

Personalized Rehabilitation Recognition Model upon ANFIS

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Abstract

This study applied the Adaptive Neuro-Fuzzy Inference System (ANFIS) to design a recognition model of personalized rehabilitation. In the model, the user may take a wearable sensor and follow the assigned joint-relax exercise to measure the motions of the upper limbs. The sensor that is embedded with the chips of accelerometer, gyroscope, and inclinometer produced the sample datasets due to the exercise schedule of physiotherapy assignment. All motion samples were labeled by arbitrary numbers, which can be identified to the specific motion, for the data training process. A Fuzzy Inference System (FIS) was initially designed by the steps of data pre-processing, featuring, fuzzifying, and ruling Fuzzy logics according to the sample datasets. The FIS was then trained by the ANFIS for optimization by tuning parameters of the features. In testing, the accomplished FIS could recognize the motion features by the defuzzifier that infers the label corresponding to the motion. As a result, the average recognition rate was higher than 90% when the testing motions followed the sampling schedule of the physiotherapy assignment. The model can be applied in the ubiquitous healthcare measurement for health services. The professionals can assess whether the subject obeyed the assigned program or not based on detail motions of the exercise. This approach can be enabled on the trackable interface for the physiatrists to screen the motions of routine rehabilitation.

Keywords: ANFIS, physiotherapy, rehabilitation recognition, sensor-enabled wristband, ubiquitous healthcare

1. Introduction

The physiotherapy provides the rehabilitation program for the patients who are weakened on motions. The therapeutic exercise is thus designed to flex the joints of their injured limbs. The physical therapists scheme the rehabilitation programs including the joint kinematics for those disabled parts, e.g. flexion, extension, abduction, adduction, pronation, supination, rotation, and deviation [1]. Many clinical studies of healthcare services advised that the routine exercises with a scheduled rehabilitation period are helpful in healing [2]. The physiatrists request daily practice at home, or with facilities in the hospital, for the patients and observe their performance to adjust the health promotion program of joint motions.

The modern healthcare services with internet technique offered Ubiquitous Healthcare Measurement (UHM) for patients to support self-management for homely rehabilitation. The physiatrists are able to screen the daily records of the patients via the UHM for evaluating whether the assigned exercise needs progressive revision or not [3]. The UHM enables rehabilitation in a wireless area network by wearing non-imaging monitoring devices to record the motion data of patients with privacy [4-5]. Therefore, a wristband with accelerometer and gyroscope was widely used to detect human activities such as housekeeping, falling, walking, and sporting in recent years [6]. With Bluetooth technology, the sensor wristband can efficiently transport the measurement data to a smartphone for the UHM. The personalized rehabilitation data can be measured by a Bluetooth sensor and be recognized by the proper algorithms for management [7-8].

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For the study of activity recognition, the algorithms involving Artificial Neural Network (ANN), Backward Propagation Neural Network (BPNN), Fuzzy logic theory, etc. are popular for computation. The rule-based Fuzzy Inference System (FIS) is quite appropriate for the tendency of stationary motions (e.g. rehabilitation) [9]. A Fuzzy set involves Membership Functions (MFs) to fuzzify the input and output features; then, the logic rules based on if-then syntax are scripted to defuzzify the MFs for inference (i.e. defuzzification) [10-11]. In the FIS, the Mamdani and Sugeno models perform two MF types, which the MFs of output features are respectively formatted by geometrical-shape functions and linear-expression crisps [12-13]. The Adaptive Neuro-Fuzzy Inference System (ANFIS) enables a data training process to adjust the FIS parameters for improving the inference capability [14]. In general, the FIS was suggested to recognize the inferable features of the rehabilitation exercises in the UHM.

This study suggested a prototype of the rehabilitation model, which applied ANFIS to recognize the personalized motions. A wearable sensor compliant with Bluetooth protocol was employed to collect data. The ANFIS enables an adaptive data training process based on the Fuzzy logic rules to achieve personalized recognition.

2. Methodology

The proposed model requests the ANFIS to recognize the rehabilitation exercises. The user wears a Bluetooth-compliant sensor JY-61 that embeds the chips of accelerometer, gyroscope, and inclinometer into the device to detect 3-axis components of accelerations, angular velocities, and tilt angles, respectively.

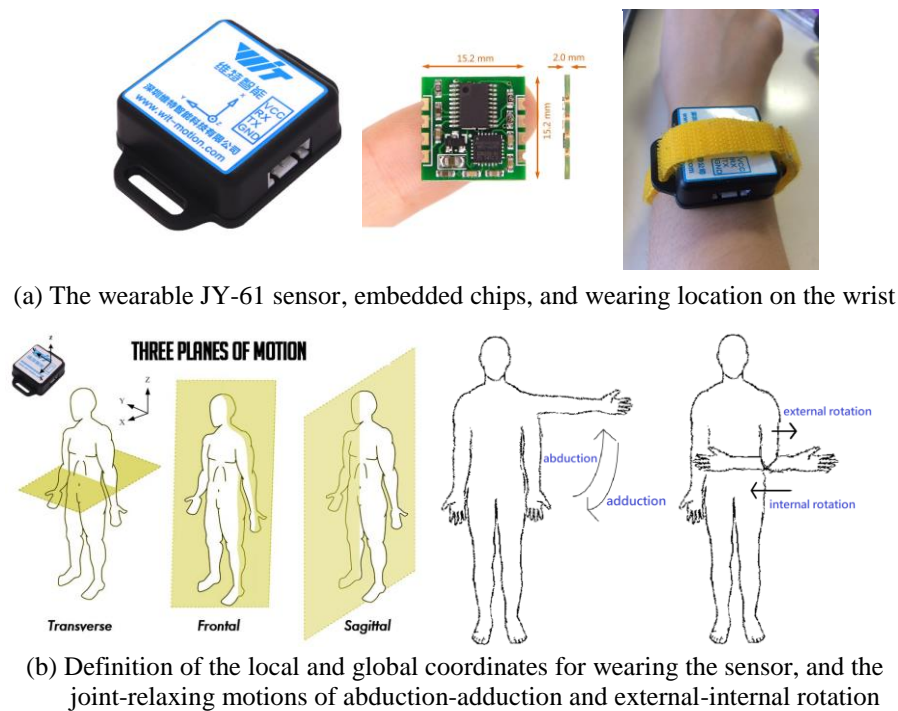
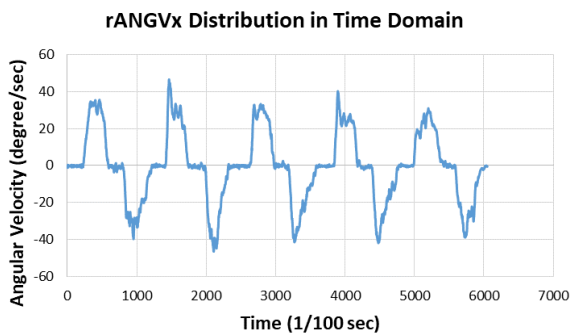


Fig. 1 Prepared instrument and exercises for the personalized rehabilitation recognition

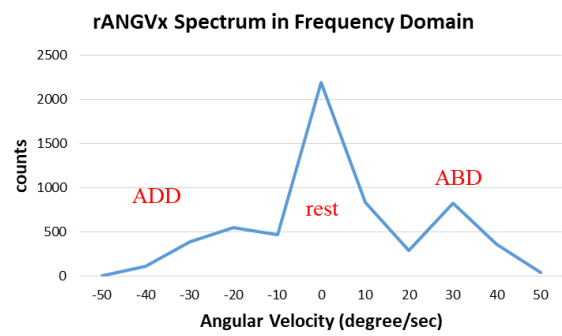
2.1. Exercise design

We took three rehabilitation exercises as an example, in which the user wore the sensor on the wrist in the measurement. The sensor was able to send 100 datasets of signals per second. As shown in Fig. 1, the neutral position of the human body is the global coordinate, and the center of the sensor is the local coordinate. The motions of the exercise were designed by global coordinates, but the sensor signals were measured in local coordinates. When the exercise was activating, the sensor data were corresponding to the initial position of the sensor. Two exercises including abduction, adduction, and rotation of the shoulder and elbow were applied to measure the range of motion regarding the upper-limb joints. For the exercises addressed below, the sensor was worn on the wrist and each exercise cycle was repeated five times.

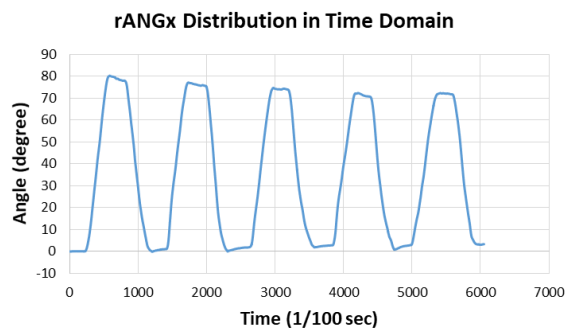
with the proper MFs can yield a Fuzzy set available for the same output motions. The MFs of output feature, which is initially designed as the Mamdani-type function, must be converted to the Sugeno-type crisp set before the training process in the ANFIS. Besides, the amount of the output crisps for the Sugeno-type Fuzzy set must be a multiplication of those in the input features.



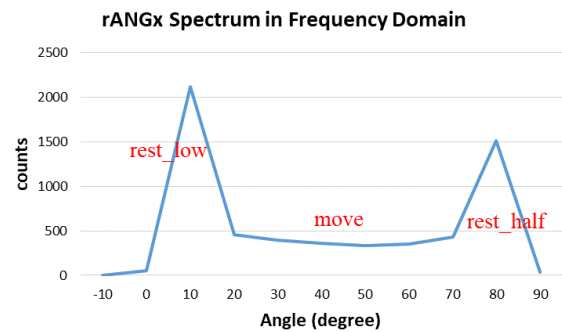
(a) The feaure rANGVx in time-domain distribution



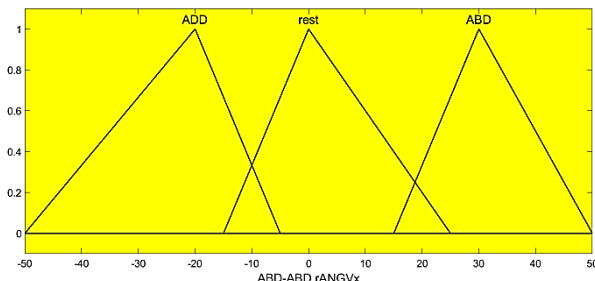
(b) The feature rANGVs in frequency-domain spectrum



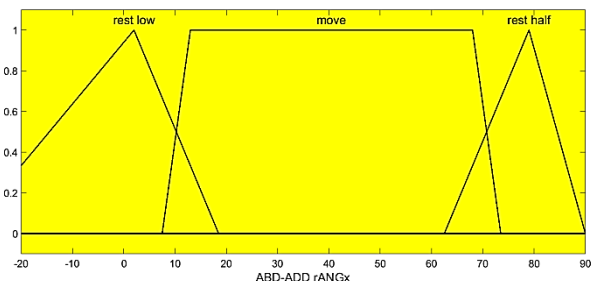
(c) The feaure rANGx in time-domain distribution



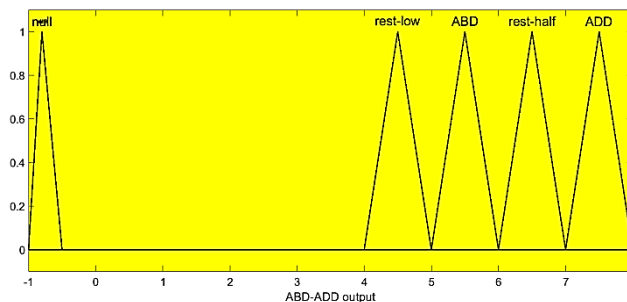
(d) The feature rANGs in frequency-domain spectrum



(e) The MFs of rANGVx feature



(f) The MFs of rANGx feature



(g) The MFs of ABD-ADD output feature

Fig. 3 Example of data transform between time and frequency domains for the features of the shoulder exercise

(d) We defined the if-then-based Fuzzy rules to control the logic of input and output features in each cyclic epoch. With the rules, the input MFs indicate the consistent output MFs, while the number of the output MFs and the rules must be identical. For an example of the FIS structure of the abd-add motions, we created five dummy rules that represent five virtual motions and designed four rules that satisfy four real motions. The initial FIS will be tuned by the ANFIS, which applies the method

of Root Mean Square Errors (RMSE) in a data training process, to optimize the MF parameters of the FIS for each epoch.

(e) We defuzzified the trained FIS with the capable MFs and the Fuzzy rules to infer the motion labels in recognition. The process of defuzzification computes participation degrees of the input MFs based on the rules. The test datasets were employed for evaluation. The inferred motion labels were compared with the assigned schedule to evaluate if they are indexed in the expected motion range. We proposed a quartile motion-label scheme to verify the recognition rate of the FIS. The scheme splits the data distribution of motion into four sets (i.e. cut at 25%, 50%, 75%), and it evaluates the accuracy of each quartile set. The sets of 25% and 75% are usually counted as changing the motion, while the data set around 50% (i.e. the middle portion) can be a confidence interval of the reliable motion labels.

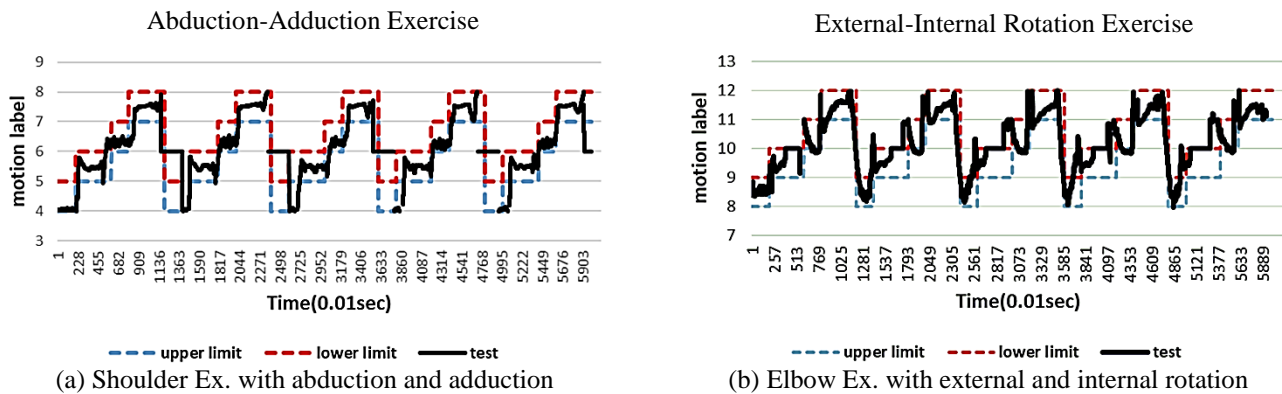


Fig. 4 The inference diagrams of the test data versus the sampling schedule

3. Results and Discussion

The trained FIS models of the exemplified exercises were evaluated by applying the test datasets. The diagrams of both exercises as shown in Fig. 4 compare the labeled test data with the inferred motion labels. The inferred motion labels are observed to fit within the defined range if the motion cycles follow the schedules. The inference diagram displays a visualized chart of both inferred and scheduled motions to track the measurement. When the inferred motion labels were not shown in the range of scheduled motion labels, it would report the outlier movements with respect to the assigned motions. The user is able to obtain a personalized FIS model that is trained by the sample dataset based on the guideline for recognition in measurement. The healthcare professionals can assess rehabilitation performance for improving the therapeutic procedure.

Table 1 The recognition rates based on quartile scheme for the test data of scheduled exercises

Shoulder Ex with abduction-adduction			
motion	25%	50%	75%
rest_low	1	0.97	1
ABD	1	1	0.8
rest_half	1	1	1
ADD	0.87	1	1
average	0.97	0.99	0.95
Elbow Ex with external-internal rotation			
motion	25%	50%	75%
rest_inside	1	1	1
ER	1	0.41	0.03
rest_outside	1	0.38	0.03
IR	0.71	1	0.87
average	0.939	0.70	0.48

The recognition accuracy of the chosen motions was evaluated by the quartile schemes as shown in Table 1. The outlier data were aware of moving too fast, which may lead to the angular velocity over the maximum of sample data. The average rates of recognition for the Shoulder Ex, which performed steady motions by the schedule, were about 0.99 due to the middle

(50%) of the quartile scheme. The rates of the Elbow Ex, which did not move stably from external to internal rotation and probably caused data shifts, were ranged from 0.93, 0.70, and 0.48 with respect to 25%, 50%, and 75% portions. This evaluation suggests that the middle of motion data is acceptable for recognition.

We further verified classification performance by combining both exercises and retrieving the middle section of motion data in every second. The subject can randomly choose either shoulder or elbow exercises, but the movement should follow the guide as the best for validation. The sensitivity, specificity, and accuracy of the shoulder exercise are calculated as 0.942, 0.998, and 0.951, respectively; while they reached 0.995, 0.614, and 0.703 for the elbow exercise.

3.1. Benefits

The proposed model follows the process of the supervised algorithm in machine learning to label the motion data based on the scheduled exercise. With the ANFIS, it is available for generating a personalized model of rehabilitation recognition. The proposed Bluetooth-compliant sensor is able to provide plentiful sample datasets in the training procedure. The personal movement features can be chosen to initialize the MFs of FIS with the Fuzzy rules for data training in the ANFIS process. Our approach suggests a confidence interval of the motion to extract proper data, e.g. the middle of each scheduled motion period. The model is achievable for recognizing rehabilitation exercises in healthcare, which is enough for practical application [15].

3.2. Limitations

The same feature can measure a variety of exercises within the same range of motions, e.g. the features “rANGVx” and “rANGx” for both of the shoulder and elbow exercises in this study. However, they cannot be combined in an exercise by a unique FIS. Therefore, the user needs to wear more sensors for measuring this complex exercise. In addition, the sensor usually detects unstable noises for irregular motions, which the features are ambiguous in recognition. If the user does not follow the exercise schedule and the tracking data are probably shifted, the measurement is not reliable for the report. In rehabilitation, the physiotherapist used to design simple exercises for the patient.

4. Conclusions

We applied the ANFIS to establish a recognition prototype of personalized rehabilitation model for ubiquitous healthcare measurement in this study. The Bluetooth-compliant sensor embedded with the chips of the accelerometer, gyroscope, and inclinometer can be worn to measure the motion data of the rehabilitation exercises. The model presents two exercises with joint-relax motions for the shoulder and elbow. In which, the user wore the sensor on the wrist and obeyed the motion schedule to move the limbs. Each motion dataset is labeled by an arbitrary number within a defined range. An initial FIS with the Fuzzy logic rules was created by the sample datasets; then, the steps of data preprocessing, feature visualizing, fuzzifying, data training, and defuzzifying were processed in the ANFIS. The ANFIS repeated the data training cycles to accomplish the trained FIS, which can defuzzify the test data upon rule-based Fuzzy logics to infer the motion labels and recognize the exercise. In approach, the average recognition rate due to the quartile motion-labels scheme was higher than 90% if the user faithfully followed the assigned schedule. This approach can be promoted to the UHM for comprehensive health services in the future.

Conflicts of Interest

The authors declare no conflict of interest.

Acknowledgement

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