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1 **Glassy carbon electrode modified with**
2 **7,7,8,8-tetracyanoquinodimethane and graphene oxide triggered**
3 **a synergistic effect: low-potential amperometric detection of**
4 **reduced glutathione**

5
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23 **Abstract**

24 A sensitive electrochemical sensor based on the synergistic effect
25 of 7,7,8,8-tetracyanoquinodimethane (TCNQ) and graphene oxide (GO) for
26 low-potential amperometric detection of reduced glutathione (GSH) in pH 7.2
27 phosphate buffer solution (PBS) has been reported. This is the first time that the
28 combination of GO and TCNQ have been successfully employed to construct an
29 electrochemical sensor for the detection of glutathione. The surface of the glassy
30 carbon electrode (GCE) was modified by a drop casting using TCNQ and GO. Cyclic
31 voltammetric measurements showed that TCNQ and GO triggered a synergistic effect
32 and exhibited an unexpected electrocatalytic activity towards GSH oxidation,
33 compared to GCE modified with only GO, TCNQ or TCNQ/electrochemically
34 reduced GO. Three oxidation waves for GSH were found at -0.05, 0.1 and 0.5 V,
35 respectively. Amperometric techniques were employed to detect GSH sensitively
36 using a GCE modified with TCNQ/GO at -0.05 V. The electrochemical sensor showed
37 a wide linear range from 0.25 to 124.3 μM and 124.3 μM to 1.67 mM with a limit of
38 detection of 0.15 μM . The electroanalytical sensor was successfully applied towards
39 the detection of GSH in an eye drop solution.

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43 **Keywords:** Electrochemical sensor; 7,7,8,8-tetracyanoquinodimethane (TCNQ);

44 Graphene oxide; reduced glutathione

45 **1. Introduction**

46 Glutathione (GSH, γ -glutamyl-L-cysteinyl-glycine), the most abundant tripeptide
47 thiol in eukaryotic and mammalian cells, performs a high number of physiological
48 roles including protection against nitrosative and oxidative stress (Areias et al., 2016).
49 GSH has been found in both mammalian and plant tissue over the concentration range
50 from 1 to 10 mM (Valero-Ruiz et al., 2016), and its levels are an indicator of various
51 diseases such as HIV, cancer, Alzheimer's disease, and diabetes (Harfield et al., 2012).
52 Therefore, developing sensitive and selective methods for GSH detection has attracted
53 a lot of attention for medical diagnosis.

54 Electrochemical determination of GSH is gaining momentum among other
55 analytical methods due to its simplicity, high sensitivity, low cost and fast analysis
56 (Harfield et al., 2012). The electrochemical oxidation of GSH at bare GCE requires
57 high overpotential. As a result, various electrocatalysts have been utilized either
58 modified on the electrode surface or placed in solution as a mediator to decrease the
59 overpotential of GSH. The reported modification materials and mediators found in
60 literature are thoroughly reviewed in **Table 1**. The electrochemical techniques most
61 commonly employed are differential pulse voltammetry (DPV) and amperometric
62 detection. However, a key problem with the analysis of GSH utilizing DPV is that the
63 voltammetric peak resulting from the electrochemical oxidation of GSH may overlap
64 with the electroactive coexisting species such as ascorbic acid (AA), uric acid (UA),
65 dopamine (DA) and cysteine (CYS). When amperometric detection is employed, the
66 oxidation potential of GSH is required to be much lower than these coexisting species

67 to prevent their interference.

68 7,7,8,8-Tetracyanoquinodimethane (TCNQ) is an effective electron transfer
69 mediator due to the presence of four cyano groups and π conjugation bonds, which
70 can form organic charge-transfer complexes and ion-radical salts such as K (TCNQ)
71 and Na (TCNQ) (Zamfir, et al., 2013; Paczosa-Bator et al., 2015). In addition, TCNQ
72 has attracted considerable interest in the fabrication of electrochemical sensors for
73 carbamate drugs (Zamfir, et al., 2013), K^+ (Paczosa-Bator et al., 2015),
74 acetylcholinesterase inhibitors (Rotariu et al., 2012) and ascorbic acid (Murthy and
75 Anita, 1994). GO is a highly oxidized derivative of graphene, which possesses a large
76 amount of oxygen functional groups such as hydroxyl, epoxide, carboxyl, and
77 carbonyl groups (Zhu et al., 2010). The oxygen functional groups can increase the
78 charge transfer resistance, but play an essential role in the electrocatalytic oxidation of
79 some small molecules including AA (Uhma et al., 2011), DA (Xiong and Jin, 2011),
80 dihydroxybenzene isomers, and L-methionine (Zhang et al., 2014). To the best of our
81 knowledge, we have reported for the first time the fabrication of an electrochemical
82 sensor using GCE modified with TCNQ and GO for the detection of GSH. In addition,
83 the modified GCE sensor with TCNQ/GO showed an unexpected electrocatalytic
84 activity towards GSH oxidation at a low potential compared to electrodes modified
85 with only GO, TCNQ and TCNQ/electrochemically reduced GO (rGO). Furthermore,
86 TCNQ and GO also showed a synergistic effect on the electrocatalytic oxidation of
87 GSH with the oxidation overpotential decreasing greatly. Finally, based on the
88 TCNQ/GO/GCE electrode, sensitive amperometric determination of GSH was

89 successfully achieved.

90 **2. Experimental**

91 *2.1. Chemicals and solutions*

92 TCNQ, GSH, CYS, DA, AA, and UA were purchased from Sigma-Aldrich. GO
93 was acquired from Nanjing XFNano Materials Tech Co., Ltd. All other chemicals
94 were of analytical reagent grade, and doubly distilled water was used to prepare all
95 the solutions. 0.1 M phosphate buffer solution (PBS, pH 7.2) was employed as the
96 background electrolyte.

97 *2.2. Apparatus*

98 Scanning electron microscopy (SEM) images were obtained with a Hitachi SU8010
99 (Japan) scanning electron microscope. A CHI 842C electrochemical workstation
100 (Austin, TX, USA) was used to perform all the electrochemical experiments with a
101 conventional three-electrode system, which included a GCE as the working electrode,
102 a platinum coil as an auxiliary electrode, and an Ag/AgCl (saturated KCl) as the
103 reference electrode.

104 *2.3. Electrode preparation and modification*

105 Prior to each experiment, GCE with a geometric area of 0.07 cm² was polished with
106 1, 0.3, and 0.05 μm alumina paste to a mirror finish, subsequently, the electrode was
107 rinsed with water, and finally an ultrasonic treatment in water and ethanol was applied,
108 respectively. GO modified GCE was prepared by dropping a 5 μL of 1 mg/mL GO
109 aqueous solution on the cleaned electrode and kept to dry at room temperature. Due to
110 the low surface tension of acetone solution, TCNQ modified electrodes were prepared

111 by a drop casting method via solvent evaporation (Nafady et al., 2006). Briefly, the
112 GO modified GCE or bare GCE was dipped in a 10 mM fresh solution of TCNQ in
113 acetone for one minute and then kept in air to dry face down. To fabricate rGO
114 modified GCE, firstly, the GO/GCE was electrochemically reduced in pH 4.0 acetate
115 buffer by amperometric method for 500 s at -1.2 V, then the electrode was modified
116 with TCNQ using the similar method as TCNQ/GO/GCE. The electroactive surface
117 areas of these electrodes could be calculated by the Randles–Sevcik equation
118 (Supplementary information).

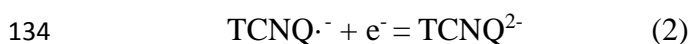
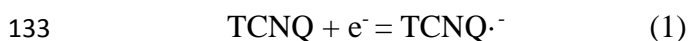
119 **3. Results and discussion**

120 *3.1. SEM Characterization of TCNQ modified electrodes*

121 The electrode surface characterization was analyzed by SEM. **Fig. 1** shows the
122 SEM images of TCNQ modified electrode by a drop casting method. As shown in **Fig.**
123 **1D, E, and F**, irregular TCNQ plates erected on the surface of GCE without GO due
124 to gravity. However, in the presence of GO, rhombic TCNQ plates structures were
125 formed and lay on the surface of GO/GCE (**Fig. 1A, B, and C**), those structures
126 formation were attributed to the π - π interaction between GO and TCNQ. The size of
127 the formed TCNQ crystals were found to be over the range from 5 to 30 μm .

128 *3.2. Electrochemical properties of TCNQ modified electrodes*

129 Next, the electrochemical properties of TCNQ modified electrodes were
130 investigated. TCNQ exhibits two electrochemically reversible one-electron waves,
131 which were associated to the generation of $\text{TCNQ}^{\cdot-}$ and TCNQ^{2-} by using the
132 following equations:



135 **Fig. 2A Inset** shows the CVs of TCNQ immobilized on GCE by a drop casting
136 method in 0.1 M pH 7.2 PBS. It can be seen that a pair of typical redox peaks
137 appeared at 0.5 and -0.15 V, respectively. Surface-immobilized TCNQ also undergoes
138 a remarkable ‘inert zone’ in which no faradaic reaction yields, suggesting a typical
139 solid-solid phase transformation in terms of nucleation and growth (Gómez and
140 Rodríguez-Amaro, 2006). Further, with the increasing cycle, the voltammetric peak
141 heights decay due to the dissolution of TCNQ into the solution (Bond et al., 1998).
142 The results obtained are in good agreement with previous reports (Gómez and
143 Rodríguez-Amaro, 2006; Bond et al., 1998). The electrochemical behaviour of
144 immobilized TCNQ on the surface of GO or rGO was also studied, as shown in **Fig.**
145 **2B and C Inset**. Both CVs differ considerably from that obtained at TCNQ/GCE. The
146 electrochemical processes at the GCE modified with TCNQ/GO showed three pairs of
147 redox waves (**Fig. 2B Inset**). According to Eqs. (1) and (2), the two corresponding
148 oxidation peak potentials were observed at -0.05 and 0.36 V, and the corresponding
149 reduction waves appeared at -0.15 and 0.10 V, respectively. The peak 3 showed in Fig.
150 2B Inset is due to the electrochemical behavior of the oxygen functional species on
151 GO, which can also be found in **Fig. 2D** (Yuan et al., 2013c; Ndamanisha et al., 2009).
152 When the GCE was modified with TCNQ/rGO, two electrochemical processes were
153 identified and the corresponding oxidation and reduction waves changed to -0.17 and
154 0.13 V, and -0.32 and 0.05 V, respectively. In addition, the two electrochemical

155 processes became much more reversible than that obtained at TCNQ/GO/GCE. This
156 was attributed to the fast electron transfer rate of rGO. The results also showed that
157 the dissolution of TCNQ in solution decreased at the TCNQ/GO/GCE due to the π - π
158 interaction between TCNQ and GO.

159 *3.3. Electrocatalytic oxidation of GSH based on TCNQ modified electrodes*

160 The electrochemical oxidation of GSH using various modified electrode surfaces in
161 0.1 M pH 7.2 PBS by cyclic voltammogram (CV) at a scan rate of 0.1 V/s was also
162 investigated, as shown in **Fig. 2**. When the GCE was modified with GO an oxidation
163 peak was observed at 0.22 V due to the GSH oxidation reaction to GSSG (**Fig. 2D**).
164 This is caused by the electrocatalytic activity of oxygen functional species present on
165 GO towards the oxidation of GSH. The oxidation peak of GSH appeared at 0.7 V
166 when the GCE was modified with TCNQ (**Fig. 2A**). Upon addition of GSH to the
167 solution, three oxidation waves emerged at the TCNQ/GO/GCE with the
168 corresponding oxidation peak potentials of -0.05, 0.1, and 0.5 V, respectively shown
169 in **Fig. 2B**. These three enhanced oxidation waves were attributed to the
170 electrocatalysis of TCNQ \cdot^- , oxygen functional groups, and TCNQ $^{2-}$ with the oxidation
171 of GSH. In addition, the catalytic current at 0.1 V is much higher than that obtained at
172 GO/GCE (**Fig. 2D**) with a much lower oxidation potential. The introduction of TCNQ
173 enhanced the electrocatalytic activity of oxygen functional groups present on GO.
174 However, there was no electrocatalytic current observed until 0.35 V when the GCE
175 surface was modified with TCNQ/rGO, even though rGO has high electrical
176 conductivity and fast electron transfer rate. The comparison results showed that

177 TCNQ and GO had a synergistic effect, which exhibited unexpected electrocatalytic
178 activity towards the oxidation of GSH. The electrocatalytic mechanism proposed is
179 shown by equations 3 and 4:



182 The electrochemical detection of GSH in physiological samples had presented a major
183 obstacle due to the presence of electroactive species such as AA, DA, UA, and CYS
184 which often coexists with GSH. The ultra-low overpotential of GSH shown at the
185 TCNQ/GO/GCE may overcome the interferences from these interfering species. Next,
186 the selectivity of the proposed electrochemical sensor (modified GCE with TCNQ/GO)
187 was investigated by CV. **Fig. 3** shows the CVs of TCNQ/GO/GCE in the absence
188 (dotted line) and presence (solid line) of 0.2 mM AA (A), 5 mM CYS (B), 0.2 mM
189 DA (C), and 0.2 mM UA (D) in 0.1 M 7.2 pH PBS at a scan rate of 0.1 V/s. The
190 oxidation peak for UA was found to be at 0.38 V, which is much higher than the first
191 and second oxidation wave of GSH because of the ultra-low overpotential of GSH at
192 the TCNQ/GO/GCE. Two pairs of redox peaks were observed for DA. Further
193 experiments indicated that the first oxidation process for DA at 0.23 V is essential to
194 form the second oxidation. Therefore, the oxidation potential of DA is also higher
195 than the first two oxidation waves of GSH. AA and CYS had a similar electrocatalytic
196 oxidation as GSH, but the electrocatalytic current is lower than that of GSH. It was
197 reported that the concentration of GSH in the cells can be up to 10 mM (Mesiter,
198 1988), while the basal level of AA in the extracellular fluid of the central nervous

199 system, is approximately 0.1 μM , and the physiological level of AA is about 0.1 mM
200 (El-Said et al., 2010). Considering the far higher level of GSH compared to AA in
201 physiological samples and high sensitivity for GSH detection of this method, the
202 influence of AA may be decreased and even ignored by diluting the sample. In
203 addition, AA can be removed from the sample by adding ascorbate oxidase (Silva, et
204 al. 2013) before analysis. Therefore, it is possible to apply the method for the detection
205 of GSH in biological fluids.

206 *3.4. Amperometric sensing of GSH based on a GCE modified with TCNQ/GO*

207 Next, we investigate the electrochemical detection of GSH on a GCE modified with
208 TCNQ/GO using amperometric techniques. **Fig. 4** shows the amperometric response
209 of TCNQ/GO/GCE to the successive additions of GSH in a stirring pH 7.2 PBS
210 solution. Due to the high electrocatalytic activity of the TCNQ/GO/GCE towards the
211 GSH oxidation, much lower potentials (-0.05 or 0.1 V) were used. For -0.05 V and 0.1
212 V amperometric sensing, the measured current increased with the GSH concentrations,
213 and a linear response was observed over a concentration range of 0.25-124.3 μM
214 ($R^2=0.9928$, $I/\mu\text{A}=0.029+2.09 \text{ C/mM}$) and 124.3 μM -1.67 mM ($R^2 =0.9989$,
215 $I/\mu\text{A}=0.37+0.35 \text{ C/mM}$), and 0.25-174.3 μM ($R^2=0.9956$, $I/\mu\text{A}=0.37+0.34 \text{ C/mM}$)
216 and 174.3 μM -1.18 mM, ($R^2=0.9972$, $I/\mu\text{A}=0.50+0.78 \text{ C/mM}$), respectively. The limit
217 of detection was calculated to be 0.15 μM and 0.10 μM (S/N=3), respectively. The
218 analytical performance of GSH with the GCE modified with TCNQ/GO reported in
219 this work and other modified materials and mediators found in literature are
220 thoroughly reviewed in **Table 1**. The oxidation potential of GSH at the

221 TCNQ/GO/GCE (-0.05 V) is much lower than those other materials or mediators but
222 higher than catechol (-0.16 V) illustrated in Table 1. The TCNQ/GO/GCE also
223 displayed a wide linear range for the detection of GSH compared to other electrodes.
224 It should be noted that, with the addition of high GSH concentrations, the
225 amperometric responses decreased with time, suggesting that further GSH oxidation
226 was greatly hindered. This may be caused by the passivation of electrode due to the
227 binding of the sulfur moiety to the electrode surface generated by the oxidation of
228 GSH because the concentration of GSH reached a high level in the detection cell with
229 the successive additions of GSH (Harfield, et al., 2012). The similar phenomenon was
230 also reported in the previous literature (Yuan, et al., 2013c).

231 In order to assess the anti-interference performance of TCNQ/GO/GCE, the
232 interference effect was also examined at the TCNQ/GO/GCE with 25 μ M GSH in the
233 presence of 4 μ M AA, 4 μ M CYS, 25 μ M DA, and 25 μ M UA by using amperometric
234 technique (Supplementary information). The results showed that the presence of these
235 electroactive species with the added concentration did not interfere with the
236 determination of GSH due to the low detection potential at which was applied. This is
237 also in agreement with the interference test by CV method in section 3.3.

238 The stability of the electrochemical sensor was investigated by a continuous
239 operation and successive performance. After 2300 s of continuous operation of 25 μ M
240 GSH, 98% of its initial value was retained (Supplementary information). After being
241 stored in air for one week and two weeks, respectively, the electrode had a 12% and
242 18% decrease in current response (Supplementary information). In addition, the RSD

243 was 4.7% for ten successive analysis of 25 μ M GSH using the same electrode. This
244 excellent stability of the presented sensor was due to the π - π interaction between GO
245 and TCNQ.

246 *3.5. Analysis of GSH in real samples*

247 The applicability of the sensor was further evaluated by the analysis of GSH in an
248 eye drop solution (purchased from Wuhan Wujing Medicine Co., Ltd, China). 2.0 μ L
249 sample without pretreatment was directly added to a stirring PBS solution at pH 7.2
250 (8.0 mL) for amperometric detection. The GSH concentration in the eye drops
251 solution was found to be 60.8 mM, which is in agreement with the labeled value (65.0
252 mM). The recoveries were also estimated by adding GSH standards to the above
253 solution. The results showed that the sensor gave the acceptable recoveries over the
254 range between 94.7% and 106.1%.

255 **4. Conclusions**

256 A simple TCNQ and GO modified GCE was prepared and used for the
257 electrocatalytic oxidation of GSH at physiological pH. The results showed that TCNQ
258 and GO triggered an outstanding synergistic effect which enhanced the
259 electrocatalytic activity towards the oxidation of GSH. As a result, the oxidation
260 potential of GSH decreased to an ultra-low value (-0.05 V). Based on the TCNQ and
261 GO modified GCE, low potential amperometric detection of GSH was achieved with
262 wide linear range and low detection limit. The electrochemical protocol was
263 successfully applied towards the detection of GSH in a real sample (eye drop solution)
264 with a recovery from 94.7 to 106.1%. As an effective electrocatalysts, the TCNQ and

265 GO opens a new potential application in biosensing.

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375 **Figure captions**

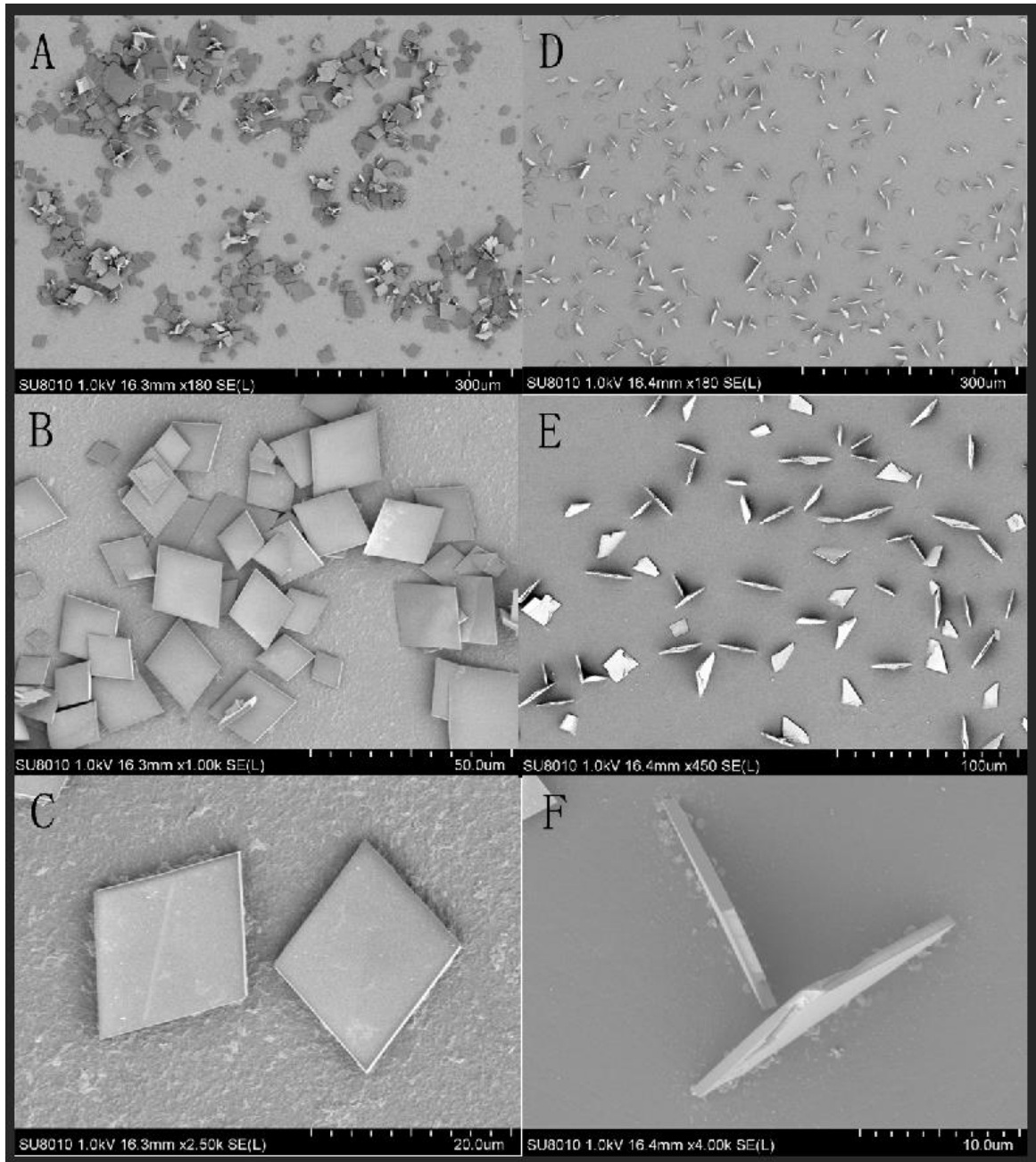
376 Fig. 1 SEM images of TCNQ/GO/GCE (A, B, and C) and TCNQ/GCE (D, E, and F)
377 at different magnifications by a drop casting method.

378 Fig. 2 CVs of TCNQ/GCE (A), TCNQ/GO/GCE (B), TCNQ/rGO/GCE (C), and
379 GO/GCE (D) in the presence (solid line, first cycle) and absence (dotted line, steady
380 state cycle) of 5 mM GSH in 0.1 M 7.2 pH PBS at a scan rate of 0.1 V/s. *Inset* (A, B,
381 C) first twenty cycles for corresponding electrodes.

382 Fig.3 CVs of TCNQ/GO/GCE in the absence (dotted line) and presence (solid line) of
383 0.2 mM AA (A), 5 mM CYS (B), 0.2 mM DA (C), and 0.2 mM UA (D) in 0.1 M 7.2
384 pH PBS at a scan rate of 0.1 V/s. *Inset* is the CV of 5 mM GSH in the same condition.

385 Fig. 4 Amperometric detection of GSH by successive additions of GSH into a stirring
386 pH 7.2 PBS solution at the TCNQ/GO/GCE at -0.05 (curve 1) and 0.1 V (curve 2).
387 *Inset* (A): The corresponding calibration plot; (B): amplified response of the
388 TCNQ/GO/GCE to lower concentration of GSH.

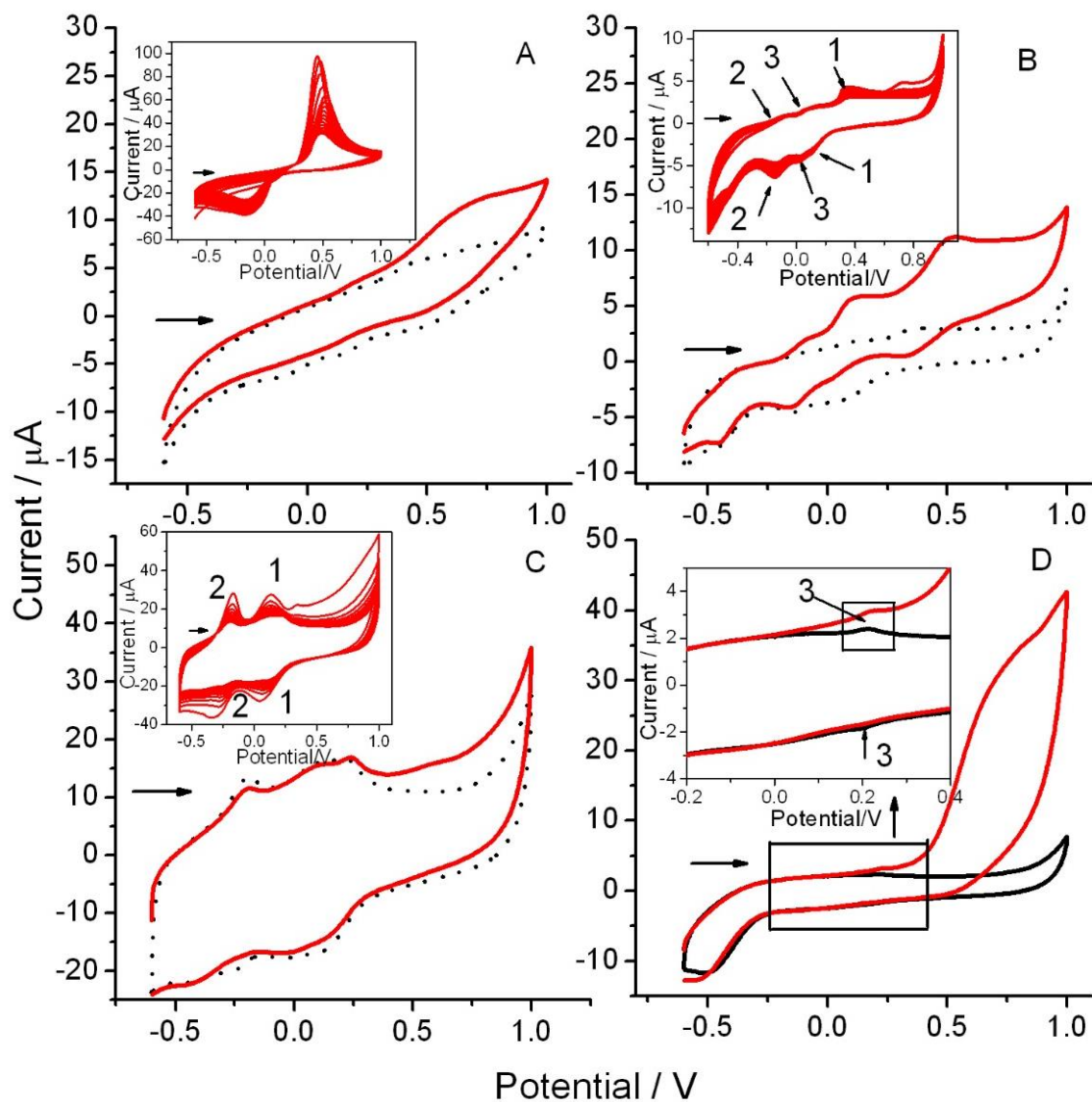
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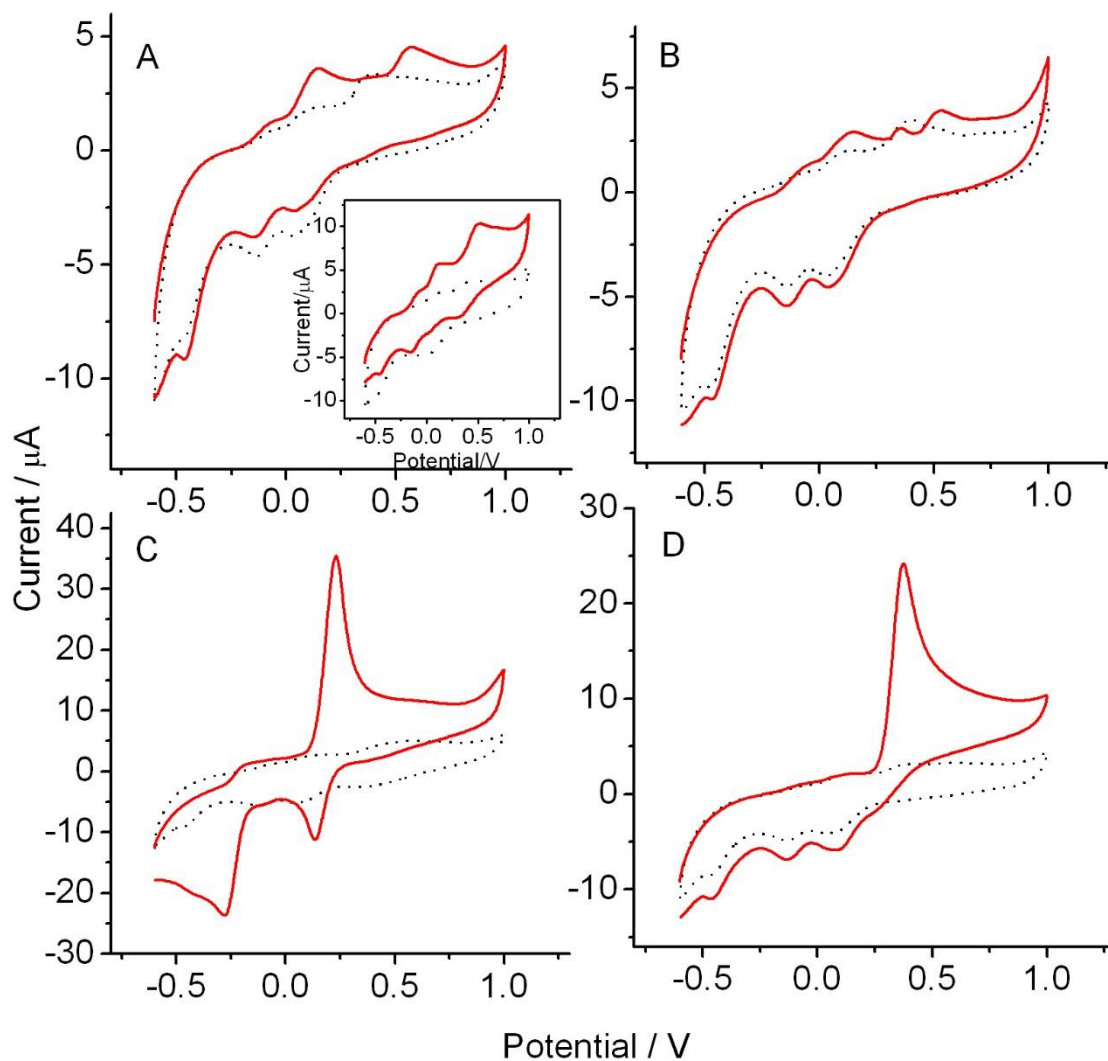
391 Figure 1. SEM images of TCNQ/GO/GCE (A, B, and C) and TCNQ/GCE (D, E, and F) at
 392 different magnifications by a drop casting method.

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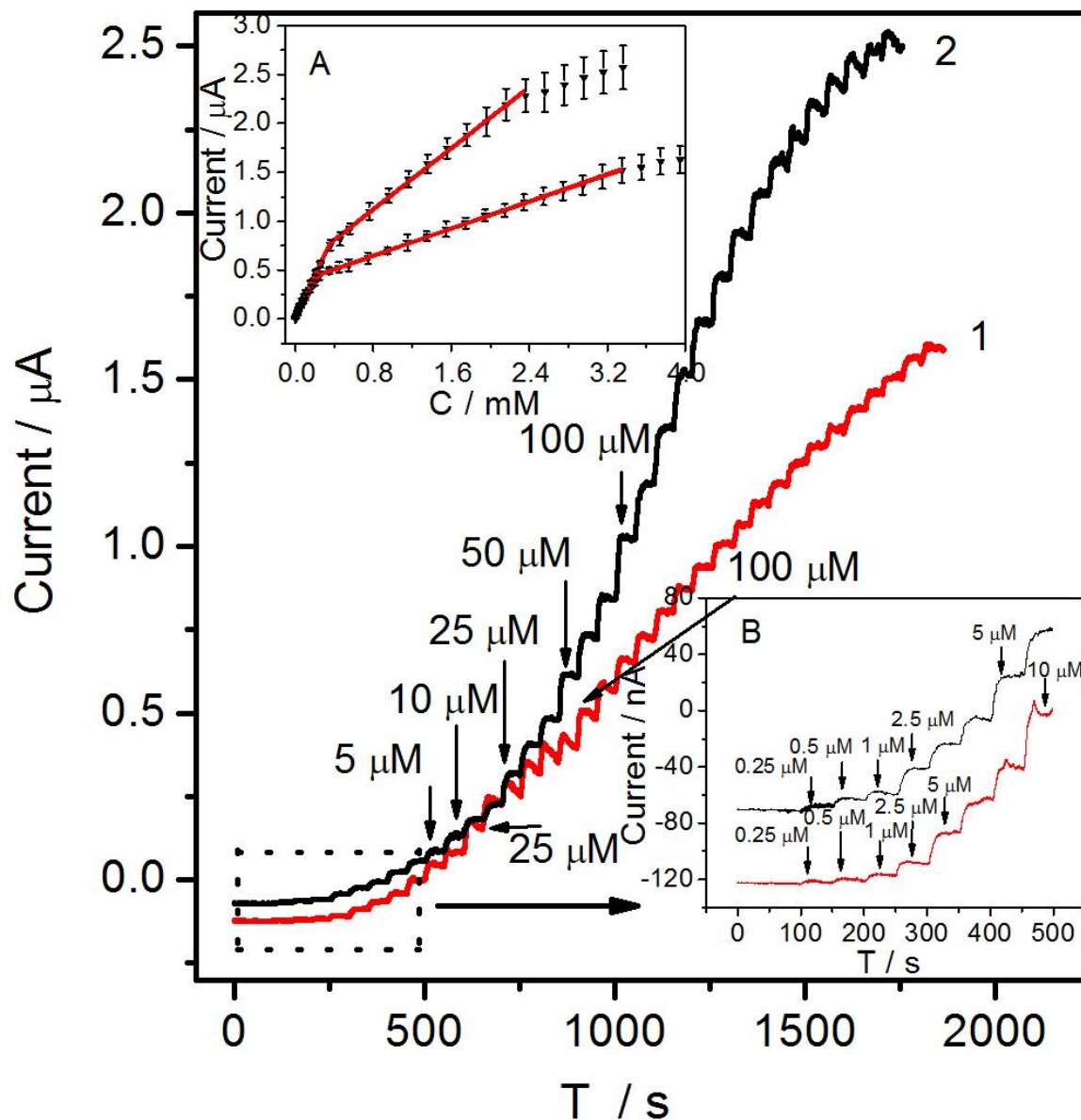
395 Figure 2. CVs of TCNQ/GCE (A), TCNQ/GO/GCE (B), TCNQ/rGO/GCE (C), and GO/GCE (D)
 396 in the presence (solid line, first cycle) and absence (dotted line, steady state cycle) of 5 mM GSH
 397 in 0.1 M 7.2 pH PBS at a scan rate of 0.1 V/s. *Inset* (A, B, C) first twenty cycles for corresponding
 398 electrodes.



399

400 Figure 3. CVs of TCNQ/GO/GCE in the absence (dotted line) and presence (solid line) of 0.2 mM
 401 AA (A), 5 mM CYS (B), 0.2 mM DA (C), and 0.2 mM UA (D) in 0.1 M 7.2 pH PBS at a scan rate
 402 of 0.1 V/s. *Inset* is the CV of 5 mM GSH in the same condition.

403



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405 Figure 4. Amperometric detection of GSH by successive additions of GSH into a stirring pH 7.2
 406 PBS solution at the TCNQ/GO/GCE at -0.05 (curve 1) and 0.1 V (curve 2). *Inset (A)*: The
 407 corresponding calibration plot; (B): amplified response of the TCNQ/GO/GCE to lower
 408 concentration of GSH.

409

410 **Table 1.** Analytical performances for GSH detection based on various modification

411 materials and mediators by different electrochemical methods.

Materials or mediators	Method	pH	OP/V	Linear range	LOD	References
NiO ^{MI}	DPV	7.2	0.6 ^a	0.2 mM ~ 6.0 mM	0.2 mM	Chee et al., 2011

NiO microflower ^{MI}	AMP	5.0	0.4 ^a	10 μ M ~ 0.62 μ M; 0.6 mM ~ 3.6 mM	10 μ M	Pang et al., 2012
Electrodeposited NiO ^{MI}	AMP	5.0	0.4 ^a	12.5 μ M ~ 2.3 mM	2 μ M	Yuan et al., 2013b
NiO _x /Cu ₂ O ^{MI}	AMP	7.0	0.3 ^a	2 μ M ~ 1.3 mM	0.3 μ M	Yuan et al., 2013a
Poly-m-aminophenol ^{MI}	AMP	4.0	0.5 ^a	0.1 μ M ~ 5 μ M	0.095 μ M	Oztekin et al., 2011
CoPcTF ^{MI}	AMP	7.4	0.18 ^a	1 μ M ~ 818 μ M	0.2 μ M	Wang et al., 2011
CNT-SPE ^{MI}	CV	7.0	0.4 ^b	10 μ M ~ 100 μ M	3 μ M	Lee et al., 2015
MPT-HP- β -CD ^{MI}	AMP	7.0	0.58 ^a	1 μ M ~ 580 μ M	0.87 μ M	Li et al., 2015
Pd-IrO ₂ ^{MI}	AMP-CE	3.0	0.85 ^a	10 μ M ~ 800 μ M	2 μ M	Xu et al., 2002
Electrochemical modified GO ^{MI}	AMP	5.0	0.23 ^a	5 μ M ~ 875 μ M; 875 μ M ~ 4.08 mM	5 μ M	Yuan et al., 2013
Co-based metal-organic coordination polymer ^{MI}	AMP	7.2	0.4 ^a	2.5 μ M ~ 0.95 mM	2.5 μ M	Yuan et al., 2014
NiHCF-gold ^{MI}	LSV	4.0	0.65 ^a	1 μ M ~ 1.4 mM	0.5 μ M	Pandey and Pandey, 2012
Ag/CNT//polyaniline ^{MI}	CV	6.0	0.4 ^a	0.3 μ M ~ 3.5 mM	0.30 μ M	Narang et al., 2012
Manganese dioxide ^{MI}	AMP	7.5	0.45 ^a	0.5 μ M ~ 10 μ M	0.2 μ M	Eremenko et al., 2012
Cobalt phthalocyanine ^{MI}	CV	7.4	0.1 ^c	0.08 mM ~ 1 mM	~	Pereira-Rodrig ues et al., 2006
Mesoporous carbon/CoO ^{MI}	DPV	4.0	0.25 ^a	4 μ M ~ 28 μ M	~	Hou et al., 2009
Mesoporous carbon ^{MI}	AMP	7.2	0.15 ^a	0.28 mM ~ 3 mM	~	Ndamanisha et

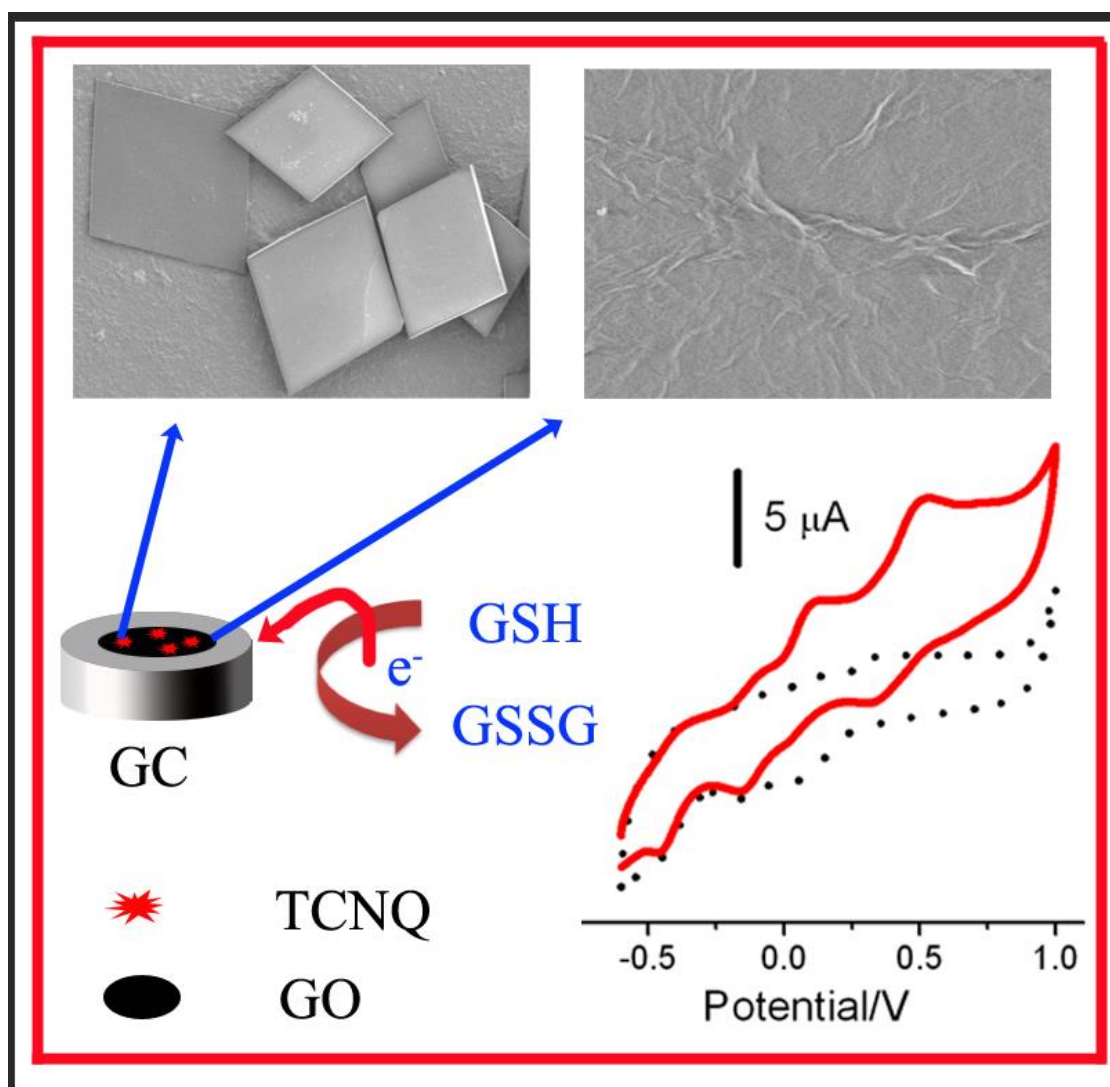
						al., 2009
Acetaminophen ^{MI}	DPV	7.0	0.32 ^c	100 μ M ~ 2.7 mM	0.37 μ M	Chatraei and Zare, 2011
NiHCF/CTAB/AuNPs ^{MI}	DPV	6.5	0.45 ^a	0.2 μ M ~ 1 μ M;	0.08 μ M	He et al, 2013
Nanoscale Copper Hydroxide ^{MI}	CV	7.2	0.15 ^a	1 μ M ~ 50 μ M; 0.1 mM ~ 1.8 mM	0.03 μ M	Safavi et al., 2009
Nano-TiO ₂ /ferrocene carboxylic acid ^{MI}	DPV	7.0	0.75 ^a	0.1 μ M ~ 12 μ M	0.098 μ M	Raof et al., 2009
NHPDA/FePt/CNT ^{MI}	CV	7.0	0.41 ^a	4 nM ~ 340 μ M	1 nM	Karimi-Maleh et al., 2014
Ethynylferrocene–NiO/MWCNT ^{MI}	CV	6.0	0.48 ^a	0.01 μ M ~ 200 μ M	6 nM	Shahmiria et al., 2013
benzamide derivative-MWCNT ^{MI}	SWV	7.0	0.29 ^a	0.09 μ M ~ 300 μ M	0.05 μ M	Ensafia et al., 2013
CoPc immobilized on nitrogen-doped graphene ^{MI}	AMP	13	-0.05 ^c	1 μ M ~ 8 mM	1 μ M	Xu et al., 2015
Au nanoparticles ^{MI}	DPV	7.4	0.33 ^a	20 μ M ~ 200 μ M	0.082 μ M	Atta et al., 2012
CNT–ionic liquid–epinephrine ^{MI}	DPV	7.0	0.28 ^c	0.1 μ M ~ 30 μ M	0.04 μ M	Liu et al., 2015
FeT4MpyP-MWCNT ^{MI}	~	7.4	0 ^a	5 μ M ~ 5 mM	0.5 μ M	Luz et al., 2008
FTO ^{MI}	LSV	4.4	0.27 ^c	~	~	Mu and Yang, 2016
Pt-NiCo ^{MI}	AMP	7.4	0 ^a	0.1 μ M ~ 645 μ M	0.02 μ M	Zhang et al., 2010
TCNQ/GO/GCE ^{MI}	AMP	7.2	-0.05 ^a	0.25 μ M ~ 124.3 μ M ¹	0.15 μ M ¹	This work

			0.1 ^a 0.5 ^a	124.3 μM~1.67 mM ¹ 0.25 μM ~ 174.3 μM ² 174.3 μM-1.18 mM ²	0.1 μM ²	
Γ/I_2^{Mr}	CV	~	0.95 ^c	19.9 μM ~ 629.4 μM;	21.28 μM	Valero-Ruiz et al., 2016
4-methylesculetin–boric acid ^{Mr}	CV	8.0	0.22 ^a	~	~	Salehzadeh and Nematollahi, 2013
Pyrroloquinoline Quinone ^{Mr}	AMP	3.5	0.50 ^a	~	13.2 μM	Inoue and Kirchhoff, 2000
4,4'-biphenol ^{Mr}	CV	7.0	0.35 ^a	~	~	Shayani-Jam and Nematollahi, 2011b
Acetaminophen ^{Mr}	CV	7.0	0.45 ^a	~	~	Shayani-Jam and Nematollahi, 2010a
Rutin ^{Mr}	DPV	7.0	0.27 ^a	0.5 μM ~ 25 μM	0.08 μM	Huang et al., 2015
Catechol ^{Mr}	CV	7.0	0.40 ^b	10 μM ~ 60 μM	3.0 μM	Lee et al., 2015
Catechol ^{Mr}	CV	7.4	-0.16 ^a	1 μM ~ 500 μM	0.5 μM	Zhao et al., 2016
$[IrCl_6]^{2- Mr}$	CV	7.0	0.72 ^a	~	~	Medina-Ramos et al., 2013
Catechol derivatives ^{Mr}	CV	7.3	0.25	~	~	Pacsial-Ong et

412 Where MI = material; Mr = mediator; OP = oxidation potential; a = vs. Ag/AgCl electrode; b = vs.
 413 Ag electrode; c = vs. Saturated Calomel Electrode; AMP = Amperometric; NHPDA =
 414 N-(4-hydroxyphenyl)-3,5-dinitrobenzamide; DPV = Differential Pulse Voltammetry; LSV =
 415 Linear Sweep Voltammetry; SWV = Square Wave Voltammetry; AMP-CE = Amperometric
 416 method coupled with capillary electrophoresis; SPE = screen-printed electrode; MPT-HP- β -CD =
 417 2-Hydroxypropyl- β -Cyclodextrin enveloped 10-methylphenothiazine; FeT4MpyP = iron(III)
 418 tetra-(N-methyl-4-pyridyl)-porphyrin; FTO = fluorine doped tin oxide; ITO = indium tin oxide;
 419 CoPcTF = Cobalt phthalocyaninetetrasulfonate; CNT = carbon nanotube; MWCNT =
 420 multiwall carbon nanotube; NiHCF = nickel hexacyanoferrate; ¹, obtained at 0 V; ²,
 421 obtained at 0.1 V.

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425 **Graphical Abstract:** TCNQ and GO modified GCE for the electrocatalytic oxidation
 426 of GSH

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