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Biomechanical metrics of aesthetic perception in dance

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Abstract

The brain may be tuned to evaluate aesthetic perception through perceptual chunking when we observe the grace of the dancer. We modelled biomechanical metrics to explain biological determinants of aesthetic perception in dance. Eighteen expert (EXP) and intermediate (INT) dancers performed *développé arabesque* in three conditions: i) slow tempo, ii) slow tempo with relevé, and iii) fast tempo. To compare organizational metrics of kinematic data, we calculated intra-excursion variability, principal component analysis (PCA), and dimensionless jerk for the gesture limb. Observers, all trained dancers, viewed motion capture stick figures of the trials and ranked each for i) aesthetic proficiency and ii) movement smoothness. Statistical analyses included group by condition repeated measures ANOVA for metric data; Mann-Whitney U rank and Friedman’s rank tests for non-parametric rank data; Spearman’s rho correlations to compare aesthetic rankings and metrics; and linear regression to examine which metric best quantified observers’ aesthetic rankings, $p < 0.05$. The goodness of fit of the proposed models were determined using Akaike Information Criteria (AIC). Aesthetic and smoothness rankings of the dance movements revealed differences between groups and condition, $p < 0.0001$. EXP were rated more aesthetically proficient than INT dancers. The slow and fast conditions were judged more aesthetically proficient than slow with relevé ($p < 0.0001$). Of the metrics, PCA best captured the differences due to group and condition. PCA also provided the most parsimonious model to explain aesthetic rankings. By permitting organization of large data sets into simpler groupings, PCA may mirror the phenomenon of chunking in which the brain combines sensory-motor elements into integrated units of behavior. In this representation the chunk of information which is remembered, and to which the observer reacts, is the elemental mode shape of the motion rather than physical displacements. This suggests that reduction of redundant information to a simplistic dimensionality is related to the experienced observer’s aesthetic perception.

Key words: Akaike Information Criteria, chunking, dimensionless jerk, principal component analysis, variability

51
52 **INTRODUCTION**

53 In 1623, the astronomer Galileo Galilei observed that the universe "is written in the
54 language of mathematics" (Tegmark, 2008). More recently, Max Tegmark wrote "our external
55 physical reality is a mathematical structure" (Tegmark, 2008). Perception of dance (visual) or
56 music (auditory) is perception of reoccurring shapes and patterns. These shapes and patterns,
57 in the abstract, are based on numerical relationships, which are expressions of space and time.
58 In movement analysis, we employ biomechanical mathematics to describe and analyze
59 movement. Here, we ask, is there an biomechanical metric that relates to our aesthetic
60 perception of the dancer?

61
62 *Aesthetic perception*

63 When two dancers perform the same movement, a movement practiced multiple times
64 on a daily basis, how does the viewer intuitively know that one dancer embodies greater
65 aesthetic proficiency or is more pleasing (Calvo-Merino, Ehrenberg, Leung, & Haggard, 2010;
66 Calvo-Merino, Jola, Glaser, & Haggard, 2008; E. S. Cross, Kirsch, Ticini, & Schutz-Bosbach,
67 2011)? Dance (and music) has been a medium for communities to interrelate since primitive
68 societies (I. Cross, 2012; Kraus, Hilsendager, & Gottschild, 1991). As dance moved to the
69 performance venue, it became removed from group communal interaction to one of observer –
70 performer or audience and dancers. This assumes there are aesthetic properties to dance
71 movement and that the audience experiences an aesthetic response of some sort (Bläsing et
72 al., 2012). Depending upon their movement experience, observers may evaluate their aesthetic
73 experience in several ways; through cognitive judgement or affective appreciation (valence) of
74 dance movement based upon qualities such as movement amplitude, velocity, difficulty, or
75 control; while others may include their own familiarity and physical ability in their aesthetic
76 appreciation (Chatterjee, 2003; E. S. Cross, Kirsch, Ticini, & Schütz-Bosbach, 2011; Leder,
77 Belke, Oeberst, & Augustin, 2004; Montero, 2012; Torrents, Castaner, Jofre, Morey, & Reverter,
78 2013). The information-processing model presented by Leder et al. (2004) suggests that there
79 are two types of output in aesthetic processing: aesthetic emotion and aesthetic judgement
80 (Leder et al., 2004). To date, the majority of research on dance aesthetics has focused on
81 emotional liking: the observers' perception of affect and affective response to dance (Calvo-
82 Merino et al., 2008; Christensen, Nadal, & Cela-Conde, 2014; Kirsch, Drommelschmidt, &
83 Cross, 2013; Orgs, Hagura, & Haggard, 2013). The cognitive aesthetic evaluation of technical
84 proficiency such as control, accuracy, and fluidity, the focus of this study, has been less studied.

85 With no external goal to quantify a score, can we quantify the difference in the viewer's
86 aesthetic judgement of these two dancers performing the same movement? What is the
87 relationship between this perception of dance, in this case a ballet sequence, and its
88 biomechanical organization? Does the observer perceive dance movement with some
89 organizational strategy for recall? Does the concept of chunking for the purpose of extracting
90 meaningful event features, while suppressing extraneous information, relate to a kinematic
91 metric?

92

93 *Linear and nonlinear metrics in human movement*

94 A dynamic systems approach offers determination of coordinative patterns that may be
95 overlooked in more traditional linear kinematic measures organized around measures of
96 centrality. Movement patterns in high and low skilled subjects or those with dysfunction can be
97 considered adaptations to the constraints of mechanics, environment, and task. Most
98 movements, such as walking, display stereotypical spatial-temporal patterns, which suggests
99 that human movements organize degrees of freedom into functional coupled relationships to
100 achieve the task. These constraints, resulting from what are apparently complex motions,
101 consist of significantly less active degrees of freedom than an unconstrained system. These
102 degrees of freedom are patterns of joint movements rather than individual articulations.
103 Because motor behavior is also inherently variable, the challenge is to identify coordination
104 patterns that may distinguish different groups of subjects, with greater skill or disability, or
105 between conditions of differing levels of difficulty. A widely applied method in structural
106 dynamics is to describe complicated movements in terms of a small number of underlying
107 modes of vibration (e.g. principal component analysis). Could principal component analysis
108 (PCA) also be related to the manner in which elements are chunked into larger combinations as
109 as part of the aesthetic perception of movement?

110 Coordination variability can be assessed by approaches such as angle-angle plots, PCA,
111 vector coding, and entropy. Seemingly contradictory research findings suggests that there is an
112 'optimal' coordination variability in healthy, skilled subjects, no matter what the movement, that
113 is necessary to permit adaptation to mechanical, environmental, and task constraints (Chow,
114 Davids, Button, & Koh, 2008; Pollard, Heiderscheit, van Emmerik, & Hamill, 2005; Stergiou &
115 Decker, 2011; Wagner, Pfusterschmied, Klous, von Duvillard, & Muller, 2012). This lies between
116 the higher and lower variability reported in populations with less skill or neurologic and
117 musculoskeletal dysfunction (Hamill, van Emmerik, Heiderscheit, & Li, 1999; Hein et al., 2012;

118 Kiefer et al., 2013). The majority of analyses, to date, have focused on sports activities that
119 have an end goal such as speed or accuracy.

120 Patterns of variability (e.g. simple v. complex skills, injured v. healthy subjects) may not
121 be generalizable and may differ depending on the movement to be analyzed (e.g. basketball
122 dunk v. ballet movement). To date, dynamic systems approaches have been applied to the
123 analyses of dance movements in only limited fashion (Hollands, Wing, & Daffertshofer, 2004;
124 Reeve, Hopper, Elliott, & Ackland, 2013; Smith, Siemienski, Popovich, & Kulig, 2012; Torrents
125 et al., 2013; Vincs & Barbour, 2014). Are certain metrics sensitive to determine differences due
126 to skill level or condition difficulty in ballet movement?

127 Maximum smoothness theory introduced the jerk metric, the third time derivative of
128 position, as a quantitative principle of motor control as well as a way to characterize the smooth
129 gracefulness of natural movements (Hogan & Flash, 1987). This brings dance immediately to
130 mind. A number of jerk measures have been used to quantify smoothness and coordination in
131 studies that examine changes due to neurologic impairment and rehabilitation (Rohrer et al.,
132 2002; Teulings, Contreras-Vidal, Stelmach, & Adler, 1997; Yan & Dick, 2006). It has been used
133 less frequently to examine differences in skill level (Hreljac, 1993). Jerk may provide a metric for
134 the objective quantification of smoothness of motion and, by extension, to the skill level of the
135 practitioner. Recently, Hogan and Sternad (Hogan & Sternad, 2009) described the inability of
136 numerous measures of jerk to correlate with a *subjective* assessment of smoothness of
137 movement. These jerk measures, depending on their individual formulation, had dimensions of
138 time and position to appropriate powers. They proposed a dimensionless measure of jerk which
139 was found to be insensitive to periods of inactivity and more accurately reflected divergence
140 from smooth and coordinated movement. Does dimensionless jerk correlate with subjective
141 smoothness when assessed by trained dance observers?

142

143 *Aesthetic criterion of dance*

144 In ballet, the goal of movement is to meet an technical aesthetic criterion, that includes
145 specific timing and spatial relationships of upper and lower extremity placement, while making it
146 appear effortless (Autere, 2013; Cohen, 1997; Hagendoorn 2005). Previous researchers,
147 examining frequently performed ballet movements such as the *développé arabesque* and *grand*
148 *rond de jambe en l'air*, reported similar movement organization and timing across various levels
149 of expertise (e.g. expert, advanced, and intermediate dancers) (Bronner, 2012; Kwon, Wilson,
150 & Ryu, 2007; M. Wilson, Lim, & Kim, 2004). In these studies there were no differences in limb
151 angular displacement and velocity. Only kinematic control of the pelvis (e.g. three-dimensional

152 (3-D) peak angular displacement) appeared to differentiate skill level. However, the prescribed
153 timing and spatial directives may have constrained these biomechanics findings. If there is no
154 difference between the two dancers in the general shape and timing kinematics of the dance
155 movement (e.g. peak angular displacement and velocity), alternative approaches are called for.
156 Could this be due to stability (e.g. less variability), a cost function, or some other set of
157 kinematic parameters such as dimensionless jerk or nonlinear variability algorithms such as
158 principal component analysis? Furthermore, does differentiation of skill and condition by a
159 kinematic metric relate to observer perception?

160 The purpose of this study was three-fold. The first aim was to apply linear and nonlinear
161 dynamic systems approaches to determine the sensitivity of these metrics to differentiate skill
162 level and condition in a complex ballet sequence, the *développé arabesque*. The second aim
163 was to determine whether experienced observer rankings of the performers' *développé*
164 *arabesque*, viewing abstracted motion capture stick figures, for technical aesthetic proficiency
165 and movement smoothness can also differentiate skill level and condition. Finally, the third aim
166 was to compare these biomechanical metrics to the experienced observer rankings for
167 aesthetics and smoothness to determine which metric best quantified observer perceptions of
168 the dancers' *développé arabesque* sequence.

169

170 2. METHODS

171 *Subjects*

172 Dancers

173 Eighteen healthy adult dancers (12 female, 8 male), recruited from internationally
174 recognized professional dance companies and affiliated pre-professional training programs,
175 volunteered for this study. Each dancer was assigned to one of two groups with distinct levels of
176 dance expertise: i) expert and ii) intermediate. The expert (EXP) group was based on
177 employment in a professional company. The intermediate (INT) group, comprised of student
178 dancers, was determined by ballet class placement by dance faculty. During auditions, students
179 are placed into ballet technique classes that ranged from beginning to advanced levels (Ballet 1-
180 7); we selected students placed into Ballet 4 and 5, or intermediate level classes. Inclusion
181 criteria was the ability to attain the criterion dance sequence, *développé arabesque*, at a height
182 of 90° (e.g. gesture limb perpendicular to the stance limb and parallel to the floor) and exclusion
183 was a history of lower extremity injury during the previous six months that caused a dancer to
184 stop dancing for one week or more. We did not include naïve or beginner participants in this
185 study because naïve and beginner dancers were not able to meet the inclusion criteria. The

186 university Institutional Review Board approved this study. A power analysis of sample size for a
187 two group repeated measures with three conditions (2 X 3) study, with a large effect size
188 ($f=0.80$), power=0.95, and $\alpha = 0.05$, determined a sample size of 8 was necessary. Therefore,
189 the selected sample size of 18 subjects was more than sufficient. Participant demographics
190 were collected at intake.

191 The ratio of female to male dancers was the same within each group (5 females, 4
192 males). Comparison of group demographics was performed using a paired t-test for
193 independent samples. There were differences between groups in age (EXP = 25.8 ± 2.6 and
194 INT = 20.4 ± 1.5 years, $p<0.0001$) and years of dance experience (EXP = 15.22 ± 6.68 and INT
195 = 5.50 ± 5.15 years, $p=0.003$), but no difference in height (1.71 ± 0.076 m), mass (62.20 ± 8.67
196 kg), leg length (0.92 ± 0.05 m), or starting first position turnout ($107.94 \pm 11.89^\circ$).

197

198 Observers

199 Previous research has reported differences in the aesthetic experience of viewers with
200 differing levels of expertise in performing the observed movements (Calvo-Merino et al., 2010;
201 E. S. Cross, Kirsch, Ticini, & Schutz-Bosbach, 2011; Kirsch et al., 2013). Therefore, we selected
202 trained dancers to act as observers of the arabesque sequences. Experienced dancers are able
203 to rapidly process movement, developed as part of their training, and may use 'schematic
204 expectancies' to maximize their short-term memory (C. Stevens et al., 2010). Twenty seven
205 different dancers, recruited from international caliber professional dance companies and
206 affiliated pre-professional training programs, volunteered to evaluate the arabesque data for i)
207 aesthetic proficiency and ii) smoothness. Observers included nine professional and 18
208 advanced or intermediate pre-professional dancers (22 female, 5 male), They had a broad span
209 of dance experience from 4 to 40 (mean 15 ± 9) years and ranged from 18 to 55 (mean 28 ± 12)
210 years of age.

211

212 *Experimental Protocol*

213 Motion capture

214 The dance-specific task, *développé arabesque*, was a sequential, multi-joint movement
215 that required intra and inter-segmental coordination of lower and upper extremity movement
216 with changes from bipedal to unipedal postural control. It is practiced in every ballet class, and
217 consequently was well known to each subject. Each dancer's preferred *1st position* foot
218 placement (heels touching with lower extremities externally rotated) was marked on the floor,
219 measured (Bronner, 2012), and used as the starting position (Fig. 1).

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Insert Fig. 1 here

A tape recording of a metronome with voice instruction overlay provided the tempo of the movement sequence (40 or 90 beats·min⁻¹). Dancers practiced the *développé arabesque* sequence (Fig. 1A – D) for three conditions prior to data acquisition to synchronize their movements with the metronome. The dancers were instructed to emphasize spatial and temporal precision. From the starting posture (1st position), the gesture lower extremity passed through *passé* (hip and knee flexion, with ankle plantar flexion), and extended posteriorly to *arabesque* (gesture hip and knee extension with ankle plantar flexion), where it was held for one count, followed by return to the initial 1st position. Dancers performed six consecutive ‘excursions’ (or repetitions of the *développé arabesque sequence*) within one trial with the right lower extremity as gesture limb. This was followed by six consecutive ‘excursions’ with the left lower extremity as gesture limb.

The *développé arabesque* sequence was performed in three conditions to reflect differing tempo and balance constraints. For Condition 1, the *développé arabesque* was performed on flat foot at a tempo of 40 beats·min⁻¹ (Slow-flat). For Condition 2 using the same 40 beats·min⁻¹ tempo, dancers were asked to *relevé* (rise up onto the toes of the stance limb and hold) (Slow-bal) during the arabesque phase of the sequence. For Condition 3, the *développé arabesque* was performed on flat foot at a tempo of 90 beats·min⁻¹ (Fast). The excursions lasted approximately 40s in length for Conditions 1 and 2, and 18s for Condition 3.

Kinematic data were collected at a sampling rate of 120 Hz, with a 5-camera motion analysis system (Vicon 250, Oxford Metrics Ltd, Oxford, UK). A full body marker set comprised of 29 reflective, spherical markers in the Plug-In gait marker set was used to create an 11-segment model. Attire for all subjects consisted of a dark colored unitard to maximize contrast of reflective markers.

Kinematic data were reconstructed using a Vicon Bodybuilder model (Oxford Metrics Ltd, Oxford, UK). Kinematic data were filtered with a 4th order 20Hz order low pass FIR filter. Dance movements may require movement of three or more limbs; four in the case of a jeté or leap. Both upper extremities and one lower extremity are moving in the *développé arabesque*. In ballet, the gestural foot is often considered an expressive focal point. Therefore, we focused our analysis on the gestural lower extremity.

Observer rankings

254 We defined *aesthetic proficiency* as the technical accuracy of timing, dynamics, and
255 shape as performed by each dancer. We defined *smoothness* as the fluid trajectory of the lower
256 extremity gesture limb. The ranking numbers 1-18 were selected for the total number of
257 subjects, with 1 for most to 18 for least in: i) aesthetic technical proficiency, and ii) movement
258 smoothness. Aesthetic proficiency and smoothness rankings were conducted in separate
259 sessions. Ranking was selected, rather than rating, in order to compare each dancer to the
260 others within a given condition. Observers evaluated the abstracted motion capture stick figure
261 data for the left and right lower extremity as gesture limb of all subjects on a laptop computer
262 within one condition in a single viewing (add youtube movie example of stick figures). Group
263 assignment was unknown to the observers. There were six consecutive 'excursions' within one
264 trial per gesture limb. Observers were permitted to view a trial again if needed as they
265 reorganized the ranking numbers of a given condition.

266

267 *Data analysis*

268 Observer rankings

269 Mean aesthetic and smoothness observer rankings were calculated for each dancer trial
270 in each condition. For the aesthetic and smoothness rank data, the non-parametric Mann-
271 Whitney U rank test for two independent samples was used to determine group differences. The
272 non-parametric Friedman two-way ANOVA rank test (K-related samples) was used to determine
273 condition differences. Statistical significance was set at $p \leq 0.05$ for both the Mann-Whitney and
274 Friedman tests. If significance was determined in the Friedman test, post hoc pairwise
275 comparisons were conducted using the Wilcoxon signed-rank test with a Bonferroni correction
276 ($0.05/3 = 0.017$). The assumption of homogeneity of variance was checked for aesthetic and
277 smoothness rank data using Levene's test for non-parametric ranked data.

278

279 Three-D pelvis-hip angle-angle and toe displacement variability

280 Intra-excursion variability for the pelvis-hip, an important control area (Bronner, 2012),
281 was calculated on the angle-angle phase plane for all three cardinal planes. For the 3-D angle-
282 angle analysis, pelvis inclination was defined as the included angle between the normal to the
283 right anterior iliac spine (RASIS), left anterior iliac spine (LASIS), sacrum plane and global
284 vertical. The hip articulation angle was defined as the included angle between the femur
285 proximal to distal axis and the normal to the RASIS, LASIS, sacrum plane. Each trial was
286 decomposed into its constituent excursions (six per trial). The excursion commenced when the

287 toe marker on the gesture leg exceeded an altitude of 190mm and ended when the marker
288 descended below 190mm.

289 The 3-D angle of the pelvis and hip angle between the normal of the pelvis and
290 the proximal/distal axis of the gesture femur were calculated. The standard deviation
291 across the excursions of the pelvis and hip angles were calculated as a fractional basis
292 of the excursions. The pelvis-hip MSD was the mean of these standard deviations.

293 We did not normalize the temporal component of the data of these excursions as this
294 process can distort the spatial relationship between trials (Hamill, McDermott, & Haddad, 2000),
295 which was a parameter of interest. Furthermore, dancers have been found to be extremely
296 consistent when performing movements to an external tempo (Reeve et al., 2013).

297 Three-D angle-angle plots were constructed of the pelvis and hip for the
298 three conditions and an MSD value was calculated for each subject. Similarly, MSD was
299 calculated for the 3-D toe displacement using the same decomposition into its constituent
300 excursions (six per trial) and onset and offset criteria. The mean and standard deviation of the
301 gesture toe was calculated along its 3-D trajectory. The toe MSD was the mean of the standard
302 deviation along the trajectory.

303 Because each excursion had a discrete onset and offset, circular statistics were not
304 necessary. To compare pelvis-hip and toe variability for left and right gesture limbs, separate 2
305 (group) X 3 (condition) repeated measures ANOVA comparisons were conducted, with pairwise
306 comparisons. Statistical significance was set at $p \leq 0.05$ for all tests.

307

308 Principal component analysis

309 PCA is a data reduction technique for the compression of large data sets (Jolliffe, 2002)
310 and has been shown to be appropriate for feature extraction in human movement analysis
311 (Daffertshofer, Lamoth, Meijer, & Beek, 2004). PCA was used to quantify 3-D kinematic patterns
312 using the full data set. The joint angle time histories were calculated from the motion data. A 15-
313 element state vector was defined for each time instant of each trial from the angular position of
314 the pelvis (3 degrees of freedom (DOF) in a rotation sequence about the P-A axis, followed by
315 rotation about the lateral axis, followed by rotation about the S-I axis) together with the joint
316 articulations of the hip (3 DOF in a rotation sequence about the abduction/adduction axis,
317 followed by rotation about the flexion/extension axis, followed by rotation about the
318 internal/external rotation axis), knee flexion (1 DOF) and ankle dorsi/plantar flexion and
319 internal/external rotation (2 DOF) of the stance and gesture limbs. Knee flexion was defined as
320 the angle between the line from the knee joint centre to the hip joint centre and the line from the

321 knee joint centre to the ankle joint centre in the plane defined by these two lines. These
322 variables were selected as elements in the state vector as they span the domain of possible
323 lower limb motion with the exception of knee varus/valgus and ankle abduction/adduction which
324 were considered trivial.

325 The principal components were calculated for the matrix of the above vector for each
326 time in the trial. The matrix was initialized normalized, so that they have zero mean and unity
327 variance. Principal components that contributed less than 2% to the total variance in the data
328 set were eliminated. Mean dimensionality of the non-redundant state manifold count was
329 calculated for each group and condition and compared with a 2 X 3 repeated measures
330 ANOVA, with pairwise comparisons, $p \leq 0.05$.

331

332 Jerk

333 Dimensionless jerk as described by Hogan and Sternad (2009), was calculated for 3-D
334 linear displacement of the gesture toe as:

335

336 $Jerk_{\text{dimensionless}}$

$$= \frac{D^3 \int_{t_1}^{t_2} \ddot{x}(t)^2 dt}{V_{\text{mean}}^2}$$

337

338 where D = duration of the trial

339 $x(t)$ = position variable

340 v = first time derivative of the position variable

341

342 and for 3-D angular displacement of the gesture hip as:

343

344 $Jerk_{\text{dimensionless}} =$

$$D^5 \int_{t_1}^{t_2} \ddot{\theta}^2 dt$$

345

346

where θ = angular displacement

347

348

Separate 2 (group) X 3 (condition) repeated measures ANOVA comparisons for the i) 3-D linear displacement of the gesture toe; and ii) 3-D angular displacement of the gesture hip were conducted, with pairwise comparisons. Statistical significance was set at the $p \leq 0.05$ for all tests.

349

350

351

352

Correlation of observer rankings and biomechanical variables

353

Aesthetic rankings were compared to smoothness rankings, MSD for 3-D pelvis-hip angle-angle and toe displacement variability, PCA, and dimensionless jerk for 3-D hip angle and toe displacement using Spearman's rho correlations for nonparametric variables, $p \leq 0.05$.

354

355

356

Modeling rankings and movement metrics

357

We employed mixed model linear regression analysis to examine which variables, MSD, PCA, and jerk, were good predictors of each observer's aesthetic and smoothness perception. Separate regression analyses approximated the i) aesthetic; and ii) smoothness ranking data with regressors that consisted of the following:

358

Model 1) 5 predictors: PCA, jerk (hip and toe), and MSD (3-D pelvis-hip and toe);

359

Model 2) 1 predictor: PCA;

360

Model 3) 2 predictors: jerk (hip and toe);

361

Model 4) 1 predictor: toe jerk;

362

Model 5) 2 predictors: MSD (pelvis-hip and toe); and

363

Model 6) 1 predictor: MSD toe.

364

365

The goodness of fit of the proposed models were determined using Akaike Information Criteria (AIC), with the least AIC value, indicating the best fit. The AIC value is

366

367

$$AIC = 2k - 2 \ln(L),$$

368

374 Where k is the number of parameters in the model, and L is the maximized likelihood function
375 for the model. The corrected AIC value (AICc) for finite sample size where

376

377

$$\text{AICc} = \text{AIC} + 2k(k+1)/(n-k-1)$$

378

379 was selected for comparison of the models. All statistics were conducted using SPSS (SPSS v.
380 21, IBM Corp, Armonk, NY).

381

382 **RESULTS**

383 *Observer rankings*

384 The Mann-Whitney U test for group indicated that aesthetic rankings were lower for EXP
385 dancers (median = 4.10, interquartile range (IQR) = 2.20-6.20) compared to INT dancers
386 (median = 10.20, IQR = 8.20-12.00) [U=88.00, $p<0.0001$]. A non-parametric Friedman test of
387 differences among repeated measures for condition was conducted, rendering a Chi-square test
388 value of 15.267, $p<0.0001$. Post hoc Wilcoxon signed-rank test indicated that Slow-flat aesthetic
389 rankings (median = 7.75, IQR = 4.88-10.13) were significantly lower than Slow-bal (median =
390 8.30, IQR = 5.17-12.00) [$z = 2.109$, $p=0.017$]; Fast rankings (median = 7.90, IQR = 2.20-11.20)
391 were also lower than Slow-bal [$z = 3.570$, $p<0.0001$]; and Slow-flat was lower than Fast [$z =$
392 2.233, $p=0.012$]. [Note, lower rank indicated greater excellence in aesthetic proficiency
393 rankings. For smoothness results see Supplement.]

394

395

Insert Fig. 2 here

396

397 *Three-D pelvis-hip angle-angle and toe displacement variability*

398 Three-D gesture limb pelvis-hip angle-angle plots for a representative subject from each
399 group performing six excursions during each condition are seen in Fig. 3. The MSD seen in the
400 six plots demonstrate variability around the mean. Comparisons found a significant difference
401 between groups [$F(34,1)=6.532$, $p=0.015$] (Fig. 4A), with EXP displaying lower pelvis-hip angle-
402 angle MSD than INT dancers. There were no differences between conditions.

403

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407

There were group differences in 3-D toe displacement MSD [$F(34,1)=12.406$, $p=0.001$]
with EXP reflecting lower toe MSD than INT, and for condition [$F(34,1)=5.277$, $p=0.028$]. Fast
condition 3-D toe MSD was lower than the Slow-bal condition ($p=0.014$). There was an
interaction between group and condition [$F(34,1)=4.254$, $p=0.047$] (Table 1, Fig. 4B). Three-D
toe MSD was lower in EXP compared to INT dancers in the Slow-flat ($p=0.047$) and Slow-bal

408 conditions ($p=0.004$).

409

410

Insert Figs. 3 and 4 here

411

412 *Principal component analysis*

413 The PCA analysis had three effects: (1) it orthogonalized the components of the input
414 vectors so that they were uncorrelated with each other; (2) it ordered the resulting orthogonal
415 components (principal components) so that those with the largest variation came first; and (3) it
416 eliminated those components that contributed the least to the variation in the data set. The PCA
417 dimensionality of the movement reported indicates the number of mode shapes which were
418 required to account for 98% of the total variance of the motion data captured during the
419 arabesque excursions.

420 Figure 5A shows an example of five principal modes calculated for a representative INT
421 dancer. The first mode, and hence the mode contributing the most variance to the movement,
422 was predominantly a hip flexion/extension motion. The second mode was mainly a hip
423 abduction/adduction. The third mode was associated with knee flexion/extension of the support
424 limb, the fourth mode was support limb ankle internal/external rotation, and the fifth mode was
425 associated with gesture limb ankle internal/external rotation. The combination of these five
426 modes accounted for 98% of the variance of the trial.

427

428

Insert Fig. 5 here

429

430 Figure 5B shows an example of the four principal modes calculated for a representative
431 EXP dancer. The first mode consists of hip flexion/extension motion, similar to the intermediate
432 dancer. The second mode for the expert dancer was also mainly a hip abduction/adduction,
433 however the third mode was dominated by support limb ankle internal/external rotation. The
434 fourth mode was primarily support limb knee flexion/extension. These four modes accounted for
435 98% of the variance of the trial.

436 The mean dimensionality of the state manifold accounting for 98% of the variance for
437 EXP dancers was significantly lower than the mean dimensionality for INT dancers for group
438 [$F(34,1)=25.339$, $p<0.0001$] and condition [$F(34,1)=14.876$, $p<0.0001$] (Fig.6A and B). Post hoc
439 pairwise comparisons for condition indicated there were differences between Slow-bal and
440 Slow-flat ($p=0.008$) as well as Slow-bal and Fast ($p<0.0001$), with Slow-flat and Fast less than
441 Slow-bal.

442

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Insert Fig. 6 here

444

445 *Dimensionless jerk*

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Insert Fig. 7 here

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455 *Relationships between aesthetics and biomechanical variables*

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462 *Modeling rankings and movement metrics*

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Insert Table 1 here

467

468 **DISCUSSION**

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In general, observer aesthetic and smoothness rankings and biomechanical parameters were capable of distinguishing between group and condition, with the exception of 3-D toe jerk and pelvis-hip angle-angle MSD metrics. In discrimination between groups, kinematic metrics revealed that the movement of EXP dancers was smoother (e.g. lower jerk), more consistent (e.g. lower MSD), and displayed lower organizational parameters (fewer principal components) across all conditions. Differences between groups were generally greater in the Slow-flat and Slow-bal conditions compared to the Fast condition. In discerning differences between

476 conditions for both groups, there was generally an inverted horseshoe trendline to the data, with
477 Slow-bal reflecting higher rankings for aesthetics (e.g. less aesthetic proficiency) and
478 smoothness (e.g. less smooth), higher MSD, higher dimensional components, and higher jerk.
479 In contrast, the Fast condition reflected the lowest number of principal components and lowest
480 jerk. PCA provided the most parsimonious model to explain observer rankings. Each of the
481 variables are discussed further in the sections below.

482

483 *Observer rankings*

484 We chose dancer-observers who were well trained in the movements that they ranked
485 for aesthetics and smoothness. Evidence suggests that cortical regions involved in the action-
486 observation network respond more strongly when the observer sees a kinesthetically familiar
487 movement compared to one that the observer has never performed (Bläsing et al., 2012; Calvo-
488 Merino, Glaser, Grezes, Passingham, & Haggard, 2005; E. S. Cross, Hamilton, & Grafton,
489 2006). Aesthetic judgement has been linked to both action and processing fluency (Hayes, Paul,
490 Beuger, & Tipper, 2008; Reber, Schwarz, & Winkielman, 2004). Experienced dancers compared
491 to naïve observers judge the motor perceptual experience of precision, fluidity, and control
492 differently. Therefore, we selected dancers to perform the observer rankings with the
493 expectation that this expertise refines their observation of the technical aesthetic qualities of
494 dance (Montero, 2012). In this study, despite reviewing the motion capture stick figures on
495 separate occasions to rank for aesthetic proficiency or smoothness, rankings for aesthetic
496 proficiency and smoothness were highly correlated. This suggests that movement fluidity may
497 be an important component of cognitive aesthetic perception.

498 Several groups have developed dance-specific aesthetic competence evaluation
499 measures that focus on the cognitive aspects of aesthetics such as technique accuracy,
500 dynamics, and control (Angioi, Metsios, Twitchett, Koutedakis, & Wyon, 2009; Chatfield &
501 Byrnes, 1990; Krasnow & Chatfield, 2009). Each group demonstrated excellent repeatability
502 between judges in their respective measures, with sensitivity to determine change with training
503 or due to expertise. Similar judgement of competency is also used in sports competitions such
504 as diving, gymnastics and figure skating (Díaz-Pereira, Gómez-Conde, Escalona, & Olivieri,
505 2014; Looney, 2004; Pajek, Cuk, Pajek, Kovac, & Leskosek, 2013; Young & Reinkensmeyer,
506 2014). We chose to rank aesthetic judgement specific to each dancer's ballet technique for this
507 reason. Aesthetic valience may be more variable across individuals due to personal taste (Leder
508 et al., 2004).

509 Researchers have employed several ways of displaying dance movement in order to

510 study the aesthetic perception of dance. Observers have viewed dance as point light displays
511 (Sevdalis & Keller, 2011), motion capture stick figures (Sato, Nunome, & Ikegami, 2014;
512 Torrents et al., 2013), static stick figures (Daprati, Iosa, & Haggard, 2009), video (Calvo-Merino
513 et al., 2008; E. S. Cross, Kirsch, Ticini, & Schütz-Bosbach, 2011; Jola & Grosbras, 2013; Miura
514 et al., 2010), and live performance (Angioi et al., 2009; Stevens et al., 2009). Observation of live
515 and video performances are most ecologically valid and may be important to study aesthetic
516 valence. In contrast, abstraction of the dancer's movement in point-light or motion capture stick
517 figure representation allows the observer to focus on form and fluidity to make technical
518 aesthetic judgements without distraction by costumes, sets, or music.

519 Observers were able to distinguish between groups and conditions with both aesthetic
520 proficiency and smoothness rankings. It is possible that these dancer-observers were able to
521 accomplish this due to their specialized training in recognizing movement configurations,
522 encoding them (in the case of ballet, this may include verbal encoding as it has a set
523 vocabulary), and then extracting key information as part of the process of learning new
524 choreography (C. Stevens et al., 2010; Stevens, Ginsborg, & Lester, 2010). In this study, the
525 *développé arabesque* was a relatively short, well-learned phrase, enabling the observers to
526 focus on differences between the performers.

527

528 *Relationships between observer rankings and biomechanical variables*

529 Our results found that aesthetic rankings and all variables were significantly correlated.
530 The highest correlation between aesthetic proficiency and biomechanical metrics was to PCA
531 ($r=0.620$, greater than that of smoothness to PCA, $r=0.479$, see Supplement). Recently, multiple
532 factor analysis (MFA), an extension of PCA to handle multiple data tables that measure sets of
533 variables collected on the same observations, was applied to four dance movements: (1)
534 *arabesque penchée* requiring balance; (2) *tour en dehors* or turn; (3) *brisé volé en arrière en*
535 *tournant* or skater's jump; and (4) a forward fall, performed by expert dancers (Torrents et al.,
536 2013). Non-expert observers rated motion capture stick figures performing each of the
537 movements for aesthetic 'beauty.' Movement amplitude was the basic parameter used in
538 judging positive aesthetics, followed by turning velocity, and the length of time that balance was
539 maintained. In other studies, greater difficulty or faster movements were more appealing to
540 naïve observers (Calvo-Merino et al., 2008; E. S. Cross, Kirsch, Ticini, & Schütz-Bosbach, 2011).
541 These findings correspond to the lower aesthetic and smoothness rankings we found for the
542 Fast condition (lower ranking of aesthetic proficiency and smoothness indicated greater
543 excellence). However, we found that aesthetic and smoothness rankings were highest for the

544 Slow-bal condition, the more difficult of the conditions. The expertise of these observers did not
545 rank balance itself with positive aesthetics. It is likely, they perceived technical problems in the
546 performers' achievement of that condition.

547 Sato et al. (Sato et al., 2014) investigated the relationship of aesthetic competence to
548 variability of amplitude, velocity and shape in hip hop dance. Three groups of dancers with
549 differing skill levels performed the wave. Similar to this study, motion capture stick figures were
550 rated by experienced judges. Aesthetic judgement discriminated successfully between experts,
551 non-expert, and novice dancers and correlated highly with smoothness propagation of the wave.
552 Components of aesthetic technical proficiency include control, accuracy, and fluidity. Therefore,
553 it is possible that the movement smoothness is a subset of aesthetic technical proficiency,
554 explaining the high correlation ($r=0.817$) between the two parameters in our analysis.

555 There were also correlations between smoothness rankings and all variables with the
556 exception of pelvis-hip angle-angle MSD. Again, the highest correlation was to PCA. Dancers'
557 training focuses on timing and the dynamic quality of movement. Therefore, the observers, all
558 trained dancers, may have been particularly attuned to the smoothness perception parameter
559 as it relates to fluidity.

560

561 *Three-D pelvis-hip angle-angle and toe displacement variability*

562 Angle-angle MSD analyses demonstrate variability in coordination patterns during 3-D
563 joint coupling. This variability may decrease or increase with expertise depending on the task,
564 offering flexibility to achieve certain goals (Wagner et al., 2012; C. Wilson, Simpson, van
565 Emmerik, & Hamill, 2008).

566

567 In dance, the aesthetic shape and timing goals may dictate the coordination patterns.
568 Researchers have reported more stable joint coordination in dancers compared to non-dancers
569 during a rhythmic coordination task (Kiefer et al., 2011). Greater variability in pelvic motion in
570 the *développé arabesque*, measured by the coefficient of variability (CV), differentiated between
571 intermediate and expert dancers in all three planes (Bronner, 2012). The greatest variability was
572 found in intermediate dancers in the transverse plane. Similar differences for end segment 3-D
573 toe and finger CV differentiated skill level in the same study. Other dance researchers reported
574 that CV was able to distinguish between experts and novice hip hop dancers in several
575 kinematic measures (Sato et al., 2014). Both pelvis-hip angle-angle and 3-D toe MSD findings
576 in this study were similarly able to differentiate differences between skill in this study.

577 The effect that altered speed and balance constraints have on angle-angle variability is

578 less clear. One study comparing pelvis-trunk coordination and variability in walking and running
579 found no changes in variability due to speed (Seay, Van Emmerik, & Hamill, 2011). In this study
580 only 3-D toe MSD distinguished differences between conditions. Pelvis-hip control of the center
581 of mass may be a critical control parameter, particularly when the participant must stand on one
582 limb. This may explain our finding of no differences between conditions in pelvis-hip angle-angle
583 MSD.

584

585 *Principal component analysis*

586 PCA is a technique which reduces complex data sets into smaller set of principal
587 components which are capable of reproducing the original movement the as a linear
588 superposition of these modes and hence is an efficient data compression method. The
589 technique also has the effect of associating noise in the motion with components which add little
590 variance and hence can often be eliminated from the analysis.. We found that our more skilled
591 EXP dancers demonstrated lower dimensional components when compared to the INT dancers.
592 Previously, a different intra-limb organizational strategy was found in the temporal kinematics of
593 the *développé arabesque* in EXP compared to INT dancers (Bronner, 2012). This difference
594 may be reflected in the lower number of PCA nodes seen here in the EXP group.

595 Differences due to skill or practice have been reported by other researchers (Ko, Challis,
596 & Newell, 2003). In 2-D analyses, these researchers reported a shift to lower dimensional
597 components with learning, represented by two principal components (Ko et al., 2003). In a 3-D
598 learning study, Hong and Newell reported no change in the number of three principal
599 components that explained 90% of the variance (Hong & Newell, 2006). However, the
600 movement was a relatively constrained one on a ski-simulator. In a simple 3-D pointing
601 movement with an accuracy constraint, researchers reported more than 95% of the variance
602 was included in one principal component, representing ten joint angles from shoulder to wrist
603 (Tseng, Scholz, Schoner, & Hotchkiss, 2003). Using a 32 marker set and motion capture,
604 Hollands et al. (Hollands et al., 2004) reported that only a small number of principal components
605 were sufficient to describe a 15s movement phrase performed by two professional dancers.
606 Nine modes represented the dataset, with 82% of the variance represented in the first three
607 PCAs. However, the movement phrase was not described nor was any difference found
608 between the two dancers.

609 In this study, dance skill (e.g. group) had a direct effect on the number of active modes
610 of coordination. Given the complexity of the *développé arabesque* with gesture and stance
611 limbs, requiring changes in stability, balance and speed, results demonstrated a surprisingly low

612 dimensionality, ranging from four to seven dimensions in EXP and INT dancers respectively.
613 The Slow-bal condition in EXP dancers was primarily reflected in the 5th component, while the
614 Fast condition was reflected in the 3rd and 4th components. In contrast in INT dancers, Slow-flat
615 and Slow-bal were reflected in the higher 5th, 6th, and 7th components while the Fast condition
616 was primarily reflected in the 5th and 6th components. Unfortunately, there is no standard way to
617 analyze or report PCA, therefore it is not possible to directly compare our results to those
618 previously conducted on dance-related movements.

619 Singular value decomposition (SVD) is similar to PCA in pairing a large number of
620 features into a smaller subset of major movement structures (Land, Volchenkov, Blasing, &
621 Schack, 2013; Volchenkov & Blasing, 2013; Volchenkov, Blasing, & Schack, 2014). This
622 method was able to discern the level of movement expertise in both ballet dancers and golfers.

623 Our results found PCA was also able to discriminate between conditions, with Fast and
624 Slow-flat demonstrating lower dimensionality than Slow-bal. In contrast, using accelerometry,
625 PCA was not able to differentiate between conditions in walking at slow, preferred, and fast
626 speeds (Kavanagh, 2009).

627

628 *Dimensionless jerk*

629 We employed the dimensionless measure of jerk to eliminate differences between the
630 conditions due to movement duration or extent (Hogan & Sternad, 2009). We observed an
631 inverted horseshoe in hip and toe jerk histograms for both groups, with the Fast condition
632 reflecting the greatest smoothness (lower jerk) and Slow-bal condition reflecting the least
633 smoothness (higher jerk).

634 Minimal jerk theory was initially proposed to explain planning of hand movements in
635 space. It assumed that movement is based on a kinematic endpoint path trajectory, predicting
636 straight line paths and bell-shaped velocity curves with a dynamic optimization criterion to
637 maximize smoothness (Flash & Hogan, 1985). The majority of jerk research has focused on arm
638 movements based on the endpoint path trajectory. Alternatively, to explain subsequent
639 observations of the linear relationship of joint velocities when joints move in a coordinated way
640 and trajectories that are not necessarily straight lines, an optimization-based minimum angular
641 jerk model was proposed (Friedman & Flash, 2009). Subsequent comparison of this model
642 using a two-joint index finger grasping movement to other optimization models reported that
643 the best fit was the angular jerk model.

644 Researchers have demonstrated a decrease in jerk metrics with training or expertise
645 (Hreljac, 1993, 2000; Schneider & Zernicke, 1989) and increased jerk metrics with increased

646 gait speed when comparing walking and running (Hreljac, 2000). However, none of these
647 studies utilized dimensionless jerk. As described by Hogan and Sternad (Hogan & Sternad,
648 2009), the dimensionless jerk measure indicates the number of velocity fluctuations but is
649 independent of movement duration.

650 Due to the computational complexity of performing a single limb balance while moving
651 the leg (and torso) at various speeds, durations, and balance constraints, we chose to
652 investigate dimensionless minimal jerk optimization for both endpoint and angular jerk variables
653 of the gesture limb. Our results found that both angular and endpoint jerk metrics were sensitive
654 discriminators between conditions (tempo and balance), but not to discriminate differences in
655 expertise (group) in this experimental paradigm. Recently, a novel measure for quantifying
656 movement smoothness, *spectral arc-length* metric, has been proposed to overcome
657 shortcomings in existing metrics (Balasubramanian, Melendez-Calderon, & Burdet, 2012). This
658 metric warrants further investigation.

659 Interestingly, the Fast condition revealed **lower rankings in both aesthetic proficiency and**
660 **smoothness, fewer principle components, lower 3-D toe MSD, and lower jerk.** Although we
661 manipulated the arabesque sequence with speed and balance constraints, the Fast condition
662 was not performed at a maximal speed but was metronome controlled. The Fast condition may
663 have minimized demand on pelvis-hip coordination with subsequent reduction in 3-D toe MSD
664 due to diminished time in single limb weight bearing. Increased tempo may also have resulted in
665 reduced sub-movements and lower jerk.

666

667 *Modeling rankings and movement metrics*

668 For aesthetic rankings, model 2 received the least AICc value, indicating that this was
669 the most parsimonious model for the data. Model 2 modeled aesthetic ranking on the PCA
670 predictor variable. For smoothness rankings, model 2 again received the least AICc value,
671 signifying the best fitting model for the data (supplemental data).

672 AIC tells us what variables are important and which are not in establishing a model. If a
673 variable appears in a model that has a higher AICc score compared to a model that does not
674 contain that variable, then that variable can be ignored. In the case of both aesthetic and
675 smoothness rankings, the model with the least AICc value, PCA, corresponded with the highest
676 correlation values.

677 PCA, which permits the organization of large data sets into simpler groupings, may
678 reflect how the brain organizes huge amounts of sensory input into chunks (Chen, Penhune, &
679 Zatorre, 2008; Janata & Grafton, 2003), or, in the case of dance, what is known as phrases.

680 Chunking is thought to be the way in which the brain combines sensory-motor elements into
681 integrated units of behavior during motor learning. Chunking, in a dynamic process, emerges
682 spontaneously: as we learn to read, we focus on individual letters and then quickly combine
683 them into words, leading to groups of words and then whole sentences. A similar process is
684 thought to occur in both music and dance: we begin with notes or steps, which then become
685 chunked into short phrases or elemental components which can be linearly, or non-linearly,
686 combined to recreate a representation of the original experience whilst retaining minimal
687 information. Sequences become organized into fewer but larger chunks, decreasing the need
688 for cognitive control with a shift to other neural areas such as those related to motor execution
689 and ultimately, with expertise, automaticity (Sakai, Hikosaka, & Nakamura, 2004).

690 Orgs et al. (Orgs et al., 2013) suggested a hierarchical model of aesthetic perception of
691 dance movement: postures, movements, and the larger units of phrases. They suggest that
692 observer experience may affect how observers weight these hierarchical levels, with dance
693 experts focusing more on phrasing or larger chunks. Similarly, Bläsing (Blasing, 2014) reported
694 dance expertise reduced perceived segment boundaries, with, subsequently, longer phrases. In
695 competitive diving, PCA was applied to kinematic data to predict judges' technical scores,
696 reporting a high correlation between predicted and actual scores (Young & Reinkensmeyer,
697 2014). We ask, are the judges extracting fundamental patterns of coordination that reflect these
698 PCA results?

699 Various motor control theories have attempted to explain how we organize the
700 complexity of movement with its multiple degrees of freedom. Just as we may use a
701 minimization cost function of some sort to perform a motor act, the brain may seek to organize
702 what it perceives to be the simplest mode. Similarly, aesthetic perception may utilize chunking
703 to assess complex movement. PCA may provide an organizational structure of pattern
704 recognition to explain this phenomenon. PCA can reveal hidden structure within a complex data
705 set while simultaneously filtering out noise. The efficiency of smooth movement, minimization of
706 effort, and clear lines found in the expert dancer were reflected in lower PCA components.

707

708 *Limitations*

709 Perhaps ranking was not the optimal metric for aesthetic or smoothness perception. In
710 the future, we will investigate the effectiveness of Likert scales for multiple components of
711 aesthetic perception (e.g. both cognitive technical judgement and valience) that observers can
712 apply to each dancer trial separately. This does not require them to hold in their memory how
713 the other dancers performed within a given condition.

714 No movement kinetics were included in our models or analyses. Given the important
715 contribution of dynamics to the quality of dance movement, future investigation will investigate
716 whether kinematics and/or kinetic metrics are preferred determinants of aesthetic perception.

717

718 *Conclusion*

719 Our examination of a number of biomechanical metrics in a complex dance sequence
720 with shape, timing, and balance constraints found that PCA best captured the differences due to
721 expertise and condition. Further comparison between these biomechanical metrics and
722 movement aesthetic rankings found that PCA provided the most parsimonious model to explain
723 these observer rankings. If the grace of a dancer is a component reflected in aesthetic
724 perception, it was not well captured quantitatively by jerk metrics. Perhaps the way our brain
725 perceives and the way we view movement is that which simplifies the movement into the fewest
726 organizational groupings; in this case, PCA. A movement with a low PCA dimensionality is
727 highly constrained and possesses significantly fewer generalized degrees of freedom than joint
728 variables. The experienced dancers revealed lower PCA dimensionality, and it was these
729 dancers that were most ranked as most aesthetically proficient. This suggests that reduction of
730 redundant information, a simplistic dimensionality, may be an important part of observer
731 perception. Our model of the biological determinant of aesthetics suggests that the brain is
732 tuned to value movement grace, clarity, fluidity, and efficiency of intent, that is found in the
733 beauty of dance.

734 In a study employing linear and nonlinear metrics to analyze a complex movement, we
735 found that the nonlinear PCA was the most promising tool for the quantification of this art form.
736 Further study of dance biomechanics using PCA may provide insight into motor learning, motor
737 control, and neuro-aesthetics.

738

739 **Acknowledgments**

740 We thank the participating dancers and other volunteers.

741

742 **Conflict of Interest**

743 The authors declare that they have no conflict of interest.

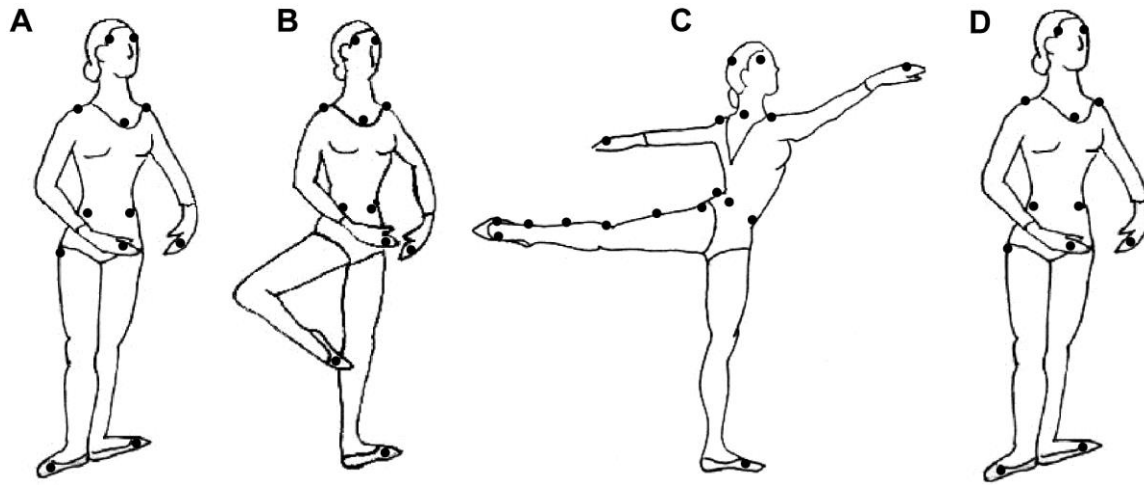
Table 1. AICc models of aesthetic rankings

Model	Predictors	Parameters	AICc	Δ AICc	F	df	p
1	5	PCA	542.475	86.556	25.734	84,1	<0.0001
		hip ang jerk			1.736	84,1	0.191
		toe jerk			1.006	84,1	0.319
		MSD pelvis-hip			0.01	84,1	0.92
		MSD toe			7.967	84,1	0.006
2	1	PCA	455.919	0	46.367	88,1	<0.0001
3	3	hip ang jerk	572.012	116.093	1.357	87,1	0.247
		toe jerk			5.063	87,1	0.027
4	1	toe jerk	520.174	64.255	8.743	88,1	0.004
5	2	MSD pelvis-hip	483.974	28.055	4.451	87,1	0.038
		MSD toe			10.978	87,1	0.001
6	1	MSD toe	485.193	29.274	17.748	88,1	<0.0001

745 Abbreviations: AICc, Akaike Information Criteria corrected; Δ AICc, change in AIC; PCA,
746 principal component analysis; ang, angular; MSD, mean standard deviation.

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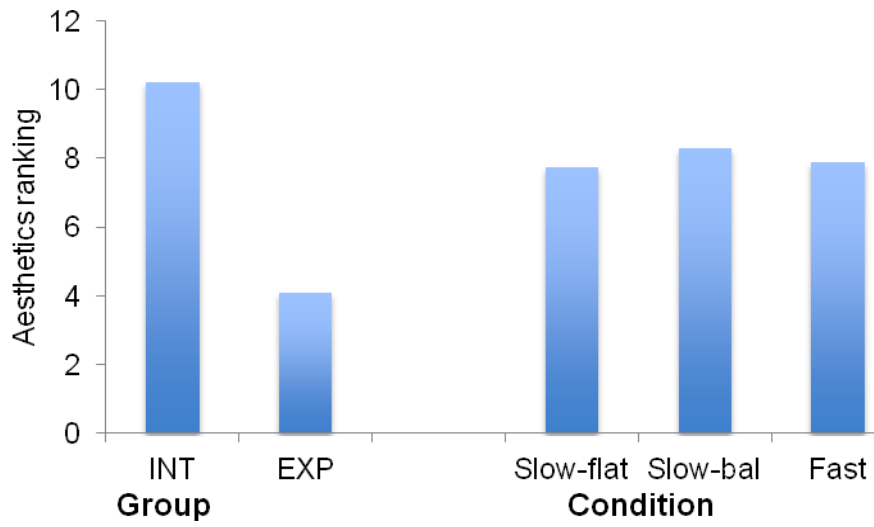
752 Fig. 1 Arabesque sequence for the Slow-flat and Fast conditions: A) First position, B) Passé,

753 C) Arabesque, D) First position. In the Slow-bal condition, the dancers rises onto their forefoot

754 during the arabesque and briefly holds it before returning to first position.

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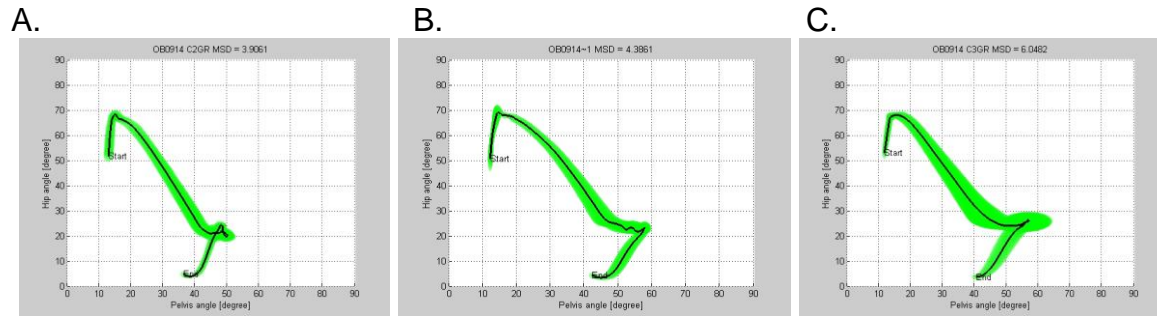
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758 Fig. 2 Aesthetic proficiency ranking. Median for Group and Condition. Note: lower ranking
759 denotes greater aesthetic excellence.

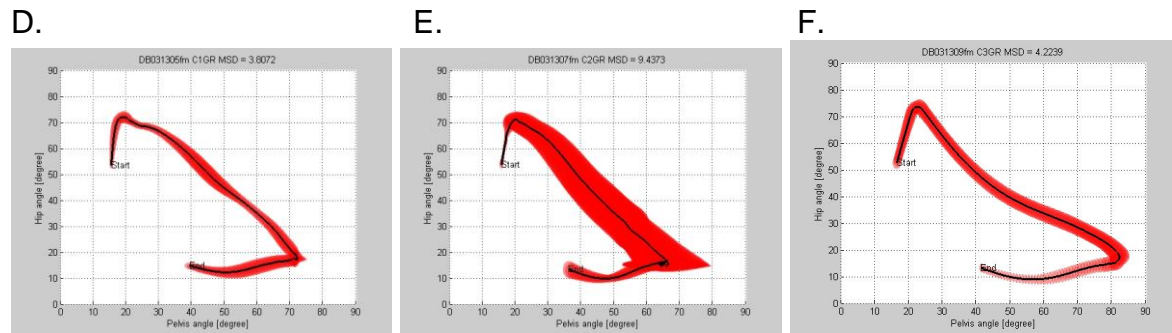
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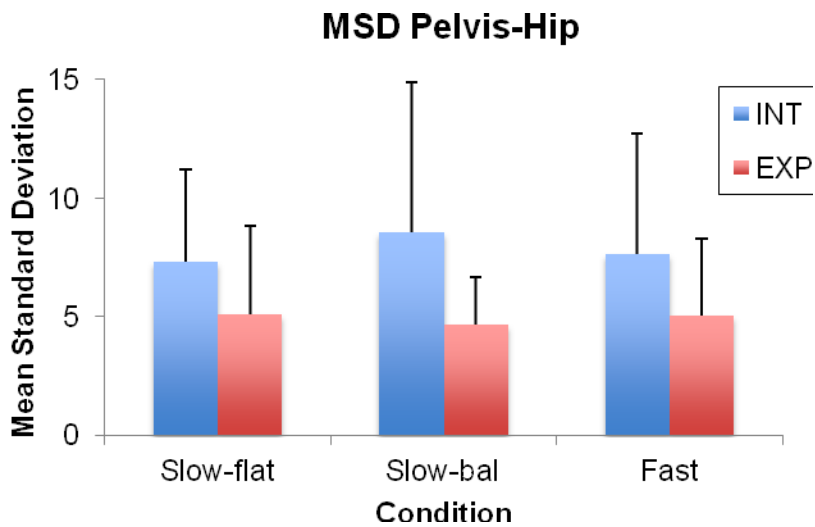


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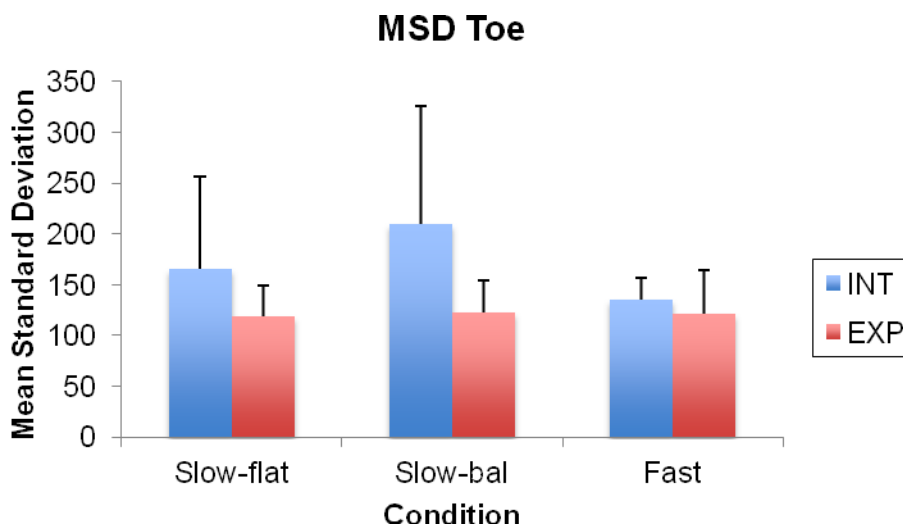
769 Fig. 3 Mean standard deviation (MSD) 3-D pelvis-hip angle-angle plots of representative
770 subjects. The pelvis is on the x-axis and hip is on the y-axis, the EXP subject is seen in green
771 and INT subject is in red. A-C. The trial was decomposed into its constituent excursions (six per
772 trial). On each plot is a line which represents the mean of the excursions together with an
773 envelope which indicates ± 1 standard deviation of the excursion trajectories. The colour of the
774 envelope is red for the INT and green for the EXP dancer. A-C. Representative EXP subject
775 performing six excursions of the three conditions: A) Slow-flat, B) Slow-bal, and C) Fast. D-F.
776 Representative INT subject performing six excursions of the three conditions: D) Slow-flat, E)
777 Slow-bal, and F) Fast.

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781 A.



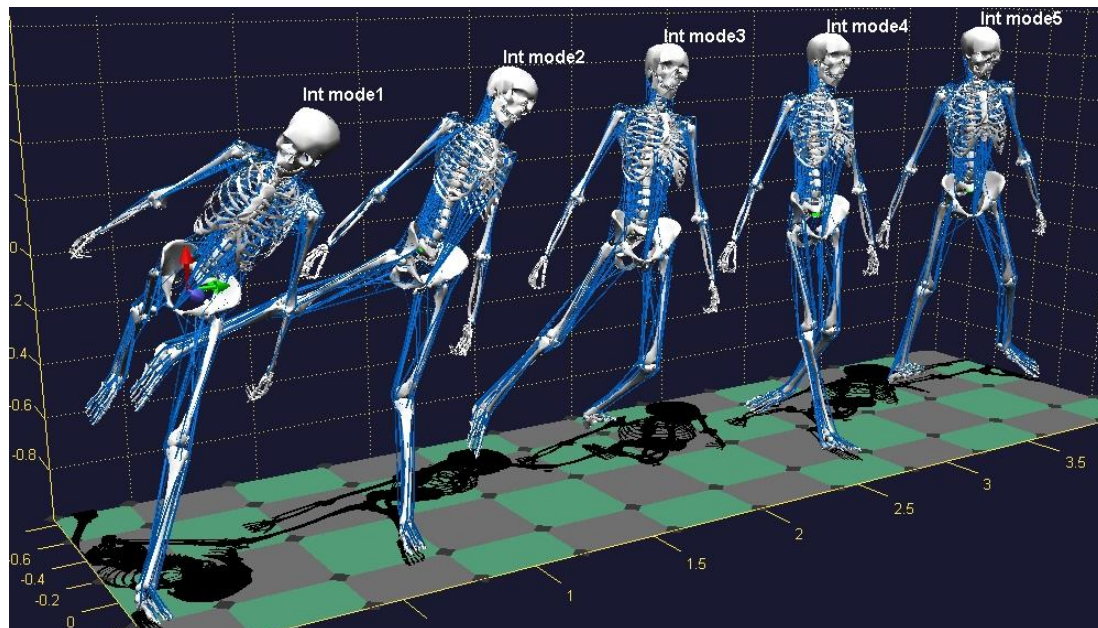
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783 B.



784
785 Fig. 4 Mean standard deviation (MSD) (SD) for 3-D segmental coordination. A) 3-D pelvis-hip
786 angle-angle; and B) 3-D toe displacement (INT group blue, EXP group red).
787

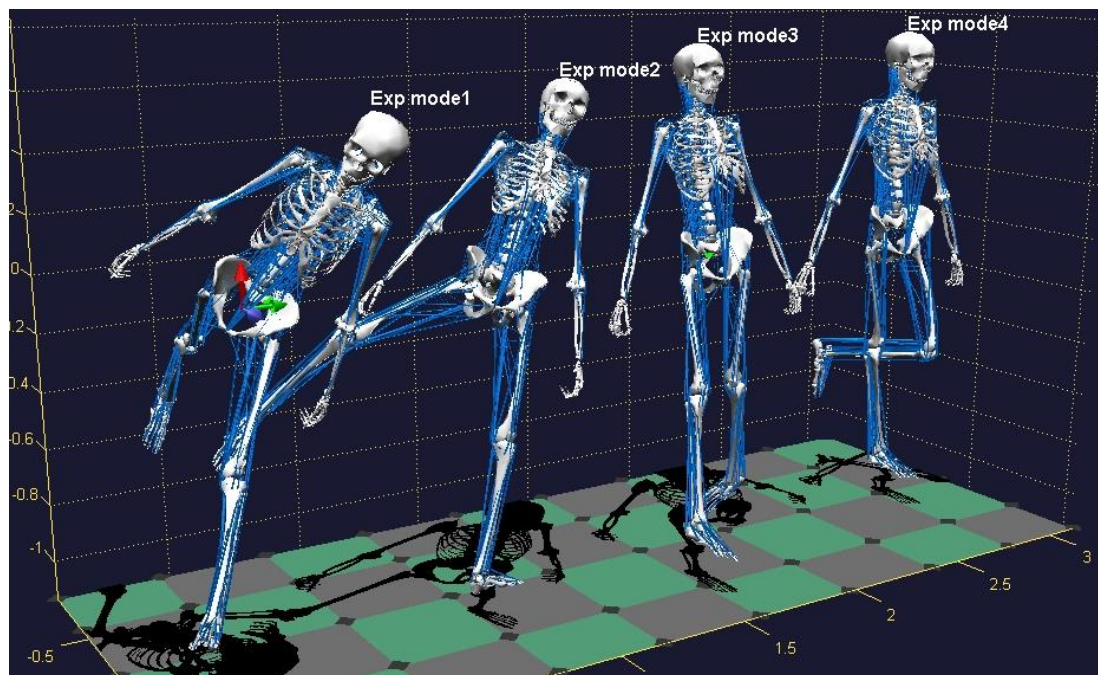
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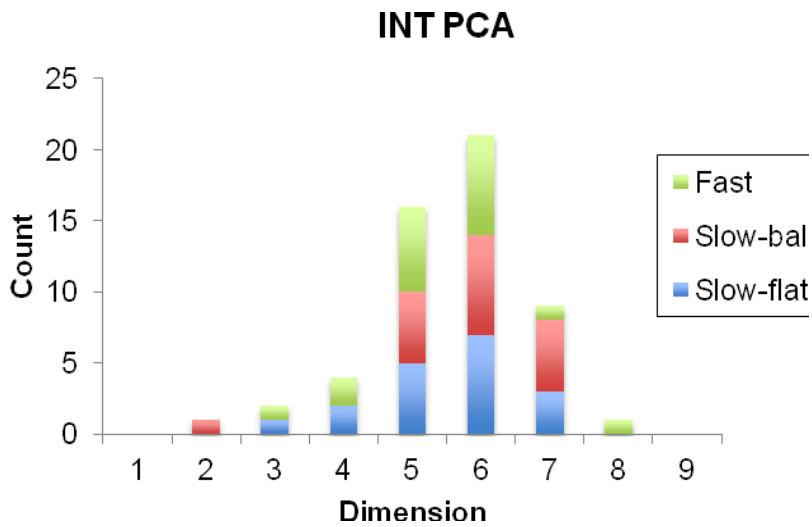
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Fig. 5 Principal components. A) Examples of the five modes which accounted for 98% of the variability of the motion of an INT dancer. B) Examples of the four modes which accounted for 98% of the variability of the motion of an EXP dancer.

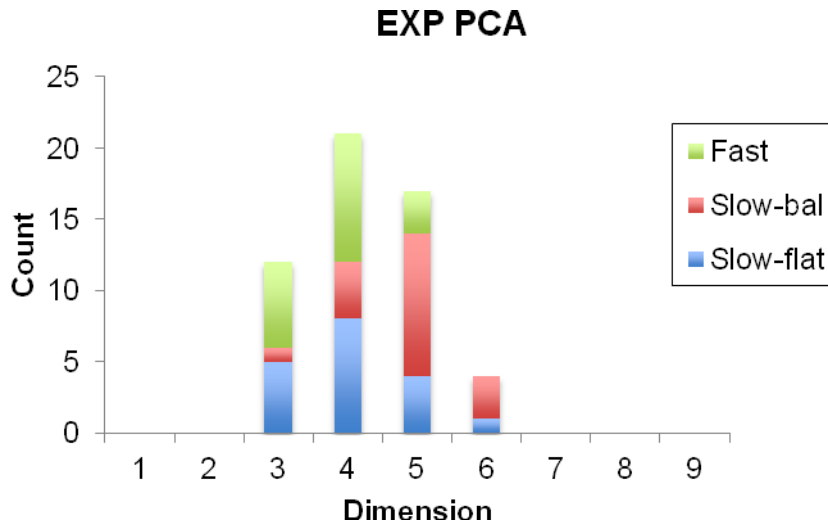
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805 Fig. 6 Principal component analysis. A) Mean dimensionality of the state manifold for the INT

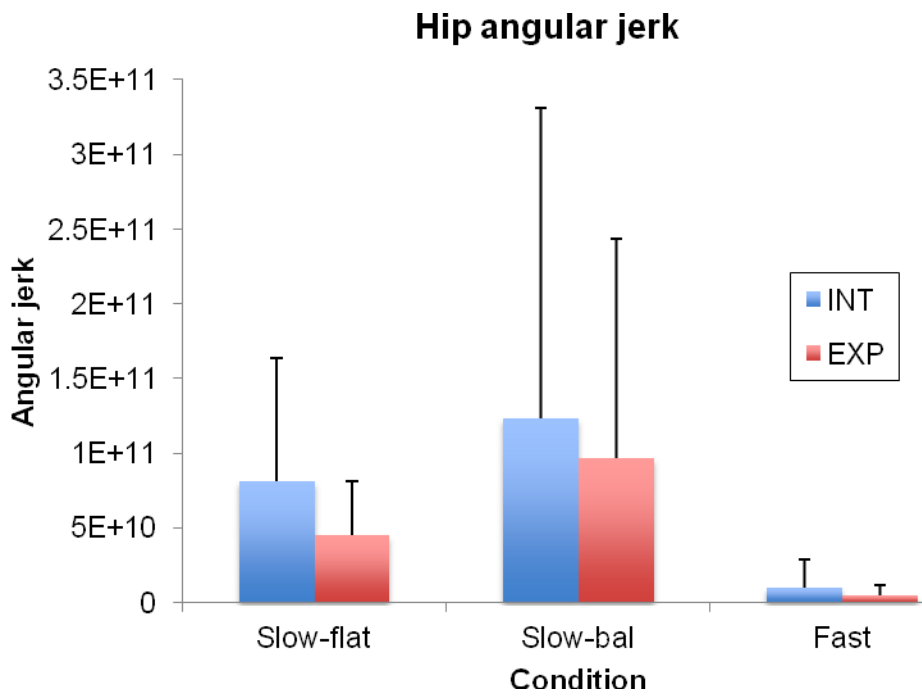
806 group; B) Mean dimension for the EXP group (Blue is Slow-flat, Red is Slow-bal, and Green is

807 Fast condition).

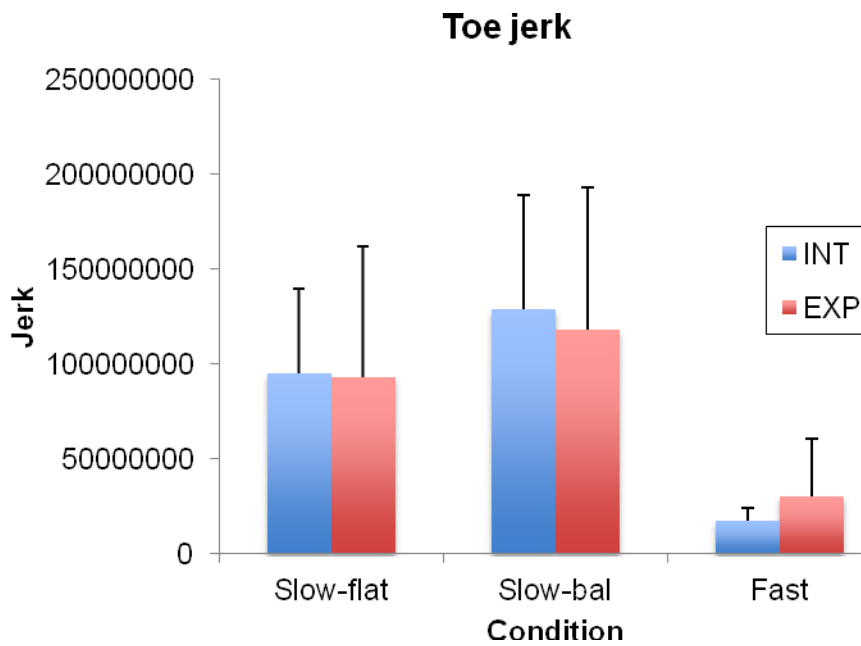
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811 A.



812
813 B.



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815
816 Fig. 7 Mean (SD) dimensionless jerk. A) Sagittal plane gesture hip angular jerk; B) 3-D gesture
817 toe jerk (INT group blue, EXP group red).

818

819 **References**

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