

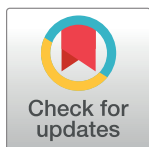
RESEARCH ARTICLE

High-resolution directed human connectomes and the Consensus Connectome Dynamics

Balázs Szalkai¹, Csaba Kerepesi^{1,3}, Bálint Varga¹, Vince Grolmusz^{1,2*}

1 PIT Bioinformatics Group, Eötvös University, H-1117 Budapest, Hungary, **2** Uratim Ltd., H-1118 Budapest, Hungary, **3** Institute for Computer Science and Control, H-1111 Budapest, Hungary

* grolmusz@pitgroup.org



OPEN ACCESS

Citation: Szalkai B, Kerepesi C, Varga B, Grolmusz V (2019) High-resolution directed human connectomes and the Consensus Connectome Dynamics. *PLoS ONE* 14(4): e0215473. <https://doi.org/10.1371/journal.pone.0215473>

Editor: Yuanquan Wang, Beijing University of Technology, CHINA

Received: November 12, 2018

Accepted: April 2, 2019

Published: April 16, 2019

Copyright: © 2019 Szalkai et al. This is an open access article distributed under the terms of the [Creative Commons Attribution License](https://creativecommons.org/licenses/by/4.0/), which permits unrestricted use, distribution, and reproduction in any medium, provided the original author and source are credited.

Data Availability Statement: The Human Connectome Project's MRI data that were applied in the present work is available at: <http://www.humanconnectome.org/documentation/S500> [5]. The graphs (both undirected and directed) that were prepared by us from the HCP data can be downloaded at the site <http://braingraph.org/download-pit-group-connectomes/>. The Budapest Reference Connectome Server [36, 37] is available at <http://connectome.pitgroup.org>. On that site, the reader can independently verify the phenomenon of the Consensus Connectome Dynamics by (i) choosing "Show options" (ii) and moving from right

Abstract

Here we show a method of directing the edges of the connectomes, prepared from HARDI datasets from the human brain. Before the present work, no high-definition directed brain-graphs were published, because the tractography methods in use are not capable of assigning directions to the neural tracts discovered. Previous work on the functional connectomes applied low-resolution functional MRI-detected statistical causality for the assignment of directions of connectomes of typically several dozens of vertices. Our method is based on the phenomenon of the "Consensus Connectome Dynamics", described earlier by our research group. In this contribution, we apply the method to the 423 braingraphs, each with 1015 vertices, computed from the public release of the Human Connectome Project, and we also made the directed connectomes publicly available at the site <http://braingraph.org>. We also show the robustness of our edge directing method in four independently chosen connectome datasets: we have found that 86% of the edges, which were present in all four datasets, get the same directions in all datasets; therefore the direction method is robust. While our new edge-directing method still needs more empirical validation, we think that our present contribution opens up new possibilities in the analysis of the high-definition human connectome.

Introduction

High-angular resolution diffusion imaging (HARDI) datasets are widely used today for the construction of connectomes or braingraphs. The nodes (or vertices) of these graphs correspond to anatomically identified [1, 2], small (1–1.5 cm²) areas of the gray matter, and two nodes are connected by an undirected edge if neural fiber tracts are discovered, connecting the gray matter areas, corresponding to the two nodes [3, 4].

The considerable advantage of the graph approach to the analysis of the human brain is that the graphs retain the relevant anatomical connection information from the MRI data, but they do not contain the—mostly irrelevant—data on the exact trajectories of the neural tracts in the white matter.

to left the "Minimum edge confidence" slider (iii) and observing the buildup of the edges on the visualization panel. If graphics problems appear then it is suggested to use another browser, e.g., Chrome. The Consensus Connectome Dynamics is visualized on a video animation on <https://youtu.be/yxlyudPaVUE> for the whole brain and on https://youtu.be/wBciB2eW6_8 for the frontal lobe only. The individual braingraphs with directed edges can be accessed at the site <http://braingraph.org/download-pit-group-connectomes/>. Each graph refers to the original HCP ID in its filename. The source code of the computer program that generated the directed connectomes is enclosed as an on-line supplementary material.

Funding: CK was supported by Momentum Grant of the Hungarian Academy of Sciences (LP2012-19/2012). VG was supported by the KH-126472 and the K-127909 grants of the National Research, Development and Innovation Office of Hungary. BV was supported by the European Union, co-financed by the European Social Fund (EFOP-3.6.3-VEKOP-16-2017-00002). The funders had no role in study design, data collection and analysis, decision to publish, or preparation of the manuscript. Uratim Ltd provided support in the form of salaries for author VG, but did not have any additional role in the study design, data collection and analysis, decision to publish, or preparation of the manuscript. The specific roles of this author are articulated in the 'author contributions' section. Data were provided in part by the Human Connectome Project, WU-Minn Consortium (Principal Investigators: David Van Essen and Kamil Ugurbil; 1U54MH091657) funded by the 16 NIH Institutes and Centers that support the NIH Blueprint for Neuroscience Research; and by the McDonnell Center for Systems Neuroscience at Washington University.

Competing interests: We have the following interests. Vince Grolmusz is a PLOS ONE Editorial Board member and is a CEO and shareholder of Uratim Ltd. There are no patents, products in development or marketed products to declare. This does not alter the authors' adherence to PLOS ONE policies on sharing data and materials.

One of the most frequently used and largest diffusion MRI datasets are the public releases of the Human Connectome Project (HCP) [5]. Numerous publications are applying HCP data in different contexts, e.g., [6–12].

Directing the connectome: The problem statement

High-angular resolution diffusion imaging methods cannot assign directions to the fiber tracts, and, consequently, to the edges of the connectomes mapped. Tractography methods can discover the trajectories, that is, the geometric curves of the fiber tracts in the white matter, but—presently—cannot determine the correct one from the two possible directions of any given fiber tract. Consequently, the connectomes of braingraphs that are prepared from the diffusion MR imaging data are *undirected graphs*.

There are enormous differences between the directed and undirected graphs. In undirected graphs, if we consider some walks, or paths, or signal propagations on the edges, all of these are allowed in both directions in all the edges. In directed graphs the edges carry unique directions, and the walks or signal propagations are allowed only in this assigned direction of the edges. Obviously, the difference is clear for everyone who has driven a car in the jungle of the one-way streets of a modern city.

Mathematically, there are also very significant differences: many graph-tasks are easy (or just trivial) for undirected graphs and hard for directed ones [13, 14]. As an easy example, let us consider an undirected, connected simple graph on n vertices with $n - 1 + \ell$ edges, and suppose we want to determine the minimum number of edges that needs to be deleted in order to make the graph cycle-free. Without even looking at the graph, we know that ℓ edges need to be deleted, since any connected graphs with more than $n - 1$ edges on n vertices contain a cycle [13, 14]. However, if we consider directed graphs and we want to get rid of all the directed cycles with the deletion of the minimum number edges, the problem becomes hard (more exactly, NP-hard, this is the famous "minimum feedback arc" problem [15]). As another example, the conditions for convergence of random walks on undirected graphs are well-understood [16–18], while they have numerous open problems on directed graphs [19].

Individual axons clearly have a well-defined direction of signal propagation from the soma to the end of the axon. Therefore, the directionality of the cerebral connections is a very relevant field of study.

Directing the connectome: fMRI-based methods

Functional MRI, on the other hand, is capable of mapping the temporal sequences of the activity of larger brain areas. Therefore, it seems to be possible to assign directions to these functional or effective connections between those larger areas of the gray matter. Several authors have attempted assigning directions to the edges of the connectomes using temporal sequences of activity changes, mostly on resting state fMRI or electro-physiology data, by applying a broad spectrum of statistical causality detection methods and models (e.g., [20–31]). The general approach of the articles listed can be described as follows: the temporal sequence of cerebral activity changes are translated to causality relations by statistical methods, and these causality relations are used to direct the connections between brain regions.

Some works criticize the feasibility of directing the functional connectomes through temporal hemodynamic sequences. The article [32] questions the inference of edge direction based on temporal precedence in these studies since the hemodynamics varies between brain regions.

Since both the fMRI data and the non-invasive electro-physiological measurements have poor spatial resolution, usually the goal of these methods is not directing the edges of the

HARDI-based, high-definition anatomical connectomes, but rather the functional connectomes on several dozens of vertices, corresponding to large areas of the gray matter, where haemodynamic activity changes were observed.

By the best of our knowledge, no significant attempts were made to direct the edges of structural connectomes (i.e., connectomes measured by HARDI) with hundreds of vertices by these methods. One possible reason is due to the poor resolution of the fMRI: it is impossible to decide that if a causality is very probable between two cortical areas A and B in the direction from A to B , then which of the hundreds of the edges, running between A and B should be directed from A to B : theoretically, even one such connection may trigger the observed haemodynamic activity in B .

Consensus connectomes

It is unusual in graph theory that hundreds of different graphs on the very same set of vertices are encountered. When we are working on braingraphs constructed from HARDI data, this is the usual scenario: the cerebral areas of the different human subjects can be corresponded to the same reference brain map [1, 2], and, consequently, the graph edges in the connectome can be compared between subjects, since the vertices or nodes are named in each subject according to the very same anatomical brain map. This process is, in fact, a non-trivial refinement of the assignment of anatomical nomenclature to cerebral areas in printed brain anatomy atlases that appeared in the last several hundred years (e.g., [33–35]).

Consensus Connectome Dynamics (CCD) is a surprising phenomenon that was observed after our construction of the Budapest Reference Connectome Server [36–38]. For the description of the CCD phenomenon, we need to clarify some functions of the Budapest Reference Connectome Server.

The webserver at the address <http://connectome.pitgroup.org> is capable of finding and visualizing connectome edges that are present in more than a pre-defined number of connectomes. More exactly, let n denote the number of all connectomes processed by the server ($n = 6$ in version 1.0, $n = 96$ in version 2.0 and $n = 418$ or $n = 476$ or $n = 477$ —depending on other settings—in version 3.0). For any k : $0 \leq k \leq n$, we say that *the frequency of an edge* is k if the edge is present in exactly k connectomes out of the n ones [39]. Clearly, if we have n connectomes then the frequency of any edge is between 0 and n : it is 0 if the edge does not appear in any connectome at all; and it is n if it appears in all the n connectomes. The *k -consensus connectome* contains all the edges with a frequency greater than or equal to k : that is, each edge in the *k -consensus connectome* is present in at least k individual connectomes.

The Budapest Reference Connectome Server is capable of generating *k -consensus connectomes* in CSV and GraphML formats for further processing and independent visualization, and on the website, users can also quickly view the resulting consensus connectomes. We note that subsequent to our work on Budapest Reference Connectome Server in 2015 and 2017 [36–38], the article [40] also covers consensus connectomes with applications in connectome error correction.

Consensus Connectome Dynamics

After the publication of the article describing the Budapest Reference Connectome Server [36], a surprising property of the server was recognized [38, 41]: when we generate *k -consensus connectomes* for $k = n$, next for $k = n - 1$, $k = n - 2$, . . . , and last for $k = 1$, then, naturally, more and more edges appear in the graphs (since the inclusion condition is weakened in every step). The surprising phenomenon is that the new edges do not appear randomly in the graph, but new edges are mostly connected to the already existing edges, forming a growing, tree-like structure

as it is shown on the video <https://youtu.be/yxlyudPaVUE>, [38, 41]. This “dynamical” observation is quantified on Fig 2 of [38], and it is statically visualized on a very large component-tree at the address http://pitgroup.org/static/graphmlviewer/index.html?src=connectome_dynamics_component_tree.graphml (for the detailed—and not entirely obvious—description of the component-tree we refer to [38]).

In [38] we called this phenomenon “Consensus Connectome Dynamics”, and hypothesized that the particular order of the appearance of the graph edges describes the order of growth of the axonal fibers of these connections in the individual brain development.

If the newly formed edges—i.e., fibers of axons—almost always are connected to the already developed edges—i.e., fibers of axons—then this hypothesis satisfyingly explains the Consensus Connectome Dynamics phenomenon, visualized on Fig 1 or at the video <https://youtu.be/yxlyudPaVUE>:

- Connections, represented by the graph edges that are present in most connectomes were grown first (e.g., edges in the n - or $n - 1$ -consensus connectomes).
- Next, the newer and newer edges were grown to be connected to the vertices of the older edges of the growing, tree-like structure, forming the k -consensus connectomes, for decreasing k values.

The newer and newer edges have gradually larger deviation, since small differences in the edge frequencies are added up in the growing structure: Clearly, if an edge e is not present in, say, 20% of the graphs, then for another edge, say f , which connects to e , will hold that the e, f edge-pair cannot be present in at least 20% of the graphs, and most probably, the e, f pair will

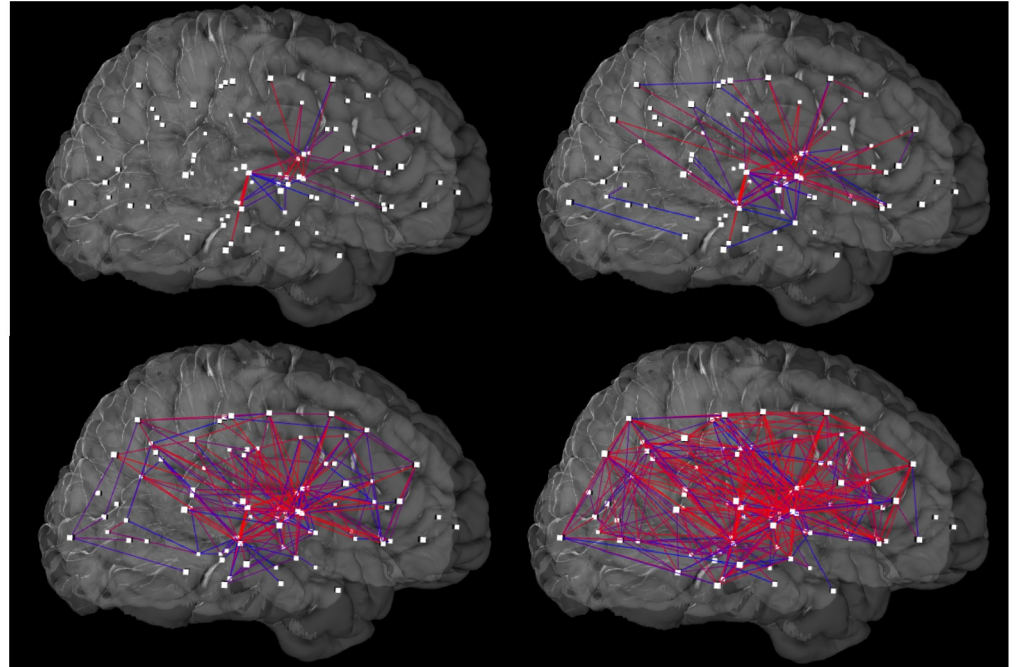


Fig 1. Four snapshots of the growing-tree-like object, prepared by the Budapest Reference Connectome Server <https://connectome.pitgroup.org>. From the upper left panel, clockwise: edges, present in at least 389 graphs; edges present in at least 322 graphs, in 230 graphs and in at least 122 graphs. (Settings for image generation: 20 k fibers, minimum edge weight 0, sagittal view).

<https://doi.org/10.1371/journal.pone.0215473.g001>

be missing from much more than 20% of all graphs, since f will be missing in some graphs, containing e . Consequently, the frequencies of the newer edges will be less than the frequencies of older edges. Therefore, we believe that the visualization at <https://youtu.be/yxlyudPaVUE>, describes *not only* the edges with gradually smaller frequencies, but also the order of growth of the connections in the human brain.

Results and discussion

In the present work, we are assigning directions to some of the edges of braingraphs, depending on the appearance of that edge in the CCD.

The edge-directing method was first described in [38]; here we clarify the method, and make the 423 directed-edge connectomes publicly available at the site <http://braingraph.org>.

We have two requirements on the edge-directing method, based on Consensus Connectome Dynamics:

- **Feasibility:** While our direct knowledge is very limited on the axonal development of the human brain in general and the directions of fiber tracts in the connectome in particular ([42, 43]), we need to build onto the available biological observations in developing our method;
- **Robustness:** The directions, assigned to the edges of the connectomes need to be as independent as possible from the selected, specific sets of connectomes in the connectome sets in CCD trials. In other words, the CCD phenomenon needs the data of dozens or hundreds of connectomes; based on these connectomes and the CCD phenomenon, we assign directions to some of the edges of the individual connectomes. However, we want these directions assigned to the edges of the individual braingraphs as independent as possible from the *particular* choice of the several dozen or several hundred connectomes included in the CCD probe.

Here we suggest an (a) Feasible and (b) Robust edge-directing method.

Feasibility

A large part of the axonal connections in the brain of mammals is developed in the embryonic state or the first several weeks after birth [43]. Microscopic studies of developing rat brains show that a considerable number of axons of the cortex (from layer V cortical neurons), in the early brain development, grow in the direction of subcortical regions [42], strengthening our CCD observation that neurons of the cortex are connected later to the subcortical structures than the connections develop between those subcortical structures.

Another important observation that forms a base of our method of directing the axonal fibers is the retrograde signaling of post-synaptic activation that stabilizes the newly formed synapses, and, consequently, prevents the retraction of the newly formed axon branches: work by numerous groups (e.g., [44–50]) witness this phenomenon.

Based on these observations, we make the following hypothesis: Neurons that are not connected to any other neuron yet, grow axons to reach other neurons.

- (i). If the branch of the axon reaches a neuron that is not connected to other neurons yet, it retracts, since the post-synaptic activity of the un-networked neuron does not stabilize the connection (i.e., the synapse).
- (ii). If the branch of the axon reaches an already “networked” neuron, that is, a neuron with connections to other neurons, then the post-synaptic activity of the “networked” neuron stabilizes the synapse and, consequently, the new connection.

Since the neuronal-level human brain graph with 80 billion neurons as vertices is unavailable today, we re-phrase the hypothesis above for the ROIs that form the 1015 vertices of our brain graphs, as follows:

ROIs that are not connected to any other ROI yet, grow axonal fibers to reach other ROIs as observed in the CCD phenomenon.

- (iii). If the fiber reaches an ROI that is not connected to other ROIs yet, the fiber retracts, since the post-synaptic activities of the un-networked neurons do not stabilize the neuronal connections.
- (iv). If the fiber reaches an already “networked” ROI, that is, an ROI with connections to other ROIs, then the post-synaptic activities of the “networked” neurons stabilize the synapses, and the new connection will survive.

We stress that—instead of the mainly unknown order or temporal sequence of axonal development on the system level—we consider the phenomenon of the Consensus Connectome Dynamics, and we direct the edges of the connectomes according to the hypotheses (iii) and (iv) above.

Robustness

The robustness of the edge direction method is built into the edge direction algorithm, as it is detailed in the “Methods” section.

Methods

The brain graphs in this study were constructed from the data of the Human Connectome Project [5], using the workflow described in [36]. The undirected brain graphs have 1015 vertices each; the whole set of 423 brain graphs can be downloaded from the site <http://braingraph.org/download-pit-group-connectomes/>.

For verifying the robustness of the edge direction method, we first divided the brain graphs of the 423 subjects into four groups, the first contained 105, the others 106 graphs each. The graphs of each four groups were used—separately—to reproduce the CCD phenomenon, and based on the order of the appearance of the edges in the four different CCD probes, we assigned directions to some of the edges. Had the resulting directed graphs been radically different for the four groups, it would have indicated that our method is not a robust method of directing the edges of brain graphs.

As we detail below, it turned out that the four directed brain graphs were very similar to each other. After obtaining these four directed graphs, we used a majority-like approach to direct the edges of the consensus brain graph for the whole population, and, in a next step, the edges of the individual brain graphs.

Computing consensus brain graphs

For each group, for $i = 1, 2, 3, 4$, we defined the consensus brain graph G_i as the multi-union of the individual connectomes. That is, for each possible graph edge we counted the subjects whose connectomes contained the specific edge. This number ranges from 0 to N_i , where $N_i = 106$, is the number of subjects in the given group. We defined the consensus brain graph as a simple graph containing all edges that were present in at least one of the subjects, where the edges are labeled (weighted) with the number of individual connectomes containing them.

Directing the edges with BFS

We defined edge directions on this brain graph G_i as follows. For each k from N_i down to 1, we defined G_{ik} as the subgraph of G_i containing all edges with frequency at least k . This means all the edges which were present in at least k subjects within the i th group. Suppose that G_{ik} is already processed, and we want to process the graph $G_{i(k-1)}$, which is an augmentation of G_{ik} with precisely those edges which are present in exactly $k-1$ individual graphs. Since G_{ik} is already processed, our task is now to direct these newly added edges only. To achieve this, we launch a BFS (breadth-first search) in $G_{i(k-1)}$, with G_{ik} as the source. This means that, for each node in $G_{i(k-1)}$, we calculate the distance of this node from G_{ik} within the graph $G_{i(k-1)}$. This distance is at least 0, is precisely 0 for the nodes of G_{ik} , is finite for the nodes connected to G_{ik} with a path of edges, and is infinite for the nodes of $G_{i(k-1)}$ not connected to G_{ik} . Nodes with infinite distance do exist because sometimes isolated edges or new, small graph components appear in $G_{i(k-1)}$.

After calculating the node distances, each edge in $G_{i(k-1)}$ will connect either two nodes of the same distance or two nodes with a distance differing by exactly 1. If an edge connects u with v , and the distance of v is exactly 1 less than the distance of u , then we direct that edge from u to v . If an edge connects two equidistant nodes, then we leave this edge undirected, and it will not acquire a direction in this consensus brain graph, not even in the subsequent steps.

This way, when we reach frequency $k=1$ and have processed $G_{i1} = G_i$, we obtain a *partially directed* version of G_i . Some of its edges will become directed, and the remaining will be left undirected. As we do this for all four of the groups, we obtain four directed brain graphs on the same set of nodes.

Directed consensus connectome

We unify these directed connectomes into one big directed consensus connectome as follows. If an edge is directed in the same direction in at least 2 of the 4 consensus graphs, and is undirected or directed in the other direction in at most 1 of the graphs, then the direction of this edge is defined as the most common value. For example, if an edge is directed forward in 2 graphs, backward in 1 graph, and is absent from the remaining graph, then the edge will become forward-directed in the result graph. On the other hand, if that edge is directed forward in 2 graphs, backward in 1 graph, and is undirected in the remaining graph, then its direction is considered ambiguous, and this edge will remain undirected in the result graph.

By running this algorithm, we could direct 48324 of the 71783 edges of the consensus brain graph for the whole population. This means that we could assign a direction to 67% of all the edges which were present in at least one of the braingraphs. We think that 67% as a very significant portion of the edges, since the edges include even those sporadic connections which were present in only one brain graph and thus cannot be oriented reliably. If we count only those edges which were present in all 4 consensus connectomes (there were 31873 such edges), then we see that 26305 of them were directed the same way in all 4 groups. This means that 82% of these 31873 edges acquired the same orientation in all 4 groups.

This proves the robustness of our method. Additionally, these numbers also show that the CCD phenomenon is robust, too.

How can we direct the individual braingraphs?

In the previous subsection we have presented a CCD-based method to direct most of the edges of the consensus connectome in a robust way. The edges of the individual braingraphs can be directed by applying the directions of the edges of the (partially) directed consensus brain-graph as follows:

Let us consider an individual brain graph G and the directed consensus brain graph \bar{G} . If an edge e of G is directed in \bar{G} , then let us direct e in the same way in G , too. If edge e of G is undirected in \bar{G} , then e will remain to be undirected in G , too.

Supporting information

S1 Table. Table gives the source C# code of the program, which computes the directions of the connectome edges.

(PDF)

Acknowledgments

Data were provided in part by the Human Connectome Project, WU-Minn Consortium (Principal Investigators: David Van Essen and Kamil Ugurbil; 1U54MH091657) funded by the 16 NIH Institutes and Centers that support the NIH Blueprint for Neuroscience Research; and by the McDonnell Center for Systems Neuroscience at Washington University.

Author Contributions

Conceptualization: Csaba Kerepesi, Vince Grolmusz.

Data curation: Vince Grolmusz.

Formal analysis: Vince Grolmusz.

Funding acquisition: Vince Grolmusz.

Investigation: Vince Grolmusz.

Methodology: Balázs Szalkai, Bálint Varga, Vince Grolmusz.

Project administration: Vince Grolmusz.

Resources: Balázs Szalkai, Csaba Kerepesi, Bálint Varga, Vince Grolmusz.

Software: Balázs Szalkai, Bálint Varga.

Supervision: Vince Grolmusz.

Validation: Balázs Szalkai, Vince Grolmusz.

Writing – original draft: Balázs Szalkai, Vince Grolmusz.

Writing – review & editing: Vince Grolmusz.

References

1. Desikan RS, Ségonne F, Fischl B, Quinn BT, Dickerson BC, Blacker D, et al. An automated labeling system for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest. *Neuroimage*. 2006 Jul; 31(3):968–980. Available from: <http://dx.doi.org/10.1016/j.neuroimage.2006.01.021> PMID: 16530430
2. Fischl B. FreeSurfer. *Neuroimage*. 2012; 62(2):774–781. <https://doi.org/10.1016/j.neuroimage.2012.01.021> PMID: 22248573
3. Hagmann P, Cammoun L, Gigandet X, Meuli R, Honey CJ, Wedeen VJ, et al. Mapping the structural core of human cerebral cortex. *PLoS Biol*. 2008 Jul; 6(7):e159. Available from: <http://dx.doi.org/10.1371/journal.pbio.0060159> PMID: 18597554
4. Szalkai B, Varga B, Grolmusz V. Graph Theoretical Analysis Reveals: Women's Brains Are Better Connected than Men's. *PLoS One*. 2015; 10(7):e0130045. Available from: <http://dx.doi.org/10.1371/journal.pone.0130045> PMID: 26132764

5. McNab JA, Edlow BL, Witzel T, Huang SY, Bhat H, Heberlein K, et al. The Human Connectome Project and beyond: initial applications of 300 mT/m gradients. *Neuroimage*. 2013 Oct; 80:234–245. Available from: <http://dx.doi.org/10.1016/j.neuroimage.2013.05.074> PMID: 23711537
6. de la Iglesia-Vayá M, Molina-Mateo J, Escarti-Fabra MJ, Martí-Bonmatí L, Robles M, Meneu T, et al. [Magnetic resonance imaging postprocessing techniques in the study of brain connectivity]. *Radiologia*. 2011; 53(3):236–245. <https://doi.org/10.1016/j.rx.2010.11.007> PMID: 21477826
7. Szalkai B, Grolmusz V. Human Sexual Dimorphism of the Relative Cerebral Area Volumes in the Data of the Human Connectome Project. *European Journal of Anatomy*. 2018; 22(3):221–225.
8. Glasser MF, Sotiropoulos SN, Wilson JA, Coalson TS, Fischl B, Andersson JL, et al. The minimal pre-processing pipelines for the Human Connectome Project. *Neuroimage*. 2013 Oct; 80:105–124. <https://doi.org/10.1016/j.neuroimage.2013.04.127> PMID: 23668970
9. Szalkai B, Varga B, Grolmusz V. Mapping Correlations of Psychological and Connectomical Properties of the Dataset of the Human Connectome Project with the Maximum Spanning Tree Method. *Brain Imaging and Behavior*. 2018 feb.; <https://doi.org/10.1007/s11682-018-9937-6>
10. Herrick R, McKay M, Olsen T, Horton W, Florida M, Moore CJ, et al. Data dictionary services in XNAT and the Human Connectome Project. *Front Neuroinform*. 2014; 8:65. Available from: <http://dx.doi.org/10.3389/fninf.2014.00065> PMID: 25071542
11. Smith SM, Beckmann CF, Andersson J, Auerbach EJ, Bijsterbosch J, Douaud G, et al. Resting-state fMRI in the Human Connectome Project. *Neuroimage*. 2013 Oct; 80:144–168. <https://doi.org/10.1016/j.neuroimage.2013.05.039> PMID: 23702415
12. Szalkai B, Varga B, Grolmusz V. The Graph of Our Mind. arXiv preprint arXiv:160300904. 2016;.
13. Lawler EL. Combinatorial optimization: networks and matroids. Courier Dover Publications; 1976.
14. Lovász L. Combinatorial problems and exercises. 2nd ed. American Mathematical Society; 2007.
15. Karp R. Reducibility among combinatorial problems. In: Miller R, Thatcher J, editors. *Complexity of Computer Computations*. Plenum Press; 1972. p. 85–103.
16. Lovasz L. Random Walks on Graphs: A Survey. In: *Combinatorics, Paul Erdos is Eighty*. Bolyai Society Mathematical Studies. Janos Bolyai Mathematical Society; 1993.
17. Lovasz L. Eigenvalues of graphs. Pazmany Peter 1/C, H-1117 Budapest, Hungary: Department of Computer Science, Eotvos University; 2007. Available from: <http://www.cs.elte.hu/~lovasz/eigenvals-x.pdf>.
18. Grolmusz V. A note on the PageRank of undirected graphs. *Information Processing Letters*. 2015; 115(6):633–634. <https://doi.org/10.1016/j.ipl.2015.02.015>
19. Brin S, Page L. The Anatomy of a Large-Scale Hypertextual Web Search Engine. *Computer Networks and ISDN Systems*. 1998; 30:107–117. [https://doi.org/10.1016/S0169-7552\(98\)00110-X](https://doi.org/10.1016/S0169-7552(98)00110-X)
20. Roebroeck A, Formisano E, Goebel R. Mapping directed influence over the brain using Granger causality and fMRI. *Neuroimage*. 2005; 25(1):230–242. <https://doi.org/10.1016/j.neuroimage.2004.11.017> PMID: 15734358
21. Penny WD, Stephan K, Mechelli A, Friston K. Comparing dynamic causal models. *NeuroImage*. 2004; 22(3):1157–1172. <https://doi.org/10.1016/j.neuroimage.2004.03.026> PMID: 15219588
22. Kim S, Putrino D, Ghosh S, Brown EN. A Granger causality measure for point process models of ensemble neural spiking activity. *PLoS Comput Biol*. 2011 Mar; 7(3):e1001110. Available from: <http://dx.doi.org/10.1371/journal.pcbi.1001110> PMID: 21455283
23. Ching ES, Lai PY, Leung C. Extracting connectivity from dynamics of networks with uniform bidirectional coupling. *Physical Review E*. 2013; 88(4):042817. <https://doi.org/10.1103/PhysRevE.88.042817>
24. Timme M, Casadiego J. Revealing networks from dynamics: an introduction. *Journal of Physics A: Mathematical and Theoretical*. 2014; 47(34):343001. <https://doi.org/10.1088/1751-8113/47/34/343001>
25. Schelter B, Winterhalder M, Dahlhaus R, Kurths J, Timmer J. Partial phase synchronization for multivariate synchronizing systems. *Phys Rev Lett*. 2006 May; 96(20):208103. Available from: <http://dx.doi.org/10.1103/PhysRevLett.96.208103> PMID: 16803212
26. Ren J, Wang WX, Li B, Lai YC. Noise bridges dynamical correlation and topology in coupled oscillator networks. *Phys Rev Lett*. 2010 Feb; 104(5):058701. Available from: <http://dx.doi.org/10.1103/PhysRevLett.104.058701>.
27. Stetter O, Battaglia D, Soriano J, Geisel T. Model-free reconstruction of excitatory neuronal connectivity from calcium imaging signals. *PLoS Comput Biol*. 2012; 8(8):e1002653. Available from: <http://dx.doi.org/10.1371/journal.pcbi.1002653> PMID: 22927808
28. Gerhard F, Kispersky T, Gutierrez GJ, Marder E, Kramer M, Eden U. Successful reconstruction of a physiological circuit with known connectivity from spiking activity alone. *PLoS Comput Biol*. 2013; 9(7):e1003138. Available from: <http://dx.doi.org/10.1371/journal.pcbi.1003138> PMID: 23874181

29. Zaytsev YV, Morrison A, Deger M. Reconstruction of recurrent synaptic connectivity of thousands of neurons from simulated spiking activity. *J Comput Neurosci*. 2015 Aug; 39(1):77–103. Available from: <http://dx.doi.org/10.1007/s10827-015-0565-5> PMID: 26041729
30. Smith SM, Miller KL, Salimi-Khorshidi G, Webster M, Beckmann CF, Nichols TE, et al. Network modeling methods for fMRI. *Neuroimage*. 2011 Jan; 54(2):875–891. Available from: <http://dx.doi.org/10.1016/j.neuroimage.2010.08.063> PMID: 20817103
31. Pillow JW, Ahmadian Y, Paninski L. Model-based decoding, information estimation, and change-point detection techniques for multineuron spike trains. *Neural Comput*. 2011 Jan; 23(1):1–45. Available from: http://dx.doi.org/10.1162/NECO_a_00058 PMID: 20964538
32. David O, Guillemain I, Sallet S, Rey S, Deransart C, Segebarth C, et al. Identifying neural drivers with functional MRI: an electrophysiological validation. *PLoS biology*. 2008 Dec; 6:2683–2697. <https://doi.org/10.1371/journal.pbio.0060315> PMID: 19108604
33. Valverde de Amusco J. Anatomia del corpo humano. Per Ant. Salamanca, et Antonio Lafreri; 1560. NLM Unique ID: 2294026R. Available from: https://www.nlm.nih.gov/exhibition/historicalanatomies/valverde_bio.html.
34. Laskowski S, Balicki S. Anatomie normale du corps humain: atlas iconographique de XVI planches / par le docteur S. Laskowski; dessinee's d'apres les preeparations de l'auteur par S. Balicki. Geneve: Braun; 1894. Available from: https://www.nlm.nih.gov/exhibition/historicalanatomies/laskowski_home.html.
35. Kiss F, Szentagothai J. Atlas of Human Anatomy. Springer; 1987.
36. Szalkai B, Kerepesi C, Varga B, Grolmusz V. The Budapest Reference Connectome Server v2.0. *Neuroscience Letters*. 2015; 595:60–62. <https://doi.org/10.1016/j.neulet.2015.03.071> PMID: 25862487
37. Szalkai B, Kerepesi C, Varga B, Grolmusz V. Parameterizable Consensus Connectomes from the Human Connectome Project: The Budapest Reference Connectome Server v3.0. *Cognitive Neurodynamics*. 2017 feb; 11(1):113–116. <https://doi.org/10.1007/s11571-016-9407-z> PMID: 28174617
38. Kerepesi C, Szalkai B, Varga B, Grolmusz V. How to Direct the Edges of the Connectomes: Dynamics of the Consensus Connectomes and the Development of the Connections in the Human Brain. *PLOS One*. 2016 June; 11(6):e0158680. Available from: <http://dx.doi.org/10.1371/journal.pone.0158680> PMID: 27362431
39. Kerepesi C, Varga B, Szalkai B, Grolmusz V. The Dorsal Striatum and the Dynamics of the Consensus Connectomes in the Frontal Lobe of the Human Brain. *Neuroscience Letters*. 2018; 673:51–55. <https://doi.org/10.1016/j.neulet.2018.02.052> PMID: 29496609
40. Roberts JA, Perry A, Roberts G, Mitchell PB, Breakspear M. Consistency-based thresholding of the human connectome. *Neuroimage*. 2017; 145:118–129. <https://doi.org/10.1016/j.neuroimage.2016.09.053> PMID: 27666386
41. Szalkai B, Varga B, Grolmusz V. The Robustness and the Doubly-Preferential Attachment Simulation of the Consensus Connectome Dynamics of the Human Brain. *Scientific Reports*. 2017; 7(16118). <https://doi.org/10.1038/s41598-017-16326-0> PMID: 29170405
42. De Carlos JA, O'Leary DD. Growth and targeting of subplate axons and establishment of major cortical pathways. *J Neurosci*. 1992 Apr; 12(4):1194–1211. <https://doi.org/10.1523/JNEUROSCI.12-04-01194.1992> PMID: 1556593
43. Lewis TL Jr, Courchet J, Polleux F. Cell biology in neuroscience: Cellular and molecular mechanisms underlying axon formation, growth, and branching. *J Cell Biol*. 2013 Sep; 202(6):837–848. Available from: <http://dx.doi.org/10.1083/jcb.201305098> PMID: 24043699
44. Hu B, Nikolakopoulou AM, Cohen-Cory S. BDNF stabilizes synapses and maintains the structural complexity of optic axons in vivo. *Development*. 2005 Oct; 132(19):4285–4298. Available from: <http://dx.doi.org/10.1242/dev.02017> PMID: 16141221
45. Cline HT, Constantine-Paton M. NMDA receptor antagonists disrupt the retinotectal topographic map. *Neuron*. 1989 Oct; 3(4):413–426. [https://doi.org/10.1016/0896-6273\(89\)90201-8](https://doi.org/10.1016/0896-6273(89)90201-8) PMID: 2577128
46. Rajan I, Witte S, Cline HT. NMDA receptor activity stabilizes presynaptic retinotectal axons and post-synaptic optic tectal cell dendrites in vivo. *J Neurobiol*. 1999 Feb; 38(3):357–368. [https://doi.org/10.1002/\(SICI\)1097-4695\(19990215\)38:3%3C357::AID-NEU5%3E3.0.CO;2-%23](https://doi.org/10.1002/(SICI)1097-4695(19990215)38:3%3C357::AID-NEU5%3E3.0.CO;2-%23) PMID: 10022578
47. Schmidt JT, Buzzard M, Borress R, Dhillon S. MK801 increases retinotectal arbor size in developing zebrafish without affecting kinetics of branch elimination and addition. *J Neurobiol*. 2000 Feb; 42(3):303–314. [https://doi.org/10.1002/\(SICI\)1097-4695\(20000215\)42:3%3C303::AID-NEU2%3E3.0.CO;2-A](https://doi.org/10.1002/(SICI)1097-4695(20000215)42:3%3C303::AID-NEU2%3E3.0.CO;2-A) PMID: 10645970
48. Ruthazer ES, Cline HT. Insights into activity-dependent map formation from the retinotectal system: a middle-of-the-brain perspective. *J Neurobiol*. 2004 Apr; 59(1):134–146. Available from: <http://dx.doi.org/10.1002/neu.10344> PMID: 15007832

49. Zou DJ, Cline HT. Control of retinotectal axon arbor growth by postsynaptic CaMKII. *Prog Brain Res.* 1996; 108:303–312. [https://doi.org/10.1016/S0079-6123\(08\)62548-0](https://doi.org/10.1016/S0079-6123(08)62548-0) PMID: 8979810
50. Schmidt JT. Activity-driven sharpening of the retinotectal projection: the search for retrograde synaptic signaling pathways. *J Neurobiol.* 2004 Apr; 59(1):114–133. Available from: <http://dx.doi.org/10.1002/neu.10343> PMID: 15007831