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1 **Original Paper**

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3 **Walking cadence required to elicit criterion moderate-intensity physical activity is moderated by**  
4 **fitness status**

5

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30 **Abstract**

31 The aims of this study were to estimate the walking cadence required to elicit a  $VO_{2R}$  (VO<sub>2</sub>R) of  
32 40 % and determine if fitness status moderates the relationship between walking cadence and %VO<sub>2</sub>R.

33 Twenty participants (10 male, mean(s) age 32(10) years;  $VO_{2max}$  45(10) mL·kg<sup>-1</sup>·min<sup>-1</sup>) completed  
34 resting and maximal oxygen consumption tests prior to 7 x 5-min bouts of treadmill walking at  
35 increasing speed while wearing an Apple Watch and measuring oxygen consumption continuously.

36 The 7 x 5-min exercise bouts were performed at speeds between 3 and 6 km·h<sup>-1</sup> with 5-min seated rest  
37 following each bout. Walking cadence measured at each treadmill speed was recorded using the Apple  
38 Watch 'Activity' app. Using Bayesian regression, we predict that participants need a walking cadence  
39 of 138 to 140 steps·min<sup>-1</sup> to achieve a  $VO_{2R}$  of 40 %. However, these values are moderated by fitness  
40 status such that those with lower fitness can achieve 40 %  $VO_{2R}$  at a slower walking cadence. The  
41 results suggest that those with moderate fitness need to walk at ~40 % higher than the currently  
42 recommended walking cadence (100 steps·min<sup>-1</sup>) to elicit moderate-intensity physical activity.  
43 However, walking cadence required to achieve moderate-intensity physical activity is moderated by  
44 fitness status.

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46 **Keywords:** wearable electronic devices, exercise, oxygen consumption, walking, Bayes theorem.

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## 57 **Introduction**

58 Low cardiorespiratory fitness (CRF) is independently associated with increased chronic disease and  
59 mortality risk (Blair et al., 1989). Regular exercise improves CRF, with small (1 MET, 3.5 mL·kg<sup>-1</sup>·min<sup>-1</sup>)  
60 increases in CRF shown to reduce all-cause mortality risk in the order of 8-14% (Dorn,  
61 Naughton, Imamura, & Trevisan, 1999). Given that improvements in CRF are influenced by the  
62 intensity of exercise (Swain & Franklin, 2006), and that government guidelines make explicit  
63 reference to the achievement of ‘moderate-to-vigorous’ intensity physical activity (MVPA), the  
64 measurement of physical activity intensity is therefore important.

65 Recently, a walking cadence of  $\geq 100$  steps·min<sup>-1</sup> in adults has been recommended as  
66 sufficient to meet the requirements of MVPA (Tudor-Locke et al., 2018). However, this estimate is  
67 based on studies that have used accelerometry (an external measure of exercise intensity), together  
68 with the use of metabolic equivalents (an indirect measure of exercise intensity). To overcome these  
69 limitations, a recent study (Serrano, Slaght, Sénéchal, Duhamel, & Bouchard, 2017) used oxygen  
70 consumption reserve (VO<sub>2</sub>R) to estimate the walking cadence required to achieve moderate-intensity.  
71 A VO<sub>2</sub>R of 40 % is considered to be the lower bound of moderate-intensity (Riebe, 2018). These  
72 authors (Serrano et al., 2017) reported that a mean (*s*) walking cadence of 115 (10) steps·min<sup>-1</sup> was  
73 required to achieve a VO<sub>2</sub>R of 40 %, suggesting that an external measure of exercise intensity  
74 (accelerometry) underestimates the walking cadence required to achieve MVPA when compared to an  
75 individualized and relative measure (VO<sub>2</sub>R). However, Serrano et al (2017) didn’t explore the effect of  
76 fitness status on the walking cadence required to elicit 40 % VO<sub>2</sub>R. Given that the participants in their  
77 study had a mean (*s*) age of 69 (8) years and VO<sub>2</sub>peak of 24 (women) and 29 (men) mL·kg<sup>-1</sup>·min<sup>-1</sup>,  
78 fitness status is likely to have had an effect on the walking cadence required to elicit 40 % VO<sub>2</sub>R. It is  
79 also unclear how these walking cadence values (100 (Tudor-Locke et al., 2018) and 115 (Serrano et  
80 al., 2017) steps·min<sup>-1</sup>) translate to modern consumer wearable devices that measure step counts.

81 We have recently reported that the Apple Watch underestimates the walking speed required to  
82 exercise at moderate intensity when measured using  $\text{VO}_2\text{R}$  (Abt, Bray, & Benson, 2018). Thompson et  
83 al. (2016) reported that because consumer wearable devices record all forms of activity, they typically  
84 overestimate the amount of MVPA achieved. This might suggest that a 100 or even 115 steps·min<sup>-1</sup>  
85 thresholds are too low when measured using a consumer wearable device, and in those with higher  
86 fitness. The rapid growth in the consumer wearable market (Peake, Kerr, & Sullivan, 2018; Phillips,  
87 Cadmus-Bertram, Rosenberg, Buman, & Lynch, 2018) would suggest that this information is  
88 important if wearable devices are to be an effective component of physical activity promotion  
89 programmes. The Apple Watch is currently the highest selling smartwatch in the world, with global  
90 accumulated sales estimated at approximately 46 million units (Dediu, 2018). Given the public health  
91 messages that incorporate step count (Tudor-Locke et al., 2011; Yamamoto et al., 2018), it is  
92 important for researchers, exercise professionals and consumers to understand how target step counts  
93 translate into criterion measures of MVPA. Therefore, the aims of this study were to estimate the  
94 walking cadence required to elicit a  $\text{VO}_2\text{R}$  of 40 % (the lower bound of moderate-intensity) and  
95 determine if fitness status moderates the relationship between walking cadence and %  $\text{VO}_2\text{R}$ .

96

## 97 **Methods**

98 Our study used a cross-sectional design where each participant completed a series of brief exercise  
99 bouts within the same laboratory session. Prior to these exercise trials each participant had their  
100 maximal oxygen consumption ( $\text{VO}_{2\text{max}}$ ) and resting oxygen consumption ( $\text{VO}_{2\text{rest}}$ ) measured.  
101 Approval to conduct the study was granted by the Department of Sport, Health and Exercise Science  
102 Ethics Committee (approval number 1516076) at The University of Hull. To approximate power and  
103 determine appropriate sample size, Bayesian power analysis was conducted using simulations from  
104 hypothesised posterior distributions (Kruschke, 2015). This involved simulating a random distribution  
105 of parameter values from hypothesised slope and intercept values based on previous research and pilot  
106 data for relationships between walking cadence and %  $\text{VO}_2\text{R}$ . These values were used to generate one  
107 thousand posterior estimates for each sample size from 10 to 40 (30,000 in total) using Integrated

108 Nested Laplace Approximation (Rue, Martino, & Chopin, 2009). This analysis determined that  
109 measurements from 20 participants would result in a 0.8 probability of a positive relationship between  
110 walking cadence and %  $\text{VO}_2\text{R}$ .

111 Recruitment of low-risk participants (Riebe, 2018) aged between 18 and 50 years from the  
112 university and local community was undertaken using written promotional material and personal  
113 communication. The exclusion criteria were: 1) men and women classified as moderate or high-risk  
114 according to the ACSM risk classification criteria (Riebe, 2018), 2) those unable to walk on a  
115 motorized treadmill, 3) current smoker, 4)  $\text{BMI} \geq 30 \text{ kg}\cdot\text{m}^2$ , 5) currently taking medication that alters  
116 the heart rate response to exercise (e.g. beta blockers), 6) people with gait disturbances.

117 Prior to the measurement of body mass, participants were asked to ensure they had voided and  
118 then instructed to remove all clothing. The mean of two measurements of nude body mass was  
119 measured to the nearest 0.1 kg using digital scales (WB-100MA Mark 3, Tanita Corporation, Tokyo,  
120 Japan). A wall-mounted stadiometer (Holtain Ltd, Dyfed, Wales, UK) was used to measure stretch  
121 stature (Norton et al., 2000).

122 In a temperature-controlled laboratory, resting oxygen consumption was measured 30 minutes  
123 prior to, and in the same session, as  $\text{VO}_2\text{max}$ . This protocol has been previously described in detail  
124 (Abt et al., 2018), but briefly, participants lay supine on a bed with their head on a pillow with oxygen  
125 consumption measured continuously from expired air using a breath-by-breath online gas analysis  
126 system to calculate  $\text{VO}_2\text{R}$  based on a method reported by Miller et al (2012).

127 Participants completed an incremental protocol on a motorized treadmill (h/p/cosmos, Pulsar,  
128 Nussdorf-Traunstein, Germany) with oxygen consumption measured continuously from expired air  
129 using a breath-by-breath online gas analysis system (Cortex Metalyzer 3B, GmbH, Germany). The  
130 breath-by-breath analyzer was calibrated prior to each test using room air and known gas  
131 concentrations of  $\text{O}_2$  and  $\text{CO}_2$ . Volume was calibrated using a 3 L syringe. The protocol commenced at  
132  $3 \text{ km}\cdot\text{h}^{-1}$  and a 1 % gradient and increased  $0.5 \text{ km}\cdot\text{h}^{-1}$  in speed every 30 s until volitional fatigue.  
133 Maximal oxygen consumption was taken as the highest 30 s mean. Based on established criteria

134 (volitional exhaustion; RER > 1.15; plateau in oxygen consumption < 150 mL·min<sup>-1</sup>), all participants  
135 were judged to have reached VO<sub>2</sub>max (Howley, Bassett, & Welch, 1995).

136 Familiarization on how to get on and off the treadmill, as well as walking at the prescribed  
137 speeds, was undertaken prior to the main trial. Participants were instructed to avoid exercise and  
138 maintain their normal diet for the 24 hours prior to the trial and avoid food and caffeinated drinks for  
139 three hours. The main trial consisted of participants completing a series of 5-min bouts of treadmill  
140 walking at a gradient of one percent at increasing speed while wearing an Apple Watch on both wrists  
141 (described below). Each bout was followed by 5-min of seated rest. The first 5-min walking bout was  
142 conducted at 3 km·h<sup>-1</sup>, with the treadmill speed increased for each successive 5-min bout by 0.5 km·h<sup>-1</sup>  
143 (i.e. 3, 3.5, 4, 4.5, 5, 5.5, and 6 km·h<sup>-1</sup>). Participants were not permitted to hold the treadmill handrails  
144 and were instructed to maintain their normal walking gait during each 5-min bout of walking. During  
145 each 5-min bout, oxygen consumption and heart rate were recorded by an online gas analysis system  
146 (as described previously), a Polar chest strap (Polar T31, Polar Electro, OY, Finland) and an Apple  
147 Watch worn on each wrist. Steps measured at each treadmill speed were recorded using the Apple  
148 Watch Activity app.

149 Immediately after each 5-min exercise period was completed, the treadmill was stopped, and  
150 participants instructed to grasp the treadmill handrails and straddle the treadmill. Participants were  
151 required to sit motionless on a stationary chair placed on the treadmill belt with each hand resting on  
152 the treadmill handrail to ensure that no activity during the recovery period contributed to the step  
153 count. Five minutes of seated rest was provided to enable each Apple Watch to update the step count.  
154 The mean oxygen consumption from the last three minutes at each treadmill speed for each watch was  
155 used for later analysis.

156 Moderate intensity exercise and steps were estimated using two first-generation (Series 0)  
157 Apple Watches running watchOS 2.0.1. Each Apple Watch was paired to an iPhone 6 running iOS 9.1.  
158 Following each 5-min rest period the number of steps as measured by each of the Apple Watches was  
159 manually recorded from the Activity app. Moderate-intensity exercise was defined as that between 40  
160 % and 59 % of VO<sub>2</sub>R (Riebe, 2018). The VO<sub>2</sub>R at each treadmill speed (exercise intensity in the

161 equation) was calculated by rearranging equation 1 (Riebe, 2018). Target  $\text{VO}_2$  was the measured  
162 oxygen consumption at each treadmill speed.

163

$$164 \quad \text{Target } \text{VO}_2 = (\text{VO}_{2\text{max}} - \text{VO}_{2\text{rest}}) \times \text{exercise intensity} + \text{VO}_{2\text{rest}} \quad (1)$$

165

166 Descriptive statistics were calculated and are presented as mean (*s*). To describe the relationship  
167 between treadmill speed and walking cadence, a series of Bayesian regression models were fitted to  
168 data from both right and left wrists. These modelled walking cadence as a linear function of speed,  
169 plus Gaussian noise using a standard linear model, a 2<sup>nd</sup> order polynomial, and a 3<sup>rd</sup> order polynomial.  
170 To determine the best model of the relationship, model fit was determined using Leave-One-Out  
171 cross-validation (LOO), a method of estimating pointwise out-of-sample prediction accuracy from  
172 fitted Bayesian models using log-likelihoods from posterior simulations of the parameter values  
173 (Vehtari, Gelman, & Gabry, 2017). The best model for describing the relationship between treadmill  
174 speed and walking cadence predicted by the Apple Watch worn on both left and right wrists was the a  
175 2<sup>nd</sup> order polynomial regression.

176 To describe the relationship between walking cadence and %  $\text{VO}_{2\text{R}}$ , a series of Bayesian  
177 regression models were fitted. These walking cadences were used to predict percentage  $\text{VO}_{2\text{R}}$ . The  
178 models fitted included basic linear models, through 2<sup>nd</sup> and 3<sup>rd</sup> order polynomial models including  
179 multilevel models that allowed individual intercepts to vary, to multilevel non-linear models fitted  
180 using thin plate splines (Wood, 2003; Zhou & Shen, 2001). Each model was fitted with errors  
181 modelled using both normal and skew normal distributions. The final models selected for best out of  
182 sample predictions were a thin plate spline multilevel regression for the right wrist and a 2<sup>nd</sup> order  
183 polynomial model for the left wrist.

184 To explore differences between the estimated walking cadence at 40 %  $\text{VO}_{2\text{R}}$  and  
185 recommendations from the review by Tudor-Locke (2018), a random normal distribution of walking  
186 cadence values was generated ( $n = 200$ , mean = 100 (4)) in R (R Core Team, 2018). This simulated  
187 distribution captured the range of walking cadences presented in the review (90 to 114 steps·minute<sup>-1</sup>)

188 (Tudor-Locke et al., 2018). This distribution was compared to the estimated walking cadence at 40 %  
189  $\text{VO}_2\text{R}$  for the right and left wrists using a Bayesian two-sample t-test. The probabilities calculated  
190 were the probability of a difference showing the percentage of the posterior distribution that falls  
191 above zero. In an attempt to explain, in part, the large variation between individual's percentage  
192  $\text{VO}_2\text{R}$ , an additional model was fitted with  $\text{VO}_2\text{max}$  included as a covariate and the interaction  
193 between  $\text{VO}_2\text{max}$  and walking cadence explored using the best out of prediction models. To determine  
194 if including sex was an important factor in predicting the relationship between %  $\text{VO}_2\text{R}$ , an additional  
195 Bayesian regression model was fitted with sex as a predictor and then compared to the same model  
196 fitted without sex. In addition, predictions for %  $\text{VO}_2\text{R}$  were made using the model for both males and  
197 females to explore any differences directly.

198 All analyses were conducted using R (R Core Team, 2018) and with the Bayesian Regression  
199 Models using 'Stan' (brms) package (Bürkner, 2017) (Stan Development Team, 2018) to implement a  
200 Hamiltonian Markov Chain Monte Carlo (MCMC) with a No-U-Turn Sampler. Weakly informative  
201 priors were used to regularize the models and avoid unreasonable parameter estimates. All models  
202 were checked for convergence ( $\hat{r} = 1$ ), with the graphical posterior predictive checks showing that  
203 simulated data under the best fitted models compared well to the observed data with no systematic  
204 discrepancies (Gabry, Simpson, Vehtari, Betancourt, & Gelman, 2019). Uncertainty in all of the  
205 estimates are reported as 95 % credible intervals.

206

## 207 **Results**

208 Written informed consent was obtained from twenty low-risk (Riebe, 2018) participants (Table 1).

209

210 TABLE ONE ABOUT HERE

211

212 Walking cadence estimated by the Apple Watch worn on right and left wrists increased from a mean  
213 (both wrists combined) of 94 steps·min<sup>-1</sup> at 3 km·h<sup>-1</sup> to 130 steps·min<sup>-1</sup> at 6 km·h<sup>-1</sup>, with maximum



214 walking cadence reached by one participant recorded as 144 steps·min<sup>-1</sup>. Oxygen consumption  
215 increased from a mean of 16 % VO<sub>2</sub>R at 3 km·h<sup>-1</sup> to 34 % VO<sub>2</sub>R at 6 km·h<sup>-1</sup> (Table 2).

216

217 TABLE TWO ABOUT HERE

218

219 The curvilinear relationship found between treadmill speed and walking cadence estimated by the  
220 Apple Watch when worn on both the right and left wrists can be best described by 2<sup>nd</sup> order  
221 polynomial (quadratic) regressions. The relationship between treadmill speed and walking cadence  
222 estimated by an Apple Watch worn on the right wrist produces the following equation:  $y = 40.91 +$   
223  $22.08x - 1.21x^2$ . The relationship between treadmill speed and walking cadence estimated by an  
224 Apple Watch worn on the left wrist produces the equation:  $y = 26.61 + 26.44x - 1.54x^2$ .

225 The Bayesian multilevel thin plate spline regression suggests that the relationship between  
226 percentage VO<sub>2</sub>R and walking cadence estimated by the Apple Watch on the right wrist is curvilinear  
227 (Figure 1). The regression suggests that 93 % of the variance in percentage VO<sub>2</sub>R is explained by the  
228 model, with 87 % of the variance being between participants, and 13 % of the variance being within  
229 participants. This model predicts that the mean walking cadence required to illicit 40 % VO<sub>2</sub>R is 138  
230 steps·min<sup>-1</sup> with a range between individuals from 126 to 147 steps·min<sup>-1</sup>. The Bayesian multilevel 2<sup>nd</sup>  
231 order orthogonal regression suggests that the relationship between % VO<sub>2</sub>R and walking cadence  
232 estimated by the Apple Watch on the left wrist is also curvilinear. Ninety two percent of the variance  
233 in percentage VO<sub>2</sub>R is explained by the model as a whole, with 86 % of the variance being between  
234 participants, and 14 % of the variance being within participants. The model predicts that the mean  
235 walking cadence required to illicit 40 % VO<sub>2</sub>R is 140 steps·min<sup>-1</sup> with a range between individuals  
236 from 126 to 147 steps·min<sup>-1</sup>.

237

238 FIGURE ONE ABOUT HERE

239

240 Including  $\text{VO}_2\text{max}$  as a covariate did not improve the  $R^2$  or the out of sample prediction (LOO).  
241 Nonetheless, this analysis provides an interesting insight into how an individual's fitness moderates  
242 the walking cadence required to achieve 40 %  $\text{VO}_2\text{R}$ . Those with a higher  $\text{VO}_2\text{max}$  need a higher  
243 walking cadence to achieve 40 %  $\text{VO}_2\text{R}$  (Figure 2). For example, an individual whose  $\text{VO}_2\text{max}$  is 50  
244  $\text{mL}\cdot\text{kg}^{-1}\cdot\text{min}^{-1}$  needs to walk at an estimated cadence of 141  $\text{steps}\cdot\text{min}^{-1}$  when wearing an Apple Watch  
245 on their right wrist to achieve 40 %  $\text{VO}_2\text{R}$ . In contrast, an individual whose  $\text{VO}_2\text{max}$  is 30  $\text{mL}\cdot\text{kg}^{-1}\cdot\text{min}^{-1}$   
246 can walk at a cadence of 131  $\text{steps}\cdot\text{min}^{-1}$  to achieve 40 %  $\text{VO}_2\text{R}$ . A similar effect is observed  
247 with the Apple Watch worn on the left wrist. However, while these walking cadence predictions are  
248 most probable for predicting 40 %  $\text{VO}_2\text{R}$ , uncertainty in the predictions of %  $\text{VO}_2\text{R}$  are high, with a  
249 95% chance that the true %  $\text{VO}_2\text{R}$  predicted by walking cadence is 40 %  $\text{VO}_2\text{R} \pm 18\%$  on average.  
250 Sex differences in predicted %  $\text{VO}_2\text{R}$  in relation to walking cadence are displayed in Table 3 and  
251 Figure 3. Sex did not improve either data fit (Bayesian  $R^2$ ) or out of sample prediction (LOO). While  
252 predictions from the model showed that the same walking cadence produced lower %  $\text{VO}_2\text{R}$  on  
253 average for males compared to females, the credible intervals suggested these differences are highly  
254 uncertain.

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256 FIGURE TWO ABOUT HERE

257 TABLE THREE ABOUT HERE

258 FIGURE THREE ABOUT HERE

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260 The Bayesian two sample t-test used to estimate differences between walking cadence estimated to  
261 elicit 40 %  $\text{VO}_2\text{R}$  and the recommendations from the review by Tudor-Locke (2018) produced very  
262 large standardised differences. There was a very high probability of the true difference being greater  
263 than 37  $\text{steps}\cdot\text{min}^{-1}$  for both the right (99 %) and left (100 %) wrists.

264

265 **Discussion**

266 The major finding of the current study is that when measured using a modern wearable activity  
267 tracker, the walking cadence required to reach the lower bound of moderate-intensity physical activity  
268 (40 %  $\text{VO}_2\text{R}$ ) is substantially higher than previously reported. The estimated walking cadences of 140  
269 and 138  $\text{steps}\cdot\text{min}^{-1}$  reported here are approximately 40 % higher than the current  $\geq 100$   $\text{steps}\cdot\text{min}^{-1}$   
270 recommendations for walking cadence required to elicit moderate-intensity (Tudor-Locke et al.,  
271 2018). These walking cadences of  $\sim 140$   $\text{steps}\cdot\text{min}^{-1}$  translate into approximately 4000 steps over a 30-  
272 minute duration. Moreover, the walking cadence required to achieve moderate-intensity physical  
273 activity is moderated by fitness status, such that those with lower fitness can walk at a slower cadence  
274 to achieve moderate-intensity. These are important findings for adults using a wearable device to  
275 monitor their physical activity and for those exercise professionals prescribing both individualized and  
276 population-based physical activity based on data from a wearable device such as the Apple Watch.

277 Our results have important implications for public health messages that use step count to  
278 promote physical activity to improve health outcomes associated with a range of chronic diseases. A  
279 number of campaigns promote a step count, typically 10,000 for adults, that should be reached as a  
280 daily target to improve health (Le-Masurier, Sidman, & Corbin, 2003; Tudor-Locke & Bassett, 2004).  
281 Based on the results of the current study it is clear that target step counts alone do not necessarily  
282 translate into criterion measures of physical activity intensity prescribed in guidelines (Tudor-Locke et  
283 al., 2011). There is no doubt that there would be some benefit from reaching step count targets  
284 associated with public health campaigns for many, given that we know that the greatest improvements  
285 in mortality are seen in those who move from being inactive to active (Blair et al., 1995; Paffenbarger  
286 et al., 1993). However, the data from the present study would suggest that some people working  
287 towards these population-based step count targets might not be completing physical activity at a high  
288 enough cadence to meet the moderate-intensity guidelines to maximize health outcomes. Although  
289 some benefit for the individual is expected even from lower-intensity physical activity (below 40 %  
290 HRR) (Carson et al., 2013; Pruitt et al., 2010), our results have important implications for goal setting,  
291 individualized prescription and managing expectations of the associated changes to health parameters  
292 and fitness levels for both the individual and exercise professional.

293 The implications from our results are numerous. First, the feedback provided to users of  
294 activity trackers needs to include a measure of intensity, rather than step count alone. This feedback  
295 should be individualized based on the physiological response and educate the user concerning the  
296 walking cadence required to reach (at a minimum) the lower bound of moderate-intensity. Second,  
297 public health recommendations need to go beyond daily step count targets to include targets based on  
298 walking cadence (intensity). Lastly, the current suggestion that a walking cadence of approximately  
299 100 steps·min<sup>-1</sup> will allow most people to achieve moderate-intensity physical activity (Tudor-Locke  
300 et al., 2018) appears to be a substantial underestimation. Our study, using directly measured VO<sub>2</sub>R,  
301 clearly shows that even in those with lower fitness (~30 mL·kg<sup>-1</sup>·min<sup>-1</sup>), approximately 130 steps·min<sup>-1</sup>  
302 would be required to reach the lower bound of moderate-intensity physical activity. It must be said  
303 that the value of 100 steps·min<sup>-1</sup> recommended by Tudor-Locke et al. (2018) is clearly a mean and  
304 therefore masks the normal distribution of walking cadences between individuals.

305 Our study is not without limitations. The Apple Watches used in our study were first  
306 generation (Series 0) devices running watchOS 2.0.1, and therefore might not represent the capability  
307 of the most recent Apple Watch released (Series 4). That being said, it is not clear how the latest  
308 Apple Watch would produce different walking cadence values compared to the Series 0 device used  
309 here as the step count measured by pre-Series 4 Apple Watches has been reported to have high  
310 agreement and low (< 2 %) mean absolute percent error compared to manually counted steps  
311 (Fokkema, Kooiman, Krijnen, Van Der Schans, & De Groot, 2017; Veerabhadrapa et al., 2018). We  
312 also relied on the Apple Watch for our step count values rather than manually counting steps.  
313 Although we did this in order to examine the ‘real world’ relationship between walking cadence as  
314 measured by a wearable device and VO<sub>2</sub>R, our results need to be interpreted in light of this. However,  
315 the studies cited above (Fokkema et al., 2017; Veerabhadrapa et al., 2018) suggest that the  
316 relationships we report here should not be affected substantially by using walking cadence as  
317 measured by the Apple Watch rather than manually counted steps. Bunn, Jones, Oliviera and Webster  
318 (2019) reported that the Apple Watch meets the Consumer Technology Association standard for both  
319 walking and running, with a mean absolute percentage error of < 4 % compared with manually

320 counted steps. This study was also carried out under controlled laboratory conditions, and therefore  
321 the relationships we report here may differ compared to those under free-living conditions and  
322 warrants further investigations. Future research now needs to examine how consumer wearable  
323 devices might help and/or guide the user to achieve individualised intensity targets. This might include  
324 using a combination of both volume (total steps) and relative intensity (% HRR), such that people are  
325 encouraged to move more but also to reach a target step count at a relative intensity high enough for  
326 the individual to achieve substantial health benefits.

327

### 328 **Conclusion**

329 Our study, using directly measured  $\text{VO}_2\text{R}$ , shows that individuals with moderate levels of fitness  
330 require approximately  $140 \text{ steps}\cdot\text{min}^{-1}$  to reach the lower bound of moderate-intensity physical activity  
331 ( $40\% \text{VO}_2\text{R}$ ). Moreover, the walking cadence required to achieve moderate-intensity physical activity  
332 is moderated by fitness status, such that those with lower fitness can walk at a slower cadence to  
333 achieve moderate-intensity. Consequently, the public health recommendation that walking at  $\sim 100$   
334  $\text{steps}\cdot\text{min}^{-1}$  will allow most people to reach moderate-intensity substantially underestimates the  
335 required walking cadence required to maximize health outcomes. Therefore, step count should be used  
336 in conjunction with a suggested walking cadence (intensity) based on an individual's fitness status to  
337 improve the tailoring of this public health message.

338

### 339 **Acknowledgements**

340 None.

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471 **Table and figure legends**

472

473 Table 1. Demographic data for all participants and also separately for female and male.

474

475 Table 2. Mean (*s*) walking cadence measured by Apple Watch on left and right wrists together with  
476 the mean (*s*) directly-measured % VO<sub>2</sub>R during 5-min stages of treadmill walking.

477

478 Table 3. Predicted % VO<sub>2</sub>R (95% credible interval) for female and male participants for a range of  
479 walking cadence values. Data were generated by Apple Watch's worn on the left and right wrists.

480

481 Figure 1. The curvilinear relationships observed between walking cadence estimated by Apple  
482 Watches worn on the left and right wrists and %  $\text{VO}_2\text{R}$ . Grey shaded area is the 95 % credible interval.

483

484 Figure 2. The effect of fitness status ( $\text{VO}_2\text{max}$ ) on the curvilinear relationship observed between  
485 walking cadence estimated by Apple Watch worn on the right wrist and %  $\text{VO}_2\text{R}$ . Grey shaded areas  
486 are 95 % credible intervals.

487

488 Figure 3. The effect of sex (female/male) on the curvilinear relationship observed between walking  
489 cadence estimated by Apple Watch worn on the left and right wrist and %  $\text{VO}_2\text{R}$ . Grey shaded areas  
490 are 95 % credible intervals.

491