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1 Wireless power transfer using relay resonators

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6 This paper presents an advanced design configuration of a wireless power transfer system using
7 overlapping relay coil techniques for free loading position. The work undertaken investigates the
8 tuning position of prototype relay coils in a horizontal configuration in order to evaluate power
9 transfer efficiency versus increasing operating distance between the transmitter and receiver coils.
10 A prototype relay coil system was evaluated to determine the optimum distance between the
11 transmitter and receiver. Finite element magnetic simulation was used to appraise the magnetic
12 field distribution and power transfer efficiency with respect to a strongly coupled magnetic
13 resonance condition. Experimental and simulation results analysis suggest that the proposed design
14 could achieve 85%–90% efficiency within a 4 cm operational distance. Finally, the experimental
15 results were analyzed and compared with the simulation results. *Published by AIP Publishing.*

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16 Wireless Power Transfer (WPT) is now ubiquitous fol-
17 lowing on from developments at MIT (Massachusetts
18 Institute of Technology), i.e., approximate 60 W of power
19 was transferred between two 60 cm diameter coils which
20 were separated by a distance of 2 m.¹ WPT systems are now
21 used for powering electronic devices such as wireless charg-
22 ing, radio frequency identification devices (RFIDs), sensor
23 networks, medical implanted devices (cardiac pacemakers),
24 electric vehicles, maglev trains, and many more.^{2–4}

25 WPT can be classified as non-radiative or radiative
26 based on the system implemented in the power transfer pro-
27 cess. The non-radiative type refers to near-field power trans-
28 fer and it is applied in short or medium ranged applications
29 where the operational distance is below the transmitted
30 signal wavelength. Additionally, the transmitter-receiver dis-
31 tance of the short-ranged application is less or equal to the
32 diameter of the transmitter coil. Capacitive and inductive
33 coupling power transfer methods are forms of the short-
34 ranged applications. The inductive coupling technique
35 function on the principle of magnetic induction, i.e., a trans-
36 mitting coil induces an EMF within the receiver coil via a
37 magnetic field variation. The operational frequencies of a
38 WPT system depend on the inductance and capacitance val-
39 ues of the coils. For capacitive coupling, energy is trans-
40 ferred through an electric field, the quantity of energy
41 transferred being directly proportional to the frequency.^{5,6}
42 For medium range applications, the transmitter-receiver dis-
43 tance varies between one to ten times the diameter of the
44 transmitter coil with an operational frequency range of
45 10 kHz–200 MHz. An inductively coupled system using mul-
46 tiple coils as advantages over other systems (non-multiple
47 coils) by the extension of the power transfer distance
48 between the transmitter to receiver. The coupled magnetic
49 resonance system (CMRS) and inductive power transfer
50 method are forms of the medium ranged applications.^{5,6} The
51 MIT research group described the detailed working principle

of CMRS system.⁷ This radiative type is known as far-field
power transfer. However, the operational distance is two
times higher than the transmitted signal wavelength. Its
implementation is based on electromagnetic wave propaga-
tion in far field distance usually in the range of kilometers.
Essentially, it exists in two forms: directive and non-
directive. Currently, the directive form is used for remotely
powering electric vehicles (evs), and the non-directive form
is used in applications such as power transfer between omni-
directional RF broadcast and portable devices, transfer of
optical power through laser beams, and other applications.⁶
There have been several studies over the last few years to
enhance the efficiency of the WPT system for short, medium,
and long distances using relay resonators between the trans-
mitter and receiver coils.^{5–24} For example, Choi and Lee⁵
investigated the optimal position of relay coils from the
tested measured results without verifying the experimental
results with theory or simulation. In another paper, Ahn and
Hong³ demonstrated the WPT for multiple loads over vari-
ous distances and verified the optimum conditions with mea-
sured results. Park *et al.*⁸ discussed the magnetic field
repeater concept for the maximum power transfer for the
wireless system and provided the guidelines to select the
optimum repeater positions and number between the trans-
mitter and receiver. They verified their concept experimen-
tally and found that this concept could double the coupling
coefficient between the transmitter and receiver circuit.
However, it was observed that the coupling was not consid-
ered for nonadjacent and adjacent cases. Zhang *et al.*¹⁰ stud-
ied relay coupling but did not demonstrate the optimal power
transfer efficiency at the resonance frequency due to the
effect of nonadjacent coupling. Therefore, prior research in
this field discusses the theoretical background and investi-
gates the performance of a test prototype without magnetic
simulation or verification of experimental results with simu-
lation. An exception to this is the work of Zhang *et al.*¹¹ who
simulated the magnetic WPT system using simple transmit-
ter and receiver coils and verified the simulated results with
measured results. However, Zhang *et al.*¹¹ did not use relay

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91 resonators or repeaters to extend the wireless power transfer
 92 distance between the transmitter and receiver. Magnetic simu-
 93 lation for a magnetic WPT system is necessary to be able to
 94 appreciate the optimum size and flux linkage of the transmitter
 95 and receiver resonators as the magnetic coupling and the reso-
 96 nance condition are the main factors in achieving the maxi-
 97 mum power transfer. This paper presents the design concept of
 98 an overlapping relay resonator structure in horizontal configu-
 99 re for WPT as opposed to the previous nonoverlapping
 100 technique of vertical and horizontal relay resonators. This
 101 design is particularly beneficial for low power medical applica-
 102 tions and also for free loading mobile charging applications. In
 103 development, this design concept was simulated using the
 104 FEA magnetic simulation software package to aid understand-
 105 ing of the flux linkage and magnetic coupling factor of the
 106 structure. An experimental circuit prototype was built and
 107 tested using off-shelf components in order to acquire experi-
 108 mental data relating to the performance and operational wire-
 109 less power transfer distance limit. The simulated power
 110 transfer efficiency with the variation of distance was compared
 111 and verified. Finally, the efficiency comparison between this
 112 study and other prior studies are discussed with conclusions

$$R_{TX} = R_{tx} + R_s \quad R_{RX} = R_{rx} + R_L.$$

113 A typical induction coupling WPT consists of a trans-
 114 mitter and a receiver circuit, as shown in Fig. 1. The circuit
 115 generates and transfers electrical energy between two reso-
 116 nant coils through varying magnetic fields. Since both coils
 117 are closely coupled and operate at the same resonant fre-
 118 quency, high energy transfer can be achieved with small
 119 leakage. This magnetic resonance coupling can be applied
 120 between one transmitting coil and many receiving coils for
 121 concurrent charging the multiple devices.⁷ The resonant fre-
 122 quency of the system can be calculated from $f_0 = \frac{1}{2\pi\sqrt{LC}}$,
 123 where L and C represent the inductive and capacitive quanti-
 124 ties of the circuit. k is the coupling coefficient between the
 125 transmitter circuit and receiver circuit. V_s is the source of
 126 power for the transmitter circuit, R_s is the resistance of the
 127 source, R_{tx} is the resistance in the transmitter circuit, R_{rx} is
 128 the resistance in the receiver circuit, R_L is the load, C_1 is the
 129 series connected transmitter capacitance, C_2 is the series
 130 connected receiver capacitance, L_{TX} is the inductance in the
 131 transmitter circuit, and L_{RX} is the inductance in the receiver
 132 circuit. The system's mutual inductance, i.e., where the mag-
 133 netic field generated by a coil causes voltage induction in the
 134 coil adjacent, is found via¹²

$$M = k\sqrt{L_{TX}L_{RX}}, \quad (1)$$

135 where the coupling coefficient, k , between the adjacent coils
 136 has been defined as¹⁸

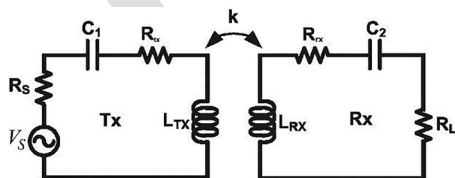


FIG. 1. Equivalent circuit model of the transmitter-receiver WPT system.

$$k = \frac{1}{\left| 1 + 1.6 \left(\frac{h^2}{r_t * r_r} \right)^{\frac{3}{2}} \right|}, \quad (2)$$

where h is the center to center distance between adjacent
 coils, r_t is the transmitter coil radius, and r_r is the receiver
 coil radius. It is necessary to match the load impedance with
 the source impedance to transfer maximum power at the load
 end. Since both the magnetic field strength and coupling fac-
 tor gradually decrease with the distance, the power transfer
 distance of a magnetically coupled WPT system will depend
 on the size and properties of the magnetic material and the
 coil dimensions. High Q-factor transmitter and receiver coils
 could compensate the low magnetic coupling to increase the
 power transfer distance to a certain degree. However, an
 excessive Q-factor could represent excessive reactance for
 each load resulting in an increase of the existing magnetic
 field which could pose a risk to body tissue. The relay coils
 implementation as shown in Fig. 2 could be a suitable option,
 i.e., to improve the magnetic coupling over a longer distance
 which will increase the power transfer distance from the
 transmitter to the receiver end.

It can be seen from the schematic circuit in Fig. 2 that
 the typical relay coil WPT comprises of basic transmitter
 and receiver circuit with n number of resonators.

The transformer coupling principle proposes that the
 product of capacitance and inductance in circuit must be the
 same to have a resonant circuit¹⁰

$$f_{TX} = f_1 = f_2 = f_3 = f_4 = f_5 = f_6 = f_7 = f_{RX}, \quad (3)$$

$$L_{TX} \times C_1 = L_A \times C_3 = L_A \times C_3 = \dots \dots \dots L_{RX} \times C_2. \quad (4)$$

The wireless system power transfer efficiency is described as
 the ratio of the power dissipated at the load to the power
 input to the transmitter and is derived by summing the total
 dissipated power in the coils and the load.¹²

Applying Kirchhoff's voltage law to solve the circuit,
 the power transfer efficiency is given by⁹

$$\eta = \frac{P_L}{P_{in}}, \quad (5)$$

$$\eta = \frac{\frac{1}{2}R_L|I_n|^2}{\frac{1}{2}R_{tx}|I_{tx}|^2 + \frac{1}{2}R_a|I_1|^2 + \dots + \frac{1}{2}R_{n-1}|I_{n-1}|^2 + \frac{1}{2}(R_L + R_n)|I_n|^2} = \frac{R_L}{R_{tx} \left| \frac{I_{tx}}{I_n} \right|^2 + R_a \left| \frac{I_1}{I_n} \right|^2 + \dots + R_{n-1} \left| \frac{I_{n-1}}{I_n} \right|^2 + (R_L + R_n)}$$

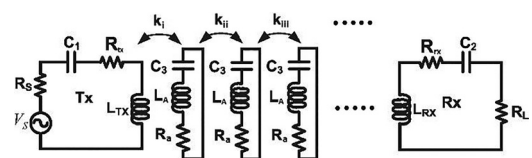


FIG. 2. Equivalent circuit model of the WPT system with n resonators.

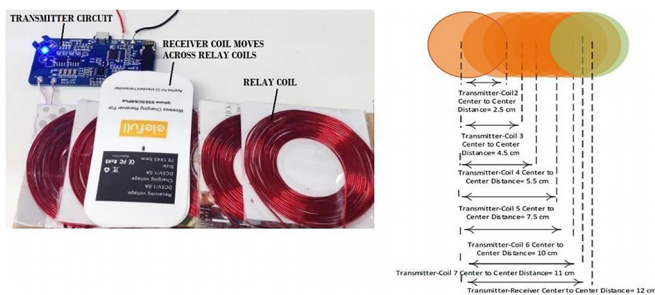


FIG. 3. Practical setup of the horizontal design for wireless power transfer.

167 The current ratio $\frac{I_n}{I_n} \dots \frac{I_{n-1}}{I_n}$ can be realized using inverse
 168 matrix on the resolved matrix form of the circuit. Therefore,
 169 $\eta = f(C_3, \dots, C_2, R_L)$. It should be noted that C_1 and R_s are
 170 related to impedance matching and not the power transfer
 171 efficiency. So, for maximum power transfer analysis, realiza-
 172 tion of C_3, \dots, C_2, R_L are critical.

173 Figure 3 shows the prototype of the relay coils WPT sys-
 174 tem which was built using off-shelf components and charac-
 175 terized experimentally. The design is implemented using
 176 seven overlapping relay coils alternately placed at approxi-
 177 mately center to center distances as shown.

178 Essentially, 3-D FEA magnetic transient simulation
 179 using Infolytica package was carried out to determine the
 180 flux linkage and power transfer efficiency over the distance.
 181 Finally, the measured results were analyzed and discussed
 182 with the simulation results.

183 The components used to implement the WPT system
 184 include commercial Qi transmitter and receiver. The trans-
 185 mitter circuit consists of an inverter circuit integrated with a
 186 ferromagnetic transmitter coil. The maximum input voltage
 187 of the transmitter circuit is 5 V (dc) recommended by the
 188 manufacturer, and the output of the inverter will provide
 189 50 mV (rms) sinusoidal voltage to the transmitter coil for
 190 magnetic induction.¹³ The receiver comprises of a copper
 191 coil, a ferromagnetic layer, and the rectifier circuit;¹³⁻¹⁵ relay
 192 coils are made of copper having 20 number of turns which
 193 have been tuned at a resonance frequency to maximize the
 194 power transfer. The operation of wireless power transfer sys-
 195 tem at the resonant frequency is necessary to achieve the
 196 maximum output power and efficiency. The resonant fre-
 197 quency of the transmitter and receiver circuit is 220 kHz, and
 198 the relay coils are tuned with this frequency to achieve the
 199 maximum efficiency. The distance of the each relay coil
 200 from the transmitter circuit, as shown in Fig. 3, is the

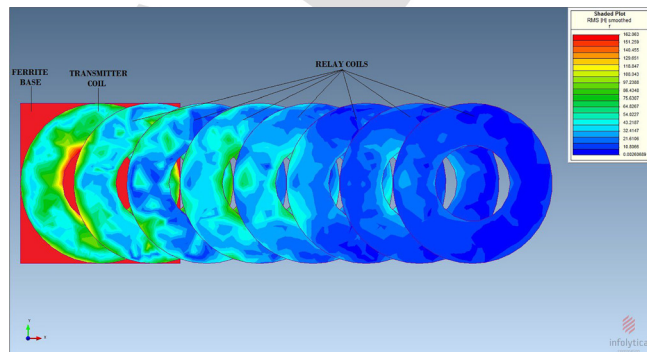


FIG. 4. 3-D transient simulation model of the WPT system.

TABLE I. Coil parameters used in simulation.

	No. of turns	Resistance (mΩ)	Inductance (μH)	Inner radius (cm)	Outer radius (cm)
Transmitter coil	10	180	24	1.2	2.3
Relay coils	20	232	24	1.5	3
Receiver coil	35	135	8	1.1	2.2

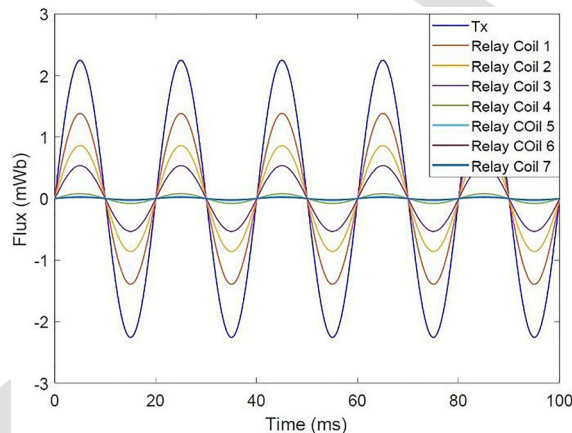


FIG. 5. Effective flux linkage for all the coils.

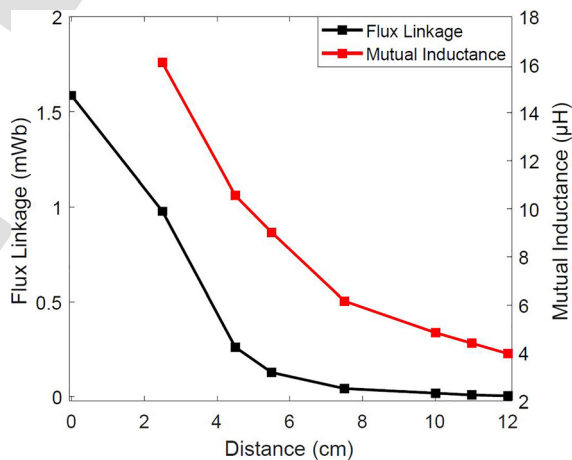


FIG. 6. Flux linkage and calculated mutual inductance over operational distance of the relay resonators.

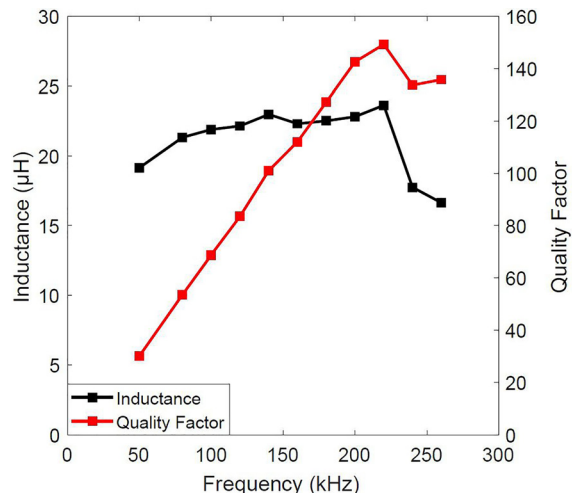


FIG. 7. Relay coil inductance values and quality factor with the variation of frequency.

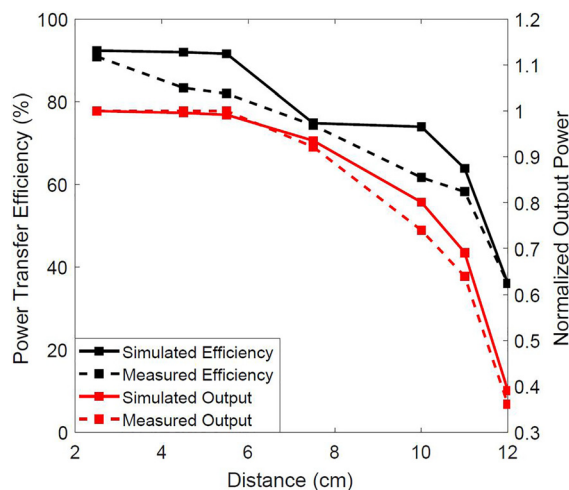


FIG. 8. Measured and simulated output power and efficiency of the relay coils.

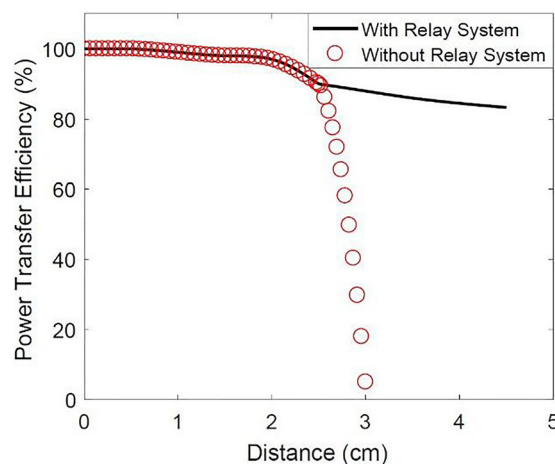


FIG. 9. Measured and simulated output power.

201 optimum distance for this configuration, i.e., that would
202 allow connectivity and transmission to subsequent coils.

203 Figure 4 presents the descriptive model of WPT system
204 with relay coils which has been used in the finite element
205 magnetic simulation. The first coil integrated with the ferrite
206 material is the transmitter coil, and the subsequent coils are
207 the relay coils. Table I shows the coil parameters used in the
208 simulation. The transmitter coil is driven by a sinusoidal
209 voltage source with the magnitude of 50 mV (rms) at 50 Hz
210 frequency. Figure 5 shows the sinusoidal flux variation over
211 the time period of the WPT system for individual coils. In
212 order to understand the flux linkage over the operational dis-
213 tance, the rms values of the flux linkages were plotted, as
214 shown in Fig. 6. The distance between the center of the
215 transmitter and receiver coils varied due to the change in
216 position of the receiver coil across the relay coils resonator.
217 The distances represent the points where the different relay
218 coils are placed. It can be seen from the graph that the flux
219 linkage decreases near exponentially over distance with the
220 flux linkage dropping by 65% at the 4th coil from the trans-
221 mitter, at the 7th coil, and beyond power transfer is not
222 achievable as the flux linkage reduction is 92%. Initially, the
223 inductance and the quality factor (Q) of the relay coils were
224 measured with the variation of frequencies. Figure 7 shows
225 the measured inductance and the calculated Q factor for 20
226 turn coils. The quality factor, Q, is determined using the

formula $Q = \frac{\omega L}{R}$ from the measured inductance and resistance
values.

229 An LCR meter was used to measure the inductance and
230 resistance of the coils at different frequencies. The coil
231 exhibits a maximum quality factor 150 at 220 kHz frequency.
232 Several relay coils with different number of turns were used
233 in the experiment to evaluate the quality factor variation
234 with frequency.

235 The experimental results suggest that the coil perfor-
236 mance is critically affected by the number of turns and the
237 wire gap of the coil. The coupling factor (k) and the mutual
238 inductance of the WPT system have been evaluated using
239 Eqs. (2) and (1), respectively, to evaluate how they affect the
240 performance of power and efficiency over the distance across
241 the relay coils between 2 cm and 12 cm. It can be seen from
242 Fig. 6 that the mutual inductance is significantly reduced
243 over the operational distance.

244 The transmitter circuit is supplied by a 5 V DC source,
245 and the input/output voltage and power of the WPT system
246 have been measured to characterize the prototype. The mea-
247 sured output power for 2.5 cm and 12 cm distance are 2.5 W
248 and 0.9 W, respectively. Figure 9 shows the measured and
249 simulated normalized output power and power transfer effi-
250 ciency against the different distances/position of the receiver
251 coil across the relay resonators. Measured and simulated out-
252 put powers were normalized based on the maximum simu-
253 lated output power.

TABLE II. Comparison with previous works.

Reference	Coil dimension: r_t , and r_r (mm)	Operating frequency (MHz)	Efficiency without relay coils (%)	Efficiency with relay coils (%)	Operational distance (mm)
Rakhyani <i>et al.</i> ²⁵	32, 11	0.70	28	77%, 2 relay coils	30
Rashid ²⁶	130, 130	38.15	4.5	25%, 1 relay coil 75%, 2 relay coils	1000
Zhang <i>et al.</i> ¹⁰	81, 81	8	10	46%, 2 relay coils	300
Bhutada <i>et al.</i> ²⁷	...	4–12	40	93%, 2 relay coils	500
Zhu <i>et al.</i> ²⁸	23, 22	0.25	15.9	36.3%, 2 relay coils	20
Wang <i>et al.</i> ²⁰	8.5, 6	200	...	30%, 2 relay coils	7
This work	23, 22	0.22	35	85%–90%, 7 overlapping relay coils	27

Figure 8 shows the comparison between measured and simulated power transfer efficiency for the relay coil system. It can be seen that the simulated results are closely matched with the measured results and that the efficiency drops from 90% to 35% over a 10 cm distance. The receiver output power was also measured without a relay coil to evaluate the operational distance and efficiency with and without a relay coil.

Figure 9 clearly indicates that without a relay coil the efficiency will drop from 85% to 0% within very short operational distance of between 2 cm and 3 cm.

Both mutual inductance and the power transferred both decrease with increasing the distance between the transmitter and receiver coils. It can be seen that high power transfer can be achieved with a low source impedance which will provide the low I^2R_s loss in the system.

This study has investigated the tuning position of prototype overlapping relay coils in a horizontal design for distance extension of WPT and evaluated power transfer efficiency with the increase in operating distance between the transmitter and receiver coils.

Table II summarizes the comparison between this study and previous research^{20–23} with and without relay coils and demonstrated that the relay coil WPT system will increase the efficiency significantly compared to a system without a relay coil. However, the efficiency and the operational distance depend on the coil dimension and magnetic material of the transmitter and receiver coils. It can be seen from Table II that the overlapping relay resonators show the highest WPT efficiency compared to the previous findings. Additionally, the overlapping relay coils design of the WPT system would enhance a wide range of applications such as implantable medical devices, i.e., cardiac pacemaker, nerve simulator, and retinal prosthesis with other applications such as wireless charging and wearable sensing devices.¹⁶

The design configuration is simulated using the FEA magnetic software, and the simulated results have been analyzed and compared with the measured results. The measured results suggest that the prototype is capable of achieving 85%–90% efficiency within a 4 cm distance from the transmitter coil. The relay coil resonators have been built and tested for the purpose of extending power transfer. This is particularly beneficial in health and medical applications and also in mobile charging applications due to small power requirements. These areas are undergoing further study. The eventual goal is to optimize the relay coils and transmitter/receiver coils using the magnetic simulation software with the horizontal array configuration. Furthermore, this horizontal configuration is compared with the vertical array configuration to optimize the design.

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