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# Nanoscale structure and mechanical properties of a Soft Material

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# **Nanoscale structure and mechanical properties of a Soft Material**

by

Hossein Salahshoor Pirsoltan

A Thesis

of the

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Civil Engineering

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APPROVED:

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## Abstract

Recently, hydrogel have found to be promising biomaterials since their porous structure and hydrophilicity enables them to absorb a large amount of water. In this study the role of water on the mechanical properties of hydrogel are studied using *ab-initio* molecular dynamics (MD) and coarse-grained simulations. Condensed-Phased Optimized Molecular Potential (COMPASS) and MARTINI force fields are used in the all-atom atomistic models and coarse-grained simulations, respectively. The crosslinking process is modeled using a novel approach by cyclic NPT and NVT simulations starting from a high temperature, cooling down to a lower temperature to model the curing process. Radial distribution functions for different water contents (20%, 40%, 60% and 80%) have shown the crosslinks atoms are more hydrophilic than the other atoms. Diffusion coefficients are quantified in different water contents and the effect of crosslinking density on the water diffusion is studied. Elasticity parameters are computed by constant strain energy minimization in mechanical deformation simulations. It is shown that an increase in the water content results in a decrease in the elastic. Finally, continuum hyper elastic model of contact lens is studied for three different loading scenarios using Finite Element Model.

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# 1. Introduction

## 1.1. Hydrogel

Hydrogels have extensive applications in engineering due to their hydrophilic and biocompatible nature (Wichterle and Lim 1960). They are three dimensionally crosslinked polymeric networks that can absorb and retain huge amounts of water, even up to thousand times of the network's dry weight (Harland et al, 1992). Since early 1960s that Wichterle and Lim used hydrogels as biomaterials, significant efforts have been devoted to use hydrogels in the biomedical and pharmaceutical applications (Peppas *et al.* 2000, Langer and Peppas 2003), especially for drug delivery (Peppas 1997) and tissue engineering applications (Lee and Mooney 2001), which are due to the polymer's excellent biocompatibility and smart stimulus-response properties. In order to comply with rapidly increasing demands in medical treatment and health care, a large variety of hydrogels have been made and tested so far on the basis of recent progresses in organic synthesis techniques that can realize exactly-tailored molecular architectures according to the suggested design. Although these materials have had significant contributions to medical treatment and health care, there are still strong demands for gels with improved properties such as higher biocompatibility, more favorable mechanical properties, sensitivity, and so on. For instance, relatively good mechanical stability and high oxygen permeability is required for use in contact lenses, which is one of the earliest biomedical applications of hydrogels, according to Friends *et al.* 1995. As another example, integrating hydrogels as cartilage replacement requires high toughness. Articular cartilage is a composite with collagen fibrils reinforcing a proteoglycan gel matrix (Peppas *et al.*2006, Wainwright *et al.* 1986). The extension to break of cartilage is approximately 100%. In contrast, most synthetic gels have a very low toughness when fully swollen (Calvert 2009). The need to design hydrogels for other promising applications such as

wound-healing bioadhesives, artificial kidney membranes, artificial skin, maxillofacial, sexual organ reconstruction materials, and drug delivery vehicles is getting critical. There are various approaches to improve properties of hydrogels: to redesign given synthetic materials, to hybridize synthetic materials with biomaterials, and to modify given biomaterials. In order to accomplish any of these, molecular mechanisms leading to physical properties of each class of biomaterials need to be understood. Thus, we will focus on the understanding of the molecular mechanisms at an atomic/molecular level to provide valuable information to design new materials using computational approaches to obtain various desirable properties.

## **1.2. Atomistic Modeling**

Computational science is one of the most promising and rapidly expanding branches of science. Computers provide the opportunity to model different materials and study their chemical and physical properties. Prior to the advent of computational approaches, various properties could only be predicted using theoretical approaches that provided a crude description of materials. Computer simulations, however, have provided useful information for problems in various fields such as biology, chemistry, and physics, as well as economics and psychology after it played an essential role in developing nuclear weapons and code breaking in the early 1950s (Frenkel and Smith 2001), demonstrating its various capabilities. High performance computers have since accelerated the growth of computational methods in almost every field of science and technology.

Among various computer simulation methods, molecular and ab-initio simulation methods have provided direct routes from the microscopic structural details of materials to the

macroscopic properties. The use of molecular simulation methods should be dependent on the properties of interest due to the multi-scale characteristics of materials systems for given distance and time scale, as shown in Figure 1 (Lee 2011).

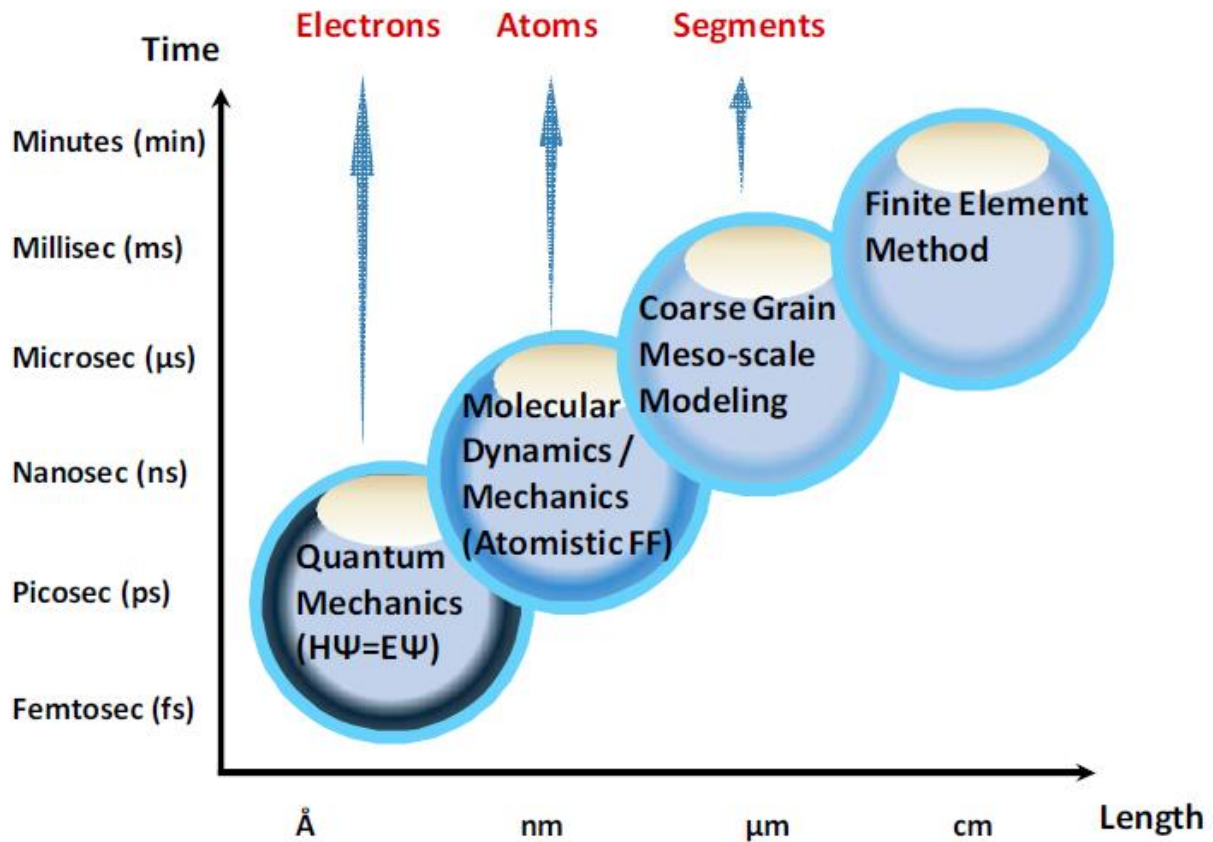


Figure 1. The hierarchical multi-scale paradigm in molecular simulation

In essence, the electronic structure of materials dictates their properties. Thus, bottom-up approaches, all away from the atomic or even sub-atomic to the macroscopic structure give a better insight into the mechanisms affecting different properties of materials. In other words, quantum mechanics (QM) simulations should be used to obtain useful information on electronic properties of materials by calculating electronic wave functions up to several Angstroms and

picoseconds. Since QM methods determine state of all electrons, QM results in accurate geometries and energies of the system. Since, QM simulations are computationally expensive and nearly impractical given today's technology for systems containing over several hundreds and thousands of atoms, a different approach is considered.

Quantum mechanics can be approximated with molecular mechanics (MM) and molecular dynamics (MD) by averaging over the electron wave functions. This method allows us to investigate the structure and energetic of larger systems with up to hundred nanometers in dimension or even micron scales. In MM or MD, the atoms are considered as soft spheres bonded to each other with springs. Energies and forces derived from this approximation can be used in classical physics formulas to obtain dynamic trajectories, conformations or optimized geometries. MD simulations allow for the study of comparatively large systems and have emerged as an effective tool for the characterization of the mechanical and thermal behavior of nanostructures.

Further up in the hierarchy, lie simulation methods requiring even more crude approximations to maintain computational feasibility for systems operating on longer time and distance. Since polymeric systems are complex, it is still not feasible to completely describe them using MD technique. Chapter two discusses MD approach in more detail.

MD simulations have been extensively employed to characterize the molecular structure of biomaterials. It should be noted however, that there have been only a limited number of MD simulation studies on hydrogel systems.

Tamai and Tanaka carried out MD simulations for hydrogel models of poly(vinyl alcohol), poly(vinyl methyl ether), and poly(N-isopropylacrylamide) hydrogels to study polymer-water

interaction in hydrogels by analyzing the hydrogen bond structure and dynamics. The range for degree of polymerization (DP) of the polymer chain is 11-161 and the range for number of water molecules is 5 to 215. They have also performed MD simulations of poly(vinyl alcohol) with 81 or 161 DP and pure water over a wide temperature range of 150-400 K to study effects of polymer chains on structure and dynamics of supercooled water in hydrogels. They used 150 to 216 water molecules and a simulation time range of 1 to 40 ns.

Oldiges *et al.* have simulated poly(acrylamide) hydrogels to investigate the local structural and mobility effects between dilute aqueous acetonitrile solution, water, and crosslinked poly(acrylamide). They used 12 to 59 DP of acrylamide molecules with the range of 300 to 390 for water molecules.

Recently, Jang *et al.* have also applied full-atomistic simulations to hydrogel systems made of poly(ethylene glycol) and poly(acrylic acid) double network to investigate its structure and mechanical properties. They built a three dimensional nanostructured interpenetrating network of poly(ethylene glycol) and poly(acrylic acid) in presence of water molecules to find a network structure that can achieve excellent mechanical properties to replace human cornea (Lee 2011). However, there is not much systematic investigation available in the literature. Thus, it is critical to study the equilibrated structure, mechanical properties, and transport properties of hydrogels with various water contents and the effects of water percentage on the mechanical properties of hydrogel. The water content of a hydrogel can be described as a percentage of the weight of water (Dumitriu 2002) as follows

$$\text{Water content (\%)} = (\text{weight of water} / (\text{weight of water} + \text{weight of dry gel})) \times 100$$

The water content of hydrogel plays an important role in the use of hydrogels in biomedical applications, because it affects the solute diffusion and the optical and mechanical properties of



the hydrogels. In general, the low water content of the hydrogel ranges from 20 to 50%. A hydrogel with over 90% water content is considered a super-absorbent hydrogel. For instance, the U.S. Food and Drug Administration (FDA) classifies the water content of the hydrogel contact lenses as low water content ( $>50\%$ ) and high water content ( $<50\%$ ).

### **1.3. Objectives**

The objective of this research is to understand the structure-property relationships of hydrogels using MD simulations intended to create new material design guidelines for the construction of fine-tuned nanostructured hydrogel systems. The detailed research objectives are as follows:

1. Defining crosslinking protocols for hydrogels: Since hydrogels are crosslinked polymers and crosslinking process needs bond creation, a crosslinking protocol needs to be defined.
2. Investigating the role of water molecules on the equilibrated structure
3. Investigating the effect of water on the mechanical properties.
4. Proposing a coarse-grained model for the hydrogel, which allows for longer simulations.
5. Contact lens, as a remarkable application of hydrogels, is modeled in continuum scale using Finite Element Method.

## Chapter 2: Computational Backgrounds

### 2.1. Molecular Dynamics Simulations

Molecular Dynamics (MD) simulations study the evolution of a system throughout the time. Molecules in the real world are constantly fluctuating and changing conformation to respond to external environment. MD simulations consist of the numerical solution of classical equations of motion to determine the positions and velocities of atoms at finite temperatures. At a given temperature, initial velocity of a particle is usually estimated by a random distribution (Maxwell-Boltzmann distribution). Once an initial velocity is prescribed, it is updated using the calculated accelerations. MD techniques usually use Cartesian coordinates, resulting in  $3N$  degrees of freedom for  $N$  particles in the system. Thus, the forces, velocities, and accelerations are independently obtained at each degree of freedom for each particle. The total force,  $F_x$ , in the  $x$  direction is the opposite of the gradient

$$F_x = -\frac{\partial}{\partial x} V \quad (2-1)$$

where  $V$  is the potential energy and  $x$  is the coordinate in  $x$  direction. Newton's equation of motion is used to calculate the acceleration.

$$m_i \ddot{x} = F_x \quad (2-2)$$

where  $m_i$  is the mass of particle  $i$ .

#### 2.1.1. Verlet Algorithm

After computing all the forces between particles, we can update velocities from accelerations by integrating Newton's equation of motion. Different numerical algorithms have been developed

for integrating Newton's equation of motion, such as Verlet algorithm (Verlet 1967), leap-frog algorithm (Potter 1973), velocity-verlet algorithm (Swope 1982).

Verlet, initially used method of integrating the equations of motion using Taylor series expansion which uses the positions  $r(t)$ , accelerations  $a(t)$ , and the previous position  $r(t-\delta t)$  to predict new positions  $r(t+\delta t)$ . Modifications to the basic Verlet algorithm have been proposed by Potter. In this scheme, so called leap frog scheme, the current position  $r(t)$  and accelerations  $a(t)$  with the midstep velocities  $v(t-(\delta t/2))$  are used to obtain the next mid-step velocities  $v(t+(\delta t/2))$ . The velocities leap over the positions and the positions leap over the velocities. Swope *et al.* introduced the velocity-Verlet algorithm, because both the basic Verlet and leap frog algorithms do not describe the velocities in a satisfactory manner. The velocity-Verlet algorithm needs to store positions, accelerations, and velocities at the same time to minimize round-off error. This algorithm takes the following form

$$r(t + \delta t) = r(t) + \delta t v(t) + \frac{1}{2} \delta t^2 a(t) \quad (2-3)$$

$$v(t + \delta t) = v(t) + \frac{1}{2} \delta t [a(t) + a(t + \delta t)] \quad (2-4)$$

The new positions at time  $t+\delta t$  are calculated using equations 2 and 3 and the velocities at mid-step  $v(t+(\delta t/2))$  are calculated using Equation 4.

$$v\left(t + \frac{1}{2} \delta t\right) = v(t) + \frac{1}{2} \delta t a(t) \quad (2-5)$$

The forces and accelerations at time  $t+ \delta t$  are then calculated, and the velocity move is completed as follows (Equation 6):

$$v(t + \delta t) = v\left(t + \frac{1}{2} \delta t\right) + \frac{1}{2} \delta t a(t + \delta t) \quad (2-6)$$

### 2.1.2. Ensembles

Ensemble is an assembly of all possible microstates, defined by given constraints. For example, a simple way to create a thermodynamic ensemble is to maintain a constant total energy, volume, and number of particles in a system to produce a microcanonical (NVE) ensemble of conformations. In the same way, canonical (NVT) ensemble assembly of all states with fixed number of particles, volume, and temperature and isobaric-isothermal (NPT) ensemble fixed number of particles, pressure, and temperature. Once ensemble is formed, relative free energies, average densities, and other thermodynamic properties can be calculated.

### 2.1.3. Energy Minimization

Energy minimization is typically performed by perturbing atoms in order to reduce the net force applied to atoms by the force field potentials. Since a minimized structure usually has a well-mannered geometry and rarely has large forces on any atom, it is preferred to start a molecular dynamics simulation with a minimized structure. Energy minimization can be carried out in Cartesian coordinates by optimizing in 3N-dimensional space where N is the number of particles in the system. The path chosen is the gradient,  $\nabla$ , as follows

$$\nabla_x = \frac{\partial}{\partial x} V \quad (2-7)$$

Each Cartesian component, x, of the gradient is the derivative of the potential energy of the force field with respect to that component.

Figure 2 shows a generalized schematic structure of a MD simulation (Buyukozturk 2011).

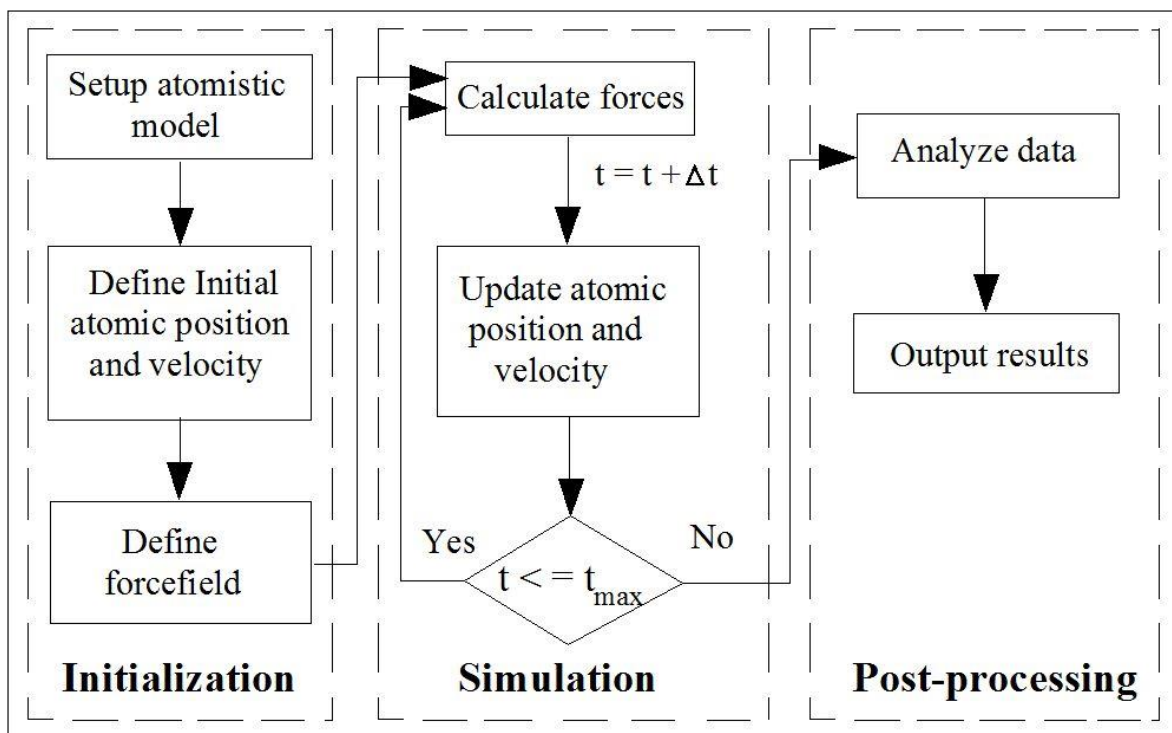


Figure 2. Numerical Approach for MD Simulation.

#### 2.1.4. Force Field

Force field plays a crucial role in a MD simulation. It contains the main set of parameters (approximations) of the molecular system examined. Based on the force fields, the forces are calculated which are necessary to calculate the new atomic positions. Basically, there are three different categories of force fields: Empirical, Semi-empirical and quantum-based force fields. Empirical potentials are forms with parameters that are fitted to experimental data and were commonly used in past. On the other hand, in the ab-initio based potentials the parameters are calculated by electronic structure calculations. Due to efforts to develop high quality force fields, accurate force fields are available for many organic, inorganic and biological systems. For instance, DREIDING (Mayo et al 1990) or CVFF (Dauber-Osguthorpe et al 1988 and Maple et

al 1988) are well-known generic force fields and CHARMM (Brooks et al 1983) or AMBER (Weiner et al 1984 and Weiner et al 1986) are well developed force fields to describe biological systems. The force field used in the all-atom MD simulations in this study is Condensed-Phased Optimized Molecular Potential (COMPASS) developed by Sun et al 1998, which is explained in detail in Chapter 3. In this section, we only mention the overall structure of all force field types. The total energy is expressed by force field for a molecular system as a sum of valence (or bonded) interactions and nonbonded interactions

$$E_{\text{Total}} = E_{\text{valence}} + E_{\text{nonbonded}} \quad (2-7)$$

The valence interactions can be broken down into bond stretch, bond angle bending, dihedral angle torsion, and inversion term

$$E_{\text{valence}} = E_{\text{bond}} + E_{\text{angle}} + E_{\text{torsion}} + E_{\text{inversion}} \quad (2-8)$$

The first valence term in a force field is a bond stretch term. The simplest form for it is harmonic bond potential:

$$E_b = \frac{1}{2} K_b (R - R_0)^2 \quad (2-9)$$

where  $R$  is the bond distance in units of Angstrom ( $\text{A}^\circ$ ),  $R_0$  is the equilibrium bond distance and  $K_b$  is the force constant in unit of  $(\text{kcal/mol})/\text{A}^{\circ 2}$ . In harmonic bond potential, the bond is considered as a spring with equilibrium bond length of  $R_0$  and spring constant  $K_b$ . Also, there are other forms for expressing stretch bond potential, which can also capture the  $R=\infty$  (interpreted as a broken bond). Morse potential is one of the most famous potentials for this purpose:

$$E_b = D_0 [e^{-\alpha(R-R_0)} - 1]^2, \quad \alpha = \sqrt{K_b / 2D_0} \quad (2-10)$$

$R_0$  and  $K_b$  are the same as in harmonic bond potential.  $D_0$  is the bond energy in units of kcal/mol and  $\alpha$  is the Morse scaling parameter. The scaling parameter allows the bond energy to go to  $D_0$  for large  $R$ .

The second valence term in a force field is a bond angle bend as illustrated in Figure 3. The most basic and common bond angle form is a harmonic potential

$$E_a = \frac{1}{2} K_\theta (\theta - \theta_0)^2 \quad (2-11)$$

where  $\theta$ ,  $\theta_0$  and  $K_\theta$  are the bond angle, equilibrium bond angle and the force constant in units of (kcal/mol)/A<sup>2</sup>.

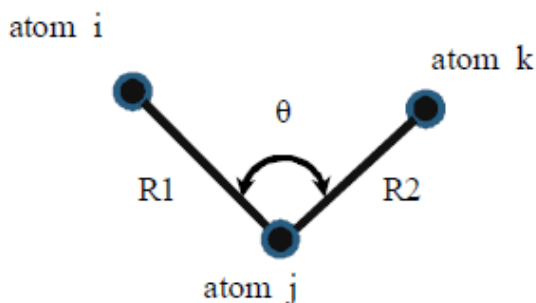


Figure 3. Bond Angle Bend.

The third valence term in a force field is a dihedral angle torsion term. Given any two bonds  $ij$  and  $kl$  attached to a bond  $jk$ , the dihedral angle is defined as the angle between the  $ijk$  plane and the  $jkl$  plane as illustrated in Figure 4. The torsional expression is usually defined as below:

$$E_\phi = \sum_{n=1}^p \frac{1}{2} K_{\phi,n} [1 - d \cos(n\phi)] \quad (2-12)$$

where each  $K_{\theta,n}$  is one half the rotational barrier in units of kcal/mol,  $n=1,2,3,4,5,6$  is the periodicity of the potential and  $d=\pm 1$  is the phase factor. For  $d=+1$ , the conformation is in the minimum value while for the  $d=-1$ , it is in the maximum value.

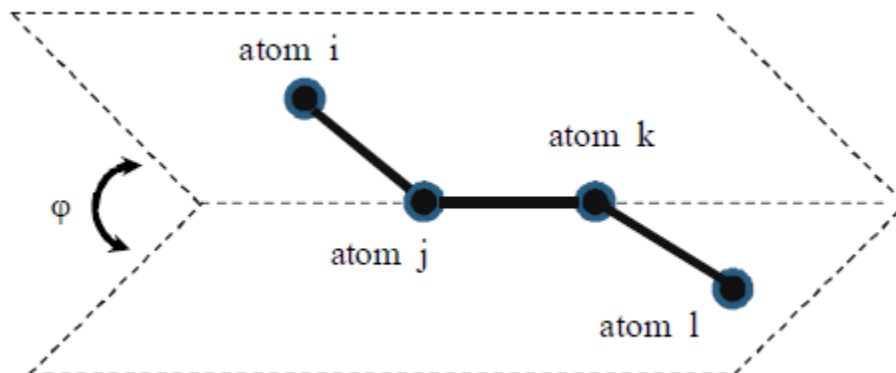


Figure 4. Torsion Angle.

The last valence term is the inversion. Given an atom  $i$  having three distinct bonds  $ij$ ,  $ik$  and  $il$ , the force field may contain terms affecting the energy involved in planarizing the center atom  $i$  as shown in Figure 5. The inversion term can be expressed as in following

$$E_{\omega} = \frac{1}{2} C (\cos \omega - \cos \omega_0)^2, \quad K_{\omega} = C \sin^2 \omega_0 \quad (2-13)$$

where  $K_{\omega}$  is the force constant in unit of kcal/mol and  $\omega$  is the angle between the  $il$  axis and the  $ijk$  plane. If  $\omega_0 = 0^\circ$ , the potential term has a minimum for the planar structure.



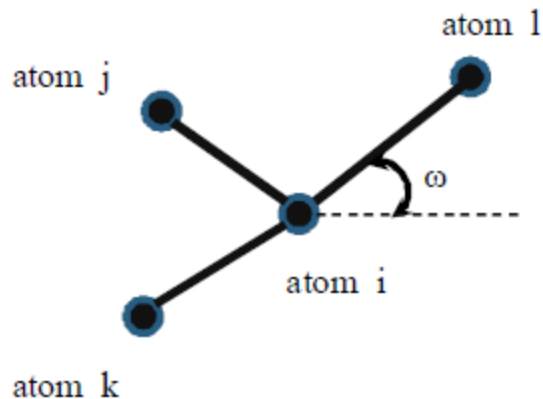


Figure 5. Scheme of Inversion.

The nonbonded interactions consist of electrostatic, van der Waals and hydrogen bond term

$$E_{\text{nonbonded}} = E_{\text{electrostatic}} + E_{\text{vdW}} + E_{\text{hbond}} \quad (2-14)$$

The first term is electrostatic interactions, which is important to describe packing of organic molecules and the structure of inorganic systems. The total electrostatic interaction energy can be calculated by evaluating the Coulombic interaction between each pair of atoms in the system

$$E_{\text{electrostatic}} = C_0 \sum \frac{q_i q_j}{\epsilon r_{ij}} \quad (2-15)$$

where  $C_0 = 332.0637$  is a conversion factor giving  $E_{\text{electrostatic}}$  in kcal/mol,  $q_i$  and  $q_j$  are the charges in electron units,  $\epsilon$  is the dielectric constant (1 for vacuum),  $r_{ij}$  is the distance between atom  $i$  and  $j$  in units of  $\text{Å}$ .

The second nonbonded term is the van der Waals interactions. The van der Waals interactions contain the attractive and repulsive forces between molecules. The most common form is the Lennard-Jones 12-6 potential

$$E_{\text{vdW(LJ12-6)}} = D_0 \left[ \left( \frac{R_0}{R} \right)^{12} - 2 \left( \frac{R_0}{R} \right)^6 \right] \quad (2-16)$$

where  $D_0$  is well depth and  $R_0$  is the equilibrium distance (in  $\text{Å}$ ). The main drawback of this form is that it requires only two parameters,  $D_0$  and  $R_0$ . For  $R < R_0$ , the Lennard-Jones potential may be too repulsive at short ranges. A more reasonable form, the exponential-6 potential and Morse potential (Equations 16 and 17, respectively) allows three parameters to describe the inner wall (short ranges) more realistically.

$$E_{vdW(\text{exp-6})} = D_0 \left\{ \left[ \left( \frac{6}{\zeta - 6} \right) \exp^{\zeta \left( 1 - \frac{R}{R_0} \right)} \right] - \left[ \left( \frac{6}{\zeta - 6} \right) \left( \frac{R_0}{R} \right)^6 \right] \right\} \quad (2-17)$$

$$E_{vdW(\text{Morse})} = D_0 (\chi^2 - 2\chi), \quad \chi = \exp \left[ -\frac{\gamma}{2} \left( \frac{R}{R_0} - 1 \right) \right] \quad (2-18)$$

The last nonbonded term in a force field is H bond. Some force fields like CHARMM and DREIDING use a hydrogen bond potential to describe the interaction between atoms involved in hydrogen bonds. The general form of hydrogen bond is Lennard-Jones 10-12 potential, as expressed below:

$$E_{\text{hbond}(LJ12-10)} = D \left[ 5 \left( \frac{R_0}{R} \right)^{12} - 6 \left( \frac{R_0}{R} \right)^{10} \right] \quad (2-19)$$

where  $D_0$  is the hydrogen bond strength in kcal/mol and  $R_0$  is equilibrium distance in  $\text{Å}$  (Lee 2011).

### **Chapter 3: Atomistic Modeling of Crosslinked Polymers**

Crosslinked polymers are one of the main types of compounds that are usually consisted of an epoxy group and a curing agent. They exhibit excellent properties, i.e. high modulus and fracture strength, low creep and high-temperature resistance and thus widely used as coatings, adhesives, composites, etc. In order to design and manipulate these properties, we need to gain a better understanding of the molecular structure. MD simulations can shed light on the atomic structure of the crosslinked polymers and how the macro properties are affected by the microstructure. For this purpose, we need a crosslinking protocol that can be used to model the crosslinked polymers. In this thesis, a crosslinking protocol is described in detail which is proposed by Wu and Xu 2006.

This crosslinking algorithm is performed on a set of resin epoxies and the results are validated by experiment. The epoxy system used in this study is based on Diglycidyl Ether of Bisphenol-A (DGEBA), which is commercially known as EPON 828. The curing agent used with the epoxy (DGEBA) is Aminoethyl Piperazine (AEP), commercially known as EPICURE 3200, as shown in Figure 6.

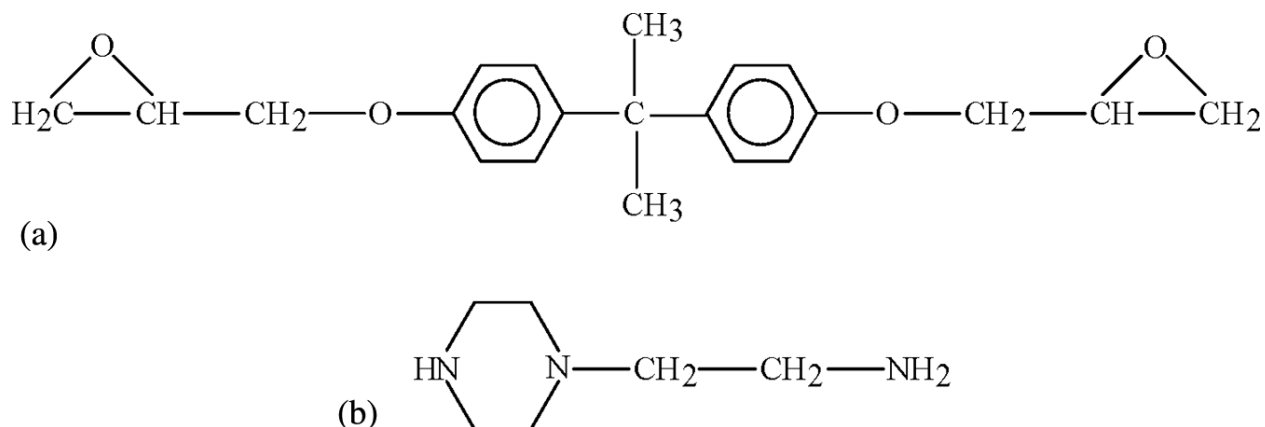


Figure 6. The chemical structure of: (a) Diglycidyl Ether of Bisphenol-A (DGEBA); (b) Aminoethyl Piperazine (AEP).

### 3.1. Crosslinking Protocol

To facilitate the procedure, four basic assumptions are implemented.

1. Epoxy resin component is less mobile than curing agent component.
2. Primary amine hydrogen has the same reactivity as the secondary amine hydrogen.
3. The etherification reactions can be neglected.
4. The reactions are diffusion-controlled.

According to these assumptions, the following simulation procedure was employed:

Step 1: Two two-dimensional (2D) active models for small molecules DGEBA and AEP are constructed on an atom by atom basis. Energy minimization was performed on these two molecules to achieve reasonable three-dimensional model. Partial charges of atoms were assigned using Qeq method (Rappe and Goddard 1991). hydrogens on end groups are removed and “reactive” molecular segments with the carbon and nitrogen end groups are left.

Step 2: An amorphous epoxy model was constructed by using self-avoiding random walk method of Theodorou and Suter, 1985. The 3D unit cell was built with 15 resin molecules and 10

agents. The molecules were packed into the cell with a density of  $1.16 \text{ g/cm}^3$ . Periodic Boundary Conditions (PBC) are imposed to the system to eliminate the boundary effects.

Step 3: An energy minimization is performed for 1000 steps. Then a cyclic isothermal (NVT) and isothermal-isobaric (NPT) is performed in the room temperature (298 K) to relax the initial unit cell model. The resulting physical mixture was analyzed in order to identify the reactive sites in close proximity. One of the reactive site's carbons in DGEBA was first chosen. Then a search of nearby reactive site's nitrogen in AEP is conducted. The reaction occurs between a pair of such reactive sites when their distance is within a reaction cutoff distance of  $4 \text{ \AA}$ .

Step 4: The temperature is raised to 500K and then the system is further cooled down by a rate of  $100 \text{ K}/100 \text{ ps}$ . At each step, NVT and NPT dynamic simulations are performed. The time length of both NVT and NPT simulations are 100ps. Then the system is checked for the distance between the reactive sites and if they are closer than the cutoff distance, bonds are created.

Step 5: The cooling down process is repeated (Step 4) and at each step, the reactive site's distances are measured. This process is repeated until the temperature reaches the initial room temperature. The time step for all the dynamic simulations are assumed as 1 fs.

Crosslinking protocol is then applied to the unit cell, elastic properties of the systems are studied through a uniaxial deformation. The Young Modulus of the polymer was computed performing a dynamic simulation, while applying a force of  $0.5 \text{ kcal/mol/\AA}$ . This force was exerted to the system by applying a strain amplitude of 0.003 to the cell. Drieding (Mayo et al 1990) and Condensed-Phased Optimized Molecular Potential (COMPASS) (Sun 1998) force-fields are among the most common force-fields in simulations of epoxy polymers. They have been previously used to study the mechanical properties of epoxy polymers (Wu and Xu 2006,

Grujicic et al 2007, Lu and Dunn 2010). Both force-fields were used in this study and the results are presented and compared in the proceeding section.

### **3.2. Results**

Molecular modeling of the polymer was performed by the methodology prescribed earlier. The temperature of the system was initially raised to 500K and then, the system was cooled down to room temperature with a rate of 100 K/20 ps. The cyclic NVT and NPT simulations were performed at each cooling step, which helped the system to relax and reach to its minimum energy configuration. Using this procedure, the bonds between the epoxy and the agents were established through the reactive sites. COMPASS and DRIEDING force-fields have been previously used to study mechanical properties of epoxies. In this study, we have used both force-fields to model the DGEBA/AEP polymer and derive the mechanical properties. The results in each case are compared with experimental values.

Once the molecules have been placed within the super cell, a series of alternating MD simulations and static energy minimizations (molecular mechanics simulations) were used to establish the equilibrated molecular structure at the corresponding density. The molecular structures were gradually equilibrated to minimize any residual stresses in the model. After constructing the super cell and a preliminary dynamics simulation, the second step was initiated to simulate the crosslinking procedure. 20,000 time steps of NVT simulations were performed at room temperature (298 K). Afterwards, the system's temperature was gradually raised to 500 K. It can be observed that after relaxing the system in the 500 K (third simulation) the Young's

Modulus values decrease as illustrated in Figure 7. This process was repeated for the temperatures at 400K and 300K.

The first step to verify the mechanical properties is to compute the elastic properties at nano-scale. In order to calculate the components of the elastic stiffness matrix,  $C_{ij}$ , predefined strain was applied to the polymer and virial stresses  $\sigma_{ij}$  were computed. At each step of the model, cyclic NVT and NPT simulations at different temperatures were performed and the elastic constants,  $C_{ij}$ , were derived using the second derivative of potential energy with respect to strain.

$$C_{ij} = \frac{1}{V} \frac{\partial^2 u}{\partial \varepsilon_i \partial \varepsilon_j} = \frac{\partial \sigma_i}{\partial \varepsilon_j} \quad (3-1)$$

The stiffness matrix is derived as below:

$$\begin{pmatrix} 9.5541 & 5.7885 & 4.6630 & -1.3357 & 0.9755 & 0.1614 \\ 5.7885 & 1.2595 & 3.2319 & -1.6605 & -0.7725 & -0.8707 \\ 4.6630 & 3.2319 & 5.5935 & -0.0736 & -0.3619 & 1.4038 \\ -1.3357 & -1.6605 & -0.0736 & 1.4437 & 0.3329 & 0.5144 \\ 0.9755 & -0.7725 & -0.3619 & 0.3329 & 0.5757 & -1.0205 \\ 0.1614 & -0.8707 & 1.4038 & 0.5144 & -1.0205 & 0.8290 \end{pmatrix}$$

Figure 7 presents the results for COMPASS force-field and DRIEDING force-field. The glass transition temperature,  $T_g$ , of the DGEBA/AEP polymer is about 388 K (Garcia et al 2011). Hence, the sudden raise of the temperature beyond the polymer's  $T_g$  will impose different mechanical behavior. The fourth step is dynamic and relaxation simulations at 400 K. Accordingly, some fluctuations in total energy and Young's Modulus of the polymer (in comparison with experiment) were observed in the fourth step of the simulations. Generally, at temperatures close to the  $T_g$ , the behavior of the system needs to be simulated more accurately

with a different approach. In terms of mechanical behavior, the material is in a transition state which leads to these fluctuations. Hence, these fluctuations were expected and were not considered in this study.

In the last step the temperature was set back to the room temperature. There is a remarkable difference observed between the Young's modulus in second and fifth step which were both performed at the room temperature. This difference clearly shows the effect of the crosslinking process in the mechanical behavior of the polymer, Figure 7.

Figure 7 present the computed Young's modulus as a function of the simulations step for both COMPASS and DREIDING force field. The DREIDING force field shows fewer fluctuations but the results are significantly different from the experimental data. Meanwhile, the computed Young's modulus using the COMPASS force field approached to the experimental values as the simulation progressed. It is also clear from these results that the DREIDING force field is not suitable for modeling cross-linking process in the cross-linked epoxy studied here, since the Young's modulus does not significantly change as the simulation progresses.

Using COMPASS force field, the final computed Young Modulus is about 2.31 GPa. The experimental data (Grujicic et al 2007) show the Young's Modulus of DGEBA/AEP polymer is in the range of 2.7-2.9 GPa. Hence, the suggested simulation process is capable of modeling the mechanical properties of cross-linked polymers.



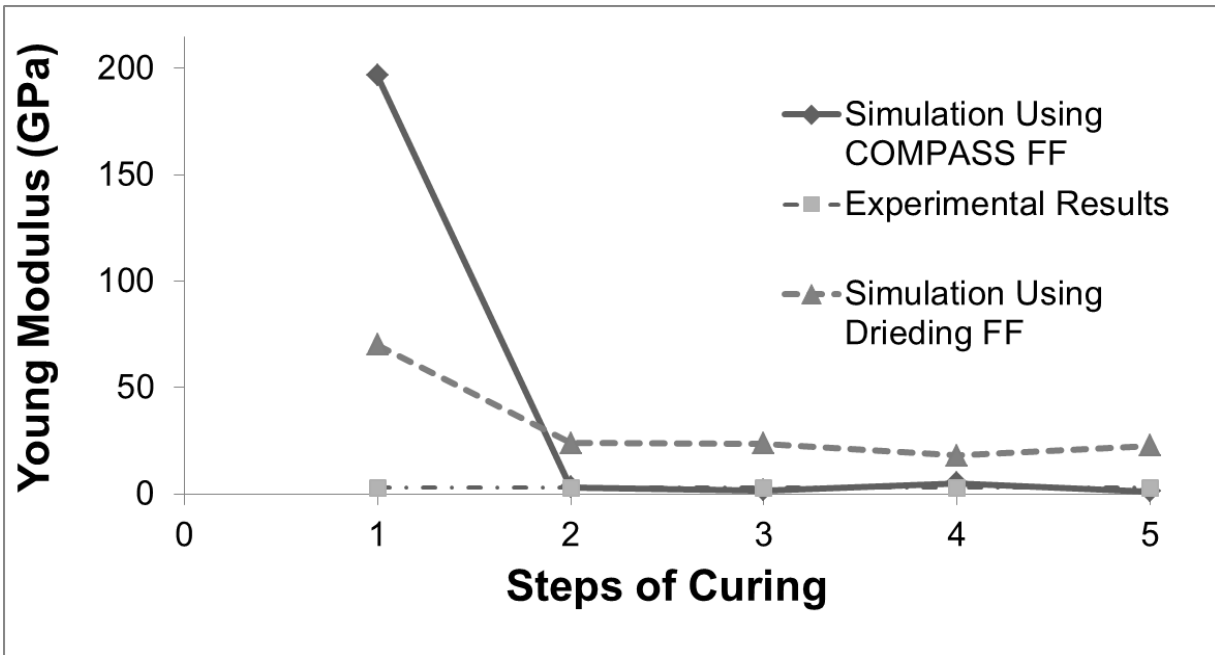


Figure 7. Variation of epoxy Young's modulus as the simulations of curing process progresses using Drieding and COMPASS force-fields. The thermal step for cross-linking is 100 K from 298 raised to 500 and cooled back to 298 again.

## Chapter 4: All-Atom Molecular Dynamics Simulation

### 4.1. Introduction

Hydrogels are three-dimensionally crosslinked polymer networks that can absorb and retain large amount of water, even up to thousands of their dry weight (Lowman et al 1999 and Hoffman 2012). They do not dissolve in water due to the presence of covalent bonds in the crosslinks zones. Among different properties of hydrogels, we are interested in the mechanical properties. Toughness and strength are required for many functional applications of gels.

Molecular Dynamics (MD) simulations have been employed to study various properties of hydrogels including the equilibrated structure, mechanical properties, diffusivity of water and ions. Jang *et al.* have studied mechanical properties of double network (DN) hydrogels. They obtained stress-strain curves for DN hydrogels by applying uniaxial deformation up to 300%. Lee *et al.* have studied the structure and mechanical properties of crosslinked hydrogels in both blocky and random hydrogels. E. Chiessi *et al.* have studied dynamics of polymer and water in hydrogels. Swelling of hydrogels is one of the most characteristic properties of hydrogels which occurs in an aqueous solution by absorbing the solvent. This process is influenced by many factors. J. Walter *et al.* have studied swelling behavior of hydrogels by proposing a realistic MD model of hydrogels obtained by the experiments on freeze-dried hydrogel. Also, Y. Wu. *et al.* focused on the diffusivity of water and ions in hydrogels. They have shown in their studies that by increasing the crosslinking density, the diffusion coefficients decrease.

In this study, a novel method is applied to model the crosslinking process and studying mechanical properties of hydrogels using molecular dynamics simulations. Stiffness matrices

and Elastic Modulus is calculated by applying a uniaxial strain to the system. The simulation details are presented in the next section.

## 4.2. Simulation Details

### 4.2.1. Model Construction

The epoxy and curing agent used for this study are Polyethylene glycol diglycidyl ether (PEGDGE) and the Jeffamine which is poly-oxy-alkylene-amines, respectively (see Figure 1). The chemical structure of the PEGDGE and Jeffamine are built separately, and the end hydrogen atoms are removed to provide reactive atom sites at the end groups, where the crosslinks will form. The two polymer molecules are then packed into an amorphous unit cell which is constructed using self-avoiding random walk method of Theodorou and Suter 1985. The unit cell is built with a PEGDGE:Jeffamine ratio of 1 to 4, having a density of  $1.086 \text{ g/cm}^3$ . Also, the water molecule is packed into the system to reach different values for volume percent of water. Five different systems are modeled containing 0, 20, 40, 60 and 80 wt%.

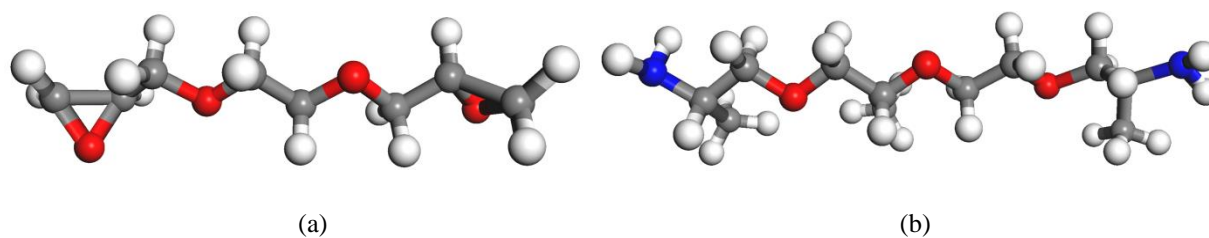


Figure 8. Chemical structure of epoxy and curing agent with oxygen, nitrogen, carbon and hydrogen as red, blue, grey and white respectively: (a) Polyethylene glycol diglycidyl ether (PEGDGE); (b) polyoxyalkyleneamine (Jeffamine).

#### 4.2.2. Crosslinking process

Conventional MD is not capable of modeling the crosslinking process which involves formation and breaking of bonds. On the other hand, with the present computational resources, sophisticated electronic structure calculation methods, such as *ab-initio* method, are very costly and impractical, if not impossible, for macromolecules (e.g. polymers) and large systems. New statistical methods have therefore been developed that allow for such calculations in a more tractable way. The method developed by Wu and Xu et al 2006, is an example of such methods. The main simplifying hypothesis in this technique is that it considers same reactivity for all the end groups. The charge distribution is calculated using QEq method (Rappe and Goddard, 1991). The process is modeled through cyclic canonical (NVT) and isothermal-isobaric (NPT) ensembles. First a geometry optimization and energy minimization is performed in the room temperature (298 K). Next, the system's temperature is raised to 358K. The system is then cooled down step by step at a rate of 10K/50ps. In each step, after the completion of NVT and NPT simulations, the proximity of reactive sites are examined and if they are within a radius of 2 Å from each other, bonds are created. This process is repeated until the system reaches the initial temperature. Nose-Hoover and Andersen algorithms are used as thermostat and barostat, respectively.

#### 4.2.3. Force field and simulation parameters

A crucial point in atomistic simulations is choosing a forcefield that result in an accurate enough approximation of the potential energy hypersurface in which the nuclei moves. The potential energy can be described as follows:

$$E_{total} = E_{valence} + E_{cross-term} + E_{non-bonded} \quad (4-1)$$

The valence energy consists of the bond-stretching term, bending energy and the four body terms including a dihedral bond-torsion angle term and an inversion (out-of plane interaction) term:

$$E_{valence} = E_{stretching} + E_{bendeing} + E_{dihedral\ torsion} + E_{inversion} \quad (4-2)$$

The cross-term accounts for the energy changes induced by the change in the bond length and the angle changes in the surrounding atoms as illustrated in the equation 3:

$$E_{cross-term} = E_{bond-bond} + E_{angle-angle} + E_{bond-angle} + E_{end\_bond-torsion} + E_{middle\_bond-torsion} + E_{angle-torsion} + E_{angle-angle-torsion} \quad (4-3)$$

The last term in the Eq. 1 (the non-bonded term) consists of Inter and Intra-molecular interactions, including hydrogen bonds (H-bonds), van der Waals interactions which are the induced dipole-dipole interactions (also named as London forces) and finally, the Coulomb interactions which account for electrostatic interactions.

$$E_{non-bonded} = E_{vdW} + E_{Coulomb} + E_{H-bond} \quad (4-4)$$

The condensed-phased optimized molecular potential (COMPASS) which has proved to be a promising force field for organic and inorganic systems, is used in this study (Sun 1998, Sun et al 1998 and Grujicic et al 2007). It is well parametrized for non-bonded interactions which makes it a good fit for long chain molecules like biomaterials or polymers and systems where the vdW is the governing interaction (Lu and Dunn 2010, Salahshoor and Rahbar 2012). The COMPASS force field uses the following expressions for various components of the potential energy:

$$E_{bond} = \sum_b [K_2(b - b_0)^2 + K_3(b - b_0)^3 + K_4(b - b_0)^4] \quad (4-5)$$

$$E_{angle} = \sum_\theta [H_2(\theta - \theta_0)^2 + H_3(\theta - \theta_0)^3 + H_4(\theta - \theta_0)^4] \quad (4-6)$$

$$E_{torsion} = \sum_\phi [V_1[1 - \cos(\phi - \phi_1^0)] + V_2[1 - \cos(2\phi - \phi_2^0)] + V_3[1 - \cos(3\phi - \phi_3^0)]] \quad (4-7)$$

$$E_{oop} = \sum_x K_x \chi^2 \quad (4-8)$$

$$E_{bond-bond} = \sum_b \sum_{b'} F_{bb'} (b - b_0)(b' - b_0') \quad (4-9)$$

$$E_{angle-angle} = \sum_\theta \sum_{\theta'} F_{\theta\theta'} (\theta - \theta_0)(\theta' - \theta_0') \quad (4-10)$$

$$E_{bond-angle} = \sum_b \sum_\theta F_{b\theta} (b - b_0)(\theta - \theta_0) \quad (4-11)$$

$$E_{end\_bond-torsion} = \sum_b \sum_\phi F_{b\phi} (b - b_0)[V_1 \cos \phi + V_2 \cos 2\phi + V_3 \cos 3\phi] \quad (4-12)$$

$$E_{middle\_bond-torsion} = \sum_b \sum_\phi F_{b'\phi} (b' - b_0')[F_1 \cos \phi + F_2 \cos 2\phi + F_3 \cos 3\phi] \quad (4-13)$$

$$E_{angle-torsion} = \sum_\theta \sum_\phi F_{\theta\phi} (\theta - \theta_0) \times [V_1 \cos \phi + V_2 \cos 2\phi + V_3 \cos 3\phi] \quad (4-14)$$

$$E_{angle-angle-torsion} = \sum_\phi \sum_\theta \sum_{\theta'} K_{\phi\theta\theta'} \cos \phi (\theta - \theta_0)(\theta' - \theta_0') \quad (4-15)$$

$$E_{Coulumb} = \sum_{i>j} \frac{q_i q_j}{\epsilon r_{ij}} \quad (4-16)$$

$$E_{vdW} = \sum_{i>j} \left[ \frac{A_{ij}}{r_{ij}^9} - \frac{B_{ij}}{r_{ij}^6} \right] \quad (4-17)$$

Where  $b$ ,  $\theta$ ,  $\Phi$  and  $\chi$  are the bond length, bond-angle, dihedral torsion angle and the inversion or out of plane angle respectively. Also,  $q$  is the atomic charge,  $\epsilon$  is dielectric constant and  $r_{ij}$  is the

interatomic distance between the atoms  $i$  and  $j$ . Finally,  $b_0$ ,  $K_i$  ( $i=2-4$ ),  $\theta_0$ ,  $H_i$  ( $i=2-4$ ),  $\Phi_i^0$  ( $i=1-3$ ),  $V_i$  ( $i=1-3$ ),  $F_{bb'}$ ,  $b_0'$ ,  $F_{\theta\theta'}$ ,  $\theta_0'$ ,  $F_{b\theta}$ ,  $F_{b\phi}$ ,  $F_{b'\phi}$ ,  $F_i$  ( $i=1-3$ ),  $F_{\theta\phi}$ ,  $K_{\phi\theta\theta'}$ ,  $A_{ij}$  and  $B_{ij}$  are the system dependent parameters implemented in the Material Studio 6.0 software package, which is used in this study.

### 4.3. Results and Discussion

#### 4.3.1. Crosslinking process

As mentioned before, the crosslinking process is performed by creating reactive sites and cyclic NVT and NPT dynamics simulations. To this end, H-atoms are removed from  $N_{\text{Jeff}}$  (end nitrogen atoms in the Jeffamine) and  $C_{\text{PEGDGE}}$  (end carbon atoms in the PEGDGE). These are shown in blue and grey in Fig 1. Figure 2 shows the hydrogel structure before and after crosslinking. In order to mimic the natural crosslinking process, a probability of 70% is imposed when creating bonds. In other words, about 70 percent of crosslinks are created. This is clearly seen in the Figure2. (b) where some  $N_{\text{Jeff}}$  atoms are still not connected to any carbon atoms of PEGDGE.

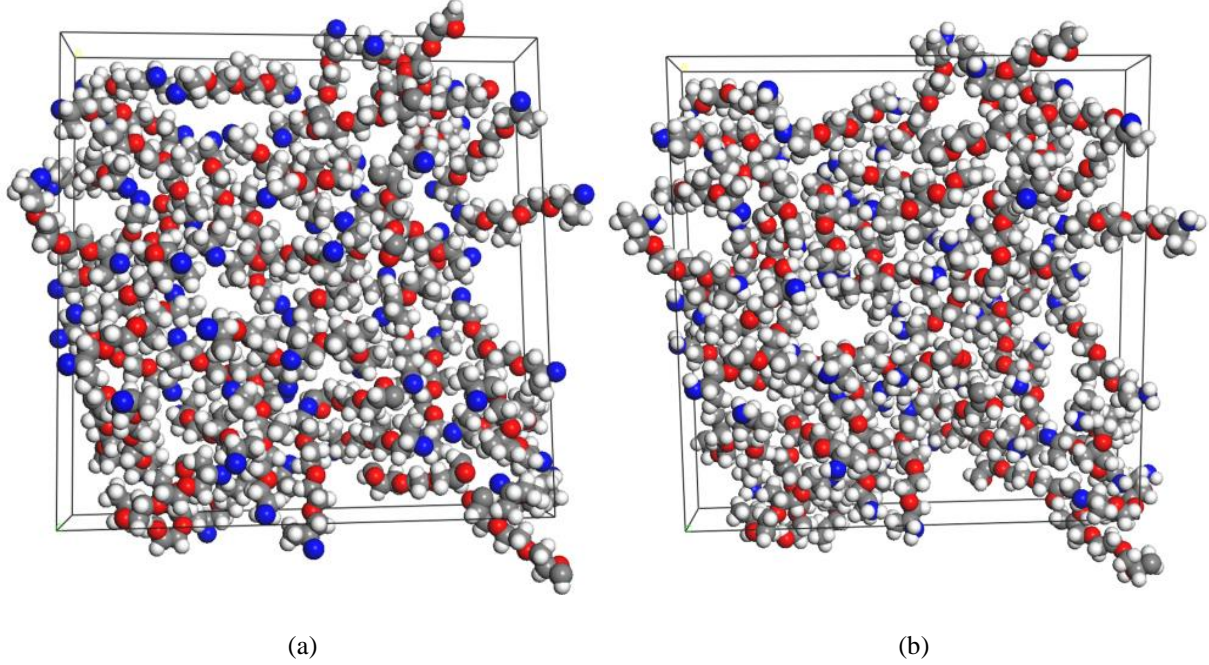


Figure 9. The hydrogel initial model without water: (a) before crosslinking; (b) after crosslinking.

The distribution of  $N_{\text{Jeff}}$  and  $C_{\text{PEGDGE}}$  atoms before and after the crosslinking provides a better insight into the process. This is analyzed by radial distribution function (RDF).  $g_{A-B}(r)$  is the probability density of finding atoms A and B at a distance  $r$  averaged over the equilibrium trajectory, so that:

$$g_{A-B}(r) = \left( \frac{n_B}{4\pi r^2 dr} \right) / \left( \frac{N_B}{V} \right) \quad (4-18)$$

where  $n_B$  is the number of B particles located at a distance  $r$  in a shell of thickness  $dr$  from A particle,  $N_B$  is the total number of B particles in the system, and  $V$  is the total volume of the system.  $g_{N_{\text{Jeff}}-C_{\text{PEGDGE}}}(r)$  characterizes the relative configuration of N and C atoms in the curing agent and epoxy quantitatively. Figure 3 shows the RDF of the system before and after the crosslinking simulations. Basically, the two RDFs are for a pair of atoms once in two different



molecules and then in a continuous polymer system packed in a unit cell. The graph demonstrates a discontinuous RDF for the system before crosslinking and a smooth, continuous curve after the crosslinking, which is due to the created crosslinks. The graph is a quantitative proof for bond creations between the Jeffamine and PEGDGE molecules.

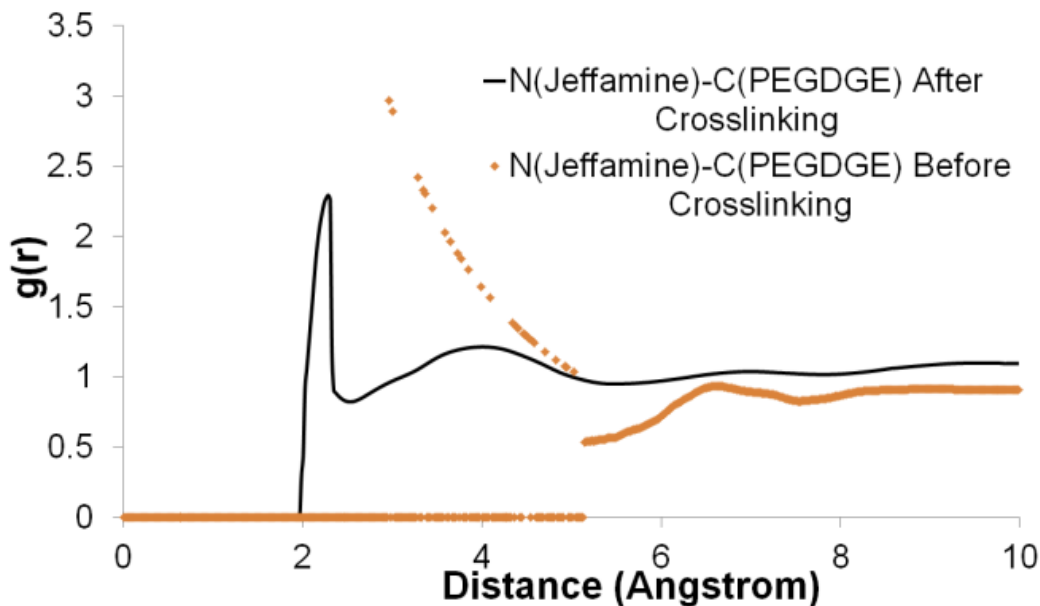
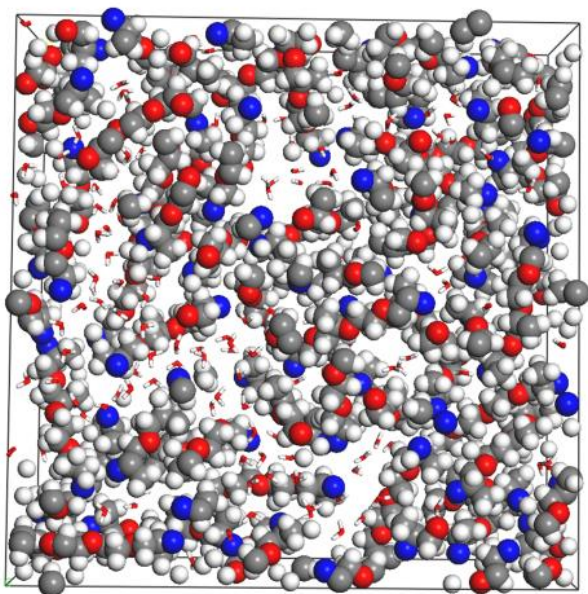


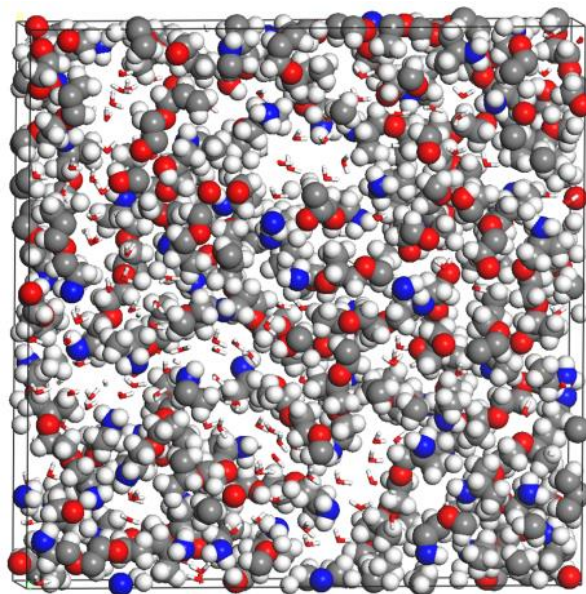
Figure 10. Radial Distribution Function of NJeff – CPEGDGE pair for the initial model: (a) before crosslinking; (b) after crosslinking.

#### 4.3.2. Equilibrated structure and the role of water

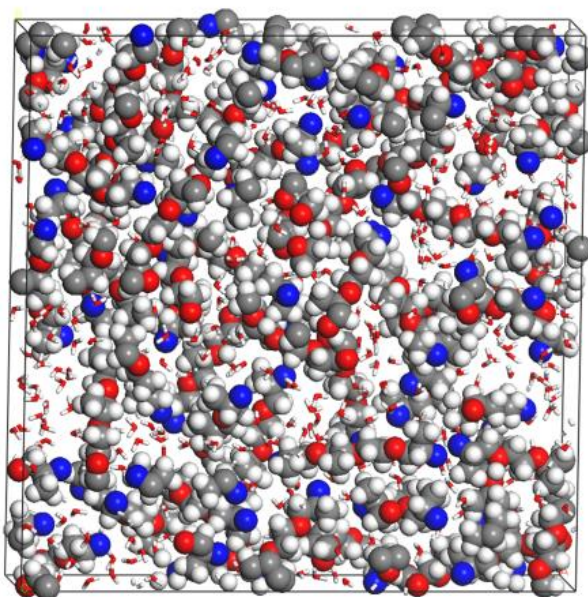
The structure of hydrogel is equilibrated and studied for 20, 40, 60 and 80 volume percent of water content. For each system, the crosslinking process is performed. Also, an energy minimization is performed on the final crosslinked structure to reach the minimum energy configuration of the system. This is done via NVT simulation of the system at the room temperature with a time step of 1 fs and for a duration of 50 ps. The final equilibrated structures before and after the crosslinking with various water percentages are presented in Figure 4.



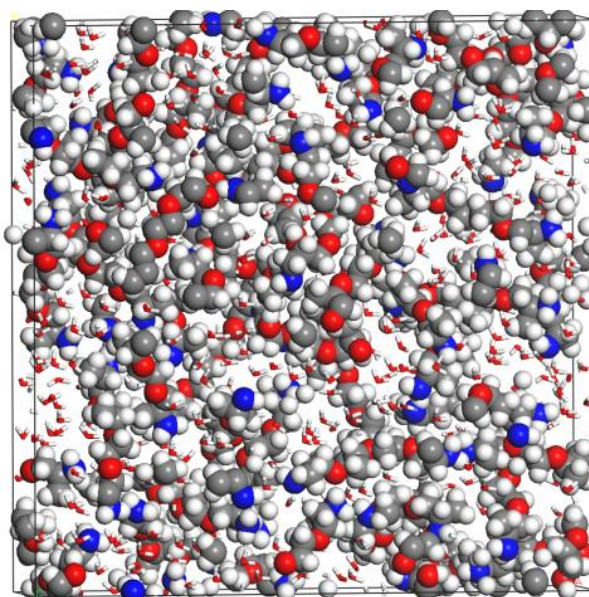
(a)



(b)



(c)



(d)

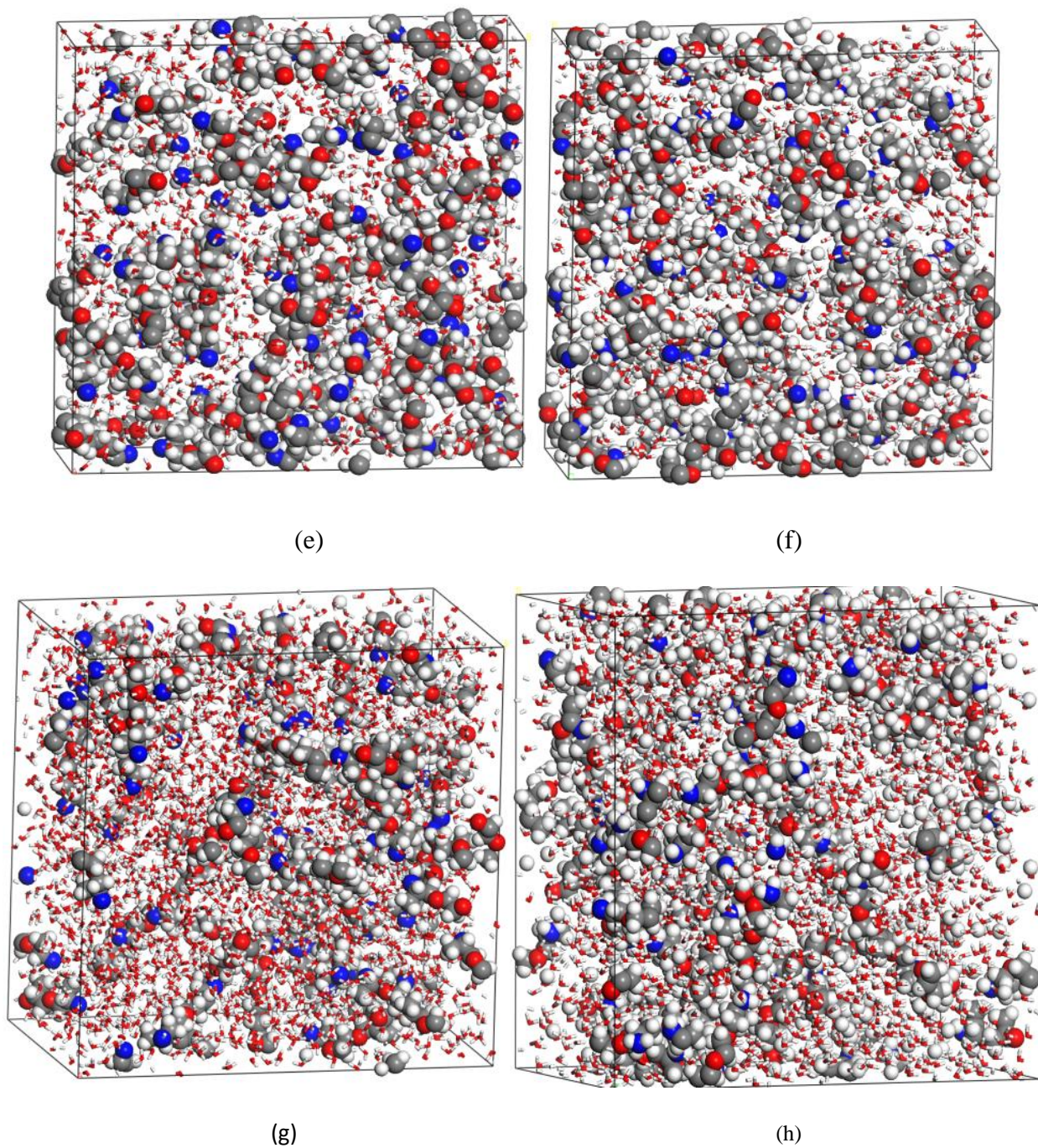
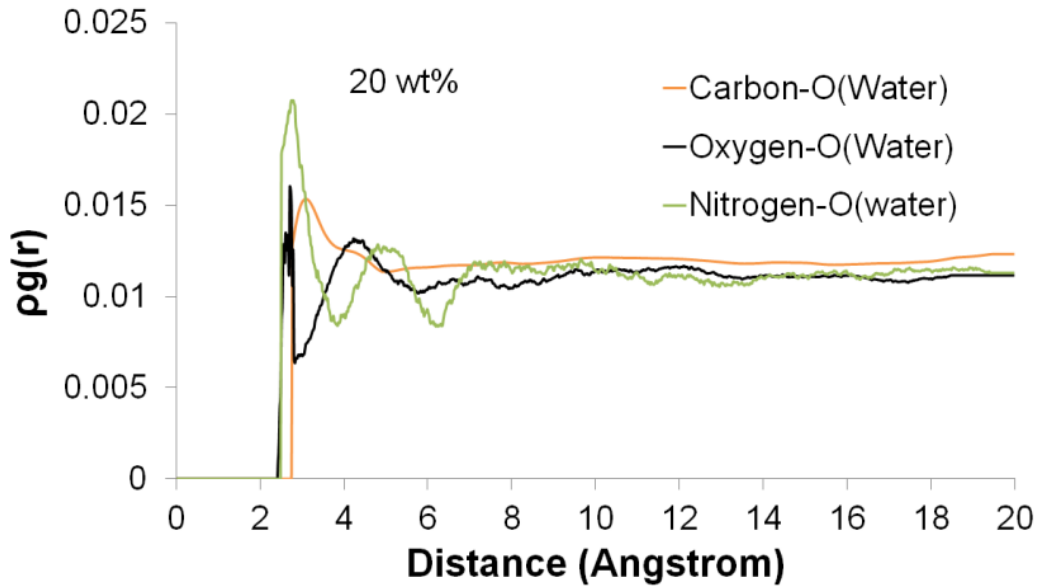


Figure 11. Equilibrated hydrogel structures: (a) 20 wt% before crosslinking ; (b) 20 wt% after crosslinking; (c) 40 wt% before crosslinking ; (d) 40 wt% after crosslinking; (e) 60 wt% before crosslinking ; (f) 60 wt% after crosslinking; (g) 80 wt% before crosslinking; (h) 80 wt% after crosslinking

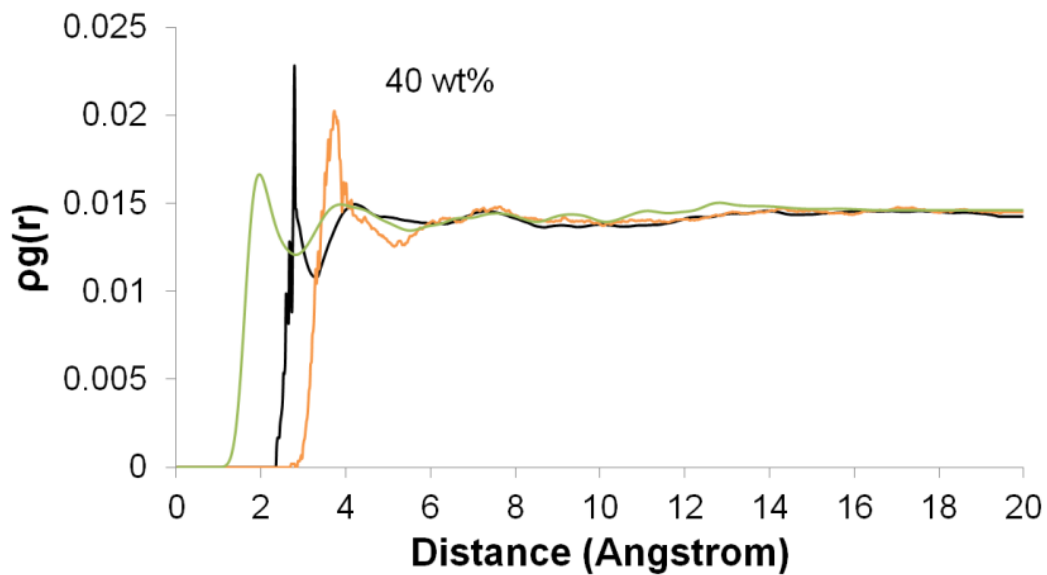
The system evolves through the dynamics simulation to reach its minimum energy configuration.

The effect of water content on the distances between different atoms in the final and evolved

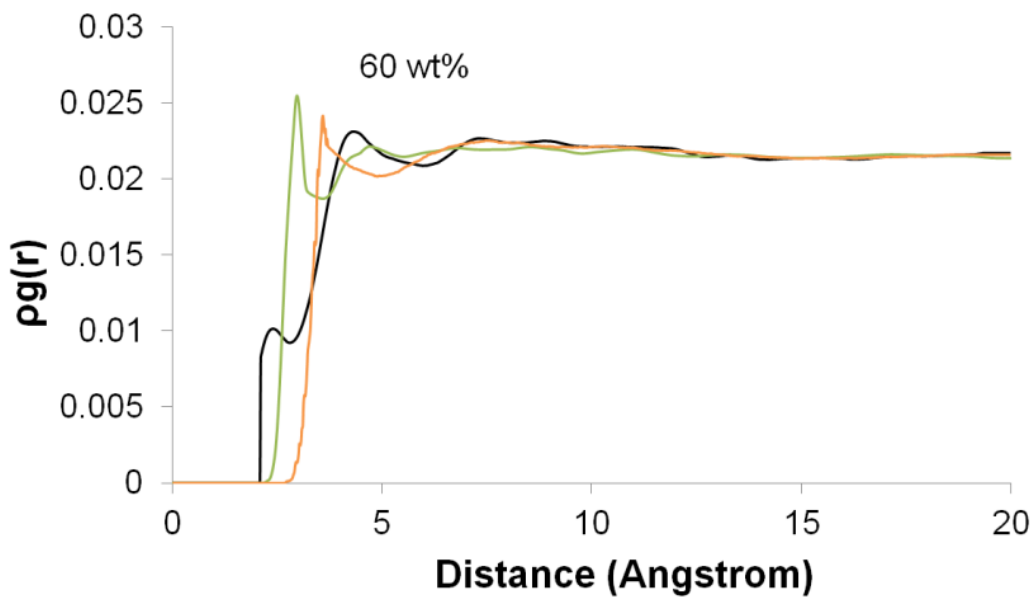
structures is studied using RDFs (see Figure 5). In order to directly compare the intensities, the product of RDF and the number density ( $\rho g(r)$ ) is used instead of  $g(r)$ . Figure 5 depicts  $\rho g_{\text{Oxygen-O(Water)}}(r)$ ,  $\rho g_{\text{Nitrogen-O(Water)}}(r)$  and  $\rho g_{\text{Carbon-O(Water)}}(r)$  for different water contents. These results show that the intensity of  $\rho g(r)$  increases with the increase in water content. The Nitrogen and Oxygen atoms of the crosslinked hydrogel contain negative charges, while the Carbon atoms have positive charge. As water content increases, the electrostatic interactions dominate more, thus the probability of finding a carbon atom near the water molecules increases. Since the N atoms are only present in Jeffamine molecule, they are the zones where the crosslinks are built ( $N_{\text{Jeff}}$ ). Analysis of RDFs proves that the water molecules are closer to the crosslink zones.



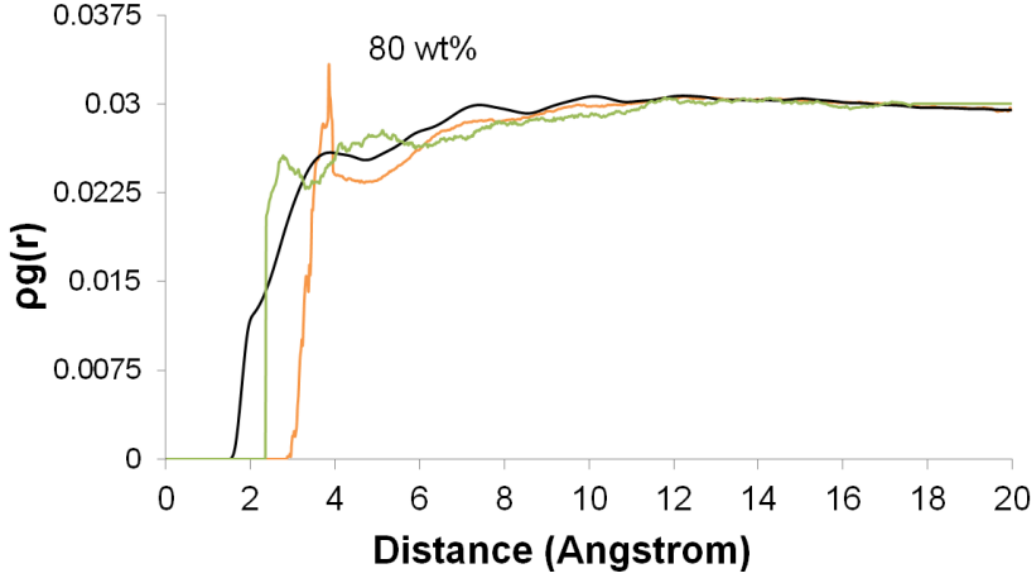
(a)



(b)



(c)



(d)

Figure 12. Radial Distribution Function for Oxygen-O(Water, Nitrogen-O(Water) and Carbon-O(Water) pairs for different water contents: (a) 20 wt%; (b) 40 wt%; (c) 60 wt%; (d) 80 wt%.

#### 4.3.2. Effect of crosslinking on Diffusion coefficients

Based on the MD simulations, the coefficients of the effective diffusion  $D$  ( $D$  in equilibrium diffusion) is computed for the water molecules in the hydrogel with different water contents using the mean-square displacement (MSD) formula (Allen and Tildesley 1987). According to the Equations below, the MSD of water molecules are computed before and after the crosslinking process:

$$MSD = \frac{1}{NM} \sum_i^N \sum_k^M \langle |r_i(t_k + \Delta t) - r_i(t_k)|^2 \rangle \quad (4-19)$$

$N$ : Number of particles (in here, water molecules)

$M$ : Number of Time Series.

$r_i$ : Location of particle.

$t_k$ : Starting time of the  $k^{\text{th}}$  time series.

After computing the MSD, determination of diffusion coefficient  $D$ , is performed using the Einstein's equation as follows:

$$D = \lim_{t \rightarrow \infty} \frac{1}{6t} MSD \quad (4-20)$$

Instead of using an infinitely long running time as indicated in the equation, the 500ps simulations time for the evaluation stage was found to be long enough to reach to linear portion of MSD, indicating the equilibrium diffusion stage of water molecules in the MD simulations.

Figure 13 demonstrates the effect of crosslinking on the diffusion coefficients. It is obviously seen that crosslinking decreases the diffusion coefficients and thus decreasing the mobility of water molecules. Also, by increasing the water content, the diffusion coefficients increase. The results are consistent with the hydrophilicity of the crosslink zones.

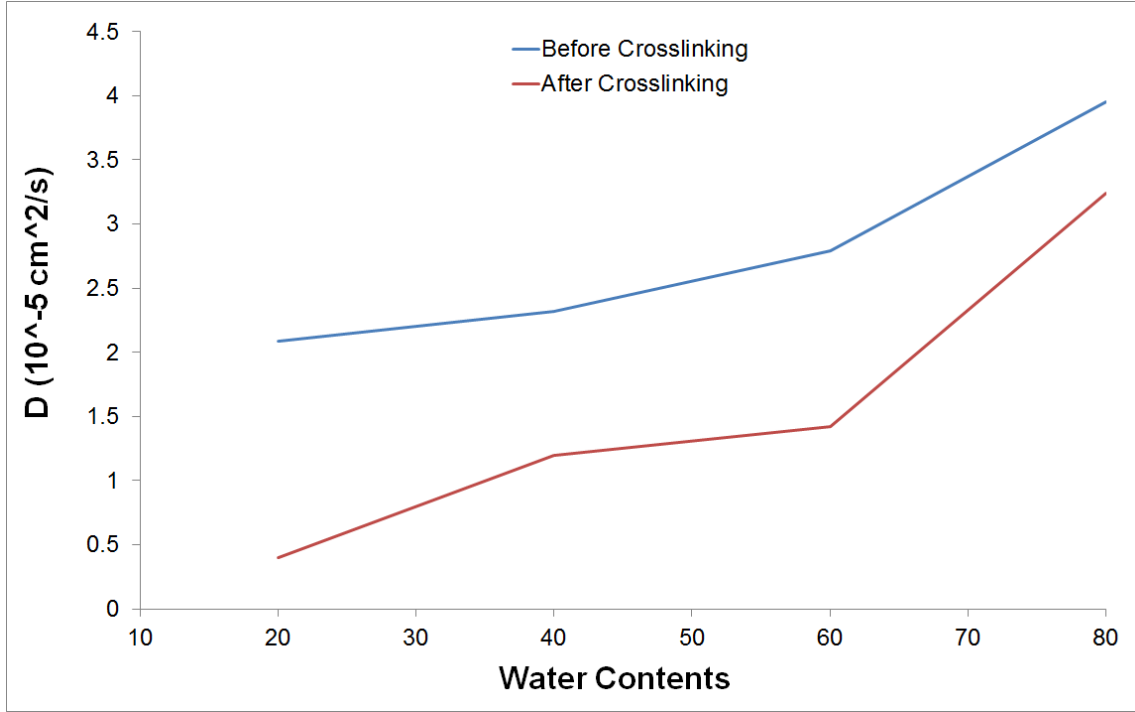


Figure 13. Diffusion coefficients for water molecules in different water contents, both before and after crosslinking.

#### 4.3.3. Elastic Properties of hydrogels

Mechanical properties of hydrogel are studied by applying a predefined strain to unit cell. For a uniaxial testing, a total strain amplitude of 0.003 is applied to the simulation box which is enforced equally at each simulation step (every 1 fs). The stress is calculated from the uniaxial test in the x-direction using the virial relation:

$$\sigma_{ij} = \frac{1}{2\Omega^i} \sum_{j(\neq i)} r_{ij} \otimes f_{ij} \quad (4-21)$$

where  $\Omega^i$  is a small volume around an atom  $i$ . The interatomic force  $f_{ij}$  applied on atom  $i$  by atom  $j$  is:



$$f_{ij} = \frac{\partial E(r_{ij})}{\partial r_{ij}} \frac{r_{ij}}{\|r_{ij}\|} \quad (4-22)$$

This procedure is performed for the systems with different water contents. After computing  $\sigma_{xx}, \sigma_{yy}, \sigma_{zz}$  independently for the simulation box, the three stress values are averaged to compute the elastic modulus. Finally, the  $6 \times 6$  stiffness matrices are computed, by applying a unit displacement in each degree of freedom, for different water contents:

$$0 \text{ wt\%} \Rightarrow C_{ij} = \begin{pmatrix} 6.7650 & 3.0836 & 4.6568 & -0.5538 & -0.6347 & 0.4578 \\ 3.0836 & 9.6250 & 4.6229 & -0.1655 & -0.0066 & 1.2009 \\ 4.6568 & 4.6229 & 11.9052 & -0.5518 & -0.8331 & 0.5603 \\ -0.5538 & -0.1655 & -0.5518 & 1.7093 & -0.5200 & -0.0709 \\ -0.6347 & -0.0066 & -0.8331 & -0.5200 & 1.6852 & 0.3397 \\ 0.4578 & 1.2009 & 0.5603 & -0.0709 & 0.3397 & 2.1630 \end{pmatrix}$$

$$20 \text{ wt\%} \Rightarrow C_{ij} = \begin{pmatrix} 10.0473 & 2.9468 & 3.6788 & -0.0066 & 0.3673 & 0.6654 \\ 2.9768 & 7.7488 & 4.1584 & 0.5323 & 0.3339 & 0.2095 \\ 3.6788 & 4.1584 & 9.1498 & -0.1284 & -0.1745 & -0.0464 \\ -0.0066 & 0.5323 & -0.1284 & 1.6645 & 0.3879 & -0.1146 \\ -0.3676 & 0.3339 & -0.1745 & 0.3897 & 2.3715 & -0.7634 \\ 0.6654 & 0.2095 & -0.0464 & -0.1146 & -0.7634 & 1.4606 \end{pmatrix}$$

$$40 \text{ wt\%} \Rightarrow C_{ij} = \begin{pmatrix} 6.5619 & 3.3001 & 4.0905 & -0.2213 & -0.0032 & -0.3711 \\ 3.3001 & 7.7734 & 4.2747 & -0.1413 & 0.0666 & -0.5896 \\ 4.0905 & 4.2747 & 7.1310 & -0.0827 & 0.5737 & -0.6408 \\ -0.2213 & -0.1413 & -0.0827 & 2.6061 & -0.1855 & 0.1544 \\ -0.0032 & 0.0666 & 0.5737 & -0.1855 & 1.7400 & -0.4800 \\ -0.3711 & -0.5896 & -0.6408 & 0.1544 & -0.4800 & 0.9157 \end{pmatrix}$$

$$60 \text{ wt}\% \Rightarrow C_{ij} = \begin{pmatrix} 5.7631 & 3.4711 & 3.3436 & -0.0054 & -0.1865 & -0.1339 \\ 3.4711 & 4.7573 & 3.8203 & -0.0708 & -0.4171 & -0.3931 \\ 3.3436 & 3.8203 & 6.9301 & -0.2693 & 0.0132 & -0.1272 \\ -0.0054 & -0.0708 & 0.2693 & 1.5602 & -0.2298 & 0.1333 \\ -0.1865 & -0.4171 & 0.0132 & -0.2298 & 1.8788 & -0.3903 \\ -0.1339 & -0.3931 & -0.1272 & 0.1333 & -0.3903 & 2.4970 \end{pmatrix}$$

$$80 \text{ wt}\% \Rightarrow C_{ij} = \begin{pmatrix} 4.9663 & 4.5360 & 3.3063 & 0.3025 & 0.6299 & -0.1029 \\ 4.5360 & 6.5612 & 4.6907 & -0.6374 & 0.1067 & -0.2596 \\ 3.3063 & 4.6907 & 5.7067 & -0.0107 & 0.6878 & 0.6421 \\ 0.3025 & -0.6374 & 0.0107 & 1.6099 & 0.4820 & 0.2120 \\ 0.6299 & 0.1067 & 0.6878 & 0.4820 & 0.7627 & -0.9780 \\ -0.1029 & -0.2596 & 0.6421 & 0.2120 & -0.9780 & 0.5030 \end{pmatrix}$$

Elastic moduli are calculated after energy minimizations in different water contents. Fig .6 illustrates elastic modules for 20, 40, 60 and 80 wt%. Water molecules act as lubricators allowing more deformation in the hydrogel under a specific stress. Therefore the stiffness of hydrogel decreases with the increase in water content.

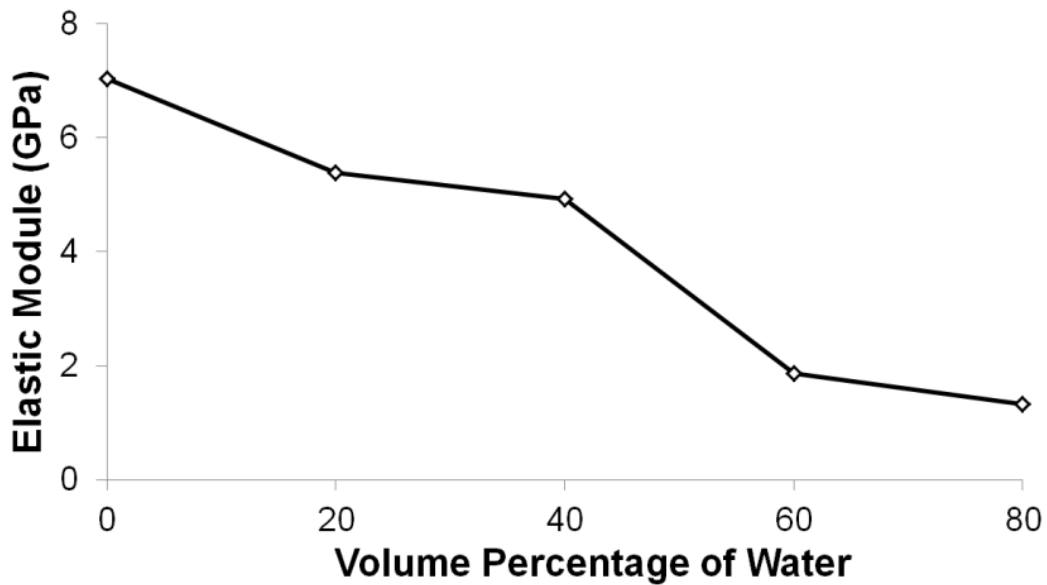


Figure 14. Change in elastic modulus vs water content.

#### **4.4. Conclusion**

Molecular dynamic simulation is used to study the effect of water on the equilibrated structure and mechanical properties of crosslinked hydrogel. The hydrogel consisted of Polyethylene glycol diglycidyl ether (PEGDGE) as epoxy and the Jeffamine which is poly-oxy-alkylene-amines as curing agent. Different water contents (from 0 to 80 wt%) are examined. COMPASS forcefield is employed for the simulations. Radial distribution functions, calculated for systems with various water contents, indicate that the crosslinks are more hydrophilic within the hydrogel structure. Mechanical properties are studied by applying strain to the system and the stiffness matrices and elastic modulus are calculated for different water percentages. The results show that the elastic modulus decreases by increasing the water content.

## **Chapter 5: Coarse-Grained model of Hydrogel**

### **5.1. Introduction**

The use of coarse grained (CG) models in a variety of simulation techniques has proven to be a valuable tool to probe the time and length scales of systems beyond what is feasible with traditional all atom (AA) models. Using all-atom methods, long simulations are very costly and even close to impossible and they limit us to small length and especially time scales. A promising strategy to overcome these limitations is to decrease number of degrees of freedom by grouping atoms into pseudoatoms (or particles) referred to as beads (Gautieri et al 2010). This represents the basis of the so-called coarse-grained approach, where, starting at the nanoscale, it is possible to derive parameters for higher hierarchical levels, up to the macroscale by systematically feeding information from smaller, more accurate to larger, coarser levels. Coarse-Graining models were initiated for modeling huge biomolecules (Marrink et al, 2007).

Among different CG models, MARTINI coarse-grained model, developed by Marrink and co-workers is used in this study. The MARTINI model provides suitable level of coarse-graining, as it retains information about the chemistry. In the following section, the MARTINI approach for the CG modeling is described.

### **5.2. MARTINI Model**

#### **5.2.1. Interaction Sites**

The general mapping rule is that four heavy atoms (that is non-hydrogen atoms) are grouped together into one bead, i.e. on average four heavy atoms are represented by a single interaction

center. For ring structures a different mapping is introduced, as will be explained below. In order to keep the model simple, we still consider only four main types of interaction sites: polar (P), nonpolar (N), apolar (C), and charged (Q). Each particle type has a number of subtypes, which allow for a more accurate representation of the chemical nature of the underlying atomic structure. Within a main type, subtypes are either distinguished by a letter denoting the hydrogen-bonding capabilities (d=donor, a=acceptor, da=both, 0=none), or by a number indicating the degree of polarity (from 1, low polarity, to 5, high polarity).

### 5.2.2. Bonded and Nonbonded Interactions

The form of the nonbonded interactions is the Lennard-Jones 12-6 potential energy function. In addition to the LJ interaction, charged groups bear a full charge  $q_{i,j}$  interacting via a shifted Coulombic potential energy function:

$$U_{el}(r) = \frac{q_i q_j}{4\pi\epsilon_0\epsilon_r r} \quad (5-1)$$

with relative dielectric constant  $\epsilon_r=15$  for explicit screening.

Among bonded interactions, the form for the bond stretch is weak harmonic potential with an equilibrium distance  $R_{\text{bond}} = \sigma = 0.47$  nm and a force constant of  $K_{\text{bond}} = 1250$  kJ mol<sup>-1</sup> nm<sup>-2</sup>. The LJ interaction is excluded between bonded particles, because they are on average somewhat closer to each other than neighboring nonbonded particles.

Also for bending potential, weak harmonic potential of the cosine type is used. Again, a set of parameters are defined for this form. Also for most of linear chainlike molecules, a standard

force constant of  $K_{\text{angle}} = 25 \text{ kJ mol}^{-1}$  with an equilibrium bond angle  $\theta_0 = 180^\circ$  is the best initial choice.

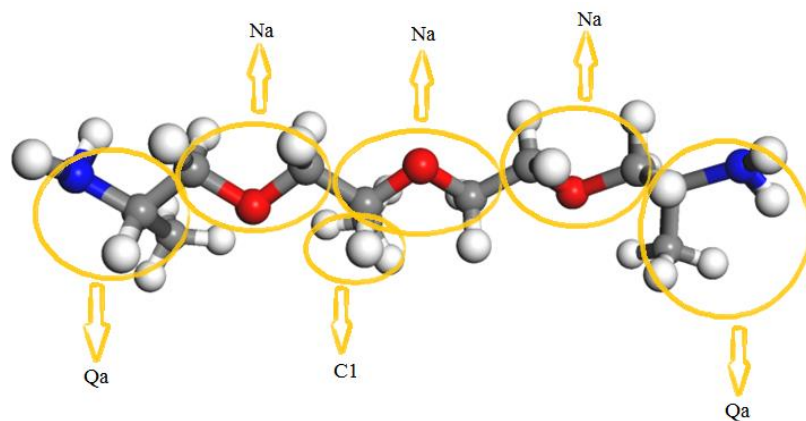
Basically, the force graining recipe consists of three steps:

1. Mapping onto CG representation: The first step is to divide the molecule into small chemical building blocks, ideally of four heavy atoms each. Because most molecules cannot be entirely mapped onto groups of four heavy atoms, however, some groups will represent a smaller or larger number of atoms. There are different strategies for modulation of building blocks, especially for certain compounds like those having ring structures, described in Marrink *et al.* 2007.
2. Selecting bonded interactions: For most molecules the use of a standard bond length (0.47 nm) and force constant of  $K_{\text{bond}} = 1250 \text{ kJ mol}^{-1}\text{nm}^{-2}$  seems to work well. Ring structures needs additional adjusting. Also, the values defined before for the bending parameters are also working for most molecules.
3. Optimization: Since, coarse graining procedure does not lead to a unique assignment of particle types and bonded interactions, the structure should be optimized. Validating the results with the all-atom model is also popular.

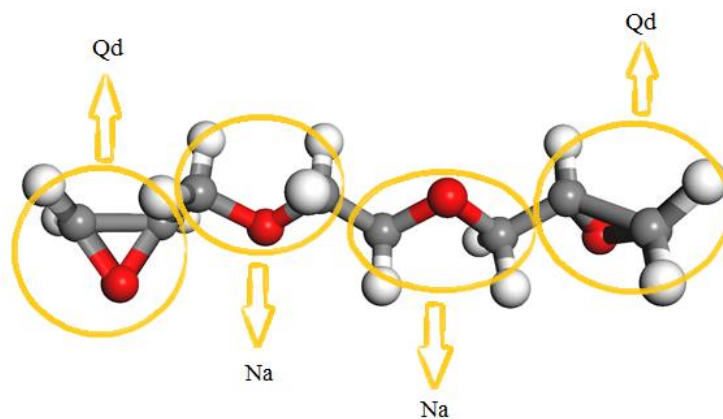
### 5.3. Coarse-Grained model for the Hydrogel

Coarse-grained models of the PEGDGE and Jeffamine are built according to the MARTINI model. According to the Figure 15, the beads are assigned to the all-atom model. According to the crosslinking protocol prescribed earlier in chapter 3, the end groups of the two molecules are assigned as charged groups, one as Qa (Charged, acceptor) and the other one as Qd (Charged donor). The CG model of the Jeffamine and PEGDGE are shown in the Figure 16. Also, the

water molecules are assigned as one bead. Since, water is highly polar molecules, it is assigned as type P4 (Very Polar).



(a)



(b)

Figure 15. Coarse-Grain model for: (a) Jeffamine. (b) PEGDGE. The Nitrogen, Oxygen, Carbon and Hydrogen atoms are shown in blue, red, grey and white, respectively.

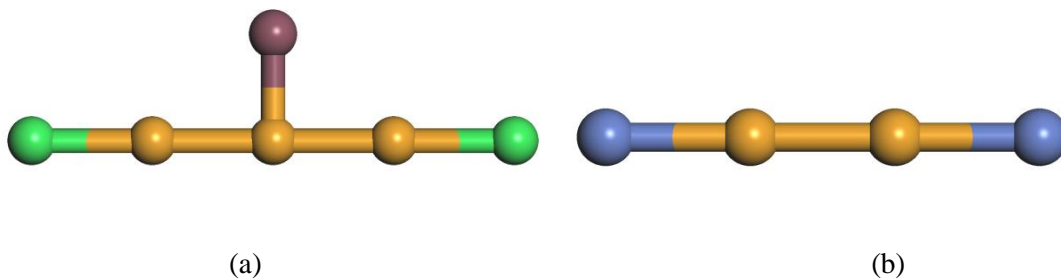


Figure 16. CG model for the: (a) Jeffamine. (b)PEGDGE.

The CG model for the Jeffamine, PEGDGE and water are packed in an amorphous cell, using the random walk method developed by Theodorou and Suter. The total density for the unit cell is  $1.3096 \text{ g/cc}^3$ . Periodic Boundary Conditions are applied for the system and the initial unit cells dimension is  $50 \times 50 \times 50 \text{ \AA}^3$ . Four different models unit cells are created containing 20, 40, 60 and 80 percent water content. Also, the same crosslinking protocol is applied for the system. The main focus in here is to study the mechanical properties of hydrogel and the effect of water content on the elastic properties. The results are validated with the experimental data.

#### 5.4. Results and Discussion

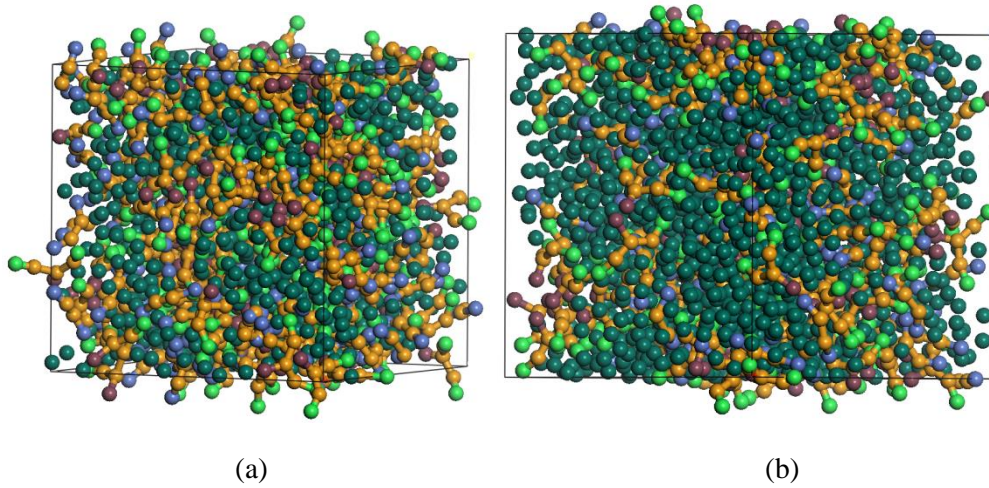
The first step after constructing the unit cells of the hydrogels is energy minimization. For this purpose, for each of the systems, 5000 steps of geometry optimization is performed. Then two dynamic simulations of NVT and NPT are performed sequentially. The time length for each dynamic simulation is 5 ns with the time step of 1 fs. Through these dynamic simulations, the system finds its minimum energy and the desired volume and pressure. Table I, shows the final dimensions of the unit cells in different water contents after the initial minimization.



Table 5-1. Cell dimensions, Before and after the initial 10 ns minimizaion.

Water Content (%)	Initial Dimension (A°)	Final Dimension After the minimizations (A°)
20	50×50×50	63.99×63.99×63.99
40	50×50×50	68.58×68.58×68.58
60	50×50×50	72.54×72.54×72.54
80	50×50×50	76.61×76.61×76.61

Figure 17, shows the final structure after the initial minimization for different water contents.



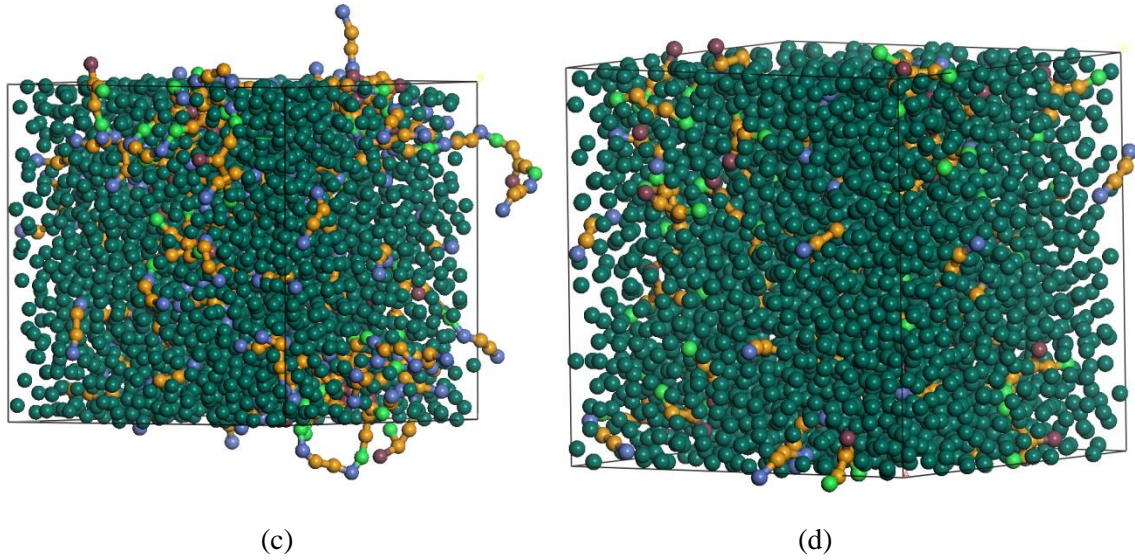
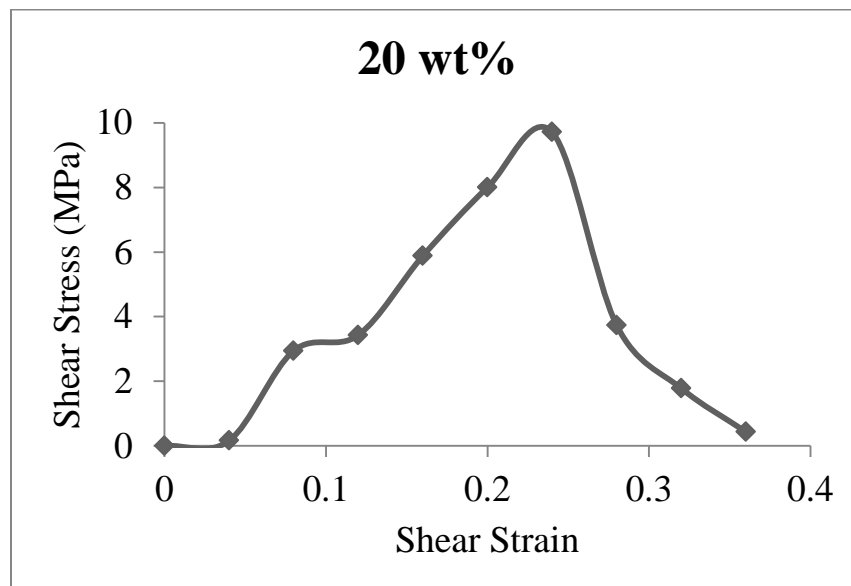
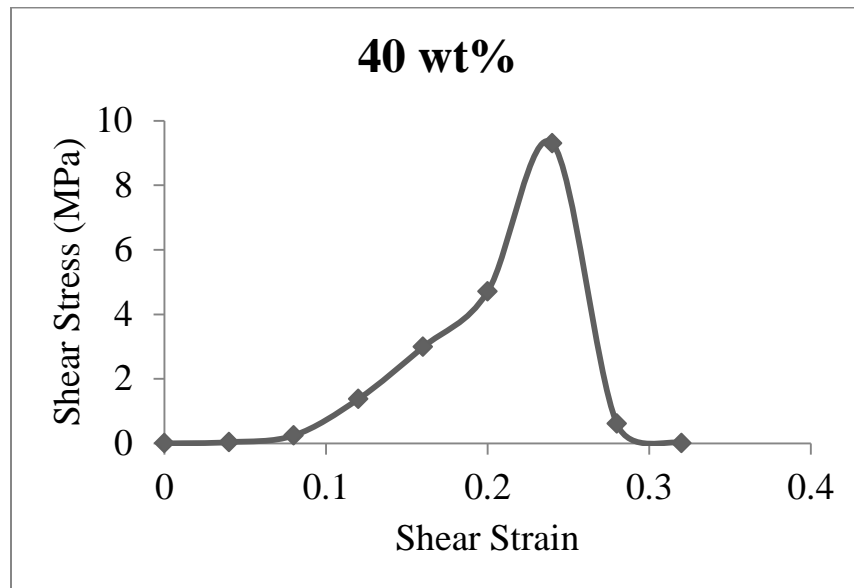


Figure 17. The structure after minimizations: (a). 20wt%, (b). 40wt%, (c). 60wt%, (d). 80wt%.

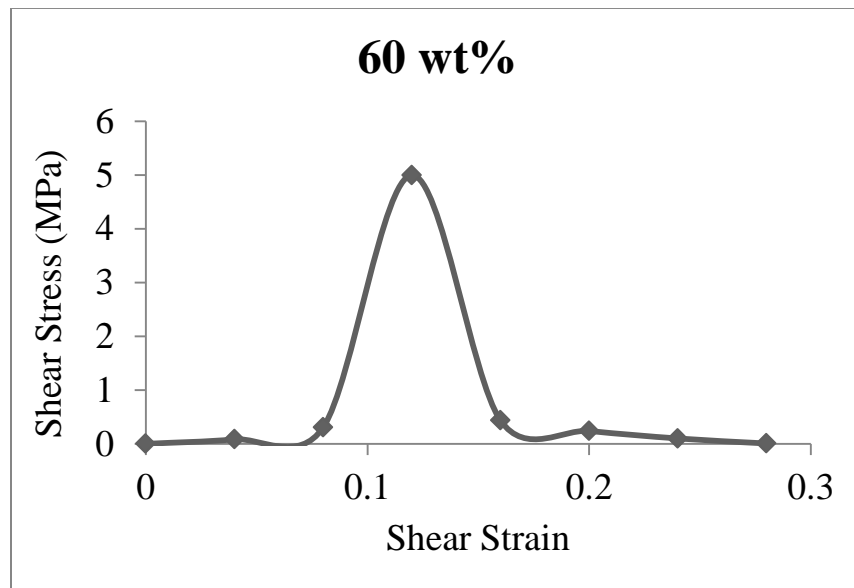
After the optimization and minimization steps, shear strain is applied to the system. The shear is applied to the system step by step with a rate of  $1e-5$ , through NPT dynamic simulations. Each NPT simulation (applying shear) is performed within 4 ns with the time step of 10 fs. The Berendsen algorithm is chosen for the thermostat and barostat. In order to optimize and stabilize the pressure, each shear simulation is followed by a 1 ns dynamic NVT simulation.



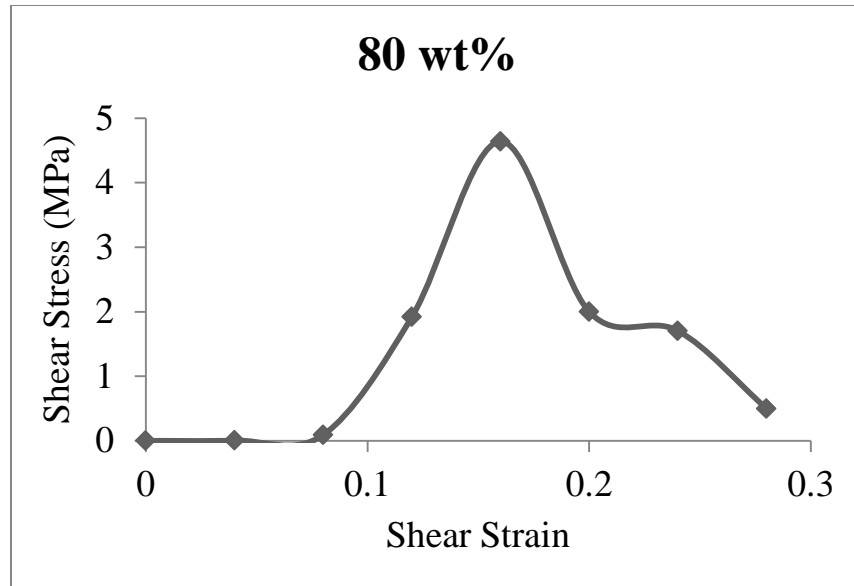
(a)



(b)



(c)



(d)

Figure 18. Stress-Strain Curves for the CG-Hydrogel containing different water percentages.

The shear simulations are performed for the systems with several water contents, from 20 to 80 wt%. Figure 18 shows the stress-strain curves for the unit cells, demonstrating the role of water on the mechanical properties. The results illustrate that by increasing the water content, the shear strength decreases, while this drop occurs significantly after the 40 wt%. Thus we can conclude around 40 percent water content, is the crucial amount for the hydrogels.

## Chapter 6: Hydrogels in Continuum Scale

### 6.1. Introduction

Contact lenses are one of the most popular applications of hydrogels. They are generally grouped in four categories based on the water content as low water content (below 50 wt%), high water content (greater than 50 wt%) and on whether the lens surface is considered to be ionic (reactive) or non-ionic (less reactive). Most daily used lenses are in the low water content category, having around 40% water content. In this chapter, mechanical behavior of contact lenses in continuum scale is studied using Finite-Element Method (FEM).

The stress-strain curve derived from the CG model for the 40 wt% hydrogel is implemented as the material behavior of the contact lens. Three different scenarios based on the loading situations are considered for contact lens, each representing a simplified situation which happens in reality: Contact lens under a point load, Contact lens in a contact by a rigid plate and when a uniform displacement is applied to the perimeter of the contact lens.

A diameter of 12 mm and a thickness of 0.5 mm is considered for the contact lens. All the simulations are performed using ABAQUS 6.12.

### 6.2. Mechanical Scenarios

#### 6.2.1. Case I: Point Load

In this scenario, a point nodal force is applied to the model. Material behavior is hyperelastic and the values are implemented according to the results of the CG simulation. Fig. 19 shows the initial model after meshing. Quad meshes are assigned with the total number of 6582 elements.

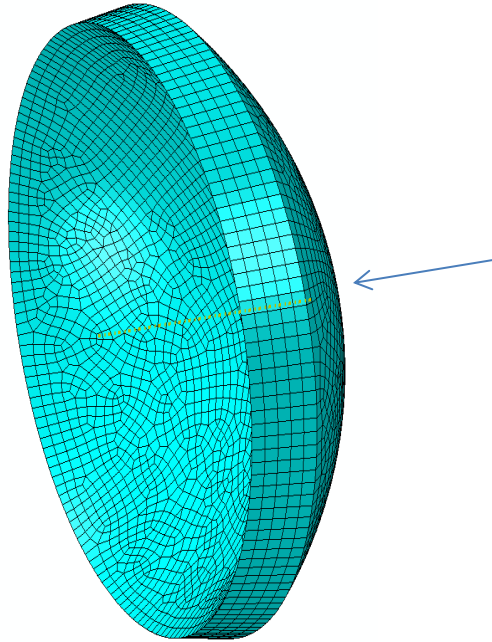
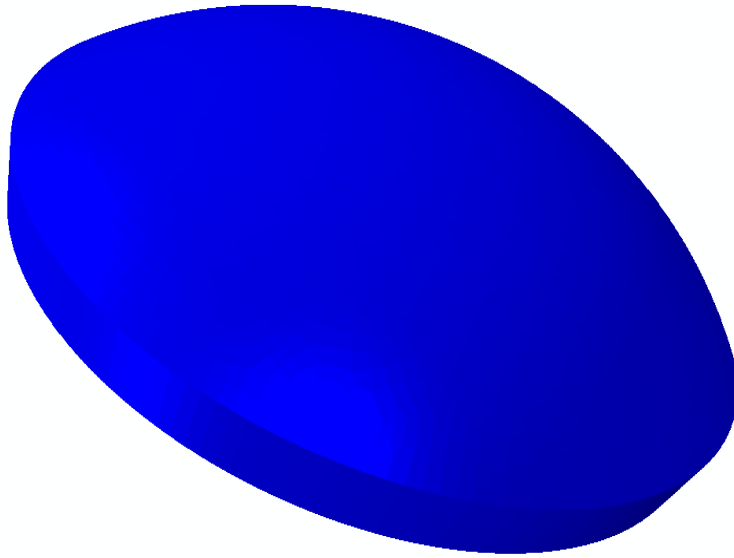
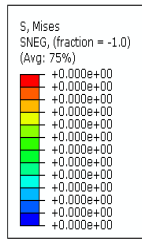


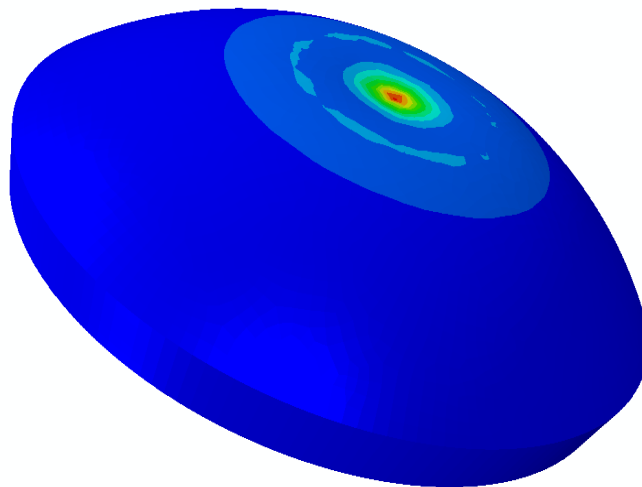
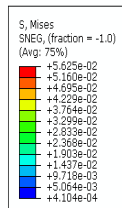
Figure 19. Mesh assigned model and the load direction.

5 mN load is applied to the system, while the perimeter of the lower side is fixed. Fig 20 shows the contours of stress during the loading process. The deformation steps are shown through four

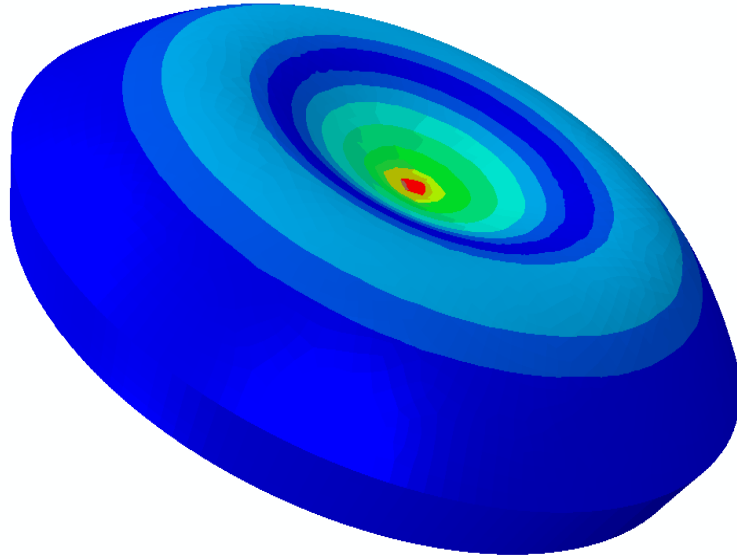
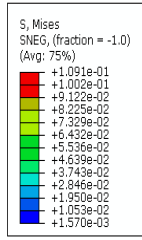
steps in the next Figure.



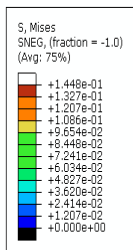
(a)



(b)



(c)



Ste  
Tot

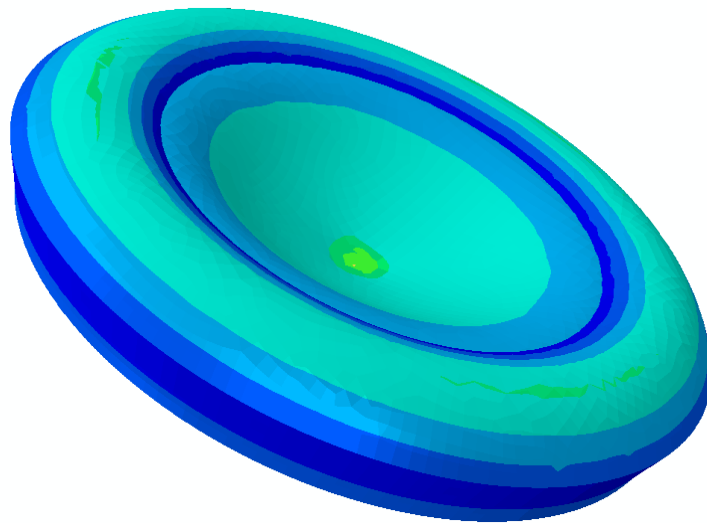


Figure 20. Hydrogel Deformation Due to The Point Load.



The load displacement graph is presented in Fig. 22 for the node that the force is applied to. The change in the graph slope is due to the hyper elasticity, where the material undergoes more deformation in a constant force.

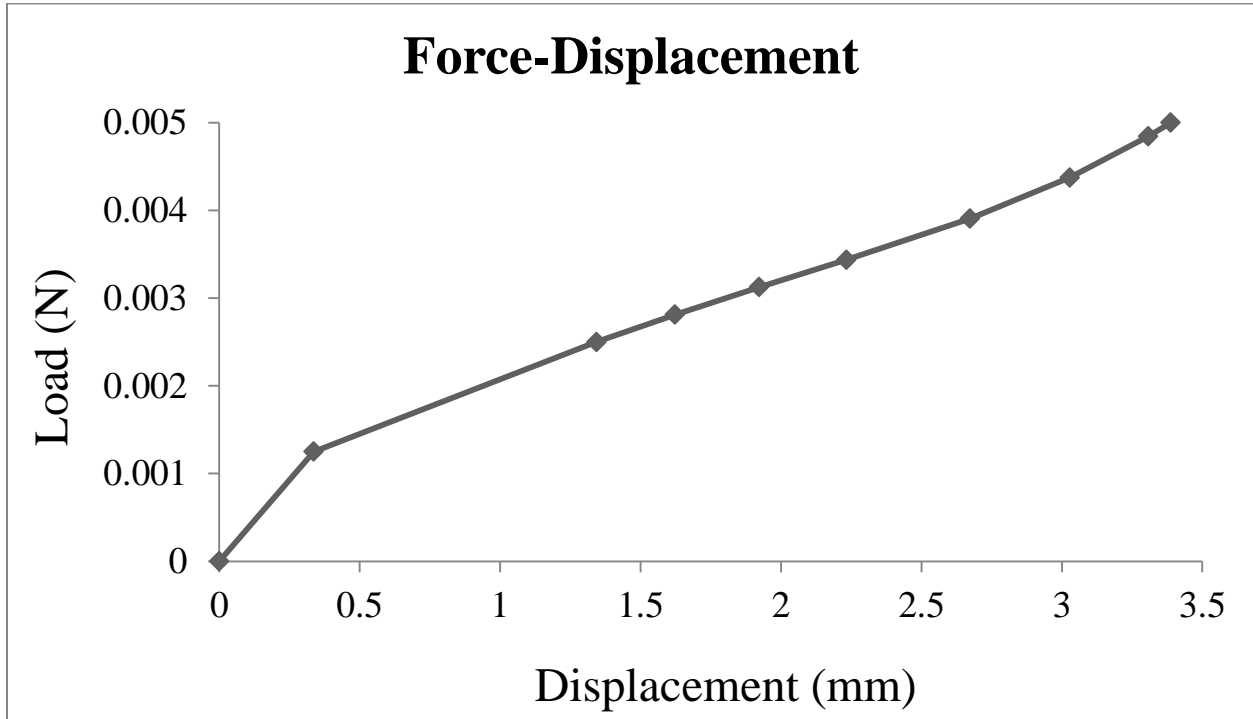


Figure 21. Load-Displacement for the Hydrogel Due to The Point Load.

### 6.2.2. Case II: Contact by a Rigid Plate

This type of loading is a simplification for the contact between the finger and the lens. Since contact lens is a soft material and relatively small, the finger surface is considered as a rigid plate. As shown in the Fig. 22, the rigid plate has an initial distance with the lens surface. The perimeter of the lower side of lens is fixed and a vertical displacement is applied to the rigid plate. The initial distance between the rigid plate and the lens surface is 0.8 mm.

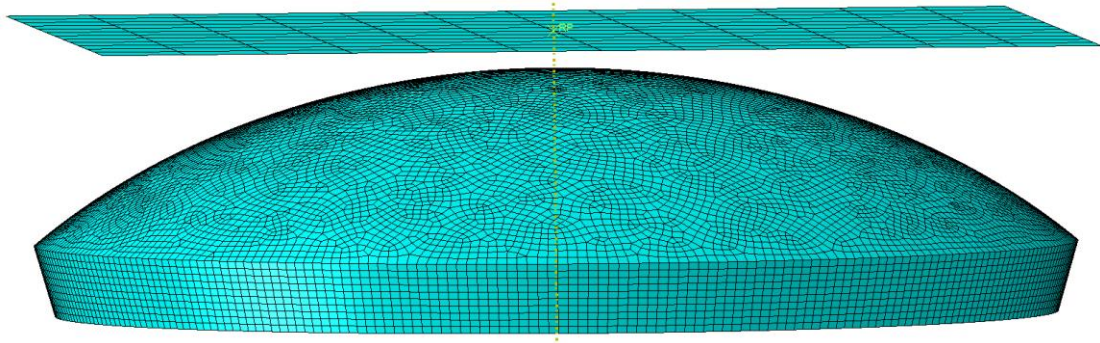
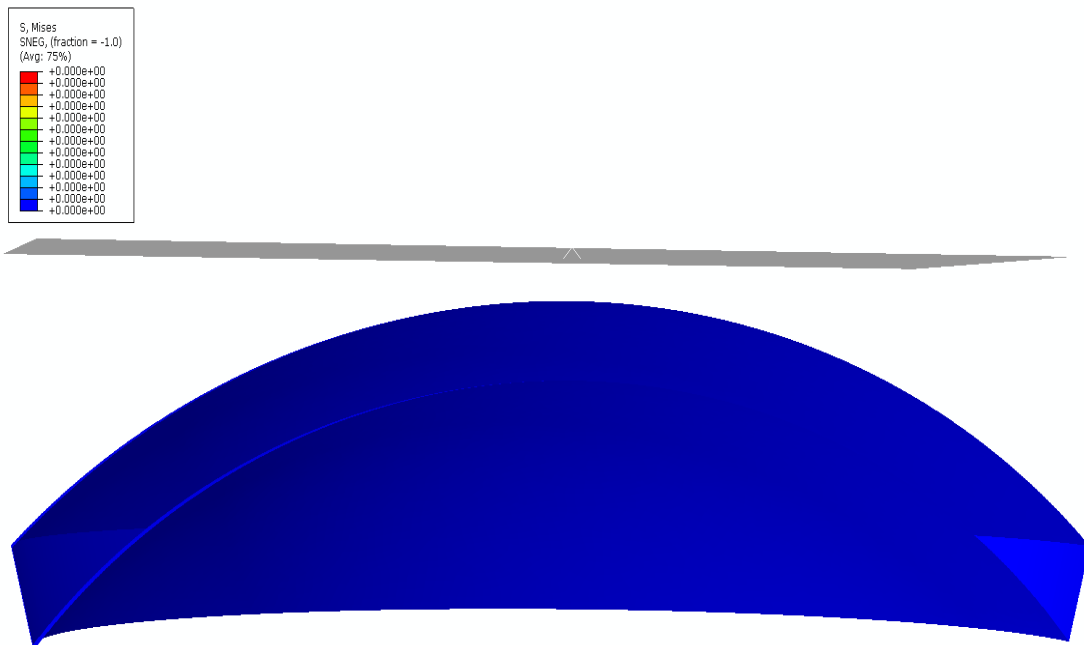
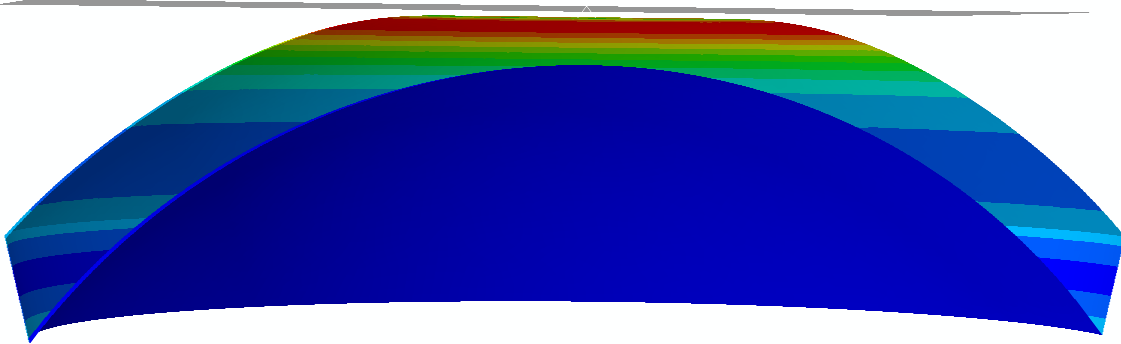
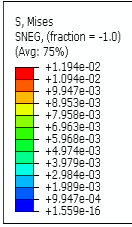


Figure 22. Initial Contact Model.

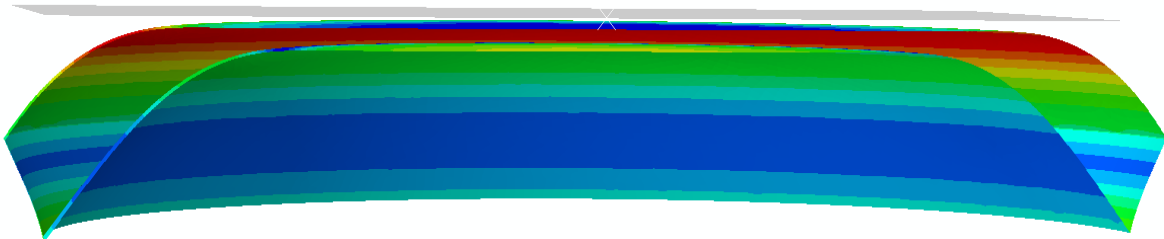
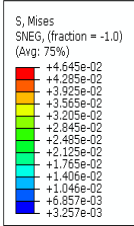
Deformation mechanism and the stress distribution for the hydrogel are shown in the following figure.



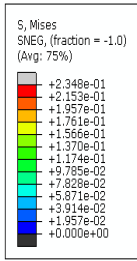
(a)



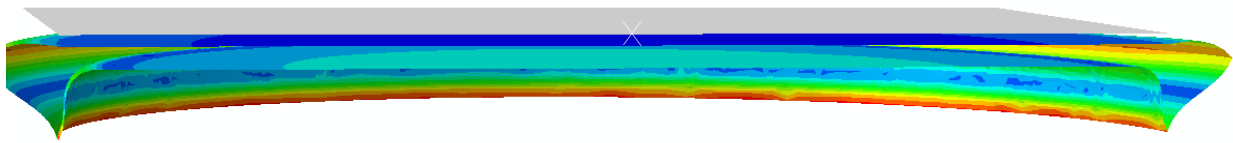
(b)



(c)



Step: Step-1 Frame: 12  
Total Time: 1.000000



(d)

Figure 23. Stress distribution due to the contact between hydrogel and rigid plate.

To investigate the mechanical behavior of the gel, the force-displacement graph is calculated and shown in Fig. 23. Due to the hyper elastic behavior of the gel, a softening regime occurs followed by a hardening regime. In this scenario, deformation mechanism is more similar to punching rather than buckling. Thus lens resists a greater force in comparison with the point load.

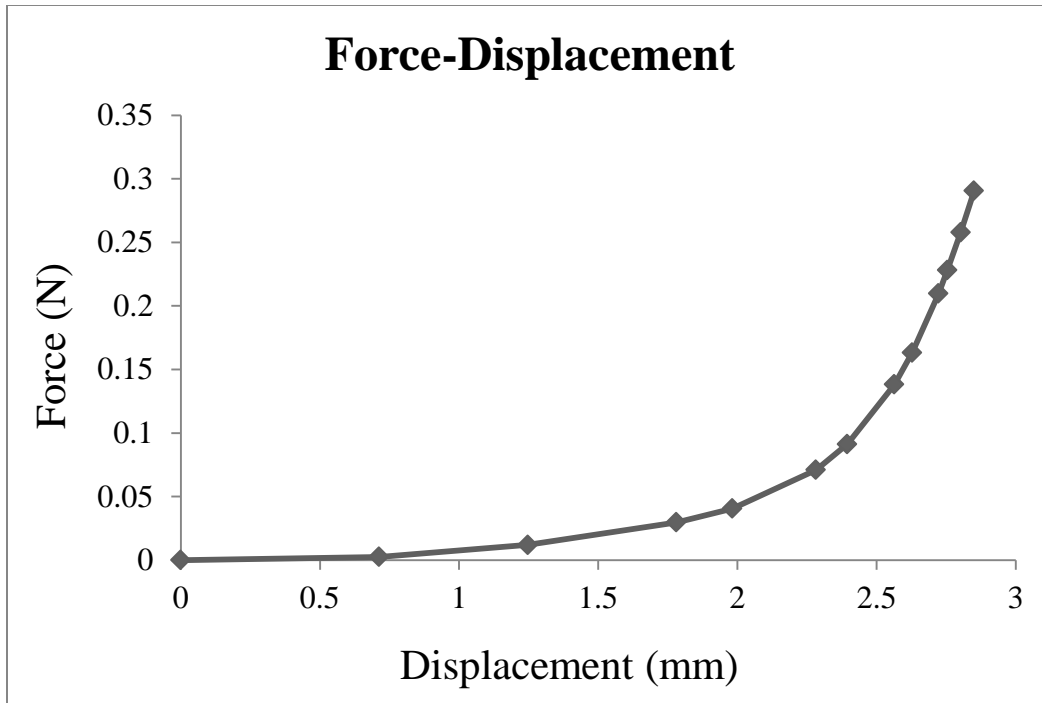


Figure 24. Force.vs.Displacement for the contact scenario.

### 6.2.3. Case III: Uniform Side Pressure

One of the main issues about the contact lenses, is in removing them from the eye. There several aspects for this problem including the adhesion between the eye and contact lens and how it may damage the eye or the lens. In this study, we are trying to model effect of adhesion by a distributed load on the inner side of the lens. Beside, a uniform loading is applied from the lens side to mimic the situation when the lens is removed by hand. The only boundary condition for this problem is that the symmetry line of the model can only deform in the Y or vertical direction. In other words, if we cut the model in two equal pieces from the symmetry line, the only degree of freedom for the cut section is in the vertical direction. The model including the boundary conditions and the applied loads are all shown in the Fig 24.

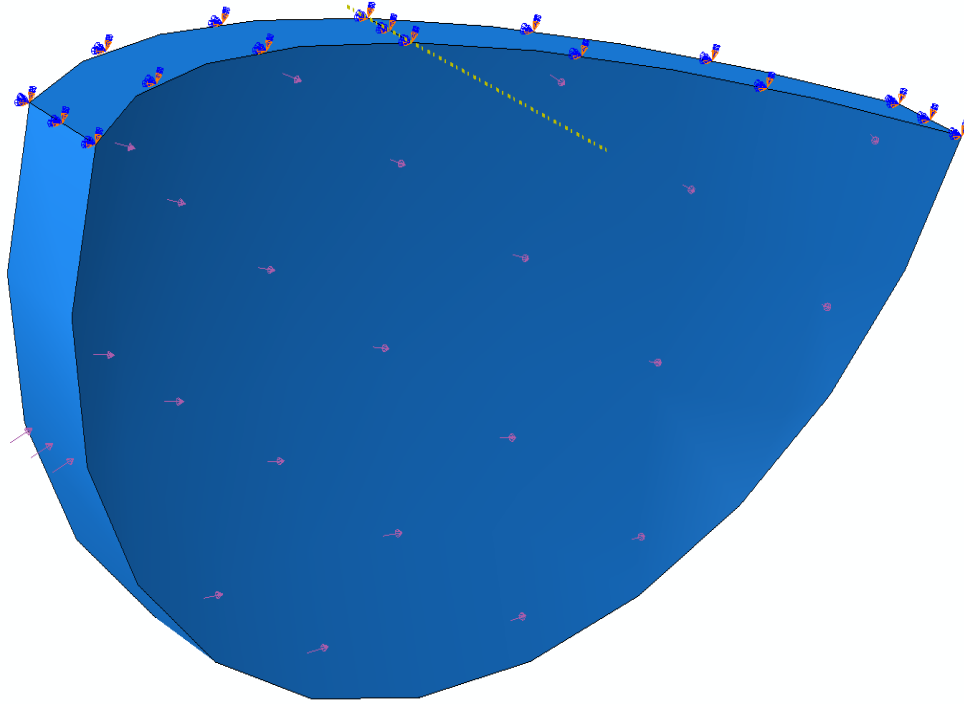
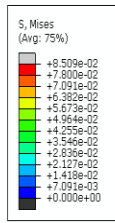


Figure 25. Uniform displacement model.

The distributed load on the inner surface of the model (Adhesion force) equal 5 Pa. Also the side load equals to 2 mN. The following figure shows the deformed lens and the stress distribution in the model. Due to the buckling mechanism and high nonlinearity of the geometry and material, the applied loads are considered to be small and the meshes are very fine. The total number of the elements of the model is 5116.



Step: Step-1 Frame: 6  
Total Time: 1.000000

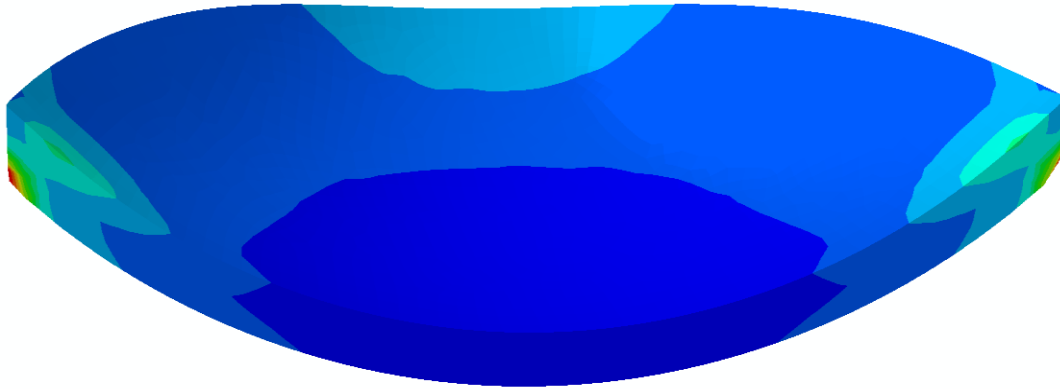


Figure 26. Stress contour for the deformed hydrogel.

In order to study the mechanical behavior of the system, force displacement graph is calculated for a node in the cut section. The results demonstrate the buckling behavior, where there is a fall in the force displacement section.

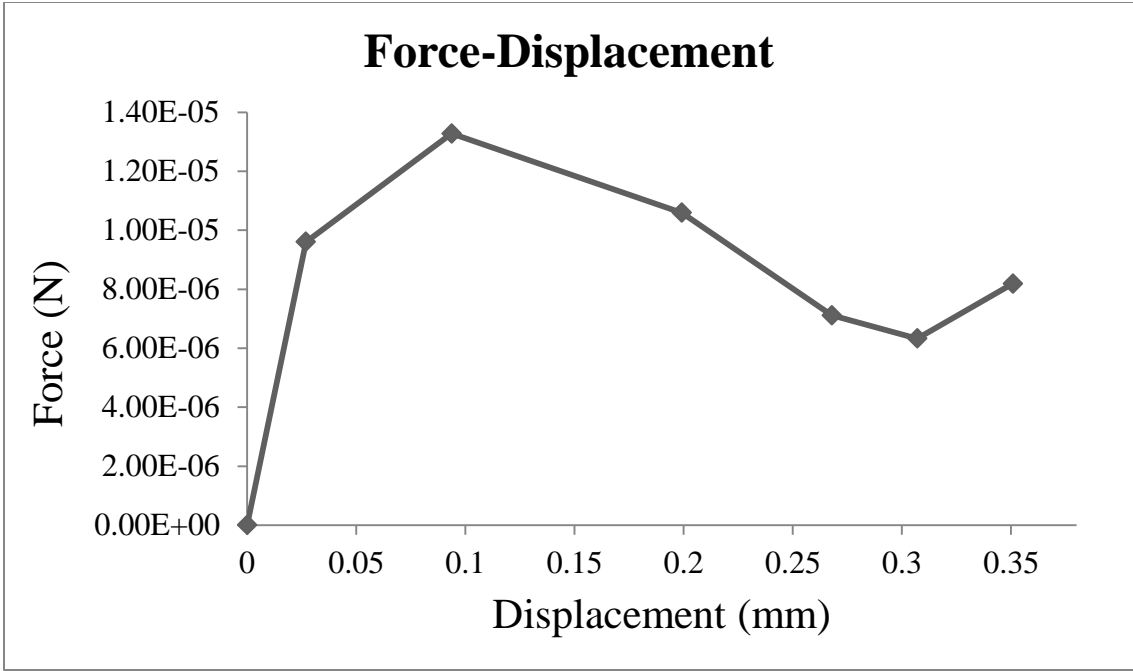


Figure 27. Force s Displacement for the hydrogel in the uniform displacement scenario.



## 7. Summary

In this research, crosslinked hydrogels are studied through different scales. Molecular dynamics simulations are performed to study the equilibrium structure and the effect of water on the elastic properties of hydrogels. Analysis of structure through radial distribution functions shows that the crosslink zones are the more hydrophilic parts of hydrogel. Also, the diffusion coefficients are quantified for different water percentages, before and after the crosslinking. The elastic properties are calculated. Since water molecules act as lubricators, an increase in water content results in a decrease in Young Modulus. Coarse-Grained simulations are employed to study the mechanical properties. A coarse-grained model is developed for the hydrogel using MARTINI force-field. Shear simulation are performed for different water contents and the stress strain curves are reported. The results show that the coarse-grained model captures the mechanical properties more accurately and it has a good agreement with the experiment. Moreover, the results show that the 40% water content is a crucial point and greater amounts of water leads to a decrease in mechanical properties. Finally, continuum model of contact lens is studied under three different loading scenarios of: point load, contact and uniform side pressure.

## 8. Recommendations and Future Work

There are several recommendations to continue the current research, among which is:

1. In this study effect of water on the mechanical properties are studied using atomistic simulations. This research could be expanded to investigate the effect of temperature on the elastic properties.
2. Coarse-Grained simulations are performed using the existing parameters of MARTINI forcefield for polymers. DFT simulations could provide more accurate model of the hydrogels and the parameters for the non-bonded interactions could be modified.
3. Tough hydrogels will be the ultimate solution for the cartilage replacement, as one the biggest issues in biomedical engineering. In order to enhance the mechanical properties of hydrogels, reinforcements could be applied. Studying adhesion mechanisms between the fibers and the hydrogel using atomistic simulations will help to improve the toughening mechanisms.
4. Employing bottom-up approaches for designing hydrogels can't be done, unless multi-scale models are developed. In an up scaling paradigm, micro structure of the hydrogels will be manipulated to reach to desired macro scale properties.

## References

Allen, M. P, Tildesley, D. J, “Computer Simulation of Liquids”, New York: Oxford University Press, 1987.

Brooks, B. R., Bruccoleri, R. E., Olafson, B. D., States, D. J., Swaminathan, S. and Karplus, M. “Charmm: a Program for Macromolecular Energy, Minimization, and Dynamics Calculations,” *Journal of Computational Chemistry*, 4:187-217, 1983.

Büyüköztürk, O., Buehler, M. J., Lau, D, Tuakta, C. “Structural Solution Using Molecular Dynamics: Fundamentals and a Case study of Epoxy-Silica Interface” *International Journal of Solids and Structures*. 48:2131–2140, 2011.

Calvert P. “Hydrogels for soft machines”. *Adv Mater*, 743–56, 2009.

Chiessi, E, Cavalieri. F, Paradossi, G, “Water and Polymer Dynamics in Chemically Cross-Linked Hydrogels of Poly(vinyl alcohol): A Molecular Dynamics Simulation Study”, *J. Phys. Chem. B*. 111:2820-2827, 2007.

P. Dauber-Osguthorpe, V.A. Roberts, D.J. Osguthorpe, J. Wolff, M. Genest, A.T. Hagler. “Structure and energetics of ligand binding to proteins: E. coli dihydrofolate reductase-trimethoprim, a drug-receptor system”, *Proteins: Structure, Function and Genetics*, 4:31-47, 1988.

Dumitriu, S. Dekker. M, “Polymeric Biomaterials,” New York, 2002.

Frenkel, D. and Smith, B. “Understanding molecular simulation “, Academic Press, San Diego, 2001.

Friends, G. D., Kunzler, J. F. and Ozark, R. M. “Recent Advances in the Design of Polymers for Contact-Lenses,” *Macromolecular Symposia*, 98:619-631, 1995.

Garcia, F. G, Leyva, M. E, Alencar de Queiroz, A. A., Simoes, A. Z., “Durability of Adhesives Based on Different Epoxy/Aliphatic Amine Networks”, *International Journal of Adhesion and Adhesives*, 31:177, 2011.

Gautieri, A, Russo, A, Vesentini, S, Redaelli, A, Buhler, M. J, “Coarse-Grained Model of Collagen Molecules Using an Extended MARTINI Force Field”, *Journal of Chemical Theory and Computations*, 6:1210-1218, 2010.

Grujicic, M, Sun, Y. P, Koudela, K. L, “The effect of Covalent Functionalization of Carbon Nanotube Reinforcements on The Atomic-Level Mechanical Properties of Poly-Vinyl-Ester-Epoxy”, *Applied Surface Science*, 253:3009, 2007.

Harland, R. S., Prud’Homme, R. K., Eds. “Polyelectrolyte Gels: Properties, Preparation and Applications”. *American Chemical Society*. Washington, DC, 1992.

Hoffman, A. S, “Hydrogels for Biomedical Applications”, *Advanced Drug Delivery Reviews*; 64:18–23 (2012).

Jang, S. S., Goddard, W. A. and Kalani, M. Y. S. “Mechanical and transport properties of the poly(ethylene oxide)-poly(acrylic acid) double network hydrogel from molecular dynamic simulations,” *Journal of Physical Chemistry B*, vol. 111:1729-1737, 2007.

Jang, S. S., Goddard, W. A., Kalani, M. Y. S., Myung, D. and Frank, C. W. “Mechanical and transport properties of the poly(ethylene oxide)- poly(acrylic acid) double network hydrogel from molecular dynamic Simulations,” *Journal of Physical Chemistry B*, 111:14440, 2007.

- Langer, R. and Peppas, N. A. “Advances in biomaterials, drug delivery, and bionanotechnology,” *AIChE Journal*, 49:2990-3006, 2003.
- Lee, K. Y. and Mooney, D. J. “Hydrogels for tissue engineering,” *Chemical Reviews*, 101:1869-1879, 2001.
- Lee, S. G, Brunello. G. F, Jang, S. S, Bucknall, D. G. “Molecular Dynamics Simulation Study of P(VP-co-HEMA) Hydrogels: Effect of Water Content on Equilibrium Structures and Mechanical Properties” *Biomaterials*, 30:6130–6141, 2009.
- Lee, S. G. “Structure-property Relationship of Hydrogel: Molecular Dynamics Simulation Approach” *PhD Dissertation*, Georgia Institute of Technology, 2011.
- Lowman, A. M, Peppas, N. A, Mathiowitz, E. “Hydrogels” *Encyclopedia of controlled drug delivery*. John Wiley & Sons, 397–406, 1999.
- Lu, Z, Dunn, M. L, “van der Waals Adhesion of Graphene Membranes”, *Journal of Applied Physics*, 107:044301, 2010.
- Maple, J. R, Dinur, U, Hagler, A. T, “Derivation of force fields for molecular mechanics and dynamics from ab initio energy surfaces”, *Progress of National Academy of Sciences of the United States of America*, 85: 5350-5354, 1988.
- Marrink, S. J, Risselada, H. J, Yefimov, S, Tieleman, D. P, de Vries, A. H, “The MARTINI Force Field: Coarse Grained Model For Biomolecular Simulations”, *Journal of Physical Chemistry B*, 111:7812-7824, 2007.

Mayo, S. L., Olafson, B. D. and Goddard, W. A. "Dreiding - a generic force-field for molecular simulations," *Journal of Physical Chemistry*, 94: 8897-8909, 1990.

Oldiges, C. and Tonsing, T. "Molecular dynamic simulation of structural, mobility effects between dilute aqueous CH<sub>3</sub>CN solution and crosslinked PAA - Part 1. Structure," *Physical Chemistry Chemical Physics*, 4: 1628-1636, 2002.

Oldiges, C., Tonsing, T. and Wittler, K. "Molecular dynamics simulation of structural, mobility effects between dilute aqueous CH<sub>3</sub>CN solution and crosslinked PAA - Part 2. Dynamics," *Physical Chemistry Chemical Physics*, 4: 5135-5141, 2002.

Oldiges, C., Wittler, K., Tonsing, T. and Alijah, A. "MD calculated structural properties of clusters in liquid acetonitrile/water mixtures with various contents of acetonitrile," *Journal of Physical Chemistry A*, 106: 7147-7154, 2002.

Peppas, N. A., Huang, Y., Torres-Lugo, M., Ward, J. H. and Zhang, J. "Physicochemical, foundations and structural design of hydrogels in medicine and biology," *Annual Review of Biomedical Engineering*, 2: 9-29, 2000.

Peppas, N. A. "Hydrogels and drug delivery," *Current Opinion in Colloid & Interface Science*, 2: 531-537, 1997.

Peppas NA, Hilt JZ, Khademhosseini A, Langer R. "Hydrogels in biology and medicine: from fundamentals to bionanotechnology". *Adv Mater* , 1345-60, 2006.

Potter, D. E. "Computational Physics," John Wiley & Sons, New York, 1973.

Rappe, A. K, Goddard, W. A, "Charge Equilibration For Molecular Dynamics Simulations", *The Journal of Physical Chemistry*, 95, 3358, 1991.

Salahshoor, H, Rahbar, N, “Nano-scale Fracture Toughness and Behavior of Graphene/Epoxy Interface”, *Journal of Applied Physics*, 112:023510-1-6, 2012.

Sun, H. “COMPASS: An ab initio force field optimized for condensed-phase applications overview with details on alkane and benzene compounds”. *Phys. Chem. B* 102:7338, 1998.

Sun, H, Ren, P, Fried, J. R, “The COMPASS force field: Parameterization and Validation for Phosphazens”, *Computational and Theoretical Polymer Science*, 8 (1/2) 229, 1998.

Swope, W. C., Andersen, H. C., Berens, P. H. and Wilson, K. R. “A computer-simulation method for the calculation of equilibrium-constants for the formation of physical clusters of molecules - application to small water clusters,” *J Chem Phys*, 76: 637-649, 1982.

Tamai, Y., Tanaka, H. and Nakanishi, K. “Molecular dynamics study of polymer-water interaction in hydrogels .2. Hydrogen-bond dynamics,” *Macromolecules*, 29: 6761-6769, 1996.

Tamai, Y. and Tanaka, H. “Effects of polymer chains on structure and dynamics of supercooled water in poly(vinyl alcohol),” *Physical Review E*, 59: 5647-5654, 1999.

Tamai, Y. and Tanaka, H. “Structure and dynamics of poly(vinyl alcohol) hydrogel,” *Molecular Simulation*, 21: 283-301, 1999.

Theodorou, D. N, Suter, U. W, “Detailed Molecular Structure of a Vinyl Polymer Glass”, *Macromolecules*. 18, 1467, 1985.

Verlet, L. “Computer Experiments on Classical Fluids .I. Thermodynamical Properties of Lennard-Jones Molecules,” *Physical Review*, 159: 98, 1967.

Wainwright SA, Biggs WD, Currey JD, Gosline JM. Mechanical design in organism. Princeton, NY: Princeton University Press; 1986.

Walter, J, Ermatchkov, V, Vrabec, J, Hasse, H., “Molecular Dynamics and Experimental Study of Conformation Change of Poly (N-isopropylacrylamide) Hydrogels in Water” *Fluid Phase Equilibria*. 296:164–172, 2010.

Weiner, S. J., Kollman, P. A., Case, D. A., Singh, U. C., Ghio, C., Alagona, G., Profeta, S. and Weiner, P. “A New Force-Field for Molecular Mechanical Simulation of Nucleic-Acids and Proteins,” *Journal of the American Chemical Society*, 106: 765-784, 1984.

Weiner, S. J., Kollman, P. A., Nguyen, D. T. and Case, D. A. “An All Atom Force-Field for Simulations of Proteins and Nucleic-Acids,” *Journal of Computational Chemistry*, 7:230-252, 1986.

Wichterle, O. and Lim, D. “Hydrophilic gels for biological use”, *Nature*, 185: 117-118, 1960.

Wu, Y, Joseph, S, Aluru, N. R, “Effect of Cross-Linking on The Diffusion of Water, Ions, and Small Molecules in Hydrogels” *J. Phys. Chem. B*. 113:3512–3520, 2009.

Wu, C, Xu, W, “Atomistic Molecular Modeling of Crosslinked Epoxy Resin”, *Polymer*, 47:6004-6009, 2006.