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# A Hybrid and Adaptive Tool-path Generation Approach of Rapid Prototyping and Manufacturing for Biomedical Models

G.Q. Jin<sup>1</sup>, W.D. Li<sup>1\*</sup>, L. Gao<sup>2</sup>, K. Popplewell<sup>1</sup>

<sup>1</sup> Faculty of Engineering and Computing, Coventry University, Coventry CV1 5FB, UK

<sup>2</sup> State Key Laboratory of Digital Manufacturing Equipment and Technology, Huazhong University of Science and Technology, Wuhan 430074, PR China

\* Corresponding author: Tel: +44 (0)2476 88 8940; Email: weidong.li@coventry.ac.uk

## ABSTRACT

In this paper, a hybrid and adaptive tool-path generation approach, which is able to improve geometrical accuracy and build time of Rapid Prototyping/Manufacturing (RP/M) for complex biomedical models, is presented. Firstly, NURBS (Non-Uniform Rational B-Spline)-based curves were introduced to represent the boundary contours of sliced layers to keep the high-fidelity information of original models. Secondly, a hybrid tool-path generation algorithm was then developed to generate contour and zigzag tool-paths. The contour tool-paths are used to fabricate the boundary and neighboring regions of each sliced layer to preserve geometrical accuracy, and zigzag tool-paths for the internal region of the layer to simplify computing processes and speed up fabrication. Thirdly, based on developed build time and geometrical accuracy analysis models, algorithms were designed to generate an adaptive speed of the RP/M's nozzle/print head for the contour tool-paths to address the geometrical characteristics of each layer, and to identify the best slope degree of the zigzag tool-paths towards achieving the minimum build time. Finally, five case studies of biomedical models with different geometrical characteristics and complexity were used to verify and demonstrate the improved performance of the approach in terms of processing effectiveness, geometrical accuracy and algorithm robustness.

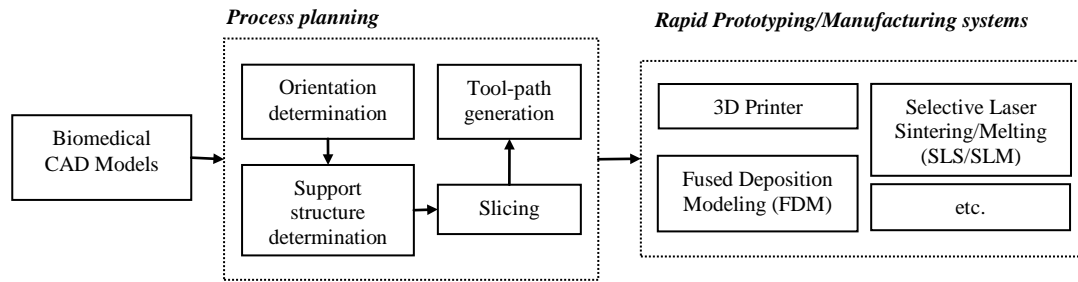
**Keywords:** Rapid Prototyping, Rapid Manufacturing, Tool-path Generation, Biomedical Model

## 1. Introduction

In healthcare applications, a biomedical model of a patient offers surgeons a direct, full understanding of a patient's anatomy that cannot be obtained from Computed Tomography (CT) and Magnetic Resonance Imaging (MRI) images. Such a model can help surgeons identify diseases more easily for diagnosis and treatment planning, and reduce the risk of medical and operation problems. However, biomedical models such as anatomy model and patient specific implants are usually characterized with highly customized and complex geometry. It is difficult for the conventional manufacturing and machining processes such as forming, casting, turning and milling, etc. to fabricate the models. The Rapid Prototyping/Manufacturing (RP/M) technology has been identified as an innovative manufacturing technology in recent years [1]. Different from conventional forming and machining processes, it is an additive forming process by adding materials, layer-by-layer, as specified by a Computer-Aided Design (CAD) systems. The distinguished advantage of RP/M is that it is a mould-less process, suitable for free-form and complex geometrical model realization [2]. This kind of geometric flexibility of the RP/M technology and the complexity of biomedical models are the main reasons that RP/M is increasingly used in biomedical applications [3]. For complex biomedical models, it still needs to improve the current process planning strategies in the RP/M software packages significantly in the aspects of build time and geometrical quality. For instance, it could take tens of hours to process relatively small parts resulting in high cost of prototype manufacturing. Another challenging issue is geometrical inaccuracy inherent from the additive forming mechanism of RP/M, which is the obstacle to achieve high geometrical quality of biomedical products. Owing to quickly developed healthcare markets, it is imperative to develop more effective algorithms in RP/M to minimize build time and improve geometrical accuracy in order to meet the high-quality design and functional requirements of complex biomedical models [4].

Process planning is a critical task in RP/M to determine the build efficiency and geometrical accuracy. It consists of four essential tasks, i.e., orientation determination, support structure determination, slicing and tool-path generation (shown in Figure 1). The research presented in this paper focuses on the tool-path generation strategy in process planning to balance and optimize the build efficiency and geometrical accuracy of RP/M. A tool-path is the trajectory of the nozzle (e.g., in a Fused Deposition Modeling (FDM) system)/print head (e.g., in a 3D Printer) in a RP/M process to fill the boundary and interior areas of each sliced layer. Various types of

tool-path strategies and algorithms, such as zigzag, contour, spiral and partition patterns, were developed with different considerations on the build time, cost, geometrical quality, warpage, shrinkage, strength and stiffness of a RP/M model [5-11].



**Figure 1** Process planning and tool-path generation for RP/M systems.

In this paper, a novel tool-path generation approach was developed to improve the RP/M model representation, tool-path generation and nozzle/print head speed control to be adaptive to the various geometrical properties of complex biomedical models. The approach includes the following algorithms:

- A slicing algorithm was designed to represent the boundary (contour) of each sliced layer in a Non-Uniform Rational B-Spline (NURBS) curve. The NURBS-based representation can enhance the geometrical accuracy of a model during RP/M and replaces STL (Stereolithography)-based representation strategy, which is a de facto but less accurate standard to support RP/M in industries;
- For each layer, a hybrid tool-path generation algorithm was designed to generate a series of contour and internal offset tool-paths along the NURBS-based represented boundary of the model to improve the geometrical quality during RP/M, and zigzag tool-paths for the internal area of the model to simplify computing and fabrication processes. Also, an adaptive speed algorithm was developed to optimize the speed of the RP/M's nozzle/print head adaptively for the various geometries of the model so as to improve the efficiency of contour tool-paths and with the most suitable slope degree of zigzag tool-paths leading to the shortest build time.
- To demonstrate the performance of this research in terms of processing efficiency and geometrical accuracy, five case studies of biomedical models with different geometrical characteristics and complexity were used for research verification.

## 2. Related Works

### 2.1 Model representation of RP/M

In RP/M, STL has been a widely adopted data standard. However, STL is less inaccurate in geometrical representation and needs much more storage spaces for a complex model than parametric mathematical representation themes, such as NURBS, Bezier, B-Spline, etc. Recently, there are active research and development to introduce parametric mathematical representation to better support models of RP/M. In [12-13], arcs, lines and Bezier curves were used to describe the cross-sectional contour geometries of sliced layers. In the approach, a macro-AutoSection software package was developed to collect the sliced contour data and to support the RP/M process for a commercial Selective Laser Sintering (SLS) machine. In [14], an approach was developed to use lines, arcs and circles to represent the sliced contours of an AutoCAD solid model in an ASCII DXF file. Material information such as material type can also be saved to support RP/M. Ma et al. used NURBS to represent a RP/M model so as to obtain more accurate and smoother surface. In the meantime, a selective hatching strategy was applied to reduce build time and improve geometrical quality by fabricating the kernel region of the model using thicker sliced layers and the skin region of the model using thinner sliced layers [15]. In [16], a slicing algorithm was developed to use STEP and NURBS to represent a RP/M model. The algorithm consists of five steps: (1) to determine the orientation of a model to minimize build height, (2) to define the NURBS surface of the model, (3) to generate a boundary volume data structure, (4) to use a bi-sectional iteration routine method to solve the inter-sectional points, and (5) to categorize inter-sectional points to support an optimized RP/M process. Four models in different representation formats were used to validate the developed algorithm. In [17], a B-spline curve was reconstruction from cloud data to represent the contour curve of the model. Cloud point data was segmented to a number of layers along the fabrication direction of RP/M. The points were then projected to generate a 2D band on the mid-plane layer. A number of scattered points were

picked up along the band and a B-spline curve was fitted to represent the contour curve of the layer. In [18], NURBS-based curves, surfaces, and solids are used to represent the anatomical modeling for RP/M fabrication. Cloud point data was first obtained from CT and MRI. The commercial medical imaging processing software (MIMICS) and computer-aided design software packages were then used for generating NURBS-based curves of the anatomical modeling.

In order to reduce modeling time and shorten overall time-to-market for Reverse Engineering (RE)-based products, research was developed to integrate the RE technology and RP/M representation by modeling point from cloud data generated by a Coordinate Measurement Machine (CMM) to support RP/M. A novel algorithm was designed to build a bridge between scattered points, and a slicing algorithm was designed to integrate RE-based data and RP/M [19]. The research has the following steps: (1) part digitization, (2) segmentation, (3) NURBS or B-Spline-based surface construction based on the segmented cloud data, and (4) slicing processing. An approach to generate a RP/M slicing file directly from image data was presented [20]. A digital camera was used to generate the cross-sectional images of a RE-based product, and the contour data of the product was computed and an algorithm was developed to generate a STL file and a RP/M slicing file from the contour data.

Some of the above research successfully adopted parametric representation such as Bezier, B-Spline and NURBS to improve the geometrical quality of RP/M models. However, a research gap exists between the parametric representation and the tool-path generation, and a smart tool-path solution is imperative to address the different geometrical characteristics of complex biomedical models in order to improve the build efficiency and geometrical accuracy of RP/M.

## 2.2 Tool-path generation in RP/M

In RP/M, a tool-path is the trajectory of the nozzles/print head to fill the boundary and interior of each sliced layer. The design of tool-paths will determine the geometrical quality, strength and stiffness of a model to be built, and efficiency of the RP/M process. Various types of tool-path patterns have been developed for RP/M, such as zigzag, contour, spiral and some space filling curves. A summary is shown in Table 1, and more explanations are given below.

**Table 1** A summary of tool-path generation approaches in RP/M.

<i>Works</i>	<i>Tool-path patterns</i>	<i>Major characteristics</i>
Misra and Chang [5-6]	Zigzag	The approach fills a layer along the X, Y or a specific direction, and it is easy for approach implementation but poor on geometrical quality.
Yang and Genesan [7-8]	Contour	The approach builds a layer along its contour and offset curves following the boundary of the model. It ensures good geometrical quality but takes longer during model build compared to the zigzag tool-path generation.
Bertoldi et al. [9]	Recursive Hilbert's curve	More suitable for some regular boundaries and special geometric models. The build time will be longer than that of other conventional tool-path generation methods.
Lou et al. [10]	Spiral	More suitable for some special geometrical models due to improved computation.
Chiu et al. [11]	Fractal curve	It is only suitable for some special fractal models.

The zigzag tool-path generation is a typical method used in RP/M systems. Tool-paths will fill models line-by-line along specific directions [5-6]. Though easy to implement, the generation has the following drawbacks: (1) if a model for RP/M is complex or has some hollow structures inside, some typical RP/M systems like SLS/Selective Laser Melting (SLM) and Fusion Deposition Modeling (FDM) have to position and reposition the print heads/nozzles frequently, leading to a poor building quality; (2) the model usually will have a warpage problem, which is caused by the fact that the tool-path will be along the same direction to build the whole model. The contour tool-path generation, which is another typical method, can improve the geometrical quality of models effectively by following the geometrical trend of the boundary contours [7-8]. Meanwhile, the method overcomes the warpage problem based on that fact that the tool-path direction is changed constantly along the contour curves of sliced layers. Nevertheless, when a boundary contour is irregular or has a hollow, island or ring structure, such as biomedical models, the computation process of the algorithms will be complicated.

For some special requirement, such as strength, stiffness and model bonding for some parts made by RP/M, space filling curves with pre-defined shapes were also been used for tool-path generation. A fractal approach was developed to generate Hilbert curve-based tool-paths for a FDM RP/M system [9]. Based on the method,

shrinkage during the RP/M fabrication process can be minimized but build time will be usually longer than that of traditional tool-path generation methods. The spiral tool-path generation was widely used in NC machining, especially for 2D pocket milling and uniform pocket cutting [10]. It can also be applied to solve the problems of zigzag tool-paths in the FDM process, but be more suitable for some special geometrical models due to complex computation. A novel method was developed to generate the tool-path of RP/M from the mathematical model of a fractal model [11]. It first generates a slab grid in each layer that consists of a number of pixels, and then checks the interior property of each pixel in the slab grid to create the slab model of the fractal model. The boundary of slab model is refined and the tool-path of RP/M can be generated from these boundaries. However, these research works could be only suitable for fractal models.

Based on the potentials of the above research in different conditions, it is expected to develop a smart and hybrid (combined) strategy to leverage the advantages of various tool-path generation strategies to be suitable for complex models in the RP/M processes.

### 2.3 Evaluation models and strategies in RP/M

Build time is an important factor to be considered in RP/M. Some build time analysis and prediction models were developed. A detailed study of the laser scan mechanism in a SLS process was made in [21]. With the measurement results of different scan patterns and curing depths, formulas, which can be used to predict the total build time and the resultant curing depth for different laser powers, beam diameters and input curing depths of the SLS process, were developed. The work, however, only considered the total laser scan time and total recoating time, while more factors contributing to the total build time need to be incorporated to further improve the predictor. A build time analysis model for a FDM process was developed in [22]. The method takes account not only the deposition time, idle time, and nozzle repositioning time, but also cleaning time in the analysis model. Some parameters used to speed up the build time of FDM, including layer thickness, road width, table speed and repositioning distance and so on were identified. However, the research is specific for some deposition-based (FDM) RP/M processes.

To minimize build time spent on on-fabrication motion of tool-path generation, some heuristics algorithms were designed. The Asymmetric Traveling Salesman Problem (TSP) and Integer Programming (IP) was combined to design the time model [23]. From the model, two enhanced Genetic Algorithms (GA) were introduced to achieve the minimum time of the non-fabrication motion of RP/M. Another algorithm was developed for minimizing non-fabrication time by optimally connecting different tool-path segments [24]. The non-fabrication time problem was first formulated as a standard TSP in which precedence constraints were considered, and then some heuristic methods were applied to solve this problem. The disadvantage of the method is that it is difficult to be applied to complex biomedical models such as those including hollows and complex contours.

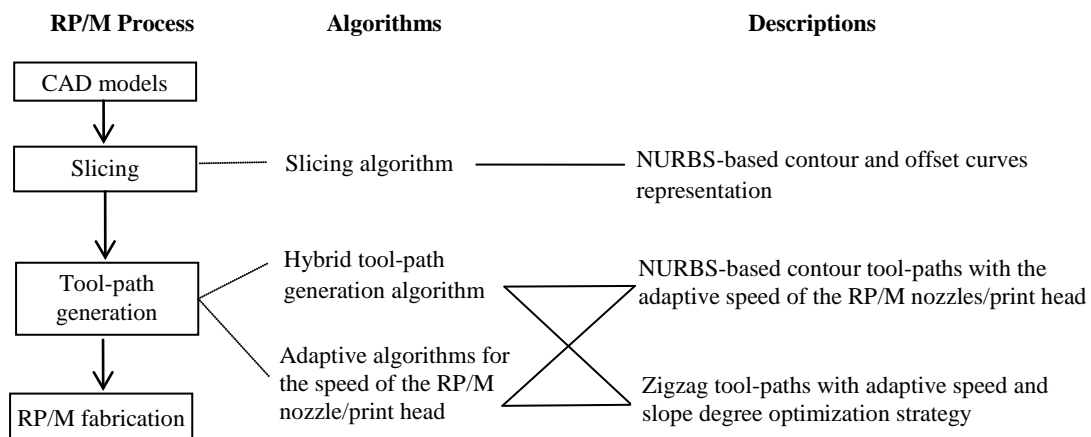
In RP/M, another important issue is how to evaluate the geometrical quality. Geometrical errors interaction and transferring mechanisms in the RP/M process were studied, in which a physical model was used to define the error interactions and transferring mechanisms [25-26]. Based on the geometrical approximation techniques, a geometrical model was developed to describe the relationships of geometrical errors. Then, based on a developed mathematical model, the effect of transformation of local errors was analyzed to obtain the global errors of multiple layers. The problem of the aforementioned method is that the described geometrical errors only involve profiling error, layer inclination and layer thickness variations, while other elements affecting the geometrical accuracy of RP/M process should be considered as well to further improve the mathematical analysis model. The effect of process parameters on the surface roughness of SLS was studied with the help of central rotatable composite design (CCD) of experiments [27]. Analysis of variance was made to study various surface roughness based on different build orientation, laser power, layer thickness, beam speed, and hatch spacing. A trust-region-based optimization method was employed to obtain a set of process parameters for obtaining the best surface finish. In [28], an approach to assess surface quality on textured surface in a FDM system was developed. The method developed a benchmark polygon model with different feature sizes and aspect ratios for fabrication in a FDM system with different build orientations. Based on that, the verification of surface quality with different texture dimensional parameters on textured surfaces of the model was analyzed. However, the testing results are still limited to a specific process.

Based on the above observations, innovative and adaptive strategies are desirable to develop more suitable and sensible build time mathematical module and geometrical accuracy mathematical module to evaluate various tool-path generation approaches, with a bid to further reduce the total build time and enhance geometrical accuracy during RP/M processes.

### 3. Research Methodology and Algorithms

The developed methodology and algorithms are shown in Figure 2, which consists of the following two phases:

- Phase 1: A slicing algorithm is used to represent the boundary contour of each sliced layer as a closed NURBS curve to maintain the representation accuracy of an original biomedical model;
- Phase 2.1: A hybrid tool-path algorithm is used to generate contour and zigzag tool-paths for each layer to meet both the geometrical accuracy and build efficiency requirements. The contour tool-paths are used to fabricate the region along the boundary of each sliced layer to improve the geometrical quality of the model. The zigzag tool-paths are used to fabricate the interior region of the model to improve the computation and fabrication efficiency;
- Phase 2.2: Build time and geometrical accuracy analysis models are used for contour and zigzag tool-path computation and evaluation. Based on the models, adaptive nozzle/print head speed algorithms are designed to address the different geometrical characteristics of the model and achieve minimum build time. They include an algorithm to optimize the speed of the RP/M's nozzle/print head along the contour tool-paths, and an algorithm to obtain the best slope degree of the RP/M's nozzle/print head along the zigzag tool-paths.



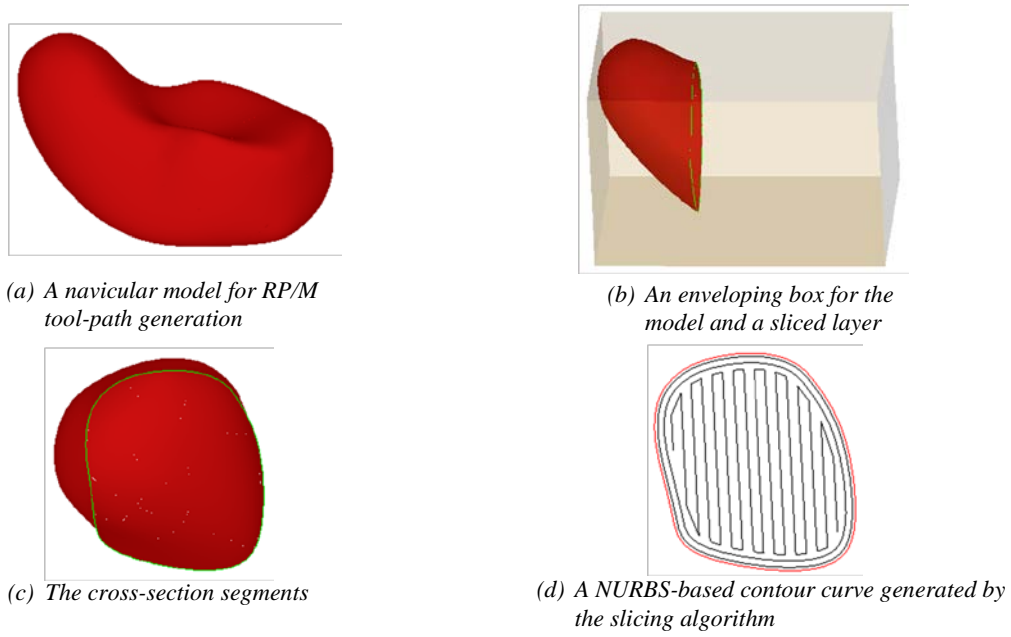
**Figure 2** The process of algorithms for tool-path generations.

#### 3.1 Phase 1 – slicing and NURBS-based contour curve representation

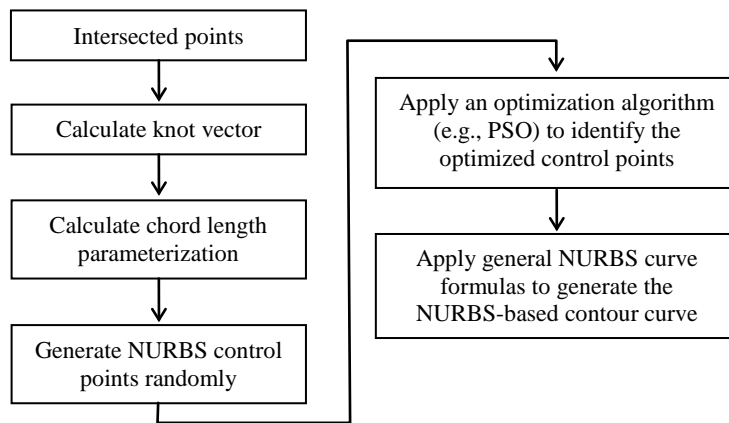
In this research, cloud data from a biomedical model is reconstructed as an IGES/IGS model using the Quick Surface Reconstruction (QSR) and Digitized Shape Editor (DSE) modules in CATIA V5™. The reconstructed model is then read into the developed software platform, which was developed based on the C++ programming language in an open-source CAD kernel system - the Open CASCADE [29]. In the process, a container is created to envelop the model, and the shortest edge of the enveloping box is determined as the orientation direction (Z axis) to minimize the build time. A series of sliced layers perpendicular to the orientation direction are set. The NURBS-based curve representation is introduced to model the geometrical contour between a sliced layer and the model. In Figure 3, a navicular model of human left feet is used to illustrate the above process.

In order to establish the NURBS-based contour curve on the boundary between a sliced layer and the model (the boundary will be represented as  $C^{i,1}$  in the following), a fitting algorithm based on the intersected points between the sliced layer and the model is used here [30]. A flow of the algorithm is shown in Figure 4. The generated contour curves can be further classified into two types defined as follows:

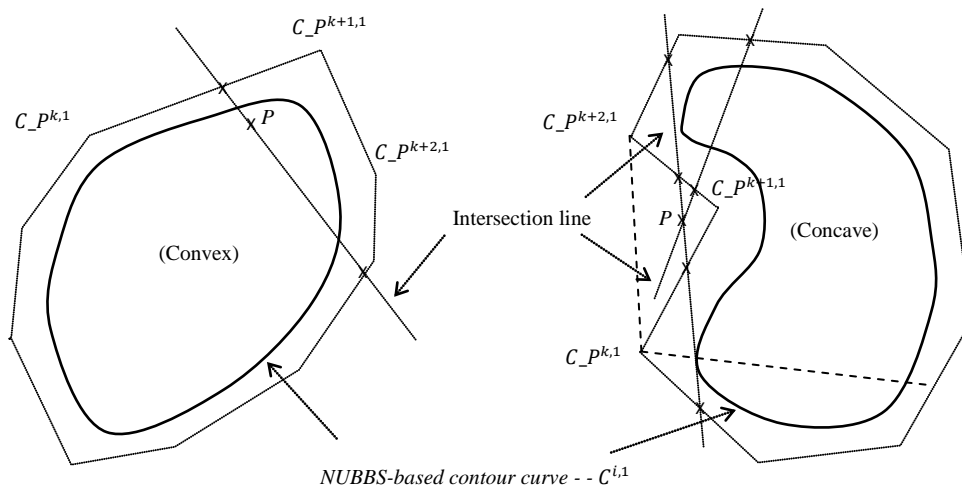
- A control point  $C_{P^{k+1,1}}$  and its two neighbor control points  $C_{P^{k,1}}$  and  $C_{P^{k+2,1}}$  form a triangle. Choose a random point  $P$  on the boundary or inside of the triangle, and draw a line to pass it. If the line only has two intersected points with the box formed by all the control points (the grey area in Figure 5), and  $P$  is between the two intersected points, the control point  $C_{P^{k+1,1}}$  is defined as convex; Otherwise, the control point  $C_{P^{k+1,1}}$  is concave;
- If all the control points of a NURBS-based contour curve are convex, the curve is defined as a Type I contour curve. Otherwise, the curve is a Type II contour curve.
- Two examples for a *Type I* contour curve and a *Type II* contour curve respectively are illustrated in Figure 5.



**Figure 3** An example to illustrate the slicing process of the developed approach.



**Figure 4** The flow of generating a NURBS-based contour curve of a sliced layer.



**Figure 5** Examples of two different types of contour curves.

### 3.2 Phase 2.1 – offset curve generation and an adaptive speed algorithm for contour tool-paths

#### Offset curve generation for a Type I or Type II contour curve

##### Type I contour curve

Based on the central point of the control points of the above generated contour curve, each control point for a new NURBS-based curve that offsets the contour curve (i.e., offset contour curve) is computed in the following.

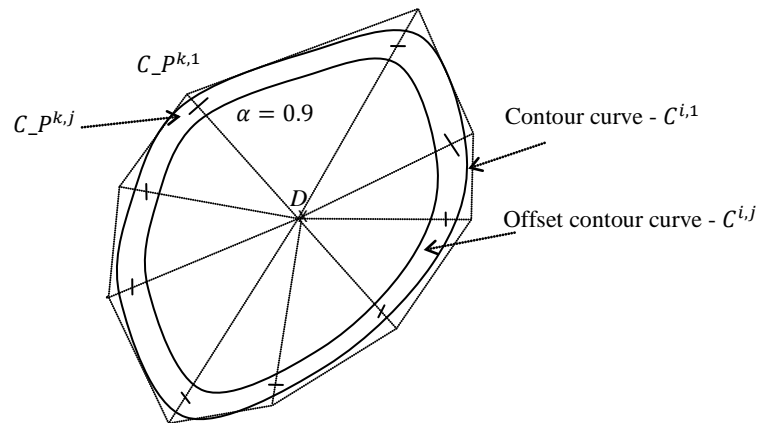
$$C_{P^{k,j}} = D + \alpha \cdot (C_{P^{k,1}} - D) \quad (1)$$

where  $C_{P^{i,j}}$  represents an offset contour curve in the  $i^{\text{th}}$  layer;  $D$  represents the geometric central point of the control points of the contour curve;  $\alpha$  is the ratio to generate the new control points of the offset contour curve (e.g.,  $\alpha$  is set 0.9 in the following example). It is determined by the diameter of the RP/M's nozzles/print head and the overlapping rate between two neighbor tool-path lines.

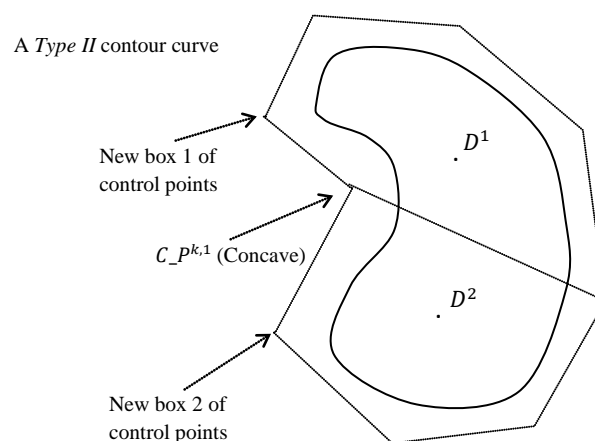
For instance, in Figure 6, a new control point  $C_{P^{k,j}}$  of an offset contour curve is computed as follows.

$$x(C_{P^{k,j}}) = x(D) + 0.9(x(C_{P^{k,1}}) - x(D)), \text{ and}$$

$$y(C_{P^{k,j}}) = y(D) + 0.9(y(C_{P^{k,1}}) - y(D)).$$



**Figure 6** New control points of an offset contour curve along boundary.



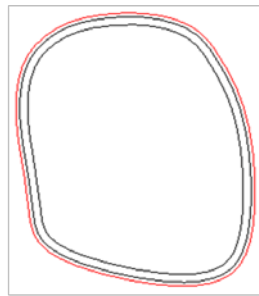
**Figure 7** An example for processing a Type II contour curve.



*Type II contour curve*

In the box of the control points of a *Type II* contour curve, each concave point will be connected with another control point in the box to separate the box as two or more control point boxes, where each control point is convex. An example is shown in Figure 7. In each box, new control points for offset contour curves are generated using the above Formula (1). Then all the control points in a control point box are then used to generate an offset contour curve.

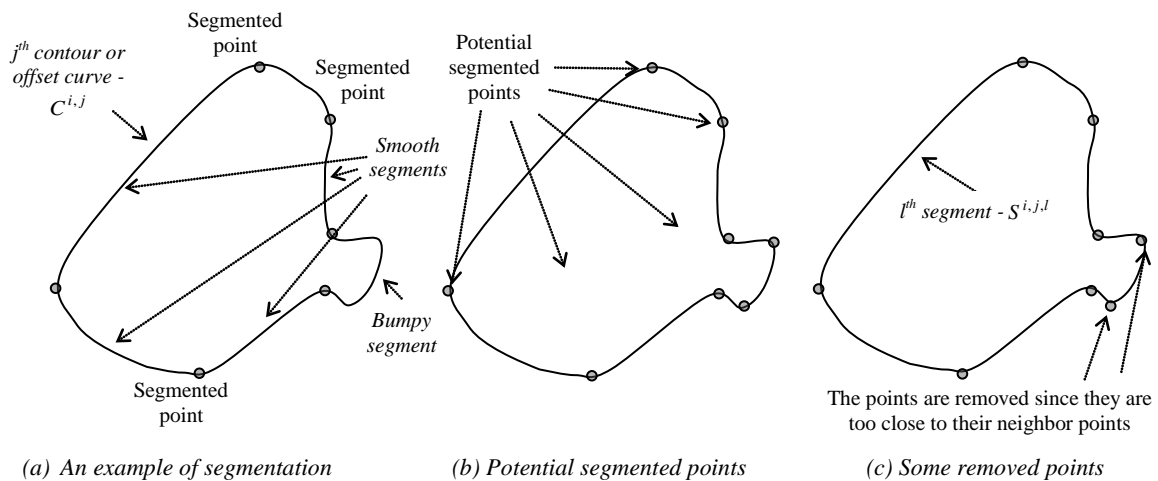
With a series of  $\alpha$ , the control points and the offset contour curves can be generated. Figure 8 shows the generated contour and offset tool-paths for the tibia model. Along the contour curve and its series of offset contour curves, NURBS-based contour tool-paths can be interpolated.



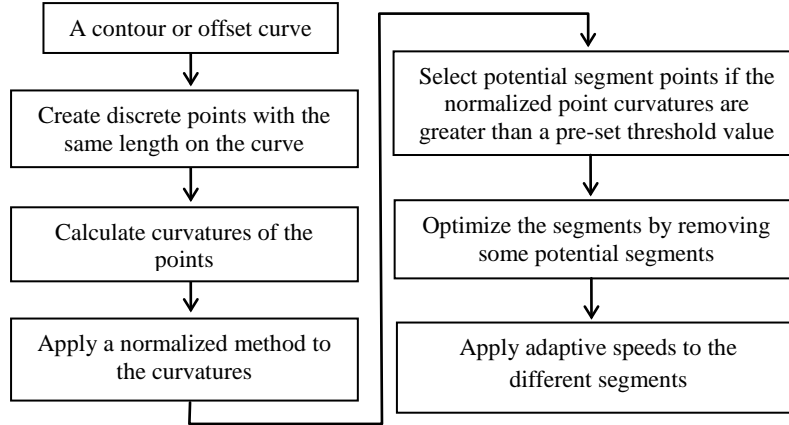
**Figure 8** Contour and offset tool-paths generated for the navicular model.

Adaptive speed algorithm of the RP/M's nozzle/print head along the contour tool-paths

In order to further optimize the build time, a contour or offset curve on a sliced layer is segmented according to its geometrical characteristics (e.g., curvature). For instance, the segmented points in Figure 9(a) are used to divide the curve as bumpy and smooth segments. According to the smoothness of a segment, an adaptive algorithm is applied to slow down the speed of the RP/M's nozzle/print head in the bumpy segments while keeping a higher speed in the smooth segments to ensure better build quality and optimized build efficiency. The flow of the segmentation and adaptive algorithm of the RP/M's nozzle/print head is shown in Figure 10. Explanations are expanded below.



**Figure 9** Examples to illustrate the segmentation process for the adaptive speed algorithm.



**Figure 10** The flow of the segmentation and adaptive speed algorithm for tool-paths.

A series of discrete points with the same length along a contour or offset curve are set. The curvatures of the points are normalized according to the following formula:

$$Normalization(P^t) = \frac{P_{curvature}^t - Min_{curvature}}{Max_{curvature} - Min_{curvature}} \quad (2)$$

where  $P_{curvature}^t$  represents the curvature of Point  $t$  on the curve;  $Min_{curvature}$  and  $Max_{curvature}$  stand for the minimum and maximum curvatures of all the points respectively.

A threshold is set to filter out the discrete points with low curvatures, and the discrete points passing the threshold are kept as potential segmented points (see the example in Figure 9(b)). Another threshold is set to remove those potential segmented points which distance from their neighbor potential segmented points is within this threshold (see the example in Figure 9(c)). Based on the segmentation process, the build time of the tool-paths on each contour or offset curve can be defined below.

$$Time(C^{i,j}) = \sum_{l=1}^m (Time(S^{i,j,l})) \quad (3)$$

where  $Time$  represents build time;  $C^{i,j}$  represents the  $j^{th}$  contour or offset curve on the  $i^{th}$  layer (a set of tool-paths will be generated along each curve);  $S^{i,j,l}$  represents the  $l^{th}$  segment in  $C^{i,j}$ ;  $m$  is the total number of the segments in  $C^{i,j}$ .

$Time(S^{i,j,l})$  is further computed in the following. An adaptive speed algorithm for the RP/M's nozzle/print head along the tool-paths was developed. An example shown in Figure 11 is used to illustrate the concepts in the algorithm and the computation of  $Time(S^{i,j,l})$ .

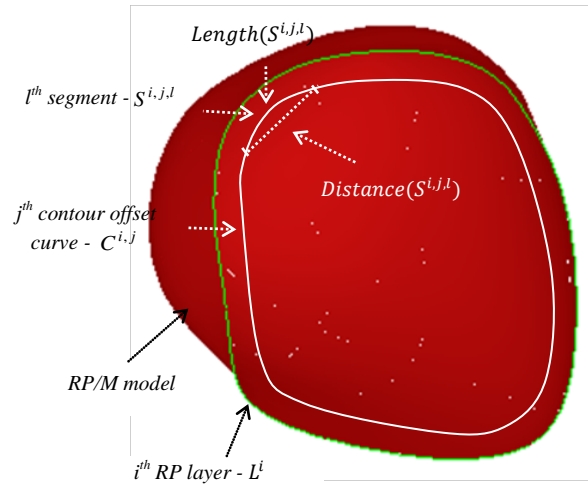
The speed of the RP/M's nozzle/print head along a contour-based tool-path can be defined below.

$$V^{i,j,l} = \frac{Distance(S^{i,j,l})}{Length(S^{i,j,l})} \cdot V_{max} \quad (4)$$

where  $V^{i,j,l}$  represents the speed of the RP/M's nozzle/print head on the segment  $S^{i,j,l}$ ;  $Length(S^{i,j,l})$  represents the curve length of the segment;  $Distance(S^{i,j,l})$  represents the straight line length from the start point to the end point of the segment;  $V_{max}$  stands for the maximum speed of a specific RP/M machine.

The build time spent on the segment  $S^{i,j,l}$  is then computed as the following.

$$Time(S^{i,j,l}) = \frac{Length(S^{i,j,l})}{V^{i,j,l}} = \frac{(Length(S^{i,j,l}))^2}{Distance(S^{i,j,l})} \cdot \frac{1}{V} \quad (5)$$



**Figure 11** Illustration of the concepts of adaptive speed strategy based on the contour curve.

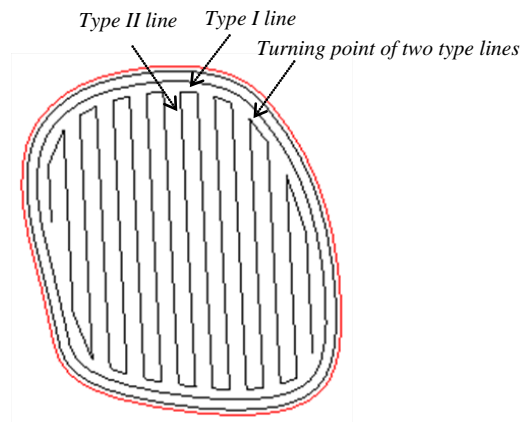
In the end, the total build time of RP/M for contour and offset tool-paths based on the boundary of the  $i^{th}$  layer of RP/M is calculated below:

$$Time(L^i) = \sum_{j=1}^n Time(C^{i,j}) \quad (6)$$

where  $Time$  represents build time;  $L^i$  represents the  $i^{th}$  sliced layer;  $C^{i,j}$  represents the  $j^{th}$  contour or offset curve on the  $i^{th}$  layer (a set of tool-paths will be generated along each curve);  $n$  is the total number of the contour and offset curves on the  $i^{th}$  layer.

### 3.3 Phase 2.2 – zigzag-based tool-path generation and adaptive algorithm for the zigzag tool-paths

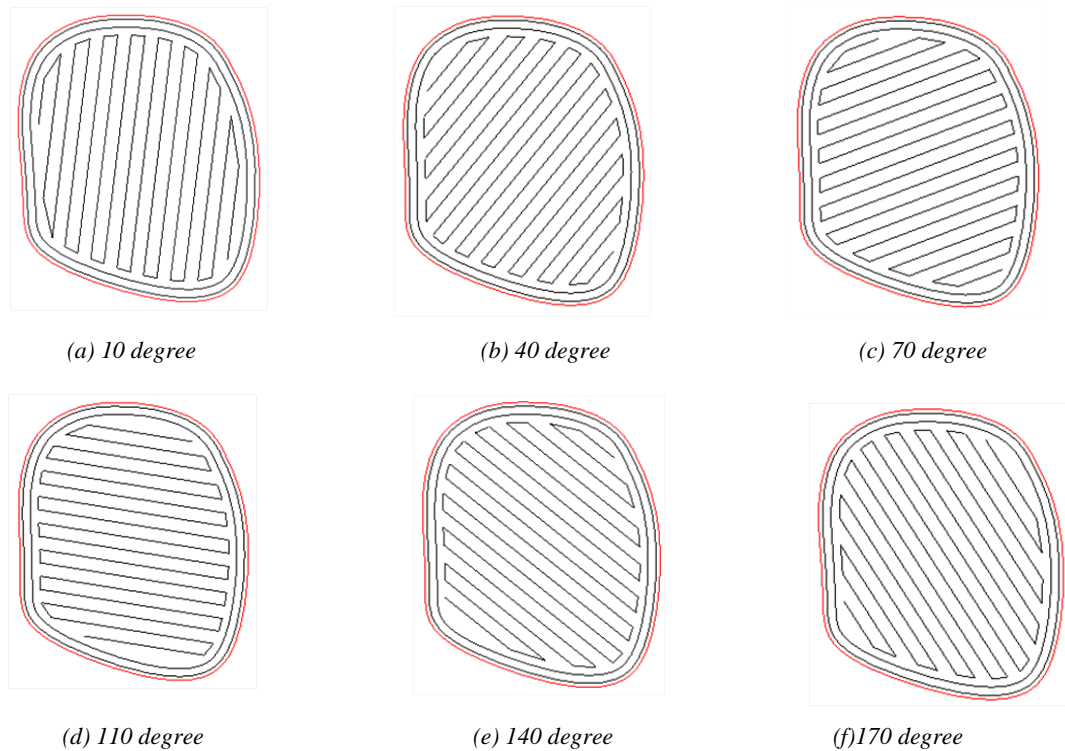
When the contour or offset curves and related tool-paths have been generated, zigzag lines and tool-paths will be then planned for the internal region of the model. The slope of the zigzag lines are chosen randomly and the overlapping rate between two neighbor zigzag lines can be decided by users (e.g., 50% step-over). In zigzag, there are two types of lines: a *Type I* zigzag line forms the main tool-paths, and a *Type II* zigzag is the connection line between two neighboring *Type I* lines. An example of the two type lines are shown in Figure 12.



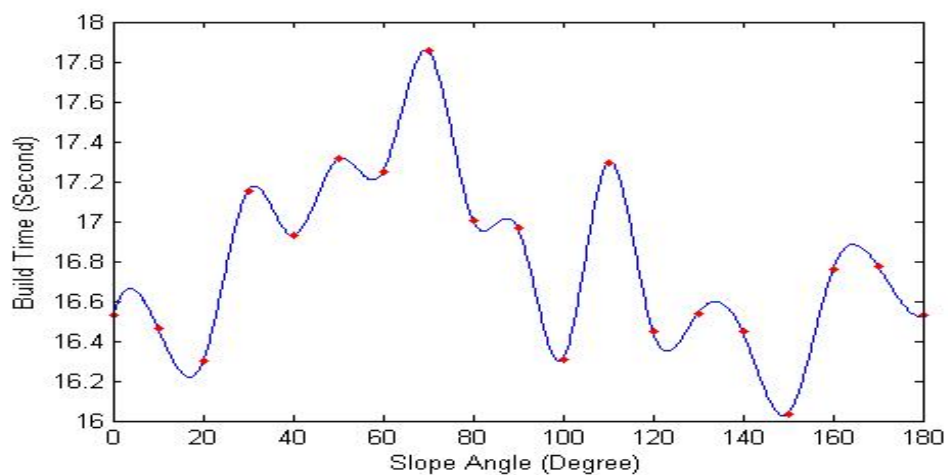
**Figure 12** Two type lines in zigzag tool-paths.

An adaptive algorithm was developed for the zigzag tool-path generation. In the adaptive algorithm, there are two strategies.

The first strategy is to obtain the most suitable slope of the zigzag direction for minimum length of tool-paths. In order to do obtain it, the direction of tool-paths can be rotated in a scope of  $[0^\circ, 180^\circ]$ . In the example of Figure 13, the slope degree can be incrementally changed, and the minimum length of tool-paths can be obtained from the interpolation curve of the results with the incremental changes. A Spline function was used for the interpolation curve. Figure 14 shows the interpolation curve built based on results of different slope degrees. From the curve, it can be obtained that at 148.3 degree the total length of the tool-paths will be minimum.



**Figure 13** Incremental degrees of slopes for the minimum build time computing.



**Figure 14** The Spline interpolation curve for the best slope degree of zigzag tool-paths.

The second strategy is to control and manage the velocity of the RP/M's nozzles/print head along zigzag tool-paths adaptively. That is, for a *Type I* or *Type II* line, the nozzle/print head starts from a minimum speed, accelerates afterwards towards a maximum speed, and then decelerates to the minimum speed at the end of the entire line. The design is aimed to improve the efficiency of the RP/M process by accelerating or decelerating the nozzle/print head according to the geometrical characteristics. As thus, the following assumptions are made:

- The speed of the nozzle/print head from all the turning points of the two type lines is the minimum speed (represented as  $V_{min}$ );
- The maximum speed that the nozzle/print head can achieve is  $V_{max}$ . The values of  $V_{max}$  and  $V_{min}$  will be set according to the specification of a RP/M machine. Here an assumption is made to make  $V_{max}$  twice of  $V_{min}$ ;
- The speed of the nozzle/print head in the zigzag tool-paths is either uniformly accelerated or deceleration with an acceleration as  $\beta$ .

Based on that, the adaptive strategy can be further represented as follows.

$$V_{max} = 2V_{min} \quad (7)$$

$$V_{max} = V_{min} + \beta t \quad (8)$$

where  $t$  is the time used to speed up the nozzle/print head from the minimum speed to the maximum speed, and  $\beta$  is the acceleration.

From Formulas (12) and (13),  $t$  can be deduced as:

$$t = \frac{V_{min}}{\beta} \quad (9)$$

On the other hand,

$$Length = \frac{1}{2}\beta t^2 + V_{min}t \quad (10)$$

The following will be obtained if Formulas (14) and (15) are combined:

$$Length = \frac{3V_{min}^2}{2\beta} \quad (11)$$

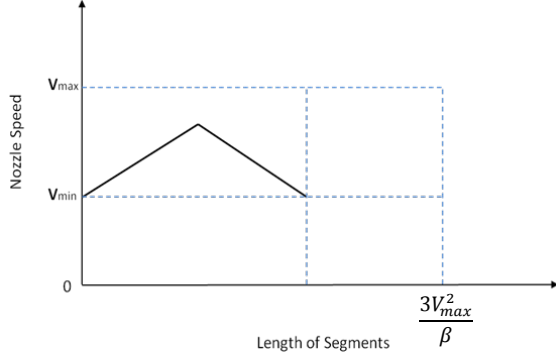
Based on the above analysis, there are three cases for the RP/M's nozzle/print head to move on a segment:

- If the length of the segment is less than  $\frac{3V_{min}^2}{\beta}$ , the nozzle/print head's speed could not reach the maximum speed  $V_{max}$  (shown in Figure 15(a));
- If the length of the segment is equals to  $\frac{3V_{min}^2}{\beta}$ , the nozzle/print head's speed just reach the maximum speed  $V_{max}$  in the middle of the segment (shown in Figure 15(b));
- If the length of the segment is less than  $\frac{3V_{min}^2}{\beta}$ , the nozzle/print head's speed reach the maximum speed  $V_{max}$  before the middle of the segment (shown in Figure 15(c)).

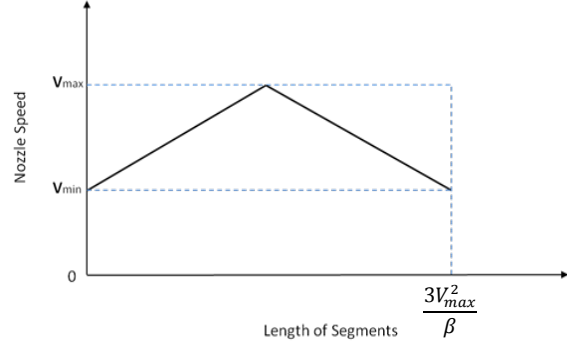
To summarize the above formulas, the time of a *Type I* or *Type II* line of zigzag will be computed as follows:

$$Time(L_i^{i,k}) = \begin{cases} \frac{2V_{min}}{\beta} & \text{if } Length(L_i^{i,k}) = \frac{3V_{min}^2}{\beta} \\ \frac{-2V_{min}}{\beta} + \sqrt{\left(\frac{2V_{min}}{\beta}\right)^2 + \frac{4Length(L_i^{i,k})}{\beta}} & \text{if } 0 < Length(L_i^{i,k}) < \frac{3V_{min}^2}{\beta} \\ \frac{2V_{min}}{\beta} + \frac{\beta * Length(L_i^{i,k}) - 3V_{min}^2}{2\beta * V_{min}} & \text{if } \frac{3V_{min}^2}{\beta} < Length(L_i^{i,k}) \end{cases} \quad (12)$$

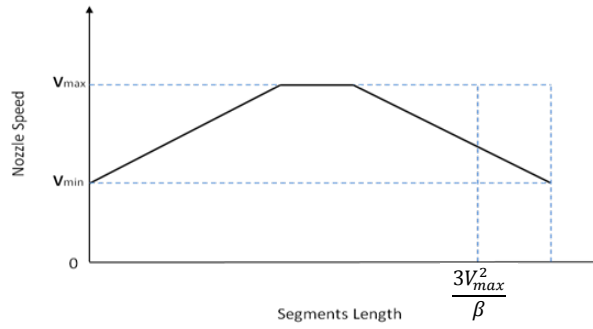
$$Time(L_{II}^{j,k}) = \begin{cases} \frac{2V_{min}}{\beta} & \text{if } Length(L_{II}^{j,k}) = \frac{3V_{min}^2}{\beta} \\ \frac{-2V_{min}}{\beta} + \sqrt{\left(\frac{2V_{min}}{\beta}\right)^2 + \frac{4Length(L_{II}^{j,k})}{\beta}} & \text{if } 0 < Length(L_{II}^{j,k}) < \frac{3V_{min}^2}{\beta} \\ \frac{2V_{min}}{\beta} + \frac{\beta * Length(L_{II}^{j,k}) - 3V_{min}^2}{2\beta * V_{min}} & \text{if } \frac{3V_{min}^2}{\beta} < Length(L_{II}^{j,k}) \end{cases} \quad (13)$$



(a) The length of a segment is less than  $\frac{3V_{min}^2}{\beta}$



(b) The length of a segment equals  $\frac{3V_{min}^2}{\beta}$



(c) The length of a segment is more than  $\frac{3V_{min}^2}{\beta}$

**Figure 15** Three cases of a segment and the speed of the RP/M's nozzle/print head.

### 3.4 Geometrical accuracy analysis model

The tolerance distribution of RP/M can be defined as three scenarios: (1) negative, (2) positive, (3) a combination of both (showed in Figure 16). In this research, the negative tolerance distribution is used for geometrical accuracy analysis of RP/M models.

The geometrical accuracy of a RP/M model can be calculated below:

$$Accuracy(R) = (G_{model} - G_{error}) / G_{model} * 100\% \quad (14)$$

where  $Accuracy(R)$  represents the geometrical accuracy;  $G_{model}$  is the whole volume of the model;  $G_{error}$  is the whole volume error of the RP/M model.

$G_{error}$  can be computed below:

$$G_{error} = \sum_{i=1}^n G_{error}^i \quad (15)$$

where  $i \in [1, n]$  is the index of a sliced layer;  $n$  is the total number of the layers;  $G_{error}^i$  is the geometrical error on the  $i^{th}$  layer of the model.

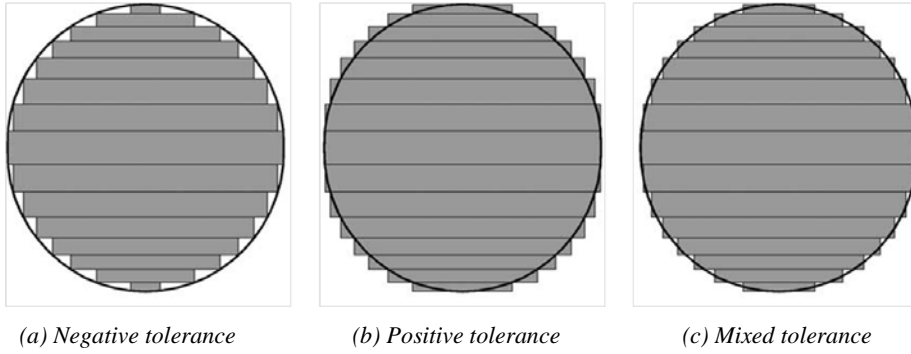
$G_{error}^i$  is from a type I error  $G_{error\_type1}^i$  and a type II error  $G_{error\_type2}^i$  (showed in Figure 17). The two errors are defined as follows:

- A type I error  $G_{error\_type1}^i$  is accumulated between consecutive layers, and it is the principle error of RP/M. It is affected by the thickness of the layer: the thicker of the layer, the greater of the type I error.
- A type II error  $G_{error\_type2}^i$  is accumulated along the boundary of every layer. It is in the boundary area which is not filled during the RP/M process.

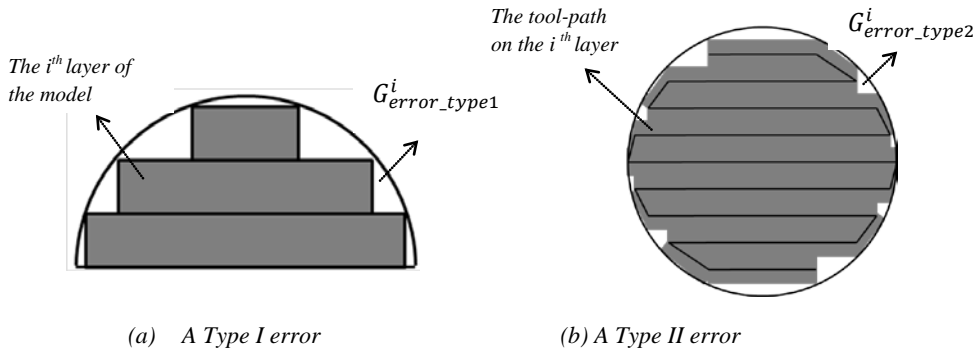
$G_{error}^i$  is computed below:

$$G_{error}^i = f(G_{error\_type1}^i, G_{error\_type2}^i) = V_{model}^i - S_{RP/M}^i * H_{thickness}^i \quad (16)$$

where  $V_{model}^i$  is the volume of the  $i^{th}$  layer;  $S_{RP/M}^i$  is the area covered by the tool-paths of RP/M on the  $i^{th}$  layer;  $H_{thickness}^i$  is the thickness of the  $i^{th}$  layer.



**Figure 16** Different tolerance distribution methods of RP/M [15].



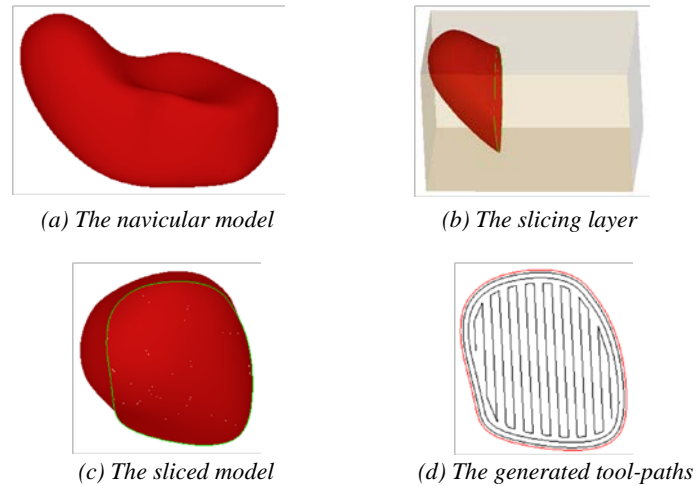
**Figure 17** Geometrical errors calculation of RP/M.

#### 4. Case Studies and Algorithm Validation

Five complex biomedical models, which were first created by CT scanning to obtain the cloud data and then reconstructed as IGES/IGS format models in CATIA V5™ with QSR and DSE modules, were tested to validate the effectiveness and robustness of the developed algorithms and strategies. The minimum and maximum speeds of the RP/M nozzle/print head were defined as 10mm/s and 20mm/s respectively, and the acceleration of the nozzle/print head was 20mm/s<sup>2</sup> ( $V_{min} = 10\text{mm/s}$ ;  $V_{max} = 20\text{mm/s}$ ;  $\beta = 20\text{mm/s}^2$ ). All results were obtained in a Pentium Dual-Core CPU 2.10GHz, 2GB RAM system.

##### Case study 1 – a navicular model

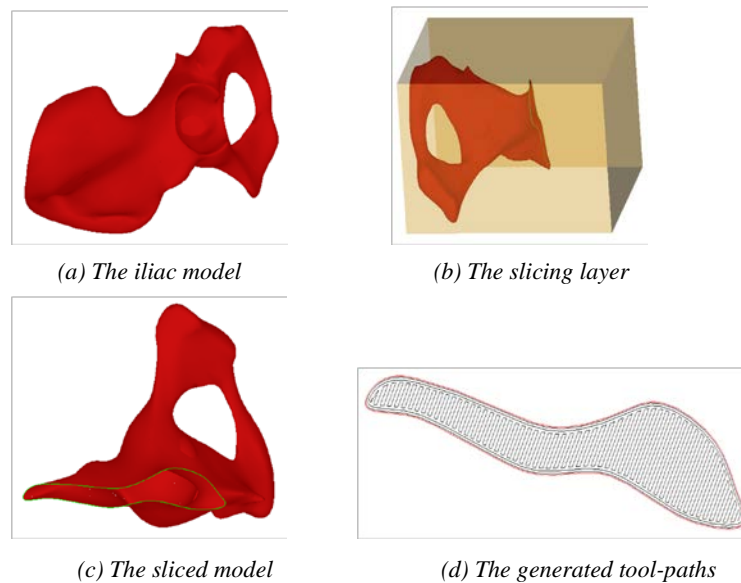
The first model is a navicular model, which was used to validate this research. The length, width, height and volume of the navicular model are 43.827mm, 28.366mm, 27.261mm and 9938mm<sup>3</sup> respectively. The process for the NURBS-based contour curve generation, and the generation of contour-based tool-paths and zigzag tool-paths are shown in Figure 18. The total build time for the shown layer of the tibia model = 3.338+16.035 = 19.373 seconds (contour tool-paths + zigzag tool-paths).



**Figure 18** Model 1 – a navicular model.

Case study 2 – an iliac model

The second model is an iliac model. The main slicing and tool-path generation is shown in Figure 19. The length, width, height and volume of the iliac model are 207.24mm, 153.47mm, 128.26mm and 282260mm<sup>3</sup> respectively. The total build time for the shown layer of the iliac model = 13.379+39.567 = 52.946 seconds.

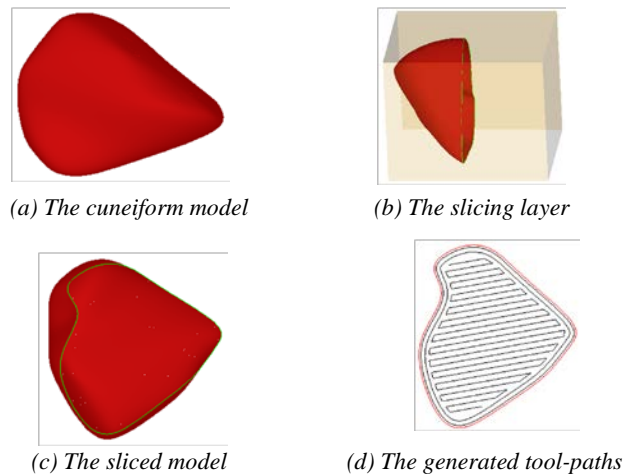


**Figure 19** Model 2 - an iliac model.

Case study 3 – a cuneiform model

The third biomedical model is a cuneiform model. The length, width, height and volume of the cuneiform model are 29.620mm, 24.544mm, 23.607mm and 5897mm<sup>3</sup> respectively. Figure 20 shows the process and geometrical results with the developed approach. The total build time for the shown layer of the talus model = 3.752+22.670 = 26.422 seconds.

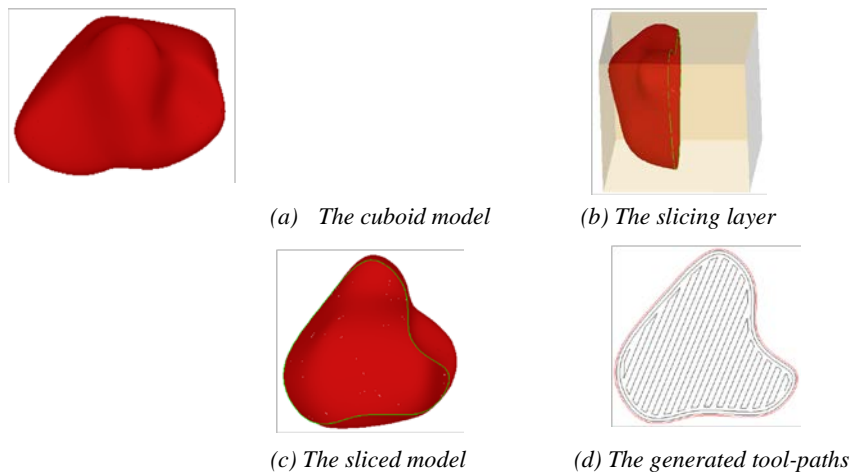




**Figure 20** Model 3 - a cuneiform model.

Case study 4 – a cuboid model

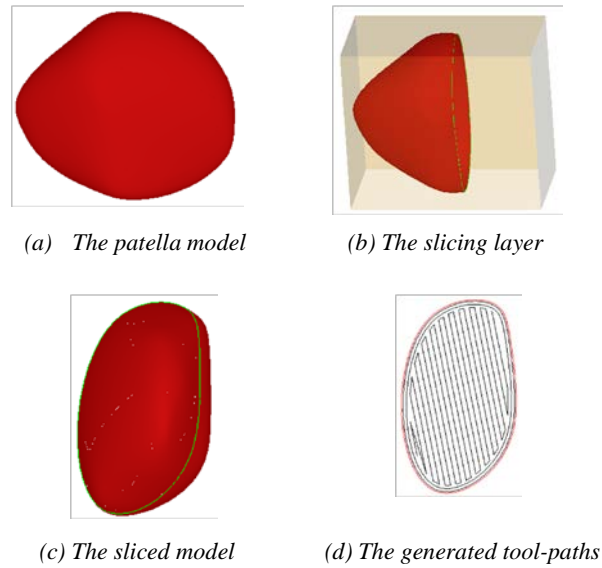
The fourth model is a cuboid model. The length, width, height and volume of the human ear model are 31.823mm, 31.380mm, 31.235mm, and 10380mm<sup>3</sup> respectively. The main slicing process and the generation of mixed tool-paths are shown in Figure 21. The total build time for the shown layer of the ear model = 5.168+32.110 = 37.278 seconds.



**Figure 21** Model 4 - a cuboid model.

Case study 5 – a patella model

The fifth model is a patella model. The length, width, height and volume are 44.963mm, 39.006mm, 23.972mm and 16108mm<sup>3</sup> respectively. Figure 22 shows the main slicing process and tool-path generation process for this model. The total build time for the shown layer of the patella model = 5.222 +32.621 = 37.843 seconds.



**Figure 22** Model 5 - a patella model.

## 5. Comparisons and Analysis

### 5.1 Build efficiency comparisons

The five biomedical models (shown in Figure 18-19, 21, 23 and 25) were also used for build efficiency comparisons. Table 2 shows the comparison results between this developed approach and typical zigzag tool-path generation approach in a uniform speed. All results were obtained in a Pentium Dual-Core CPU 2.10GHz, 2GB RAM system.

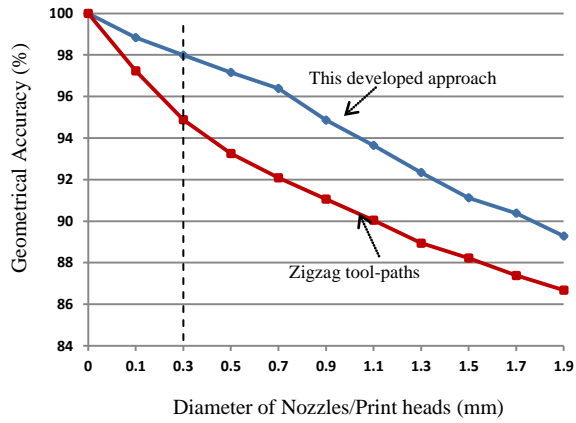
**Table 2** Build time comparisons between this approach with zigzag tool-paths in uniform and adaptive speeds.

Build time Models	This approach (s)	Zigzag in uniform speed (s)	Reduced build time (%)
1	19.373	25.767	33.005
2	52.946	68.567	29.504
3	26.422	33.476	26.697
4	37.278	46.751	25.412
5	37.843	50.365	33.089

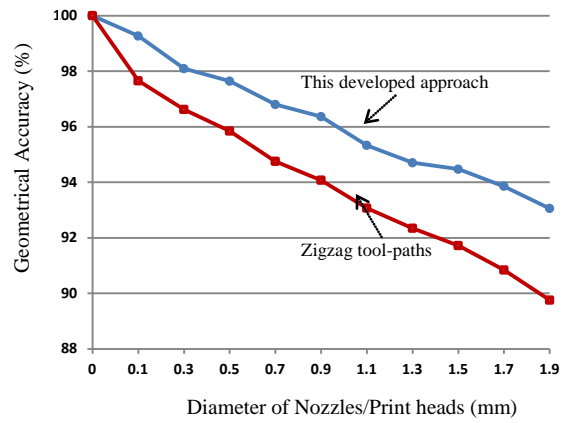
From the above data, it can be observed that the build time of this developed approach can be reduced about 30% compared to that of the zigzag tool-path generation approach in uniform speed. Also, the geometrical accuracy of this developed hybrid and adaptive tool-paths algorithm will be better than that of the zigzag tool-path generation approaches. The geometrical accuracy comparisons are explained below.

### 5.2 Geometrical accuracy comparisons

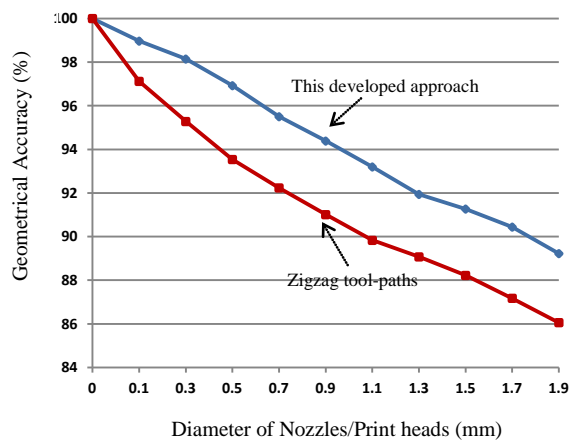
Figure 23 shows the comparisons of geometrical accuracy between this developed approach and typical zigzag tool-path generation approaches. The series of comparisons are based on an incremental 0.1mm of the diameter of RP/M nozzle/print head each time from 0mm until 1.9mm. All results were obtained in a Pentium Dual-Core CPU 2.10GHz, 2GB RAM system.



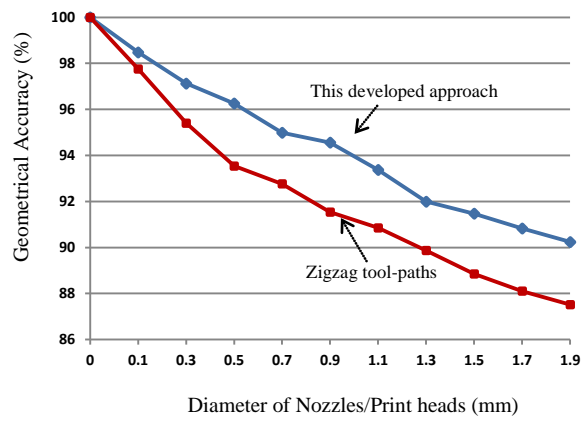
(a) Model 1



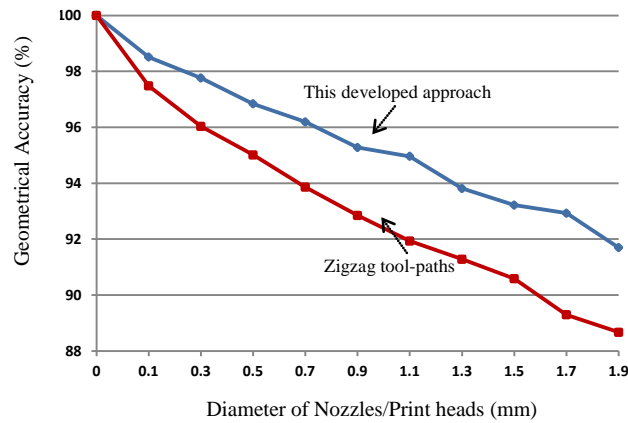
(b) Model 2



(c) Model 3



(d) Model 4



(e) Model 5

**Figure 23** Geometrical accuracy comparisons.

Compared with the typical zigzag tool-path generation approach, the developed adaptive tool-path generation approach can achieve much better geometrical accuracy of RP/M. For instance, for the model one, the geometrical accuracy is 97.986% by this developed approach with the diameter of RP/M's nozzle/print head set as 0.3 mm, while the geometrical accuracy is only 94.884% of the typical zigzag tool-path generation approaches. With the increased diameter of the nozzle/print head, the difference gap between the two approaches is further increased. Therefore, this approach can achieve an overall improvement and a better balance of build efficiency and geometrical accuracy.

## 6. Conclusions

In this paper, adaptive tool-path generation algorithms and strategies have been presented to improve geometrical accuracy and to reduce build time for biomedical model fabrication in RP/M. A series of tool-path generation optimization strategies in RP/M process planning were developed, including a slicing algorithm and NURBS-based representation, the hybrid contour and zigzag tool-path generation, adaptive speed control strategies, and the build time and geometrical accuracy analysis modules for the RP/M systems. In a summary, the features and contributions of the research are as follows:

- In order to maintain the geometrical accuracy of original biomedical models during the RP/M process, a NURBS to represent-based slicing algorithm was designed. This algorithm can enable to establish a good original data source and ensure high information fidelity for further RP/M tool-path generation;
- Another challenging issue in RP/M is how to achieve a good balance between build efficiency and geometrical quality of models. The developed hybrid tool-path generation algorithms can effectively trade off the two objectives for an overall optimization. In meantime, the speed algorithms of contour and zigzag tool-paths for RP/M's nozzle/print head can be used to further minimize build time and adaptive to various biomedical models according to their geometrical characteristics;
- In RP/M, it is essential to evaluate the build time and geometrical accuracy of a built model. In order to do so, mathematical models to analyze the build time and the geometrical accuracy of models with different parameters were designed. With the models, an effective guideline for parameter setting in a RP/M system can be introduced for algorithm evaluation and optimization, in a bid to reduce build time and improve geometrical accuracy;
- Five biomedical models with different complex shapes and geometries were used to verify and demonstrate that the developed approach has achieved significantly improved performance in terms of algorithm effectiveness, robustness and generality. The research provides a promising solution to be applicable to practical cases in biomedical industries.

Research is being undertaken in adaptive thickness adjustment to further improve the build efficiency and geometrical accuracy of complex biomedical models in the RP/M processes. Relevant research is expected to be reported in future.

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