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Journal of Drug Delivery & Therapeutics. 2018; 8(2):96-101

Available online on 15.03.2018 at http://jddtonline.info



Journal of Drug Delivery and Therapeutics Open Access to Pharmaceutical and Medical Research

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Research Article

DESIGN AND CHARACTERIZATION OF SUSTAINED RELEASE MATRIX TABLETS OF METFORMIN HYDROCHLORIDE USING COMBINATION OF HYDROPHILIC POLYMERS

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ABSTRACT

Sustained release system is types of modified drug delivery system that can be used as an alternative to conventional system. Among different dosage forms, matrix tablets are widely accepted for oral sustained release Metformin hydrochloride has relatively short plasma half-life, low absolute bioavailability. The need for the administration two to three times a day when larger doses are required can decrease patient compliance. Sustained release formulation that would maintain plasma level for 8-12 h might be sufficient for daily dosing of metformin. Sustained release products are needed for metformin to prolong its duration of action and to improve patient compliances. They are capable of reducing the dose intake, minimize the blood level oscillation dose related adverse effect and cost thus improves the patient compliance in the therapeutic management of diabetes. The Metformin hydrochloride matrix Sustained release tablets were prepared using different hydrophilic polymers in various proportions as release retarding agent to prolong the drug release and to improve the patience compliance. The tablets were evaluated for various tests like hardness, friability, disintegration and *in-vitro* dissolution studies.

Keywords: Matrix Tablets, Metformin hydrochloride, Hardness, Friability, Disintegration and in-vitro dissolution studies

Article Info: Received 9 Jan, 2018; Review Completed 3 March, 2018; Accepted 3 March, 2018; Available online 15 March, 2018



Cite this article as:

Singh A, Rajput DS, Gopalrao AA, Chauhaan D, Mafidar R, Bhowmick M, Rathi J, Mathur R, Design and characterization of sustained release matrix tablets of metformin hydrochloride using combination of hydrophilic polymers, Journal of Drug Delivery and Therapeutics. 2018; 8(2):96-101

DOI: <u>http://dx.doi.org/10.22270/jddt.v8i2.1672</u>

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INTRODUCTION

Sustained release system is types of modified drug delivery system that can be used as an alternative to conventional system. Among different dosage forms, matrix tablets are widely accepted for oral sustained release1. Sustained release systems have benefits like patient compliance, avoidance of multiple dosing, cost effectiveness, flexibility, increased plasma drug concentration, reduction of side effects; broad regulatory acceptance and they overcome the problems associated with conventional drug delivery system. Metformin hydrochloride an orally administered biguanide, which is widely used in the management of and the type -II diabetes, is an oral anti-hyperglycemic agent, shows incomplete absorption from the gastrointestinal tract and the absolute bioavailability is 50 - 60 % with relatively

short plasma half-life of 1.5 -4.5 h. The aim of this work is to prepare matrix tablets containing Metformin hydrochloride, as a model drug, using different polymers and evaluate its release characteristics. ¹⁻⁶

MATERIALS AND METHODS

MATERIALS

Metformin HCl powder was a gift from USV Ltd, Mumbai, India. Microcrystalline cellulose, talc, magnesium stearate, polymers such as HPMC and sodium alginate were purchased from S. D. Fine Chem. Labs. (Mumbai, India). All other ingredients used throughout the study were of analytical grade and were used as received.

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METHODS

➢ Formulation of sustained release tablet⁷⁻⁹

Sustained Release Tablets of Metformin HCL with other excipients were prepared by direct compression. The weight of Metformin HCL was kept constant in all the prepared tablets at 400 mg/tablet. Different ratio grades of HPMC & SODIUM ALGINATE were chosen as polymeric materials. Micro crystalline cellulose (MCC) was selected as tablet diluent for increasing the compressibility and flowability of the ingredients as well as to maintain the tablets at constant weight of 400 mg. Magnesium stearate was used as a lubricant at concentration of 2% by weight of tablet. To make powder mixtures, the drug, polymer and MCC were thoroughly mixed for 30 min by means of pestle and mortar. This powder mixture was then lubricated with magnesium stearate then compressed into tablets in 6 mm rotary tablet punching machine. The force of compression was adjusted so that hardness of all the prepared tablets ranges from 5.5-6.5 kg/cm. The detailed compositions of the prepared matrix tablets formulations are given in (Table no.1)

Table 1: Formulation of sustained released tablet having ratio 1:2

S.No.	Ingredient	Formulation for polymer ratio 1:2
1.	Metformin HCL	300 mg
2.	Talc	10 mg
3.	Hydroxypropyl methylcellulose (HPMC)	10 mg
4.	Sodium alginate	20 mg
5.	Magnesium stearate	10 mg
6.	Micro crystalline cellulose (M.C.C.)	50 mg

Table 2: Formulation of sustained released tablet having ratio 2:1

S.No.	INGREDIENT	FORMULATION FOR POLYMER RATIO 2:1
1.	Metformin HCL	300 mg
2.	Talc	10 mg
3.	Hydroxypropyl methylcellulose (HPMC)	20 mg
4.	Sodium alginate	10 mg
5.	Magnesium stearate	10 mg
6.	Micro crystalline cellulose (M.C.C.)	50 mg

1) Angle of Repose ^{10,11}

The angle of repose was determined by fixed funnel method. A funnel was kept vertically in a stand at a specified height above a paper place on a horizontal surface. The funnel was closed was closed and granules was filled in funnel. Then funnel was opened to release the granules on the paper to form a smooth conical heap. The height and radius of heap was measured and the angle of repose was calculated by using the following formula.

$\Theta = \tan^{-1} h/r$

Where Θ = Angle of repose, h = height of heap and r = radius

Table 3: Relationship between Angle of Repose (Θ) and flow properties

Angle of repose (Θ)	FLOW
(Degrees)	
<25	Excellent
25-30	Good
30-40	Passable
>40	Very poor

2) Bulk Density^{10,11}

A known amount of granules was transferred into a 25ml measuring cylindrical carefully level the granules without compacting and measure the bulk volume. The bulk density was determined by using the formula:

Bulk Density = Weight of granules / bulk volume

3) Tapped Density^{10,11}

Tapped density was determined by digital bulk density apparatus. A known amount of granules was transferred into the measuring cylinder and tapped upto 100 times and measure the tapped volume. The tapped density was determined by using the formula:

Tapped Density = Weight of granules / tapped volume

4) Compressibility Index^{10,11}

Compressibility Index was determined by the following formula:

Compressibility Index =

[Tapped density – Bulk density / Tapped density]× 100

Table 4: I	Relationship	between	Compressibility	Index
	and f	low prop	oerties	

% CARR'S COMPRESSIBILTY INDEX	FLOW
5-15	Excellent
12-16	Good
18-21	Fair to passable
23-35	Poor
33-38	Very poor
>40	Very

5) Hausner's Ratio^{10,11}

Hausner's ratio was determined by following formula:

Hausner's ratio = Tapped density / Bulk density

6) Hardness^{10,11}

In the measurement of hardness, the crushing strength of the tablets is measured. It gives the tablets breaking force and the strength of the physical tablets are represented by the hardness. Hardness was measured using a Pfizer hardness tester. Hardness to be measured of ten tablets. The hardness were measured in newton. The average hardness, relative standard deviation, standard deviations were reported. The hardness of the tablets were measured during start and between the compression.

7) Weight variation $test^{10,11}$

To study weight variation, 20 tablets of each formulation were collected randomly during compression and weighed using an electronic balance to obtain average weight of each tablets. Also, the individual tablet was weighted.

Limit: Weight of individual tablet should be in the limit of average weight $\pm 5\%$

8) Friability¹²⁻¹⁴

The test was carried out using ROCHE FRIABILATOR. Ten tablets were taken and carefully dedusted prior to testing the tablets were weighed accurately, and placed the tablets in the drum. The drum was allowed to be rotated 100 times, and after that the tablets were removed. Removed loose dust form the tablets as before, and weighed accurately.

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The % loss was determined by using following formula:

% Weightloss
$$=$$
 $\frac{\text{Initial Weight} - \text{Final Weight}}{\text{Initial Weight}}$

A maximum loss of mass not greater than 1.0% is considered acceptable.

9) Uniformity of drug content¹²⁻¹⁴

Five tablets were weighed individually and powdered. The powdered equivalent to average weight of tablet was weighed and drug was extracted in 0.1 N HCL. Undissolved material was filtered out. Filtrate was analysed in UV spectrometer at 237 nm after suitable dilution. Absorbence value was substituted in the equation of standard curve of Metformin HCL determined earlier.

Drug content was calculated by following formula.

$$DrugContent = \frac{Actual drug content}{Theoritical drug content} x 100$$

10) In-vitro Dissolution Studies¹²⁻¹⁶

In-vitro drug release study of tablets was performed in USP dissolution apparatus Type – 2 (Paddle). The dissolution test was performed using 900 ml of phosphate buffer 6.8 ph. at $37 \pm 0.0.5$ °C with 50 rpm. A sample (5 ml) was withdrawn from the dissolution apparatus and volume equivalent to the amount of sample withdrawn was replaced with fresh dissolution dissolution medium. The sample were filtered and diluted to suitable concentration with phosphate buffer 6.8 ph. Absorbances of these solutions were measured at 237 nm using a UV spectrophotometer. Cumulative percentage drug dose was calculated using an equation obtained from standard curve.

11) In-Vitro Drug Release Kinetic Study

Kinetic model had described drug dissolution from solid dosage form were the dissolved amount of drug is a function of test time. In order to study the exact mechanism of drug release from the tablet, drug release data was analyzed according to zero order, first order, Higuchi square root, korsemeyer, Peppas model. The regression coefficient R^2 value nearer to 1 indicating the model fitting of the release mechanism.

RESULT AND DISCUSSION

1) Melting Point: The melting point of experimental drug shown in table.

Table 5: Melting point of drug

TEST	DRUG	SPECIFICATION	OBERVATION
Melting point	Metformin HCL	222 -226 [°] c	223-227 [°]

2) Determination of Wavelength Of Maximum Absorbance

The wavelength of maximum absorbence (λ max) in 0.1 N HCL was found to be 235 nm and the graph is shown in figure.

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3) Solubility Of Drug

The solubility of drug in different solvent in shown in table.

Table 6: Solubility of drug in different solvent

S.No.	Solvent	Solubility
1	Distilled Water	Freely soluble
2	0.1N HCL	Soluble
3	Ethanol (95%)	Slightly soluble
4	Methylene chloride	Practically insoluble
5	Acetone	Practically insoluble



Figure 1: Calibration curve of Metformin on 0.01N HCL

5) Evaluation of precompression parameters

Table 7: Evaluation of precompression parameters

Parameters	Hydrophilic Formulations		
() () () () () () () () () ()	Polymer ratio 1:2	Polymer Ratio 2:1	
Carss's Index (%) $(n = 3)$	5.00±0.02	2.44±0.06	
Hausner'sRatio(n=3)	1.052 ± 0.06	1.025 ± 0.08	
Angle of Repose(n=3)	33.69±0.09	35.31±0.04	
Length(mm)(n=20)	15.088±0.03	15.136±0.01	
Hardness(kP)(n=20)	33.2±0.01	33.2±0.08	
Weight(mg)(n=20)	399.4±0.04	401.8±0.02	
Thickness(mm)(n=20)	8.096±0.06	8.152±0.01	
Friability (%) (n=10)	0.0197±0.03	0.107±0.06	
ContentUniformity (%) (n=20)	100.268 ± 0.05	100.315±0.04	

6. Evaluation of post compression parameter

The results of post compression parameters such as hardness, Friability, Weight variation and Drug content uniformity are shown in table.

Table 8: Result of post compression parameters of formulation

Batches	Hardness (kg/cm ²⁾	Friability (%)	Weight Variation	Drug Content Uniformity
F1	12.4	0.70	Passes	90.12
F2	14.52	0.66	Passes	92.65
F3	15	0.62	Passes	96.15

1) In Vitro Dissolution Study: The results obtaining in vitro release studies were plotted Cumulative % release against time. These results indicated that the release rate was limited by the drug particles dissolution rate and erosin of the different polymer ratio.

4) Calibration Curve



Figure 2: Dissolution Profile of Formulations

	% Drug Release		
Time	1 monte	Batch No.	9
(1115.)	F1	F1 F2	
	Marketed Drug	Polymer Ratio 2:1	Polymer Ratio 1:2
1	40.85	28.79	23.14
2	59.21	44.63	42.25
3	70.68	55.16	53.67
4	85.53	68.25	64.03
6	94.12	82.32	78.89
8	96.23	92.57	87.76
10	97.45	95.27	93.86

Table 9: Release kinetic Study

2) Kinetic Release Study

> Kinetics of Metformin Hydrochloride sustained released formulation:

The optimized batch F_6 was subjected to graphical treatment to assess the kinetic of drug release from 1:2 polymer ratio tablet. The optimized formulation F6 was subjected to Zero order, first order, Hixson-Crowell,

Higuchi and Korsmeyer-Peppas model to study the in vitro kinetic release mechanism.

From, in vitro kinetic release mechanism study it was found that the drug released kinetic of the sustained release formulation of optimized batch F6 follow diffusion mechanism for drug release from the 1:2 polymer ratio tablet.

Table 10: Zero order kinetic Model

S. No.	Time in hour	Cum.% Drug release
1.	0.5	11.6
2.	1	26.13
3.	2	42.26
4.	3	53.77
5.	4	64.02
6.	6	79.31
7.	8	87.56
8.	10	93.68

S. No.	Time in hour	Log Cum.% Drug retained
1.	0.5	1.946
2.	1	1.868
3.	2	1.761
4.	3	1.664
5.	4	1.556
6.	6	1.315
7.	8	1.094
8.	10	0.801

Table 11: First order kinetic Model



Figure 3: First order kinetic Model

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Figure 4: Zero order kinetic Model

CONCLUSION

The present work deals with the aim to formulate and evaluate the sustained release tablet of Metformin HCL. From results obtained, it was concluded that the formulation of sustained release tablet of Metformin HCL containing hydrophilic polymers HPMC and sodium alginate were capable of exhibiting sustained release properties They are capable of reducing the does intake minimize the blood level oscillation does related adverse effect and cost thus improves the patient compliance in the therapeutic management of diabetes.

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