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Postural muscle activity patterns during standing at rest and on an oscillating floor

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Abstract

Postural muscle activity pattern was examined in the eyes-closed state after adequate adaptation to floor anteroposterior oscillation. Twenty-three subjects were

5 grouped almost evenly according to dominance of anterior or posterior postural muscles in the trunk and thigh during quiet stance. In the posterior-dominant group, this dominance was maintained at every frequency in most subjects. In the anterior-dominant group, this dominance was maintained in most subjects at 0.1 and 0.5 Hz but changed to posterior dominance at 1.0 and 1.5 Hz in about half the subjects.

10 Periodicity of muscle activity was evaluated by EMG amplitude spectrum at the floor oscillation frequency. Periodicity of posterior-dominant muscles in the trunk and thigh increased with increasing oscillatory frequency. In the trunk, the periodicity did not differ significantly between posterior-dominant and anterior-dominant groups. However, in the thigh, periodicity was significantly lower in the anterior-dominant muscles. This

15 was considered to be caused by nonperiodic alternating action of the anterior and posterior muscles. In the lower leg, posterior dominance was observed in quiet stance and at all oscillation frequencies. Periodicity of soleus and gastrocnemius increased at higher frequencies and was higher in gastrocnemius than in soleus. The periodicity

difference between both muscles decreased with increasing oscillation frequency.

1. Introduction

In quiet stance, the body generally inclines forward with the ankles acting as a pivotal axis, and the posterior muscles of the body are continuously activated. The standing posture is maintained predominantly by posterior muscles, the so-called Guy-and-Derrick principle [2]. Invariably, only the posterior muscles in the lower legs are activated to maintain quiet stance [1,18,19]. The relative positional relationship of body segments during this quiet stance is similar under conditions of weightlessness [7], suggesting that relatively stable mechanisms for posture maintenance exist. However, many previous studies have shown that remarkable individual variation exists regarding patterns of postural muscle activity in the trunk and thigh during quiet stance. Continuous activity in the anterior muscles of the trunk has been reported in around 25% of subjects [2,3]. Continuous activity of the anterior muscles of the thigh is also observed in a few subjects [1,4,19,20,27,29,32]. However, it has not been elucidated whether the anterior or posterior postural muscle dominance is a general principle for all postural muscles throughout the body under both static and dynamic conditions.

Postural control is a basic element of voluntary movement and the two processes of upper- and lower-limb movement and postural control are inextricably linked

[6,14,21,31]. When an individual moves the arm while standing at rest, postural muscle activity precedes activity of the arm target muscles [5,28]. We reported that onset timing of postural muscle activation was adjusted depending on quiet standing position [12,13].

We therefore presumed that subjective posterior or anterior dominance of postural muscle activity during quiet stance would largely be maintained in dynamic movement.

The present study focused on dominance of postural muscle activity in dynamic postural control during various frequencies of floor oscillation in the anteroposterior direction. We previously reported that the improvement in steadiness of standing posture reached a plateau for a total of 5 minutes during floor oscillation [11]. Moreover, the anteroposterior position of the center of foot pressure (CFP) in the standing posture during floor oscillation shifts forward as oscillation frequency rises [8,22] and the momentum of the anteroposterior direction around the ankle joint changes according to the distance of CFP position from the heel [24]. As CFP position shifts forward, the activity of triceps surae increases while that of tibialis anterior changes very little [10]. Therefore, dominance of posterior muscle activity is likely to be more noticeable in the lower leg during floor oscillation. However, this postulated change in trunk and thigh muscle activity has not been discussed in relation to dominance of anterior or posterior muscle activity.

It has been reported that in the lower leg, periodic muscle activity corresponding to floor oscillation curve increases at relatively higher frequencies of oscillation, with continuous muscle activity not related to the oscillation decreasing in the way between directional changing points of oscillation and periodic ballistic activity increasing where oscillation direction changes [8]. However, the periodicity of the trunk and thigh muscles has not been sufficiently investigated. The trunk muscles may play a functional role in keeping the trunk vertical and maintaining a perceptual axis of the direction of gravity. The thigh muscles, in addition to assisting in this trunk function, adjust the positional relationship between the trunk and leg to maintain the equilibrium of the entire body [12,17,23]. Therefore, it is highly possible that the trunk and thigh muscles show different characteristics of activation.

Muscles of the lower leg vary in terms of contraction properties. Soleus (Sol) exhibits continuous activity in quiet stance while gastrocnemius medialis (GcM) demonstrates burst activity, indicating that the former is predominantly supportive and that the latter has a stabilizing element [16,25]. Moreover, inhibition of Sol and facilitation of GcM follows rapid dorsiflexion of the ankle joint in the preparation phase before a phasic arm movement [33], while GcM is activated selectively in running [9]. It has not been elucidated whether the activity and periodicity of these lower leg

muscles change with gradual increase of the dynamic element of postural control, such as that caused by changing the frequency of floor oscillation.

In this study, we investigated postural muscle activity after adaptation of postural control to floor oscillation, in subjects who exhibited dominant activation of either the anterior (anterior-dominant group) or posterior postural muscles (posterior-dominant group) of the trunk and thigh during quiet stance. Working hypotheses were as follows.

(1) Intergroup differences would be observed in the proportion of subjects exhibiting change in dominance as frequency of floor oscillation was altered.

(2) Regarding dynamic postural control, during floor oscillation at higher frequencies, higher periodicity would occur on the dominant side.

(3) Differences in the muscle activity and periodicity of Sol and GcM would decrease as floor oscillation frequency increased.

2. Methods

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2.1. Subjects

In a preliminary experiment, electromyograms (EMG) of the anterior and posterior

muscles of the trunk, thigh, and lower leg were recorded during quiet stance for 61 adults aged 18–25 years. Twenty-three subjects (10 men and 13 women) were selected based on EMG of the postural muscles of the trunk and thigh and grouped according to whether activity of the anterior or posterior muscles was dominant (anterior-dominant group, n=12; posterior-dominant group, n=11). For the lower leg, all subjects demonstrated posterior dominance. All subjects were free of any neurologic or orthopedic impairment. Mean values for age, height, weight, and foot length were 20.1 years (SD = 1.9), 163.0 cm (SD = 8.7), 55.0 kg (SD = 7.4), and 23.9 cm (SD = 1.4), respectively. Informed consent was obtained from all subjects following explanation of the experimental protocol.

2.2. Apparatus

All measurements were taken with subjects standing on a force platform (WAMI, WA1001) mounted on an oscillation table (60 cm long, 60 cm wide, and 27 cm high, Electric Control Group, PW0198). The platform contained three load cells which recorded CFP position in the anteroposterior direction. The table was sinusoidally oscillated in the anteroposterior direction with 2.5 cm amplitude and 0.1, 0.5, 1.0, and

1.5 Hz frequencies. An electrical signal from a potentiometer attached to the table was used to detect table position and to measure oscillation frequency using a frequency counter (Advantest Co. Ltd., TR-5822).

Surface electrodes (Medicotest, M-00-S) were arranged in a bipolar configuration to
5 record surface EMG activity of following muscles: rectus abdominis (RA) at the level
of the navel, lumbar paraspinal (LP) at the level of the iliac crest, rectus femoris (RF),
the long head of biceps femoris (BF), tibialis anterior (TA), GcM, and Sol, all on the
right side. After shaving and cleaning the skin with alcohol, electrodes were aligned
along the major axis of the muscle with an inter-electrode distance of about 3 cm. Input
10 impedance was reduced to below 5 k Ω . Signals from the electrodes were amplified
($\times 1000$ – $\times 4000$) and band-pass filtered (1.6 Hz to 1.5 kHz) with an EMG amplifier
(NEC-Sanei, BIOTOP-6R12).

For subsequent analysis, the signals from the potentiometer, force platform, and
electrodes were sent to an on-line computer (Iiyama, M533MS) via an A/D converter
15 (Canopus, ADJ-98) at 1000 Hz with 12-bit resolution. The signal from the force
platform was also sent to another on-line computer (NEC, PC9801CV21) via an A/D
converter (I/O data, PIO9045) at 20 Hz with 12-bit resolution, and mean CFP position
in the anteroposterior direction was computed.

2. 3. Procedure

Subjects performed the following tasks while standing barefoot on the force
5 platform with eyes closed and with the feet 10 cm apart and parallel. They were
instructed to keep their arms hanging freely by their sides and to maintain a relaxed
standing posture without intentional flexion of knee and hip joints.

First, this quiet stance was maintained for 10 sec, after which the table was
oscillated for 60 sec, constituting one trial. A set of 5 oscillation trials was performed at
10 each oscillation frequency, which was increased sequentially as described above.
Subjects had seated rest periods of one minute between trials and of 3 minutes between
sets.

In order to normalize the EMG between each oscillation trial, the following
procedure was followed: pivoting at the ankles with the rest of the body kept aligned,
15 subjects gradually leaned forward from the quiet stance over around 5 sec, maintained
this extreme forward-leaning posture for 3 sec, and gradually leaned then backward
over around 10 sec, before maintaining this extreme backward-leaning posture for a
further 3 sec.

2. 4. Data analysis

Data from the last 5 sec of maintaining quiet stance and the last 50 sec of table
5 oscillation were analyzed.

The mean position of CFP in the anteroposterior direction was calculated as relative
distance (%) from the heel to the total foot length. The mean speed of CFP fluctuation in
the anteroposterior direction during floor oscillation was calculated using the weighted
5-point moving average method.

10 EMGs were band-pass filtered at 20–100 Hz using the Butterworth method and
were then full-wave rectified. Relative muscle activity (RMA) was calculated using the
following formula to determine anterior or posterior dominance of muscle activity in the
trunk, thigh, and lower leg.

$$\text{RMA (\%)} = (\text{EMG}_x - \text{EMG}_{\min}) / (\text{EMG}_{\max} - \text{EMG}_{\min}) \times 100$$

15 In this formula, EMG_x represents the mean EMG amplitude in each trial; EMG_{\min} , the
minimum mean EMG amplitude over a 100-ms period, obtained during quiet stance or
forward or backward leaning; and EMG_{\max} , the maximum mean EMG amplitude,
obtained over a 1-sec period while maintaining extreme forward- or backward-leaning

posture. Muscle activity dominance was determined by comparing relative muscle activities between the anterior and posterior sides in each body segment, and was defined as the side on which relative muscle activity exceeded 110% of that in the opposite side.

5 Muscle activity exhibited periodicity during maintenance of stance on the oscillation table. In order to compare this periodicity between muscles, each 20 ms epoch of the rectified EMG trace was averaged and this averaged value was normalized by the EMG mean amplitude across 50 sec. Using this normalized data, FFT analysis with frequency resolution at 0.024 Hz and Hanning windows was performed, and amplitude spectrum
10 at the frequency corresponding to the floor oscillation was calculated (Fig. 1).

For each oscillation cycle, EMG activity pattern in the anterior and posterior muscles was determined for each body segment. Muscle activity lasting at least 67 ms (10% of one cycle time at the highest oscillation frequency (1.5 Hz)) was identified as an increase in muscle activity.

15 Analyses were performed using BIMUTAS-II software (Kissei Comtec Co. Ltd.).

2. 5. Statistical analysis

The effects of trial number on mean speed of CFP fluctuation and oscillation frequency in each parameter of EMG activity were assessed by ANOVA or Friedman test depending on whether the significant difference in variance was observed. Post-hoc multiple-comparison analysis was performed using the Newman-Keuls procedures and
5 Tukey test to further examine differences suggested by ANOVA and Friedman test, respectively. The Chi-squared test was used to assess difference in number of subjects whose dominant side changed. Alpha level was set at $p < 0.05$. All statistical analyses performed using Excel 2000 (Microsoft Corp.) with Stat Mate III (ATMS Co. Ltd.).

10 **3. Results**

Representative data for two subjects during the 5th trial at 0.5 and 1.5 Hz are shown in Fig. 2. The top panel shows an example of posterior dominance of trunk and thigh muscle activity during quiet stance and the bottom panel shows an example of anterior
15 dominance. In both subjects, posterior dominance was observed for the lower leg, and the mean position of CFP during floor oscillation tended to shift forward compared with that during quiet stance. However, individual differences were observed in the muscle activities of the trunk and thigh during floor oscillation.

In the posterior-dominant subject, this dominance was maintained in the trunk and thigh during floor oscillation, and activity of these muscles tended to increase at higher oscillation frequencies. At both oscillation frequencies, alternating action of anterior and posterior muscles was rarely observed, and periodicity of activity corresponding to
5 oscillation frequency was observed in the posterior muscles.

In the anterior-dominant subject, dominance of anterior muscle activity was observed in the trunk and thigh at 0.5 Hz. At 1.5 Hz, however, dominance in the thigh changed from anterior to posterior, and alternating action in the thigh muscles was clearly observed.

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3.1. Mean speed and position of CFP fluctuation

During floor oscillation, mean speed of CFP fluctuation in the anteroposterior direction decreased rapidly until the 3rd trial for each frequency ($F_{4,88} > 5.54, p < 0.001$),
15 exhibiting no significant change thereafter (Fig. 3). The following descriptions therefore all refer to data collected during the 5th trial.

Fig. 4 shows the mean position and fluctuation range (\pm SD) of CFP in the anteroposterior direction during quiet stance and floor oscillation in the

posterior-dominant and anterior-dominant groups. No significant intergroup difference in mean position was found for either the trunk or thigh. At 0.5 Hz and above, mean position of CFP shifted anteriorly compared with that when standing at rest (posterior-dominant group: $F_{4,40} = 3.89$, $p < 0.01$; anterior-dominant group: $F_{4,44} = 20.60$,
5 $p < 0.001$). Moreover, range of fluctuation increased only in the forward direction.

3. 2. Anterior/posterior dominance of muscle activity during floor oscillation

Table 1 shows the number of subjects for whom dominant side was maintained
10 during floor oscillation. Dominant side remained unchanged in all of the trunk posterior-dominant group. In the trunk anterior-dominant group, dominant side was maintained in 10 subjects at 0.5 Hz and in 8 subjects at 1.0 and 1.5 Hz. In the thigh posterior-dominant group, dominant side was maintained in 9 subjects at 0.5 Hz and in
10 subjects at 1.0 and 1.5 Hz. Significantly fewer subjects in the thigh anterior-
15 dominant group maintained this dominance at 1.0 Hz when compared to the thigh posterior-dominant group (6 vs. 10, $\chi_1^2=4.54$, $p<0.05$). In the lower leg, posterior dominance was maintained by all subjects throughout oscillation.

Each above-mentioned group was further analyzed according to whether or not

dominance was maintained through all oscillation frequencies. Fig. 5 shows relative muscle activity among subjects who maintained posterior dominance. All subjects in the trunk posterior-dominant group maintained this pattern, and posterior (LP) activity was significantly greater at 0.5 Hz and above than during standing at rest ($F_{4,40} = 20.93$, $p < 0.001$). Posterior dominance of the thigh muscles was maintained in 9 of 11 subjects. In these 9 subjects, activities of posterior and anterior muscles (BF and RF) were significantly greater at 1.0 and 1.5 Hz than during standing at rest ($F_{4,32} > 4.35$, $p < 0.01$). In the lower leg, the activities of GcM and Sol were significantly greater at 0.5 Hz and above than during standing at rest ($F_{4,88} > 13.28$, $p < 0.001$). Activity of GcM was significantly greater than that of Sol only at 0.5 Hz ($p < 0.05$). Dominance changed in only 2 subjects with posterior dominance of the thigh, and these subjects demonstrated slightly higher activities of the anterior muscles than of the posterior muscles at higher oscillation frequencies.

Fig. 6 shows relative muscle activity in subjects who maintained anterior dominance (left panel) and in those in whom anterior dominance changed to posterior dominance (right panel). In the trunk and thigh anterior-dominant group, dominant side was maintained in 7 and 5 subjects, respectively, and no significant change in activities of anterior and posterior muscles was seen across all oscillation frequencies.

In subjects in whom anterior dominance of the trunk and thigh changed to posterior dominance (n=5 and 7, respectively), activity of the posterior muscles significantly increased in the higher oscillation frequencies (trunk anterior-dominant group: $F_{4,16} = 16.21, p < 0.001$; thigh anterior-dominant group: $F_{4,4} = 7.13, p < 0.05$), while activity of the anterior muscles showed no significant change. In the trunk anterior-dominant group, activity of the posterior muscles was significantly greater than that of anterior muscles at 1.5 Hz ($p < 0.05$).

3. 3. Periodicity of muscle activity

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Fig. 7 shows the amplitude spectrum of dominant muscle activation during floor oscillation. In the trunk and thigh, the periodicity of posterior muscle activity increased significantly with increasing oscillation frequency (trunk: $F_{3,50} = 8.22, p < 0.001$, thigh: $F_{3,50} = 3.80, p < 0.05$), while that of anterior muscles, particularly in the thigh, was higher at 0.5 Hz and above than at 0.1 Hz (thigh: $F_{3,34} = 5.00, p < 0.01$), and showed no significant difference when frequency exceeded 0.5 Hz. The periodicity of posterior muscles at 1.0 and 1.5 Hz was significantly higher than that of anterior muscles ($p < 0.01$) in the thigh. The periodicity of posterior dominant muscles in the trunk was lower

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than that of thigh ($F_{1,100} = 11.43, p < 0.001$); this difference was significant at 1.5 Hz.

In the lower leg, the periodicity of GcM and Sol was significantly higher at 0.5 Hz and above than at 0.1 Hz ($F_{3,66} > 9.32, p < 0.001$). The periodicity of GcM was significantly higher than that of Sol at all frequencies ($p < 0.01$) and that of GcM was maximal at 0.5 Hz. The periodicity of Sol was significantly higher at 1.5 Hz than at 0.5 Hz ($p < 0.05$). The difference in periodicity between both muscles was greatest at 0.5 Hz and decreased significantly at 1.5 Hz ($F_{3,66} > 7.75, p < 0.001$).

The pattern of muscle activity in each oscillation cycle was categorized into anterior or posterior dominant, alternating, and simultaneous. The number of cycles analyzed for each subject was 5, 25, 50, and 75 cycles at 0.1, 0.5, 1.0, and 1.5 Hz, respectively. Table 2 shows the relative number (%) of cycles in which alternating activity was observed. In the trunk and thigh posterior-dominant group, only posterior activity was observed in the great majority of cycles (particularly in the trunk), alternating activity was observed in few cycles, and simultaneous activity was observed very infrequently (0–2% of cycles). In the trunk and thigh anterior-dominant group, alternating activity was observed in comparatively more oscillation cycles (29–43%) at 0.5 Hz and above. In the lower leg, for which all subjects demonstrated posterior dominance, alternating activity was observed at similar levels to the trunk and thigh anterior-dominant group, however,

most of the anterior muscle (TA) activity was in the form of bursts (Fig. 2).

4. Discussion

5 Steadiness of standing posture during floor oscillation improved rapidly until the 3rd
trial and reached a plateau thereafter, in accordance with a previous study [11]. We
therefore considered that this stage reflected adequate postural adaptation and was
suitable for determination of postural muscle activity.

10 *4.1. Dominant side of muscle activity*

In the lower leg, dominance of the posterior muscles was maintained at every
oscillation frequency in all subjects and this dominance became more prominent as
frequency of floor oscillation was increased. During floor oscillation, forward shift of
15 CFP was observed; thought to be related to altered activity of the posterior muscles in
the lower leg. An increase of acceleration in the anteroposterior direction corresponding
to the oscillation frequency causes an increase in the movement amplitude of CFP. If the
mean position of CFP does not shift forward, this increase should lead to the activation

of the anterior leg muscles. The forward shift of the center of mass should inhibit the activity of these anterior muscles. This phenomenon may have a role in preventing falls because the backward base area to maintain backward leaning posture is small due to the location of the ankle joint in the foot.

5 In the trunk and thigh, dominance of either anterior or posterior muscles was maintained at 0.1 Hz. Therefore it is probable that dominance of muscle activity in the trunk and thigh is maintained in relatively static conditions. At frequencies of 0.5 Hz and above, dominance was maintained in most subjects in the posterior-dominant group. In addition, dominance of the posterior muscles became more prominent in these
10 subjects as floor oscillation frequency was increased. This probably indicates increased forward leaning of the trunk and thigh caused by forward shift of CFP during floor oscillation. These phenomena suggest that postural control based on dominance of the posterior postural muscles does not preclude the necessity for forward shift of CFP.

In the trunk and thigh anterior-dominant group, anterior muscle dominance was
15 maintained in more than 80% of subjects at 0.5 Hz, and in over half the subjects at 1.0 and 1.5 Hz. This suggests that maintenance of standing posture using dominance of either posterior or anterior postural muscles is a comparatively basic requirement of postural control, even at relatively high oscillation frequencies.

However, change in dominance was also observed, albeit in less than half the subjects. This individual difference in dominance would suggest complicated factors related to selection of active muscles during floor oscillation at high frequency. These factors are postulated to include 1) the requirement for forward shift of CFP, 2) maintenance of a perceptual axis of the direction of gravity by keeping the trunk vertical, and 3) adjustment of positional relationship between the trunk and leg to maintain the body equilibrium [12,17,23].

4.2. Periodicity of activity in the dominant muscles

Low periodicity of muscle activity in the dominant side was observed in every measured region at 0.1 Hz. This muscle activity is likely to be strongly related to the antigravitational supportive functions involved in maintaining the standing posture, which do not necessarily correspond to the lower oscillation frequencies.

Greater periodicity of posterior muscle activity was observed with increasing oscillation frequency. In addition, the main pattern of muscle activity during one oscillation period in the posterior-dominant group was posterior dominance only, with alternating activity occurring very rarely. Hence, in the posterior-dominant group,

postural muscle activity intensified at higher frequencies in a contraction-relaxation manner according to the Guy-and-Derrick principle.

Periodicity of posterior-dominant muscles in the trunk, particularly at 1.5 Hz, was lower than that in the thigh. The incidence of alternating activity of the posterior trunk muscles was extremely low at every frequency. This suggests that the postural supportive element of posterior-dominant muscle activity is stronger in the trunk than in the thigh, particularly at 1.5 Hz. In the trunk, periodicity of the anterior muscles was similar to that of the posterior muscles at every frequency. In the thigh, periodicity of the anterior muscles was lower than that of the posterior muscles at 1.0 and 1.5 Hz. In both anterior- and posterior-dominant groups of the thigh, alternating activity was observed relatively more often at 1.0 and 1.5 Hz. This suggests that when anterior muscle activation is dominant, particularly in the thigh, the periodicity of the anterior muscles at 1.0 and 1.5 Hz falls with increasing nonperiodic alternate action of anterior and posterior muscles.

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4.3. Activation of GcM and Sol

Relative muscle activity of GcM and Sol increased at oscillation frequencies of 0.5

Hz and above, with GcM tending to show higher activation. However, difference in relative muscle activity between these muscles decreased with increasing oscillation frequency. A similar pattern was observed for the periodicity of GcM and Sol activity. These results suggest that, at 0.5 Hz, GcM plays a relatively important role in the control of torque around the foot joint, and that Sol contributes strongly to the maintenance of the joint stiffness by generating relatively constant tension [15]. This is related to the fact that the periodic change in the floor oscillation was predictable, and that activation of GcM is selectively controlled by the supraspinal nervous system [9,33]. It is conceivable that the dynamic element of postural control increases in place of the supportive element according to the increase in floor oscillation frequency. The increase in the periodicity and activity of Sol at high frequencies in the present study indicates that, in contrast to GcM, dynamic activity of Sol is relatively enhanced. In the seated position, GcM is reported to have a close relationship with high-speed eccentric contraction, in marked contrast to Sol [26,30]. It can be inferred from these findings that the difference in Sol activity depends on whether maintenance of posture is the main task.

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Figure legends

Fig. 1. FFT analysis of the periodicity of muscle activity. (A) Normalized EMG of Sol from 27 to 35 sec in the 5th trial at 0.5 Hz is presented. (B) The maximum amplitude spectrum is observed at the frequency corresponding to the floor oscillation.

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Fig. 2. Typical examples of CFP position and muscle activity in 2 subjects. Data from 20 to 30 sec during the 5th trial at 0.5 and 1.5 Hz are presented.

Fig. 3. Mean speed of CFP fluctuation in the anteroposterior direction during floor oscillation. Plotted values are means and standard deviations across all subjects.

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Fig. 4. Mean position and fluctuation range of CFP in the anteroposterior direction. Plotted values are means and standard deviations for trunk posterior- and anterior-dominant groups.

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Fig. 5. Relative activities of posterior and anterior muscles among subjects that maintained posterior dominance. Plotted values are means and standard deviations for posterior and anterior muscles for each body segment. Asterisks indicate significant

differences ($p < 0.05$).

Fig. 6. Relative muscle activities of posterior and anterior muscles in the anterior-dominant group. Data from those that maintained this dominance and for those in whom dominance changed are presented in the left panel and right panel, respectively. Plotted values are means and standard deviations for posterior and anterior muscles in each body segment. Asterisks indicate significant differences ($p < 0.05$).

Fig. 7. Amplitude spectrum of the dominant muscle groups during floor oscillation. Plotted values are means and standard deviations for posterior and anterior muscles in each body segment. Asterisks indicate significant differences ($p < 0.05$).

Table 1

Subjects in whom anterior/posterior dominance of muscle activity was maintained during floor oscillation

Body segment	Muscle dominance in QSP	Total number of subjects	Frequency of floor oscillation			
			0.1 Hz	0.5 Hz	1.0 Hz	1.5 Hz
Trunk	posterior	11	11	11	11	11
	anterior	12	12	10	8	8
Thigh	posterior	11	11	9	10	10
	anterior	12	11	10	6	7
Lower leg	posterior	23	23	23	23	23

QSP: quiet standing posture, *: $p < 0.05$

Table 2

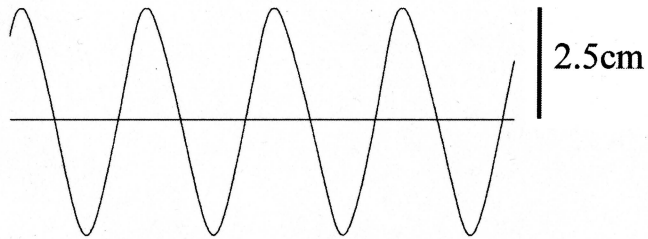
Relative number (%) of cycles in which alternating activity was observed

Body segment	Muscle dominance in QSP	Total cycle	Frequency of floor oscillation			
			0.1 Hz	0.5 Hz	1.0 Hz	1.5 Hz
			5	25	50	75
Trunk	posterior		0	1	2	3
	anterior		12	40*	40*	29
Thigh	posterior		4	18	23	29*
	anterior		10	43*	32	38*
Lower leg	posterior		5	36*	40*	29*

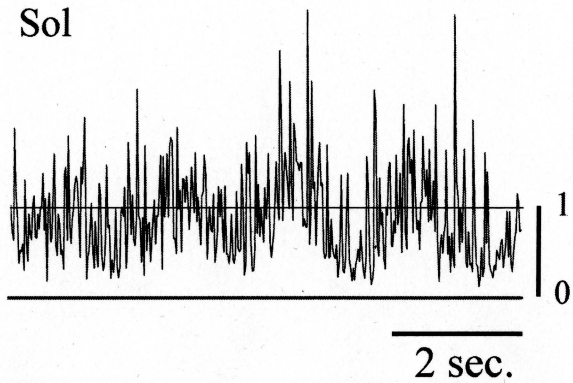
QSP: quiet standing posture, *: $p < 0.05$ vs. 0.1 Hz

A

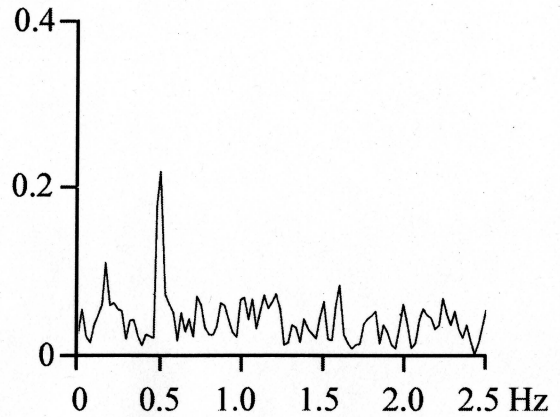
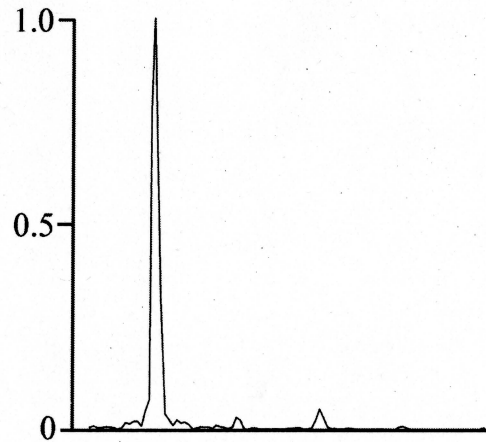
Table



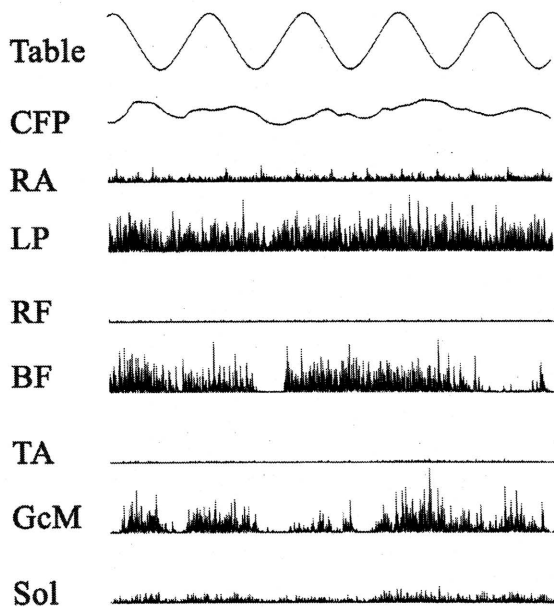
Sol



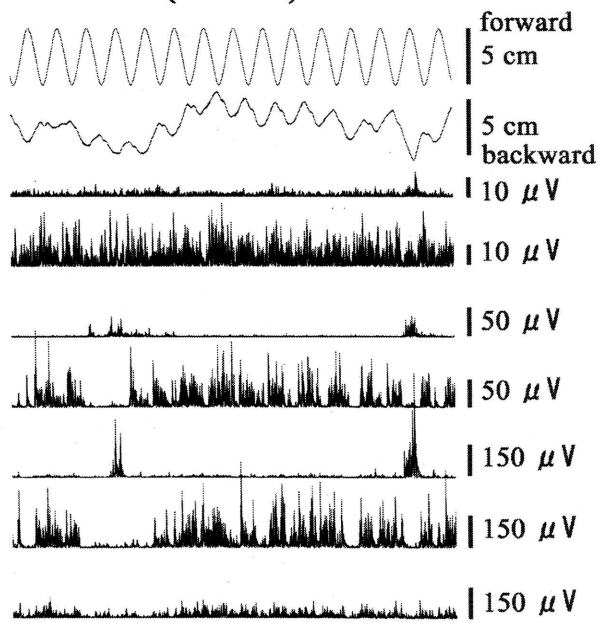
B



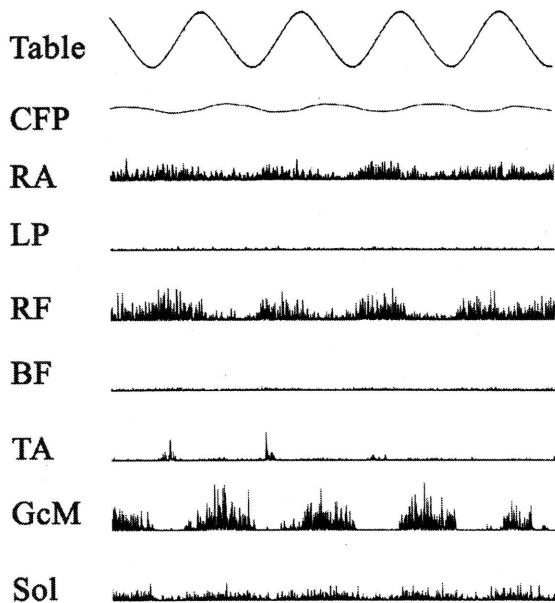
Subj. TK (0.5 Hz)



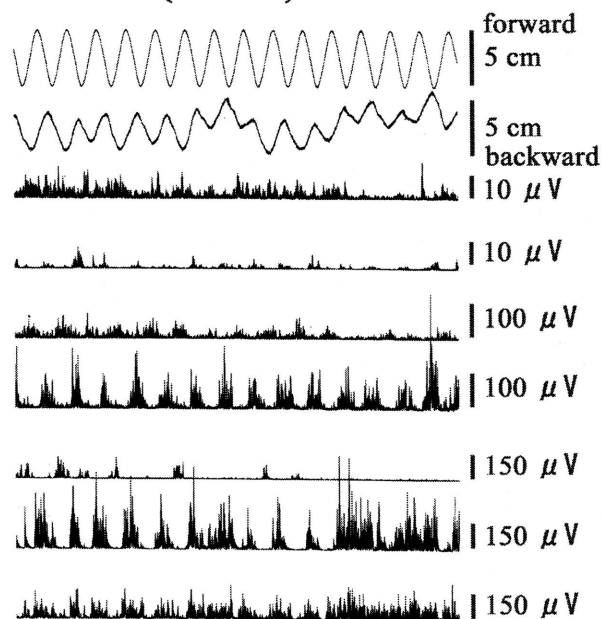
(1.5 Hz)



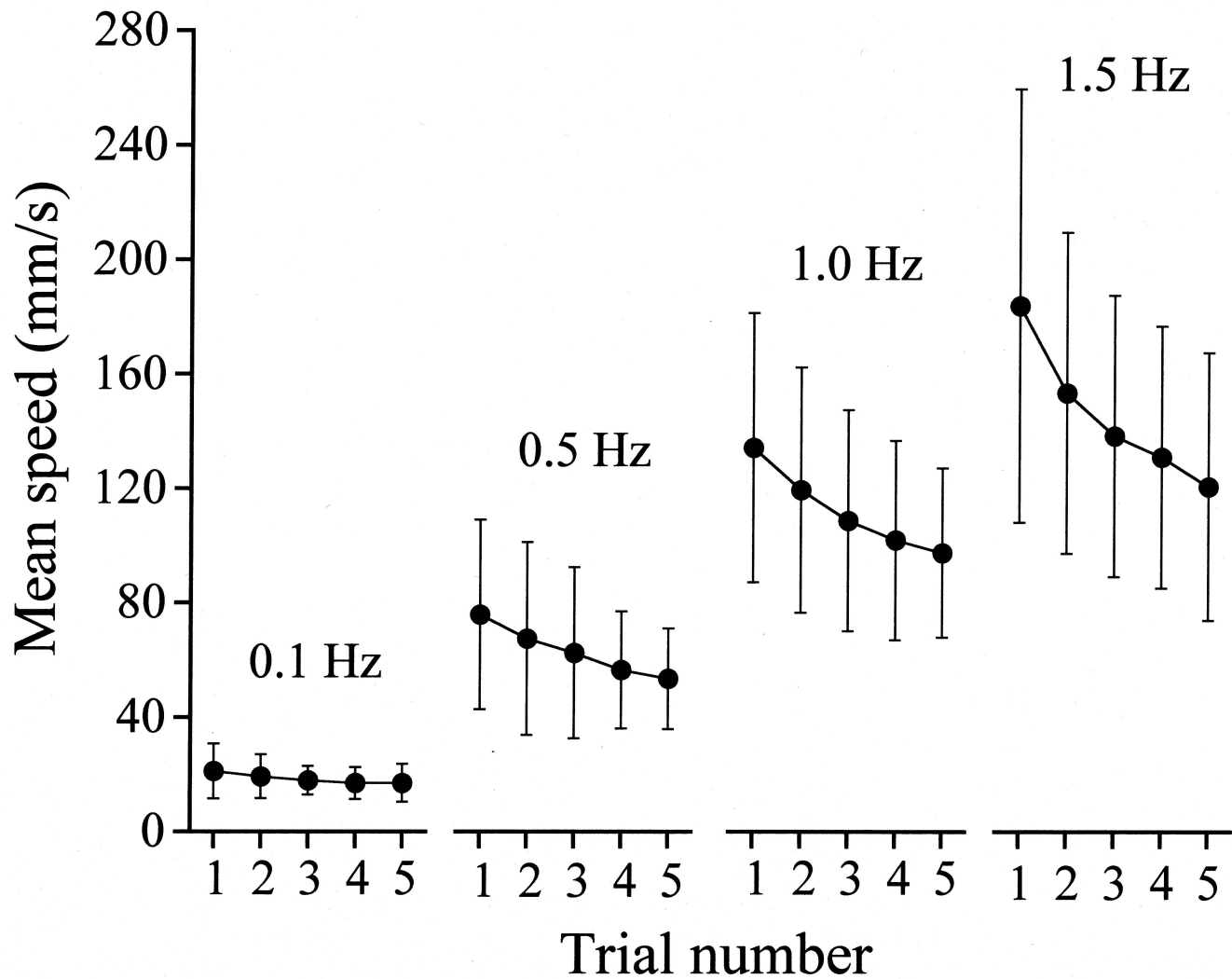
Subj. KU (0.5 Hz)

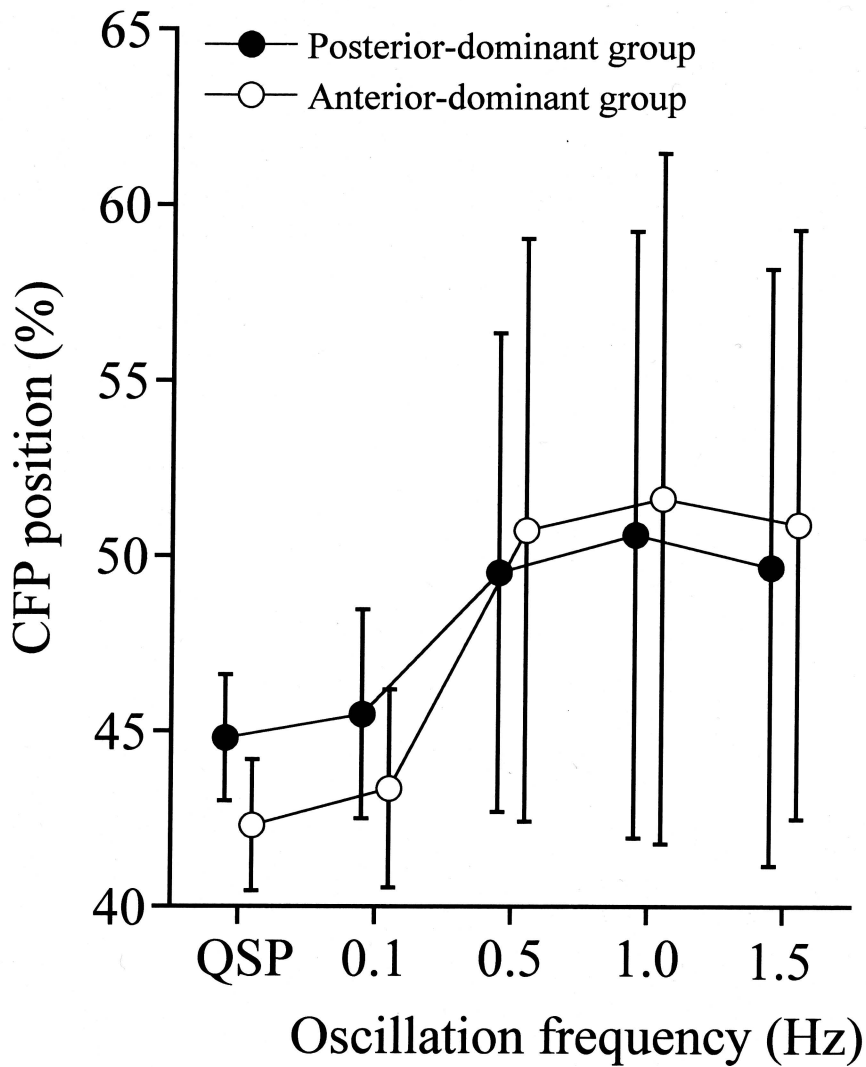


(1.5 Hz)

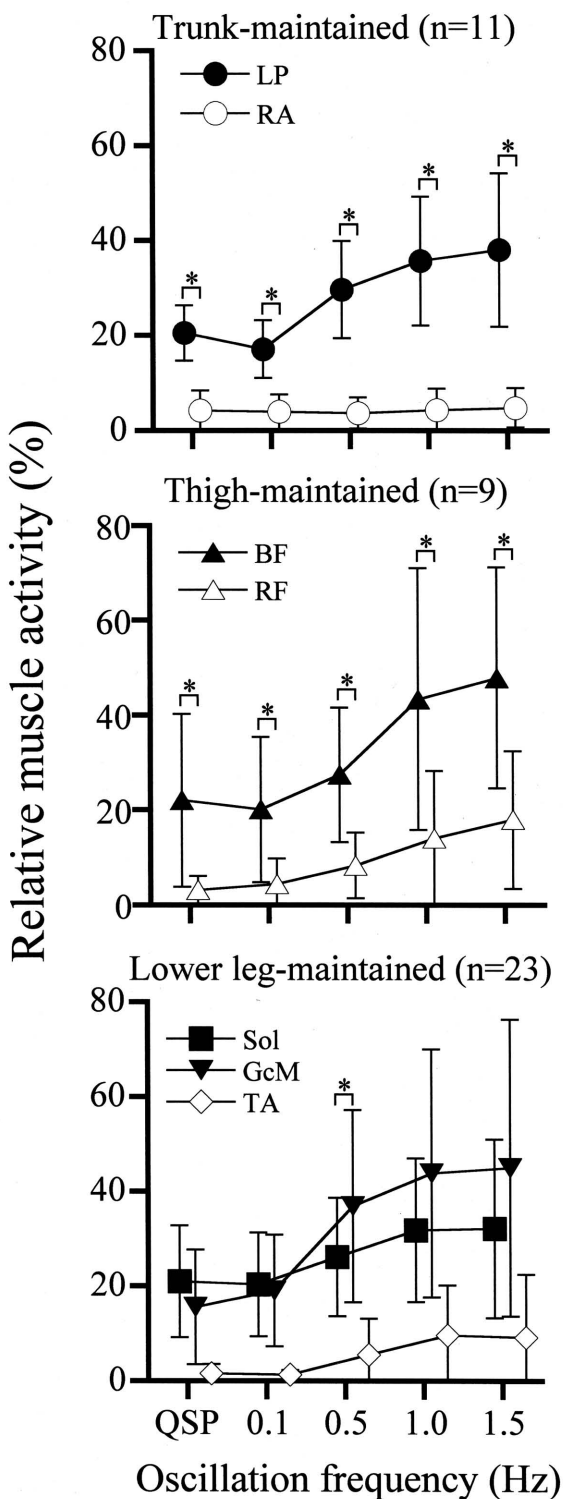


2 sec.

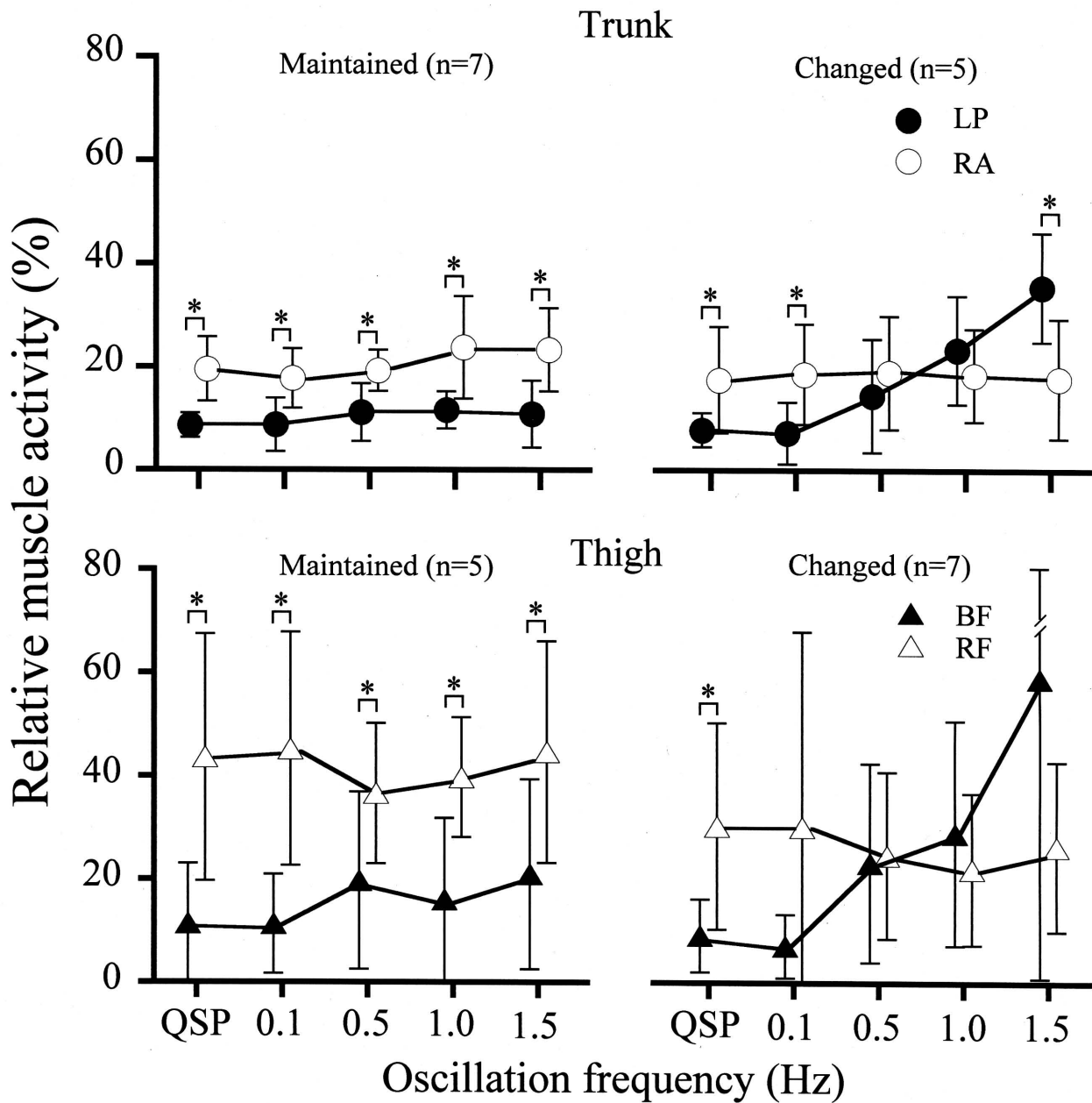




Posterior-dominant group

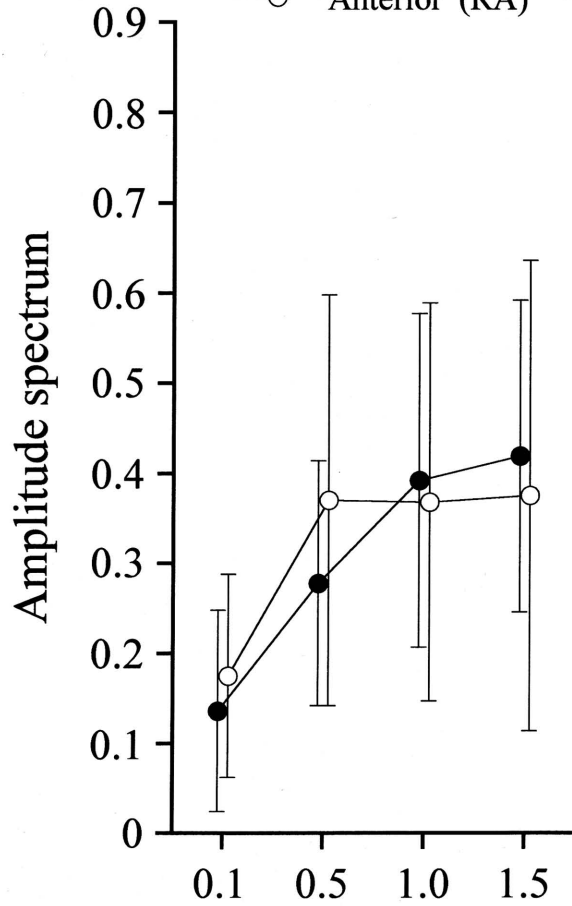


Anterior-dominant group



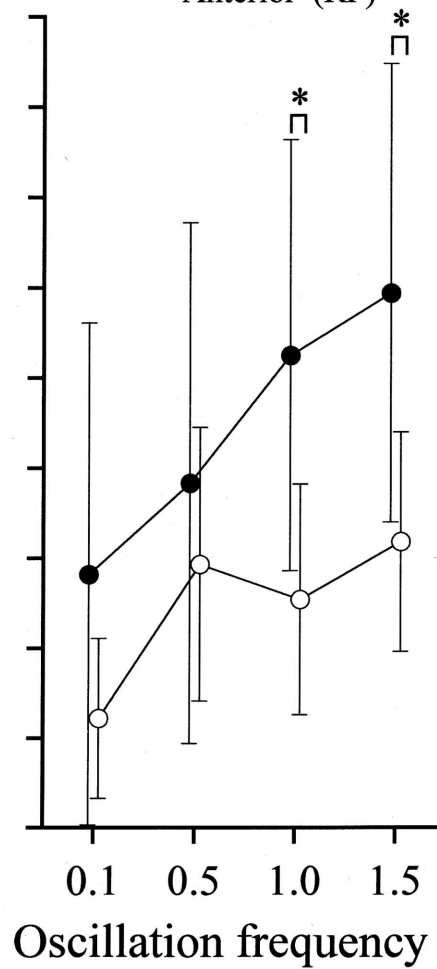
Trunk

- Dominant muscle
- Posterior (LP)
 - Anterior (RA)



Thigh

- Dominant muscle
- Posterior (BF)
 - Anterior (RF)



Lower leg

- Dominant muscle
- Posterior (GcM)
 - Posterior (Sol)

