# AGREEMENT BETWEEN THE WHITE MATTER CONNECTIVITY BASED ON THE TENSOR-BASED MORPHOMETRY AND THE VOLUMETRIC WHITE MATTER PARCELLATIONS BASED ON DIFFUSION TENSOR IMAGING

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## ABSTRACT

We are interested in investigating white matter connectivity using a novel computational framework that does not use diffusion tensor imaging (DTI) but only uses T1-weighted magnetic resonance imaging. The proposed method relies on correlating Jacobian determinants across different voxels based on the tensor-based morphometry (TBM) framework. In this paper, we show high agreement between the TBM-based white matter connectivity and the DTI-based white matter atlas. As an application, altered white matter connectivity in a clinical population is determined.

***Index Terms***— structural connectivity, brain network, tensor-based morphometry, white matter atlas

## 1. INTRODUCTION

We aim to investigate white matter connectivity using a novel computational framework that does not rely on diffusion tensor imaging (DTI) [1]. This new method instead uses T1-weighted MRI and relies on correlating Jacobian determinants (JD), which quantifies local tissue volume based on tensor-based morphometry (TBM) [2].

The idea of correlating local morphological features to construct a structural brain network had been considered earlier [3, 4]. The previous works mainly focused on the cortico-cortical connectivity using cortical thickness [3], which is defined along the gray matter. However, cortical thickness cannot be used in directly characterizing the connectivity within the white matter. To overcome the limitation of the previous studies, we has proposed to use the JD in constructing the white matter connectivity [1]. Previously, we demonstrated that it is possible to use T1-weighted MRI in characterizing a population-based white matter connectivity without validation [1].

In this paper, we focus on validating the proposed method against the existing DTI-based white matter atlas (ICBM-DTI-81) [5]. We demonstrate that there is high agreement between the TBM-based connectivity and the DTI-based white matter atlas. As an application, we compare the TBM-based network of children who experienced early maltreatment to the normal controls and determine the regions of abnormal white matter connectivity.

## 2. METHODS

### 2.1. Subjects and preprocessing

T1-weighted MRI were collected using a 3T GE SIGNA scanner 32 children who experienced maltreatment in their early stage of life in orphanages in East Europe and China but later adopted to the families in US (post-institutionalized; PI) and age-matched 33 normal controls (NC). Two groups were matched for age. The mean age for PI is $11.19 \pm 1.73$ years while that of NC is $11.48 \pm 1.62$ years. There are 13 boys and 19 girls in PI, and 20 boys and 13 girls in NC. A study-specific template construction and non-linear normalization of individual images were done by Advanced Normalization Tools (ANTS) [6].

The correspondence should be sent to M.K.C (mkchung@wisc.edu). This work was supported by National Institutes of Health Research Grants MH61285 and MH68858 to S.D.P., funded by the National Institute of Mental Health and the Childrens Bureau of the Administration on Children, Youth and Families as part of the Child Neglect Research Consortium, as well as National Institute of Mental Health Grant MH84051 to R.J.D. This research was also supported by World Class University program through the Korea Science and Engineering Foundation funded by the Ministry of Education, Science and Technology (R31-10089) to M.K.C.

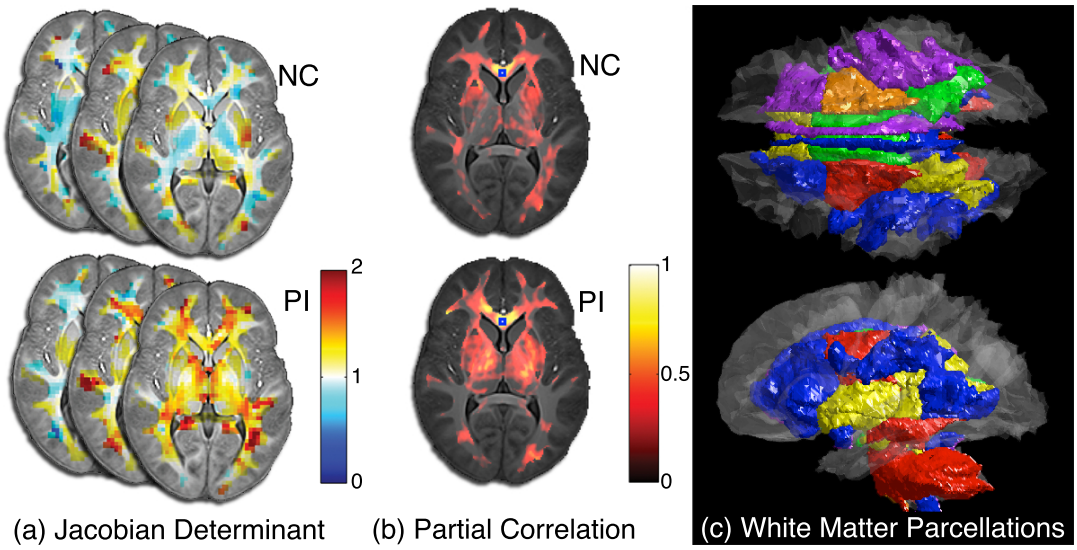


**Fig. 1**. Illustration of TBM-based connectivity. First JD is computed (a), partial correlation is computed factoring out age and gender by taking the genu of the corpus callosum as the seed (b). Then it is compared to given the white matter parcellations based on DTI (c).

### 2.2. Partial correlation on Jacobian determinants

Once we obtain the deformation field from the individual MRI to the template, we compute JD. The JD maps were smoothed with a Gaussian kernel with 2mm FWHM. Then we correlate JD across different voxels. The details on constructing JD-based correlation maps is given in [1]. Among the 336363 voxels with white matter density larger than $0.8$, 12484 voxels were subsampled at every 3mm as possible network nodes. For the nodes $i$ and $j$, we computed partial correlations $\widehat{\rho_{ij}}$ of JD while factoring out the confounding effect of age and gender. This is done as follows:

(1) Fit the general linear model (GLM) of the form

$$\text{JD} = \lambda_0 + \lambda_1 \cdot \text{age} + \lambda_2 \cdot \text{gender} + \text{noise}$$

at each node independently using the least squares method.

(2) Compute the residual between the observation and the model fit at each node.

(3) Compute the Pearson correlation between the residuals on the nodes $i$ and $j$. This Pearson correlation is the partial correlation.

We will only consider positive correlations as conventionally investigated in the many structural brain network studies [7]. This process of constructing TBM-based white matter connectivity is illustrated in Fig. 1

### 2.3. Connectivity between parcellations

The constructed partial correlation maps were compared against the DTI-based white matter atlas (ICBM-DTI-81) [5]. In the atlas, 50 anatomical subregions in white matter were manually parcellated by radiologists guided by the fractional anisotropy (FA) map and the orientation map based on DTI. The atlas does not segment all the white matter voxels into partitions, but only labels reliably identifiable voxels that correspond to the major fiber bundles such as corpus callosum, corona radiata and longitudinal fasiculus.

The ICBM-DTI-81 white matter parcellations are given in the MNI-152 template space. In order to normalize the white matter parcellations into our study-specific template, we first warped the MNI-152 T1-weighted template into our template, then applied the warping field to the parcellations. Fig. 1 (c) shows the superimposition of the 50 parcellations onto our template space. We assume that, if the white matter connectivity obtained from TBM follows that of DTI, the connectivity within a parcellation will be greater than the connectivity between different parcellations. Note that we should not expect any connectivity between different white matter parcellations.

The $\mathcal{C}_k$ be the region containing a collection of nodes that belongs to the $k$-th parcellation. We do not have any nodes in $\mathcal{C}_{49}$ and $\mathcal{C}_{50}$ possibly because the parcellations are too small, thus they are excluded in the further analysis. The connectivity matrix $\boldsymbol{X} = (X_{mn})$ between the parcellations is given by averaging partial correlations $\widehat{\rho_{ij}}$ over all possible connections:

$$X_{mn} = \frac{1}{N} \sum_{i \in \mathcal{C}_m, j \in \mathcal{C}_n} \widehat{\rho_{ij}}, \tag{1}$$

where $N$ is the total number of correlations.

The diagonal elements in $\boldsymbol{X}$ measure connectivity within

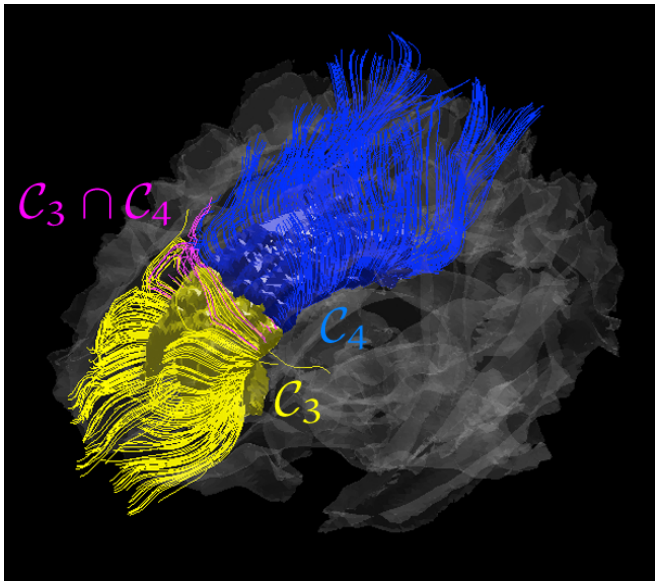


**Fig. 2**. An example of DTI fiber tracts that pass through the distinct parcellations $\mathcal{C}_3$ (yellow) and $\mathcal{C}_4$ (blue) and tracts that pass through $\mathcal{C}_3$ and $\mathcal{C}_4$ simultaneously (magenta).

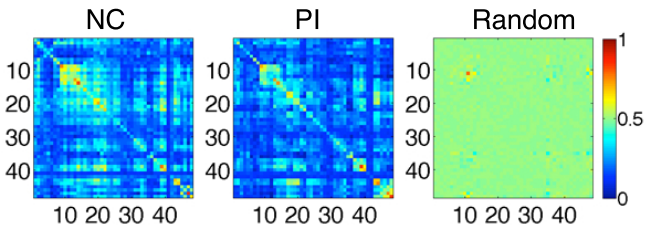


**Fig. 3**. Estimated connectivity matrices $X_{mn}$ for NC, PI and one of random networks

each parcellation. We will call the diagonal term as *within-connectivity* in this paper. The off-diagonal elements measure connectivity between two different parcellations, and will be called as *between-connectivity*. It is expected that there is no or minimal connectivity between distinct white matter parcellations. Fig. 2 shows the small number of tracts passing through both $\mathcal{C}_3$ (the genu of corpus callosum) and $\mathcal{C}_4$ (the midbody of corpus callosum) simultaneously, which usually occurs at the boundary of the two parcellations. Hence, *if the TBM-based connectivity map really follows the underlying white matter fibers, the within-connectivity should be relatively larger than the between-connectivity*.

To test our hypothesis, we constructed a null model of having no meaningful connections with 500 random networks. The random networks are generated by simulating $\rho_{ij}$ as uniformly random variables in $[0, 1]$. Then the corresponding connectivity matrix is also computed following (1). Connectivity matrices for NC-, PI-networks and one of 500 random networks are shown in Fig. 3. Then we tested if the

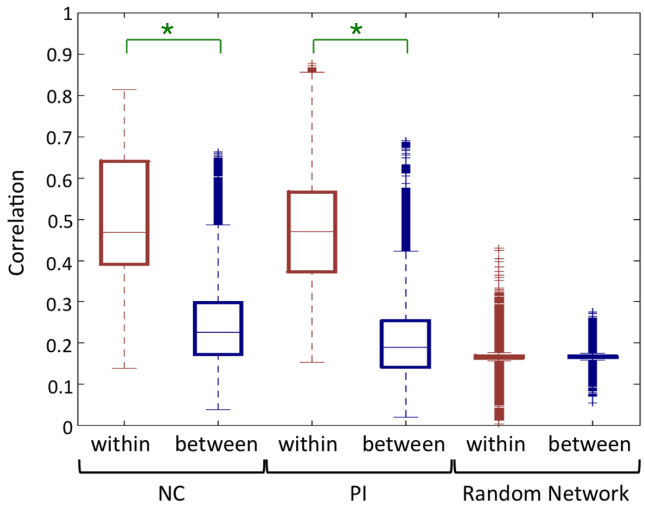


**Fig. 4**. The Wilcoxon rank sum test was applied to testing the between- and within-connectivity difference in the NC-, PI- and random networks. Significant differences are indicated with asterisks at $\alpha = 0.001$ level.

median of the within-connectivity is different to the median of the between-connectivity using the Wilcoxon rank sum test. Since we have only one connectivity matrix for a group, we used the jackknife resampling technique for inferences. In the jackknife resampling on $k$ subjects, one subject is removed and the remaining $k - 1$ subjects are used to generate a single network. This process is repeated for each subject to produce $k$ networks.

We also tested if the connectivity is locally different between PI and NC. We only tested on the diagonal elements $X_{mm}$ since the off-diagonal elements are supposed to be noise. The resulting $p$-values were corrected for multiple comparisons using the Bonferroni procedure.

## 3. RESULTS

The median of the within-connectivity is significantly greater than that of the between-connectivity both in the NC- and PI-networks ($p < 0.001$) whereas the difference is not significant in the random networks ($p = 0.37$) (Fig. 4). *The result demonstrates that the proposed TBM-based connectivity really follows the underlying white matter fiber structures.*

In the local inference on the network differences, we found significant differences in the within-connectivity between the NC and the PI ($p < 0.01$, Bonferroni corrected). The regions of significant network differences are shown in Fig. 5. We found smaller connectivity at the genu of corpus callosum (GCC) connecting anterior regions of hemispheres, and at the left superior corona radiata (SCR-L) connecting hypothalamic projection to the superior regions of neocortex (blue). We also found greater connectivities at three fiber

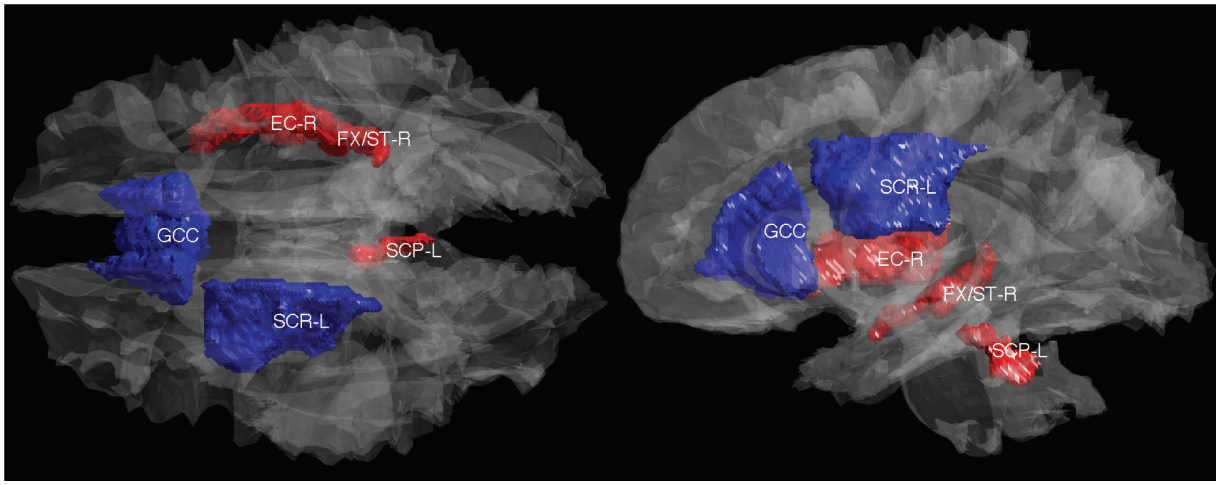


**Fig. 5**. White matter parcellations that show significant group differences in the connectivity between NC and PI. The mean correlation is greater in the PI than the NC (red) at the right external capsule (EC-R), the right fornix and stria terminalis (FX/ST-R) and the left superior cerebellar peduncle (SCP-L). The mean correlation is smaller in the PI than the NC (blue) at the genu of corpus callosum (GCC) and the left superior corona radiata (SCR-L).

bundles at . the right external capsule (EC-R), the right fornix and stria terminalis (FX/ST-R) and the left superior cerebellar peduncle (SCP-L) (red).

## 4. DISCUSSION

The within-connectivity is significantly greater than the between-connectivity in the human brain. The result suggests that the connectivity maps obtained in TBM is in agreement with the existing white matter fiber bundles. However, a further study that directly compares the TBM connectivity to DTI tractography results is needed.

In addition, we found the within-connectivity was locally different between the groups in few pacellations. According to a recent review [8], severe stress during the early developmental stage is found to related to atrophy in brain structures including the corpus callosum. Our result may be related to an altered integrity of white matter connectivity due to stressful early maltreatment.

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