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# Applications of Biotechnology in Development of Biomaterials: Nanotechnology and Biofilms

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10 Biotechnology is the application of biological techniques to develop new tools and products for medicine and industry. Due to various properties including chemical stability, biocompatibility, and specific activity, e.g. antimicrobial properties, many new and novel materials are being investigated for use in biosensing, drug delivery, hemodialysis, and other medical applications. Many of these materials are less than 100 nanometers in size. Nanotechnology is the engineering discipline encompassing designing, producing, testing, 15 and using structures and devices less than 100 nanometers. One of the challenges associated with biomaterials is microbial contamination that can lead to infections. In recent work we have examined the functionalization of nanoporous biomaterials and antimicrobial activities of nanocrystalline diamond materials. In vitro testing has revealed little antimicrobial activity against *Pseudomonas fluorescens* bacteria and associated biofilm formation that enhances recalcitrance to antimicrobial agents including disinfectants and antibiotics. Laser scanning confocal microscopy studies further demonstrated properties and characteristics of the 20 material with regard to biofilm formation.

## A INTRODUCTION

In recent years the development of nanotechnology has allowed 25 the development of new materials to combat microbial biofilm formation on biomaterials. These advances in the use of nanostructured materials for medical applications have resulted from two primary considerations. First, there is a natural evolution to nanoscale materials as novel processing, 30 characterization, modeling techniques, and technology for necessary manipulation and manufacturing becomes available. Second, specific interactions between biological structures (e.g., tissues and other cellular processes) and nanostructured materials may allow for devices with specific functionalities to be 35 developed.

Nanocrystalline diamond has recently been considered for use in preventing microbial growth (Leis et al., 2010). Diamondlike carbon-silver, diamondlike carbon-platinum, and diamondlike carbon-silver-platinum composite films have been prepared using 40 a novel multicomponent target pulsed laser deposition process (Morrison et al., 2005). Silver and platinum form nanoparticle arrays within the diamondlike carbon matrix that can be attributed to the high surface energy of noble metals relative to carbon. Diamondlike carbon-silver-platinum composites exhibit 45 significant antimicrobial efficacy against *Staphylococcus* bacteria (Morrison et al, 2005). Robust antimicrobial function has been observed in diamondlike carbon-silver-platinum composite films; this functionality is tentatively attributed to the formation of a galvanic couple between silver and platinum that enhances silver 50 ion release (Narayan et al, 2005). Diamondlike carbon-metal composite films may provide higher hardness, corrosion resistance, and antimicrobial functionalities to next generation

cardiovascular, orthopaedic, biosensor, and other biomedical devices. New applications of the antimicrobial properties of diamond-like carbon-silver-platinum nanocomposites may include catheters and other devices (Narayan et al., 2006).

Novel antimicrobial silver ion complex resin compositions comprising a silver-thiosulfate ion complex loaded onto an organic anion exchange resin have been proven successful (Capelli, 2006). These silver thiosulfate ion complex resin compositions are able to release stable antimicrobial silver ion complexes over time when placed in a saline environment. These antimicrobial silver-ion complex resins can be useful in the treatment and prevention of infections and diseases.

A stabilized composition having antibacterial, antiviral and/or antifungal activity utilizing a silver compound in the form of a complex with primary, secondary or tertiary amines has also proven effective for use in urine catheters (Pedersen; et al., 2002).

The complex is associated to one or more hydrophilic polymers, remains stable during sterilization, and retains antimicrobial activity without giving rise to darkening or discoloration of the dressing during storage. An antimicrobial latex composition comprising a homogeneous blend of a natural/synthetic rubber latex and protein silver, and a second antimicrobial latex composition comprising a homogeneous blend of a cationic natural rubber latex or a cationic synthetic polymer latex and a water-soluble silver compound has also been developed (Umemura et al., 1990).

Atomic layer deposition (also known as molecular layering or atomic layer epitaxy) is a thin film growth technique in which alternating controlled surface chemical reactions occur between gaseous precursor molecules (Alyssouri et al., 2003, Puurunen, R. L. and Vandervorst, W. 2004). The self-terminating gas-solid reactions allow for material to be applied in a layered methodology. Individual reactions are separated by purge steps that involve saturation with an inert gas. By saturating the substrate at each individual reaction, all surfaces of a given substrate can receive a uniform coating of thickness and composition. The atomic layer deposition cycles can be repeated

to control precisely the coating thickness of any applied inorganic antimicrobial agent at the nano scale including TiO (Narayan, 2009).

Atomic layer deposition has also been used to coat the surfaces of proposed biomaterials including nanoporous alumina membrane in order to reduce the pore size in a controlled manner (Cameron et al, 2000). Recent work on unmodified nanoporous alumina membranes has shown that release of biological molecules in nanoporous alumina membranes is determined by the diameters of the pores (Kipke et al., 2004). Narayan et al., 2009, demonstrated that titanium oxide (TiO) coating can reduce the pore size in a controlled manner, maintain a narrow pore size distribution, prevent aluminum ions from leaching into the surrounding tissues, and create a biocompatible antimicrobial pore/tissue interface under the right conditions. In that work microbial results showed a significant decrease in the amount of microbial attachment to membranes treated with TiO with both *Staphylococcus aureus* and *Escherichia coli*.

Biofilm are aggregates of microorganisms in which cells adhere to each other and/or to a surface. The associated cells are frequently embedded within a self-produced matrix of extracellular polymeric substance (EPS). Biofilm EPS is a polymeric conglomeration generally composed of extracellular DNA, proteins, and polysaccharides that can become highly organized, making it resistant to biocides. Biofilms may form on living or non-living surfaces, and represent a prevalent mode of microbial life in natural, industrial and hospital settings (Atlas et al., 2003).

Biofilm formation in medical devices is inherently disruptive as it can lead to health concerns including infection (Hall-Stoodley, Costerton, and Stoodley, 2004). All novel biomaterial for use in medical devices must be tested to determine their resistance to biofilm development. In this study, the resistance of nanocrystalline diamond to growth of microbial biofilms in a continuous perfusion environment was examined.

## MATERIALS AND METHODS

CDC Bioreactors: A rotating disc reactor CDC biofilm reactor (Biosurface Technologies, Bozeman, MT, USA) containing

silicon, silica glass, roughened silica glass, nanocomposite samples fixed to silica glass, and coated polycarbonate circular samples was used for microbial testing. The CDC biofilm bioreactor and all operating components were autoclaved prior to the testing. This CDC reactor consists of a 1-L vessel with an effluent spout at approximately 400 ml, which is connected to a waste bottle. Continuous mixing of the bulk fluid is ensured by a magnetically driven (RET digi-visc, IKA Labortechnik, Wilmington, MA, USA) baffled stir bar. A polyethylene lid supports eight independent rods, which each can house three removable circular disks. The lid also contains three stainless steel ports allowing the connection of two sterile (0.2 µm) vent filters (Millex®-FG, Millipore, Bedford, MA, USA) and an inlet for the diluted growth medium. All materials and growth medium were autoclaved prior to use. Low concentrations (1%) of Peptone-Trypticase-Yeast extract-Glucose (PTYG) medium was used (Brigmon et al., 1998) as the growth medium. Initially, reactors were operated in batch mode for 24 h to establish the biofilms on the various substrata in 1% PTYG medium. Following the period of batch growth, the system was operated in chemostat mode by continuously pumping the 1% PTYG medium *Pseudomonas fluorescens* flow rate of 2 ml/min for 72 h.

The nanocrystalline diamond material was described previously by Lewis et al, 2010. Briefly, the nanocrystalline diamond samples were mounted on coupons on the rotating disc of the reactor.

*Pseudomonas fluorescens* (strain #B252) was the biofilm forming microorganism tested as previously described (Lewis et al., 2010).. List of materials including controls placed in CDC biofilm bioreactor is as follows

1. Frosted glass
2. Clear Glass
3. Nanocrystalline diamond
4. Half nanocrystalline diamond, half smooth.
5. Control-coupon only-no material.

#### Bioreactor Sampling

Coupon samples were removed at the three time points along with 4-1 ml aliquots of medium were aseptically removed at the following time points  
Time 0 – 1 ml Liquid

Time 1-1h 25 min Liquid +coupons

Time 2- 18h 10 min Liquid+coupons

Time 3-24h 10 min Liquid+coupons

All samples were immediately frozen @ -20°C for later analysis.

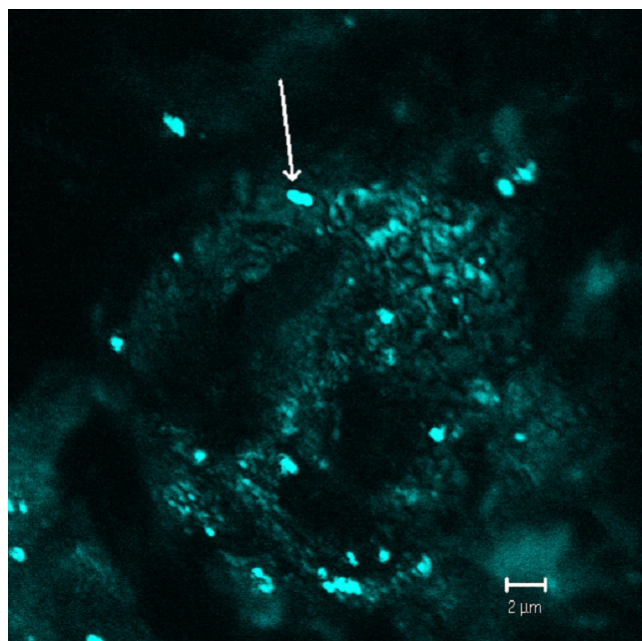
The bioreactor was maintained and mixed the entire test in a sterile lab hood @ 25°C.

#### Microbial Analysis

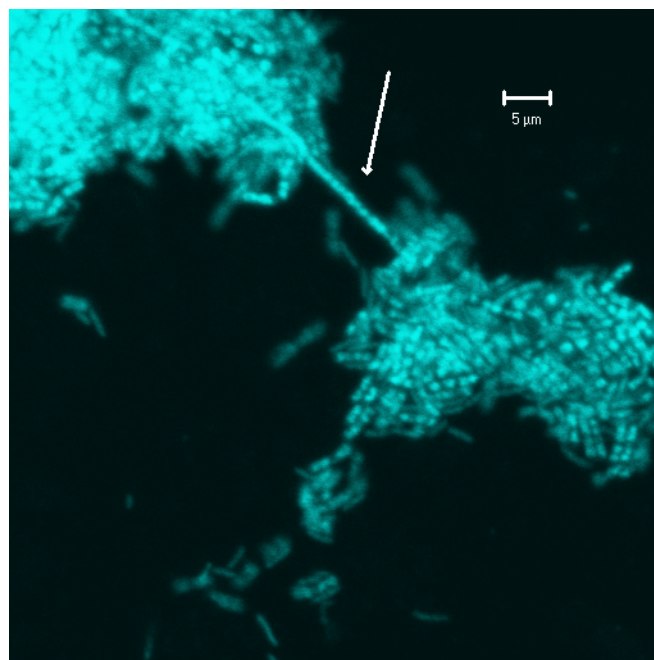
Bacteria densities were determined by Acridine Orange Direct Counts (AODC) as previously described (Brigmon et al., 1998). Digital mages of the stained cells on the coupons and materials were obtained using a laser confocal scanning microscope (Model LSM 510 Carl Zeiss Inc., Germany). Coupon samples were thawed, air dried in a sterile laminar flow hood, and then stained with 4, 6 diamidino-2-phenylindole (DAPI) to determine total microbial cells per microscopic field (Kastner et al., 2000). Images of the stained cells were obtained using a laser confocal scanning microscope (Model LSM 510 Zeiss, Germany).

#### Results

*P. fluorescens* densities in the Bioreactor medium ranged from 2.98 X 10<sup>5</sup> cells/ml at Time 0 to 1.56 X 10<sup>5</sup> cells/ml at Time 3. Flow though rate of medium was maintained at 2 ml/minute At sampling time 1 after one hour and twenty-five minutes there was little difference observed between the controls (frosted glass, clear glass, coupon, and half coupon only) and the diamond material so far as microbial attachment. All samples had some *P. fluorescens* cells attached as demonstrated by the LSCM image in Figure 1. The cells attach although the CDC bioreactor is constantly swirling the individual coupon holders. Some cells can be observed elongating and dividing indicating early biofilm formation. Note the orientation of the attached on the surface in Figure 1.



**Figure 1.** Attachment of *Pseudomonas fluorescens* cells mounted on coupon with transect showing scale after 1 hour 25 minutes.



**Figure 2.** *Pseudomonas fluorescens* cells forming a biofilm on the nanocrystalline diamond material after 18 hour 10 minutes.

5  
 At sampling time two, 18 hours and ten minutes after continuous exposure, biofilm was covering most of the control surfaces. Growth of *P. fluorescens* demonstrated partial coverage of the nanocrystalline diamond as shown in the LSCM image in Figure 10 2. The biofilm was up to 8  $\mu\text{m}$  thick in some areas while others sections there was little growth. Note the cross-bridging occurring in Figure 2 (arrow). Once the two larger clumps of cells shown here are ‘tethered’ in this manner they will form larger biofilms. This demonstrates the biofilm as it grows in 15 organization and structure. As the density of the biofilm increases so does the recalcitrance of the microbial cells on the inner layers to drug and/or biocide treatment such as antibiotics. Biofilm formation is also resistance to the body’s natural immunological defenses such as antibody production and or 20 macrophage activity.

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*P. fluorescens* colonization on nanocrystalline diamond coating after 24 hr incubation was examined using a laser scanning confocal microscope (Figure 3A). This image shows a much larger more organized biofilm and smaller cell colonies. This 30 particular larger biofilm formation on the slide center is roughly 40  $\mu\text{m}$  by 60  $\mu\text{m}$  size. The longer side is oriented with the flow of the CDC Bioreactor. Biofilms form with an initial attachment of cells that then begin dividing and forming a colony. Colonization allows more cells from the circulating medium to attach and 35 grow. Figure 2 shows apparent attachment between *P. fluorescens* colonies that over time form larger units.

Figure 3B is a side three dimensional view of *P. fluorescens* colony and biofilm formation on the nanocrystalline diamond 40 surface observed in Figure 3A. Note the depth of the biofilm is up to 10  $\mu\text{m}$  indicating robust growth.

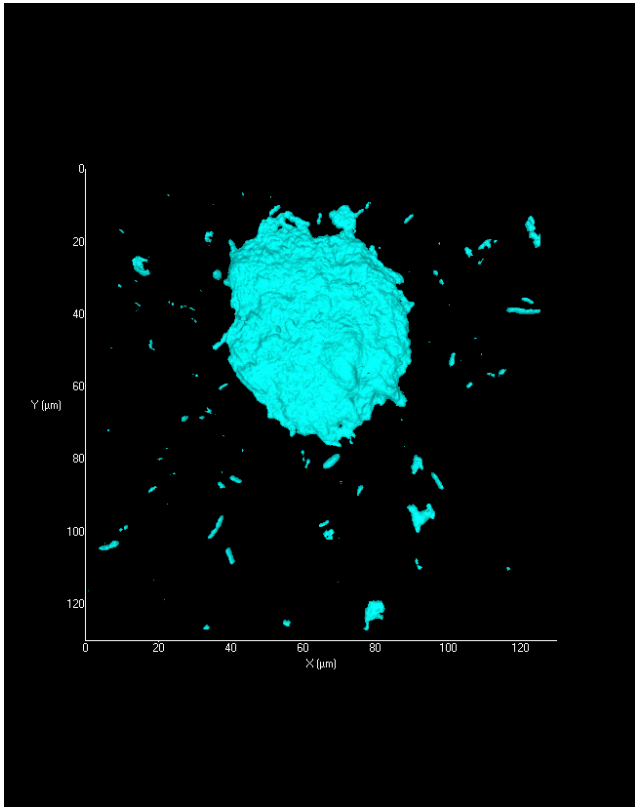


Figure 3A. Laser scanning confocal microscope three-dimensional image of *P. fluorescens* on nanocrystalline diamond. The image was taken after 24 hr in the reactor.

Growth of *P. fluorescens* was similar on the nanocrystalline diamond as compared to glass controls at all sampling times. On closer observation at 1300X with LSCM the surface of the mounted nanocrystalline diamond material appeared rough and angular, allowing microbial attachment and/or entrapment and subsequent colonization on the glass surface.

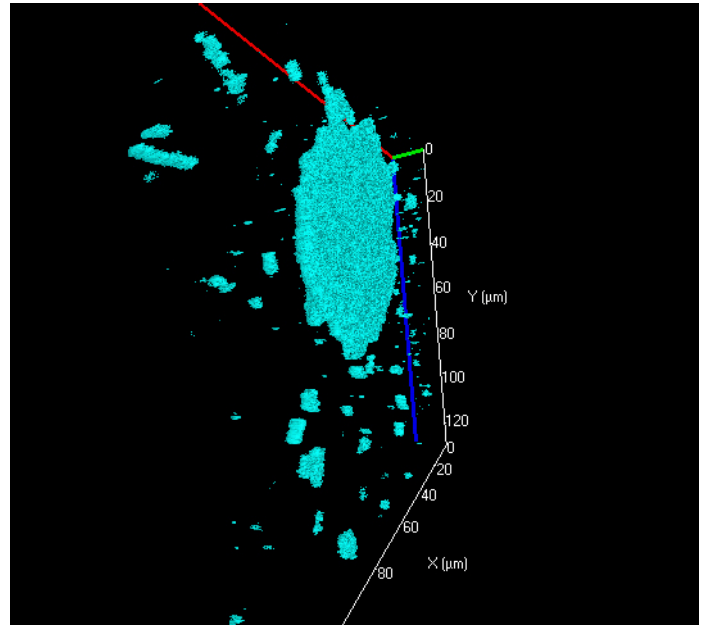


Figure 3B. Three dimensional side image of the same field as Figure 3A of *P. fluorescens* growth on a nanocrystalline diamond coating taken after 24 hr. This image shows a biofilm attached to the nanocrystalline diamond coating as well as smaller clumps of cells.

## Discussion

Lewis et al. recently compared microbial growth on nanocrystalline diamond coated silicon wafers that were immersed in growth medium containing *Pseudomonas fluorescens* [Lewis et al., 2010]. The results of that work demonstrated that nanocrystalline diamond coatings of surfaces did not prevent *P. fluorescens* growth under operant conditions. Another study demonstrated that *Streptococcus mutans*, a microorganism of concern in dental-related biofilms, uses a peptide pheromone quorum-sensing signal transduction system to stimulate the uptake and incorporation of foreign DNA. Experimentally the signal peptide can be chemically synthesized and added to cultures to stimulate transformation indicating microbial adaptation to changing environments in biofilms (Li et al., 2001). When there are mixed culture biofilms it may be possible for transfer of genetic information including antimicrobial resistance. Thus there is the possibility of microbial resistance to new surface treatment strategies. The pathogenesis of many orthopaedic infections has been related to the presence of microorganisms in biofilms (Patel, 2005). If the

nanocrystalline diamond material had been milled or made smoother it may have changed the results found here. As described in the results the roughed surface of the nanocrystalline diamond appeared to aid microbial attachment.

5 Quorum sensing is a biochemical signalling process many microbial species use to control their metabolism according to environmental conditions. The colony to colony connections observed by *P. aeruginosa* cells in Figure 2 could be due to  
10 quorum sensing. Many bacteria use quorum-sensing systems in microbial colonies to regulate several physiological properties, including the ability to incorporate foreign DNA, tolerate acid, biofilm formation, and virulence (Cvitkovitch et al., 2003). Successful inhibition of quorum sensing in a *P. aeruginosa*  
15 biofilm by a halogenated furanone compound could lead to novel antimicrobial agents (Hentzer et al., 2002). Either organic compounds such as furanone or inorganic nanomaterials like TiO<sub>2</sub> that affect biofilm architecture and enhance microbial detachment that lead to a loss of bacterial biomass from surfaces would be  
20 useful for biomedical applications.

## Conclusions

Under these conditions nanocrystalline diamond coatings did not inhibit *P. fluorescens* attachment and biofilm formation in the CDC Biofilm Reactor (Lewis et al., 2010). It is evident that once  
25 initial microbial attachment and colonization occurs, subsequent biofilm formation is hard to control (Figure 3A & B). Combining potential antimicrobial materials may be necessary for optimal biomedical applications. Additional nanostructured materials with titanium and zinc coatings may be useful for  
30 inhibiting microbial attachment/colonization for certain biomedical applications including catheters. Silicon materials are associated with less inflammation than polymeric materials that are currently used for local drug delivery. In addition, these materials may provide greater flexibility in their applications,  
35 since there are often difficulties when pharmacologic agents and polymers are dissolved in a given solvent. Nanostructured materials prepared using atomic layer deposition may also be useful for delivering a pharmacologic agent at a precise rate to a specific location in the body. Delivery could be based on the  
40 pharmacokinetics of the specific agent. These materials may serve as the basis for “intelligent” drug delivery systems,

orthopaedic implants, or self-sterilizing medical and veterinary devices.

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