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Microstructure, Phase Transformations, and Properties of Hot-Extruded Ni-Rich NiTi Shape Memory Alloy

Z. Lekston, M. Zubko, K. Prusik, and D. Stróż

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Processing of NiTi shape memory alloys strongly influences their microstructure, phase transformations, mechanical, and shape memory properties. Hot forging, hot swaging, or hot rolling are efficient techniques for obtaining the desired shape, but during multiple operations the material must be heated and worked in the temperature range from 700 to 900 °C. During these processes, intense oxidation takes place. In order to reduce it, the hot-pack working is applied. The hot extrusion is more effective for reduction of ingot, billet, and rod diameters than hot forging, hot swaging, or hot rolling. Also, during hot extrusion the material surface undergoes considerably less oxidation. In the present work, results of the characterization by differential scanning calorimetry, low-temperature x-ray powder diffraction, and three-point bending and free recovery ASTM F2082-06 tests of the samples after hot direct extrusion and heat treatment are presented. The obtained alloy after hot direct extrusion exhibits desired shape memory effect. The phase transformations during cooling and heating cycle occur with the presence of the R phase. The range of the characteristic temperatures for the obtained material gives possibility for further medical applications. After annealing at 400 and 500 °C, the characteristic temperatures shift to higher values.

Keywords hot direct extrusion, LTXRD, NiTi shape memory alloy, one-way shape memory effect, phase transitions

1. Introduction

NiTi alloys with near-equiatomic composition, commonly known as Nitinol alloys, exhibit shape memory and superelastic effects (Ref 1, 2). They are also materials used in the medical applications (Ref 3-10). For their wider usage development of easier and more effective ways of metalworking is necessary. Melting, casting, metalworking, and heat treatments of NiTi shape memory alloys strongly influence their microstructure, phase transformations, mechanical, and shape memory properties (Ref 11, 12). Due to the fact that molten titanium is highly reactive, the NiTi alloys must be melted in high vacuum or in an inert gas atmosphere (Ref 12, 13). Vacuum induction melting (VIM) and vacuum arc remelting (VAR) are commonly used for production of NiTi shape memory alloys. In VIM process usually high-purity, high-density, and low-porosity graphite crucibles and molds are used (Ref 11, 13-15). CaO crucibles are preferred for extenuation of carbon content in NiTi melts. Unfortunately, such crucibles are not resistant to thermal shock and often crack during

melting process (Ref 13). The main advantage of VIM method is the obtained homogeneity of chemical composition of the ingot, because electrical eddy currents and electrodynamic forces induced in the graphite crucible and in the metallic charges result in the whirling and mixing of the melt (Ref 12, 16). High-quality NiTi alloys can be produced by VAR method, however, multiple re-melts are required to achieve acceptable homogeneity (Ref 16). The larger size ingots in the industrial production of NiTi shape memory alloys are routinely produced using the VIM/VAR double-melt process (Ref 16). After casting and homogenization heat treatment, the ingots must be hot worked to semi-finished products. Depending on the final product shape, various techniques such as press forging, rotary forging, extrusion, swaging, bar rolling, and sheet rolling, wire drawing may be used in the hot working stage (Ref 11, 13). Following hot working, Nitinol alloys are cold worked and heat-treated to obtain final dimension and shape and with desired physical and mechanical properties. During cold drawing of wires, multiple reductions of diameters and frequent inter-pass annealing at 600-800 °C is require (Ref 16).

During the hot working intense, oxidation of the material surface takes place. To prevent oxidation, the NiTi billets have been canned in mild steel for hot working. This technique was used for swaging, forging, and extrusion (Ref 13). The direct and indirect extrusion are applied to production of tubes and hot working of ingots and billets (Ref 17, 18). Direct extrusion of NiTi ingots could be performed without protective sleeve at temperatures of 950-1050 °C with the extrusion ratios of 11:1 and 6:1 (Ref 18). During indirect extrusion, the NiTi billets were canned into a protective Cu alloy and processed at temperature of about 900 °C with extrusion ratios from 27:1 to 18:1 (Ref 19). The wire of functionally graded TiNi shape memory alloy which varies in Ti-Ni compositions along the wire axis was laboratory fabricated by new pulse current pressure sintering and the subsequent hot extrusion process. A billet of 5 mm in diameter was hot extruded into a wire of

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2 mm in diameter. Hot extrusion process was carried out at 800 °C with extrusion ratio 6.25 (Ref 20). Recently, the laboratory direct extrusion test was performed to provide the cold work of the Cu-Zn-Al shape memory alloy in the as cast rod condition. The diameter was reduced from 12 to 10 mm at extrusion ratio 1.44 (Ref 21).

In the present studies, the shape memory alloy with nominal composition Ni_{50.8}Ti_{49.2} obtained by conventional VIM technique is presented. The alloy has promising characteristics for medical application. The hot direct extrusion without protective sleeve was applied for processing of the studied material. The aim of this study was to examine the possibility of using hot extrusion for rough metalworking of NiTi ingots obtained by VIM method at the laboratory scale and to determine the phase composition, temperature, and the sequence of phase transitions and to investigate the shape memory effect. In this work, the characteristic temperatures of phase transformations hysteresis and one-way shape memory effect obtained by differential scanning calorimetry (DSC) method, low-temperature x-ray powder diffraction (LTXRD) technique, and three-point bending and

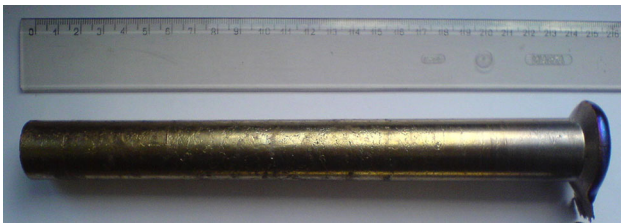


Fig. 1 The 900 g NiTi ingot obtained after vacuum induction melting



Fig. 2 Laboratory press (1000 kN) equipped with attachment for hot direct extrusion. By *A* the steel ram is marked, *B* is the container, *C* is the mounting position of extrusion die inside in container. By *D* electrical furnace for heating samples up to about 1100 °C is marked

free recovery ASTM F2082-06 (TPBFR) tests of the samples after hot direct extrusion and heat treatment are presented.

2. Material Processing

The studied alloy was prepared from high purity (>99.99 wt.%) nickel and titanium rods using Balzers VSG-10 vacuum induction melting furnace. In order to reduce the carbon contamination of the ingot the high-quality, low-porosity, and high-density graphite crucible and graphite mold were used. The melting process was started when in the furnace 5×10^{-3} Pa vacuum was obtained. The ingot of 900 g (Fig. 1) was homogenized in the electrical vacuum furnace at 900 °C for 48 h in the vacuum of 2×10^{-5} Pa. After homogenization, the ingot was cut into two parts. One of them was packed in steel pipe and subsequently hot forged and the second one was hot direct extruded using laboratory 1000 kN press equipped with electrical furnace for heating the samples up to 1100 °C (Fig. 2). The extrusion process was carried out at about 900 °C. As a lubricant MoS₂ was used. The extrusion die and the rod obtained after hot direct extrusion is presented on Fig. 3. In the last step, the obtained rod was straightened and thin oxidation layer was removed by machining. The diameter of material was



Fig. 3 Extrusion die and a rod after hot direct extrusion

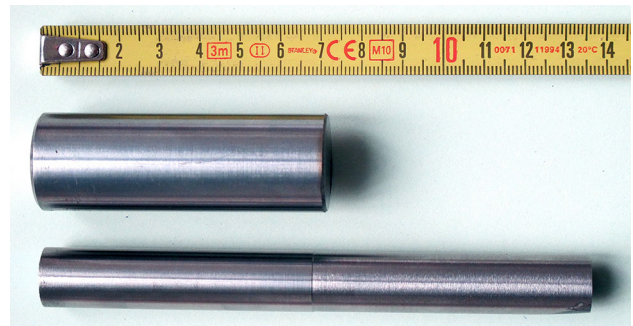


Fig. 4 Billet and extruded rod of studied material after removing of oxide layer. The reduction of diameter is from 25 to 15 mm

reduced from 25 to 15 mm at extrusion ratio 2.34 (Fig. 4). Samples for further studies were cut from the obtained resulting material (Fig. 5).

3. Experimental

The x-ray powder diffraction measurements in 2θ range from 37° to 47° were performed on a PANalytical Empyrean

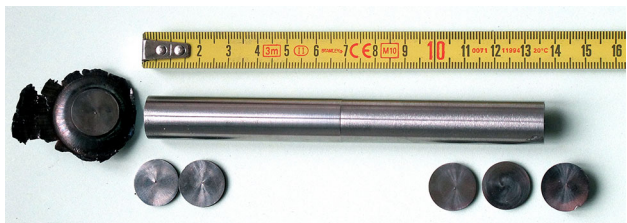


Fig. 5 The straight-extruded NiTi rod after removing the oxide layer by the machining. Cut samples prepared for investigations are also shown

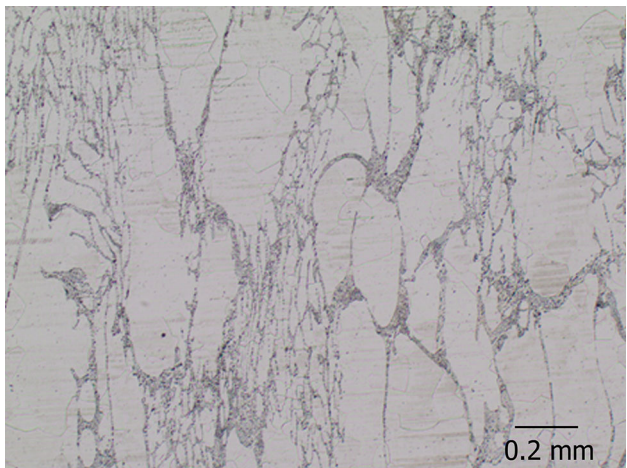


Fig. 6 Microstructure of the extruded alloy—longitudinal cross-section (optical microscopy)

diffractometer equipped with Anton Paar TTK450 low-temperature chamber at temperatures from -180 to 250°C . The measurements were performed with 5°C steps resulting heating rate of $0.7^\circ\text{C}/\text{min}$. DSC measurements were performed on Mettler Toledo DSC1 calorimeter during cooling and heating at rate of $10^\circ\text{C}/\text{min}$. Shape recovery studies were carried out using three-point bending and free recovery ASTM F2082-06 tests with heating rate of $10^\circ\text{C}/\text{min}$. The microstructure was studied by optical microscope Olympus GX-51 and JEOL JSM 6480 scanning electron microscope attached with the IXRF energy dispersion detector.

4. Results

The optical micrograph of the central part of the extruded rod is shown in Fig. 6. The average grain size is about $50\text{--}80\ \mu\text{m}$. Significant differences of microstructure have not been observed on cross sections of the central part, head, and foot parts of the rod after extrusion. The images show elongation of some grains after hot extrusion. Additionally,

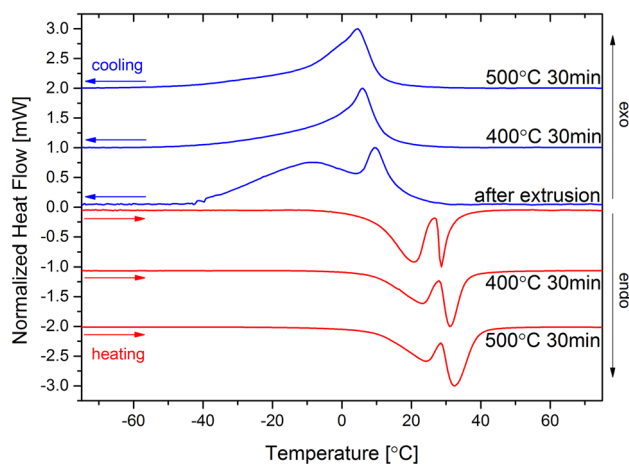


Fig. 8 DSC measurements recorded during cooling and heating cycle for samples after hot extrusion and after further annealing at 400 and 500°C for $30\ \text{min}$

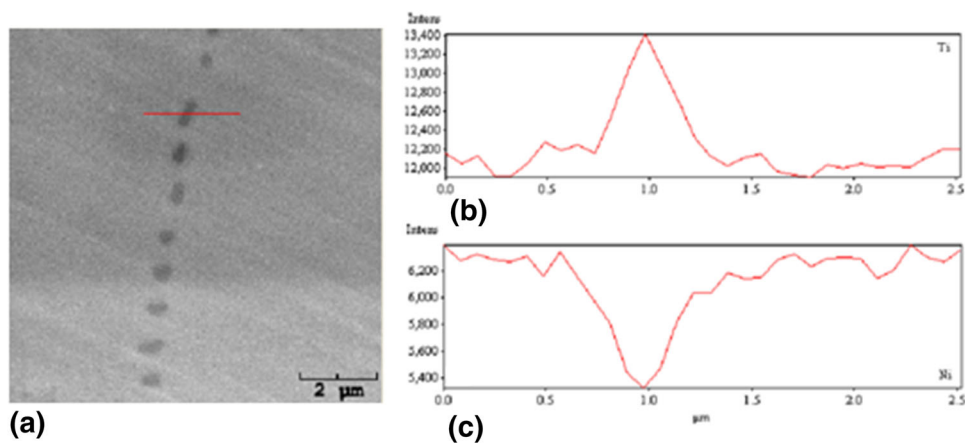


Fig. 7 SEM image of the eutectics region (a) and the Ti (b) and Ni (c) distribution along the red line in (a)

some eutectics in the grain boundary regions were observed. Since x-ray diffraction did not show any other than B2 phase in these samples, the EDS experiments along the line passing the eutectics region were carried out (Fig. 7). It occurred that the second phase in the eutectics is slightly enriched in titanium and reduced in nickel. However, the changes are very small. Generally, it looks as if during extrusion the sample undergoes dynamical recrystallization. The structure and phase composition of the extruded samples will be the subject of following study.

Performed DSC measurements (Fig. 8) show that the samples after hot direct extrusion and further annealing at 400 and 500 °C undergo two-step phase transformation during cooling and heating which can be explained by the existence of the R phase transition. During cooling, the phase transitions are not resolved as clearly as upon heating. From the DSC measurements, it is also visible that the characteristic temperatures shift slightly with increasing annealing temperature. The

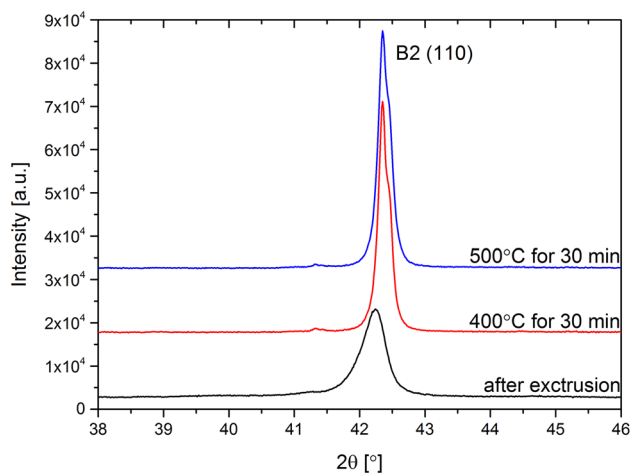


Fig. 9 X-ray powder diffraction patterns recorded at temperature of 35 °C for samples after hot extrusion and after further annealing at 400 and 500 °C for 30 min

M_s temperature shifts toward lower values whereas A_f temperature shifts toward higher values increasing the hysteresis loop.

Figure 9 shows x-ray powder diffraction patterns recorded at 35 °C for samples after extrusion and further annealing at 400 and 500 °C for 30 min. In all the presented diffraction patterns only B2(110) peak is observed which indicates that the studied material below human body temperature has structure of B2 parent phase and is suitable for medical applications.

Color maps of the temperature dependence of LTXRD patterns collected during cooling cycle (Fig. 10) show phase transformations. The B2 → R transition is visible as B(110) peak splitting into R(011) and R($\bar{1}$ 01) peaks. R → B19' phase transition is visible as appearance of martensite diffraction peaks (marked by M) and slowly disappearing of R phase peak doublet. During heating, the phase transformation occurs also with the existence of the R phase but the phases coexist in a smaller temperature range. LTXRD measurements have advantage over the DCS measurements because they provide also additional information about phases coexistence during phase transformations (Ref 22). Based on the LTXRD measurements, it is possible to determine the narrow temperature range where only R phase is present during cooling as well as during heating cycle.

LTXRD measurements can be also used in order to obtain the characteristic temperatures of phase transitions. In our studies, the obtained from this method A_f temperatures are lower than the ones from DSC and shape recovery measurements (Table 1). This is caused by different heating rates used in both cases (Ref 23). In the x-ray measurements, the rate of the temperature change was 0.7 °C/min while in the DSC and

Table 1 Comparison of A_f temperatures obtained from DSC, shape recovery, and LTXRD measurements

| | DSC, °C | Shape recovery, °C | XRD, °C |
|--------------------|---------|--------------------|---------|
| After extrusion | 31.9 | 28.5 | 21.5 |
| Annealed at 400 °C | 35.9 | 35.5 | 22.8 |
| Annealed at 500 °C | 39.4 | 40.8 | 23.9 |

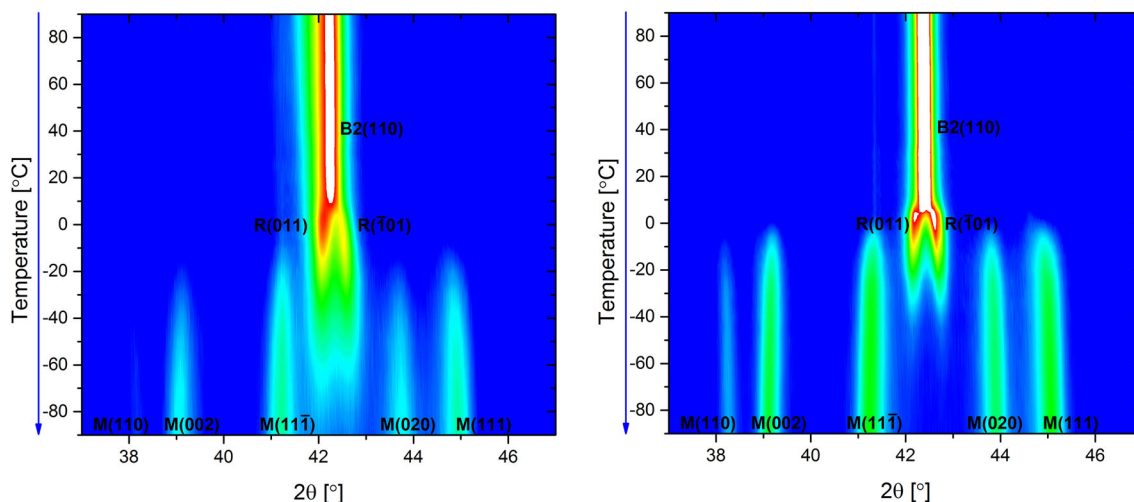


Fig. 10 Color maps of the temperature dependence of LTXRD patterns collected during cooling cycle for sample after hot extrusion (left) and after additional annealing at 500 °C for 30 min (right)

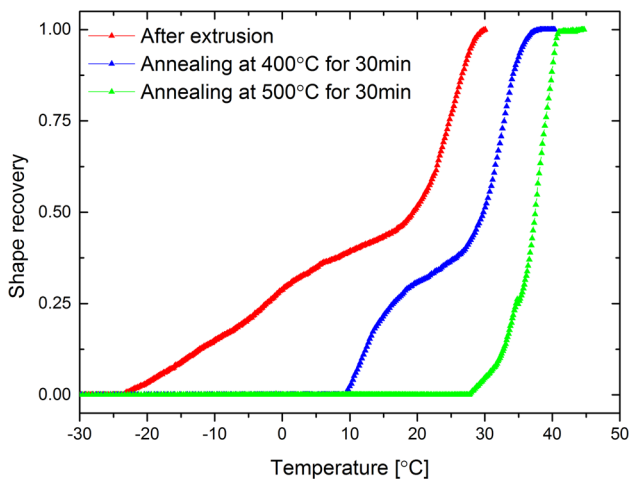


Fig. 11 Shape recovery curves of the studied samples

shape recovery measurements it was 10 °C/min. High heating/cooling rates might influence the transformation detection. Therefore, it looks that the x-ray studies in which the temperature changes were slow, are more trustful for the characteristic temperatures determination.

In Fig. 11, shape recovery curves of the studied samples are presented. The obtained curves clearly show that the materials have the desired shape memory properties. With increasing annealing temperature, the characteristic temperatures of the phase transformations shift to the higher values. On the obtained curves, the two-step character of phase transitions is also visible. The obtained characteristic temperatures are in the good agreement with the ones obtained from the x-ray powder diffraction measurements and DSC measurements. More detailed studies of shape recovery in the function of temperature will be done after successive reduction of rod diameter in next process of hot direct extrusion.

5. Conclusions

The applied hot direct extrusion process is very effective for rough and fast processing of ingots in order to obtain less-oxidized rods for further plastic working by hot rolling and hot drawing. The proposed laboratory technology allows to obtain NiTi rod with reduction of diameter from 25 to 15 mm and to preserve of desired shape memory properties of the processed material.

The sample after hot direct extrusion and samples additionally annealed at 400 and 500 °C for 30 and 60 min were tested. The measurements showed that in all studied samples occurs the reversible transformation $B2 \leftrightarrow R \leftrightarrow B19'$. Based on the analysis of the diffraction patterns recorded in the function of temperature, the characteristic temperatures of phase transitions were determined. For all studied samples, the M_s temperature is within the range from -5 to 5 °C. During the heating cycle, the transformation to the parent B2 phase occurs in the temperature range from 20 to 35 °C. Phase transition temperature determined from x-ray diffraction patterns are in good agreement with the temperatures obtained from DSC measurements. With annealing temperature increasing the characteristic temperatures of the phase transformation slightly shift toward higher values. This

tendency has been confirmed in the shape recovery measurements. For the studied alloy, the A_f temperature is below human body temperature which makes them useful in medical application. The forged and extruded rods are currently processed by hot rotary forging and hot or cold drawing and annealing to wires of different diameters.

Acknowledgments

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References

1. H. Funakubo, Ed., *Shape Memory Alloys*, Gordon and Breach Science Publishers, Amsterdam, 1987
2. K. Otsuka and X. Ren, Physical Metallurgy of Ti-Ni-Based Shape Memory Alloys, *Prog. Mater. Sci.*, 2005, **50**, p 511–678
3. T.M. Duerig, A. Pelton, and D. Stoeckel, An Overview OD Nitinol Medical Applications, *Mater. Sci. Eng. A*, 1999, **273–275**, p 149–160
4. A.R. Pelton, D. Stoeckel, and T.W. Duerig, Medical Uses of Nitinol, *Mater. Sci. Forum*, 2000, **327–328**, p 63–70
5. L.G. Machado and M.A. Savi, Medical Applications of Shape Memory Alloys, *Braz. J. Med. Biol. Res.*, 2003, **36**, p 683–691
6. J. Drugacz, Z. Lekston, K. Januszewski, and H. Morawiec, Use of TiNiCo Shape-Memory Clamps in the Surgical Treatment of Mandibular Fractures, *J. Oral Maxillofac. Surg.*, 1995, **53**, p 665–672
7. T. Yoneyama and S. Miyazaki, Ed., *Shape Memory Alloys for Biomedical Applications*, Woodhead Publishing Limited, Cambridge, 2009
8. Z. Lekston, J. Drugacz, and H. Morawiec, Application of Superelastic NiTi Wires for Mandibular Distraction, *Mater. Sci. Eng. A*, 2004, **378**, p 537–541
9. H. Morawiec, Z. Lekston, K. Kobus, M. Węgrzyn, and J. Drugacz, Superelastic NiTi Springs for Corrective Skull Operations in Children with Craniosyntosis, *J. Mater. Sci. Mater. Med.*, 2007, **18**, p 1791–1798
10. Z. Lekston, D. Stróż, and M. Jędrusik-Pawłowska, Preparation and Characterization of Nitinol Bone Staples for Cranio-Maxillofacial Surgery, *J. Mater. Eng. Perform.*, 2012, **21**, p 2650–2656
11. S.M. Russell, Nitinol Melting and Fabrication, *SMST-2000 Conference Proceedings*, S.M. Russel and A. Pelton, Ed., 30 April to 4 May, 2000 (Asilomar), SMST, 2001, p 1–9
12. M.H. Elahinia, M. Hashemi, M. Tabesh, and S.B. Bhaduri, Manufacturing and Processing of NiTi Implants: A Review, *Prog. Mater. Sci.*, 2012, **57**, p 911–946
13. C.M. Jackson, H.J. Wagner, and R.J. Wasilewski, *55-Nitinol—The Alloy with a Memory: Its Physical Metallurgy, Properties and Applications*. Report NASA-SP 5110, Washington, DC, 1972, p 1–86
14. J. Frenzel, Z. Zhang, K. Neuking, and G. Eggeler, High Quality Vacuum Induction Melting of Small Quantities of NiTi Shape Memory Alloys in Graphite Crucibles, *J. Alloys Compd.*, 2004, **385**, p 214–223
15. N. Nayan, C.N. Saikrishna Govind, K. Venkata Ramaiah, S.K. Bhaumik, K. Suseelan Nair, and M.C. Mittal, Vacuum Induction Melting of NiTi Shape Memory Alloys in Graphite Crucible, *Mater. Sci. Eng. A*, 2007, **465**, p 44–48
16. M.H. Wu, Fabrication of Nitinol Materials and Components, *SMST-2001 Conference Proceedings*, Y.Y. Chu and L.C. Zhao, Ed., September 2–6, 2001 (Kunming), SMST-SMM, 2001, p 285–292, *Mater. Sci. Forum*, 2002, **394–395**, p 285–292

17. K.B. Müller, Hot Extrusion of Nickel-Titanium (Nitinol), *SMST-2000 Conference Proceedings*, S.M. Russel and A. Pelton, Ed., 30 April to 4 May, 2000 (Asilomar), SMST, 2001, p 43–51
18. A. Tuisi, P. Bassani, A. Mangioni, L. Toia, and F. Butera, Fabrication Process and Characterization of NiTi Wires for Actuators, *SMST-2004 Conference Proceedings*, M. Mertmann, Ed., 2004, p 501–508
19. K.B. Müller, Extrusion of Nickel-Titanium Alloys Nitinol to Hollow Shapes, *J. Mater. Process. Technol.*, 2001, **111**, p 122–126
20. R. Matsui, F. Yoshida, and H. Kyogoku, *SMST-2007 Conference Proceedings*, S.M. Russel and A. Pelton, Ed., December 3-5, 2007, Tsukuba, Japan SMST, 2007, p 33–38
21. S.M. Quawabah, Effect of Direct Extrusion on the Microstructure, Microhardness, Surface Roughness and Mechanical Characteristics of Cu-Zn-Al Shape Memory Alloy, SMA, *Jordan J. Mech. Ind. Eng.*, 2012, **6(2)**, p 175–181
22. Z. Lekston and M. Zubko, Low-Temperature XRD Study of Phase Transformations in NiTi and TiNiCo Shape Memory Alloys Used for the Preparation of the Prototypes of Medical Implants, *Solid State Phenom.*, 2013, **203–204**, p 125–128
23. K. Nurveren, A. Akdogan, and W. Huang, Evolution of Transformation Characteristics with Heating/Cooling Rate in NiTi Shape Memory Alloys, *J. Mater. Process. Technol.*, 2008, **196**, p 129–134