

Ocular drug delivery from contact lenses: mimetizing the hydrodynamic conditions of the eye

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Introduction

Results

- Currently, most *in vitro* drug release studies for ophthalmic applications are carried out in static sink conditions. Although this procedure is simple and useful to make comparative studies, it does not describe adequately the drug
- \Rightarrow MFC inner chamber with **volume of 45 µL**.
- \Rightarrow Considering a flow rate of 3µL/min, the fluid flows in the cell

uniformly (Figure 2). Symmetric and very regular paths are followed from the inlet pipe to the eight exiting pipes.



release kinetics in the eye, considering the small tear volume and flow rates found *in vivo*.

In a normal situation, the human eye contains a tear volume that ranges from 6.2 to 30.0 μ L [1] and the tear flow rate assumes values between 0.9 and 2.1 μ L/min [2]. The use of contact lenses increases the tear turnover to values of the order 1.4-4.3 μ L/min [2].

In order to predict in a more reliable way the drug release kinetics in the eye, it is crucial to develop microfluidic models that mimic, as close as possible, the hydrodynamic conditions of the eye.

Drug eluting contact lens

Objectives

- Design and validation of a microfluidic cell to mimic the continuous, volumetric flow rate of tear fluid and its low volume;
- ii) Comparison of drug release profiles of anti-inflammatory, diclofenac (DCF), from a soft contact lens material obtained in static sink and in dynamic conditions;
- iii) Estimation of the drug released in vivo efficacy.

Possibility of numerically simulate other inner chamber

volumes and flow rates.

Different release kinetics for the same drug/hydrogel pair.



Figure 3. DCF fractional cumulative mass release



Figure 2. Representation of the fluid paths inside the microfluidic cell

Methods

① Microfluidic cell (MFC)

A MFC of poly(methylmethacrylate) with a cylindrical inner chamber of 45 μ L was designed and fabricated.



The flow inside the microfluidic cell was modeled through the numerical solution of the Navier-Stokes and continuity equations using the Star-CCM+ simulation package.

② Drug release experiments

- *Static*: Diclofenac loaded 2-hydroxyethyl methacrylate (PHEMA) samples were immersed in 4 mL of PBS solution in closed vessels, at 36 °C, under stirring (180 rpm). At predetermined time intervals, 800 µl aliquots of the supernatant were collected and replaced by the same volume of fresh PBS solution.

From the release results in dynamic conditions it is possible to estimate the concentration of DCF released from PHEMA hydrogels in a volume equivalent to the tear film.
Considering that....

The recommend posology for **DCF is 8.5 µg/day** (5 x 1 drop).



 \rightarrow Results suggest the studied drug/hydrogel pair shall be effective during \approx 5 days.

Conclusions

- *Dynamic*: drug release experiments in the microfluidic cell were performed at 36° C and a continuous flow of PBS of 3 µL/min.

③ In vivo efficacy

The *in vivo* efficacy of anti-inflammatory released in dynamic conditions was estimated through comparison to the daily dose delivered by topical application.

- A microfluidic cell was successfully fabricated to approximate in vitro ocular drug release experiments to the eye tear film in vivo hydrodynamic conditions.
- Experimental results shown that DCF release kinetics is affected by the release conditions; dynamic conditions developed in this study are expected to be closer to the *in vivo* conditions when compared with common sink conditions.
- ✓ Results suggest the studied drug/hydrogel pair shall be effective during \approx 5 days.

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