



UNIVERSITI PUTRA MALAYSIA

***IMPROVEMENT OF THORACIC HYBRID PET/CT REGISTRATION USING
HYBRID FEATURE WITH COMBINED INTENSITY MULTIMODAL
DEMON WITH PET SINOGRAM FILTERING***

SITI SALASIAH BINTI MOKRI

FK 2016 59



**IMPROVEMENT OF THORACIC HYBRID PET/CT REGISTRATION USING
HYBRID FEATURE WITH COMBINED INTENSITY MULTIMODAL
DEMON WITH PET SINOGRAM FILTERING**

By

SITI SALASIAH BINTI MOKRI

**Thesis Submitted to the School of Graduate Studies, Universiti Putra Malaysia, in
Fulfilment of the Requirements for the Degree of Doctor of Philosophy**

May 2016



© COPYRIGHT UPM

COPYRIGHT

All material contained within the thesis, including without limitation text, logos, icons, photographs and all other artwork, is copyright material of Universiti Putra Malaysia unless otherwise stated. Use may be made of any material contained within the thesis for non-commercial purposes from the copyright holder. Commercial use of material may only be made with the express, prior, written permission of Universiti Putra Malaysia.

Copyright © Universiti Putra Malaysia



DEDICATIONS

To my beloved parents, my family members and especially to my children,

Aliff Mustaqim, Ariff Muhaymin and Aqiff Muhammad.



Abstract of thesis presented to the Senate of Universiti Putra Malaysia in fulfilment of the requirement for the degree of Doctor of Philosophy

**IMPROVEMENT OF THORACIC HYBRID PET/CT REGISTRATION USING
HYBRID FEATURE WITH COMBINED INTENSITY MULTIMODAL DEMON
WITH PET SINOGRAM FILTERING**

By

SITI SALASIAH BINTI MOKRI

May 2016

Chair: Prof. Dr. M. Iqbal Bin Saripan, Ph.D.

Faculty: Engineering

Accurately registered and fused PET/CT images are required for better tumor interpretation and the following tumor management in oncology and radiotherapy purposes. Although the hybrid PET/CT machine is supposedly solves the problem of misregistration between the PET/CT images, the offered solution is not optimal. The nonlinear misregistration due to physical and physiological motions stays on, declining the performance of the hybrid PET/CT machine. Therefore, the aim of this thesis is to solve the misregistration problem inflicting the PET/CT images acquired from the hybrid PET/CT scanner. Overall, the proposed registration method consists of three major steps. The first step is to perform 3D hybrid mean-median filtering based on the weighted average scheme on the PET sinogram domain. The second step is to segment selected structures of the thorax region which are the lungs, the heart and the tumor in both PET/CT images using a specific segmentation method for each structure excluding the heart in the PET image in which the segmentation is manually done. The main focus at this part is to design segmentation methods for the PET lung and the CT heart as these two subjects are rarely addressed. These segmented structures are used as “features” in the third stage where hybrid feature combined intensity multimodal demon registration is carried out to register both images. This method which is an improved version of multimodal demon registration uses a combination of mutual information (MI), sum of conditional variations (SCV) and multimodality independent neighborhood descriptive (MIND) similarity measures. The PET sinogram filter is tested on the NCAT based PET sinograms generated using ASIM PET simulator of different signal to noise ratio (SNR) and is compared with standard filter as used in analytical filtered-backprojection (FBP) reconstruction method. Aside from FBP, the improvement made by the filter on the iterative maximum likelihood expectation maximization with median root prior (MRP-MLEM) reconstruction method is also investigated. The filter significantly improves the global and local SNR of the PET image by more than 40% and more than 150% when compared to Hanning filtered FBP and MRP-MLEM reconstructed images without filtering. In terms of contrast to noise

ratio (CNR), the proposed filter constantly generates improved CNR for all datasets in both analytical and statistical reconstruction methods. In the second stage, the proposed segmentation methods are evaluated on simulated NCAT based PET/CT and 21 clinical patient datasets. Apart from satisfactory subjective evaluation through visual displays, the segmentation of two structures, CT heart and PET lung are validated against expert segmentation on 10 datasets. The achieved mean Dice and Jaccard coefficients for both structures are more than 0.8. Then, the proposed improved intensity multimodal demon registration is tested on simple images and various types of medical images and the registration results are satisfactory. Specific to PET/CT registration problem, the proposed hybrid feature intensity multimodal registration method is tested on the simulated NCAT PET/CT images acquired at different breathing phases as well 21 clinical hybrid PET/CT datasets. Experimental results show that the combination of SCV and MIND based similarity measures produces the best registration result for PET/CT misregistration problem. In particular to clinical datasets experiment, the mean NMI improvement achieved by the proposed hybrid feature combined intensity multimodal demon registration is twice than the established free form deformation (FFD) registration method. The success of the registration of the patient datasets is also validated through improved lung volume overlap between the PET lung and the CT lung post registration according to Jaccard and Dice coefficients calculations. The registration method increases the Jaccard and Dice measures by 7.78% and 4.46% in average respectively after registration.

Abstrak tesis yang dikemukakan kepada Senat Universiti Putra Malaysia sebagai memenuhi keperluan untuk ijazah Doktor Falsafah

**PENAMBAHBAIKAN REGISTRASI PET/CT PADA TORAKS
MENGUNAKAN HIBRID FITUR DENGAN KOMBINASI KEAMATAN
MULTIMODAL DEMON DENGAN PENAPISAN SINOGRAM PET**

Oleh

SITI SALASIAH BINTI MOKRI

Mei 2016

Pengerusi: Prof. Dr. M. Iqbal Bin Saripan, Ph.D.

Fakulti: Kejuruteraan

Registrasi dan jajaran imej PET/CT yang tepat adalah perlu bagi mencapai proses interpretasi dan pengurusan tumor yang baik di dalam aplikasi onkologi dan radioterapi. Walau pun mesin hibrid PET/CT dikatakan dapat menyelesaikan masalah misregistrasi PET/CT, penyelesaian yang ditawarkan oleh mesin ini adalah tidak optimum. Masalah misregistrasi tak linear yang disebabkan oleh gerakan pesakit dan fisiologi masih wujud lalu mengurangkan prestasi mesin tersebut. Oleh itu, tesis ini bertujuan untuk menyelesaikan masalah misregistrasi yang terdapat di antara imej PET/CT dari mesin hibrid PET/CT disebabkan oleh gerakan fizikal dan fisiologi. Algoritma registrasi yang dicadangkan mengandungi tiga langkah utama. Langkah pertama adalah menjalankan proses penapisan menggunakan penapis purata-median 3D berasaskan purata pemberat terhadap data sinogram PET. Langkah kedua ialah melakukan segmentasi struktur-struktur yang terpilih di bahagian toraks (paru-paru, jantung dan tumor) pada kedua-dua imej. Oleh itu, tesis ini mencadangkan algoritma segmentasi khusus bagi setiap struktur kecuali jantung yang terdapat pada imej PET di mana proses segmentasi dijalankan secara manual. Fokus utama diberikan kepada segmentasi paru-paru PET dan jantung CT kerana kedua-dua subjek kurang diberi perhatian di dalam literasi penyelidikan. Segmentasi struktur-struktur yang diperolehi dijadikan sebagai ciri yang akan digunakan di dalam kaedah registrasi hibrid ciri-keamatan pelbagai modaliti demon pada langkah seterusnya. Kaedah ini merupakan versi tambah-baik registrasi pelbagai modaliti demon yang menggunakan gabungan metrik kesamaan *mutual information* (MI), *sum of conditional variations* (SCV) dan *multimodality independent neighborhood descriptor* (MIND). Penapis sinogram PET diuji ke atas sinogram PET NCAT tersimulasi dengan SNR yang berbeza yang dijana menggunakan simulator ASIM PET dan dibandingkan dengan kaedah rekonstruksi imej FBP. Selain FBP, sebarang penambahbaikan ke atas kaedah rekonstruksi imej menggunakan kaedah rekonstruksi *maximum likelihood expectation maximization with median root prior* (MRP-MLEM) turut dikaji. Penapis yang digunakan menambahbaik

SNR global dan lokal imej PET masing-masing sebanyak 40% dan 150% apabila dibandingkan dengan FBP berasaskan Hanning dan MRP-MLEM tanpa penapisan sinogram. Penapis yang dicadangkan juga menambahbaik CNR pada imej untuk setiap data yang digunakan pada kedua-dua kaedah rekonstruksi analitikal dan statistik. Pada tahap yang kedua, kaedah segmentasi yang dicadangkan diuji pada imej PET/CT simulasi NCAT dan 21 data pesakit. Selain daripada penilaian subjektif yang memuaskan melalui visual, segmentasi kedua-dua struktur, paru-paru PET dan jantung CT dibandingkan dengan segmentasi oleh pakar ke atas 10 data. Bacaan purata Dice dan Jaccard untuk kedua-dua struktur adalah melebihi 0.8. Kaedah registrasi tambah baik berasaskan keamatan pelbagai modaliti demon yang dicadangkan diuji ke atas imej mudah dan pelbagai jenis imej perubatan dan keputusan registrasi adalah memuaskan. Untuk masalah misregistrasi PET/CT, kaedah registrasi hibrid ciri-keamatan pelbagai modaliti demon dilaksanakan ke atas imej PET/CT simulasi NCAT yang diambil pada fasa pernafasan yang berbeza dan juga terhadap 21 imej pesakit. Keputusan eksperimen menunjukkan gabungan metrik kesamaan SCV dan MIND menghasilkan keputusan registrasi yang terbaik. Khususnya, keputusan eksperimen ke atas data pesakit menunjukkan bahawa kaedah registrasi yang dicadangkan menghasilkan penambahbaikan peratusan NMI sebanyak dua kali ganda berbanding nilai yang diperolehi dengan menggunakan kaedah registrasi "free form deformation" (FFD). Kejayaan proses registrasi juga disahkan melalui ukuran tindihan isipadu paru-paru CT dan PET sebelum dan selepas registrasi berdasarkan pengiraan Jaccard dan Dice. Kaedah registrasi yang dicadangkan menambahbaik ukuran Jaccard dan Dice masing-masing sebanyak 7.78% dan 4.46% secara purata selepas proses registrasi.

ACKNOWLEDGEMENTS

Alhamdulillah. All thanks and prayers to the Almighty Allah for His endless blessing and granting me patience to accomplish this thesis.

First of all, I would like to take this opportunity to express my sincere appreciation to my supervisor, Prof. Dr. M. Iqbal Saripan for his support, outstanding supervision, encouragement and examples. His unfailing guidance enables me to complete this thesis at the end.

My deepest appreciation and gratitude also goes to Prof. Dr. Abdul Jalil Nordin, the Dean of UPM Faculty of Medicine and Health Science (the former Director of UPM Nuclear Imaging Diagnostic Center (PPDN-UPM)) cum my co-supervisor for his endless contributions, co-operation and guidance in facilitating the research work. Great appreciation is also expressed to my second co-supervisor, Prof. Dr. Mohammad Hamiruce bin Marhaban for his valuable remarks and advices.

I would like to acknowledge the efforts made by Dr. Noraini Sarina binti Abdullah (PPDN-UPM) who provides the expert segmentation of thoracic structures that are used as part of the research work. I am extremely grateful to her over the time spent to finish this task. Also goes to Dr. Fathinul Fikri bin Saad (the Director of PPDN-UPM) who always provides the resources and inputs concerning the medical aspects related to the research.

Many thanks to Ministry of Education Malaysia and my employer Universiti Kebangsaan Malaysia for their generous and significant financial contributions which allow me to focus on my studies and my research. I also would like to express my appreciation to my internal and external examiners for examining my thesis and also to the academic and non-academic staff members of Faculty of Engineering, UPM for providing the facilities and convenient space for me to work on my research.

Last but not least, to my beloved parents, my siblings, my family, my children and my dear friends who support me throughout my phd journey. Thank you for the support, patience, trust and belief in my undertakings.

I certify that a Thesis Examination Committee has met on 12 May 2016 to conduct the final examination of Siti Salasiah Mokri on her thesis entitled “Improvement of Thoracic Hybrid PET/CT Registration Using Hybrid Feature with Combined Intensity Multimodal Demon with PET Sinogram Filtering” in accordance with the Universities and University Colleges Act 1971 and the Constitution of the Universiti Putra Malaysia [P.U.(A) 106] 15 March 1998. The Committee recommends that the student be awarded the Doctor of Philosophy.

Members of the Thesis Examination Committee were as follows:

Y.M. Raja Syamsul Azmir bin Raja Abdullah, PhD

Associate Professor
Faculty of Engineering
Universiti Putra Malaysia
(Chairman)

Abd. Rahman bin Ramli, PhD

Associate Professor
Faculty of Engineering
Universiti Putra Malaysia
(Internal Examiner)

Fakhrul Zaman bin Rokhani, PhD

Senior Lecturer
Faculty of Engineering
Universiti Putra Malaysia
(Internal Examiner)

Troy Farncombe, PhD

Associate Professor
McMaster University
Canada
(External Examiner)

ZULKARNAIN ZAINAL Ph.D.

Professor and Deputy Dean
School of Graduate Studies
Universiti Putra Malaysia

Date: 23 August 2016

This thesis was submitted to the Senate of Universiti Putra Malaysia and has been accepted as fulfilment of the requirement for the degree of Doctor of Philosophy. The members of the Supervisory Committee were as follows:

M. Iqbal Saripan, Ph.D.

Professor
Faculty of Engineering
Universiti Putra Malaysia
(Chairman)

Abdul Jalil bin Nordin, M.D.

Professor
Faculty of Medicine and Health Science
Universiti Putra Malaysia
(Member)

Mohammad Hamiruce Marhaban, Ph.D.

Professor
Faculty of Engineering
Universiti Putra Malaysia
(Member)

BUJANG KIM HUAT, Ph.D.

Professor and Dean
School of Graduate Studies
Universiti Putra Malaysia

Date:

Declaration by graduate student

I hereby confirm that:

- this thesis is my original work;
- quotations, illustrations and citations have been duly referenced;
- this thesis has not been submitted previously or concurrently for any other degree at any other institutions;
- intellectual property from the thesis and copyright of thesis are fully-owned by Universiti Putra Malaysia, as according to the Universiti Putra Malaysia (Research) Rules 2012;
- written permission must be obtained from supervisor and the office of Deputy Vice-Chancellor (Research and Innovation) before thesis is published (in the form of written, printed or in electronic form) including books, journals, modules, proceedings, popular writings, seminar papers, manuscripts, posters, reports, lecture notes, learning modules or any other materials as stated in the Universiti Putra Malaysia (Research) Rules 2012;
- there is no plagiarism or data falsification/fabrication in the thesis, and scholarly integrity is upheld as according to the Universiti Putra Malaysia (Graduate Studies) Rules 2003 (Revision 2012-2013) and the Universiti Putra Malaysia (Research) Rules 2012. The thesis has undergone plagiarism detection software.

Signature: _____ Date: _____

Name and Matric No.: SITI SALASIAH MOKRI (GS30921)

Declaration by Members of Supervisory Committee

This is to confirm that:

- the research conducted and the writing of this thesis was under our supervision;
- supervision responsibilities as stated in the Universiti Putra Malaysia (Graduate Studies) Rules 2003 (Revision 2012-2013) are adhered to.

Signature: _____
Name of Chairman of
Supervisory
Committee: _____

Signature: _____
Name of Member of
Supervisory
Committee: _____

Signature: _____
Name of Member of
Supervisory
Committee: _____

TABLE OF CONTENTS

	Page
ABSTRACT	i
ABSTRAK	iii
ACKNOWLEDGEMENTS	v
APPROVAL	vi
DECLARATION	viii
LIST OF TABLES	xiii
LIST OF FIGURES	xv
LIST OF ABBREVIATIONS	xxii
CHAPTER	
1	INTRODUCTION 1
1.1	Background 1
1.2	Problem Statement 2
1.3	Aim and Objective 5
1.4	Scope and Limitations 5
1.5	Thesis Contributions 7
2	LITERATURE REVIEW 9
2.1	Introduction 9
2.2	Computed Tomography Imaging (CT) 9
2.3	Positron Emission Tomography (PET) Imaging 11
2.3.1	PET acquisition process 11
2.3.2	PET 2D and 3D Imaging 13
2.3.3	Filtered back-projection (FBP) image reconstruction algorithm 14
2.3.4	Iterative image reconstruction method 16
2.4	Hybrid PET/CT Scanner 18
2.5	Respiratory Motion Artefacts in PET/CT 19
2.6	Image Registration 21
2.6.1	Multimodal similarity measures: MI and NMI 23
2.6.2	Free form deformation (FFD) registration method 24
2.6.3	Demon registration method 25
2.7	Review of PET/CT Registration 26
2.8	Review of Filtering in Sinogram Domain 30
2.8.1	Anisotropic diffusion filter (ADF) 32
2.8.2	Nonlocal means filter (NLM) 33
2.8.3	Adaptive Modified Probability Curvature Motion PET sinogram filter (AMPCM) 34
2.9	Review of Structures Segmentation in PET/CT images 35
2.9.1	Spatial Fuzzy C Means Clustering (SFCM) 37

	2.9.2	Distance Regularized Level Set Segmentation (DRLSE)	38
	2.10	Summary	39
3		METHODOLOGY	40
	3.1	Introduction	40
	3.2	Overview of the Proposed Registration Method for PET/CT	40
	3.3	PET Sinogram Filter	42
	3.3.1	Proposed hybrid mean median sinogram filter	43
	3.4	Structures Segmentation in PET/CT	56
	3.4.1	Lung segmentation in CT	58
	3.4.2	Lung segmentation in PET	63
	3.4.3	Heart segmentation in CT	68
	3.4.4	Semiautomatic tumour segmentation in PET and CT	73
	3.5	Hybrid Feature Combined Intensity Multimodal Demon Registration for PET/CT	75
	3.5.1	Proposed multimodal demon registration	76
	3.6	Experimental Setup	81
	3.6.1	Simulation data for PET sinogram	81
	3.6.2	Validation for the proposed structures segmentation methods	83
	3.6.3	Validation of the proposed combined intensity multimodal demon method and the proposed hybrid feature intensity combined multimodal demon for PET/CT	84
	3.7	Conclusions	86
4		RESULTS AND DISCUSSIONS	88
	4.1	Introduction	88
	4.2	Results and Discussions for the Proposed Sinogram Filter	88
	4.2.1	Comparison with FBP reconstructed images filtered with NLM, ADF and AMPCM	88
	4.2.2	Comparison with FBP and MLEM-MRP reconstruction methods	89
	4.3	Results and Discussions of the Proposed Structures Segmentation Methods	98
	4.3.1	CT lung segmentation results	98
	4.3.2	PET lung segmentation results	100
	4.3.3	CT heart segmentation results	103
	4.3.4	PET/CT tumour segmentation results	106
	4.4	Results and Discussions for the Proposed Multimodal Demon Registration	111
	4.4.1	Combined intensity demon registration for 2D monomodal images	111

4.4.2	Combined intensity demon registration for 2D multimodal images	113
4.4.3	Proposed demon registration for PET/CT images	120
4.5	Conclusions	143
5	CONCLUSION	145
5.1	Conclusions	145
5.2	Suggestions for Future Research	148
	REFERENCES	149
	APPENDICES	162
	BIODATA OF STUDENT	183
	LIST OF PUBLICATIONS	184



LIST OF TABLES

Table		Page
2.1	Normal human tissue HU number	10
2.2	Normal organ FDG activity concentration	13
2.3	Previous registration methods for separate PET/CT	27
3.1	SNR of images filtered based on <i>m1</i> , <i>m2</i> and <i>m3</i>	51
3.2	DRLSE parameters for heart segmentation at S_{index}	69
3.3	Radioactive concentrations in each organ of NCAT phantom	81
3.4	Sinogram datasets with defined counts (M)	83
3.5	Clinical PET and CT image information	85
4.1	Parameters used in the proposed sinogram filter	91
4.2	NMSE and average global SNR comparison (FBP)	93
4.3	Local SNR comparison (FBP)	93
4.4	NMSE and average global SNR comparison (MRP-MLEM)	94
4.5	Local SNR comparison (MRP-MLEM)	94
4.6	Max, Min, Mean and Std of segmentation indexes for PET lung	102
4.7	Max, Min, Mean and Std of segmentation indexes for CT heart	106
4.8	Comparison using intensity multimodal demon using different/combination of similarity metric on different images	118
4.9	Comparison of intensity multimodal demon using different/combination of similarity metric on NCAT simulated images	122
4.10	Feature demon registration parameters for each structure for NCAT based PET/CT	126
4.11	Comparison between sole combined intensity multi-modal demon (CMB) and hybrid feature combined intensity multi-modal demon for simulated NCAT PET/CT images	131

4.12	Comparison between FFD and the proposed method on PX PET and CT images registration	133
4.13	Comparison between FFD and the proposed hybrid feature combined intensity multi-modal demon for clinical datasets (P1-P21) in terms of NMI achievement	138
4.14	Lung volume Jaccard coefficient before and after registration for patient datasets (P1-P21)	140
4.15	Lung volume Dice coefficient before and after registration for patient datasets (P1-P21)	141



LIST OF FIGURES

Figure	Page	
2.1	CT scanning process	10
2.2	Photons radiation by the PET isotope	11
2.3	A coincidence event detection (Left) and the sinogram (Right)	12
2.4	Parallel projections at an angle θ	12
2.5	PET imaging (Left) 2D and (Right) 3D	14
2.6	Illustration of central slice theorem	15
2.7	Illustration on system model, H_{ij}	16
2.8	GE Discovery LS PET/CT machine with bed positioning	18
2.9	CT, PET and fused PET/CT images	18
2.10	Respiration process	19
2.11	Misregistration in PET/CT	20
2.12	General framework of image registration technique	22
2.13	Mutual information concept	24
3.1	General workflow of the proposed hybrid feature intensity demon for PET/CT registration problem	42
3.2	Simple square image (a) Noise free FBP (b) Noisy Hanning FBP	43
3.3	FBP reconstructed images using 1D, 2D and 3D mean filters	43
3.4	Directional masks	45
3.5	Noise free (Left) and Hanning filtered FBP (Right) simulated image	47
3.6	Control parameter images (a) $m1$ (b) $m2$ (c) $m3$	49
3.7	Reconstructed images (a) Noise free image (b) sinogram filtered using $m1$ (c) sinogram filtered using $m2$ (c) sinogram filtered using $m3$	49

3.8	Zoomed images (a) Noise free image (b) sinogram filtered using m3 (c) sinogram filtered using m2 (c) sinogram filtered using m1	50
3.9	Plot of H when $T_s = 0.7$ and $A_d = 0.01$	52
3.10	(Top) Streak artefacts using Equation 3.1 filtering scheme (Bottom) Reduced streak artefacts using Equation 3.14 filtering scheme	52
3.11	Division of regions in the proposed filter	53
3.12	Illustration of 3D bow tie shaped concept	54
3.13	Two 3D bow tie shaped mask (Mask A)	55
3.14	Comparison of reconstructed images using standard mean filters and 3D bow tie shaped mask mean filter	55
3.15	Zoomed image for images in Figure 3.14	56
3.16	Flow diagram of main structures segmentation	57
3.17	Local histogram analysis to determine threshold value to separate T_0 (Top) Whole CT histogram (Bottom) Local histogram at [500,1000]	59
3.18	Two seed points in the slice before tracheal bifurcation	60
3.19	Lower airway structures segmentation	61
3.20	Generation of boundary line to separate the left and right lungs	62
3.21	Step by step process of lung segmentation in CT	62
3.22	(a) PET image (b) Masked PET image (c) Enhanced PET image	63
3.23	Pruned edges (a) Before pruning (b) After pruning	64
3.24	Procedure to extract lung boundary on the 30 th slice (a) CT lung boundary (b) PET edges (c) Extracting points on PET edges that are closest to the CT points respectively (d) Bridging two endpoints	64
3.25	An example of lung core	65
3.26	An illustration that shows uptake heterogeneity at the lungs	66
3.27	Global threshold determination (T4) (Top) Single peak local histogram (Below) Two peaks local histogram	67

3.28	Spatial fuzzy clustering results on (a) Lung core (b) Lung VOI with number of cluster $K=3$, (c) Lung VOI $K=4$, (d) Lung VOI $K=5$ (e) Lung VOI $K=6$; (f) Lung VOI $K=7$	67
3.29	Flowchart for lung segmentation in PET	68
3.30	The calculation of the heart centroid on S_{index} (a) Lung mask (b) Convex hull image of the lung mask (c) The resulted distance transform image	69
3.31	Fitting an ellipse on segmented heart at S_{index} (a) edge function image (b) gross segmented heart after DRLSE (d) fitting a 2D ellipse on the gross segmented heart	70
3.32	(Above) The axial and coronal planes that cross the centroid at S_{index} are determined. (Below) At the coronal plane (a) Lung mask (b) convex hull image (d) distance transform image	70
3.33	Determination of important slice indexes at the coronal plane	71
3.34	Generation of 3D shape for 3D gross heart segmentation	71
3.35	Derivation of edge function in the DRLSE third stage (a) Enhanced edge image (b) thresholded inversed edge image (c) as masked with bounded ellipse	72
3.36	Graphical interpretation of the parameters to construct the ideal 3D ellipse	73
3.37	Flow chart of the proposed heart segmentation algorithm in non-contrast CT	74
3.38	The proposed hybrid feature combined intensity multi-modal demon registration block diagram	79
3.39	NCAT emission (top) and attenuation (bottom) images	82
3.40	Datasets with extreme cases of lungs condition/masses	85
4.1	Reconstructed images with the simulated sinogram pre-filtered with (a) NLM (b) ADF (c) AMPCM (d) Proposed filter	90
4.2	Reconstructed images (zoomed) with the simulated sinogram pre-filtered with (a) NLM (b) ADF (c) AMPCM (d) Proposed filter	90
4.3	Images comparison using dataset S1	91
4.4	Images comparison using dataset S2	91

4.5	Images comparison using dataset S3	92
4.6	Images comparison using dataset S4	92
4.7	Region of interest (ROI) for local SNR quantification	93
4.8	Region of interest in calculating CNR	94
4.9	CNR comparison for dataset S1-S4	95
4.10	1D profiles corresponding to reconstructed (a) Hanning FBP (b) Proposed FBP (c) MRP-MLEM (d) Proposed MRP-MLEM for simple image	96
4.11	1D profiles corresponding to reconstructed (a) Hanning FBP (b) Proposed FBP (c) MRP-MLEM (d) Proposed MRP-MLEM for NCAT PET image	97
4.12	Segmented CT lungs in NCAT based image	98
4.13	Sequential slices of segmented lungs of a patient dataset	99
4.14	Segmented CT lung in Patient 3	99
4.15	Line separating the left and the right lungs as generated by the algorithm for four diferent patient datasets	100
4.16	Segmented PET lung in NCAT based PET image	101
4.17	Segmented PET lungs for Patient 12	101
4.18	Segmentation similarity indexes for PET lung	102
4.19	Segmented CT heart in NCAT based CT image	104
4.20	Segmented CT heart for Patient 1	104
4.21	Segmentation similarity indexes for CT heart	105
4.22	Segmented tumour in PET and CT images for Patient 11	107
4.23	Segmented tumour in PET and CT images for Patient 21	108
4.24	Segmented tumour in PET and CT images for Patient 13	109
4.25	Segmented tumour in PET and CT images for Patient 12	110
4.26	Registration results for mono-modal (Image 1)	111

4.27	Registration results for mono-modal (Image 2)	112
4.28	Registration results for mono-modal (Image 3)	112
4.29	Registration results for mono-modal (Image 4)	112
4.30	Registration results for multi-modal (Image 1)	113
4.31	Registration results for multi-modal (Image 3)	114
4.32	Registration results for multi-modal (Image 4)	115
4.33	Registration results for multi-modal (Image 5)	116
4.34	Registration results for multi-modal (Image 6)	116
4.35	Registration results for multi-modal (Image 7)	117
4.36	Registration results for multi-modal (Image 8)	117
4.37	Registration results for multi-modal Image 9 (MRI prostate) with combined intensity multi-modal demon registration	119
4.38	Demon registration of the segmented structure based on distance transform images (Top) and the registered images after the structure deformation (Bottom)	119
4.39	Improved registration results for multi-modal Patient 9 (prostate MRI) after structure registration followed with combined intensity multi-modal demon registration	120
4.40	Registration results between simulated NCAT PET-SNR16/CT with combined intensity multi-modal demon	123
4.41	Registration results between simulated NCAT PET-SNR13/CT with combined intensity multi-modal demon	124
4.42	Registration results between simulated NCAT PET-SNR6/CT with combined intensity multi-modal demon	125
4.43	Structures registration results using distance transform based feature demon registration	126
4.44	Registration results between simulated NCAT PET-SNR16/CT using hybrid feature combined intensity multi-modal demon	128
4.45	Registration results between simulated NCAT PET-SNR13/CT using hybrid feature intensity demon	129

4.46	Registration results between simulated NCAT PET-SNR6/CT using hybrid feature combined intensity multi-modal demon	130
4.47	Coloured fused registered PX PET/CT images	132
4.48	Registration results on PX PET/CT images using hybrid feature combined intensity multi-modal demon registration	132
4.49	Registration results for P11	135
4.50	Registration results for P7	135
4.51	Registration results for P12	136
4.52	Registration results for P5	136
4.53	Registration results for P18	137
A.1	Segmented CT Lungs for Patient 4	162
A.2	Segmented CT Lungs for Patient 9	162
A.3	Segmented CT Lungs for Patient 15	162
A.4	Segmented CT Lungs for Patient 17	163
A.5	Segmented PET Lungs for Patient 15	163
A.6	Segmented PET Lungs for Patient 16	163
A.7	Segmented PET Lungs for Patient 17	164
A.8	Segmented PET Lungs for Patient 19	164
A.9	Segmented PET Lungs for Patient 20	164
A.10	Segmented CT heart for Patient 5	165
A.11	Segmented CT heart for Patient 6	165
A.12	Segmented CT heart for Patient 7	165
A.13	Segmented CT heart for Patient 9	166
A.14	Segmented CT heart for Patient 10	166
B.1	Registration results for P8	167
B.2	Registration results for P20	168

B.3	Registration results for P21	169
B.4	Registration results for P10	170
B.5	Registration results for P14	171
B.6	Registration results for P15	172
B.7	Registration results for P16	173
B.8	Registration results for P1	174
B.9	Registration results for P2	175
B.10	Registration results for P7	176
B.11	Registration results for P13	177
B.12	Registration results for P9	178
B.13	Registration results for P3	179
B.14	Registration results for P4	180
B.15	Registration results for P6	181
B.16	Registration results for P19	182

LIST OF ABBREVIATIONS

ADF	Anisotropic diffusion filter
AMPCM	Adaptive modified probabilistic curvature motion
BM3D	Block matching 3 dimensional
CMB	Combined intensity demon
CNR	Contrast to noise ratio
CT	Computed Tomography
DCT	Discrete cosine transform
DIBH	Deep Inspiration Breath Hold
DICOM	Digital imaging in communication and medicine
DRLSE	Distance regularised level set
EPD	Edge preserved denoising
FBP	Filtered Backprojection
FDG	Fluorodeoxyglucose
FFA	Free fatty acid
FFD	Free form deformation
GUI	Graphical user interface
FOV	Field of view
HU	Hounsfield unit
ICA	Independent component analysis
LOR	Line of response
MAP	Maximum a posteriori
MI	Mutual information
MIND	Multimodality independent neighbourhood descriptor
MLEM	Maximum Likelihood Expectation Maximisation

MRP	Median Root Prior
MRI	Magnetic Resonance Imaging
NCAT	NURBS cardiac and torso phantom
NCC	Normalised cross correlation
NLM	Non local means
NMI	Normalised mutual information
NMSE	Normalised mean square error
NSCLC	Non-small cell lung cancer
NURBS	Non uniform rational b-spline
OSEM	Ordered subset expectation maximisation
PC	Phase correlation
PD	Proton density
PET	Positron Emission Tomography
PPDN-UPM	Pusat Pengimejan Diagnostik Nuklear – Universiti Putra Malaysia
RFP	Ratio false positive
RFN	Ratio false negative
ROI	Region of interest
RIU	Ratio image uniformity
SCV	Sum of conditional variance
SFCM	Spatial fuzzy C means
SNR	Signal to noise ratio
SPECT	Single Photon Emission Computed Tomography
SSD	Sum square distance
SUV	Standardised uptake value

TBD	Texture based denoising
TNM	Tumour-lymph node-metastasis
TPS	Thin plate spline
TV	Total variation
VOI	Volume of interest



CHAPTER 1

INTRODUCTION

1.1 Background

There are two types of medical imaging devices that are commonly used in oncology cancer diagnosis and radiation therapy. The first type is anatomical based devices such as Computed Tomography (CT) and Magnetic Resonance Imaging (MRI) (Alessio et al., 2004). The second type is functional based devices such as Single Photon Computed Tomography (SPECT) and Positron Emission Tomography (PET) (Alessio et al., 2004). PET image depicts the distribution of the radiotracer that is injected into the patient prior to the scanning session. With this knowledge, the radiologist and physician are able to interpret physiological processes such as metabolism and blood flow as well as to assess the acuteness of any cancerous cells. At the early stage, the PET scanner is mainly used for oncologic cancer diagnosis. However, the localisation of possible metastatic cancer based on the PET image alone could be less than accurate due to the noisy, blurry, low resolution characteristics of the image itself. Thus, the idea of integrating PET and CT images for cancer diagnosis comes into sight (Pan & Mawlawi, 2008). The CT image provides the necessary anatomical descriptions such as the size and the shape of the lesion while the PET image tells about the degree of malignancy. The integration of PET/CT images improves the accuracy of the localisation in general.

The physical integration of PET and CT images coming from separate machine is not as straightforward. Due to patient and biological motions such as respiration, heart and bowel movement during screening period, misalignment between the two images may occur (Goerres et al., 2002). Thus, an accurate spatial registration technique to correct the misregistration is needed. In general, there are three approaches to register the PET/CT images; visual, hardware based and computer based registration methods (Townsend et al., 2004). Traditionally, visual registration is done with the physician comparing both images side by side. It is an exhaustive process and inconsistent registration interpretation might occur among different physicians. Hardware based hybrid PET/CT machine emerges based on the idea of physically integrating the PET and CT machines into a single device. There is a centralised operating system with a single scanning bed. As a result, the use of hybrid PET/CT machine compared to standalone PET and CT machines, increases the localisation of metastatic cancer, improves the sensitivity to malignancy and effectively minimises the involved cost. In addition, the CT transmission data is used for noise attenuation correction of the PET emission data. Pelosi et al., (2004) reported a higher percentage of having false interpretation of lesion localisation in independent PET and CT images (15.3%) as compared to hybrid PET/CT (3.4%).

Although hybrid PET/CT scanner literally restrains the patient motion, the problem of misregistration at the thorax region due to the respiratory/heart/bowel movements remains (Mawlawi & Townsend, 2008). During whole body hybrid PET/CT acquisition, CT scanning is performed in less than a minute with the patient engages in breath-hold, compared to PET scan that can lasts up to 20 minutes with the patient engages in tidal breathing. The unmatched respiratory phase between the PET and CT acquisitions produces unaligned PET/CT images at the thorax and the abdomen. As CT transmission data is used for PET attenuation correction, the misregistration leads to the attenuation correction artefacts that eventually cause inaccurate tumour localisation and size estimation (Nehmeh & Erdi, 2008; Osman et al., 2003). Goerres et al., (2002) found that a maximum displacement of 8.29 cm in the diaphragm between the PET and CT images acquired at maximum inspiration. To solve physiologically induced misregistration between the PET/CT images acquired from combined PET/CT scanner, software based registration technique is used (Camara et al., 2007). Thus, this thesis aims to develop a non-gated postprocessing software based registration technique to solve the PET/CT misalignment problem. In brief, the developed technique is based on hybrid feature intensity multimodal demon registration framework which consists of three major steps: filtering the PET sinogram, segmenting the main structures in the PET/CT images and registering the images using the segmented features and improved intensity based demon registration.

1.2 Problem Statement

Postprocessing image registration software is important for both separate and combined PET/CT systems for better image interpretation and analysis. In thoracic oncology PET/CT diagnosis and radiotherapy, both the functional PET and anatomical CT images are integrated so that accurate oncological diagnosis, radiotherapy planning and monitoring processes can be achieved. Integrating these two images therefore requires good registration strategy as these images are taken at different time and place. Misregistered PET/CT images will cause inaccurate interpretation (underestimation/overestimation) gross tumour volume and tumour malignancy due to variation in standardized uptake value (SUV) in PET as well as inaccurate tumour localisation as the anatomical (CT) and physiological (PET) information do not correlated very well. Exact tumour localisation is important in radiotherapy so that an optimal target volume to be irradiated can be identified while reducing the impact of radiation on healthy tissues. In terms of radiotherapy monitoring, an exact quantification of standardised uptake value is required for the physician to reliably decide the next course of treatment.

Since its beginning until today, the hybrid PET/CT persistently fails to accurately register both the PET/CT images. The PET/CT misregistration problem in hybrid PET/CT scanner is in fact an inherent issue (Pan & Mawlawi, 2008; Sureshbabu & Mawlawi, 2005; Mawlawi & Townsend, 2009; Nye & Faber, 2011; Shekhar et al., 2005 and Alessio et al., 2004) due to nonlinear respiratory, cardiac and bowel

motions apart from the patient motion. These motions result in heavily affected misregistration at the thorax and the abdomen compared to the other regions of the body. The most significant artefact is the so called “banana artefact” in the PET image (Sureshababu & Mawlawi, 2005). The artefact shows underestimated low activity region at the lung base (the diaphragm). Induced misregistration at the thoracic region is mainly due to respiratory motion and the different scan times between the PET and CT scan. The CT scan takes less than one respiratory cycle while the PET scan takes up to 8 minutes per bed position. In obvious, there will always be respiratory phase mismatch in terms of the misaligned lung volumes of the two images. The CT image is considered taken at a certain respiratory phase while the PET image is an image averaged over multiple respiratory cycles and cardiac positions. There are several studies that have been conducted to investigate the frequency of having misregistration at these areas. For example, Pan et al., (2005) reported a percentage of 50% out of 100 patient studies experienced significant diaphragm misalignment between the hybrid PET/CT images with some of the cases showed greater than 2 cm mismatch error. In addition Gould et al., (2007) presented a percentage of 40% false positive results in their cardiac PET/CT diagnostic purpose owing to misregistration artefacts.

Nye & Faber (2011) listed several proposed approaches to compensate misregistration artefacts. One example is to instruct the proper breathing protocol named as deep inspiration breath hold (DIBH) to the patient for both CT and PET exams (Nehmeh et al., 2007). However, DIBH requires a breathing coach and the additional respiratory monitoring hardware to be integrated into the hybrid PET/CT machine. The other approach is to specify specific CT protocols slow CT scan, low-pitch CT and cine CT) so that the CT scan can be conducted under free breathing. Another approach is based on respiratory gating (Nehmeh et al. 2008). In this technique, several PET images of different respiratory bins are generated using the gating mechanism. The respiratory motion is estimated from the gated PET emission data and then the motion fields are used to register the static CT image with the PET image of similar respiratory bin. However, this method results in reconstructed PET bin image with reduced signal to noise ratio (SNR) and it requires additional hardware to be embedded in the PET/CT machine, thus increases cost (Nehmeh et al. 2008).

Thus, the thesis aims to improve the image registration between the PET/CT images of hybrid scanner through software based registration algorithm. Although the existing hybrid machines are equipped with commercial registration and fusion software tools, most of the registration software (Steffen et al., 2013; Gong, O’keefe & Scott, 2005) normally solves rigid deformation that is irrelevant for thoracic region. Besides, (Weigert et al., 2008) also concluded that the tested rigid and non-rigid commercial registration software on the whole body combined PET/CT datasets in their experiment failed to meet sufficient registration quality as required. Thus far, there are a number of registration methods have been proposed for thoracic PET/CT images and few works are actually tested their algorithms on combined PET/CT datasets (Jin et al., 2013; Camara et al., 2007; Moreno et al., 2006; Shekhar et al., 2005).

None of these methods considers the pre-processing the PET sinogram through filtering in order to obtain a better quality PET image. It is a well-known fact that the reconstructed PET image is blurry and noisy. These inherent characteristics of the PET image are due to random and scatter effects and the design of the electrical parts that constitute the whole PET machine. Evidently the quantification and interpretation of tumour based on noisy and blurry PET image will be less than accurate. Therefore, the reconstructed PET image should be smoothed and enhanced to attain better tumour interpretation. In terms of solving the PET/CT misregistration problem, the use of a better quality, smoothed and enhanced PET image in the registration process will likely generate better registration accuracy than using blurry, noisy PET image. Based on this notion, this thesis proposes a 3D hybrid mean-median PET sinogram filter as a pre-processing step in the proposed registration framework. Besides improving the registration accuracy, the proposed method is considered as a mean to improve the conventional PET reconstruction method that is filtered back projection (FBP) and advanced reconstruction methods such as iterative maximum likelihood estimation maximisation (MLEM) in PET reconstruction subject (Alessio & Kinahan, 2006). Another aspect that is overlooked in the previous literature is a dedicated registration step for the heart structure. Some of the previous works mainly focused on the lung structure in their integrated intensity-feature based registration by assuming that the heart will be accurately aligned following the deformation fields of the lung registration. However, this assumption is not always valid (Faber et al., 2010). Thus, an independent heart registration is required during the feature based registration implementation. Apart from the heart, the other identified structures are the tumour and the lungs. One might argue on the necessity to have a specific heart registration for thoracic oncologic PET/CT study as it is mainly used for lung cancer diagnosis and management. However, there are reported findings on cardiac masses detection in whole body oncology PET/CT study (Mallia et al., 2009; Zhang, Li & Jiang, 2008).

Due to this reason, a separate heart registration is proposed in this thesis so that a thorough, extensive investigation of any malignancy at the heart region can be conducted from the well registered PET/CT images. Although (Moreno et al., 2006) has raised the idea of specific heart registration, it has not been practically implemented in their work. They also suggested that the heart should remain rigid during the whole registration process. However, this thesis adopts the approach of independently deforming the heart through non-rigid deformation based on the findings of Bond et al., (2008). They have found that the heart region was better aligned using translation and deformable transformation compared to translation or rigid transformation alone. In order to independently register the heart, the heart regions in both PET/CT images need to be identified or segmented. Therefore, the second step in the proposed registration framework in this thesis performs main structures segmentation in both PET/CT. These structures are the lungs, the heart and the tumour. Automatic segmentation of the whole heart is not an option. It should be done manually due to the inconsistency of the heart uptake of varying patients' datasets (Fukuchi et al., 2007).

Third, based on the latest work by Jin et al., (2013) on PET/CT registration problem, the thesis attempts to improve their modified multimodal intensity demon registration through feature integration as well as merging different similarity measures in their technique so that the algorithm is designed to be more robust towards various medical images as well as simple images. The current work by Jin et al., (2013) showed an improvement of their work in registering PET/CT images compared to the previously proposed method (Mattes et al., 2003). Originating from this work, the multimodal intensity demon registration can be made superior by merging different similarity measures to define the demon energy. The superiority can be justified by testing the algorithms on different kinds of medical and simple images. In specific to thoracic PET/CT registration problem, the newly improved multimodal intensity demon can be combined with feature based demon registration serially in order to obtain optimal registration accuracy.

1.3 Aim and Objectives

The aim of the research is to develop a postprocessing image registration technique for PET/CT images acquired from hybrid PET/CT scanner focusing at the thoracic region. The aim is achieved by specifying the following objectives:

- i. To develop a filter for the PET sinogram data in order to obtain a better quality PET image.
- ii. To develop segmentation framework for structures (the lung, the tumour and the heart) in thoracic PET and CT images.
- iii. To improve the original monomodal demon registration method that works for multimodal registration problem in order to obtain improved registration accuracy between PET/CT images.

1.4 Scope and Limitation of the Study

The thesis studies on improving the registration between PET/CT images acquired from combined hybrid PET/CT scanner. To achieve this, three major steps are identified. The first step is to filter the PET sinogram raw data. Second, is to segment three main structures, which are the lungs, the heart and possible tumours in both images. The third step is to perform hybrid feature-intensity registration based on modified demon registration that can works for multimodal registration cases. A 3D hybrid mean-median filter is proposed to filter the PET sinogram. To evaluate the efficacy of the sinogram filter, four PET sinograms with different SNR are simulated using ASIM PET simulator software (Elston et al., 2012). The simulated phantom used which is inputted into the software is based on NURBS cardiac and torso phantom (NCAT) developed by Segars (2001).

The proposed sinogram filter is tested on the four datasets and is compared with standard mean and median filters as well as four established edge preserving filters, namely Non-local means filter (Buades, Coll, & Morel, 2005), Anisotropic Diffusion filter (Perona & Malik, 1990) and Adaptive Modified Probability Curvature Motion filter, the latest proposed PET sinogram filter by Alrefaya & Sahli, (2013). The comparison is made based on the quality of the reconstructed PET image using FBP method. Another evaluation is to investigate the percentage of improvements made by the filter on the reconstructed image using FBP and iterative based statistical reconstruction method namely Maximum Likelihood Maximisation Estimation – Median Root Prior (MLEM-MRP), (Alenius, Ruotsalainen & Astla, 1998). The image quality is assessed according to visual displays, signal to noise ratio (SNR), local signal to noise ratio, contrast to noise ratio (CNR) and edge preserving quality through the display of the line profile. The limitation of the filter analysis is the lack of the real PET sinogram acquired from hybrid PET/CT machine. This is because the real sinogram could not be retrieved from the hybrid PET/CT machine Biograph 6, Siemens Medical Solutions Incorporated. This hybrid machine which is attached to the UPM Nuclear Diagnostic Imaging Centre (PPDN-UPM), Universiti Putra Malaysia, Malaysia supplies the PET/CT datasets used in the segmentation and registration experiments of this thesis.

The second step deals with segmenting important structures which are the lungs, the heart and the possible tumours, in the PET/CT images. The proposed method for lungs segmentation in CT image is based on thresholding and region growing. The lung segmentation in CT image is considered trivial due to distinct intensity of the lung regions across CT datasets. In opposite, the lung segmentation in PET image is considered difficult. The proposed method uses a combination of edge refinement and spatial fuzzy C mean clustering (Chuang et al., 2006). In terms of heart segmentation in non-contrast enhanced CT image, the thesis proposes an automated determination of the heart volume of interest based on the obtained CT lung volume. Then the fine heart structure is obtained through slice by slice Distance Regularised Level Set (DRLSE) method (Li et al., 2010).

Finally the possible tumours in the PET and CT images are segmented semi automatically using thresholding, region growing and DRLSE methods. The limitation of the proposed structures segmentation methods at this stage is the disability of the methods to handle any PET/CT patient datasets with serious pathology conditions such as patients infected with pleural effusion (fluid build-up) in their lungs due to chronic malignancy, liver failure and others (Yao, Han & Summers, 2009). Apart from this, the proposed methods also could not be applied on PET/CT datasets in which the patients bearing high density very large lung tumours that attached to the chest wall and the mediastinum. In this case, the attached tumours tend to be excluded from the lung boundary due to their intensity similarity with the chest wall. These two examples of severities impede the reliable estimation of the lung boundary in both the CT images and the following PET images as well as the estimation of the initial CT heart volume of interest (VOI).

Therefore, the tested segmentation algorithms are performed on 21 patient datasets out of 27 datasets archived from the previously mentioned hybrid PET/CT machine in which 6 patient datasets show serious lung pathologies. The segmentation results are analysed using visual displays as well as comparison with manual delineation by the expert. The latter analysis is done by measuring several overlapping metrics between the automated segmented structures with that of the manual segmented structures. These metrics are Jaccard coefficient, Dice coefficient, False positive ratio and False negative ratio. Only 10 out of 21 datasets are used to be compared with manual ground truths.

The third step is to register the 21 clinical PET/CT datasets and to analyse any registration improvement before and after the registration process. The proposed filter is based on demon registration that is improved by integrating feature based demon registration as well as upgrading the demon capability to work for multimodal registration. Apart from visual displays, registration analysis is also done based on global similarity metric normalised mutual information (NMI) achievement pre- and post-registration in percentage and comparing the proposed filter with established, commercialised registration technique which is free form deformation method (Rueckert et al., 1999). The use of NMI mutual information is considered a reliable and competent measure to compare the improvement of the proposed registration method on the combined PET/CT datasets post-registration (Modat et al., 2010; Pekar, Gladilin & Rohr, 2006) as the registration accuracy correlates well with the improved NMI measure (Rivest et al., 2010). The registration improvement is also inspected in terms of the lung volume overlap improvement between the PET lung and the CT lung after registration.

1.5 Thesis Contribution

The main contribution of this thesis is the registration improvement between the PET/CT images acquired from hybrid PET/CT machine. To achieve this goal, this thesis proposes an improved registration method that comprises of three major steps, where each of them represents three different image processing areas; filtering, segmentation and registration. In the first step, *first*, this thesis contributes in the development of a new filter on the PET sinogram data in order to obtain a better, enhanced PET image. The filter uses a combination of 3D mean and median filters of specified masks. The mean and median values are estimated according to a weighted average scheme that considers the “similarity” among the voxels which constitute each mask. Furthermore, the filter improves the quality of the PET image when both analytical filtered backprojection (FBP) and statistical iterative reconstruction method, to be specific median root prior – maximum likelihood expectation maximisation (MRP-MLEM) are used.

The second contribution of this thesis is the proposed segmentation framework for structures in the thoracic region in PET/CT images in particular for the heart in non-contrast CT and the lungs in the PET image. Published methods to perform segmentation of these two structures are uncommon. In this thesis, an automated heart segmentation for non-contrast CT is proposed in which the initial heart volume of interest (VOI) is identified automatically compared to manual determination of the VOI in the previously reported work. On the other hand, the PET lungs are segmented using fuzzy based clustering on the priorly estimated lung core. Implementing fuzzy clustering on the lung core allows a fixed number of clusters to be used in the clustering scheme rather than having to heuristically determine the parameter as applied in the previous works.

The third contribution is the improvement on the original demon registration for multimodal image registration problem. The previously proposed intensity based multimodal demon using mutual information (MI) is improved by combining two other similarity measures, which are sum of conditional variance (SCV) and multimodality independent neighbourhood descriptor (MIND) in its formulation. This increases the robustness of the method and improves the registration accuracy. The modified multimodal demon has been experimented on various types of simple as well as medical images.

REFERENCES

- [1] Alenius, S., Ruotsalainen, U., & Astola, J., "Using local median as the location of the prior distribution in iterative emission tomography image reconstruction," *IEEE Transactions on Nuclear Science*, vol. 45, no. 6, pp. 3097–3104, 1998.
- [2] Alessio, A.M., & Kinahan, P.E., "PET image reconstruction," Nuclear Medicine, 2nd edition, Mosby, 2006.
- [3] Alessio, A. M., Kinahan, P. E., Cheng, P. M., Vesselle, H., & Karp, J. S., "PET/CT scanner instrumentation, challenges, and solutions," *Radiologic Clinics of North America*, vol. 42, no. 6, pp. 1017–32, 2004.
- [4] Alessio, A.M., Kohlmyer, S., Branck, K., Chen, G., Caldwell, J., & Kinahan, P. "Cine CT for attenuation correction in cardiac PET/CT," *Journal of Nuclear Medicine*, vol. 48, pp. 794-801, 2007.
- [5] Ali, R., Gunduz-Demir, C., Szilágyi, T., Durkee, B., & Graves, E. E., "Semi-automatic segmentation of subcutaneous tumours from micro-computed tomography images," *Physics in Medicine and Biology*, vol. 58, no. 22, pp. 8007–19, 2013.
- [6] Alrefaya, M., & Sahli, H., "A Novel Adaptive Probabilistic Nonlinear Denoising Approach for Enhancing PET Data Sinogram," *Journal of Applied Mathematics*, pp. 1–14, 2013.
- [7] Alterovitz, R., Goldberg, K., Pouliot, J., Hsu, I-CJ., Kim, Y., Noworolski, S.M. & Kurhanewicz, J. "Registration of MR prostate image with biomechanical modeling and nonlinear parameter estimation," *Medical Physics*, vol. 33, pp. 446-454, 2006.
- [8] Andia, B. I. Nonstationary and Nonlinear Sinogram Filtering for Tomographic Image Reconstruction. PhD Thesis. Department of Electrical Engineering, Notre Dame: Indiana, 2003.
- [9] Antonio, M.I. Nonlinear registration of thoracic PET and CT images for the characterization of tumours: Application to radiotherapy. PhD Thesis. Telecom Paris. 2007.
- [10] Audette, M.A., Ferrie, F. P., & Peters, T. M., "An algorithmic overview of surface registration techniques for medical imaging," *Medical Image Analysis*, vol. 4, no. 3, pp. 201-217, 2000.
- [11] Aykac, D., Hoffman, E. A., McLennan, G., & Reinhardt, J. M., "Segmentation and analysis of the human airway tree from three-dimensional X-ray CT

- images," *IEEE Transactions on Medical Imaging*, vol. 22, no. 8, pp. 940–50, 2003.
- [12] Bajcsy, R., & Kovačič, S., "Multiresolution elastic matching," *Computer Vision, Graphics, and Image Processing*, vol. 46, no. 1, pp. 1–21, 1989.
- [13] Balda, M., Hornegger, J., & Heismann, B., "Ray contribution masks for structure adaptive sinogram filtering," *IEEE Transactions on Medical Imaging*, vol. 31, no. 6, pp. 1228–1239, 2012.
- [14] Ballangan, C., Wang, X., Fulham, M., Eberl, S., Yin, Y., & Feng, D., "Automated delineation of lung tumors in PET images based on monotonicity and a tumor-customized criterion," *IEEE Transactions on Information Technology in Biomedicine*, vol. 15, no. 5, pp. 691–702, 2011.
- [15] Bartz, D., Mayer, D., Fischer, J., Ley, S., del Rio, A., Thust, S., Strasser, W., "Hybrid segmentation and exploration of the human lungs," *IEEE Transactions on Ultrasonics, Ferroelectrics and Frequency Control*, pp. 177–184, 2003.
- [16] Belhassen, S., & Zaidi, H., "A novel fuzzy C-means algorithm for unsupervised heterogeneous tumor quantification in PET," *Medical Physics*, vol. 37, no. 3, pp. 1309–24, 2010.
- [17] Beyer, T., Kinahan, P.E., Townsend, D.W., & Sshin, D., "X-ray CT for attenuation correction of PET data," *Proceedings of IEEE Nuclear Science Symposium and Medical Imaging Conference*, 1994, pp. 1573–1577.
- [18] Bian, Z., Ma, J., Huang, J., Zhang, H., Niu, S., Feng, Q., Chen, W., "SR-NLM: a sinogram restoration induced non-local means image filtering for low-dose computed tomography," *Computerized Medical Imaging and Graphics*, vol. 37, no. 4, pp. 293–303, 2013.
- [19] Binhu J., Supe S., Pawar Y., "Intensity Modulated Radiation Therapy: A Clinical Perspective," *Reports of Practical Oncology and Radiotherapy*, vol. 14, pp. 95–103, 2005.
- [20] Bond, S., Kadir, T., Hamill, J., Casey, M., Platsch, G., Burckhardt, D., Declerck, J., "2008). Automatic registration of cardiac PET/CT for attenuation correction," in *IEEE Nuclear Science Symposium Conference Record*, 2008, pp. 5512–5517.
- [21] Brown, L.G., "A survey of image registration techniques," *ACM Computing Survey*, vol. 24, pp. 325–376, 1992.
- [22] Buades, A., Coll, B., & Morel, J.-M., "A Non-Local Algorithm for Image Denoising," in *IEEE Computer Society Conference on Computer Vision and Pattern Recognition*, 2005, vol. 2, pp. 60–65

- [23] Bundschuh, R. A., Martínez-Möller, A., Essler, M., Nekolla, S. G., Ziegler, S. I., & Schwaiger, M., "Local motion correction for lung tumours in PET/CT--first results," *European Journal of Nuclear Medicine and Molecular Imaging*, vol. 35, no. 11, pp. 1981–1988, 2008.
- [24] Burger, C., Goerres, G., Schoenes, S., Buck, A., Lonn, A., & Von Schulthess, G., "PET attenuation coefficients from CT images: experimental evaluation of the transformation of CT into PET 511 keV attenuation coefficients," *European of Journal of Nuclear Medicine and Molecular Imaging*, vol. 27, pp. 922-927, 2002.
- [25] Cachier, P., Bardin E., Dormont, D., Pennec X., & Ayache, N., "Iconic feature based nonrigid registration: The PASHA algorithm," *Computer Vision Image Understanding*, vol. 89, no. 2, pp. 272-298, 2003.
- [26] Cahill, N.D., Noble, J.A., & Hawkes, D.J., "Demon algorithms for fluid and curvature registration," in *IEEE International Symposium on Biomedical Imaging: From Nano to Macro*, 2009, pp. 730-733.
- [27] Camara, O., Delso, G., Colliot, O., Moreno-Ingelmo, A., & Bloch, I., "Explicit incorporation of prior anatomical information into a nonrigid registration of thoracic and abdominal CT and 18-FDG whole-body emission PET images," *IEEE Transactions on Medical Imaging*, vol. 26, no. 2, pp. 164–78, 2007.
- [28] Chuang, K.S., Tzeng, H.L., Chen, S., Wu, J., & Chen, T.J., "Fuzzy c-means clustering with spatial information for image segmentation," *Computerized Medical Imaging and Graphics*, vol. 30, no. 1, pp. 9–15, 2006.
- [29] Crum, W.R., Hartkend, T., & Hill, D. L., "Nonrigid image registration: theory and practice," *British Journal Radiology*, vol. 77, pp. 140-153, 2004.
- [30] Dey, J., Pan, T., Choi, D.J., Robotis, D., Smyczynski, M.S., Pretorius, P.H., King, M.A., "Estimation of Cardiac Respiratory-Motion by Semi-Automatic Segmentation and Registration of Non-Contrast-Enhanced 4D-CT Cardiac Datasets," *IEEE Transactions on Nuclear Science*, vol. 56, pg. 3662-3671, 2009.
- [31] El Naqa, I., Yang, D., Apte, A., Khullar, D., Mutic, S., Zheng, J., Deasy, J. O., "Concurrent multimodality image segmentation by active contours for radiotherapy treatment planning," *Medical Physics*, vol. 34, no. 12, pp. 4738–49, 2007.
- [32] Elston, B., Comtat, C., Harrison, R., & Kinahan, P. ASIM: An analytic PET simulator. *Monte Carlo Calculations in Nuclear Medicine: Applications in Diagnostic Imaging*, CRC Press. 2012.

- [33] Exarhos, D., Tavernaraki, A., Baltouka, A., Tavernaraki, K., Kyratzi, I., Sykara, A., Chondros, D., "Imaging of Cardiac Tumors and Masses," *Hospital Chronicles*, 2010.
- [34] Faber, T. L., Santana, C. A., Piccinelli, M., Nye, J. A., Votaw, J. R., Garcia, E. V., & Haber, E., "Automatic Alignment of Myocardial Perfusion Images with Contrast Cardiac Tomography," in *IEEE Nuclear Science Symposium Conference Record*, 2010, pp. 2996–2997.
- [35] Foster, B., Bagci, U., Ziyue Xu, Dey, B., Luna, B., Bishai, W., Mollura, D. J., "Segmentation of PET images for computer-aided functional quantification of tuberculosis in small animal models," *IEEE Transactions on Bio-Medical Engineering*, vol. 61, no. 3, pp. 711–24, 2014.
- [36] Frangi, A. F. Three-dimensional model-based analysis of vascular and cardiac images. Utrecht University, The Netherlands, 2001.
- [37] Fukuchi, K., Ohta, H., Matsumura, K., & Ishida, Y., "Benign variations and incidental abnormalities of myocardial FDG uptake in the fasting state as encountered during routine oncology positron emission tomography studies," *The British Journal of Radiology*, vol. 80, no. 949, pp. 3–11, 2007.
- [38] Goerres, G. W., Kamel, E., Heidelberg, T.-N. H., Schwitter, M. R., Burger, C., & von Schulthess, G. K., "PET-CT image co-registration in the thorax: influence of respiration," *European Journal of Nuclear Medicine and Molecular Imaging*, vol. 29, no. 3, pp. 351–60, 2002.
- [39] Gong, S., O'keefe, G., & Scott, A., "Comparison and Evaluation of PET/CT Image Registration," in *International Conference of the IEEE Engineering in Medicine and Biology Society*, 2005, pp. 1599–603.
- [40] Gould K. L., Pan, T., Loghin, C., Johnson, N. P., Guha, A., & Sdringola, S., "Frequent diagnostic errors in cardiac PET/CT due to misregistration of CT attenuation and emission PET images: a definitive analysis of causes, consequences and correction," *Journal of Nuclear Medicine*, vol. 48, pp. 1112–1121, 2007.
- [41] Han, X.-H., Chen, Y.-W., Kitamura, K., Ishikawa, A., Inoue, Y., Shibata, K., Mukuta, Y., "ICA-Based noise reduction for PET Sinogram-Domain Images," in *IEEE/ICME International Conference on Complex Medical Engineering*, 2007, pp. 1655–1660.
- [42] Happonen, A. Decomposition of Radon Projections into Stackgrams for Filtering, Extrapolation, and Alignment of Sinogram Data. PhD Thesis. Department of Information Technology, Tampere University of Technology, 2005.

- [43] Heinrich, M. P., Jenkinson, M., Bhushan, M., Matin, T., Gleeson, F. V., Brady, S. M., & Schnabel, J. A., "MIND: modality independent neighbourhood descriptor for multi-modal deformable registration," *Medical Image Analysis*, vol. 16, no. 7, pp. 1423–35, 2012.
- [44] Hill, D.L.G., Batchelor, P.G., Holden, M., & Hawkes, D.J., "Medical image registration," *Physics Medical Biology*, vol. 46, pp. 1-45, 2001.
- [45] Hoh, C. K., Huang, S. C. H., & Hoffman, E. J., " Utilization of 3-D elastic transformation in the registration of chest X-ray CT and whole body PET," in *IEEE Nuclear Science Symposium. Conference Record, 1996*, vol. 3, pp. 1903–1907.
- [46] Hu, S., Hoffman, E. A., & Reinhardt, J. M., "Automatic lung segmentation for accurate quantitation of volumetric X-ray CT images," *IEEE Transactions on Medical Imaging*, vol. 20, no. 6, pp. 490–8, 2001.
- [47] Huang, J., Ma, J., Liu, N., Feng, Q., & Chen, W., "Projection data restoration guided non-local means for low-dose computed tomography reconstruction," in *IEEE International Symposium on Biomedical Imaging: From Nano to Macro*, 2011, pp. 1167–1170. .
- [48] Hutton, B.F., Braun, M., Thruftjell, L., & Lau, D.Y.H., "Image registration: an essential tool for nuclear medicine," *Nuclear Medical Molecular Imaging*, vol. 29, pp. 559-577, 2002.
- [49] Irving, B., Taylor, P., & Todd-Pokropek, A., "3D segmentation of the airway tree using a morphology based method," in *Proceedings of International Workshop Pulmonary Image Analysis*, 2009, pp. 297-307.
- [50] Ishikawa, A., Kitamura, K., Mizuta, T., Tanaka, K., Amano, M., & Inoue, Y., "Implementation of noise reduction for PET using hybrid nonlinear wavelet shrinkage method," in *IEEE Nuclear Science Symposium Conference Record*, 2007, vol. 4, pp. 3000–3003.
- [51] Jiao, J., Markiewicz, P., Burgos, N., Atkinson, D., Hutton, B., Arridge, S., & Ourselin, S. "Detail-Preserving PET Reconstruction with Sparse Image Representation and Anatomical Priors," *Information Processing in Medical Imaging*, vol. 24, pp. 540-551, 2015.
- [52] Jin, S., Li, D., Wang, H., & Yin, Y., "Registration of PET and CT images based on multiresolution gradient of mutual information demons algorithm for positioning esophageal cancer patients," *Journal of Applied Clinical Medical Physics*, vol.14, no. 1, 3931, 2013.
- [53] Kachelriess, M., Watzke, O., & Kalender, W. A., "Generalized multi-dimensional adaptive filtering for conventional and spiral single-slice, multi-slice, and cone-beam CT," *Medical Physics*, vol. 28, no. 4, pp. 475–90, 2001.

- [54] Khodadad, D., Ahmadian, A., Banaem, H. Y., Ay, M. R., & Fard-Esfahan, A., "CT and PET Image Registration: Application to Thorax Area," *Journal of Image and Graphics*, 1, pp. 171–175, 2013.
- [55] Kim, Y., Yoon, S., & Yi, J., "Effective sinogram-inpainting for metal artifacts reduction in X-ray CT images," in *IEEE International Conference on Image Processing*, 2010, pp. 597–600.
- [56] Korfiatis, P., Skiadopoulos, S., Sakellaropoulos, P., Kalogeropoulou, C., & Costaridou, L., "Combining 2D wavelet edge highlighting and 3D thresholding for lung segmentation in thin-slice CT," *The British Journal of Radiology*, vol. 80, no. 960, pp. 996–1004, 2007.
- [57] Kroon, D., & Slump, C. H., "Coherence Filtering to Enhance the Mandibular Canal in Cone-Beam CT data," *IEEE-EMBS Benelux Chapter*, 2009.
- [58] Li, C., Xu, C., Gui, C., & Fox, M. D., "Distance regularized level set evolution and its application to image segmentation," *IEEE Transactions on Image Processing*, vol. 19, no. 12, pp. 3243–54., 2010.
- [59] Li, T., Li, X., Wang, J., Wen, J., Lu, H., Hsieh, J., & Liang, Z., "Nonlinear sinogram smoothing for low-dose X-ray CT," *IEEE Transactions on Nuclear Science*, vol. 51, no. 5, pp. 2505–2513, 2004.
- [60] Loeckx, D., Slagmolen, P., Maes, F., Vandermeulan, D. & Suetens, P., "Nonrigid image registration using conditional mutual information," *IEEE Transactions on Medical Imaging*, vol. 29, pp. 19-29, 2010.
- [61] Lu, H., Cheng, J.-H., Han, G., Li, L., & Liang, Z., "3D distance-weighted Wiener filter for Poisson noise reduction in sinogram space for SPECT imaging," *Medical Imaging*, pp. 905–913, 2001.
- [62] Lu, H., Reyes, M., Serifovic, A., Šerifović, A., Weber, S., Sakurai, Y., Cattin, P. C., "Multi-modal diffeomorphic demons registration based on point-wise mutual information," in *IEEE International Symposium on Biomedical Imaging: From Nano to Macro*, 2010, pp. 372–375.
- [63] Maier, A., Wigstrom, L., Hofmann, H. G., Hornegger, J., Zhu, L., Strobel, N., & Fahrig, R., "Three-dimensional anisotropic adaptive filtering of projection data for noise reduction in cone beam CT," *Medical Physics*, vol. 38, no. 11, pp. 5896–909, 2011.
- [64] Maintz J. B. A., & Viergever, M.A.A., "A survey of medical image registration," *IEEE Transactions of Medical Imaging*, vol. 2, pp. 1-36, 1998.
- [65] Mallia, A., Travaini, L., Trifiro, G., & Paganelli, G., "Detection of a cardiac mass by [18F]FDG-PET/CT: a rare case," *Ecancermedicalscience*, vol. 3, pp. 152, 2009.

- [66] Manduca, A., Yu, L., Trzasko, J. D., Khaylova, N., Kofler, J. M., McCollough, C. M., & Fletcher, J. G., "Projection space denoising with bilateral filtering and CT noise modeling for dose reduction in CT," *Medical Physics*, vol. 36, no. 11, pp. 4911–9, 2009.
- [67] Mansoor, A., Baqci, U. Foster, B., Xu, Z., Papadakis, G.Z., Folio, L.R. Udupa, J.K., & Mollura, D.J., "Segmentation and Image Analysis of Abnormal Lungs at CT: Current Approached, Challenges and Future Trends," *Radiographics*, vol. 35, pp. 1056-1076, 2015.
- [68] Martinez-Möller, A., Souvatzoglou, M., Navab, N., Schwaiger, M., & Nekolla, S. G., "Artifacts from misaligned CT in cardiac perfusion PET/CT studies: frequency, effects, and potential solutions," *Journal of Nuclear Medicine*, vol. 48, no. 2, pp. 188–93, 2007.
- [69] Mattes, D., Haynor, D. R., Vesselle, H., Lewellen, T. K., & Eubank, W., "PET-CT image registration in the chest using free-form deformations," *IEEE Transactions on Medical Imaging*, vol. 22, pp. 120--128, 2003.
- [70] Mawlawi, O., & Townsend, D.W., "Multimodality imaging: an update on PET/CT technology," *European Journal of Nuclear Medicine and Molecular Imaging*, vol. 36, pp. 15-29, 2009.
- [71] McQuaid, S. J., Lambrou, T., & Hutton, B. F., "A novel method for incorporating respiratory-matched attenuation correction in the motion correction of cardiac PET-CT studies," *Physics in Medicine and Biology*, vol. 56, no. 10, pp. 2903–15, 2011.
- [72] Meyer, C. R., Boes, J. L., Kim, B., Bland, P. H., Zasadny, K. R., Kison, P. V, Wahl, R. L., "Demonstration of accuracy and clinical versatility of mutual information for automatic multimodality image fusion using affine and thin-plate spline warped geometric deformations," *Medical Image Analysis*, vol. 1, no. 3, pp. 195–206, 1997.
- [73] Modat, M., Vercauteren, T., Ridgway, G. R., Hawkes, D. J., Fox, N. C., & Ourselin, S., "Diffeomorphic demons using normalised mutual information, Evaluation on Multi-Modal Brain MR Images," *SPIE Medical Imaging*, pp. 6232K–76232K–8, 2010.
- [74] Modersitzki J. Numerical Methods for Image Registration. Oxford University Press. New York. 2004.
- [75] Moltz, J.H., Kuhnig, J.M., Boremann, L., & Peitgen, H., " Segmentation of juxtapleural lung nodules in CT scan based on ellipsoid approximation," *First International Workshop on Pulmonary Image Processing*, 2008.

- [76] Montgomery, D. W. G., Amira, A., & Zaidi, H., "Fully automated segmentation of oncological PET volumes using a combined multiscale and statistical model," *Medical Physics*, vol. 34, no. 2, pp. 722–36., 2007.
- [77] Moreno, A., Delso, G., Camara, O., & Bloch, I., "Non-linear registration between 3D images including rigid objects: Application to CT and PET lung images with tumors," *Workshop on Image Registration in Deformable Environments*. 2006, pp. 31–40.
- [78] Moreno, A., Takemura, C. M., Colliot, O., Camara, O., & Bloch, I., "Using anatomical knowledge expressed as fuzzy constraints to segment the heart in CT images," *Pattern Recognition*, vol. 41, no. 8, pp. 2525–2540, 2008.
- [79] Moreno-Ingelmo, A. Non-Linear Registration of Thoracic PET and CT Images for the Characterization of Tumors: Application to Radiotherapy. PhD Thesis. Telecom ParisTech. 2007.
- [80] Morten Bro-nielsen, C. G., "Fast Fluid Registration of Medical Images," in *Proceedings of the 4th International Conference on Visualization in Biomedical Computing*, 1996, pp. 265–276.
- [81] Nehmeh, S. A., & Erdi, Y. E., "Respiratory motion in positron emission tomography/computed tomography: a review," *Seminars in Nuclear Medicine*, vol. 38, no. 3, pp. 167–76, 2008.
- [82] Nehmeh, S.A., Erdi, Y. E., Meirelles, G.S., Squire, O., Larson, S.M., Humm, J.L., & Schoder, H., "Deep inspiration breath hold PET," *Journal Nuclear Medicine*, vol. 48, pp. 2226, 2007.
- [83] Nguyen, V., & Lee, S., "Incorporating anatomical side information into PET reconstruction usin nonlocal regularization," *IEEE Transactions on Image Processing*, vol. 22, pp. 3961-3973, 2013.
- [84] Nye, J. A., & Faber, T. L., "Current state of hybrid imaging: attenuation correction and fusion," *Journal of Nuclear Cardiology*, vol. 18, no. 4, pp. 729–40, 2011.
- [85] Oliveira F.P.M., & Tavares, J.M.R.S, "Medical image registration: a review," *Computer Methods Methods in Biomechanics and Biomedical Engineering*, vol. 17.2, pp. 73-93, 2014.
- [86] Osman, M. M., Cohade, C., Nakamoto, Y., Marshall, L. T., Leal, J. P., & Wahl, R. L., "Clinically significant inaccurate localization of lesions with PET/CT: frequency in 300 patients," *Journal of Nuclear Medicine*, vol. 44, no. 2, pp. 240–3, 2003.
- [87] Otsu, N., "A threshold selection method from gray-level histograms," *IEEE Transactions on Systems, Man and Cybernetics*, vol. 9, no. 1, pp. 62 – 66, 1979.

- [88] Pan, T., & Mawlawi, O., "PET/CT in radiation oncology," *Medical Physics*, vol. 35, pp. 4955-4966, 2008.
- [89] Pan, T., Mawlawi, O., Nehmeh, S. A., Erdi, Y.E., Luo, D., Liu, H.H., Castillo, R., Mohan, R., Liao, Z., and Macapinlac, H.A., "Attenuation correction of PET images with respiration-averaged CT images in PET/CT," *Journal of Nuclear Medicine*, vol 46, pp. 1481-1487, 2005.
- [90] Pelosi, E., Messa, C., Sironi, S., Picchio, M., Landoni, C., Bettinardi, V., Fazio, F., "Value of integrated PET/CT for lesion localisation in cancer patients: a comparative study," *European Journal of Nuclear Medicine and Molecular Imaging*, vol. 31, no. 7, pp. 932–9, 2004.
- [91] Peltonen, S., Tuna, U., & Ruotsalainen, U., "Low count PET sinogram denoising," in *IEEE Nuclear Science Symposium and Medical Imaging Conference Record, 2012*, pp. 3964–3967.
- [92] Pennec, X., Cahier, P., & Ayache, N., "Understanding the demon algorithm: 3D nonrigid registration by gradient descent", in *Medical Image Computing and Computer Assisted Intervention, MICCAI 1999*, pp.597-606.
- [93] Perona, P., & Malik, J., "Scale-space and edge detection using anisotropic diffusion," *IEEE Transactions on Pattern Analysis and Machine Intelligence*, vol. 12, no. 7, pp. 629–639, 1990.
- [94] Pickering, M. R., Muhi, A. A., Scarvell, J. M., & Smith, P. N., "A new multi-modal similarity measure for fast gradient-based 2D-3D image registration," in *Proceedings of International Conference of the IEEE Engineering in Medicine and Biology Society*, 2009, pp. 5821–4.
- [95] Pluim, J. P. W., Maintz, J. B. A., & Viergever, M. A., "Mutual-information-based registration of medical images: a survey," *IEEE Transactions on Medical Imaging*, vol. 22, no. 8, pp. 986–1004, 2003.
- [96] Prokop, M., & Galanski, M., *Computed Tomography of the Body*. Thieme. Stuttgart. 2003
- [97] Rabie, T., " Adaptive hybrid mean and median filtering of high-ISO long-exposure sensor noise for digital photography," *Journal of Electronic Imaging*, vol. 13, no. 2, pp. 264, 2004.
- [98] Ramos, C. D., Erdi, Y. E., Gonen, M., Riedel, E., Yeung, H. W., Macapinlac, H. A., Larson, S. M., "FDG-PET standardized uptake values in normal anatomical structures using iterative reconstruction segmented attenuation correction and filtered back-projection," *European Journal of Nuclear Medicine*, vol. 28, no. 2, pp. 155–64., 2001.

- [99] Rigaud, B., Simon, A., Castelli, J., et al., "Evaluation of Deformable Image Registration Methods for Dose Monitoring in Head and Neck Radiotherapy," *BioMed Research International*, vol. 2015, Article ID 726268, 2015.
- [100] Risser, L., Heinrich, M. P., Ruekert, D., & Schnabel, J. A., "Multi-modal diffeomorphic registration using mutual information: Application to the registration of CT and MR pulmonary images," in *Proceedings of MICCAI Workshop on Pulmonary Image Analysis*, 2011, pp. 35–44.
- [101] Rivest, D. R. C., Riauka, T. A., Murtha, A. D., & Fallone, B. G., "Assessment of a commercially available automatic deformable registration system," *Journal of Applied Clinical Medical Physics*, 2010.
- [102] Rizzo, G., Cattaneo, G. M., Castiglioni, I., Reni, M., Vanni, D., Pasquali, C., Fazio, F., "Integration of CT/PET images for the optimization of radiotherapy planning," in *Conference Proceedings of the IEEE Engineering in Medicine and Biology Society*, 2001, vol. 3, pp. 2756–2758.
- [103] Rueckert, D., Sonoda, L. I., Hayes, C., Hill, D. L., Leach, M. O., & Hawkes, D. J., "Nonrigid registration using free-form deformations: application to breast MR images," *IEEE Transactions on Medical Imaging*, vol. 18, no. 8, 712–21, 1999.
- [104] Schäfers, K. P., & Stegger, L., "Combined imaging of molecular function and morphology with PET/CT and SPECT/CT: image fusion and motion correction," *Basic Research in Cardiology*, vol. 103, no. 2, pp. 191–9., 2008.
- [105] Segars, W. P. Development and application of the new dynamic NURBD based cardiac torso (NCAT) phantom. PhD Thesis. Biomedical Engineering, University of North Carolina, 2001.
- [106] Shekhar, R., Walimbe, V., Raja, S., Zagrotsky, V., Kanvinde, M., Wu, G., & Bybel, B., "Automated 3-dimensional elastic registration of whole-body PET and CT from separate or combined scanners," *Journal of Nuclear Medicine*, vol. 46, no. 9, pp. 1488–96, 2005.
- [107] Shojaii, R., Alirezaie, J., & Babyn, P., "Automatic lung segmentation in CT images using watershed transform," in *IEEE International Conference on Image Processing, 2005*, vol. 2, pp. 1270-1273.
- [108] Slomka, P. J., Dey, D., Przetak, C., Aladl, U. E., & Baum, R. P., "Automated 3-dimensional registration of stand-alone (18)F-FDG whole-body PET with CT," *Journal of Nuclear Medicine*, vol. 44, no. 7, pp. 1156–67, 2003.
- [109] Staring, M., Klein, S., & Pluim, J. P. W., "Nonrigid registration with adaptive content-based filtering of the deformation field," *Medical Imaging*, pp. 212–221, 2005.

- [110] Stearns, C. W., "Context-sensitive angular filtering of PET transmission data," in *Proceedings of IEEE Nuclear Science Symposium*, 1995, vol. 3, pp. 1332–1334.
- [111] Steffen, I. G., Hofheinz, F., Rogasch, J. M., Furth, C., Amthauer, H., & Ruf, J., "Influence of rigid coregistration of PET and CT data on metabolic volumetry: a user's perspective," *EJNMMI Research*, vol. 3, no. 1, pp. 85, 2013.
- [112] Suh, J. W., Scheinost, D., Dione, D. P., Dobrucki, L. W., Sinusas, A. J., & Papademetris, X., "A non-rigid registration method for serial lower extremity hybrid SPECT/CT imaging," *Medical Image Analysis*, vol. 15, no. 1, pp. 96–111, 2011.
- [113] Sun, X., Zhang, H., & Duan, H., "3D computerized segmentation of lung volume with computed tomography," *Academic Radiology*, vol. 13, no. 6, pp. 670–7, 2006.
- [114] Sun, T. & Mok, G., S., P., "Techniques for respiration-induced artifacts reductions in thoracic PET/CT", *Quantitative Imaging in Medicine and Surgery*, vol. 2, pp. 46-52, 2012.
- [115] Sureshbabu, W., & Mawlawi, O., "PET/CT imaging artifacts," *Journal of Nuclear Medicine Technology*, vol. 33, pp. 156-161, 2005.
- [116] Tang, C., Xie, X., & Du, R., "Multi-modal image registration based on diffeomorphic demons algorithm," in *Proceedings of SPIE*, 2013, pp. 88781N.
- [117] Thirion, J.-P., "Fast Non-Rigid Matching of 3D Medical Images," Technical Report 2547, Institut National de Recherche en Informatique et en Automatique, pp. 37, 1995.
- [118] Tomasi, C., & Manduchi, R., "Bilateral Filtering for Gray and Color Images," in *Proceedings 6th International Conference on Computer Vision*, 1998, pp. 839–846.
- [119] Townsend, D. W., Carney, J. P. J., Yap, J. T., & Hall, N. C., "PET/CT today and tomorrow," *Journal of Nuclear Medicine*, vol. 45 Suppl 1, 4S–14S, 2004.
- [120] Utsunomiya, D., Nakaura, T., Honda, T., Shiraishi, S., Tomiguchi, S., Kawanaka, K., Yamashita, Y., "Object-specific attenuation correction at SPECT/CT in thorax: optimization of respiratory protocol for image registration," *Radiology*, vol. 237, no. 2, pp. 662–669, 2005.
- [121] Vastil, M., Peltonen, S., & Ruotsalainen, U., "Weighted Butterfly Window Structure for Two-dimensional Sinogram Filtering," in *Proceedings of International Workshop on Nonlinear Signal and Image Processing*, 2007, pp. 160-163.

- [122] Vercauteren, T., Pennec, X., Perchant, A., & Ayache, N., "Diffeomorphic demons: efficient non-parametric image registration." *NeuroImage*, vol 45, S61–72, 2009.
- [123] Viola, P., & Wells, W. M. , " Alignment by maximization of mutual information," in *Proceedings of IEEE International Conference on Computer Vision*, 1995, pp. 16–23.
- [124] Von Schulthess, G.K. *Clinical Molecular Anatomic Imaging: PET, PET/CT and SPECT/CT*. Philadelphia, Pa: Lippincott, Williams & Wilkins, 2003
- [125] Wang, J., Li, T., Lu, H., & Liang, Z., "Penalized weighted least-squares approach to sinogram noise reduction and image reconstruction for low-dose X-ray computed tomography," *IEEE Transactions on Medical Imaging*, vol. 25, no. 10, 1272–83, 2006.
- [126] Weigert, M., Pietrzyk, U., Müller, S., Palm, C., & Beyer, T., " Whole-body PET/CT imaging: combining software- and hardware-based co-registration," *Zeitschrift Für Medizinische Physik*, vol. 18, no. 1, pp. 59–66, 2008.
- [127] Weiss, E., Wijesooriya, K., Dill, S. V., & Keall, P. J., "Tumor and normal tissue motion in the thorax during respiration: Analysis of volumetric and positional variations using 4D CT," *International Journal of Radiation Oncology, Biology, Physics*, vol. 67, no. 1, pp. 296–307, 2007.
- [128] Wells, W. M., Viola, P., Atsumi, H., Nakajima, S., & Kikinis, R., "Multi-modal volume registration by maximization of mutual information," *Medical Image Analysis*, vol. 1, no. 1, pp. 35–51, 1996.
- [129] Wu, X., Liu, S., Wu, M., Sun, H., Zhou, J., Gong, Q., & Ding, Z., "Nonlocal denoising using anisotropic structure tensor for 3D MRI," *Medical Physics*, vol. 40, pp. (101904-1)-(101904-11), 2013.
- [130] Xiong, Z., & Zhang, Y.A., "A critical review of image registration methods," *International Journal of Image and Data Fusion*, vol. 1, pp. 137-158, 2010.
- [131] Yan, J., & Yu, J., "A Nonlinear Variational Model for PET Reconstruction," in *IEEE International Conference on Pattern Recognition*, 2006, vol. 4, pp. 699-702.
- [132] Yang, F., & Grigsby, P. W., "Delineation of FDG-PET tumors from heterogeneous background using spectral clustering," *European Journal of Radiology*, vol. 81, no. 11, 3535–41, 2012.
- [133] Yao, J., Han, W., & Summers, R.M., "Computer aided evolution of pleural effusion using chest CT images," in *Proceedings IEEE International Symposium on Biomedical Imaging*, 2009, pp. 241-244.

- [134] Yu, J. N., Fahey, F. H., Gage, H. D., Eades, C. G., Harkness, B. A., Pelizzari, C. A., & Keyes, J. W., "Intermodality, retrospective image registration in the thorax," *Journal of Nuclear Medicine*, vol. 36, no. 12, 2333–8, 1995.
- [135] Zhang, M., & Gunturk, B. K., "Multiresolution bilateral filtering for image denoising," *IEEE Transactions on Image Processing*, vol. 17, no. 12, pp. 2324–2333, 2008.
- [136] Zhang, M., Li, B., & Jiang, X., "PET/CT imaging in a case of cardiac liposarcoma." *Journal of Nuclear Cardiology: Official Publication of the American Society of Nuclear Cardiology*, vol. 15, no. 3, pp. 473–475, 2008.
- [137] Zheng, G.L., *Medical Image Reconstruction A Conceptual Tutorial*. Higher Education Press, Beijing and SpringerVerlag Berlin Heidelberg, 2010.
- [138] Zitova, B., & Flusser, J., "Image registration methods: a survey," *Image Vision Computing*, vol. 21, pp. 977-1000, 2003.