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Research Article

Effect of Zirconium Oxide and Zinc Oxide Nanoparticles on Physicochemical Properties and Antibiofilm Activity of a Calcium Silicate-Based Material

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The aim of the present study was to evaluate the antibiofilm activity against *Enterococcus faecalis*, compressive strength. and radiopacity of Portland cement (PC) added to zirconium oxide (ZrO_2), as radiopacifier, with or without nanoparticulated zinc oxide (ZnO). The following experimental materials were evaluated: PC, PC + ZrO_2 , PC + ZrO_2 + ZnO (5%), and PC + ZrO_2 + ZnO (10%). Antibiofilm activity was analyzed by using direct contact test (DCT) on *Enterococcus faecalis* biofilm, for 5 h or 15 h. The analysis was conducted by using the number of colony-forming units (ZrO_2). The compressive strength was performed in a mechanical testing machine. For the radiopacity tests, the specimens were radiographed together with an aluminium stepwedge. The results were submitted to ANOVA and Tukey tests, with level of significance at 5%. The results showed that all materials presented similar antibiofilm activity (P > 0.05). The addition of nanoparticulated ZrO decreased the compressive strength of ZrO_2 and ZrO does not interfere with the antibiofilm activity and provides radiopacity to Portland cement. However, the presence of ZrO_2 (5% or 10%) significantly decreased the compressive strength of the materials.

1. Introduction

Calcium silicate- (CS-) based materials, such as mineral trioxide aggregate (MTA), have been widely used in dentistry for different applications, including pulp capping and pulpotomy, sealing of radicular or furcation perforations, internal or external resorption, apexification, and root-end filling in endodontic surgery due to its excellent biological and adequate physicochemical properties [1–4].

Portland cement (PC) is the main component of MTA [1, 5] and both show similar physicochemical and biological characteristics [6, 7]. It has been reported that Portland cement exhibits biocompatibility and high compressive

strength allowing this material to be also suitable for medical indications, such as in orthopedic applications [8]. However, PC does not exhibit the radiopacity required to differentiate from surrounding anatomic structures. So MTA composition includes bismuth oxide ($\rm Bi_2O_3$) as radiopacifier agent [3, 9–11].

Despite advantages of MTA when compared to other materials, it is well documented that ${\rm Bi_2O_3}$ interferes with some properties of the material. Bismuth oxide interferes with the hydration mechanism of MTA and precipitation of calcium hydroxide in the hydrated paste [12]. Furthermore, the association of ${\rm Bi_2O_3}$ changes the microstructure of the cement by acting as flaws within the cement matrix [13]

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and, consequently, increases the porosity and solubility of the Portland cement reducing its resistance [13, 14]. Regarding the biocompatibility, it has been shown that $\mathrm{Bi}_2\mathrm{O}_3$ interferes with cell growth [15], increases the cytotoxicity of the material [16], and promotes inflammatory reaction on subcutaneous tissue [14].

Thus, the association of PC with other radiopacifier agents has been studied [10, 11, 17–19]. Among several radiopacifiers studied in association with PC, zirconium oxide (ZrO₂) has demonstrated satisfactory results [18, 19]. The association of PC with 30% of ZrO₂ exhibits radiopacity, compressive strength, setting time, water absorption, and solubility similar to MTA ProRoot and resulted in a calcium silicate hydrated calcium hydroxide and a minimum amount of monosulfate and ettringite (natural hydrous calcium aluminum sulfate) [17]. It was already observed that the association of PC with ZrO₂ promoted satisfactory pH, solubility, calcium ions release, and setting time [14]. It was also verified that zirconium oxide added to Portland cement promoted better biological response than association of bismuth oxide to PC in rat subcutaneous tissue [14].

The addition of nanoparticulated substances to different materials can improve some properties, such as the antimicrobial activity. Zinc oxide (ZnO) is currently being investigated as an antibacterial agent in both microscale and nanoscale formulations. Results have indicated that ZnO nanoparticles show antibacterial activity greater than for microparticles [20]. Besides, it was already demonstrated that the use of nanoparticulated zinc oxide (ZnO) increases the antimicrobial activity of some products, including against biofilms of *Staphylococcus aureus* and *Enterococcus faecalis* [21–24].

The antimicrobial potential of MTA and PC has been evaluated by using agar diffusion test, showing that PCbased cements have antimicrobial activity against some microorganisms [25]. Additionally to agar diffusion test, the antibiofilm activity can be performed by direct contact test (DCT) on Enterococcus faecalis biofilm as proposed by Faria-Júnior et al. [26]. When evaluated by this method, the Sealapex and MTA Fillapex sealers promoted reduction of bacteria on biofilms. The authors concluded that the direct contact test is a reliable method to evaluate the antibiofilm activity of cements after their initial setting. Studies on the antibiofilm activity of MTA and MTA- and PC-based materials have not been reported. Thus, the aim of this study was to evaluate the antibiofilm activity, compressive strength, and radiopacity of PC associated with ZrO2 and nanoparticulated ZnO at different proportions (5% and 10%).

2. Materials and Methods

The evaluated radiopacifiers and the proportions used in their manipulation are described in Table 1. Since this is a preliminary study, Portland cement was used as the main component due its similar composition to commercial MTA.

2.1. Antibiofilm Activity. Bovine central incisors with completely formed roots were used as substrate for biofilm

development. The roots were sectioned longitudinally. Sections of dentin blocks measuring $5 \times 5 \times 0.7$ mm (width × length × thickness) were obtained by using a diamond disc (Isomet, Buehler, Lake Bluff, IL, USA) at low speed and under irrigation. The resulting blocks were placed in a test tube containing distilled water and sterilized by autoclaving at 121°C for 20 min.

The microbiological procedures and manipulation of the sterilized dentin blocks were carried out in a laminar flow chamber (Veco Flow Ltd., Campinas, SP, Brazil). A standard strain of *Enterococcus faecalis* (ATCC 29212) was used for biofilm formation. After the purity of the strain was confirmed by Gram staining and colony morphology, the microorganism was reactivated in 4.0 mL of sterile brain heart infusion broth (BHI, Difco Laboratories Inc., Detroit, MI, USA) and kept in an oven at 37°C, for 12 hours. The optical density of the medium was measured with a spectrophotometer (Model 600 Plus, Femto, São Paulo, SP, Brazil) set at 600 nm wavelength. Next, an aliquot equivalent to 1% of the volume used for the contamination of the specimens was added and homogenized to the sterile culture medium.

The bovine dentin blocks were placed in 24-well cell culture plates and each well received 2.0 mL of pure BHI broth containing 1% of the bacterial suspension, leaving the dentin blocks all submersed. The plates were kept in an incubator (model Q816M20, Quimis Aparelhos Científicos Ltd., Diadema, SP, Brazil) under constant agitation, in microaerophilic environment at 37°C for 14 days. The BHI medium of each specimen was completely changed every 48 h, without adding new microorganisms to assure enough nutrients for the bacterial cells.

After the postmanipulation periods of 2 days, each material sample was removed from the mould, sterilized through UV light, and positioned over one of the dentin blocks containing biofilm, which were previously washed in saline solution to remove planktonic bacteria. The dentin block/material sample assemblies were placed on 48-well plates. Over each assembly, 20 µL of sterile saline solution was dropped to avoid their drying. The plates were kept in an oven at 37°C for contact times of 5 h and 15 h. Six specimens (dentin block/material) were used for each contact period. The control group comprised noncontact of the biofilm to any cement, allowing the comparison of the results. After the contact periods elapsed, the cement discs were removed and the dentin blocks containing the remaining biofilm, including those belonging to the control group, were individually stored in test tubes containing 1 mL of sterile saline solution and glass pearls. The tubes were agitated in vortex mixer (model Q220, Quimis Aparelhos Científicos Ltd., Diadema, SP, Brazil) for 1 min to disrupt the biofilm.

Following that, serial decimal dilutions of *E. faecalis* were obtained. At the end of the dilutions, three aliquots of 20 μ L of each suspension were inoculated onto Petri dishes containing *m-Enterococcus* agar medium (Difco Laboratories, Becton, Dickinson and Company, USA). Dishes were incubated at 37°C, in microaerophilic environment, for 48 h.

Group Material Manufacturer Portland cement (PC) PC PC-CPB-40 structural Votoran, Votorantim Cimentos, Brazil $330 \,\mu\text{L}$ of distilled water PC (70%) + ZrO₂ (30%) PC-CPB-40 structural Votoran, Votorantim Cimentos, Brazil $PC + ZrO_2$ 330 μ L of distilled water ZrO2—Sigma-Aldrich Brazil Ltd., São Paulo, SP, Brazil PC-CPB-40 structural Votoran, Votorantim Cimentos, Brazil $PC (65\%) + ZrO_2 (30\%) + ZnO$ ZrO₂—Sigma-Aldrich Brazil Ltd., São Paulo, SP, Brazil $PC + ZrO_2 + ZnO$ (5%) (5%)ZnO—Nanotechnology Laboratory of the Physics Institute of São Carlos, SP, $330 \,\mu\text{L}$ of distilled water Brazil PC-CPB-40 structural Votoran, Votorantim Cimentos, Brazil $PC (60\%) + ZrO_2 (30\%) + ZnO$ ZrO₂—Sigma-Aldrich Brazil Ltd., São Paulo, SP, Brazil $PC + ZrO_2 + ZnO (10\%) (10\%)$ ZnO—Nanotechnology Laboratory of the Physics Institute of São Carlos, SP, 330 µL of distilled water Brazil

TABLE 1: Experimental materials and their manufacturers.

PC: Portland cement. ZrO₂: zirconium oxide. ZnO: zinc oxide.

The readings for each Petri dish resulted from mean CFU $\rm mL^{-1}$ in the three areas of the bacterial growth, at dilutions that generated between 5 and 50 colonies per field. From these means, the number of CFU $\rm mL^{-1}$ was calculated for each contact period of the filling cements with the biofilm developed onto the dentin blocks. Data were subjected to logarithmic transformation and the result was presented as the mean of the six specimens in each group.

2.2. Compressive Strength. The compressive strength was determined according to the method recommended by the BSI [27]. To the test, 6 specimens, measuring 12 mm in height by 6 mm in diameter, were performed as previously described [14, 28]. The specimens were maintained at 37°C and 100% relative humidity by a gauze moistened in distilled water until the tests were performed. Each experimental group was subjected to testing at 24 hours and at 21 days after manipulation of the cements [28].

The surface of each specimen was smoothed using a 600-grit sandpaper. The compression strength was evaluated using a universal testing machine (EMIC DL 2000, Emic Equipamentos, São José dos Pinhais, PR, Brazil) at crosshead speed of 0.5 mm/s with a load of 5 kN. All measurements were recorded in kg and converted to megapascal (MPa).

2.3. Radiopacity. The specimens used for radiopacity test were prepared according to the ISO 6876/200121 standard for dental root-sealing materials [29]. Six samples, with 10 mm diameter by 1.0 mm thickness, of each group were subjected to the radiopacity test [14, 25]. After the mixing of the materials, they were stored in 100% humidity at 37°C for 48 hours to set. Subsequently, they were positioned on five occlusal radiographic films (Insight-Kodak Comp, Rochester, NY, USA) and exposed, along with an aluminum stepwedge with variable thickness (from 2 to 16 mm, in 2-mm increments). An X-ray device set at 60 kV, 7 mA, 15 pulses/s, and focal distance of 30 cm was used. Radiographs were digitized using a desktop scanner (SnapScan 1236-Agfa, Deutschland) and the digitized images were imported to

the Image Tool 3.0 (UTHSCSA, San Antonio, Texas, USA). The equal-density tool was used to identify equal-density areas in the images [11]. This procedure allowed comparison between the radiographic density of the cements and the radiopacity of the different aluminum stepwedge thicknesses. The area corresponding to the specimen was selected in each radiographic image to verify the thickness of the aluminum stepwedge detected by the software as equivalent to the material's radiographic density. Thus, the radiopacity of the evaluated materials was estimated from the thickness of aluminum (in millimeters) by using a conversion equation [11]. The values recorded for each material were averaged to obtain a single value in mmAl.

2.4. Statistical Analysis. The data were subjected to normality test. Once the normal distribution was verified, data were submitted to ANOVA (parametric test) and Tukey tests ($P \le 0.05$).

3. Results

- *3.1.* Antibiofilm Activity. All experimental groups showed similar antibiofilm activity which was greater than control group (P < 0.05). The biofilm was not completely removed in any of the evaluated groups (Table 2).
- 3.2. Compressive Strength. At both periods, assessed, pure PC obtained compression strength higher than the other materials. The addition of 5% and 10% nanoparticulated ZnO decreased the compression strength at both experimental periods (Table 2).
- 3.3. Radiopacity. The addition of different radiopacifiers significantly increased the radiopacity of the materials when compared to pure PC. PC + $\rm ZrO_2$ + $\rm ZnO$ (10%) exhibited radiopacity higher than other groups (Table 2).

Tests	PC	$PC + ZrO_2$	$PC + ZrO_2 + ZnO$ (5%)	$PC + ZrO_2 + ZnO (10\%)$	Control
DCT-5 h (UFC)	$5.84^{a} \pm 0.44$	$5.67^{a} \pm 0.67$	$5.90^{a} \pm 0.40$	$5.72^{a} \pm 0.36$	$7.11^{b} \pm 0.48$
DCT-15 h (UFC)	$5.07^{a} \pm 3.78$	$5.09^{a} \pm 0.15$	$5.06^{a} \pm 0.67$	$5.15^{a} \pm 0.46$	$6.85^{\rm b} \pm 0.18$
24 h compression strength (MPa)	$32.11^a \pm 3.64$	$24.09^{b} \pm 1.22$	$0.58^{\circ} \pm 0.03$	$0.62^{c} \pm 0.06$	_
21 d compression strength (MPa)	$67.88^{a} \pm 7.35$	$57.43^{\rm b} \pm 7.0$	$30.90^{\circ} \pm 5.32$	$27.83^{\circ} \pm 4.77$	_
Radiopacity (mmAl)	$1.15^{\circ} \pm 0.12$	$3.70^{b} \pm 0.06$	$3.50^{b} \pm 0.16$	$3.92^a \pm 0.18$	_

TABLE 2: Mean and standard deviation values of the different cements tested.

Mean ± standard deviation.

Similar letters indicate statistical similarity ($P \ge 0.05$).

4. Discussion

The agar diffusion antimicrobial test allows the comparison of the antimicrobial effect of different materials, but it has limitations once its results depend directly on the material solubility. Other methods to assess antimicrobial activity use the direct contact of the materials to planktonic bacteria [30].

Notwithstanding, the microorganisms of the root canal system are organized as biofilm, which makes them more resistant. In the present study, the methodology enabled the antimicrobial effect evaluation of cements after setting on bacteria organized as biofilm, according to Faria-Júnior et al. [26], but different from the studies on materials over planktonic bacteria. *Enterococcus faecalis* is capable of surviving in alkaline environments and forming biofilm [31]. The bovine dentin substrate provides adequate biofilm formation after the period of 14 days [32].

The use of nanoparticulated ZnO was evaluated by Seil and Webster [33], demonstrating its antimicrobial effect against suspensions of *S. aureus* and *P. aeruginosa* [24]. Kishen et al. [21] showed ZnO antimicrobial effect against *E. faecalis* suspension. Shrestha et al. [22] evaluated ZnO both on biofilm and on planktonic *E. faecalis*, showing bacteria elimination in suspension and the decrease of biofilm thickness, which is in agreement with the results of this study, as observed for all materials.

Regarding MTA- and PC-based materials, their antimicrobial effect was demonstrated by Asgary and Kamrani [34] using agar diffusion test. Guerreiro-Tanomaru et al. [32] showed antimicrobial effectiveness of PC associated with different radiopacifiers, including ZrO₂.

Although ZnO has presented a satisfactory antimicrobial effect in other researches [21–23, 33], in the present study, the materials with ZnO showed partial effect on *E faecalis* biofilm. This result can be associated with the hydration reaction of MTA with ZnO particles, resulting in a material with low solubility and, consequently, reducing the antimicrobial effect.

The reduction of bacteria observed in the other groups can be related to high pH values exhibited by PC-based materials. According to Guerreiro-Tanomaru et al. [32], the pH of either pure PC or PC in addition to different radiopacifiers including ZrO₂ is about 10.2. Faria-Júnior et al. [26] observed similar results for MTA, with values close to the required to achieve effectiveness against *E. faecalis* [35].

The results of the present study demonstrated that PC associated with microparticulated ZrO₂ and nanoparticulated ZnO present an adequate radiopacity, ranging from

3.50 mmAl to 3.92 mmAl, above the minimum value recommended by ANSI/ADA specification n.57 of 3 millimeters of aluminum [36]. These findings are in accordance with those values previously observed for PC associated with ZrO₂ by Bortoluzzi et al. [10].

Regarding compression strength, all materials showed higher values at 21-day period when compared with 24-hour period. This increase in resistance occurs because of the ending of hydration phase, providing more hardness to the material. Saldana et al. [37] demonstrated that $\rm ZrO_2$ favors the mechanical properties of the material, corroborating the results observed in the present study. Notwithstanding, the values of the association PC + $\rm ZrO_2$ were smaller than PC which is in accordance with Silva et al. [14].

Furthermore, the nanoparticulated zinc oxide dramatically reduced the compressive strength of the materials, especially at 24 hours. At least in part, this finding can be related to the reaction mechanism of nanoparticles with PC and ZrO₂, culminating in a material with flaws in the microstructure and low compressive strength.

ZrO₂ seems to be an adequate alternative radiopacifier for PC since it shows biocompatibility and low toxicity [14], provides satisfactory radiopacity [10, 14] and physicochemical properties [14, 15, 17, 18], and maintains the antimicrobial activity of PC [32]. However, considering the results of the present study, further researches are needed for better comprehension of the interaction between ZnO nanoparticles and calcium silicate-based cements with ZrO₂.

MTA was formulated from commercial Portland cement combined with bismuth oxide powder for radiopacity. However, the composition, fineness, setting time, and strength of Portland cement are not controlled or guaranteed. Portland cement is an unsuitable substitute for MTA based on several characteristics that are essential to the MTA performance. Thus, this study was performed in order to evaluate the effect of the association of zinc oxide nanoparticles in physicochemical and antimicrobial properties of calcium silicate cements. Additional studies are required for this or similar associations in order to verify the possibilities for clinical use.

5. Conclusion

It can be concluded that the addition of $\rm ZrO_2$ and $\rm ZnO$ does not interfere in the antibiofilm activity and provides radiopacity to Portland cement. However, the presence of $\rm ZnO$ significantly decreased the compressive strength of the material.

Conflict of Interests

The authors declare that there is no conflict of interests regarding the publication of this paper.

References

- [1] J. Camilleri and T. R. Pitt Ford, "Mineral trioxide aggregate: a review of the constituents and biological properties of the material," *International Endodontic Journal*, vol. 39, no. 10, pp. 747–754, 2006.
- [2] M. Parirokh and M. Torabinejad, "Mineral trioxide aggregate: a comprehensive literature review—part III: Clinical applications, drawbacks, and mechanism of action," *Journal of Endodontics*, vol. 36, no. 3, pp. 400–413, 2010.
- [3] J. Tanalp, M. Karapınar-Kazandağ, S. Dölekoğlu, and M. B. Kayahan, "Comparison of the radiopacities of different rootend filling and repair materials," *The Scientific World Journal*, vol. 2013, Article ID 594950, 4 pages, 2013.
- [4] Y. Jiang, Q. Zheng, X. Zhou, Y. Gao, and D. Huang, "A comparative study on root canal repair materials: a cytocompatibility assessment in L929 and MG63 cells," *The Scientific World Journal*, vol. 2014, Article ID 463826, 8 pages, 2014.
- [5] J. Camilleri, F. E. Montesin, L. di Silvio, and T. R. Pitt Ford, "The chemical constitution and biocompatibility of accelerated Portland cement for endodontic use," *International Endodontic Journal*, vol. 38, no. 11, pp. 834–842, 2005.
- [6] C. Estrela, L. L. Bammann, C. R. Estrela, R. S. Silva, and J. D. Pécora, "Antimicrobial and chemical study of MTA, Portland cement, calcium hydroxide paste, Sealapex and Dycal," *Brazilian Dental Journal*, vol. 11, no. 1, pp. 3–9, 2000.
- [7] R. Holland, V. de Souza, M. J. Nery et al., "Reaction of rat connective tissue to implanted dentin tube filled with mineral trioxide aggregate, Portland cement or calcium hydroxide.," *Brazilian dental journal*, vol. 12, no. 1, pp. 3–8, 2001.
- [8] G. Wynn-Jones, R. M. Shelton, and M. P. Hofmann, "Development of Portland cement for orthopedic applications, establishing injectability and decreasing setting times," *Journal of Biomedical Materials Research Part B: Applied Biomaterials*, vol. 100, no. 8, pp. 2213–2221, 2012.
- [9] M. Tanomaru-Filho, G. F. Da Silva, M. A. H. Duarte, M. Gonçalves, and J. M. G. Tanomaru, "Radiopacity evaluation of root-end filling materials by digitization of images," *Journal of Applied Oral Science*, vol. 16, no. 6, pp. 376–379, 2008.
- [10] E. A. Bortoluzzi, J. M. Guerreiro-Tanomaru, M. Tanomaru-Filho, and M. A. H. Duarte, "Radiographic effect of different radiopacifiers on a potential retrograde filling material," *Oral Surgery, Oral Medicine, Oral Pathology, Oral Radiology and Endodontology*, vol. 108, no. 4, pp. 628–632, 2009.
- [11] M. A. Hungaro Duarte, G. D. de Oliveira El Kadre, R. R. Vivan, J. M. Guerreiro Tanomaru, M. T. Filho, and I. G. de Moraes, "Radiopacity of portland cement associated with different radiopacifying agents," *Journal of Endodontics*, vol. 35, no. 5, pp. 737–740, 2009.
- [12] J. Camilleri, "Hydration mechanisms of mineral trioxide aggregate," *International Endodontic Journal*, vol. 40, no. 6, pp. 462–470, 2007.
- [13] K. S. Coomaraswamy, P. J. Lumley, and M. P. Hofmann, "Effect of bismuth oxide radioopacifier content on the material properties of an endodontic Portland cement-based (MTA-like) system," *Journal of Endodontics*, vol. 33, no. 3, pp. 295–298, 2007.

- [14] G. F. Silva, R. Bosso, R. V. Ferino et al., "Microparticulated and nanoparticulated zirconium oxide added to calcium silicate cement: evaluation of physicochemical and biological properties," *Journal of Biomedical Materials Research—Part A*, 2014.
- [15] J. Camilleri, F. E. Montesin, S. Papaioannou, F. McDonald, and T. R. P. Ford, "Biocompatibility of two commercial forms of mineral trioxide aggregate," *International Endodontic Journal*, vol. 37, no. 10, pp. 699–704, 2004.
- [16] K. S. Min, H. I. Kim, H. J. Park, S. H. Pi, C. U. Hong, and E. C. Kim, "Human pulp cells response to Portland cement in vitro," *Journal of Endodontics*, vol. 33, no. 2, pp. 163–166, 2007.
- [17] J. Camilleri, A. Cutajar, and B. Mallia, "Hydration characteristics of zirconium oxide replaced Portland cement for use as a root-end filling material," *Dental Materials*, vol. 27, no. 8, pp. 845–854, 2011.
- [18] M. A. H. Duarte, P. G. Minotti, C. T. Rodrigues et al., "Effect of different radiopacifying agents on the physicochemical properties of white portland cement and white mineral trioxide aggregate," *Journal of Endodontics*, vol. 38, no. 3, pp. 394–397, 2012
- [19] A. L. G. Cornélio, L. P. Salles, M. C. da Paz, J. A. Cirelli, J. M. Guerreiro-Tanomaru, and M. T. Filho, "Cytotoxicity of Portland cement with different radiopacifying agents: a cell death study," *Journal of Endodontics*, vol. 37, no. 2, pp. 203–210, 2011.
- [20] S. Nair, A. Sasidharan, V. V. Divya Rani et al., "Role of size scale of ZnO nanoparticles and microparticles on toxicity toward bacteria and osteoblast cancer cells," *Journal of Materials Science: Materials in Medicine*, vol. 20, no. 1, pp. S235–S241, 2009.
- [21] A. Kishen, Z. Shi, A. Shrestha, and K. G. Neoh, "An investigation on the antibacterial and antibiofilm efficacy of cationic nanoparticulates for root canal disinfection," *Journal of Endodontics*, vol. 34, no. 12, pp. 1515–1520, 2008.
- [22] A. Shrestha, S. Zhilong, N. K. Gee, and A. Kishen, "Nanoparticulates for antibiofilm treatment and effect of aging on its antibacterial activity," *Journal of Endodontics*, vol. 36, no. 6, pp. 1030–1035, 2010.
- [23] B. A. Sevinç and L. Hanley, "Antibacterial activity of dental composites containing zinc oxide nanoparticles," *Journal of Biomedical Materials Research—Part B Applied Biomaterials*, vol. 94, no. 1, pp. 22–31, 2010.
- [24] J. T. Seil and T. J. Webster, "Reduced Staphylococcus aureus proliferation and biofilm formation on zinc oxide nanoparticle PVC composite surfaces," *Acta Biomaterialia*, vol. 7, no. 6, pp. 2579–2584, 2011.
- [25] M. Tanomaru-Filho, J. M. G. Tanomaru, D. B. Barros, E. Watanabe, and I. Y. Ito, "In vitro antimicrobial activity of endodontic sealers, MTA-based cements and Portland cement," *Journal of Oral Science*, vol. 49, no. 1, pp. 41–45, 2007.
- [26] N. B. Faria-Júnior, M. Tanomaru-Filho, F. L. C. V. Berbert, and J. M. Guerreiro-Tanomaru, "Antibiofilm activity, pH and solubility of endodontic sealers," *International Endodontic Journal*, vol. 46, no. 8, pp. 755–762, 2013.
- [27] British Standards Institution, Specification for Dental Glass Ionomer Cements BS 6039:1981.
- [28] I. Islam, H. K. Chng, and A. U. Jin Yap, "Comparison of the physical and mechanical properties of MTA and portland cement," *Journal of Endodontics*, vol. 32, no. 3, pp. 193–197, 2006.
- [29] International Organization for Standardization, ISO 6876: Dental Root Sealing Materials, The Organization, Geneva, Switzerland, 2001.

- [30] A. U. Eldeniz, H. H. Hadimli, H. Ataoglu, and D. Orstavik, "Antibacterial effect of selected root-end filling materials," *Journal of Endodontics*, vol. 32, no. 4, pp. 345–349, 2006.
- [31] M. Evans, J. K. Davies, G. Sundqvist, and D. Figdor, "Mechanisms involved in the resistance of *Enterococcus faecalis* to calcium hydroxide," *International Endodontic Journal*, vol. 35, no. 3, pp. 221–228, 2002.
- [32] J. M. Guerreiro-Tanomaru, A. L. G. Cornelio, C. Andolfatto, L. P. Salles, and M. Tanomaru-Filho, "pH and antimicrobial activity of Portland cement associated with different radiopacifying agents," *ISRN Dentistry*, vol. 2012, Article ID 469019, 5 pages, 2012.
- [33] J. T. Seil and T. J. Webster, "Antibacterial effect of zinc oxide nanoparticles combined with ultrasound," *Nanotechnology*, vol. 23, no. 49, Article ID 495101, 2012.
- [34] S. Asgary and F. A. Kamrani, "Antibacterial effects of five different root canal sealing materials," *Journal of Oral Science*, vol. 50, no. 4, pp. 469–474, 2008.
- [35] C. P. McHugh, P. Zhang, S. Michalek, and P. D. Eleazer, "pH required to kill *Enterococcus faecalis* in vitro," *Journal of Endodontics*, vol. 30, no. 4, pp. 218–219, 2004.
- [36] American Dental Association, "American Dental Association specification no 57 for endodontic filling materials," American National Standard, ADA, Chicago, Ill, USA, 1984.
- [37] L. Saldana, A. Mendez-Vilas, L. Jiang et al., "In vitro biocompatibility of an ultrafine grained zirconium," *Biomaterials*, vol. 28, no. 30, pp. 4343–4354, 2007.



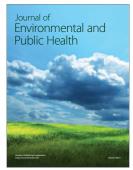














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