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Huisinga, Jessie M.; Filipi, Mary; Schmid, Kendra K.; and Stergiou, Nicholas, "Is There a Relationship Between Fatigue Questionnaires and Gait Mechanics in Persons With Multiple Sclerosis?" (2011). *Journal Articles*. 103. https://digitalcommons.unomaha.edu/biomechanicsarticles/103

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Fatigue and gait mechanics in MS patients

IS THERE A RELATIONSHIP BETWEEN FATIGUE QUESTIONNAIRES AND GAIT MECHANICS IN PERSONS WITH MULTIPLE SCLEROSIS?

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Acknowledgements: Support for this work was provided by the American Society of

Biomechanics Grant-in-Aid and the Nebraska Research Initiative.

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Acknowledgements

Support for this work was provided by the American Society of Biomechanics Grant-in-Aid and the Nebraska Research Initiative.

We certify that no party having a direct interest in the results of the research supporting this article has or will confer a benefit on us or on any organization with which we are associated AND, if applicable, we certify that all financial and material support for this research (eg, NIH or NHS grants) and work are clearly identified in the title page of the manuscript.

1 Abstract

- 2 Objective: To evaluate the reported fatigue levels and gait deficits in Multiple Sclerosis (MS)
- 3 patients to determine the relationships that may exist between fatigue in MS patients and
- 4 alterations in gait mechanics.
- 5 Design: Cross-sectional
- 6 Setting: Biomechanics laboratory
- 7 Participants: Subjects with MS (n = 32) and age- and sex-matched controls (n = 30).
- 8 Interventions: None
- 9 Main Outcome Measures: Fatigue Severity Scale (FSS), Modified Fatigue Index Scale (MFIS),
- 10 and shortform SF-36 to assess fatigue and general health. Biomechanical gait analysis was
- 11 performed to measure peak joint torques and powers in the sagittal plane at the ankle, knee, and
- 12 hip. Correlations were performed between fatigue measures and degree of deficit within each MS
- 13 patient for each joint torque and power measure.
- 14 Results: FSS was significantly correlated with deficits in ankle power generation at late stance
- and walking velocity. MFIS was significantly correlated with deficits in peak knee extensor
- 16 torque and in knee power absorption at early stance. SF-36 subscales were correlated with
- 17 several of the joint torque and power variables.
- 18 Conclusions: subjective fatigue rating scales alone should not be used as an indicator of motor
- 19 disability or of disease progression as it affects the walking performance of the MS patients
- 20 Key words: joint torque, joint power, general health, neurological disease

21 Introduction

42

22 Fatigue is one of the most common symptoms of multiple sclerosis (MS). It is reported 23 by up to 90% of patients and is described as an increased weakness with exercise or as the day 24 progresses, as an abnormal constant and persistent sense of tiredness, or as fatigable weakness exacerbated by activity or heat ^{1, 23}. Measurement of fatigue in MS patients is based primarily on 25 the patient's own reports, and as a result, the measures are inherently subjective. Fatigue ratings 26 in MS patients may be affected by the individual's performance self efficacy and altered sensory 27 input during activity. Also, ratings may be affected if an observer rates the fatigue based on 28 reports of decreased effort due to impaired motor control capabilities⁴. 29 30 Because fatigue is a subjectively reported symptom, there are currently no tests or 31 objective signs allowing the clinician to quantify its severity outside of fatigue related questionnaires ⁵. Studies to investigate relationships between fatigue scores have reported weak 32 correlations and noted that fatigue is a multi-factorial symptom which may not be fully explained 33 by one fatigue scale or another^{1, 2}. Additionally, changes in fatigue ratings do not correlate with 34 35 changes in walking performance which led researchers to suggest monitoring reports of fatigue with more objective measures⁶. Lack of correlation between fatigue ratings and walking 36 performance may exist because self-reported fatigue scales rely on subjective reporting by 37 patients and therefore cannot differentiate an inability to generate or maintain voluntary force 38 from an unwillingness to do so^4 . 39 40 MS fatigue symptoms are likely due to 'central fatigue' which indicates a problem with the neural drive to sustain muscle force⁴. Neural drive is also required to facilitate walking and 41

43 patients are compared to healthy controls. This association between specific reports of fatigue

thus is feasible to expect fatigue to be reflected as alterations in walking mechanics when MS

44 and the gait mechanics of patients with MS has not previously been investigated.

The purpose of this study was to evaluate both the reported fatigue levels in MS patients 45 and these patients' deficits in gait mechanics to determine whether relationships exist between 46 fatigue in MS patients and alterations in gait mechanics. It was hypothesized that since both 47 fatigue in MS patients and neural control of gait are mediated by supraspinal and spinal inputs⁴, 48 ⁷⁻⁹, there would be a significant relationship between reported fatigue levels and the alterations in 49 50 gait mechanics of MS patients. Additionally, alterations in walking mechanics could lead to increased metabolic cost and overall greater energy expenditure during walking ^{10, 11}. Thus, 51 persons with MS who have greater alterations in walking mechanics could have greater fatigue 52 levels. In addition to fatigue measures, general health measures were also investigated and 53 54 compared to gait measures to determine whether general health perceptions of MS patients are related to gait mechanics. Because general health perceptions are likely influenced by fatigue 55 levels, it was hypothesized that general health perceptions are also related to deficits in gait 56 mechanics. 57

58 *Methods*

59 **Multiple Sclerosis patients**. The study comprised of 32 MS patients and 30 age, weight, 60 gender and height matched healthy controls. All participants were recruited by our clinicians at 61 the University's Medical Center Department of Neurology and through advertisements placed 62 with the local chapter of the National Multiple Sclerosis Society. They provided informed 63 consent in accordance with procedures approved by the University's Medical Center Institutional 64 Review Board.

Inclusion criteria for patients with MS included cognitive competency to give informed 65 66 consent as determined by our MS clinician (coauthor MF), age ranging from 19 years to 65 years, an Expanded Disability Status Scale (EDSS) score $1 - 6.0^{12}$. There was no requirement 67 for MS disease type for inclusion in the study. Healthy controls were age 19 to 65 years and free 68 of any neurological, orthopaedic, or other co-morbid condition which could affect walking 69 mechanics. Exclusion criteria for both patient with MS and healthy controls for the study 70 included: inability to give informed consent, pregnancy or breastfeeding or within 3 months post 71 partum at the initiation of the study, any other neurological or vestibular disorder, and any other 72 co-morbid conditions which would affect gait mechanics. Controls were recruited from family 73 74 members of MS subjects and through the community to match the overall MS group characteristics but were not matched to individual subjects. 75

76 Data Collection Protocol

In order to evaluate gait mechanics, joint torques and powers from the lower extremities
were used to evaluate the overall joint muscular contributions and their responses during
locomotion. Joint torques and powers have been used successfully to classify gait mechanics in
the elderly and in patients with osteoarthritis, total joint replacement, and anterior cruciate

ligament deficiency ¹³⁻¹⁶ to make surgical decisions ¹⁷, and to evaluate treatment outcomes in 81 pathological populations ^{18, 19}. For all data collections, the subjects (patients and controls) 82 arrived at the laboratory where informed consent was obtained. Next, anthropometric data of the 83 lower extremities was measured and reflective markers were placed according to anatomical 84 location²⁰. Figure 1 shows the marker set-up from the frontal plane only. Subjects walked 85 86 through 10 meter walk-way equipped with an embedded force platform (Kistler 9281B, Kistler Instrumentation Corporation, Amhurst, NY) and surrounded with an 8 camera Motion Analysis 87 system (Eagle system, Motion Analysis Corp., Santa Rosa, CA). Figure 2 shows a subject 88 walking with a foot striking the force platform. The subject walked through the walkway from 89 90 the determined starting position while

91

INSERT FIGURE 1 AND FIGURE 2

real-time marker position (60 Hz) and force platform (600 Hz) data was collected 92 simultaneously. Once the trial was completed, the MS patient rested for at least one minute. The 93 94 same process was then repeated at least four more times to obtain five good trials with the 95 subject's footfall landing completely within the force plate without altering the stride. After five 96 successful trials, the other leg was collected using the same process. Participants typically 97 needed to complete a total of 15 walking trials in order to obtain 5 good trials on each side. Finally, the MS patients completed two fatigue specific questionnaires and a general health 98 survey, the SF-36 questionnaire. These are described below. 99

100 **Qualitative measures**

Fatigue Severity Scale. The FSS is a method of evaluating fatigue in MS patients and in
 other conditions including chronic fatigue immune dysfunction syndrome and systemic lupus
 erythmatosis. The FSS is designed to differentiate fatigue from clinical depression, since both

share some of the same symptoms. The FSS questionnaire is comprised of nine statements 104 related to the patients' subjective perception of fatigue and its consequences on everyday 105 activities. Patients are asked to rate their level of agreement (toward seven) or disagreement 106 (toward zero) with the nine statements. The FSS has been validated for use with MS patients 107 where the scale demonstrated high internal consistency with a Cronbach's alpha of 0.81^{21} . 108 *Modified Fatigue Impact Scale*. The MFIS is a modified form of the Fatigue Impact Scale 109 based on items derived from interviews with MS patients. The scale assesses the effect of fatigue 110 in terms of physical, cognitive, and psychosocial functioning with a 21-item questionnaire. The 111 MFIS has been validated for use with MS patients by Kos et al ²² who found the overall 112 Cronbach's alpha was 0.9223, 0.8813 for the physical, 0.9219 for the cognitive and 0.6496 for 113 the psychosocial subscale. 114

Short form SF-36. Eight health domains are assessed with the SF-36: Physical Function,
limitation due to Physical Health, limitation due to Emotional Problems, Energy, Mental Health,
Bodily Pain, General Health, and Social Function. The SF-36 has been used extensively to
evaluate and differentiate between groups of varying health status ^{23, 24} and has previously been
used with MS patients ^{25, 26}.

120 **Quantitative Measures**

Joint Torques & Powers. During post processing, a low-pass second order Butterworth
digital filter with a 7 Hz cutoff frequency was used to smooth the marker trajectories.
Subsequently, the joint angles were calculated for the sagittal plane during the stance phase of
walking based on the methods of Vaughan et al ²⁷ and Nigg et al ²⁸. Joint torques were then
calculated from the joint angles of the lower limb segments and the simultaneous ground reaction
forces produced based on inverse dynamics ²⁹. Joint powers were calculated based on the

129 Matlab (The MathWorks, Inc., Natick, MA).

The peak values for joint extensor and flexor torque, and joint power absorption and 130 generation (Figures 3 and 4) were identified for the ankle, knee and hip joints during the stance 131 phase according to other gait studies on joint kinetics ^{13, 30-32}. To identify the difference between 132 MS patients and controls for the joint torques and powers, the value for each peak joint torque 133 and peak joint power variable (average from 5 trials) for each MS patient was subtracted from 134 the corresponding average value of the same variable from the healthy control group (Table 3). 135 For example, for each MS subject, the differenced joint torque and joint power variables were 136 calculated as: 137

138

$d_APT = APT_{control mean} - APT_{MS subject}$

Because control subjects were recruited as a group and not matched to individual MS subjects, this methodology allowed for identification of the differences between MS patients and the entire control group rather than single control subjects.

142 INSERT FIGURE 3 HERE

143 INSERT FIGURE 4 HERE

144 Statistical Analysis

A sample of 30 MS patients and 30 matched controls yielded 80% power to detect an effect size of 0.9 for differences in gait variables between the two groups. Independent t-tests were used to compare demographic data for patients with MS to healthy controls. Pearson correlations were performed between the scores for the FSS, MFIS, each of the eight SF-36 domains and each of the differenced joint torque and power parameters. All data was assessed

- 150 for normality (Q-Q plots) and found to be normally distributed. Analyses were performed using
- 151 SPSS 16.0 statistical software (SPSS Inc, Chicago, IL) with alpha equal with 0.05. Due to the
- exploratory nature of this study, no adjustments were made for multiple comparisons.

154 *Results*

A total of 32 patients with MS and 30 healthy controls were included. The MS group and healthy controls did not significantly differ in terms of age and mass. None of patients with MS experienced a relapse of symptoms within 3 months of participating in the gait analysis. All of the MS subjects were on disease modifying, but not on symptom modifying therapies. The mean EDSS score for the MS group was 2.6 ± 0.7 which indicates a relatively mild level of motor disability.

161 INSERT TABLE 1 HERE

162 The mean scores for the Fatigue Severity Scale (FSS), Modified Fatigue Impact Scale163 (MFIS) and for each subscale of the SF-36 are listed in Table 2.

164 INSERT TABLE 2 HERE

The FSS showed a significant relationship only with walking velocity (Table 3) and peak 165 ankle power generation (A2) (Table 4). The MFIS showed a significant relationship only with 166 peak knee extensor torque (Table 3) and the peak knee power absorption (K1) (Table 4). The SF-167 36 Physical Function subscale revealed a significant relationship with several parameters from 168 the joint torques (4 out of 6; Table 3) and joint powers (6 out of 8; Table 4). The Limitation due 169 170 to Emotional Problems and Social Function subscales each showed a significant relationship with one joint torque (Table 3) and one joint power parameter (Table 4). The Limitation due to 171 Physical Function subscale showed a significant relationship with walking velocity (Table 3) and 172 with one joint power parameter (Table 4). The Energy subscale showed a significant relationship 173 with one joint power parameter (Table 4). The Bodily Pain subscale showed a significant 174 relationship with walking velocity (Table 3), two joint torque parameters (2 out of 6; Table 3) 175 and three joint power parameters (3 out of 8; Table 4). 176

177 INSERT TABLES 3 & 4 HERE

178 Importantly, all the significant relationships between the quantitative gait measures (joint

- torques and powers) and the fatigue scales (FSS and MFIS) were small or medium (0.1 to 0.3
- and 0.3 to 0.5, respectively) 33 . In contrast, the SF-36 physical function subscale revealed large
- 181 correlations (0.5 to 1.0) with walking velocity and with the joint torque and joint power
- 182 parameters (Table 3 and 4).

184 Discussion

This study outlines the relationship between reported fatigue levels and the deficits in 185 joint torques and powers during overground walking in MS patients. The FSS, which specifically 186 evaluates fatigue levels independent of depression, showed only two significant relationships 187 out of 15 (13.3%), indicating a limited relationship with the changes that occur in the gait 188 mechanics of patients with MS. The MFIS, which is an MS patient specific fatigue measure, 189 showed similar results with only two significant relationships out of 15 (13.3%). It was 190 hypothesized that fatigue and gait mechanics would reveal significant relationships because both 191 fatigue in MS patients and gait control. Because both gait and fatigue are affected by central 192 neural drive^{4, 7, 9}, it is expected that any alterations in gait mechanics would likely contribute to 193 fatigue. This hypothesis was shown to be only partially true with respect to the utilized fatigue 194 scales. With respect to SF-36, the Physical Function subscale and the Bodily Pain subscale both 195 showed relationships with the gait mechanics of patients with MS with 11 out of 15 (73.3%) and 196 6 out of 15 (40.0%) correlations, respectively, being significant. The larger number of significant 197 relationships with gait mechanics and the SF-36 subscales is partially in agreement with the 198 original hypothesis that general health perceptions would be related to gait deficit measures. 199 The lack of correlations between fatigue questionnaires (FSS and MFIS) and measures of 200 gait mechanics indicate that the use of fatigue questionnaires to infer information regarding MS 201

patient's functional capability may be inappropriate. The SF-36 subscales focus more on specific function areas and show stronger relationship with gait mechanics. Thus, we believe that it may be possible to better represent the relationship between fatigue in MS patients and their gait mechanics by expanding the fatigue questionnaires to incorporate the effects of fatigue on specific areas of physical function as the SF-36 does.

The FSS was significantly and positively related with walking velocity (Table 3) and 207 with the joint power measure A2 (Table 4). Overall, the FSS focuses on the perception of fatigue 208 and its consequences on everyday activities, so the results indicate that the worse the MS 209 210 patient's perception of fatigue was, the larger the differences in walking velocity and in power generation at the ankle (A2) during late stance between the patients and the healthy controls. The 211 decrements in power generation at the ankle (A2) during late stance indicate that the MS patients 212 213 have difficulty propelling the trunk and the leg into the swing phase and indicate that the ankle plantarflexors (soleus and gastrocnemius) are not providing sufficient power to accelerate the 214 trunk which would result in slower walking velocity ³⁴. The significant relationship between FSS 215 and walking velocity decrements in MS patients indicate that FSS is related primarily with the 216 mechanisms related to forward progression during walking. Decreased walking velocity and 217 decreased capability to maintain forward progression during walking could result in increased 218 energy expenditure during walking ³⁵ and would likely affect performance on everyday activities 219 ^{34, 36}, causing increased overall fatigue, thus demonstrating a relationship between A2 and FSS 220 221 score.

The MFIS, which outlines the effect of fatigue in terms of physical, cognitive, and 222 psychosocial functioning, was correlated decreased power absorption at the knee (K1) and 223 224 extensor torque at the knee (KET) during early stance phase. The decreased power absorption at 225 the knee (K1) and extensor torque at the knee (KET) indicate that MS patients have difficulty during weight acceptance in single stance and are not able to generate the necessary extensor 226 activity to eccentrically absorb power at the knee (negative muscle) during early stance³⁵. Loss 227 of the high efficiency negative work at the knee could result in increased metabolic energy 228 expenditure during gait³⁵ and a larger metabolic cost of walking for patients with MS. Because 229

MFIS shows a significant relationship with the amount of negative work being performed at the knee during early stance, we can speculate that the MFIS is related mostly with the overall energy expenditure of patients with MS during walking.

233 MS patients may be likely to perceive fatigue levels as higher since their ability to maintain forward progression is diminished and overall metabolic cost is likely increased during 234 walking. To maintain forward progression an increase in the frequency of muscle firing would be 235 236 necessary, but this could be difficult to maintain for an MS patient due to demyelination of nerve fiber and conduction block seen in structurally intact axons ³⁷. This conduction block is proposed 237 as the primary causation of fatigue in MS patients seen during voluntary effort⁴. The 238 correlations between FSS, MFIS, and the specified joint power measures may be a reflection of 239 240 the theorized primary causation of fatigue in MS patients.

Finally, the SF-36 subscales for Physical Function and Bodily Pain, which measure 241 overall perceptions of general health, both had negative correlations with joint parameters which 242 indicate that as differences in the gait measures between MS patients and healthy controls 243 increased, the perception of physical function capability decreased in MS patients and the 244 perceptions of bodily pain increased in MS patients. These results are not surprising since Motl 245 et al ³⁸reported that worsening MS symptoms have a direct negative relationship with self-246 247 efficacy and physical activity; hence any changes in actual physical capability levels (reflected here by joint torques and powers) would also be related to perception of physical function. The 248 same investigators also reported that with worsening of symptoms, including an increase in 249 250 bodily pain, there is a significant decrease in levels of physical activity and physical function³⁹. Because these scales are significantly related with several of the gait measures, it is fair to report 251

that the SF-36 subscales are relatively successful in reflecting the motor disability level of MSpatients.

Because alterations in joint torques and powers would likely cause changes in energy 254 expenditure during walking, it is likely that there is a relationship between gait measures and 255 fatigue in persons with MS. However, this study showed limited correlations between the FSS 256 and MFIS with gait measures. The SF-36 subscales showed more relationships with gait 257 258 measures which may indicate that the SF-36 is a better measure of overall functional status in MS patients, however, a larger follow-up study would be needed to confirm these findings. The 259 idea that fatigue specific questionnaires may not be the best tool to reflect physical disability 260 level has also been reported by others ^{6, 40, 41}. These previously published findings combined 261 with the findings of the current study indicate that subjective fatigue rating scales alone should 262 not be used as an indicator of motor disability or of disease progression as it affects the walking 263 performance of the MS patients. Instead, more quantitative measures, such as gait analysis 264 should be used to indicate the relationship between gait problems and fatigue in MS patients and 265 to support clinical decision making. 266

267 *Limitations*

Several limitations exist in this study. First, it should be noted that we included only MS patients who were ambulatory in the study. Thus, the findings of this study, in terms of usefulness of fatigue scales to indicate functional status and disability, are generalizable only to MS patients who are ambulatory without bilateral aid (EDSS < 6.0). Second, the causes of gait dysfunction in patients with MS are likely multi-factorial and this study did not attempt to differentiate which disease mechanisms, i.e. spasticity, neuropathy, muscle weakness, were specifically related to measures of fatigue and general health. Finally, reported fatigue in MS patient is also multi-

factorial. Specific medication, sleep patterns, and overall lifestyle influences may affect reports
of fatigue. By utilizing fatigue rating scales that are well established for use with patients who
have MS, this study did not seek to specify the sources of reported fatigue but only the relative
MS fatigue rating and whether those ratings were related to objective and reliable measures of
walking performance.

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- 378

- 380 Figure Legends
- **Figure 1**: Marker set from the frontal plane
- **Figure 2**: A subject walking with one foot striking the force platform
- **Figure 3**: Joint Torque figures which identify the gait variables used
- **Figure 4**: Joint Power figures which identify the gait variables used

1 Tables

- 2 Table 1: Demographic information of study participants. P-value is indicated for independent t-
- 3 test between groups.

	MS Patients	MS Patients Healthy Controls				
	(n = 32)	(n = 30)				
	Sex 5 male, 27 female 8 male; 22 female					
Age	46.3 ± 10.8 yrs	41.4 ± 12.2 yrs	p = 0.097			
EDSS	2.6 ± 0.7	-				
Height (cm)	165.0 ± 6.7	170.6 ± 11.2	<i>p</i> = 0.021			
Mass (kg)	79.9 ± 18.5	76.9 ± 18.5	<i>p</i> = 0.535			

4

- 6 Table 2: Averaged scores for each fatigue scale and for each component of the Medical
- 7 Outcomes Short Form 36 Health Survey (SF-36) for MS patients.

	MS patient score
Questionnaire Scale	mean ± SD
Faligue Severily	
Scala	4.6 ± 1.5
Modified Fatigue	
Impact Scale	42.3 ± 15.4
SF-36	
Physical function	57.8 ± 23.6
Limitation due to	
Physical Function	43.0 ± 36.1
Limitation due to	
Emotional Problems	46.8 ± 43.0
Energy	46.4 ± 22.5
Mental Health	65.0 ± 22.0
Social Function	61.9 ± 27.3
Bodily Pain	65.4 ± 22.9
General Health	50.3 ± 20.6

9 Table 3: Correlation matrix between quantitative parameters of gait mechanics (joint torques) and the qualitative self-

10 perceived measures of fatigue (Fatigue Severity Scale, Modified Fatigue Impact Scale) and functional status (SF-36) of MS

11 patients. Pearson correlation values are reported.

Qualitative Measure	Quantitative Measure						
	d_Velocity	d_ADT	d_APT	d_KET	d_KFT	d_HET	d_HFT
FSS	*0.35 (.049)	0.22	0.31	0.30	0.09	0.26	0.02
MFIS	0.34	0.20	0.14	*0.37 (.038)	-0.03	0.16	-0.09
SF-36							
Physical function	*-0.70 (.000)	*-0.54 (.002)	*-0.51 (.003)	*-0.69 (.000)	-0.15	-0.22	*-0.39 (.029)
Limitation due to	× 0.75 (0.00	0.00		0.01	0.070	0.02
Physical Function	*-0.35 (.050)	-0.09	-0.09	-0.26	0.21	-0.070	-0.02
Limitation due to							
E notional Problems	-0.11	0.04	-0.22	*-0.36 (.041)	0.32	-0.12	-0.16
Energy	0.05	0.06	0.18	-0.13	0.23	-0.12	0.16
Mental Health	0.13	0.04	0.12	-0.23	0.32	-0.06	0.31
Social Function	-0.15	-0.08	-0.08	*-0.37 (.038)	0.10	-0.01	0.05
Bodily Pain	*-0.46 (.008)	*-0.37 (.037)	-0.26	*-0.45 (.011)	-0.15	-0.03	-0.13
General Health	-0.11	-0.100	-0.08	-0.13	0.07	-0.10	0.16

12 SF-36: Medical Outcomes Survey Short Form 36 Health Survey.

13 *Significant correlations (*p*-value).

14 d_Velocity - difference in walking velocity; d_ADT - difference in Peak ankle dorsiflexion moment during early stance; d_APT -

15 difference in Peak ankle plantarflexion moment during late stance; d_KFT - difference in Peak knee flexion moment during stance;

16 d_KET - difference in Peak knee extension moment during stance; d_HFT - difference in Peak hip flexion moment during late stance;

17 d_HET - difference in Peak hip extension moment during early stance.

18 Table 4: Correlation matrix between quantitative parameters of gait mechanics (joint powers) and the qualitative self-

19 perceived measures of fatigue (Fatigue Severity Scale, Modified Fatigue Impact Scale) and functional status (SF-36) of MS

20 patients. Pearson correlation values are reported.

Qualitative Measure	Quantitative Measure							
	<i>d_A1</i>	<i>d_A2</i>	d_K1	d_K2	d_K3	<u>d_H1</u>	<i>d_H2</i>	d_H3
FSS	0.25	0.42 (.010)	0.28	0.27	0.31	0.31	0.07	0.00
MFIS	0.31	0.32	0.35 (.048)	0.33	0.11	0.21	0.07	0.10
SF-36								
Physical function	-0.38(.033)	-0.69 (.000)	-0.62 (.000)	-0.42 (.017)	-0.43 (.015)	-0.11	-0.56(.001)	0.09
Limitation due to	0.10	0.00	0.04	0.25 (0.00	0.17	0.10	0.17
Physical Function	-0.10	-0.23	-0.24	-0.37 (.035)	-0.29	-0.1/	-0.10	-0.17
Limitation due to								
E notional Problems	-0.11	-0.28	-0.29	-0.45 (.009)	-0.19	-0.04	-0.28	-0.22
Energy	-0.09	-0.01	-0.08	-0.37 (.037)	-0.15	-0.03	0.06	-0.24
Mental Health	-0.06	0.01	-0.11	-0.22	-0.02	-0.10	0.05	-0.04
Social Function	-0.18	-0.22	-0.34	-0.38 (.030)	-0.24	-0.09	-0.12	-0.32
Bodily Pain	-0.32	-0.48 (.005)	-0.50 (.003)	-0.39 (.026)	-0.14	-0.13	-0.27	0.14
General Health	-0.01	-0.20	-0.11	-0.04	-0.06	-0.15	-0.05	0.04

21 SF-36: Medical Outcomes Survey Short Form 36 Health Survey.

22 *Significant correlations (*p*-value).

23 d_A1 - difference in Peak ankle power absorption in early stance; d_A2 - difference in Peak ankle power generation in late stance;

24 d_K1 - difference in Peak knee power absorption in early stance; d_K2 - difference in Peak knee power generation in mid-stance;

25 d_K3 - difference in Peak knee power absorption in late stance; d_H1 - difference in Peak hip power generation in early stance; d_H2

- difference in Peak hip power absorption in late mid-stance; d_H3 - difference in Peak hip power generation in late stance.



Figure 1: Marker set from the frontal plane



Figure 2: A subject walking with one foot striking the force platform



Figure 3: Joint Torque figures which identify the gait variables used



Figure 4: Joint Power figures which identify the gait variables used