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Robotic Resistance Treadmill Training Improves Locomotor Function in Children With Cerebral Palsy: A Randomized Controlled Pilot Study

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Abstract

Objective

To determine whether applying controlled resistance forces to the legs during the swing phase of gait may improve the efficacy of treadmill training as compared with applying controlled assistance forces in children with <u>cerebral palsy</u> (CP).

Design

Randomized controlled study.

Setting

Research unit of a <u>rehabilitation</u> hospital.

Participants

Children with spastic CP (N=23; mean age, 10.6y; range, 6–14y; Gross Motor Function Classification System levels, I–IV).

Interventions

Participants were randomly assigned to receive controlled assistance (n=11) or resistance (n=12) loads applied to the legs at the ankle. Participants underwent robotic treadmill training 3 times a week for 6 weeks (18 sessions). A controlled swing assistance/resistance load was applied to both legs starting from the toe-off to mid-swing phase of gait during training.

Main Outcome Measures

Outcome measures consisted of overground <u>walking speed</u>, 6-minute walk distance, and <u>Gross Motor Function</u> <u>Measure</u> scores and were assessed <u>pre</u> and post 6 weeks of training and 8 weeks after the end of training. Results

After 6 weeks of treadmill training in participants from the resistance training group, fast walking speed and 6minute walk distance significantly improved (18% and 30% increases, respectively), and 6-minute walk distance was still significantly greater than that at baseline (35% increase) 8 weeks after the end of training. In contrast, overground gait speed and 6-minute walk distance had no significant changes after robotic assistance training.

Conclusions

The results of the present study indicated that robotic resistance treadmill training is more effective than assistance training in improving locomotor function in children with CP.

Keywords

Cerebral palsy, Child, Locomotion, Rehabilitation

List of abbreviations

ANOVA analysis of variance CP cerebral palsy GMFCS Gross Motor Function Classification System GMFM Gross Motor Function Measure IQR interquartile range RPE rating of perceived exertion Attaining walking ability is often an important functional goal for children with <u>cerebral palsy</u> (CP). Among the children who are diagnosed with CP, up to 90% of them have difficulty walking.<u>1</u>, <u>2</u> Reduced <u>walking</u> <u>speed</u> and <u>endurance</u> are 2 of the main functional problems.<u>3</u>, <u>4</u> <u>Ambulation</u> plays a central role in normal bone development⁵ and cardiopulmonary endurance,<u>6</u>, <u>7</u> and children who are able to ambulate are more accomplished in activities of daily living and social roles than children who use a wheelchair.⁸ The development of independent gait and efficiency of walking are often the focus of therapeutic interventions for children with CP.

The use of treadmill training has demonstrated improvement in walking capacity in some children with CP.9, 10 For instance, results have indicated improvements in gait speed,9, 11 endurance,⁹ and the Gross Motor Function Classification System (GMFCS) measures.10, 12 However, although statistically significant improvements in walking capacity with treadmill training have been shown, it remains unclear whether therapeutic effects of such training are maximized, and further evidence is needed to support treadmill training in children with CP.¹³

The results of <u>motor learning</u> studies indicated that active training is more effective than passive training in improving the efficacy of motor training.¹⁴ Thus, we postulated that active engagement from children with CP might improve the efficacy of locomotor training. We proposed that applying a resistance force to leg swing may force them to be more actively involved because they need to generate additional joint torques to counteract the load. In addition, applying a resistance force to leg swing may produce a deviation in step kinematics, that is, increase the kinematic errors, which is supported by previous studies in individuals poststroke<u>15</u>, <u>16</u> and humans with spinal cord injury.¹⁷ Error augmentation may accelerate motor learning during treadmill training,<u>18</u>, <u>19</u>, <u>20</u> resulting in improvement in the efficacy of locomotor training in children with CP.

In contrast, providing leg assistance force may facilitate leg swing, which imitates the way that <u>physical</u> <u>therapist</u> provides leg assistance during treadmill training, and improve locomotor function in children with CP through use-dependent <u>motor learning</u> mechanisms,²¹ but it may reduce the level of active engagement of children with CP. To date, there are no randomized controlled studies that have directly compared leg resistance with assistance during treadmill training in children with CP. The purpose of this study was to assess functional changes after resistance versus assistance treadmill training in children with CP. We hypothesized that children with CP in both groups would show improvements in locomotor function, which was assessed using <u>walking</u> <u>speed</u> and 6-minute walk distance, although greater improvements were expected after resistance training than after assistance training.

Methods

Participants

Participants were recruited through the <u>outpatient</u> department of the <u>Rehabilitation</u> Institute of Chicago between October 5, 2011 and July 16, 2014. Specifically, 92 children were contacted through phone calls, 69 children were excluded, and 23 children (11 boys and 12 girls) with CP were recruited to participate in this study (<u>fig 1</u>). The mean age of participants was 10.6 years (range, 6–14y). Their <u>GMFCS</u> level ranged from I to IV (I, n=1; II, n=11; III, n=8; IV, n=3).



Fig 1. Flowchart of participants' enrollment and randomization.

Inclusion criteria included (1) a diagnosis of bilateral spastic CP attributed to complications of prematurity, <u>intracranial hemorrhage</u>, and <u>periventricular leukomalacia</u> according to the definition of Bax²²; (2) aged 4 to 14 years; (3) without <u>botulinum toxin</u> treatment and orthopedic surgery or <u>neurosurgery</u> in the 6 months before the onset of training; (4) GMFCS level ranged from I to IV; (5) able to signal pain, fear, or discomfort reliably; (6) with mild <u>scoliosis</u> (Cobb angle <20°); (7) passive range of motion within functional limits; and (8) able to follow instructions on behavior tests.

Exclusion criteria included severe lower extremity <u>contractures</u>, fractures, osseous instabilities, <u>osteoporosis</u>, severe disproportional bone growth, unhealed skin lesions in the lower extremities, <u>thromboembolic diseases</u>, cardiovascular instability, and aggressive or self-harming behaviors.

All procedures were approved by the Institutional Review Board of the Northwestern University. Medical clearance for participation was requested from the primary physician of each participant. Written consent was obtained from all participants and their parents.

Apparatus

A custom-designed cable-driven robotic gait training system was used to apply controlled resistance or assistance force to both legs during treadmill walking, which was reported previously.²³ In brief, the cable-driven robotic system consists of 4 direct current motors and cable spools (fig 2). Two motors and cable spools located in the front of the Woodway^a treadmill were used to apply a controlled assistance force to the legs at the ankle, and 2 motors located at the back of the treadmill were used to apply a resistance force to the legs. The ankle trajectory signals were measured using a custom-designed, 3-dimensional position detector. The ankle position signals were used by the operator to control the timing and magnitude of loading at targeted phases of gait. An adaptive control algorithm was used to automatically adjust the amount of the resistance/assistance load on the basis of the motor performance of the participants.²³ The operator controlled the robotic system via a user interface that was programmed in LabVIEW.^b



Fig 2. Experimental setup for the robotic assistance/resistance treadmill training. Two motors and cable spools are attached to a fixed frame located in front of the treadmill and are used to apply a controlled assistance force to the legs at the ankle, and 2 motors are attached to a frame located at the back of the treadmill and are used to apply a resistance force to the legs. A computer is used to control the coordinated movement of 4 motors.

Protocol

Participants were stratified according to initial <u>gait speed</u> and were randomly assigned to receive controlled assistance or resistance loads applied to both legs at the ankle. The treadmill speed was set at the comfortable speed of each participant on a treadmill, and an overhead harness was used to provide body weight support as needed to prevent knee buckling and toe drag. Participants walked on a treadmill for 40 minutes, which was adjusted on the basis of their tolerance on the activity, excluding setup time in each training session. Training sessions were conducted 3 times a week for 6 weeks. For participants who were assigned to the assistance training group, a load that assisted swing was applied to both legs starting from the toe-off to mid-swing phase of gait. For participants who were assigned to the resistance training group, a controlled resistance load was applied to both legs. Both the treadmill speed and the resistance/assistance load were gradually increased during the course of 6 weeks of treadmill training. Body weight support was provided in 8 participants (3 in the resistance group and 5 in the assistance group), with the average support being 11.4%±4.2% of body weight at session 1 and 8.1%± 6.2% of body weight at session 18. The rating of perceived exertion (RPE),²⁴ which was used to quantify the perceived training intensity, was monitored during the course of training, and the targeted RPE was 11 to 16.

Outcome measures

Primary outcome measures included participant's self-selected and fast overground walking speed collected on a 10-m instrumented walkway (GAITRite[£])25, 26 and averaged across 3 trials, and walking distance assessed through the 6-minute timed walk.²⁷ Secondary outcome measures included clinical assessments of motor function. Specifically, dimensions D (standing) and E (walking, running, jumping) of the Gross Motor Function Measure-66 (GMFM-66) were assessed by licensed physical therapists.28, 29 Physical function was measured using the Pediatric Outcomes Data Collection Instrument.³⁰ In addition, <u>muscle tone</u> of major knee joint muscle groups was assessed clinically with the Modified Ashworth Scale (score, 0–4),³¹ which was used before the <u>GMFM</u> and <u>6-minute walk tests</u>.

Data analysis

A power analysis was performed on the basis of the results of our previous pilot study, which indicated that with a power of 0.8 and an α of .05, 11 participants per group would be required. Baseline characteristics and training parameters were compared between the 2 test groups using paired *t* tests and <u>Wilcoxon rank-sum tests</u>, as appropriate, and data normality was checked using the Shapiro-Wilk test. Repeated-measures analyses of variance (ANOVAs) were used for all parametric measures for within-group comparison. If a significant difference was detected, post hoc Tukey-Kramer tests were conducted to determine which conditions were different from each other. Modified Ashworth Scale scores were analyzed using <u>Friedman tests</u> with post hoc Wilcoxon tests. Changes in primary outcomes (ie, gait speed and endurance) were calculated by subtracting the baseline value from the values obtained at posttesting and follow-up testing and analyzed using repeatedmeasures ANOVA with main factor of treatment (resistance vs assistance training) and repeated for time (posttesting and follow-up testing). Statistical significance for all tests was set at *P*<.05.

Results

Twenty participants completed all the training and assessment sessions, with 3 participants dropping out (because of poor attendance, child's request, and participation in another study, respectively). At baseline, there were no significant differences between the 2 groups in age, overground <u>walking speed</u>, 6-minute walk distance, and <u>GMFM</u> scores (<u>table 1</u>). Treadmill training speed, distance, and time were gradually increased for both groups (P<.01) during the course of training, with no significant difference noted between the 2 groups. In addition, the training intensity, which was quantified using RPE, had no significant difference between the 2 groups (<u>table 2</u>).

Characteristic	Resistance Training	Assistance Training	Р
Age (y)	10.6±3.0	10.8±2.3	.93
Sex: male/female	6/6	5/6	NA
Race: white/other			
African American	1	1	NA
Asian	1	0	NA
Hispanic	4	5	NA
White	6	5	NA
Extremity distribution			
Diplegia	7	7	NA
Quadriplegia	5	4	NA
GMFCS level			
1	1	0	NA
II	5	5	NA
111	5	4	NA
IV	1	2	NA
Ankle braces			
None	0	2	NA
BAFO/SMO	12	9	NA
GMFM score			
Total score	63.6±8.6	60.8±9.1	.33
Dimension D	25.8±8.0	22.8±11.3	.18
Dimension E	32.3±18.2	30.4±18.0	.64

Table 1. Characteristics of the participants for baseline comparisons

Self-selected walking speed (m/s)	0.64±0.28	0.57±0.23	.35
Fast walking speed (m/s)	1.00±0.35	0.88±0.34	.28
6-min walk distance (m)	277.2±111.9	228.3±117.8	.27
MAS score	0.67±0.53	0.95±0.72	.40

NOTE. Values are mean ± SD or n. *t* tests and <u>Wilcoxon rank-sum tests</u> were used for comparison between the 2 groups.

Abbreviations: BAFO, bilateral ankle foot <u>orthosis</u>; MAS, Modified Ashworth Scale; NA, not applicable; SMO, supramalleolar orthosis.

Table 2. Training paradigms including treadmill speed, time, and training intensity at sessions 1, 9, and 18 for robotic resistance vs assistance treadmill training groups

Variable	Resistance Training	Assistance Training	Р
Session 1			
Speed (m/s)	0.42±0.15	0.42±0.19	.95
Distance (km)	0.80±0.31	0.85±0.43	.78
Time (min)	31±2	33±3	.15
RPE	12.9±2.9	11.8±1.6	.27
Peak force (N)	11.4±2.6	13.2±2.9	.18
Session 9			
Speed (m/s)	0.51±0.19	0.49±0.16	.85
Distance (km)	1.13±0.48	1.11±0.45	.95
Time (min)	36±3	37±4	.58
RPE	11.1±1.1	12.2±1.6	.23
Peak force (N)	13.3±4.1	16.4±2.2	.08
Session 18			
Speed (m/s)	0.55±0.18	0.53±0.22	.86
Distance (km)	1.13±0.42	1.28±0.57	.98
Time (min)	39±3	39±3	.93
RPE	12.0±1.8	11.3±1.5	.19
Peak force (N)	14.8±5.2	18.2±3.2	.15

NOTE. Values are mean ± SD. *t* tests were used for comparison between the 2 groups.

Robotic resistance treadmill training improved walking function in children with CP. Specifically, fast walking speed significantly increased after robotic resistance treadmill training ($F_{2,9}$ =4.12; ANOVA, *P*=.03) (fig 3). Post hoc tests indicated a significant increase from baseline to posttesting (mean increase, 18%; interquartile range [IQR], 2%–31%; *P*=.01), although there was no significant difference between baseline and follow-up testing (increase, 17%; IQR, -6% to 17%; *P*=.13). Self-selected walking speed tended to increase (mean increase, 32%; IQR, -8% to 44%), but this was not significant because of large variability across participants ($F_{2,9}$ =1.66; *P*=.21). In addition, 6-minute walk distance significantly increased after resistance training ($F_{2,9}$ =10.04; *P*=.001). Post hoc tests indicated a significant increase from baseline to posttesting (increase, 30%; IQR, 4%–45%; *P*=.01) and from baseline to follow-up testing (increase, 35%; IQR, 6%–64%; *P*=.001).







Fig 3. Average of self-selected <u>walking speed</u>, fast walking speed, 6-minute walk distance <u>pre</u> and post 6 weeks of robotic treadmill training and 8 weeks after the end of treadmill training, that is, follow-up testing. (A)

Overground walking speed for participants from the resistance treadmill training group. (B) Overground walking speed for participants from the assistance treadmill training group. (C) Six-minute walk distance for participants from the resistance training group. (D) Six-minute walk distance for participants from the assistance training group. Three trials were conducted for walking speed and averaged across participants for each group. Error bars indicate SD of each gait parameter. *Significant difference, *P*<.05.

In contrast, robotic assistance treadmill training induced modest changes in walking function in children with CP. Specifically, both fast and self-selected walking speeds had no significant changes after assistance training (mean increase, 0.4%, IQR, 0%–10%; $F_{2,9}$ =1.85; P=.19 and increase, 2%, IQR, -12% to 20%; $F_{2,9}$ =.51; P=.6 for fast and self-selected walking speeds, respectively) (see fig 3). In addition, 6-minute walk distance had no significant change after assistance training (increase, 4%; IQR, -6% to 16%; $F_{2,9}$ =.48; P=.63).

Greater functional gains were observed for participants who underwent resistance training than for those who underwent assistance training. Specifically, changes in self-selected walking speed, fast walking speed, and 6-minute walk distance after treadmill training were significantly greater for participants from the resistance group than for participants from the assistance group ($F_{1,1}$ =5.36, P=.03; $F_{1,1}$ =10; P=.003; and $F_{1,1}$ =12.23; P=.001 for self-selected walking speed, fast walking speed, and 6-minute walk distance, respectively) (fig 4). We observed no significant differences in changes in walking function between posttesting and follow-up testing (P=.75 for self-selected walking speed, P=.33 for fast walking speed, and P=.73 for 6-minute walk distance). GMFM scores significantly changed after resistance training ($F_{2,9}$ =5.21; P=.02). Post hoc tests indicated significant differences between posttesting and follow-up testing scores (P=.02), although there was no significant difference between pretesting versus posttesting scores (P=.09) (table 3). In addition, step cadence during fast walking significantly increased after resistance training ($F_{2,9}$ =6.11; P=.01). Post hoc tests indicated significant differences in step cadence between pretraining and posttraining (P=.01), although there was no significant differences after resistance training ($F_{2,9}$ =6.11; P=.01). Post hoc tests indicated significant differences in step cadence between pretraining and posttraining (P=.01), although there was no significant differences in step cadence between pretraining (P=.06) (table 4). Other spatial-temporal gait parameters had no significant changes for both groups (P>.05).



Fig 4. Changes in (A) self-selected <u>walking speed</u>, (B) fast walking speed, and (C) 6-minute walk distance after robotic resistance/assistance treadmill training and 8 weeks after the end of training, that is, follow-up testing. Data shown in the figure are the mean and SD of walking speeds and distance across participants. *Significant difference, *P*<.05.

Table 3. Self-selected <u>walking speed</u>, fast walking speed, and 6-minute walk distance, <u>GMFM</u> scores, MAS scores, and PODCI scores after robotic resistance and assistance treadmill training

Variable	Resistance				Assistance			
	Training				Training			
	Pre	Post	Follow-Up	Р	Pre	Post	Follow-Up	Ρ
Fast speed	0.98±0.39	1.13±0.38	1.09±0.35	.01 <u>*</u>	0.84±0.34	0.84±0.37	0.77±0.36	.19
(m/s)								
Self-	0.63±0.30	0.72±0.24	0.71±0.22	.22	0.54±0.22	0.52±0.18	0.50±0.19	.61
selected								
speed								
(m/s)								

6minWD	272.7±113.	336.3±104.	353.9±125.	.001 <u>*</u>	216.3±116.	230.1±119	224.7±118.	.63
(m)	0	9	8		8	.2	7	
GMFM								
score								
Total	63.7±8.7	63.4±8.2	64.9±9.4	.02 <u>*</u>	60.0±9.2	59.8±9.6	60.3±9.4	.69
score								
Dimensio	25.1±8.6	26.0±6.9	27.3±7.1	.18	21.7±11.3	21.8±11.7	20.8±11.4	.62
n D								
Dimensio	31.4±19.5	30.5±19.2	32.5±19.8	.11	29.2±18.5	28.3±17.7	28.8±19.5	.35
n E								
MAS score	0.65±0.57	0.83±0.66	0.63±0.39	.97	0.85±0.67	0.68±0.56	0.87±0.55	.20
PODCI	23.0±17.2	23.0±18.0	24.5±12.2	.84	23.0±23.6	19.5±12.1	24.0±16.0	.74
(self)								
score								
PODCI	7.5±16.2	19.1±15.5	19.0±16.8	.002*	7.9±22.8	9.8±16.4	3.9±24.5	.83
(parent)								
score								

NOTE. Values are mean ± SD. ANOVAs and <u>Friedman tests</u> were used for within-group comparison.

Abbreviations: 6minWD, 6-min walk distance; MAS, Modified Ashworth Scale; PODCI, Pediatric Outcomes Data Collection Instrument.

*Significant difference.

Table 4. Spatial-temporal gait parameters pre and post robotic resistance and assistance treadmill training

Variable	Resistance Training				Assistance Training			
	Pre	Post	Follow-Up	Р	Pre	Post	Follow-Up	Ρ
Fast walking								
Step length (m)	0.47±0.10	0.50±0.09	0.49±0.09	.26	0.42±0.10	0.42±0.09	0.40±0.10	.45
Stride length (m)	0.94±0.20	1.00±0.18	0.98±0.18	.15	0.84±0.20	0.84±0.18	0.84±0.22	.99
Cadence (step/min)	120.3±25.5	136.5±29.0	132.0±28.4	.01*	119.2±40.2	120.2±41.3	116.9±44.3	.86
Swing time (%)	38.9±4.8	39.8±3.8	40.0±3.2	.61	40.1±5.6	41.6±4.9	40.6±7.2	.72
Normal walking								
Step length (m)	0.39±0.11	0.43±0.09	0.42±0.08	.16	0.34±0.09	0.35±0.08	0.35±0.08	.83
Stride length (m)	0.78±0.22	0.86±0.18	0.85±0.16	.16	0.71±0.19	0.71±0.16	0.70±0.16	.98
Cadence (step/min)	93.2±26.3	100.6±21.8	100.7±20.8	.22	91.4±27.8	86.8±20.5	83.9±23.8	.21
Swing time (%)	33.6±4.7	35.7±1.9	36.5±2.0	.11	36.1±4.8	37.4±8.7	38.2±7.7	.78

NOTE. Values are mean ± SD. ANOVAs were used for within-group comparison.

*Significant difference.

Discussion

Applying a controlled swing resistance force to the legs during robotic treadmill training induced significant improvements in walking function of children with CP. In contrast, applying an assistance force to legs during treadmill training induced only modest changes in walking function. Furthermore, greater functional gains in walking were obtained for participants from the resistance group than for those from the assistance group.

In this study, greater improvements in walking function were observed for children who underwent resistance training than for those who underwent assistance training. One possible reason for the differences in functional gains may be that children who underwent resistance training were more actively engaged in the locomotor training session than were those who underwent assistance training. Specifically, for children who were assigned the resistance training group, the resistance load applied to both legs during the swing phase may force participants to generate additional joint torque to counteract the load and move the leg forward during treadmill training, which may require participants to increase voluntary activation through enhanced supraspinal input to the motoneuron pool and/or increase motoneuron excitability.³²

In contrast, for children who underwent assistance training, the <u>central nervous system</u> may adapt to the assistance force applied to the leg(s) during the swing phase of gait by reducing the motor output of the <u>leg</u> <u>muscles</u>,³³ probably owing to optimization of the energy cost.³⁴ Thus, a leg assistance force that is too large may encourage passive rather than active training. As a consequence, the training effect could be suboptimal. This is also consistent with a previous study, which indicated that only a modest increase in the <u>gait speed</u> of children with CP was observed after robotic training in which a passive guidance force was applied to both legs.³⁵ However, the results of a previous study in adults with <u>stroke</u> indicated that assistance and resistance training induced comparable walking functional gains.¹⁸ One possible reason may be due to the age (or the motivation level) difference of participants between the 2 studies.

In addition, the results of this study suggest that repeated exposure to force perturbations during walking may induce a prolonged retention of increased stride length in children with CP. The results of previous studies suggest that the neural system may adapt to the resistance force and show an aftereffect consisting of an increased stride length when the resistance force is removed (R. Tang et al, unpublished data, 2016), which is consistent with individuals poststroke15, 36 and humans with spinal cord injury.37, 38 Although the aftereffect after 1 session of swing resistance training is generally short-lived, the results of this study suggest that repeated exposure to a swing resistance force through long-term training, such as 18 sessions of training in this case, may induce an accumulation of increased stride length through a repeated adaptation and de-adaptation process,³⁹ which is consistent with previous results of studies involving humans with spinal cord injury¹⁹ and individuals poststroke using a split-belt paradigm.²⁰ In addition, repeated exposure to leg resistance force may enhance muscle activation of hip flexors, which may facilitate leg swing, but may have a modest effect on hip abductors, which are identified as key muscles in maintaining mediolateral balance of standing leg during walking.⁴⁰ As a result, we observed a greater increase in cadence but a smaller increase in step length because of modest change in single leg support time after resistance training.

To our knowledge, this is the first study to show the differences in walking functional gains in children with CP after robotic treadmill training with robotic resistance force versus assistance force. The functional gains obtained after robotic resistance treadmill training are comparable with, or even greater than, those obtained from previous studies using treadmill training. For instance, the functional gain in walking speed (ie, .15m/s, although <.17m/s, minimal clinically important difference)⁴¹ obtained after robotic resistance training was

comparable with, or greater than, that obtained after treadmill training with applied manual assistance force (.01-.07m/s), <u>42</u> or with robotic assistance force using the pediatric Lokomat^d (ie, .02m/s), <u>35</u> which is comparable with functional gains obtained after assistance training (ie, -.02m/s) and after robotic training using the GaitTrainer^e (ie, .12m/s). <u>43</u> Similarly, the functional gain in 6-minute walk distance obtained after resistance training (i.e., 81.2m, which is greater than <u>minimal clinically important difference</u>, i.e., 61.5m) was greater than that obtained after treadmill training with manual assistance (ie, -25.0 to -19.8m), <u>9</u>, <u>42</u> which is comparable with functional gains obtained after assistance training (ie, 13.9m) and after robotic training using the GaitTrainer (ie, 69m).

The results of this study may have some clinical applications for improving locomotor function in children with CP. For instance, to improve the efficacy of locomotor training, <u>physical therapists</u> may consider applying a resistance force to the legs and refrain from applying a manual assistance force (that is too large) to legs during locomotor training to increase the intensity and/or active involvement of children with CP.

Study limitations

This study has several limitations. For instance, the sample size was small because of the challenges of participant recruitment. In addition, the assessing physical therapists were not blinded to the group assignment, which may have potentially biased the results. We do not know whether a robotic resistance treadmill training paradigm is more effective than a conventional treadmill training paradigm, and we also do not know whether the cognitive abilities of individuals had an effect on the results. In addition, the reliability of GAITRite data from some low functional children with CP was relatively low,²⁵ which might affect the results. We also do not know whether the level of resistance/assistance load applied in this paradigm is optimized. Further studies are needed to optimize this resistance training paradigm.

Conclusions

Applying a resistance force to the legs during robotic treadmill training is more effective than applying an assistance force in improving walking function in children with CP. This suggests that active involvement of children with CP during locomotor training is crucial for improving the efficacy of treadmill training. In addition, repeated exposure to force perturbations induces a prolonged retention of improved stride length in children with CP.

Suppliers

- a. Woodway treadmills; WOODWAY USA, Inc.
- b. LabVIEW; National Instruments.
- c. GAITRite; CIR Systems Inc.
- d. Lokomat; Hocoma Inc, USA.
- e. Gait Trainer GT I; Reha-Stim, Berlin, Germany.

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