Marquette University e-Publications@Marquette

Mathematics, Statistics and Computer Science Faculty Research and Publications Mathematics, Statistics and Computer Science, Department of

8-1-2010

Noise Assumptions in Complex-Valued SENSE MR Image Reconstruction

Daniel B. Rowe Marquette University, daniel.rowe@marquette.edu

Iain P. Bruce Marquette University - Graduate Student

Noise Assumptions in Complex Valued SENSE MR Image Reconstruction. Presented at the 2010 Joint Statistical Meeting, sponsored by the American Statistical Association. Vancouver, Canada, August 4, 2010.

Noise Assumptions in Complex-Valued SENSE MR Image Reconstruction

Daniel B. Rowe, Ph.D.

(Joint with Iain P. Bruce, M.S.)

Associate Professor Department of Mathematics, Statistics, and Computer Science Marquette University



Adjunct Associate Professor Department of Biophysics Medical College of Wisconsin



August 4, 2010

Rowe, Marquette U

OUTLINE 1. Motivation

- 2. Background
- **3. Methods**
- 4. Results
- **5.** Discussion

Motivation

In MRI k-space for images is not measured instantaneously.

In parallel imaging, sub-sampled k-space points are measured in parallel and combined to form a single image.

Image and volume measurement time is decreased at the expense of increased image reconstruction difficulty and time.

The SENSE parallel imaging reconstruction technique utilizes a complex-valued least squares estimation process.

However, in SENSE the covariance is not properly modeled.

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999.

Background

In parallel imaging there is more than one receive coil.



Each coil measures a *k*-space array that is reconstructed into an aliased image then combined to form a single unaliased image.

Rowe, Marquette U

Background Image inverse Fourier Reconstruction for single coil.



Background

Each coil measures a *k*-space array that is reconstructed into an aliased image then combined to form a single image.

Rowe, Marquette U





Background

Each coil measures a *k*-space array that is reconstructed into an aliased image then combined to form a single image.



coil 2 coil 3 coil 2 coil 3





 \mathcal{V}_C

Methods The SENSE model for aliased voxel values from n coils is

$$\begin{array}{ll} a_{C} &=& S_{C} \quad v_{C} \quad + \quad \mathcal{E}_{C} \\ _{n \times 1} & & _{n \times A} \quad A \times 1 \end{array} \quad , \quad \mathcal{E}_{C} \sim CN(0, \Psi_{C}) \\ \end{array}$$
where for each voxel
$$\Psi_{C} = \Psi_{R} + i\Psi_{I}$$

 $\begin{array}{l} a_{C} \text{ is a vector of the } n \text{ complex-valued aliased voxel values} \\ v_{C} \text{ is a vector of the } A \text{ unaliased voxel values} \\ \end{array} \\ \begin{array}{l} a_{C} = a_{R} + ia_{I} \\ v_{C} = v_{R} + iv_{I} \\ \end{array} \\ \begin{array}{l} s_{C} \text{ is an } nxA \text{ matrix of complex-valued coil sensitivities} \\ S_{C} \text{ is a vector of the } n \text{ complex-valued error values} \\ \end{array} \\ \begin{array}{l} \varepsilon_{C} = \varepsilon_{R} + iS_{I} \\ \end{array} \\ \end{array}$

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999.

Methods The SENSE process



$$f(\varepsilon_{c}) = (2\pi)^{-n} \left| \Psi_{c} \right|^{-1} e^{-1/2\varepsilon_{c}^{H} \Psi_{c}^{-1}\varepsilon_{c}}, \quad H \text{ is trans$$

H is the conjugate transpose (Hermetian)

and for N_C coil measurements

$$f(a_{C}) = (2\pi)^{-n} |\Psi_{C}|^{-1} e^{-1/2(a_{C} - S_{C}v_{C})^{H} \Psi_{C}^{-1}(a_{C} - S_{C}v_{C})}$$

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999. Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956. Bruce and Rowe: In progress.

Rowe, Marquette U

Methods

From the distribution for the *n* coil measurements

$$f(a_{C}) = (2\pi)^{-n} |\Psi_{C}|^{-1} e^{-1/2(a_{C} - S_{C}v_{C})^{H} \Psi_{C}^{-1}(a_{C} - S_{C}v_{C})}$$

the voxel values can be estimated as

$$\nu_{C} = (S_{C}^{H} \Psi_{C}^{-1} S_{C})^{-1} S_{C}^{H} \Psi_{C}^{-1} a_{C}$$

with knowledge of S_C and Ψ_C .



Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999. Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956. Bruce and Rowe: In progress.

Methods

Instead of writing the model with complex numbers as

$$\begin{aligned} a_{C} &= S_{C} \quad v_{C} + \varepsilon_{C} \\ a_{\times 1} &= a_{X} A_{\times 1} + a_{X} A_{\times 1} \\ a_{C} &= a_{R} + ia_{I} \quad S_{C} = S_{R} + iS_{I} \quad v_{C} = v_{R} + iv_{I} \quad \varepsilon_{C} = \varepsilon_{R} + i\varepsilon_{I} \\ \text{ve can write the model using an isomorphism as} \\ a_{R} &= S \quad v_{R} + \varepsilon_{R} \\ a_{2n\times 1} &= a_{2n\times 2A} \sum_{2A\times 1} + a_{2n\times 1} \\ a &= \begin{pmatrix} a_{R} \\ a_{I} \end{pmatrix} \quad S = \begin{pmatrix} S_{R} & -S_{I} \\ S_{I} & S_{R} \end{pmatrix} \quad v = \begin{pmatrix} v_{R} \\ v_{I} \end{pmatrix} \quad \varepsilon = \begin{pmatrix} \varepsilon_{R} \\ \varepsilon_{I} \end{pmatrix} \end{aligned}$$

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999. Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956. Bruce and Rowe: In progress.

Rowe, Marquette U

Methods

Then the distribution for *n* coil measurements is

$$f(a) = (2\pi)^{-n} |\Psi_{SE}|^{-1/2} e^{-1/2(a-Sv)'\Psi_{SE}^{-1}(a-Sv)}$$

with

$$a = \begin{pmatrix} a_R \\ a_I \end{pmatrix} \qquad S = \begin{pmatrix} S_R & -S_I \\ S_I & S_R \end{pmatrix} \quad v = \begin{pmatrix} v_R \\ v_I \end{pmatrix} \qquad \varepsilon = \begin{pmatrix} \varepsilon_R \\ \varepsilon_I \end{pmatrix}$$

and the complex normal distribution imposes skew-symmetric

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix}$$

Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956. Bruce and Rowe: In progress.

Methods

The skew-symmetric covariance structure

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix} \quad \text{is incorrect.}$$

What this says is that cov(I, I) = cov(R, R)

and that cov(I, R) = -cov(R, I).

The proper covariance structure should be

$$\Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi_{RI}' & \Psi_I \end{pmatrix}$$

(SE for SENSE and SI for new covariance model SENSE-ITIVE)

Methods

Examine the difference between the two covariance structures

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix} \qquad \Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi'_{RI} & \Psi_I \end{pmatrix}$$

in the distribution

$$f(a) = (2\pi)^{-n} \left| \Psi_{SE/SI} \right|^{-1/2} e^{-1/2(a-Sv)' \Psi_{SE/SI}^{-1}(a-Sv)}$$

through estimates

$$v_{SE} = (S' \Psi_{SE}^{-1} S)^{-1} S' \Psi_{SE}^{-1} a$$
$$v_{SI} = (S' \Psi_{SI}^{-1} S)^{-1} S' \Psi_{SI}^{-1} a$$

Rowe, Marquette U

Results Noiseless multi-coil spatial frequency arrays are with



coil 2 coil 3 Bruce and Rowe: In progress.

Rowe, Marquette U

Results Magnitu<u>de</u>









Rowe, Marquette U

Results Phase





SENSE-ITIVE

Discussion The SENSE image reconstruction method was described.

The SENSE reconstruction written with an isomorphism.

The covariance structure of complex SENSE described.

New SENSE-ITIVE method described with proper covariance.

Results of SENSE & SENSE-ITIVE reconstruction presented.

Ghosting present in SENSE magnitude and phase images.

Better reconstruction in SENSE-ITIVE reconstruction especially phase used for complex-valued time series activation.

Thank You

Acknowledgements: Iain Bruce, Marquette University Muge Karaman, Marquette University