

## Research Article

# Titanium Oxide Nanotube Surface Topography and MicroRNA-488 Contribute to Modulating Osteogenesis

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Understanding the biocomplexity of cell behavior in relation to the topographical characteristics of implants is essential for successful osseointegration with good longevity and minimum failure. Here, we investigated whether culture on titanium oxide (TiO<sub>2</sub>) nanotubes of various diameters could affect the behavior and differentiation of MC3T3-E1 cells. Among the tested nanotubes, those of 50 nm in diameter were found to trigger the expression of the osteoblast-specific transcription factors, sp7 and Dlx5, and upregulate the expression of alkaline phosphatase (ALP). Here, we report that miR-488 was significantly induced in osteoblasts cultured on 50 nm nanotubes and continued to increase with the progression of osteoblast differentiation. Furthermore, downregulation of miR-488 suppressed the expression levels of ALP and matrix metalloproteinase-2 (MMP-2). This suppression of ALP transcription was overcome by treatment with the MMP-2 activator, bafilomycin A1. Collectively, these results suggest that 50 nm is the optimum TiO<sub>2</sub> nanotube diameter for implants, and that modulation of miR-488 can change the differentiation activity of cells on TiO<sub>2</sub> nanotubes. This emphasizes that we must fully understand the physicochemical properties of TiO<sub>2</sub> nanotubes and the endogenous biomolecules that interact with such surfaces, in order to fully support their clinical application.

## 1. Introduction

Accumulating experimental evidence suggests that nanoscale topography is an important factor for cellular recognition of the biological microenvironment and biomimetic materials used for vascular grafts, stents, and bone implants [1, 2]. Titanium (Ti) and its alloys have been widely used as implantation materials, as they provide direct physical bonding with the adjacent bone surface in orthopedic and dental surgery. The low success rate of using machined surfaces, such as those first tested as dental implants in 1965, has long indicated that the materials and particle sizes of implant surfaces are critical to the initial osseointegration and success of implants [3]. Although the current success rate is very high, implants still occasionally loosen and fail due to incomplete

osseointegration between the implantation materials and the surrounding bone [3].

Several studies have suggested that some cells can show cell-type-specific behaviors and activities on TiO<sub>2</sub> nanotubes. For example, mesenchymal stem cells showed enhanced activity on anatase-phase nanotubes (70–100 nm diameter), and proliferation of smooth muscle cells was enhanced on TiO<sub>2</sub> [4]. Furthermore, Webster et al. [5] reported that osteoblasts showed significantly greater adhesion to a nanophase surface compared to conventional aluminum and titanium surfaces.

MicroRNAs (miRNAs) are short (18–25 nucleotides) noncoding RNAs that posttranscriptionally regulate gene expression by recognizing binding sites in the 3'-untranslated

regions (3'-UTRs) of target genes [6, 7]. Growing evidence suggests that miRNAs regulate various developmental and homeostatic events in vertebrates and invertebrates. For example, miRNAs have been implicated in osteoblast differentiation [8] and osteogenesis. miR-206 is expressed in the osteoblastic cell lineage, where its expression gradually decreases in parallel with osteoblast differentiation [9]. The modulation of miR-206 expression in osteoblasts markedly affects their differentiation potential by altering the accumulation of connexin 43, and the osteoblast-specific expression of miR-206 *in vivo* triggers severe bone loss by impairing osteoblast differentiation [10]. miR-29 and miR-133 also appear to be important for osteoblast differentiation [11, 12]: miR-29 increases during the progression of osteoblastic differentiation in primary cultures of murine calvarial osteoblasts [13], while miR-133 seems to negatively regulate the differentiation of osteoblasts [14]. Recently, our laboratory demonstrated that miR-488 contributes to the regulation of matrix metalloproteinase (MMP)-2 [13]. Since MMP-2 is thought to control homeostatic and morphogenetic events during osteogenic differentiation [15], we speculate that miR-488 is involved in the formation of bone [14, 16].

Here, we studied the *in vitro* behavior of osteoblast cells cultured on vertically aligned TiO<sub>2</sub> nanotubes of different diameters. We investigated the effect of such nanostructures on osteoblast cell morphology and the kinetics of cell proliferation, examined cell responses on nanotubes versus plastic polypyrrole layers, and tested for differential expression of miR-488.

## 2. Experimental Section

**2.1. Cell Culture and Differentiation.** The differentiation of MC3T3-E1 cells (ATCC, Rockville, MD) was induced by incubation in differentiation medium (growth medium containing 50 µg/mL ascorbic acid and 10 mM 2-glycerophosphate). The medium was changed every 2 to 3 days. Differentiation was assessed by alizarin red staining. Briefly, differentiated cell layers were washed with phosphate buffered saline (PBS) and then fixed for 15 min with neutral formalin (10% formaldehyde in PBS). The fixation solution was removed and the cells were incubated in distilled water for 15 min and then with 1% alizarin red solution for 5 min. The staining solution was removed, the cells were rinsed three times with water, and the stained cultures were kept in distilled water for microscopic examination.

**2.2. TiO<sub>2</sub> Nanotube Preparation.** Ti sheets (thickness, 250 µm; purity, 99.5%; Alfa-Aesar, Ward Hill, MA) were sequentially cleaned with acetone, 70% ethanol, and water. Cleaned specimens were anodized with hydrofluoric acid (0.5 w/v%; purity, 48%; EM-Science, Gardena, CA) at 20 V for 30 minutes. The prepared TiO<sub>2</sub> nanotube specimens were washed under running water for 30 seconds, dried overnight at 80°C, and heat-treated for 2 hours at 500°C. Heat-treated specimens were cut into pieces (1.27 × 1.27) and then sterilized in an autoclave.

**2.3. Cell Culture on TiO<sub>2</sub> Nanotubes.** MC3T3-E1 cells were incubated in differentiation medium as described above and

placed on the TiO<sub>2</sub> nanotubes. After 2 days, biochemical and cellular analyses (see below) were performed.

**2.4. Immunocytochemistry.** Cells grown on cover slips were washed three times with PBS and then fixed and permeabilized as described above. For actin staining, samples were stained with Alexa488-phalloidin (Molecular Probes, Eugene, OR) prepared in PBS containing 1% (v/v) bovine serum albumin for 1 h at room temperature in a lightproof box. The samples were then washed three times with water, mounted with Gel/Mount (Biomedica, Foster City, CA), and examined under a confocal microscope (MRC 1024/ES, Bio-Rad, CA).

**2.5. Real-Time Quantitative RT-PCR of miRNA and mRNA Expression Levels.** The expression levels of various mRNAs were quantified using the appropriate real-time quantitative polymerase chain reaction- (RT-PCR-) based gene expression assay kits (Applied Biosystems, Grand Island, NY). The results were normalized with respect to the expression of GAPDH. The following primers were utilized: GAPDH, forward (Fw) 5'-tgctcgtcgtggatctgac-3' and reverse (Rv) 5'-cctgcttcaccaccttcttg-3'; ALP, Fw 5'-atctcagggcaatgaggtac-3' and Rv 5'-caccgagtgtagtcacaa-3'; *sp7*, Fw 5'-gagaagaagccattcaca-3' and Rv 5'-gcaggcaggtgacttcttc-3'; *Dlx5*, Fw 5'-ccagccagagaagaagtgg-3' and Rv 5'-tcacctgtgttcgctcagt-3'; and MMP-2, Fw 5'-atgccatcctgataacctg-3' and Rv 5'-tgatgcttccaaactcagc-3'.

**2.6. Synthesis and Transfection of the PNA-Based miRNA Inhibitor.** The FAM-conjugated PNA-based ASOs, which contained an O-linker at the N-terminus of the PNA to improve solubility, were purchased from Panagene (Korea). A scrambled PNA-based ASO was used as a negative control. The PNA-based ASO (PNA488: UUGAAAGGCUAUUU-CUUGGUC; 200 nM) was electroporated into cells using a square-wave generator (BTX-830; Gentronics, San Diego, CA) with 200 square-wave pulses of 20 msec each.

## 3. Results and Discussion

Recent studies have revealed that miRNAs can help regulate osteoblast differentiation [10, 13] and osteogenesis [17]. Many miRNAs appear to inhibit osteogenesis by repressing osteoblastic genes [18]. Hassan et al. [19] identified a novel miRNA mechanism through which BMP-2 promotes osteoblastogenesis. miR-29a and miR-29c inhibit the expression of *Dlx5* in preosteoblasts during osteogenesis [10] and miR-125b inhibits osteoblastic proliferation by targeting the ErbB2 receptor tyrosine kinase [20]. We previously showed that miR-488 is involved in regulating MMP-2 during endochondral ossification [13], indicating that miR-488 is involved in bone formation.

Here, we first examined the expression of miR-488 during osteoblast differentiation and found that it was two-fold higher in differentiated osteoblasts, as shown by alizarin red S staining, which is used to monitor calcium accumulation (i.e., mineralization) in the ECM (Figure 1(a)). To further examine

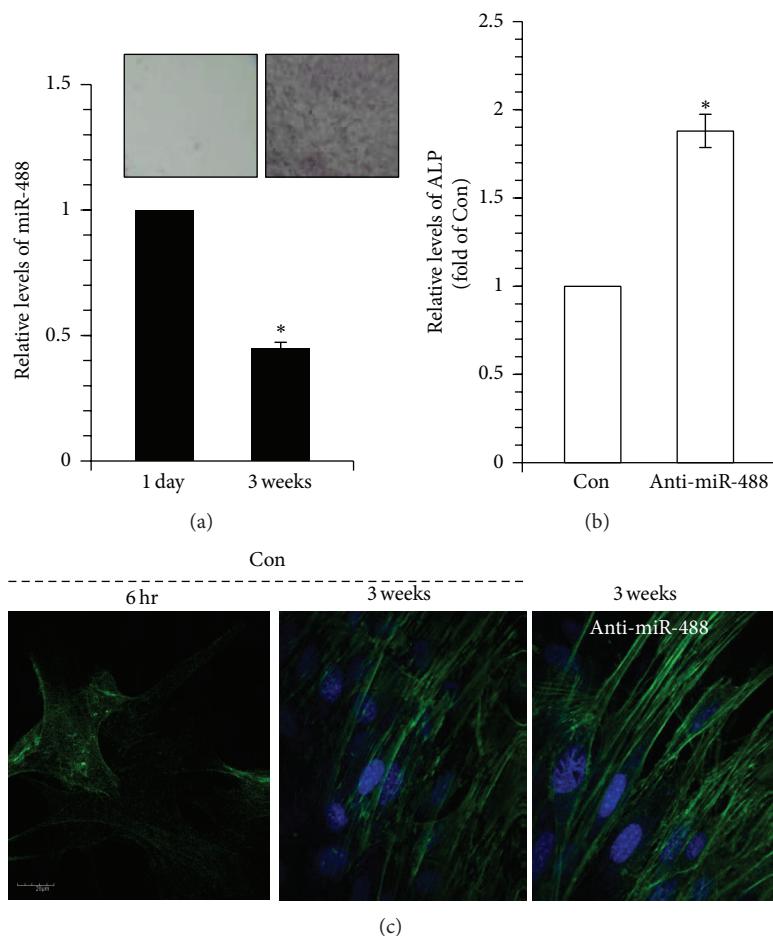


FIGURE 1: Induction of miR-488 involved in osteoblastic differentiation of MC3T3-E1 cells grown on culture dish. (a) The expression of miR-488 was measured using real-time PCR. Alizarin red S stain was used to monitor the mineralization of ECM (inserted photography). Cells were treated with PNA-based ASOs against miR-488 (anti-miR-488) or a scrambled PNA-based ASO (Con). (b) The expression of *ALP* was measured using real-time PCR. RQ of control culture was used as a control to measure fold change. (c) Cells were immunostained for F-actin with Alexa488-phalloidin. The data shown are representative of at least four independent experiments. The mean is plotted and the error bars represent 95% CI (lower/upper limit). \*  $P < 0.005$ .

the potential involvement of miR-488 in the osteoblastic differentiation of MC3T3-E1 cells, we suppressed miR-488 with PNA-based ASOs. MC3T3-E1 cells were treated with 200 nM of the anti-miR-488 inhibitor for two days, and the mRNA expression of *ALP* was determined by real-time PCR. The expression of *ALP* was elevated following treatment of cells with the miR-488 inhibitor (Figure 1(b)). These data suggest that miR-488 may negatively regulate the differentiation of osteoblasts.

Cell adhesion is a fundamental process that directly affects cell proliferation, migration, and differentiation and is involved in many biological behaviors, including the tissue integration of biomaterials [21]. The adhesion of osteoblasts to the implant material surface is essential for the success of any implant that requires osteointegration. It has been suggested that bone cells may produce stress fibers to maintain their desired morphology in the face of chronic applied tension. Since the fate of osteoblast differentiation may be determined by cell shapes *in vitro*, we performed

morphological analysis of MC3T3-E1 cells. We found that the stress fiber density was higher in cells treated for two days with the miR-488 inhibitor compared to cells treated with the scrambled control (Figure 1(c)). A recent study suggested that RhoA, which is known to affect the integrity of actin stress fibers, modulates the function and survival of osteoblasts [22]. Thus, the ability of the miR-488 inhibitor to intensify the density of stress fibers could suggest that miR-488 is functionally relevant in osteoblastic MC3T3-E1 cells.

We generated self-assembled, amorphous, heat-treated, crystallized anatase-phase TiO<sub>2</sub> nanotubes by anodizing Ti sheets in a phosphate-fluoride electrolyte at 20 V with four different diameters (30, 50, 70, and 100 nm). Upon their initial formation, TiO<sub>2</sub> nanotubes typically have an amorphous structure; thereafter, the anatase phase was produced by annealing in air at 500°C for 2 h. MC3T3-E1 cells were induced to differentiate by incubation with ascorbic acid and 2-glycerophosphate and then placed on TiO<sub>2</sub> nanotubes or culture dishes. Previously, Barthelemi et al. [15] demonstrated

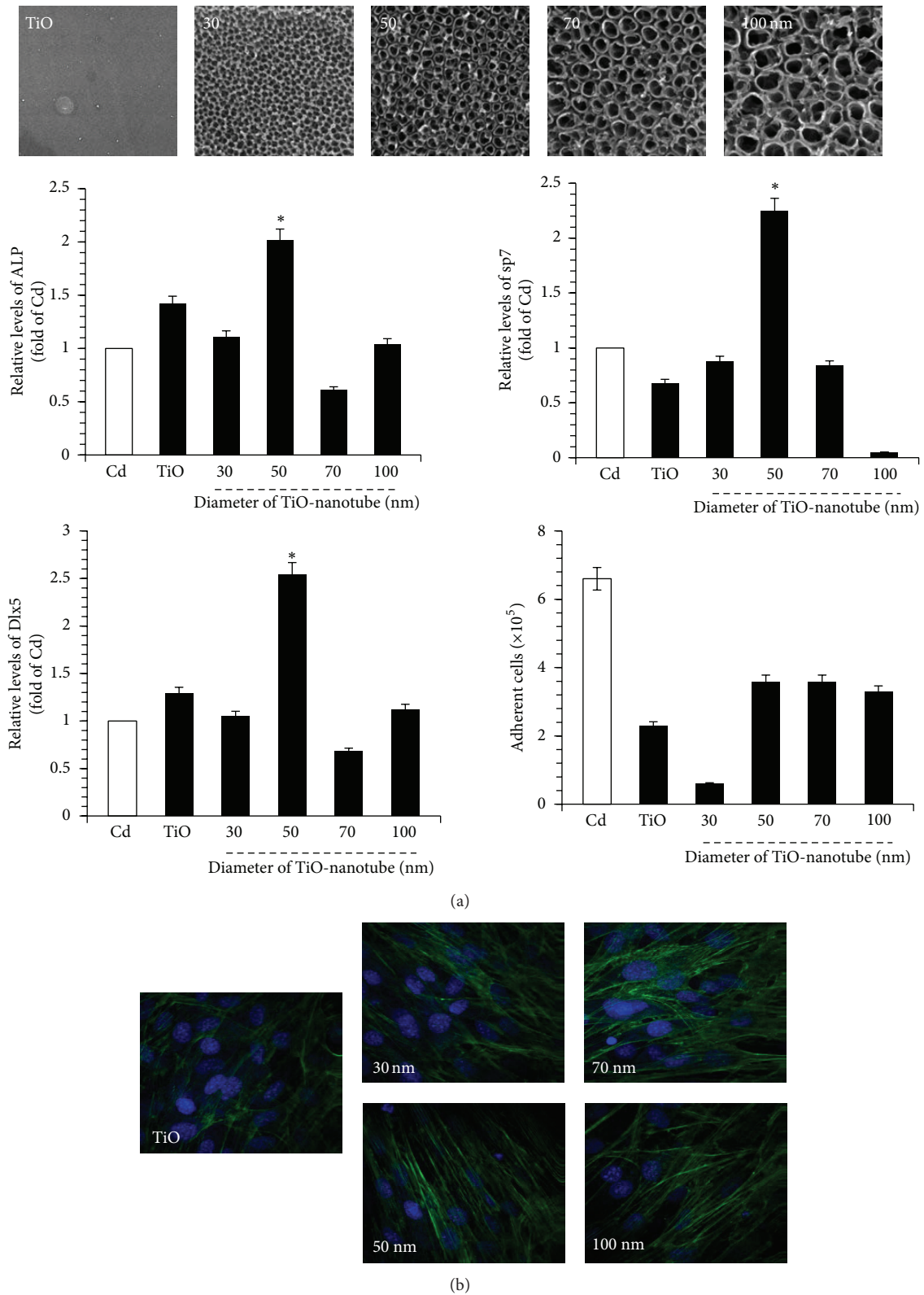


FIGURE 2: Culture on a TiO<sub>2</sub> nanotube surface affects osteoblastic differentiation of MC3T3-E1 cells. MC3T3-E1 cells were cultured on titanium oxide nanotube having various diameters (30, 50, 70, and 100 nm), titanium oxide (TiO<sub>2</sub>), or culture dish (Cd). (a) The expression of *ALP*, *sp7*, and *Dlx5* was measured using real-time PCR and cell adhesion was assayed at day 2. RQ of cells on culture dish (Cd) was used as a control to measure fold change. (b) Cells were immunostained for F-actin with Alexa488-phalloidin at day 2. Representative data is shown ( $n = 4$ ). The mean is plotted and the error bars represent 95% CI (lower/upper limit). \* $P < 0.005$ .

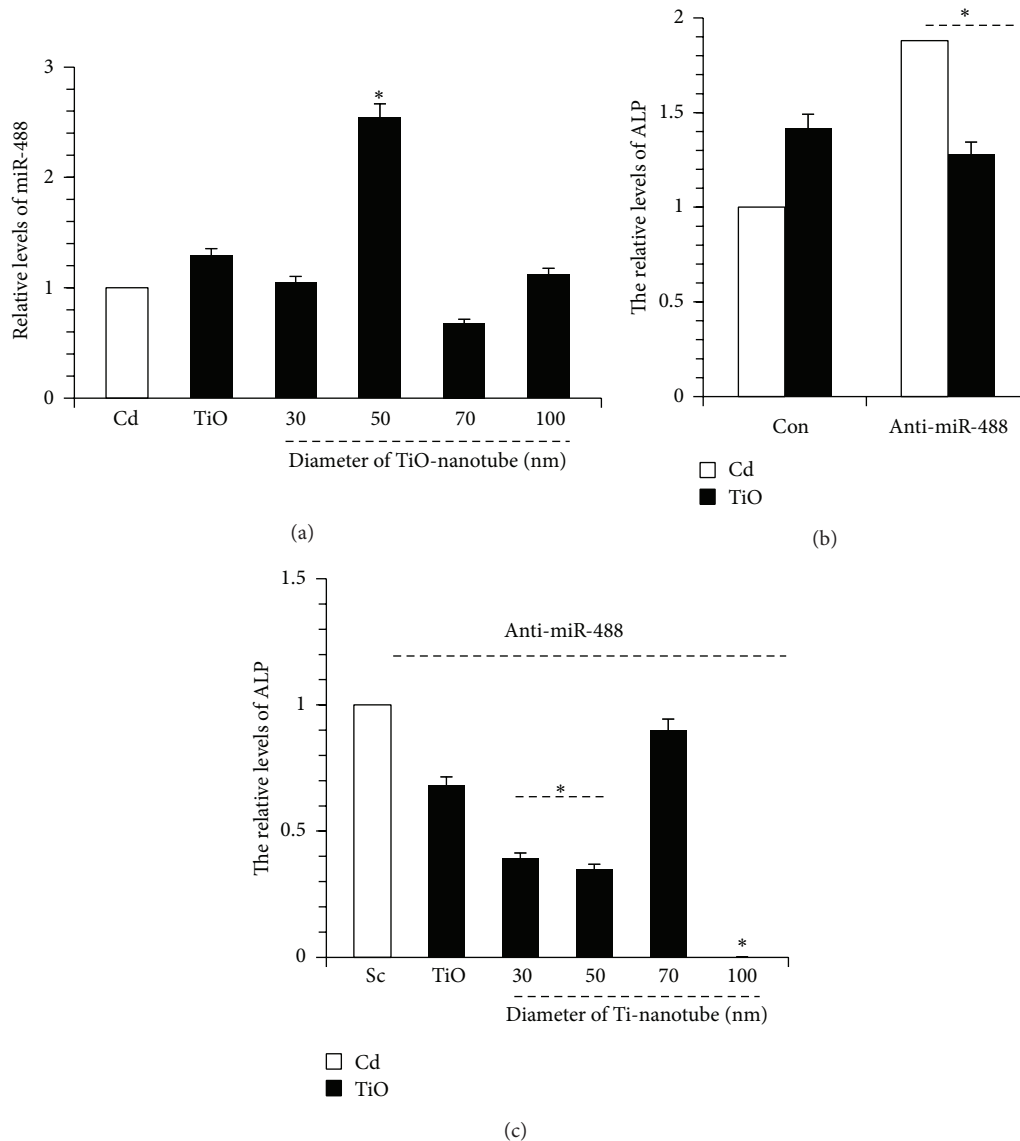


FIGURE 3: miR-488 involved in osteoblastic differentiation of MC3T3-E1 cells on TiO<sub>2</sub> nanotube surface. (a) MC3T3-E1 cells were cultured on titanium oxide nanotube having various diameters (30, 50, 70, and 100 nm), titanium oxide (TiO<sub>2</sub>), or culture dish (Cd). The expression of miR-488 was measured at day 2. RQ of cells on culture dish (Cd) was used as a control to measure fold change. (b) MC3T3-E1 cells were cultured with antisense oligonucleotides of miR-488 (anti-miR-488) or a scrambled PNA-based ASO (Con). ALP expression was measured using real-time PCR and cell adhesion was assayed. RQ of control cells on culture dish (Cd) was used as a control to measure fold change. (c) MC3T3-E1 cells were cultured on titanium oxide nanotube having various diameters (30, 50, 70, and 100 nm), titanium oxide (TiO<sub>2</sub>), or culture dish (Cd) and treated with antisense oligonucleotides of miR-488 (anti-miR-488) or a scrambled PNA-based ASO (Sc). ALP expression was measured using real-time PCR. RQ of cells treated with Sc was used as a control to measure fold change. Representative data is shown ( $n = 4$ ). The mean is plotted and the error bars represent 95% CI (lower/upper limit). \* $P < 0.005$ .

that a TiO<sub>2</sub> nanotube layer (70 nm diameter) significantly enhanced osteogenesis-related gene expression, bone implant contact, and bone deposition on pure titanium implants, indicating that 70 nm diameter nanotubes are the optimum size for osseointegration. Here, we found that the expression levels of the osteoblast-differentiation-related transcription factor-encoding genes, *ALP*, *sp7*, and *Dlx5*, were significantly increased on TiO<sub>2</sub> nanotubes compared to culture dishes;

these levels peaked in cells grown on 50 nm nanotubes and then decreased slightly with increasing tube diameter (Figure 2(a)). The density of stress fibers was also highest in cells grown on 50 nm nanotubes (Figure 2(b)). The adhesion of cells was not affected by the nanotube diameter (data not shown).

The expression level of miR-488 was significantly higher in cells grown on 50 nm nanotubes (but not those of



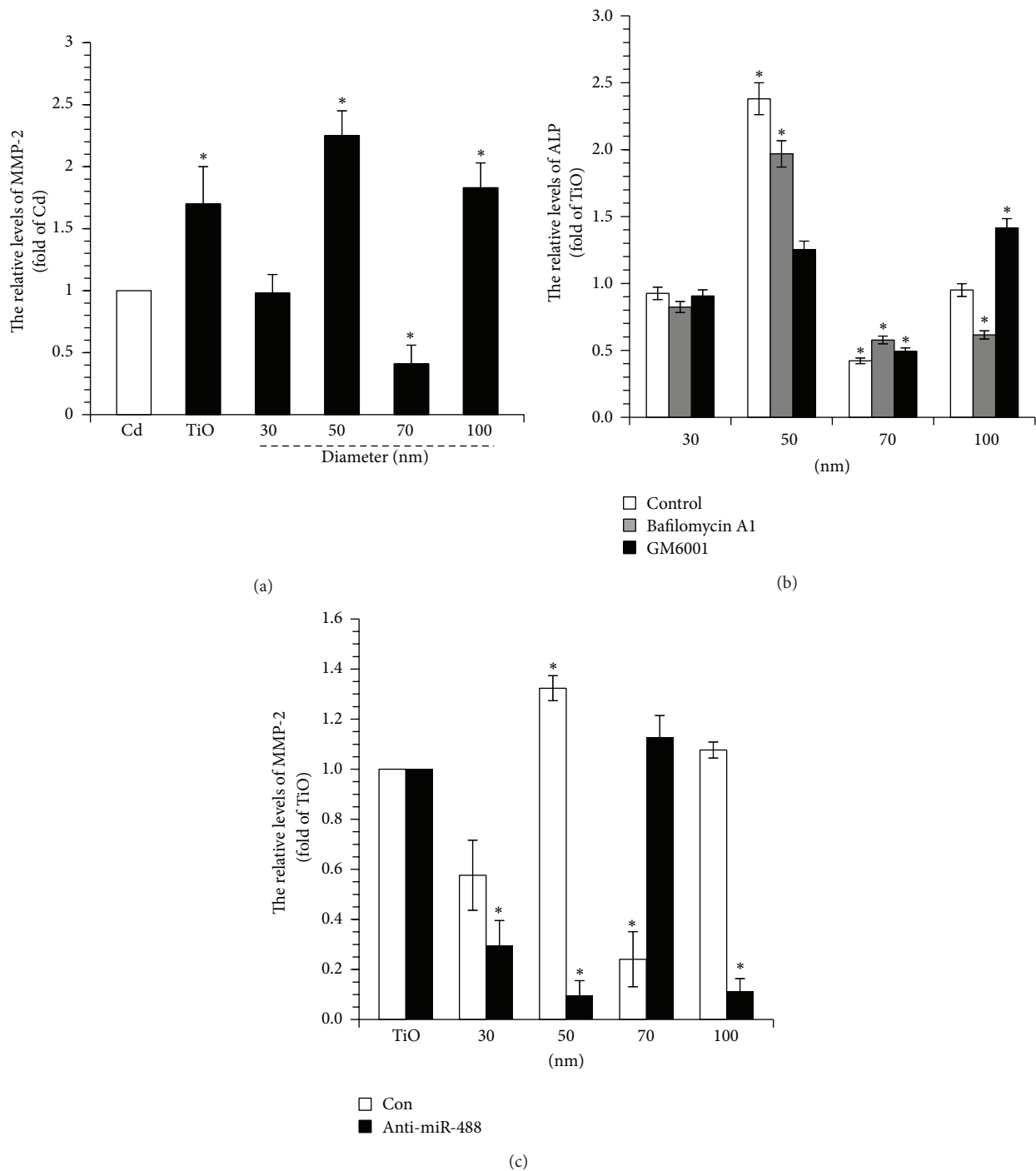


FIGURE 4: MMP-2 modulation by miR-448 affects osteoblastic differentiation of MC3T3-E1 cells on TiO<sub>2</sub> nanotube surface. (a) MC3T3-E1 cells were cultured on titanium oxide nanotube having various diameters (30, 50, 70, and 100 nm), titanium oxide (TiO<sub>2</sub>), or culture dish (Cd) and the expression of MMP-2 was measured using real-time PCR. RQ of cells on culture dish (Cd) was used as a control to measure fold change. (b) MC3T3-E1 cells were treated with bafilomycin A1 or GM6001 and the expression of ALP was measured using real-time PCR. RQ of cells on flat titanium oxide was used as a control to measure fold change. (c) MC3T3-E1 cells were cultured on titanium nanotube having various diameters (30, 50, 70, and 100 nm) and treated with antisense oligonucleotides of miR-488 (anti-miR-488) or a scrambled PNA-based ASO (Con). Expression of *MMP-2* was measured. RQ of cells on flat titanium oxide was used as a control to measure fold change. Representative data is shown ( $n = 4$ ). The mean is plotted and the error bars represent 95% CI (lower/upper limit). \*  $P < 0.005$ .

other diameters) versus those grown on culture dishes (Figure 3(a)). Interestingly, cells treated with the anti-miR-488 oligonucleotide inhibitor acted differently on plastic polypyrrene versus TiO<sub>2</sub> surfaces: the inhibitor induced *ALP* transcription in cells grown on culture dishes but slightly reduced *ALP* transcription in cells grown on TiO<sub>2</sub> (Figure 3(b)). Notably, the anti-miR-488 inhibitor suppressed the transcription of *ALP* to the greatest degree in cells plated on 50 nm TiO<sub>2</sub> nanotubes (Figure 3(c)). These data suggest that the nature of the substratum could affect the internal environment and modulate the differential capacity of osteoblasts.

Under normal physiological conditions, osteoblasts are able to degrade the organic material of the bone matrix. Osteoblast precursors express MMP-2, -8, -13, and -14, which may be involved in the degradation of bone matrix materials (e.g., type I collagen) [23]. Consistent with this observation, we found that when the miR-488 inhibitor induced the differentiation of MC3T3-E1 cells (Figure 1(a)), the induction of MMP-2 was also increased (Figure 4(a)). However, material properties such as surface chemistry and surface topography are well known to affect cellular behavior, thereby affecting cell fate [24]. Here, we found that, among cells cultured on TiO<sub>2</sub> surfaces of various diameters, MMP-2 expression and *ALP* activity were significantly increased on 50 nm nanotubes (Figure 2(a)). In addition, we found that modulation of MMP-2 activity could affect *ALP* activity in our system. Bafilomycin A1 is known to increase the activation of proMMP-2 by the abundance of active MT1-MMP on the cell surface [25, 26]. Here, we found that bafilomycin A1 treatment increased *ALP* activity in cells grown on 50 nm nanotubes. In contrast, treatment of cells with 3 μM GM6001, which has been shown to inhibit MMP-2 activity [27, 28], decreased *ALP* activity among cells grown on various-diameter nanotubes (Figure 4(b)). These data support the notion that material properties can affect cellular behaviors and responses. Interestingly, the miR-488 inhibitor had differential effects on MMP-2 expression depending on the growth substrate: it inhibited MMP-2 expression in cells grown on 50 nm nanotubes but significantly enhanced MMP-2 expression in cells grown on 70 nm nanotubes (Figure 4(c)).

These data collectively suggest that biophysical stimuli and environmental conditions could be important factors in the clinical use of TiO<sub>2</sub> nanotubes. Recent studies have shown that miR-488 is involved in several diseases, including prostate cancer [29], lung cancer [23], and panic disorder [30]. For clinical applications of TiO<sub>2</sub> nanotubes, it may therefore be necessary to investigate the relationship between the desired implant material and certain patient characteristics (e.g., miR-488 levels).

#### 4. Conclusions

One of the biggest challenges in developing implants with improved longevity and minimum failure is the control of successful osseointegration. Osteoblasts are critical for the osseointegration of endosseous implants because they synthesize/produce ECM and control its mineralization. Here,

we explored differences in the osteogenic responses of cells grown on 30 nm, 50 nm, 70 nm, and 100 nm TiO<sub>2</sub> nanotubes. We found that the 50 nm diameter yielded the best osteoblast differentiation (as assessed by *ALP* expression) and could therefore be optimal for implant use. However, we also obtained evidence suggesting that biophysical stimuli and endogenous environmental conditions could also critically affect the behavior of osteoblasts. We found that modulation of miR-488 had different effects on cells depending on their growth substrate (i.e., culture dishes or TiO<sub>2</sub> nanotubes of various diameters). These findings suggest that we need to fully understand the interactions of endogenous biological parameters (e.g., miRNAs) and the physicochemical properties of Ti nanotubes in order to optimize the clinical application of such materials in implant medicine.

#### Abbreviations

ALP:	Alkaline phosphatase
MMP-2:	Matrix metalloprotease-2
miRNA, miR:	MicroRNA
TiO <sub>2</sub> :	Titanium oxide
ECM:	Extracellular matrix.

#### Conflict of Interests

The authors declare that there is no conflict of interests regarding the publication of this paper.

#### Authors' Contribution

Yeon-Ho Kang and Bohm Choi contributed equally in this study.

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