

The efficacy of functional supports in mediating the effects of exercise on shoulder joint position sense

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Abstract.

BACKGROUND: Prolonged exercise and joint position sense are considered aetiological risk factors for shoulder injury in overhead sports.

OBJECTIVE: To investigate the efficacy of a neoprene sleeve and kinesiology tape (KT) in mediating the effect of exercise on shoulder joint position sense.

METHODS: 25 overhead sports participants (women – 10, men – 15) completed 30 maximal isokinetic repetitions at 120°/s of three shoulder exercise protocols: 9090 (seated 90° shoulder abduction, 90° elbow flexion, modified neutral (seated 45° shoulder abduction, 90° elbow flexion in the scapular plane and diagonal (seated GHJ flexion, abduction, external rotation and extension, adduction and internal rotation. Absolute error in active reproduction of passive positioning was assessed pre- and post-exercise at 10°/s. This was conducted for end range internal and external rotation, and mid-range.

RESULTS: A repeated measures general linear model revealed no significant main effect for gender or exercise in any test position. A main effect for support condition was observed pre-exercise in the KT condition, with JPS significantly ($p < 0.01$) impaired ($5.30 \pm 2.16^\circ$) relative to baseline control scores ($4.11 \pm 2.81^\circ$) in end range external rotation at the 9090 position.

CONCLUSION: Results indicated that neither neoprene nor kinesio-tape were more effective in limiting the effects of exercise on joint position sense (JPS). Healthy, un-injured overhead athletes may not need to consider taping or supportive device, indeed KT application was observed to impair JPS in specific movements.

Keywords: Joint position sense, kinesiology tape, neoprene sleeve, exercise, shoulder

1. Introduction

In overhead sports such as tennis, badminton, volleyball and cricket (bowling) extended and prolonged play is often necessary. It has been suggested that this type of repetitive and prolonged exercise may alter the normal kinematics of the gleno-humeral joint (GHJ) from a joint position sense (JPS) perspective [1]. As such it may be considered as an aetiological risk fac-

tor. Such an intrinsic risk factor may leave an athlete susceptible to a reduction in performance or indeed an increased occurrence of injury. Changes in muscle activity and function of the mechanoreceptors may be associated with injury and loss of performance as deficits in JPS may lead to failure of the rotator cuff (RC) to control stability during movement [2]. Therefore, alterations to mechanoreceptor efficacy may have a detrimental effect.

Functional instability within the GHJ may be linked to decreased proprioception and alterations in neuromuscular control [3] suggesting that alterations to JPS and afferent pathways may increase susceptibility to injury. Alterations to mechanoreceptor efficacy may

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have a detrimental effect on performance. Joint position sense (JPS) acuity is influenced by ranges of motion at a joint [4]. Similarly, there is a decrease in mechanoreceptor stimuli when the GHJ is in a lax, mid-joint position [5]. The influence of prolonged exercise on the dynamic stabilisation of the rotator cuff may be considered as an aetiological risk factor and as such extrapolated to sports requiring repetitive GHJ motions. Many recreational and amateur level athletes will strive to utilise the most effective methods to overcome and offset the negative effects of game play on the GHJ. This may be from an extrinsic aspect in the form of functional supports such as neoprene sleeves and taping such as Kinesio-tape (KT).

Only a few studies have examined the effects of supportive devices or supports on the GHJ. Conflicting results have been proposed determining that a neoprene shoulder sleeve positively affected JPS errors scores measured isokinetically [6], whilst in contrast no positive decrease in error scores when wearing a neoprene shoulder stabiliser. Indeed, for positions of mid and end of range external rotation recorded higher and hence poorer JPS error scores whilst wearing the support [7]. The effects of KT on shoulder JPS has not been examined. However, no increase in static proprioception was found on ankle JPS when compared to no taping in a group of healthy individuals [8]. The ability for an athlete to undertake their chosen sport whilst limiting the negative impact of prolonged exercise is of benefit. Supports such as neoprene sleeves and kinesio-tape may help to control and mediate the effects of prolonged exercise on GHJ structures thus maintaining stability.

This study aimed to assess the effects of an isokinetically induced exercise protocol and the application of shoulder supportive devices on joint position sense by examining active reproduction of passive positioning (ARPP) [9] of the dominant arm GHJ of athletes involved in overhead sports. The study aimed to assess ARPP angles through a functional range of motion. A comparison of the efficacy of a functional support (a neoprene shoulder sleeve) in relation to a KT functional taping technique was evaluated. The study tailored the exercise protocol to mimic the requirements of overhead sports, therefore, generating results applicable to game duration.

2. Method

2.1. Participants

Twenty-five healthy adult subjects (male, $n = 15$,

female, $n = 10$, average age 22 years, mean weight 70.5 kgs, all right hand dominant) actively involved in overhead sports and/or sports reliant on GHJ rotation were included in the study. Sports included were: Tennis, Badminton, Netball, Volleyball, Basketball, Lacrosse, Squash, Cricket Bowling and Golf. Inclusion criteria were: both gender, aged over 16 years, training at least once a week during the season, club/recreational level. Each participant was required to attend for 2 hours with a minimum of 48 hours between testing sessions. Prospective participants with a history of injury to the shoulder complex of the dominant arm within the last two years were excluded. Arm dominance was assessed as the arm they would chose to throw a ball or hold a racket [10]. The study received ethical approval from the department of sport and physical activity ethics committee at Edge Hill University in accordance with the declaration of Helsinki.

2.2. Procedure

An experimental design with three (neoprene sleeve, KT, control) \times 2 (pre and post exercise) repeated measures was performed to investigate the Gleno-humeral joint (GHJ) active reproduction of passive positioning (ARPP) absolute error scores for JPS of external rotation (ER) and internal rotation (IR) of the dominant arm. Joint position sense error scores were recorded across two time periods (pre and post exercise). The internal goniometer of the isokinetic dynamometer (IKD) measured the difference between the target position angle and the angle reproduced by the participant during ARPP.

2.3. Measurements

2.3.1. Starting test positions

Participants were required to attend on a total of three occasions to undertake each of the testing conditions. Three different GHJ positions were analysed consecutively with a 15 minute recovery period between each position [11]. These positions were assessed creating an extensive profile of shoulder function. The starting positions were: 9090 (sitting with 90° of shoulder abduction and 90° of elbow flexion [12], modified neutral (sitting with 45° of shoulder abduction and 90° of elbow flexion in the scapular plane [13] and diagonal (sitting performing flexion, abduction and external rotation and extension, adduction and internal rotation (IR) [14].

118 2.3.2. Isokinetic proprioception testing

119 Testing was performed on an isokinetic dynamometer
120 (IKD), version 3 (BiodeX Inc, Shirley, New York)
121 in the seated position with straps applied in accordance
122 with manufacturer's guidelines. Active relocation of
123 passive positioning involved the subjects being blind-
124 folded to avoid visual cues [9]. Gravity correction was
125 employed with the GHJ in neutral rotation for each po-
126 sition to allow normalisation of limb weight at a point
127 perpendicular to the floor [10,15]. Shoulder JPS ab-
128 solute error scores were recorded by taking the mean
129 of three pre-exercise repetitions and the mean of three
130 post-exercise repetitions calculated by the internal go-
131 niometer of the IKD. Testing speed for all ARPP tests
132 was 10°/s [9,16–18].

133 2.3.3. Target angles

134 Three different angles were included to provide er-
135 rror scores for end of range external rotation (ER),
136 mid-range and end of range internal rotation (IR) as-
137 sessment at each position thus assessing all potential
138 mechanoreceptors involved in JPS [19]. At the 9090
139 position the entire ROM was 120°. The start position
140 (0°) was 90° GHJ abduction, 90° elbow flexion and
141 neutral rotation. Internal rotation range of motion was
142 50° from the start position and external rotation was
143 70° from the start position. The IR angle was 40° from
144 the start position, ER angle was 60° from the start po-
145 sition and the mid-range positon was 30° from neu-
146 tral into ER. At the modified neutral position the entire
147 ROM was 100°. The start position (0°) was 45° GHJ ab-
148 duction in the frontal plane. Internal rotation (IR) range
149 of motion was 40° from the start position and exter-
150 nal rotation was 60° form the start position. The IR angle
151 was 30° from the start position, ER angle was 50° from
152 the start position and the mid-range positon was
153 50° from neutral into ER. At the diagonal position the
154 entire ROM was 90°. End of range IR was 0° with end
155 of range ER 90°. Internal rotation joint angle was 10°
156 from end of range ER, external rotation was 10° from
157 end of range IR and the mid-range angle was 45° from
158 end of range ER. The testing procedures were counter-
159 balanced for control, neoprene and KT for each partic-
160 ipant. The order of positioning i.e. 9090, modified neu-
161 tral and diagonal was not counter-balanced in order to
162 create a functionally representative protocol relating to
163 the battery of sports included.

164 2.3.4. Isokinetic exercise protocol

165 A 30 repetition isokinetic exercise protocol [20] at
166 120°/s [16] acted as the exercise component. A pilot

167 study determined that a 30 repetition isokinetic pro-
168 tocol was not sufficient to induce fatigue and sub-
169 sequently fatigue was not a variable under scrutiny.
170 The protocol employed represented an association with
171 time duration thus simulating game play. Cardiovascu-
172 lar and metabolic responses are significantly developed
173 after isokinetic endurance training [21]. As such the 30
174 repetition protocol is a valid means of administering
175 resistance capable of representing endurance training
176 observed in game play [22]. Participants were asked
177 to provide maximal effort throughout the entire ROM
178 and exercise until the researcher told them to stop. The
179 protocol carried out was identical to the position being
180 tested i.e. 9090 as specified above. A 15 minute rest
181 interval [11] allowing recovery time mimicking such
182 activities which have intervals and breaks throughout
183 game situations, was provided.

184 2.4. Supportive devices

185 2.4.1. Kinesio-tape (KT)

186 The kinesio-tape used in this study was Rock
187 Tape [23]. Application was in accordance with man-
188 ufacturer's guidelines for a shoulder throwing taping.
189 This technique was chosen as it most closely adhered
190 to the functional requirements of the overhead sports
191 included. The manufacturer [23] suggests application
192 of this type of taping be applied along fascial lines
193 whilst the fascia is on stretch. Application of the tape
194 was performed with the dominant arm in a stretched
195 position. An anterior strip of tape was applied from the
196 wrist travelling upwards across the forearm flexor mus-
197 cles, Biceps Brachii, across the Pectoralis Major mus-
198 cle finishing before the sternum. A posterior strip of
199 tape was applied in the same manner from the wrist
200 upwards across the forearm extensor muscles, Triceps
201 Brachii, Posterior Deltoid, and Upper Fibres of Trapezius,
202 finishing at the lower cervical vertebrae. The tape
203 was applied with no stretch, and can be seen in Fig. 1.

204 2.4.2. Neoprene shoulder sleeve

205 The neoprene sleeve (Fig. 2) was a non-branded
206 sleeve and dependent on the size of the participant was
207 either a size small/medium or large/extralarge. The
208 sleeve utilised Velcro both anteriorly and posteriorly
209 across the chest and superior torso respectively.

210 2.5. Statistical analysis

211 Statistical analyses and analysis parameters were de-
212 termined *a priori*. The assumptions associated with a



Fig. 1. Photograph of kinesiology tape application for shoulder throwing.



Fig. 2. Photograph of neoprene sleeve.

repeated measures general linear model (GLM) were assessed to ensure appropriateness, including consideration of residual normality and error of variance. Mauchly's test of sphericity was applied with a Greenhouse Geisser correction where appropriate. With no violation of assumptions, inferential analyses were performed using a mixed method two-way (exercise * support) repeated measures GLM to examine differences pre- and post-exercise, and between support conditions with gender pooling performed. Preliminary analyses using a three-way (exercise * support * gender) GLM revealed no main effect for gender, and no interaction between gender and exercise or support. Subsequently all data was pooled for gender to provide an experimental data set of $n = 25$. Post-hoc least square difference applications were applied where a significant main effect was observed. All statistical analyses were performed using PASW Statistics Editor 20.0 for windows (SPSS Inc, Chicago, USA). Statistical significance was set at $p \leq 0.05$.

3. Results

3.1. 9090 position

Figure 3 summarises the influence of exercise and support condition on the mean absolute joint position

sense error scores at the 9090 position. There was no significant main effect for exercise in end of range internal rotation ($p = 0.22$), mid-range ($p = 0.15$), or end of range external rotation ($p = 0.51$). Post-hoc analyses of support main effects identified a significant ($p < 0.01$) impairment in pre-exercise external rotation JPS when KT was applied ($5.30 \pm 2.16^\circ$) relative to the baseline control condition ($4.11 \pm 2.81^\circ$). In external rotation, there was also a trend ($p = 0.09$) toward impaired performance in the neoprene sleeve condition ($4.15 \pm 3.34^\circ$) relative to baseline control. At the mid-range position there was a trend toward impaired performance post-exercise in the KT trial ($5.11 \pm 2.64^\circ$) relative to both control ($3.91 \pm 2.20^\circ$; $p = 0.07$) and neoprene ($4.19 \pm 2.25^\circ$; $p = 0.10$) conditions.

3.2. Modified neutral position

Figure 4 summarises the influence of exercise and support condition on the mean absolute joint position sense error scores at the modified journal position. There was no significant main effect for exercise in end of range internal rotation ($p = 0.59$), mid-range ($p = 0.38$), or end of range external rotation ($p = 0.27$). There was no significant main effect identified for support condition, but post-hoc analyses of support main effects identified a trend ($p = 0.09$) toward impaired performance post-exercise in external rotation JPS for the neoprene trial ($5.76 \pm 1.94^\circ$) relative to the pre-exercise scores ($4.55 \pm 2.42^\circ$).

3.3. Diagonal position

Figure 5 summarises the influence of exercise and support condition on the mean absolute joint position sense error scores at the diagonal position. There was no significant main effect for exercise in end of range internal rotation ($p = 0.16$), mid-range ($p = 0.11$), or end of range external rotation ($p = 0.55$). There was no significant main effect identified for support condi-

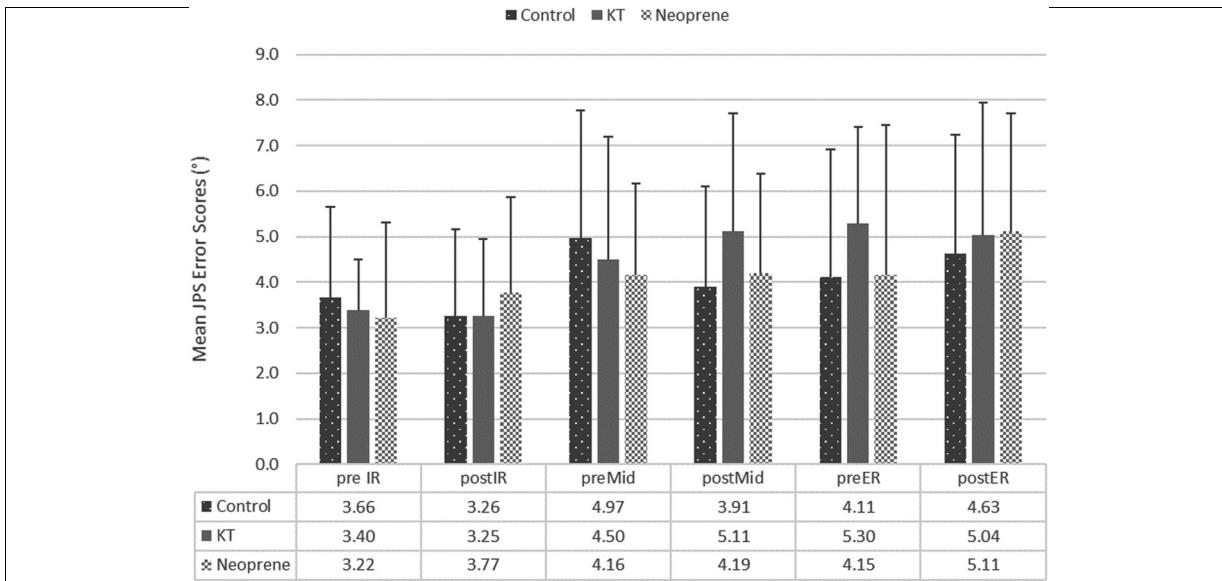


Fig. 3. The influence of joint support on JPS error scores in the 9090 position.

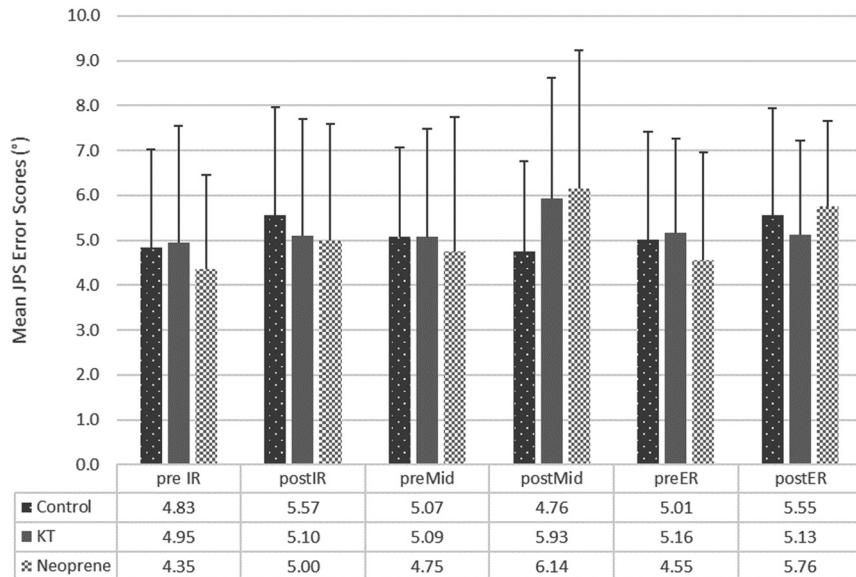


Fig. 4. The influence of joint support on JPS error scores in the modified neutral position.

273 tion, but post-hoc analyses identified a trend ($p = 0.09$)
 274 toward enhanced performance pre-exercise in external
 275 rotation JPS for the neoprene trial ($3.15 \pm 2.10^\circ$) rela-
 276 tive to the baseline control ($3.87 \pm 1.97^\circ$).

277 4. Discussion

278 The aim of this study was to quantify the efficacy of
 279 functional shoulder supports in mediating the impact

of exercise on joint position sense accuracy. The main findings of this study when assessing the mediating effects of kinesiology tape (KT) suggest that the application of KT pre-exercise created significantly poorer joint position sense error scores when compared to the control condition ($P < 0.01$) at end of range external rotation (ER) 9090 position. There was also a trend towards KT being less effective than both the neoprene sleeve and control at the mid-range 9090 position. Fur-

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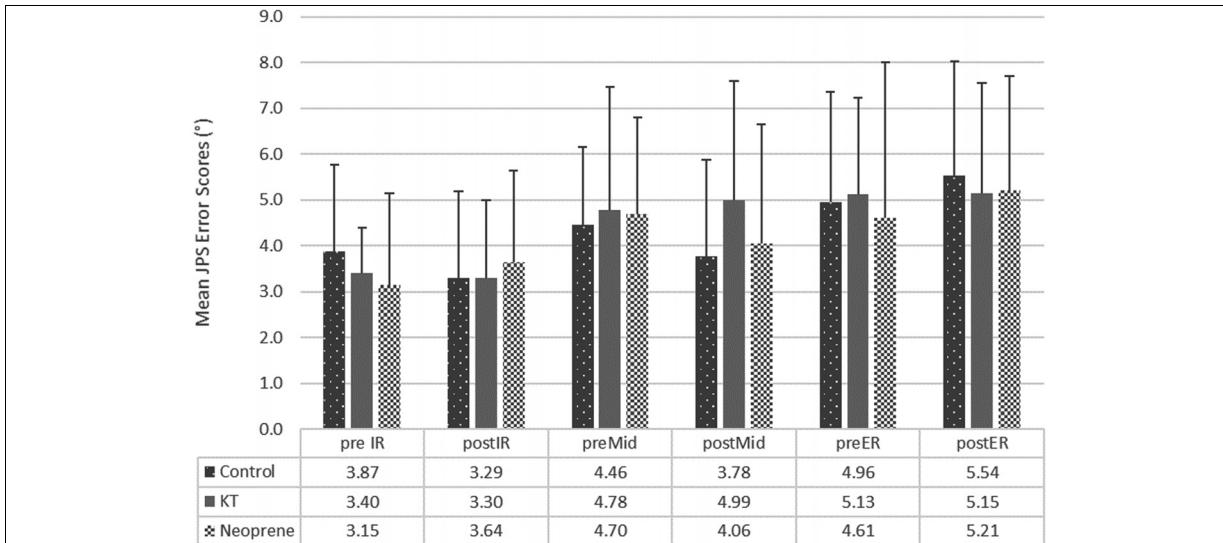


Fig. 5. The influence of joint support on JPS error scores in the diagonal position.

thermore, KT had no influence in comparison to the neoprene sleeve or control at the modified neutral or diagonal positions as no significant difference was determined at any angle. The effects of mechanical deformation related to stretch and compression [24] may suggests an association to capsular and fascial receptors such as Ruffini nerve endings and Pascinian corpuscles [25,26]. However, KT did not mediate exercise at any position at the mid-range. It has been reported that at 90° of shoulder elevation KT diminished JPS acuity but at 50° did not [27] therefore suggesting joint angles are an important factor to consider.

The neoprene sleeve appeared to be effected by both position and angle. At the 9090 position neoprene sleeve out-performed KT at the mid-range ($p = 0.07$) post-exercise suggesting that KT may impair function at this range. In comparison to the control condition of no tape, the neoprene sleeve had a trend towards being more effective at the diagonal position at the internal rotation (IR) angle ($p = 0.09$) pre-exercise, however, this was not found with the 9090 position where the neoprene sleeve was less effective post-exercise at the ER angle ($p = 0.09$). The difference in findings between studies might be attributed to methodological differences, for example not using an overhead sports population and different application of tape (y strips) when applying KT [27]. Our hypothesis for the positive JPS acuity at EOR IR and the detrimental effects at mid-range (KT) may be explained by considering a lack of stretch on the fascia mid-range as an inability for tape to provide as great a stimulus to the underlying tissue and muscle receptors [28]. At a mid-

range position muscular mechanoreceptor response is decreased [5]. This includes involvement of the Golgi tendon organ (GTO) and stretch reflex. Thus, it could be surmised that a different points in the range JPS acuity may alter. At the modified neutral position post-exercise the neoprene sleeve showed a trend towards being worse than at pre-exercise but only at the ER angle. This may suggest the stimulus provided by the neoprene sleeve may begin to become inhibitive as exercise progresses. Eight to ten participants stated that they felt the neoprene sleeve and KT were restrictive when moving in to EOR positions. Skin stimulation from cutaneous receptors [29], in this instance, may have actually have been unhelpful with particular attention paid to the movement pattern in the modified neutral position as increased kinaesthetic stimulation may have over-stimulated at EOR causing JPS to alter.

The results suggest that joint position sense error scores were effected by position, angle and exercise state. There was little difference between the neoprene sleeve and KT in comparison to no tape. The population studied were healthy overhead athletes and the results may indicate that those with perceived acceptable joint position acuity may not benefit from the application of supportive devices, indeed, these may be detrimental to performance both in pre and post exercise states. The lower IR error scores produced when the neoprene sleeve was applied at the diagonal position and the lower mid-range scores at the 9090 position may be attributed to the compressive effect of the sleeve [30] and the effect on muscle and skin receptors [31]. A greater stimulus of the GTO and mus-

353 cle spindles at the mid-range position has previously
354 been activated through stimulation of underlying muscle
355 tissue from skin receptors being initially stimulated [32]. Nonetheless, this does not explain the lower
356 error scores only at mid-range and IR range and not
357 seen at the modified neutral position.

358 With the type of JPS being assessed (ARPP) mechanoreceptors involved more in active relocation where
359 the participant actively guides the arm into position,
360 may be affected more than if the relocation was done
361 passively. Passive repositioning [33] may cause a de-
362 creased response after exercise from end of range
363 structures such as the joint mechanoreceptors. Stretch
364 may be more pertinent than compression with pas-
365 sive movements. To provide greater mechanistic un-
366 derstanding of the types of supportive device used in
367 the present study, further research might consider the
368 experimental applications provided by electromyogra-
369 phy and medical imaging. The non-significant change
370 in JPS over the duration of the exercise protocol might
371 also be attributed to conflicting mechanisms associated
372 with potentiation and fatigue. No warm-up was used
373 as this would affect the mechanoreceptors within the
374 GHJ and surrounding rotator cuff musculature when
375 JPS was being [16]. The potentiating influence of a
376 warm-up on JPS [34] might be evident over the initial
377 stages of the exercise protocol, masking the expected
378 exercise-effect [33,35] in the latter stages. The popula-
379 tion studied in the current research were overhead
380 sports participants who repeat rotational GHJ move-
381 ments many times during the course of play. This type
382 of repetition may have caused adaptation to sports spe-
383 cific demands of play thus creating an increase in stim-
384 ulus through compression and stretch [3].

385 5. Clinical and practical implications

386 Clinically, JPS acuity in the gleno-humeral joint
387 may be sufficient without the addition of supportive
388 devices. The current study utilised participants across
389 a range of sports, and it is acknowledged that whilst
390 movement patterns are similar between sports [36]
391 muscle fibre recruitment and fatigue resistance may be
392 different between sports such as tennis and volleyball
393 (speed over power). The participants used were injury
394 free, and as such the use of the supportive devices is di-
395 rected toward injury prevention rather than injury man-
396 agement. When examining knee proprioception, par-
397 ticipants with lower JPS acuity responded more ef-
398 fectively to KT than those with perceived good acu-
399 400

401 ity [37]. As such, the results of the present study cannot
402 be generalised to injured athletes, where an interven-
403 tion could potentially be more effective. The 30 repe-
404 tition protocol was sufficient to recreate the demands
405 of overhead sports but did not induce a fatigue effect.
406 Therefore, the results cannot be generalised to absolute
407 fatigue conditions.

408 6. Conclusion

409 Further study is required on the functional kinesiol-
410 ogy taping applied in this study as there is limited re-
411 search supporting or refuting its use in sport. Neoprene
412 shoulder sleeves are a less expensive and more user
413 friendly support intervention, and as such, the minimal
414 difference between KT, neoprene and no support may
415 not warrant changing training or playing habits sig-
416 nificantly in healthy overhead sports athletes. Indeed,
417 KT impaired function at mid-range post-exercise and
418 EOR pre-exercise at the 9090 position suggesting that
419 healthy, uninjured overhead athletes may not need to
420 consider taping or supportive device. The 9090 posi-
421 tion is one in which several overhead sports require
422 power and position sense together. Therefore, future
423 research may consider the application in a group of
424 subjects who have poor joint position acuity. Further-
425 more, the effects of fatigue have been more widely in-
426 vestigated in the GHJ [33,38,39] and it may be perti-
427 nent to examine supportive devices under these condi-
428 tions.

429 Conflict of interest

430 There are no financial or other potential conflicts of
431 interest associated with this research.

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