated with AD. This composition may be contained in a manufactured medication biologically acceptable for administration to a patient suffering from AD. This particular embodiment also includes a method of treatment for Alzheimer's disease, the method comprising administering the composition to a patient suffering from AD.

BRIEF DESCRIPTION OF THE DRAWINGS

Some of the features, advantages, and benefits of the present invention having been stated, others will become apparent as the description proceeds when taken in conjunc-

tion with the accompanying drawings, presented for solely for exemplary purposes and not with intent to limit the invention thereto, and in which:

FIG. 1 presents the characterization of nanoceria: (A) HRTEM image of microemulsion nanoparticles showing control particle size distribution (3-5 nm) consistent to our group's well established synthesis procedure (42). The large d spaced planes (111) primarily easily focused at 300 kV is indicated in micrographs. Smaller d spacing planes (220,311) are not marked for clear representation of micrographs. The inset shows the selected area electron diffraction pattern of nanoparticle captured at low magnification confirming the crystalline nature and fluorite structure of CNPs by calculation of each diffraction ring diameter ($L\lambda=RD$). (B) The amine functionalization of CNPs was confirmed by XPS. In the XPS two O (1s) peak corresponding two different valance state of ceria (Ce^{3+} corresponds to 531.5 eV and Ce^{4+} corresponds to 530.6 eV) and other two confirms the functionalization. Peak 1 is O—C bond that connects epichlorohydrin to the cerium oxide (534.00 eV) and peak 2 is epichlorohydrin's epoxy group (533.35 eV). (C) Shows change in the appearance of CNPs (yellow) after amine functionalization (light yellow) and PEG-conjugation (dark brown); (D) UV-VIS absorbance of ceria, NH_2 -functionalized ceria and PEG coated CNPs, showing the shift in the absorbance maximum to red and blue shift after amine functionalization (38.45 nm) and PEG-conjugation (33.41 nm) (E) FTIR spectra of PEG conjugated cerium oxide nanoparticle confirming presence of PEG on CNPs; (F) SOD mimetic activity of PEG-CNPs as compared to control, showing that surface PEG-CNPs is still active and scavenges the radical efficiently.

FIG. 2: SMFS measurements of $A\beta$ -protein with bare CNP in aqueous medium; deflection-extension spectrum (A) and corresponding force-extension of $A\beta$ with silicon substrate (B), interaction force of $A\beta$ with bare ceria nanoparticle (C), amine functionalized CNPs (D), PEG-conjugated CNPs (E), Force histogram of $A\beta$ with bare CNPs (F) and amine functionalized GNP (G). Multiple SMFS were conducted for force and histogram on each sample. The total number of force and length values analyzed were $n=204$ (for F) and $n=320$ (for G).

FIG. 3 Plaque presence is evaluated by ThT staining in control (B), $A\beta$ treated (E) cells and $A\beta$ -CNP-Ab (H). The ability of the conjugate to recognize the plaque is evaluated by TRITC labeled anti rabbit secondary antibody in control (C), $A\beta$ -treated (F) cells and $A\beta$ -CNP-Ab-treated cells (I). The ability of CNP-Ab to target only the plaque is shown in L, that is the merge of H and I. The nuclei are stained with DAPI in control (A), $A\beta$ treated (D) cells and $A\beta$ -CNP-Ab-treated cells (G). Bar=17 nm.

FIG. 4 Panel A shows cell viability evaluated by MTS assay, in control (CTR), $A\beta$ treated ($A\beta$) cells and $A\beta$ -CNP-Ab-treated cells. Data are means \pm SE, $N=6$, $p=0.025$, $*p\leq 0.05$; *, expressed vs control value. Panel B shows apoptotic cell death, evaluated as nucleosome concentration in control (CTR), $A\beta$ treated ($A\beta$) cells and $A\beta$ -CNP-Ab-treated cells. Data are means \pm SE, $N=3$, $p=0.001$, $**p\leq 0.005$ *, expressed vs control value. Panel C shows cell death, evaluated by DAPI nuclear staining and by counting condensed nuclei in control, $A\beta$ treated cells and $A\beta$ -CNP-Ab-treated cells. Data are means \pm SE, $N=3$, $p=0.03$, $*p\leq 0.05$; *, expressed vs control value. Bar=17 μ m. Panel D: Phase-contrast microscopy in control (CTR), $A\beta$ treated ($A\beta$) cells and $A\beta$ -CNP-Ab-treated cells. Bar 17 nm; On the left the neurite number in control, $A\beta$ treated cells and $A\beta$ -CNP-Ab treated cells is reported. Histograms report n° -neurites/ n° -cells. Data are means \pm SE, $N=3$, $p=0.024$, $*p\leq 0.05$. On the

right the neuritic length in control, $A\beta$ treated cells and $A\beta$ -CNP-Ab-treated cells. The neurite length was determined as neurite length/ \emptyset soma. Data are means \pm SE, $N=4$, $p=0.000$, $***p\leq 0.0005$. *, expressed vs control value.

FIG. 5 Subcellular localization of the neuronal differentiation markers β -tubulin III (β -TubIII) (green) and PPAR β/δ (red) in control (A, B; C), $A\beta$ -treated (D, E, F) cells and $A\beta$ -CNP-Ab (G, H, I) treated cells. In C, F and I the merged images are shown. Bar=17 nm. In the bottom western blotting and densitometric analyses for PPAR β/δ in control (CTR), $A\beta$ -treated ($A\beta$) cells and $A\beta$ -CNP-Ab-treated cells. Band relative densities were determined against most evident band of PVDF membrane Comassie Blu stained. Data are means \pm SE, $N=3$, $p=0.009$, $*p\leq 0.05$. *, calculated vs control value.

FIG. 6 The upper panels show immunofluorescence analysis for NF-H 200 in control (A, D), $A\beta$ -treated (B, E) cells and $A\beta$ -CNP-Ab (C, F) treated cells. D, E, and F are higher magnification pictures. Bar=17 μ m. Nuclei were stained with DAPI. Panels below show immunofluorescence analysis for GAP43 in control (G, L), $A\beta$ -treated (H, M) cells and $A\beta$ -CNP-Ab (I, N) treated cells. L, M, and N are higher magnification pictures. Bar=17 μ m. Nuclei were stained with DAPI.

FIG. 7 Panel A shows western blotting and densitometric analyses for TrkB, P75NTR and cytoplasmic pro-BDNF, in control (CTR), $A\beta$ -treated ($A\beta$) cells and $A\beta$ -CNP-Ab-treated cells. Band relative densities, were determined against most evident band of PVDF membrane Comassie Blu stained. Data are means \pm SE, $N=3$, for TrkB $p=0.04$, $*p\leq 0.05$. For P75NTR $p=0.004$, $**p\leq 0.005$; For pro-BDNF $p=0.005$, $**p\leq 0.005$. The * is calculated vs control (CTR) value. Panel B shows western blotting and densitometric analyses for extracellular and soluble pro-BDNF form assayed by immunoprecipitating the culture media from control, $A\beta$ -treated and $A\beta$ -CNP-Ab-treated cells. The immunoprecipitation assay was performed allowing the collected media to be absorbed on Protein A Sepharose A CL-4B followed by a precipitation step with a specific anti-BDNF antibody. Band relative densities were determined using TotalLab software (ABEL Science-Ware srl, Italy) and values were given as % over control. Data are means \pm SE, $N=3$, $p=0.009$, $*p\leq 0.05$ * is calculated vs control value. Panel C shows western blotting and densitometric analyses for p-ERK1,2 and p-ERK5, in control, $A\beta$ -treated cells and $A\beta$ -CNP-Ab-treated cells. Band relative densities, were determined against most evident band of PVDF membrane Comassie Blu stained. Data are means \pm SE, $N=3$, for p-ERK1: $A\beta$ vs CTR $p=0.004$, $**p\leq 0.005$; $A\beta$ -CNP-Ab vs CTR $p=0.001$, $**p\leq 0.005$. For p-ERK2: $A\beta$ vs CTR $p=0.001$, $**p\leq 0.005$. $A\beta$ -CNP-Ab vs CTR $p=0.016$, $*p\leq 0.05$. For p-ERK5: $A\beta$ vs CTR $p=0.012$, $*p\leq 0.05$; $A\beta$ -CNP-Ab vs CTR $p=0.000$, $***p\leq 0.0005$. * is calculated vs control value.

FIG. 8 shows the diffraction pattern of nanoceria showing typical peak broadening indicative of nanocrystalline particles.

FIG. 9 depicts the results of Energy dispersive X-ray spectroscopy illustrating the elemental composition which confirms that CNPs are essentially free of impurities.

FIG. 10 portrays the conjugation of Anti- β -amyloid antibody with NH_2 terminal PEG CNP.

FIG. 11 shows the ligation of the specific antibody against $A\beta$ to the nanoparticles allows the CNPs-Ab to specifically recognize the plaque, having minimum or no interaction with nearby neuronal cells. This notion is supported by the effects observed when the same antibody, utilized for the ligation, is

utilized alone to treat the cells after the A β challenge; in fact, it identifies the plaque (A, B, C) but having minimum or no effect of cell viability (D).

FIG. 12 presents preliminary experimental results showing the effects on cell viability of PEG-CNP or NH₂-CNP administered alone or after A-beta challenge indicated that PEG-CNP are more effective than NH₂-CNP in promoting neuronal survival. Nevertheless CNPs-PEG-Ab were found to be more effective as compared to PEG-CNP.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

The present invention will now be described more fully hereinafter with reference to the accompanying drawings, in which preferred embodiments of the invention are shown.

Unless otherwise defined, all technical and scientific terms used herein are intended to have the same meaning as commonly understood in the art to which this invention pertains and at the time of its filing. Although various methods and materials similar or equivalent to those described herein can be used in the practice or testing of the present invention, suitable methods and materials are described below. However, the skilled should understand that the methods and materials used and described are examples and may not be the only ones suitable for use in the invention.

Moreover, it should also be understood that any temperature, weight, volume, time interval, pH, salinity, molarity or molality, range, concentration and any other measurements, quantities or numerical expressions given herein are intended to be approximate and not exact or critical figures unless expressly stated to the contrary. Accordingly, where appropriate to the invention and as understood by those of skill in the art, it is proper to describe the various aspects of the invention using approximate or relative terms and terms of degree commonly employed in patent applications, such as: so dimensioned, about, approximately, substantially, essentially, consisting essentially of, comprising, and effective amount.

Further, any publications, patent applications, patents, and other references mentioned herein are incorporated by reference in their entirety as if they were part of this specification. However, in case of conflict, the present specification, including any definitions, will control. In addition, the materials, methods and examples given are illustrative in nature only and not intended to be limiting.

Accordingly, this invention may be embodied in many different forms and should not be construed as limited to the illustrated embodiments set forth herein. Rather, these illustrated embodiments are provided so that this disclosure will be thorough, complete, and will fully convey the scope of the invention to those skilled in the art. Other features and advantages of the invention will be apparent from the following detailed description, and from the claims.

Methods

Synthesis and characterization of CNPs CNPs of approximate size of 3-5 nm were synthesized by a microemulsion method describe elsewhere (36). After preparation, the particles were washed with acetone and water for six to eight times to remove the surfactant and other impurities. High resolution transmission electron microscopy (HRTEM), with FEI Tecnai F30 having an energy dispersive X-ray (EDX) analyzer, was carried out to study the size and morphology of the nanoparticles.

Amine Functionalization of CNPs

Prepared CNPs were suspended in 0.1 M NaOH solution and stirred for 5 minutes. Five milliliters of distilled epichlo-

rohydrin and 0.5 mL of 2 M NaOH were added and stirred at room temperature. The nanoparticles were then recovered by centrifugation and washed with water several times. Next, the nanoparticles were suspended in water and 30% ammonium hydroxide solution was added and stirred for several hours. Finally, the resulting amine functionalized nanoparticles were recovered by centrifugation, washed with water (three to four times), and dried (37).

A 5400 PHI ESCA (XPS) spectrometer was used to obtain XPS data to confirm the amine functionalization. The base pressure during XPS analysis was 10-10 Torr and Mg—K α X-radiation (1253.6 eV) at a power of 350 watts was used.

Preparation of PEG-CNPs

Polyethylene glycol (PEG) spacers with carboxy and amine terminals and having a spacer arm of 18.1 Å were selected for the study. We chose bi-functional PEG, so that one end can connect to an amine functionalized nanoparticle and the other end to the antibody. The carboxy terminal of the bi-functionalized PEG molecule was coupled to the amine functionalized CNPs using EDC and Sulfo NHS coupling chemistry. 1 mg/ml CA(PEG)₄ was dissolved in 0.05M NaCl, pH 6 buffer. 2 mM EDC and 5 mM Sulfo-NHS were added to the CA(PEG)₄ solution and stirred at room temperature. Amine functionalized CNPs were resuspended in sodium phosphate buffer, added to the reaction mixture and stirred. The molar ratio of amine functionalized ceria:CA(PEG)₄ was 1:4, used for the reaction. PEG-CNPs were recovered by centrifugation, washed with water (three to four times), and dried. UV-Visible spectroscopy and Fourier transform infrared (FTIR) spectra were obtained to confirm the PEG molecule on the nanoparticle surface using PerkinElmer Lamda750S and PerkinElmer Spectrum, respectively. Super-oxide dismutase (SOD) mimetic activity of the PEG-conjugated CNP was estimated using SOD Assay kit (Sigma-Aldrich Corp., St. Louis, Mo., USA) according to the manufacturer instructions.

Conjugation of A β Antibody with PEG-CNP

In the first step, sodium azide and other salt were removed from the anti A β antibody by centrifuging through 10 kD cut-off Centricon® (Millipore Inc.). The antibody (1 mg/ml concentration) was diluted in NaCl, pH 6 buffer. 2 mM EDC and 5 mM Sulfo-NHS were added to the antibody solution and stirred at room temperature. PEG-CNPs were resuspended in sodium phosphate buffer, added to the reaction mixture and stirred. The molar ratio of amine functionalized antibody to PEG-CNPs used for the reaction was about 1:5. PEG-ceria nanoparticles were recovered by centrifugation, washed with water (three to four times), and re-suspended in distilled water. The concentration of ceria after antibody conjugation was assayed by UV-Visible spectroscopy. Bradford assays were performed to confirm antibody conjugation to the PEG-ceria nanoparticle.

Cell Cultures

SH-SY5Y cells (ATCC) were seeded at about 1×10^4 cells/cm² and cultured for 7 divisions (DIV) in FBS-free RPMI 1640 differentiating medium containing N2 supplement in order to promote neuronal differentiation.

A β Fibril Formation

A β (25-35) is frequently used in investigating A β properties as a less expensive and more easily handled substitute for the native full-length peptide, A β (1-42). Indeed, A β (25-35) mimics the toxicological and aggregation properties of the full-length peptide, though these characteristics are enhanced; i.e., the shorter peptide is more toxic to cultured neurons, exhibits earlier toxicity, causes more severe membrane protein oxidation, and aggregates faster than the native A β (1-42) (38).

The amyloid fibrils were obtained as previously described (39). Specifically, the A β (25-35) stock solution (500 μ M) was prepared dissolving A β in FBS-free differentiating medium containing N2 supplement (pH 7.4) and stored at -20° C. The amyloid fibrils were obtained incubating A β (25-35) stock solution at 37° C. for 8 days.

Fluorimetric Assay

The amyloid polymerization status was checked by the thioflavin T (ThT) fluorescence method before each treatment (40). ThT binds specifically to amyloid fibrils, and such binding produces a shift in its emission spectrum and an increase in the fluorescent signal, which is proportional to the amount of amyloid formed (41-43). Following incubation, A β in 20 mM Tris HCl Buffer, pH 8.0, and 1.5 μ M ThT in a final volume of 2 ml were analyzed. Fluorescence was monitored by spectrofluorimetry at an excitation wavelength of 450 nm and an emission wavelength of 485 nm, as previously described (41).

Treatments

Differentiated cells were treated with A β 25-35 (12.5 μ M, f.c.) for 24 h. For nanoparticles treatment, cells were subjected for 4 h to acute challenge with A β 25-35, and were treated with an effective dose (200 nM, f.c.) of cerium oxide nanoparticles conjugated to anti-A β antibody (CNPs-Ab).

A β Plaque Detection

In order to assess if the ligation of antibody to the nanoparticles allows them to bind specifically to A β plaques, double immunofluorescence staining was performed. Briefly, cells, grown on coverslips, were fixed in 4% paraformaldehyde in PBS for 10 min at RT. Cells were then incubated with 0.05% solution of ThT and Tritc-labeled anti-rabbit IgG secondary antibody (1:100), for 20 min at RT. Nuclei were counterstained with DAPI (300 ng/ml). After extensive washings, coverslips were mounted with Vectashield mounting medium and photographed in a fluorescence microscope (AXIOPHOT, Zeiss).

Cell Viability and Death

Cells, plated in 24 multiwell plates, were incubated after treatments for 2 h with CellTiter 96 Aqueous One Solution, a metric viability test method based on 3-(4,5-dimethylthiazol-2-yl)-5-(3-carboxymethoxyphenyl)-2-(4-sulfophenyl)-2H-tetrazolium (MTS). The quantity of formazan formed, as a function of viability, was measured at 490 nm using an ELISA plate reader. All MTS assays were performed in triplicate.

After A β exposure, cells on coverslips were fixed in 4% paraformaldehyde at room temperature for 10 min, then stained with DAPI (300 ng/ml) for 20 min and examined under UV illumination using a fluorescence microscope. To quantify the apoptotic process, nuclei with both fragmented or condensed DNA and normal DNA were counted. Five fields/coverslips were counted. Data, from 3 different experiments, are expressed as a percentage of the total cells counted. For apoptosis detection, cells were seeded in 24-well plates at a density of 1×10^4 cells/cm 2 . Control and treated cells were analyzed for apoptosis using the cell death detection ELISA kit for the nucleosome detection. Absorbances at 405 nm with respect to 490 nm were recorded according to manufacturer's directions.

Morphometry

Control and treated cells, grown on coverslips, were fixed in 4% paraformaldehyde in PBS for 20 min at RT. After washings, coverslips were mounted with Vectashield $\text{\textcircled{R}}$ and phase-contrast observations were performed by an AXIOPHOT Zeiss microscope, equipped with a micrometric ocular lens. The processes longer than the cell body mean diameter (\emptyset), which should be regarded as neurites, were counted and

the results were expressed as neurite number vs. the total cell number. The neurite length was determined by comparing the neurite length with the mean diameter (\emptyset) of cell soma and reported as neurite length/soma (\emptyset).

Immunofluorescence

Control and treated cells, grown on coverslips, were fixed in 4% paraformaldehyde in PBS for 20 min at RT and permeabilized in PBS containing 0.1% Triton X-100 for 5 min at RT. Cells were then incubated with mouse anti- β -tubulin III (1:300) and anti PPAR β (1:100) diluted in PBS containing 3% BSA overnight at 4° C. The immunolocalization of GAP-43 and heavy neurofilament (NF-H) was performed by permeabilizing the fixed cells with absolute methanol for 10 min at -20° C. After that, cells were rehydrated with PBS for 5 min and incubated with anti-GAP 43 (1:300) and anti-NF-H, (1:200) antibodies, overnight at 4° C. After extensive washings with PBS, cells were treated with fluorescein-labeled anti-mouse or Tritc-labeled anti-rabbit IgG secondary antibodies (1:100 in PBS containing 3% BSA) for 30 min at RT. Nuclei were counterstained with DAPI (300 ng/ml). After extensive washings, coverslips were mounted with Vectashield mounting medium and photographed in a fluorescence microscope (AXIOPHOT, Zeiss).

Western Blot

Cells were washed in ice-cold PBS and homogenized in ice-cold RIPA buffer (10 mM Hepes, pH7.4, 10 mM KCl, 1.5 mM MgCl $_2$, 1 mM EDTA, 1 mM dithiothreitol) with a protease inhibitor mixture (100 mg/ml phenylmethylsulfonyl fluoride, 2 mg/ml aprotinin, 2 mM leupeptin, and 1 mg/ml pepstatin). The lysate was subjected to centrifugation at 600 \times g for 30 min at 4° C., and the supernatant was collected. Samples (25-50 μ g/lane) were analyzed by 10% SDS-PAGE, transferred to PVDF membranes, and blocked in Tris-buffered saline containing 5% non fat milk, and 0.1% Tween20 $\text{\textcircled{R}}$. Membranes were incubated with different primary antibodies, anti-PPAR β (1:1000), anti-BDNF (1:200), anti TrkB (1:200) anti p-75 NTR (1:100), anti p-ERK1,2 (1:200), anti-ERK1,2 (1:1000), anti-p-ERK5 (1:200) overnight at 4° C. and then probed with horseradish peroxidase-conjugated mouse or rabbit secondary antibodies (1:1000). Immunoreactive bands were visualized by chemiluminescence. Band relative densities, against most evident band of PVDF membrane Comassie Blu stained, were determined using TotalLab $\text{\textcircled{R}}$ software (ABEL Science-Ware srl, Italy) and values were given as relative units.

Immunoprecipitation Assay

The immunoprecipitation assay was performed to estimate the amount of brain-derived neurotrophic factor (BDNF) protein in the culture media obtained from control and treated cells. To immunoprecipitate BDNF, a solution of 100 μ g Protein A Sepharose A CL-4B was added to an equal amount (1000 μ g of total protein) of supernatant samples collected from each condition. The suspension obtained was allowed to shake for 2 h at 4° C. and incubated with 5 μ g of anti-BDNF primary antibody overnight at 4° C. The immunoprecipitates were then collected by centrifugation and the supernatant aspirated and discarded. Resuspended pellets were subjected to 15% SDS-PAGE, transferred to PVDF membranes and probed with specific anti BDNF antibody. After incubation with horseradish peroxidase-conjugated rabbit secondary antibodies (1:1000), the immunoreactive bands were visualized by chemiluminescence. Band relative densities were determined using TotalLab $\text{\textcircled{R}}$ software (ABEL Science-Ware srl, Italy) and values were given as percentage over control.

Statistics

Experiments were performed at least in triplicate. Data were represented as means \pm Standard Errors. Where appro-

appropriate, one-way ANOVA test followed by Scheffe's post hoc test analysis was performed using SPSS software. P values less than 0.05 were considered statistically significant.

Results

Functionalization and Characterization of CNPs

FIG. 1 shows the characterization of synthesized CNPs. In FIG. 1(A) depicts a TEM image showing well dispersed nanoparticle with a size distribution ranging approximately between 3-5 nm, (inset: X-ray diffraction pattern). The diffraction pattern showed typical peak broadening indicative of nanocrystalline particles (Suppl materials, Figure S1). X-ray spectroscopy illustrates the elemental composition which confirms that CNPs are free from any impurities (Suppl materials, Figure S2). FIG. 1B represents the high resolution XPS spectra of amine functionalized CNP, showing the evidence of complex formation. Peak 1 shows an O—C bond and represents the epichlorohydrin molecule attachment to the nanoparticle (534.00 eV) and peak 2 corresponds to epichlorohydrin's epoxy group (533.35 eV). The other two peaks are due to the presence of mixed valence state of cerium atom (Ce+3: 531.5 eV, Ce+4: 530.6 eV). FIG. 1C shows the change in the color of CNPs (dark yellow) after amine functionalization (light yellow) and PEG-conjugation (brown). Panel D presents the UV-Visible spectroscopy data showing a shift in the absorption spectrum of CNP following functionalization with NH₂ (38.45 nm) and PEG (33.41 nm). The FTIR spectra (Panel E) of PEG-CNP, confirming the PEG conjugation; SOD mimetic activity of PEG coated CNP is presented in Panel F.

The conjugation of Anti- β -amyloid antibody with NH₂ terminal PEG CNP is illustrated in scheme (Suppl materials Fig S3). The anti β antibody was attached to the PEG-CNP using EDC/Sulfo NHS coupling reaction; the table shows the amount of antibody (μ g/ml) in 5 mM PEG-CNP and CNP-NH₂ estimated by Bradford assay.

Single Molecular Force Spectroscopy of CNPs

We selected β 1-42 as a model protein to find out the interaction of the protein with bare and functionalized CNPs. FIG. 2 shows the single molecular force microscopy (SMFS) measurements carried out using a Succinimide functionalized Silicone nitride AFM tip (spring constant 0.01 N/m and tip radius of curvature 10 nm) coated with AF protein with bare CNPs. The figure shows the deflection-extension spectrum (A) and the corresponding force-extension (B) of β with silicon. FIGS. (C), (D) and (E) show the interaction of β with bare, NH₂ and PEG functionalized CNPs, respectively. Attraction force of interaction was found in case of bare CNPs with the β protein. The force histogram of β with CNPs shows that the force of the interaction is in the range of 10-250pN (204 force curve analyzed) (F). The interaction force of β is found to be higher with amine functionalized nanoparticles (2D) and force histogram shows (2G) that the amount of interaction is in the range of 250pN-500pN (320 force curve analyzed), greater than the bare CNPs, which indicates increased non specific interaction to the protein. Interestingly, minimum or no interaction has been observed with PEG-CNPs (2E). The interaction force is in the order: NH₂-CNP>Bare CNP>PEG-CNP. This is explained in terms of zeta potential of the bare and functionalized nanoparticle. As the zeta potential is changed from positive to negative (NH₂-CNP (+16 mV)<Bare CNPs (-10 mV)<PEG-CNP (-37 mV)), it minimizes the interaction with the partially negatively charged C-terminal part of the β -amyloid protein and the CNPs. Schematic diagram of CNP interaction with AFM probe functionalized with β protein is consistent with our earlier studies dealing with transferrin conjugated CNPs (24). It is noteworthy that the SMFM data suggested that

PEG attachment with CNPs decreases the nonspecific interaction and its importance is discussed later.

CNPs-Ab Targeting Plaques

In FIG. 3 while control cells are negative to the thioflavine T staining (B), the green fluorescence shows the presence of β plaque in β -treated cells with (H) or without nanoparticles (E). The nuclei, stained with DAPI (D, G), show cell aggregation in the areas closed to the β plaque, while control cells appear dispersed (A). In the same figure the ability of CNPs-Ab to bind the β plaques is assessed by double immunostaining of thT and anti-rabbit Tritic-labeled secondary antibody (C, F, I L merge) which specifically recognizes the antibody bound to the nanoparticles. Tritic-antibody labels only cells treated with both β plaque and CNP-Ab (I, L merge) not the control (C) and β -treated (F) cells. Therefore, the ligation of the specific antibody against β to the nanoparticles allows the CNPs-Ab to specifically recognize the plaque, having minimum or no interaction with nearby neuronal cells. This is supported by the effects observed when the same antibody used in the ligation is utilized alone to treat the cells after the β challenge (Suppl materials, Fig. S4); in fact, it identifies the plaque (A, B, C) but having minimum or no effect on cell viability (D).

Cell Viability and Death

Preliminary experiments (Suppl materials, Fig S5) the effects on cell viability of PEG-CNP or NH₂-CNP administered alone or after β challenge indicated that PEG-CNP are more effective than NH₂-CNP in promoting neuronal survival due to the decrease in non-specific interaction in PEG CNP. CNPs-PEG-Ab were found to be more effective as compared to PEG-CNP. Therefore, in all subsequent experiments only the PEG-CNPs-Ab (CNPs-Ab) were used. Cell viability, evaluated by MTS assay, in control and treated cells is shown in FIG. 4, panel A. β treatment leads to significant reduction in cell viability. CNPs-Ab revert this effect to the control values. In the same figure (panel B) apoptotic cell death, evaluated as nucleosome concentration, is shown. β treatment induces a significant increase in apoptotic cell death, while after CNPs-Ab treatment no significant differences are observed with respect to the control. Panel C shows the nuclear fragmentation in control and treated cells, evaluated by DAPI nuclear staining. Consistently with the apoptotic assay, β treatment leads to an increase in apoptotic nuclei, while CNPs-Ab almost restores the control condition. These results, taken together, indicate that the CNPs-Ab play a protective effect against the β cytotoxic insult.

Cell Morphology

FIG. 4, panel D, shows the contrast phase microscopy and the graphic representation of neurite length and number in control and treated cells. Control cells (CTR) show an evident neuronal clustering and neuronal aggregation, β treatment induced an evident neurite loss (β). CNPs-Ab protects cells from neurite atrophy (β -CNP-Ab). The graphical representation of number of neurite (left side), and of neurite length (right side) shows that β treatment significantly decreases neurite number and also the neurite length, while CNPs-Ab protect the neurites from β -mediated neuronal damage.

Immunofluorescence

Since we have previously demonstrated that β treatment affected the expression of peroxisome proliferator activated receptor β (PPAR β), which is a transcription factor in neuronal differentiation (25), and in neuronal maturation (26-27), in the following experiments we analyzed the cytoskeletal organization and the PPAR β / δ expression and localization in control and treated cells. In FIG. 5, double immunostaining for 13-tubulin III, a marker of early neuronal differentiation and PPAR β / δ is shown. In control cells, β -tu-

bulin III (CTR) localizes at cytoplasmic and neurite level, while PPAR β/δ is mainly localized to the nuclei (CTR, merge). After A β treatment the neurite network is no more evident (A β) and the PPAR β/δ is mainly localized to the cytoplasm (A β merge).

In the β -treated cells following CNPs-Ab an evident preservation of neurite network (A β -CNP-Ab merge) as well as of the PPAR β/δ nuclear localization is observed (A β -CNP-Ab merge), thus indicating protection of neurites by nanoceria. Regarding PPAR β/δ protein levels, A β treatment significantly downregulates the protein, while CNPs-Ab revert PPAR β/δ protein levels to the control (FIG. 5 bottom).

In FIG. 6 the heavy neurofilament 200 (NF-H) and GAP-43 localization in control and treated cells is shown. NF-H is a marker of neuronal terminal maturation, while GAP-43 is an axonal marker. In control cells a wide neuronal network is observed (A and D, G and L), while in A β -treated cells the network is completely lost (B and E, H and M). After CNPs-Ab treatment an evident preservation of the neurites is observed (C and F, I and N), thus confirming the neuroprotective effects by the presently disclosed nanoceria composition in counteracting neuronal dystrophy.

Signal Transduction Pathways

Finally, since neuronal morphology and plasticity are correlated to the brain derived neurotrophic factor (BDNF) signal transduction pathway, we assayed the BDNF, its receptors such as TrkB and p75, and the extracellular signal regulated kinases such as ERK1,2 and ERK5. Upon A β challenge, the cytoplasmic levels of BDNF immature form (pro-BDNF) show to be upregulated (FIG. 7 panel B); The same results are obtained by the immunoprecipitation assay of the culture media (FIG. 7 panel B), indicating that A β injury leads to a strong accumulation of pro-BDNF in the extracellular matrix. This significant increase in pro-BDNF may be responsible for the promotion of the neuronal death and atrophy, as it is known that the immature form of BDNF induces neuronal apoptosis via activation of a receptor complex of p75NTR and sortilin (28). This view is supported by the results obtained for p75NTR protein in our experimental condition (FIG. 7 panel A). In fact, as for pro-BDNF, A β increases p75NTR protein levels while concomitantly triggering a decrease of the specific receptor TrkB involved in the action of mature and cleaved form of BDNF. Moreover A β induces the active form of ERK1,2 (p-ERK1,2) (FIG. 7 panel C), known to be involved in apoptosis promotion. In A β -treated cells following CNPs-Ab a reduction but not a complete reversion of pro-BDNF levels is observed, while the levels of the mature form are reverted to the control values. In the same time, CNPs-Ab, significantly increase TrkB as well as the p-ERK5, involved in neuronal survival, with concomitant decrease of ERK1,2, suggesting an activation of the neuronal survival pathway BDNF/TrkB/ERK5.

Discussion

It has been previously reported that GNPs protect neurons from free radical—mediated insult initiated by UV light, H₂O₂, irradiation, and excitotoxicity (29-30). Our previous results have documented the anti-oxidant and protective role of bare cerium oxide nanoparticle in a human AD in vitro model.

In this work we have carefully designed and formulated a targeted pegylated nanoceria-based molecule suitable as therapy for AD. Design of a specifically targeted nanoparticle avoids diffusion to other areas and in the cell cytoplasm. The conjugation of CNPs with an antibody against A β 1-42 makes possible a targeted delivery of CNPs to the A β plaques.

In this composite nanoparticle we have also used the 18.1 Å length bi-functional PEG as a spacer to conjugate anti A β

antibody with amine functionalized CNPs. The SMFP data showed that the attachment of PEG to CNPs reduces non-specific interactions with A β proteins and protects the anti-oxidant properties of the CNPs while targeting the plaques. In the presently disclosed composition PEG acts as a spacer which also provides flexibility to the conjugated antibody to interact with its ligand with minimal steric hinderance.

Moreover, PEG coating will also provide the following advantages apart from the specific targeted delivery: (i) causing high disparity of nanoparticles; (ii) protecting nanoparticles from agglomerating and being cleared out from the system, (iii) minimizing the attachment of opsonin protein and suppressing uptake by macrophages, and (iv) increasing blood circulation time (31).

The immunofluorescence results obtained indicate the specific targeting of nanoceria to A β plaques without diffusion to the cell cytoplasm. It is noteworthy that the specific formulation now proposed is effective at a significantly lower concentration than bare CNPs which may decrease the potential drug side-effects. Moreover CNPs-Ab other than exerting non-specific antioxidant effects, seem to modulate at translational level proteins crucial for the neuronal signal transduction pathway leading to survival, such as TrkB and p-ERK5, which appeared significantly upregulated, and the proapoptotic signaling proteins such as BDNF/p75/p-ERK1,2, which appeared down-regulated. Consistently with the increase of the survival and plasticity pathways, the neuronal cytoskeleton, strongly damaged by A β challenge, appeared completely preserved in A β -treated cells in presence of CNPs-Ab.

Nanoparticles have been largely employed to deliver various types of drugs ranging from coenzyme Q10 (32), to protein antigens (33), plasmid DNA (34) and several other molecules. Specific nanoparticles were demonstrated to penetrate the blood-brain barrier (BBB) without altering its permeability and to be circulating in the blood for a long time (35). However, the inventive nanoceria composition disclosed herein demonstrates the use of functionalized self targeting nanoceria bound to a specific carrier for counteracting brain pathologies characterized by oxidative stress, and has shown to be effective in counteracting disease progression by improving neuronal viability while decreasing neuronal death and neurite atrophy.

Accordingly, in the drawings and specification there have been disclosed typical preferred embodiments of the invention and although specific terms may have been employed, the terms are used in a descriptive sense only and not for purposes of limitation. The invention has been described in considerable detail with specific reference to these illustrated embodiments. It will be apparent, however, that various modifications and changes can be made within the spirit and scope of the invention as described in the foregoing specification and as defined in the appended claims.

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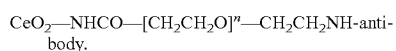
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That which is claimed:

1. A composition comprising polyethylene glycol (PEG) coated nanoparticles of Cerium oxide having an antibody bound thereto, the antibody being specific for an antigen associated with a predetermined disease condition, wherein the PEG comprises a bifunctional molecule comprising a carboxy terminal and amine terminal, the carboxy terminal being connected to an amine group on the nanoparticles and an amine terminal being connected to the antibody as follows:



2. The composition of claim 1, wherein said nanoparticles are amine functionalized to promote coating by the PEG.

3. The composition of claim 1, wherein said antibody is specifically targeted against an amyloid-beta antigen associated with a neurodegenerative disease.

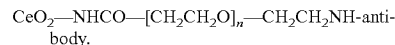
4. The composition of claim 1, wherein the nanoparticles are approximately from 3-5 nm in size prior to coating with PEG.

5. The composition of claim 1, contained in a manufactured medication biologically acceptable for administration to a patient exhibiting symptoms of the predetermined disease.

6. A composition specifically targeted to a neurodegenerative disease, said composition comprising amine functionalized nanoparticles of Cerium oxide coated with polyethylene

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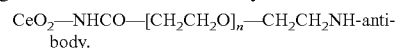
glycol and bearing an antibody specific for an antigen associated with the neurodegenerative disease; wherein the PEG comprises a bifunctional molecule comprising a carboxy terminal and amine terminal, the carboxy terminal being connected to an amine group on the nanoparticles and an amine terminal being connected to the antibody as follows:



7. The composition of claim 6, contained in a manufactured medication biologically acceptable for administration to a patient exhibiting symptoms of the neurodegenerative disease.

8. A method of treatment for a neurodegenerative disease, the method comprising administering the composition of claim 6 to a patient in need thereof.

9. A composition immunologically targeted to Alzheimer's disease (AD), said composition comprising amine functionalized nanoparticles of Cerium oxide coated with polyethylene glycol and bearing an antibody specific for an amyloid-beta antigen associated with AD, wherein the PEG comprises a bifunctional molecule comprising a carboxy terminal and amine terminal, the carboxy terminal being connected to an amine group on the nanoparticles and an amine terminal being connected to the antibody as follows:



10. The composition of claim 9, contained in a manufactured medication biologically acceptable for administration to a patient suffering from AD.

11. A method of treatment for Alzheimer's disease, the method comprising administering the composition of claim 9 to a patient suffering from AD.

* * * * *