



## Second World Conference on Nanomedicine and Drug Delivery

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# BIOMEDICAL AND RELATED APPLICATIONS OF SECOND GENERATION POLYAMIDOAMINES

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# BIOMEDICAL AND RELATED APPLICATIONS OF SECOND GENERATION POLYAMIDOAMINES

## CONTENT:

1. Synthesis and properties of PAAs
2. PAAs as cytoplasmic delivery vehicles of immunotoxines
3. PAA-cholesterol nanoparticles
4. PAA- $\beta$ -Cyclodextrin nanoparticles
5. Conclusions

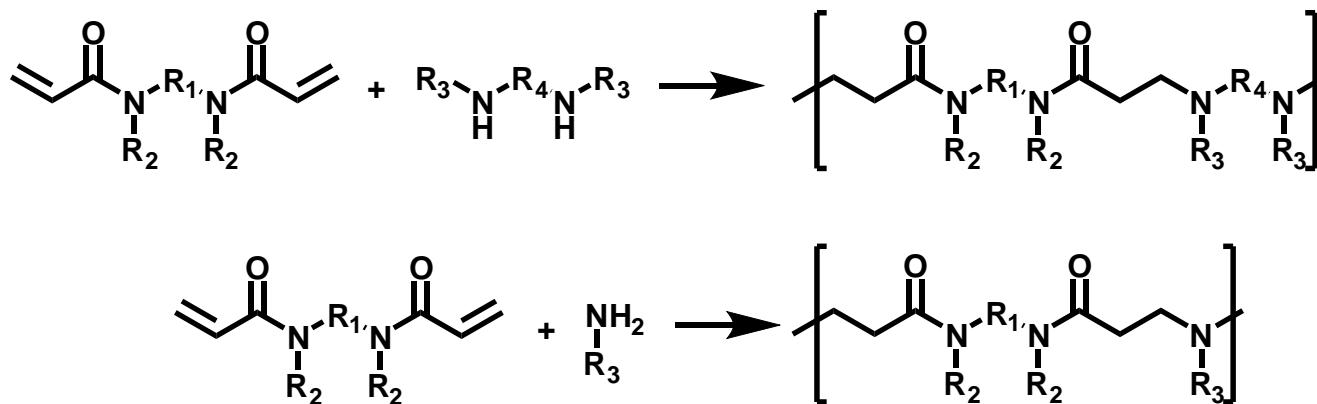


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# PAAs: INTRODUCTION



Poly(amine amide)s (PAA) are synthetic polymers containing tert-amine and amide groups regularly arranged along their polymer chain. They are prepared by Michael-type polyaddition of amines to bisacrylamides.

- Synthetic conditions:
- room temperature, N<sub>2</sub> atmosphere, 3 days;
  - no catalysts;
  - protic solvents (water, alcohols).



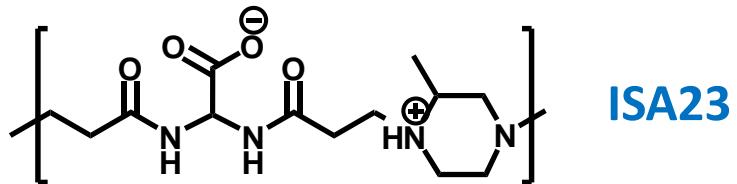
# PROPERTIES OF PAAs

- ✓ PAAs are usually water soluble;
- ✓ PAAs are polymeric bases of low to medium strength;
- ✓ PAAs are biocompatible, biodegradable and non-toxic;
- ✓ Easily functionalized with several different functional groups;
- ✓ Amphoteric PAAs show stealth properties and EPR effect.



## PAA name and structure

	$pK_a$	I.P.	Percentage of Charged Units
			$pH=5.5 \quad pH=7.4$



ISA23

$pK_{a1}=2.1$   
 $pK_{a2}=3.25$   
 $pK_{a3}=7.5$

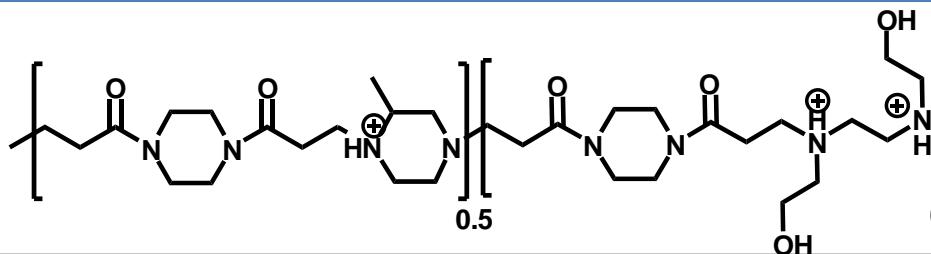
5.5

40%

(-)

2%

(-)



ISA1

$pK_{a1}=8.1$   
 $pK_{a2}=6.9$   
 $pK_{a3}=3.8$   
 $pK_{a4}=2.8$

>10

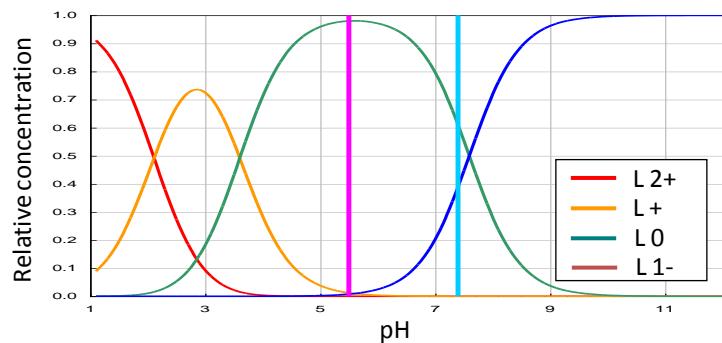
95%

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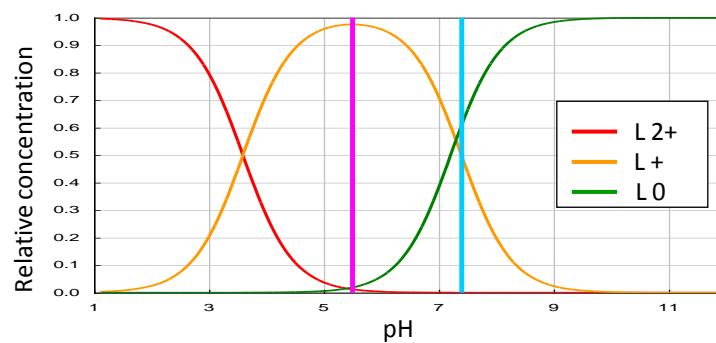
55%

(+)

ISA23



ISA1



Ferruti, P.; Manzoni, S.; Richardson, S.C.W.; Duncan, R.; Patrick, N.G.; Mendichi, R.; Casolaro, M. *Macromolecules* **2000**, 33, 7793-7800.

Franchini, J.; Ranucci, E.; Ferruti, P.; Rossi, M.; Cavalli, R. *Biomacromolecules* **2006**, 7 (4), 1215-1222.

Ranucci, E.; Ferruti, P.; Lattanzio, E.; Manfredi, M.; Rossi, M.; Mussini, P.R.; Chiellini, F.; Bartoli C. *Journal of Polymer Science: Part A: Polymer Chemistry* **2009**, 4, 6977.



# TOXICITY OF PAAs

Sample	$\overline{M_n}$	$IC_{50}$ (mg/mL) on B16F10 cells
ISA23	21500	> 5.00
ISA1	9500	3.05 ± 0.70
POLY-L-LYSINE	56500	0.05 ± 0.01
DEXTRAN	70000	> 5.00

Cytotoxicity test on B16F10 cell line.

Sample	$\overline{M_n}$	$IC_{50}$ (mg/mL) on Balb/3T3 Clone A31
ISA23	20300	> 5.00
ISA1	14500	2.17 ± 0.75
POLY-L-LYSINE	56500	0.05 ± 0.01
DEXTRAN	70000	> 5.00

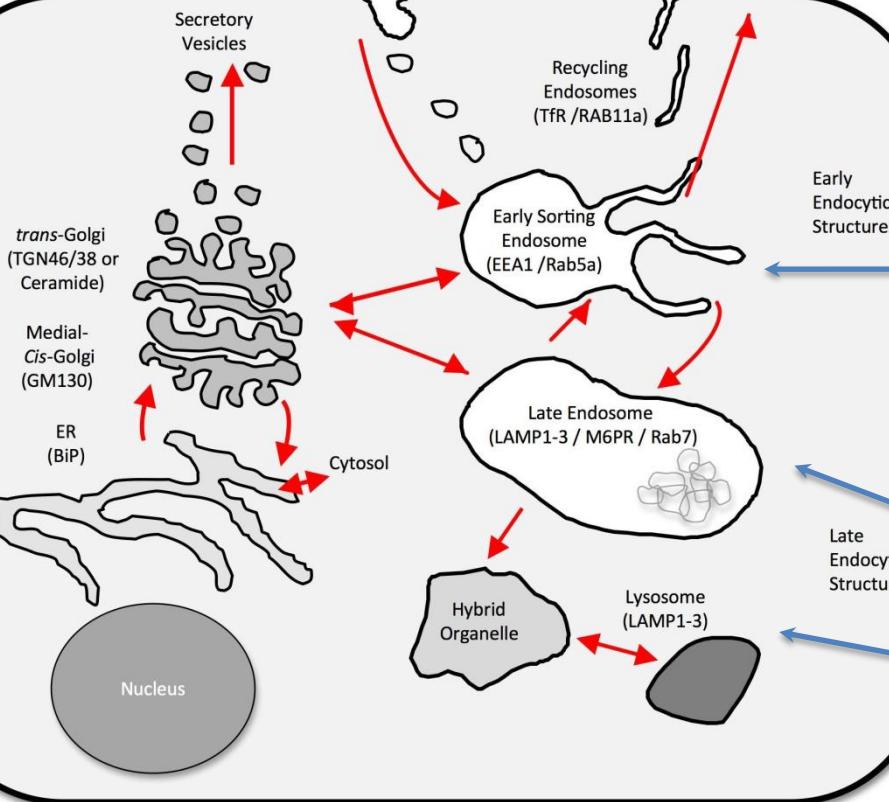
Cytotoxicity test on mouse embryo fibroblasts Balb/3T3 Clone A31 cell line.



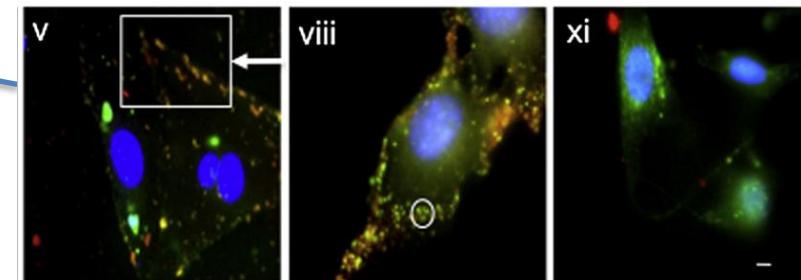
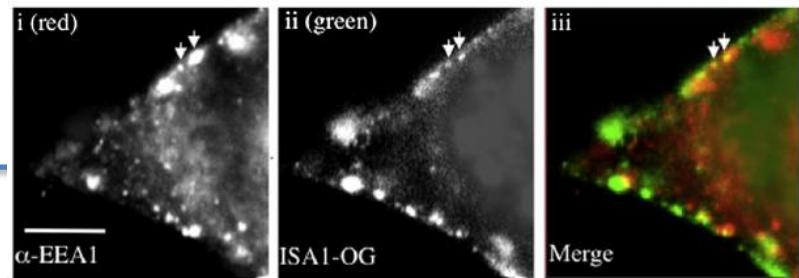
# INTRACELLULAR TRAFFICKING PAAs

Secretory pathway

Endocytic pathway



Co-localization of ISA1 with EEA1



Co-localization of ISA1 and ISA23 with lysotracker



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# PAAS AS CYTOPLASMIC DELIVERY VEHICLES OF IMMUNOTOXINES

The development and successful application of therapeutic proteins is often hindered by several difficulties, as for instance insufficient stability and shelf-life, costly production, immunogenic and allergic potential, as well as poor bioavailability and sensitivity towards proteases.

To overcome these problems, a possible approach is to **modify proteins by covalently conjugating them with water-soluble polymers**, thus increasing their plasma residence, reducing protein immunogenicity and increasing their therapeutic index.

Duncan, R. *Nat. Rev. Drug Discov.* **2003**, 2, 214-221.

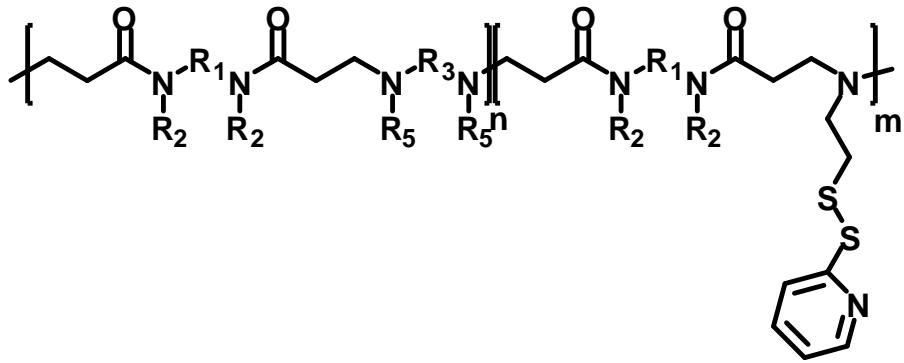
Duncan, R. *Nature Review* **2006**, 6, 688-701.



Increasing attention has been devoted to the nature of the chemical linkage between the polymer backbone and protein.

In this work, two PAAs bearing 2-ethenylidithiopyridine pendants were used to investigate their ability to mediate intracellular delivery of the ribosome-inactivating gelonin.

PAA-SSPy



GELONIN



Ribosome-inactivating protein.

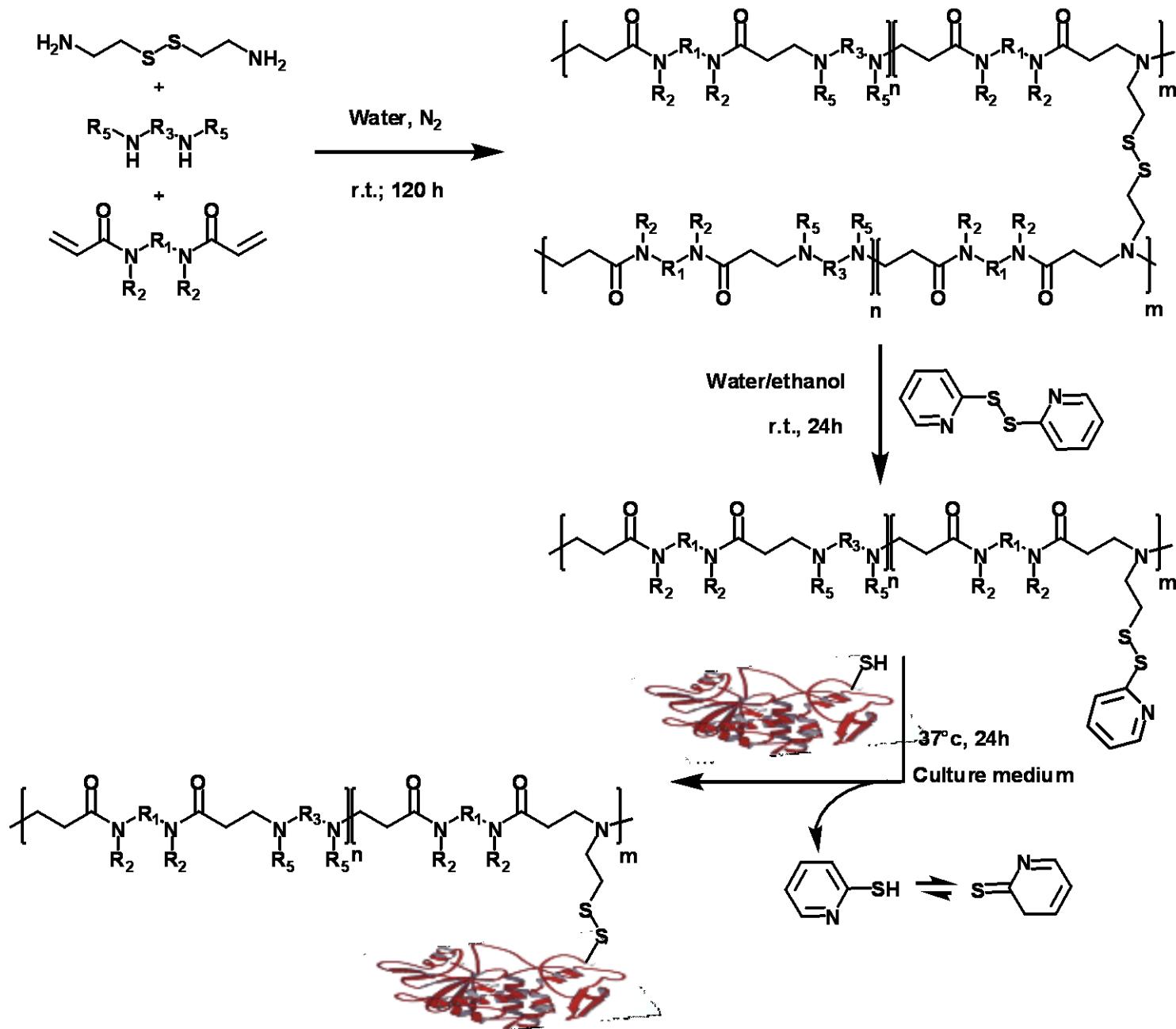
It doesn't contain the cell-binding subunit that promotes its internalization by endocytosis.

Emilitri, E.; Ranucci, E.; Ferruti, P. *J. Polym. Sci., Part A: Polym. Chem.* **2005**, *43*, 1404.

Ranucci, E.; Ferruti, P.; Suardi, M.A.; Manfredi, A. *Macromol. Rapid Commun.* **2007**, *28*, 1243-1250.

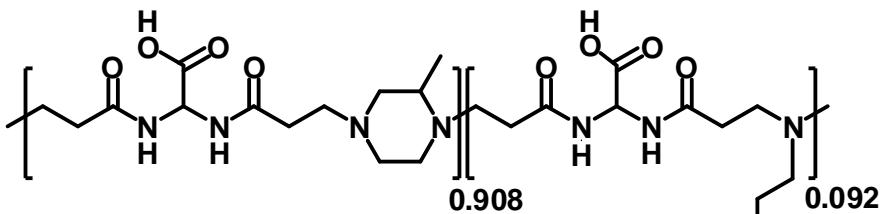


# PAAS AS CYTOPLASMIC DELIVERY VEHICLES OF IMMUNOTOXINES

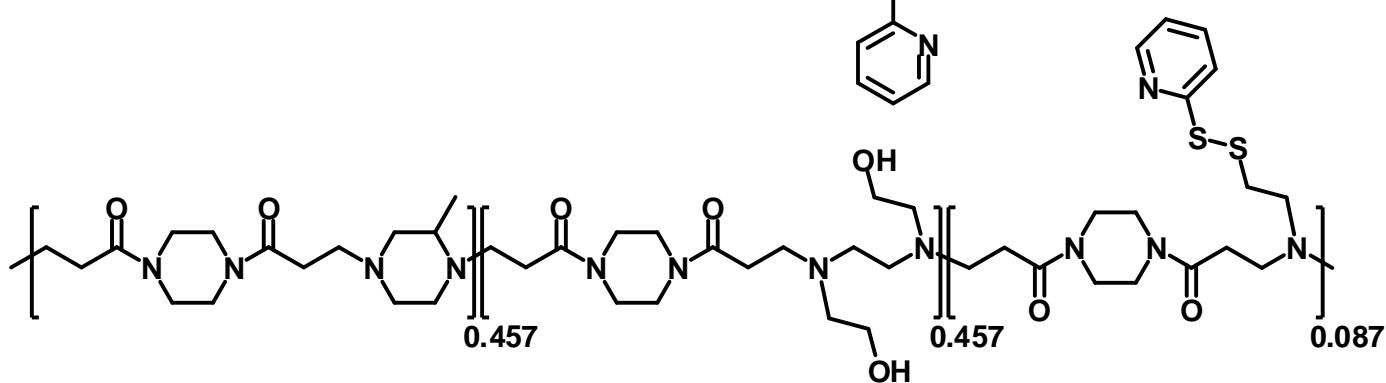


# PAAs AS CYTOPLASMIC DELIVERY VEHICLES OF IMMUNOTOXINES

**ISA23-SSPy**



**ISA1-SSPy**



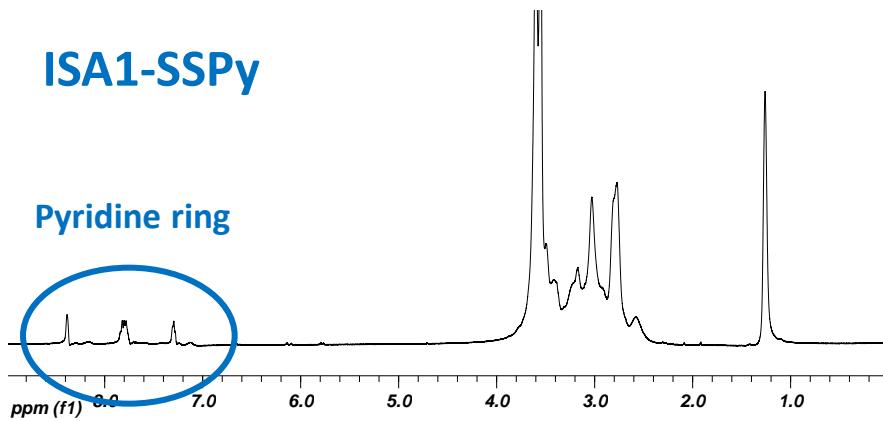
**GPC-LS**

**NMR Spectroscopy**

Sample	$\overline{M_n}$	$\overline{M_w}$	PD	% of functions
ISA1	18000	30000	1.93	8.67
ISA23	12700	23600	1.86	9.2

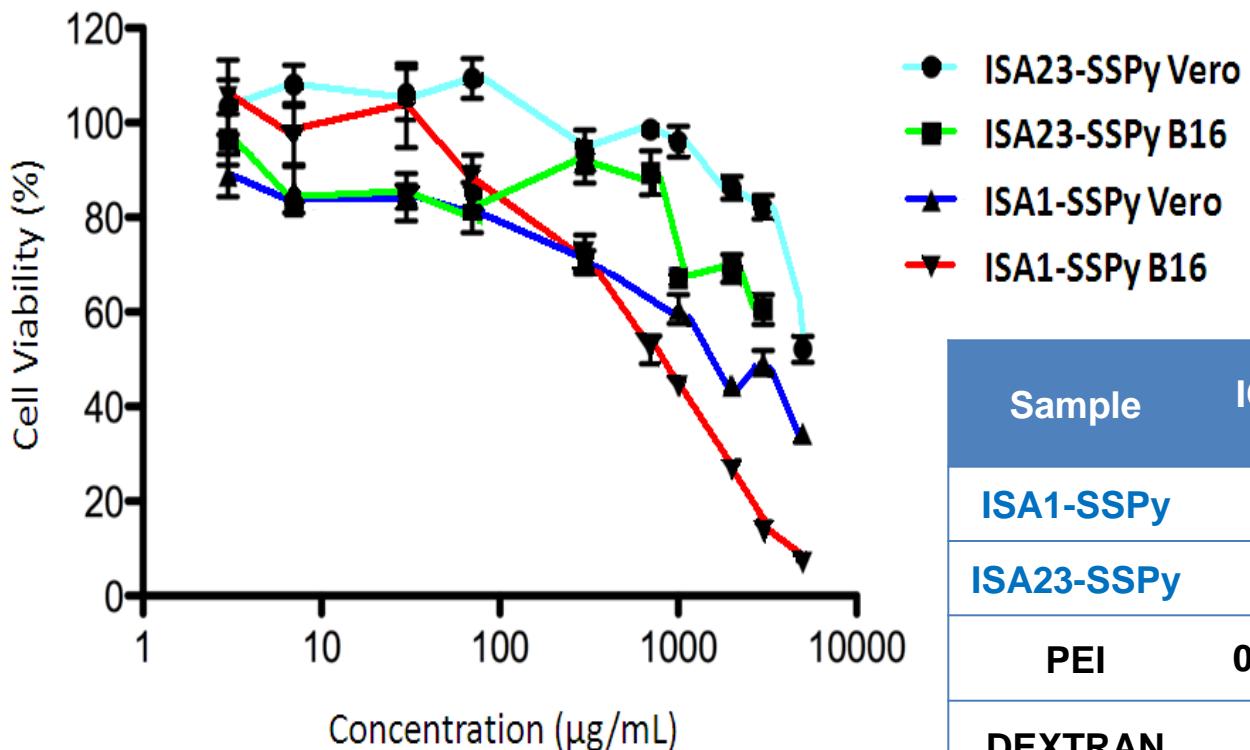
**ISA1-SSPy**

**Pyridine ring**



# PAA-SSPy CYTOTOXICITY

ISA1-SSPy and ISA23-SSPy were tested by direct contact assay for 72 hours using B16F10 and Vero cells.



Sample	$\text{IC}_{50}$ (mg/mL) on B16F10 cells	$\text{IC}_{50}$ (mg/mL) on VERO cells
ISA1-SSPy	2.5	1.5
ISA23-SSPy	> 5.00	5.00
PEI	$0.04 \pm 0.01$	$0.05 \pm 0.01$
DEXTRAN	> 5.00	> 5.00



## SUB-CLONING OF GELONIN

PAA-SSPy polymers were used to prepare PAA-gelonin complexes in which the polymeric chain was linked to the bioactive moieties by a disulfide bridge.

To achieve this aim, two types of gelonin were sub-cloned:

6H-V5-Gelonin

90    6H    V5    Gelonin    86

Gelonin-HA-Cys-6H

87    Gelonin    HA    6H    89

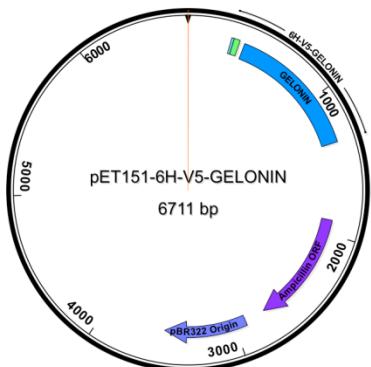
Plasmids encoding both the two protein were made by sub-cloning an open reading frame coding for gelonin into a commercially available bacterial expression cassette (pET151/D Topo).

Protein were expressed using BL21(DE3) Competent E. Coli.

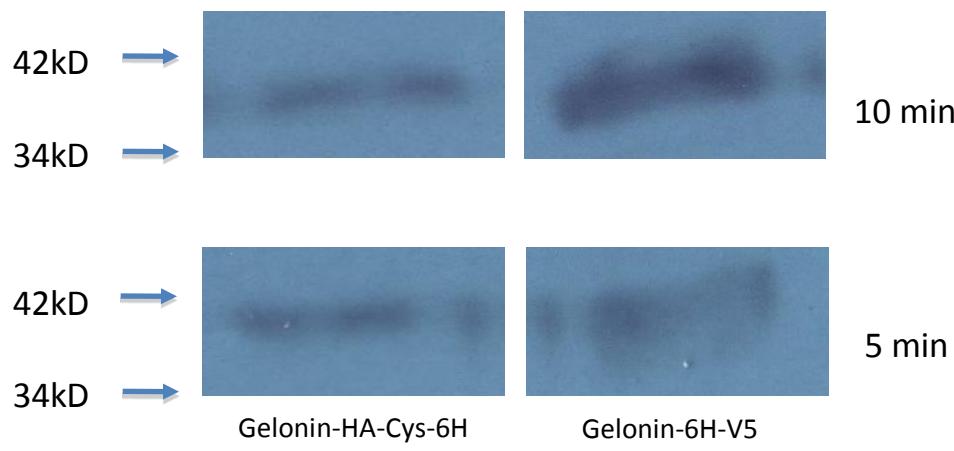


# PAAS AS CYTOPLASMIC DELIVERY VEHICLES OF IMMUNOTOXINES

## 6H-V5-Gelonin



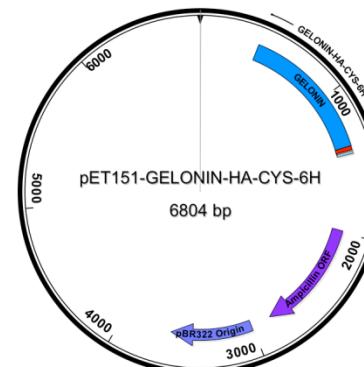
90    6H    V5    Gelonin    86



1:1000 6XHis Monoclonal Antibody

1:500 Anti-mouse Ig, horseradish whole antibody

## Gelonin-HA-Cys-6H



87    Gelonin    HA    6H    89

### Gelonin-HA-Cys-6H

```
MKGNMKVYWKIAVATWFCCCTIVL
GSTARIFSLPTNDEEETSKTLGLDTVS
FSTKGATYITYVNFLNELRVKLKPEG
NSHGIPLLRKKCDDPGKCFVLVALSN
DNGQLAIEIAIDVTSVVVGYQVRNR
SYFFKDAPDAAYEGLFKNTIKTRLHF
GGSYPSLEGEKAYRETTDLGIEPLRIGI
KKLDENAIIDNYKPTEIASSLLVIQM
VSEAARFTIENQIRNNFQQIRPAN
NTISLENKWGKLSFQIRTSGANGMF
SEAVELERANGKYYVTAVDQVKPKI
ALLKFVDKDPKTSAAELIIQNYESLV
GFDESLVGFDPYDVPDYARCAHHH
HHH.
```

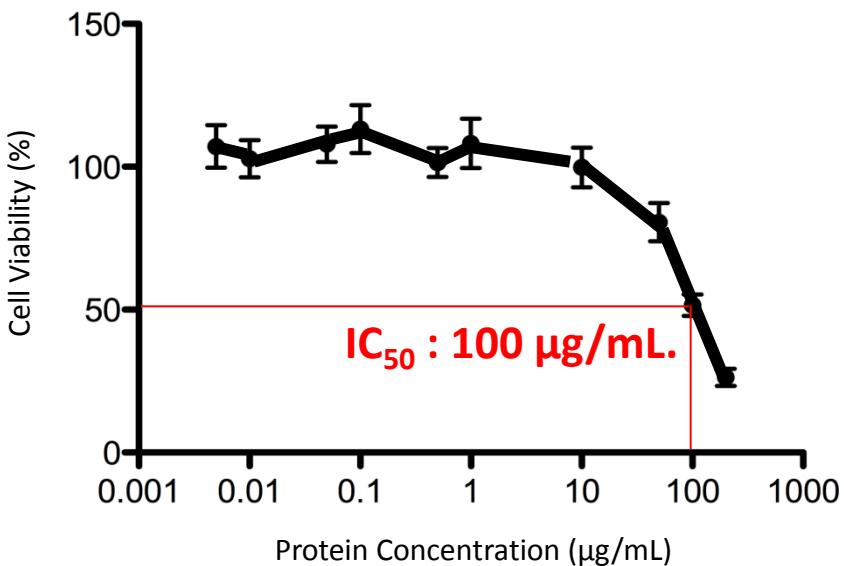
### 6H-V5-Gelonin

```
MHHHHHHGKIPNPLLGLDSTENLYF
QGIDPFTMKGNMKVYWKIAVATWFC
CTTIVLGSTARIFSLPTNDEEETSKTL
DTVSFSTKGATYITYVNFLNELRVKLKPE
GNSHGIPLLRKKCDDPGKCFVLVALSN
DNGQLAIEIAIDVTSVVVGYQVRNRSY
FFKDAPDAAYEGLFKNTIKTRLHFGGSY
PSLEGEKAYRETTDLGIEPLRIGIKKLDE
NAIDNYKPTEIASSLLVIQMVSEAARF
TFIENQIRNNFQQIRPANNTISLENK
WGKLSFQIRTSGANGMFSEAVELERA
NGKKYYVTAVDQVKPKIALLKFVDKDP
KTSLAAELIIQNYESLVGFD
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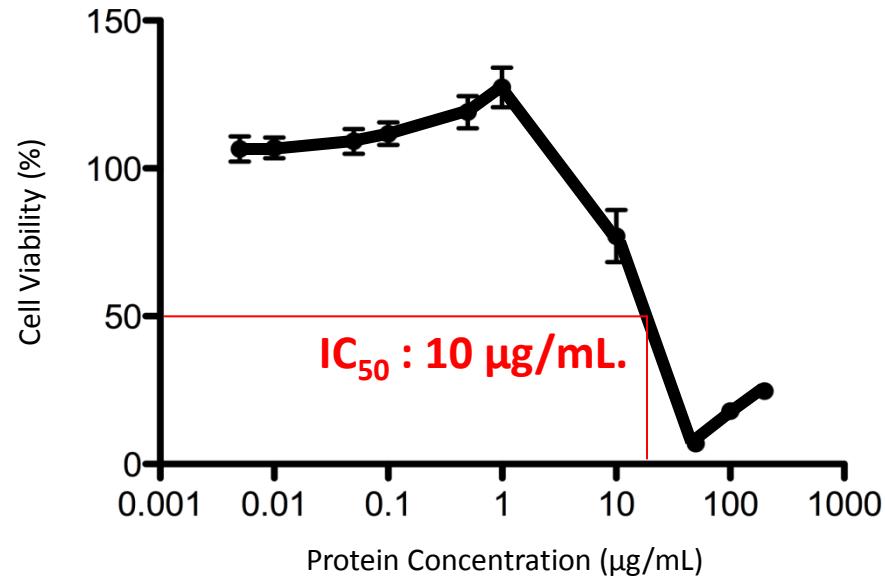


# GELONIN TOXICITY

## Gelonin-HA-Cys-6H



## 6H-V5-Gelonin



In all further experiments, non toxic concentrations of 6H-V5 Gelonin and Gelonin HA-Cys-6H were used.

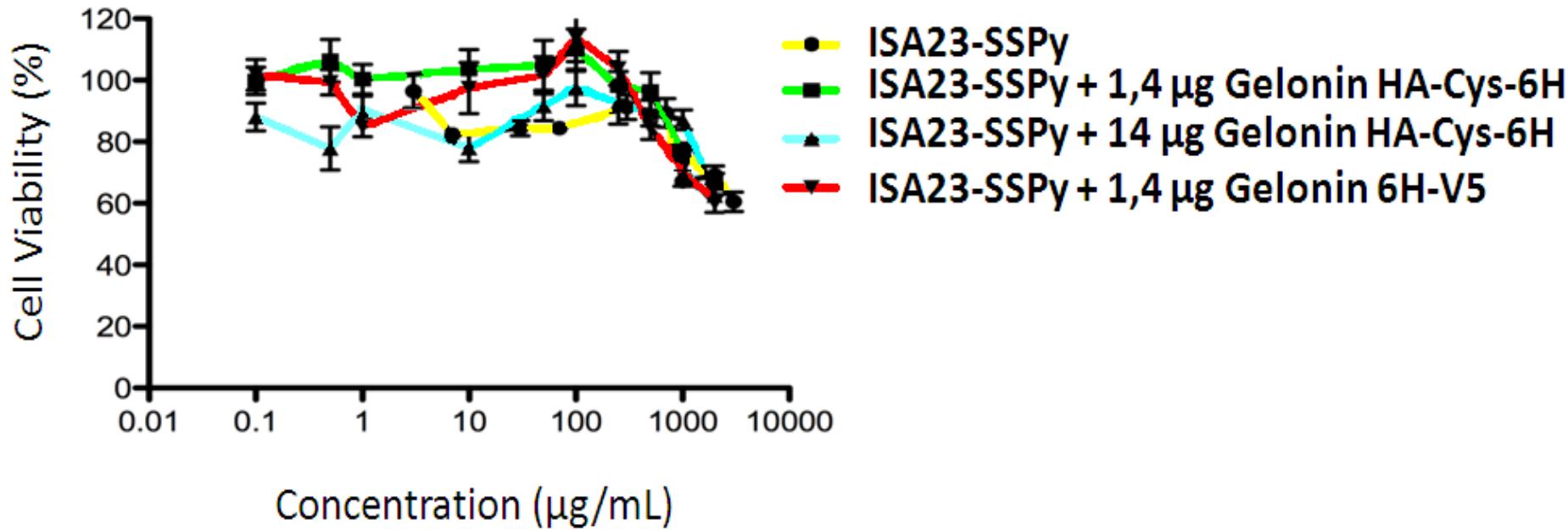
1.4  $\mu\text{g/mL}$

14  $\mu\text{g/mL}$

1.4  $\mu\text{g/mL}$

# ISA23-SS-GELONIN CONJUGATES: TOXICITY

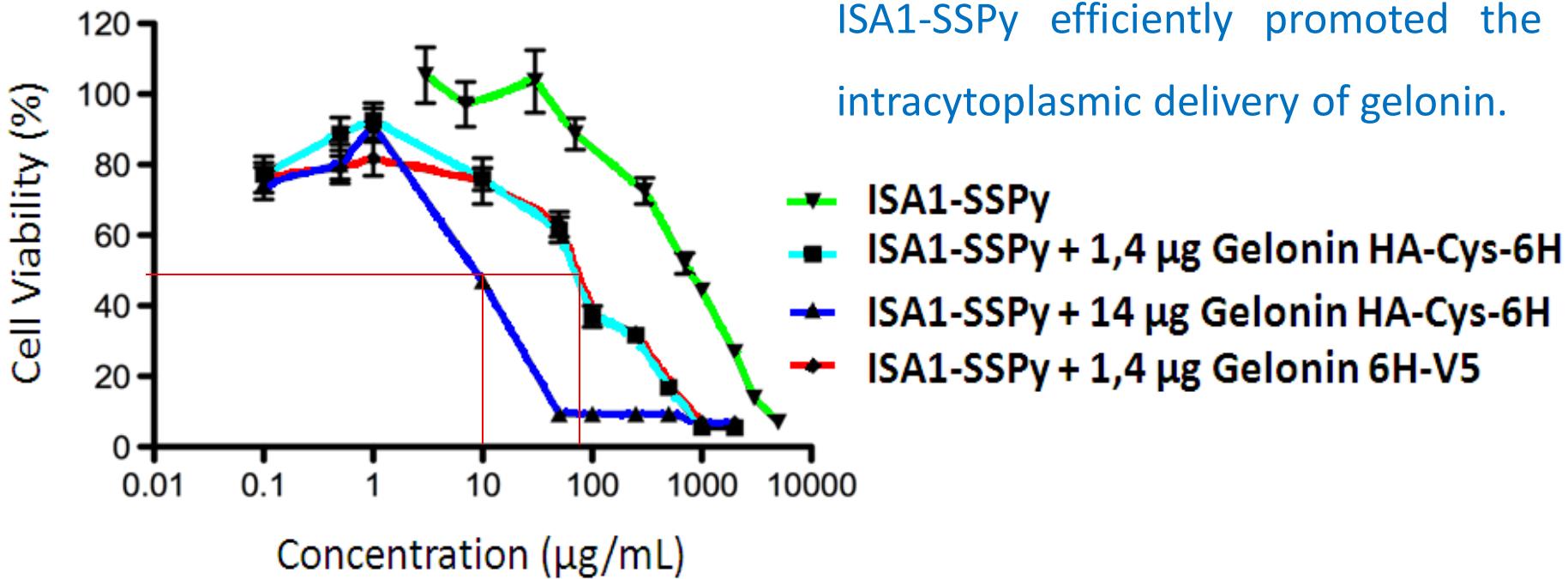
Cytotoxicity experiments were performed using fixed concentration of protein and polymer concentrations up to 2 mg/mL on B16F10 cells.



ISA23-SSPy was unable to mediate toxin delivery in  
the B16F10 cells.



# ISA1-SS-GELONIN CONJUGATES: TOXICITY



ISA1-SSPy-6H-V5 Gelonin  $\rightarrow \text{IC}_{50} : 100 \mu\text{g/mL}$

ISA1-SSPy-Gelonin HA-Cys-V5  $\rightarrow \text{IC}_{50} : 100 \mu\text{g/mL}$

ISA1-SSPy-Gelonin HA-Cys-6H (14  $\mu\text{g/mL}$ )  $\text{IC}_{50} : 10 \mu\text{g/mL}$



S.C.W. Richardson et al. *Journal of Controlled Release* 2001, 77, 225–232



Journal of Controlled Release 77 (2001) 225–232



## Poly(amidoamine)-mediated intracytoplasmic delivery of ricin A-chain and gelonin

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<sup>b</sup>Dipartimento di Scienze e Tecnologie Chimiche e dei Materiali, Università di Bari, Piazza del Monte di Pietà 46, 70139 Bari, Italy

Received 15 May 2001; accepted 7 September 2001

### Abstract

Poly(amidoamine)s (PAs) are water-soluble synthetic polymers designed to be biodegradable and biocompatible. Moreover, they display membrane disruptive properties in response to a decrease in pH. This attribute confers PAAs with endoescytotic properties *in vitro* and *in vivo*. A model system was developed to quantify their ability to promote the endosomal escape of macromolecules that may be interesting as therapeutic agents. Here, two PAAs (ISA 1 and 4) were incubated with B16F10 cells *in vitro* together with two non-persistent toxins: either ricin A-chain (RTA) or gelonin. The relatively non-toxic PAAs ISA 1 and 4 ( $IC_{50}>1.5$  mg/ml) restored activity to the inherently inert toxins. The  $IC_{50}$  values for the ISA 1/RTA and ISA 1/gelonin combinations were  $0.65\pm 0.05$  and  $0.55\pm 0.12$  mg/ml, respectively. Similarly, when ISA 4 was incubated with a non-toxic combination of RTA and gelonin the  $IC_{50}$  value decreased to  $0.37\pm 0.03$  and  $0.41\pm 0.26$  mg/ml, respectively. In contrast, the neutral polymer dextran and the PAA ISA 22 were unable to mediate this effect. These observations suggest that specific PAA-toxin combinations warrant further development as novel therapeutics. © 2001 Elsevier Science BV. All rights reserved.

**Keywords:** Ricin; Gelonin; Poly(amidoamine); Non-viral vector; Cytosolic delivery

### 1. Introduction

Poly(amidoamine)s (PAAs) have been developed as biomedical materials and water soluble drug carriers, as reviewed in Refs. [1–3]. This family of polymers is currently being developed as a synthetic alternative to fusogenic peptides as they display pH-dependent conformational changes upon protonation at reduced pH which leads to membrane per-

turbation [4–6]. This property has been shown to confer PAAs with the capacity to promote transfection of pSV-β-galactosidase [6]. Furthermore, PAAs can be designed to be biodegradable, biocompatible and non-hepatotoxic [5,7] suggesting their potential for a wide range of *in vivo* applications.

Plant and bacterial toxins have been widely explored as anticancer agents, particularly in the form of immunotoxins (reviewed in Ref. [8]). Therefore, here we chose to investigate the ability of PAAs to mediate intracellular delivery of two ribosome-inactivating toxins, ricin and gelonin. Ricin, derived from *Ricinus communis* beans [9], is a highly cytotoxic

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E-mail address: duncan@fca.ac.uk (R. Duncan).

ISA1-SSPy promoted the intracytoplasmic delivery of gelonin more efficiently than the parent ISA1

ISA1-Gelonin



$IC_{50} : 522 \mu\text{g/mL}$ .

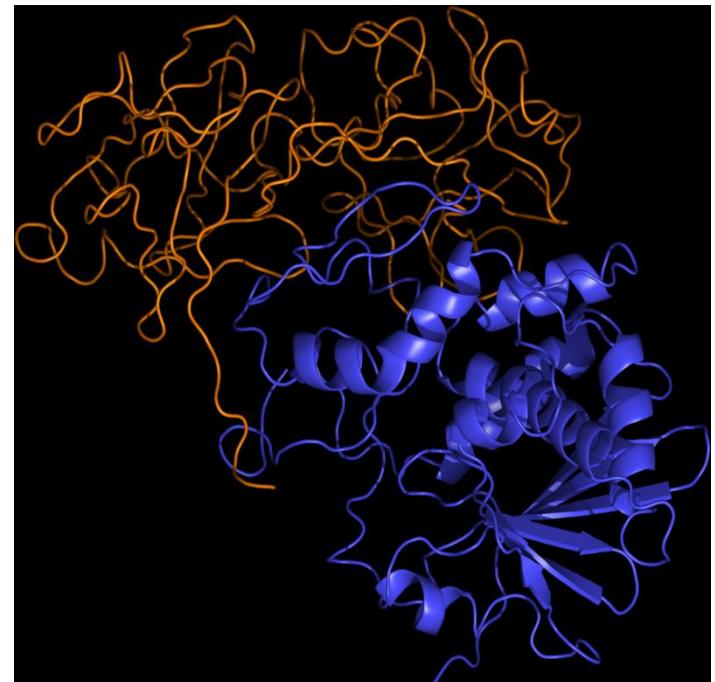


ISA1-SSPy-HA-Cys-6H and ISA1-SSPy-6H-V5 Gelonin showed same results ( $IC_{50}$ :100  $\mu$ g/mL).

ISA1-SSPy is able to interact with disulfide groups and hydrophobic domains of the protein, giving stable complexes.

Ricin structure. The **A** chain (RIP) is shown in blue and the **B** chain (cell binding sub-unit) in orange.

ISA1-SSPy acts as synthetic mimicking of the cell binding sub-unit of the Ricin toxin that mediates the internalization of gelonin into the cytosol.



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# PAA-CHOLESTEROL NANOPARTICLES

Improvement in drug controlled release is one of the main challenges of modern pharmacology in order to reduce side effects of therapies and to exploit drug potential:

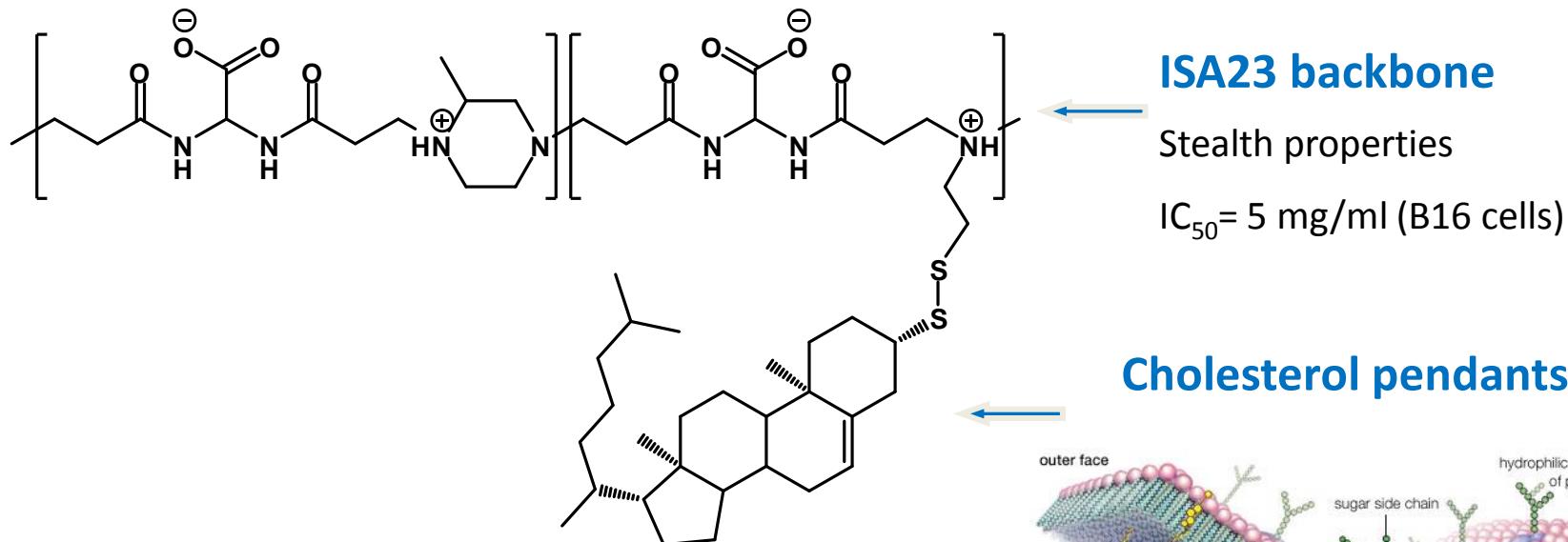
- ✓ “Solubilization” of lipophilic drugs;
- ✓ Specific targeting and release of drugs;
- ✓ Sustained release of soluble/insoluble drugs;
- ✓ Protection of proteins or genes in transfection.

The use of polymers in designing new drugs architectures, most often in the form of nanoparticles (NP) is one of the most promising possibilities to achieve these goals.

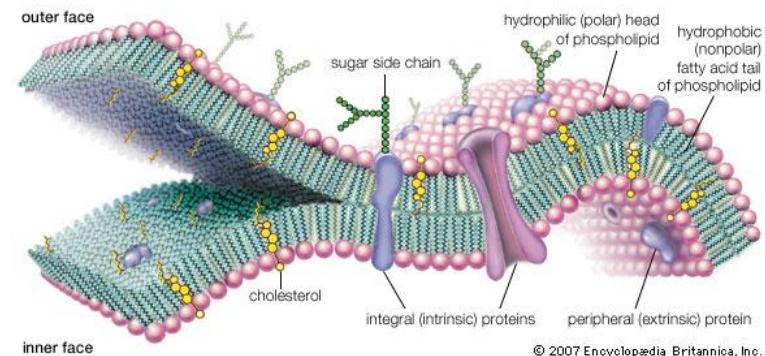


# PAA-CHOLESTEROL NANOPARTICLES

Using the PAA-SSPy precursors already shown, a family of amphoteric polymers containing cholesterol pendants linked through disulfide bonds was synthesized.



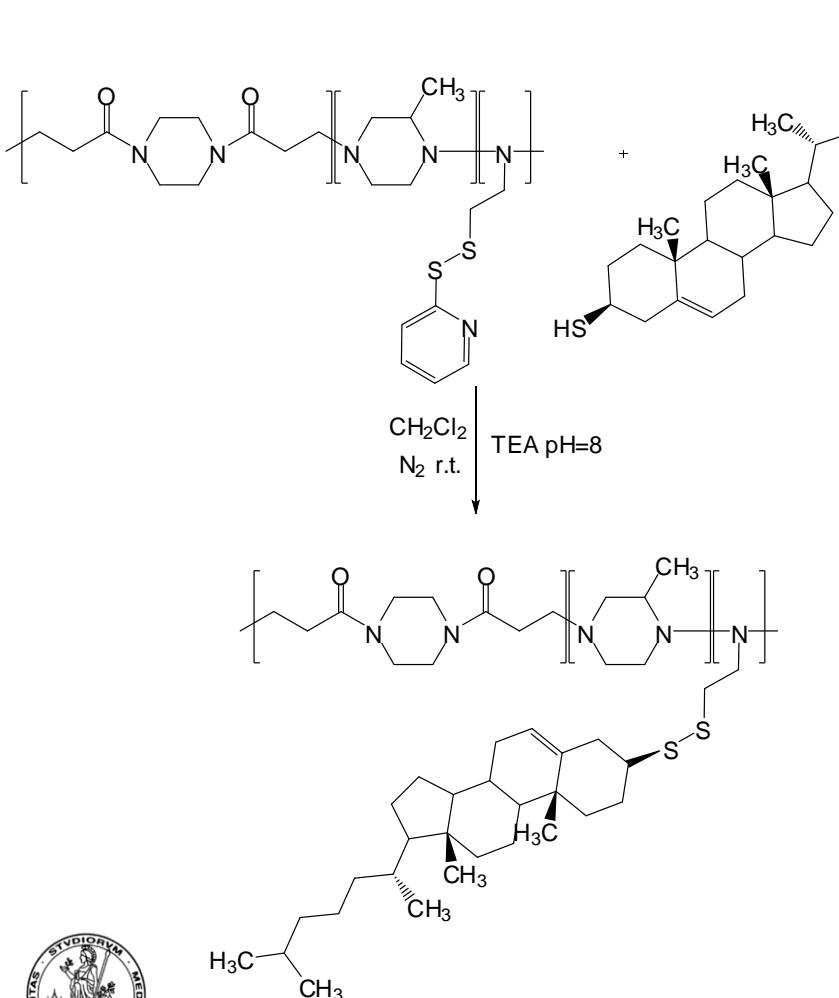
Cholesterol is an essential structural component of mammalian cell membranes, where it is required to establish proper membrane permeability and fluidity.



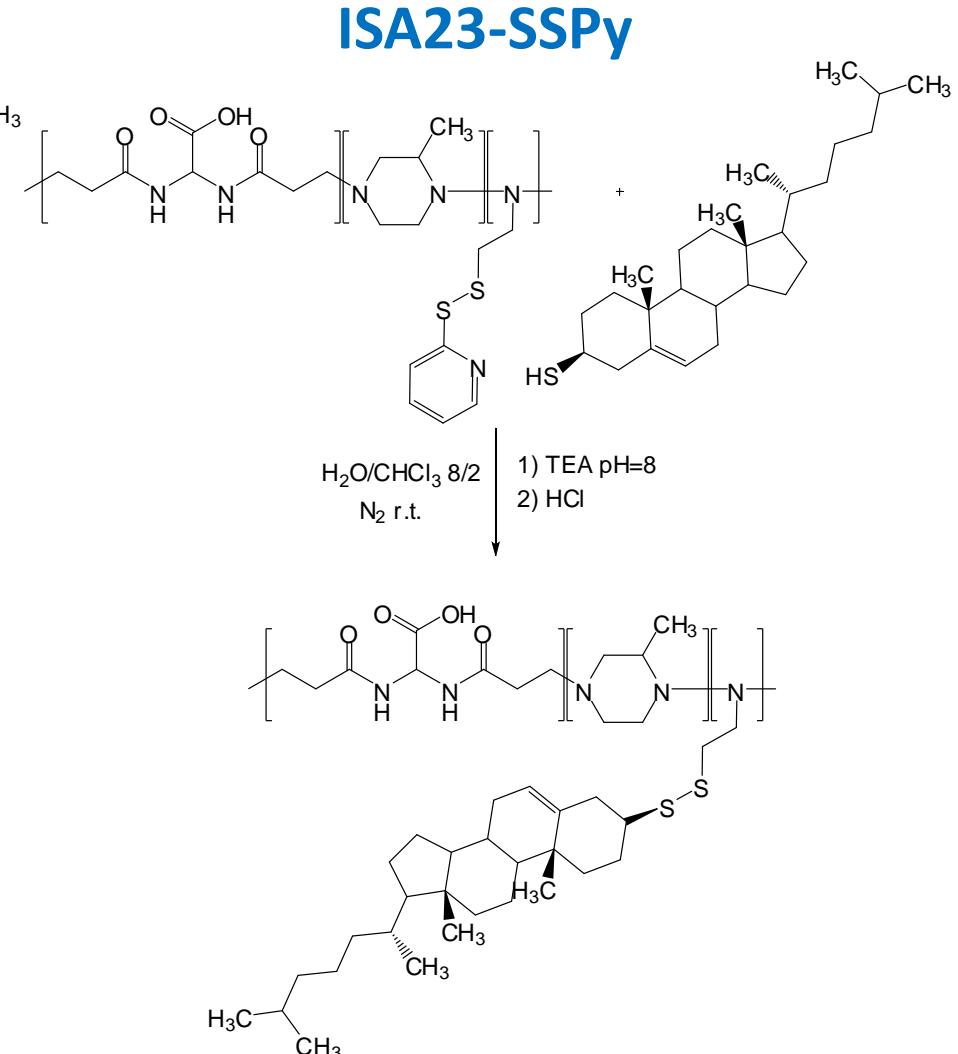
PAA-cholesterol conjugates are able to spontaneously self assemble in nanoparticles.

# PAA-SS-CHOLESTEROL CONJUGATES: SYNTHESIS

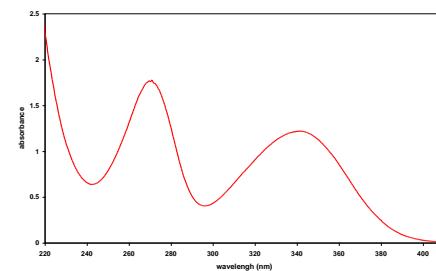
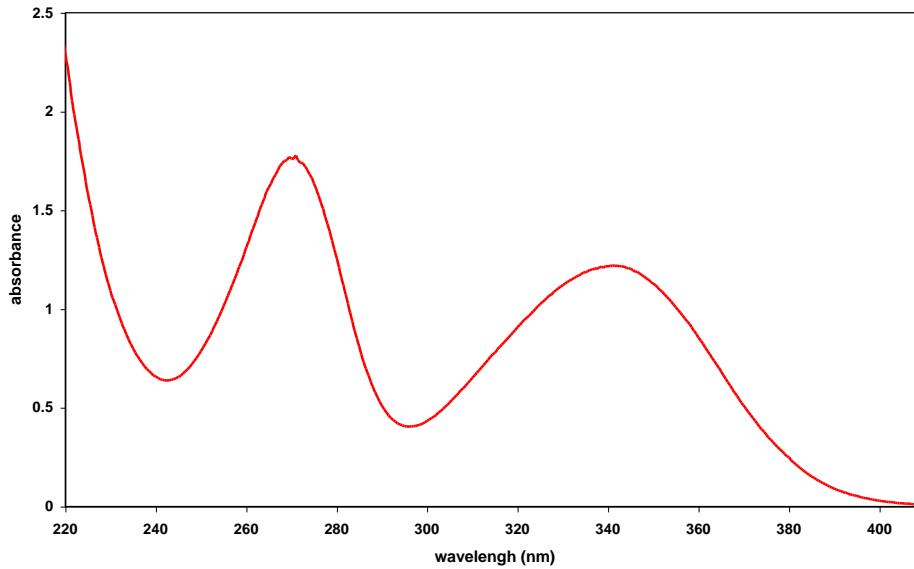
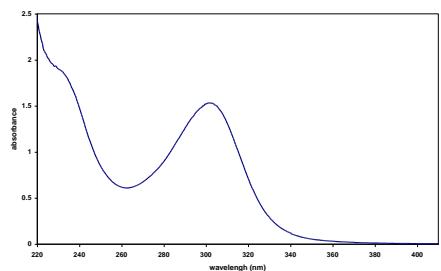
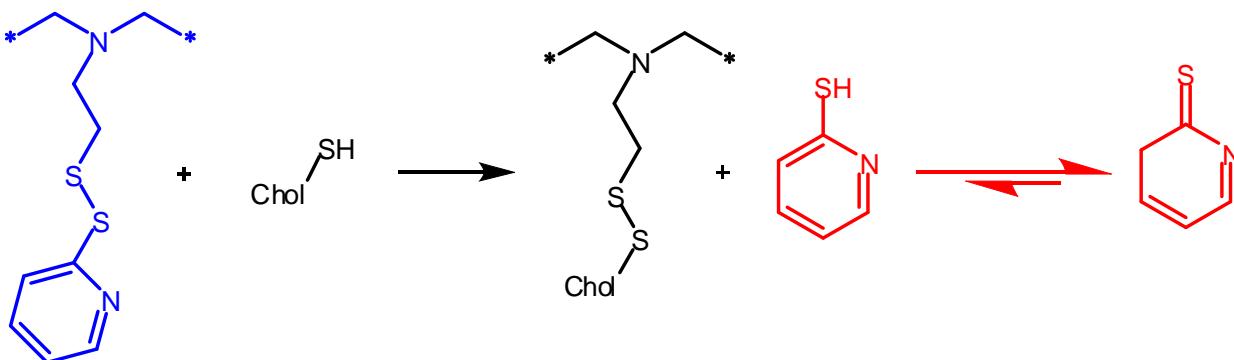
## ISA1-SSPy



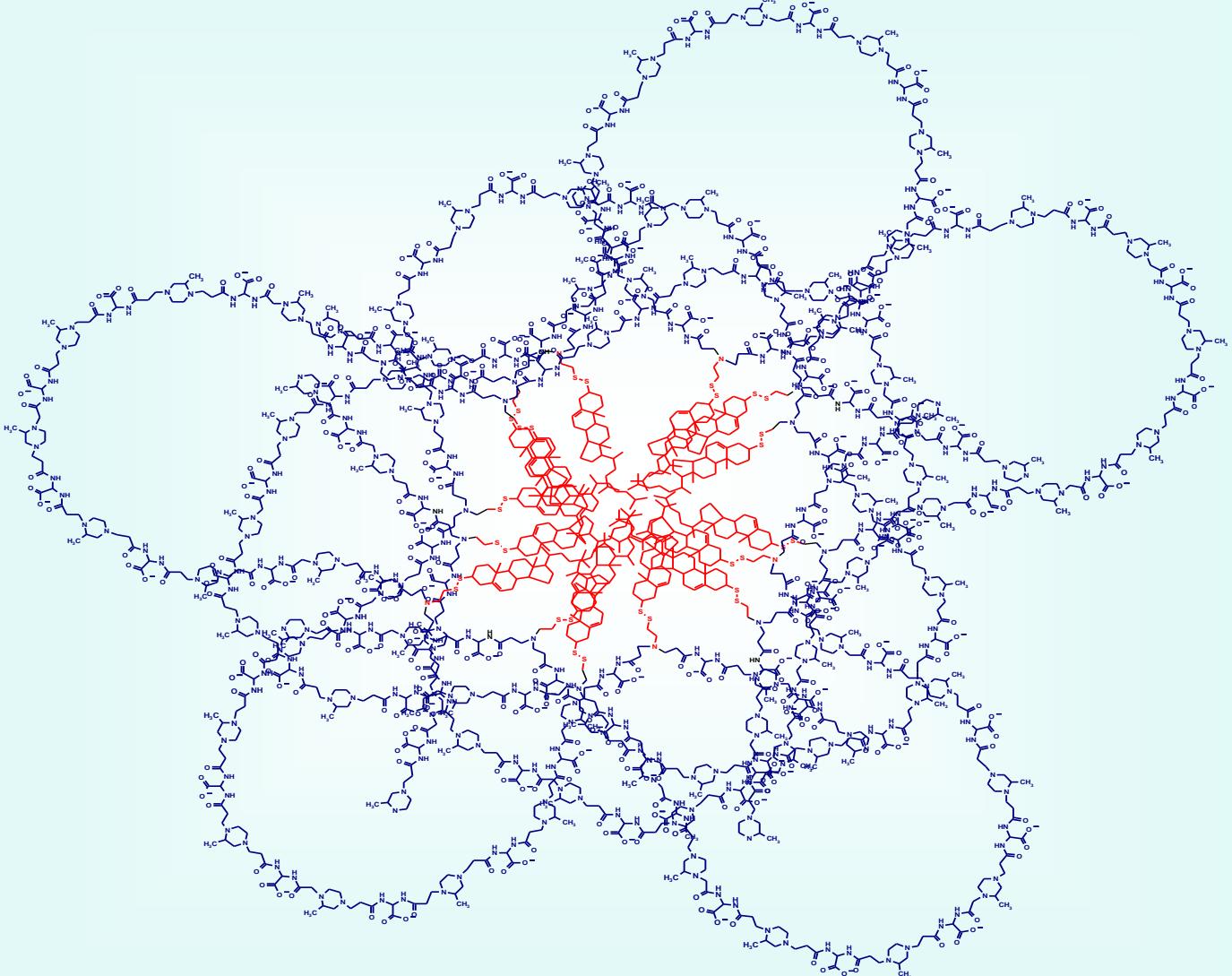
## ISA23-SSPy



## PAA-SS-CHOLESTEROL CONJUGATES: SYNTHESIS

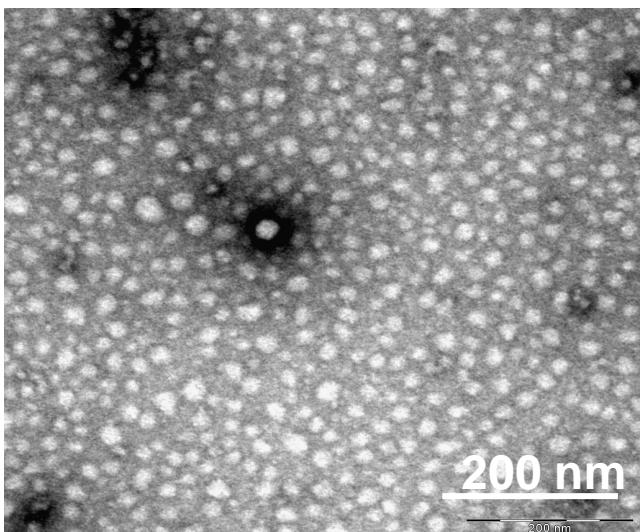


# PAA-CHOLESTEROL NANOPARTICLES



# SPONTANEOUSLY ASSEMBLED PAA-CHOLESTEROL NP

## TEM MICROGRAPH AND DLS



Sample	% Cholesterol	D (nm)	PI
ISA1-SSChol1	8	$243 \pm 16$	0.20
ISA1-SSChol2	15	$264 \pm 21$	0.18
ISA23-SSChol1	8	$124 \pm 6$	0.11
ISA23-SSChol2	15	$131 \pm 7$	0.13

D = average diameter.

PI = polydispersity index.

## CYTOTOXICITY

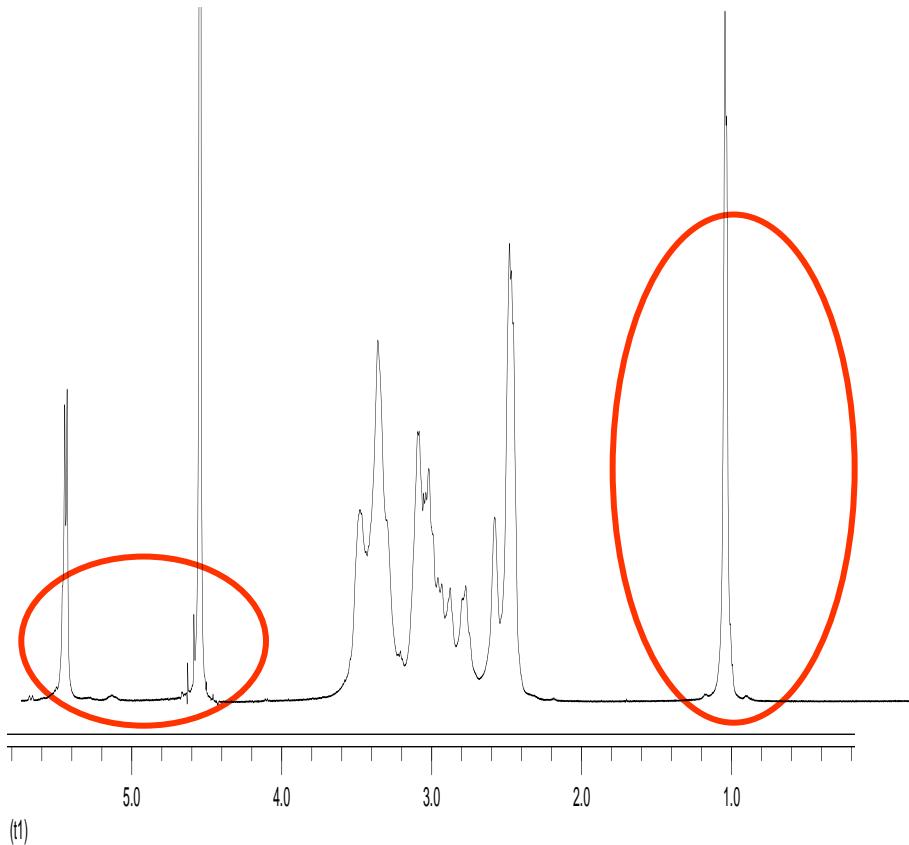
Sample	$IC_{50}$ (mg/mL) on 3T3/BALB-c cells
ISA1-SSChol	> 2
ISA23-SSChol	> 3

The cytotoxicity of PAA-cholesterol conjugates was assessed by in vitro cytotoxicity assays performed against 3T3/BALB-c Clone A31 cell lines

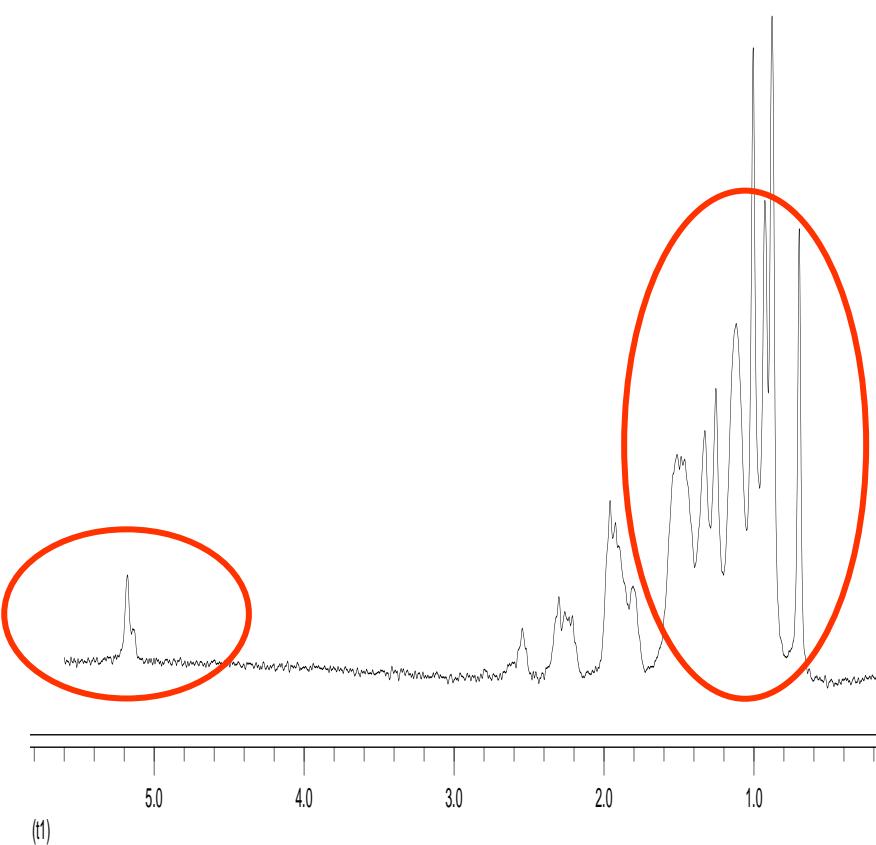


# $^1\text{H}$ NMR OF PAA-CHOLESTEROL CONJUGATES

NMR spectrum in  $\text{D}_2\text{O}$



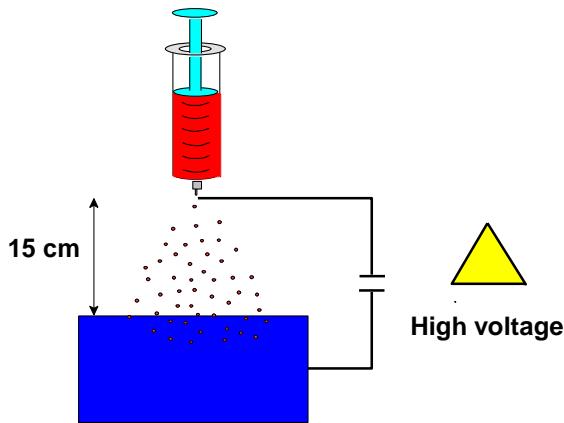
NMR spectrum in  $\text{CDCl}_3$



Ranucci, E.; Suardi, M. A.; Annunziata, R.; Ferruti, P.; Chiellini, F.; Bartoli, C. *Biomacromolecules*, 2008, 9 (10), 2693-2704



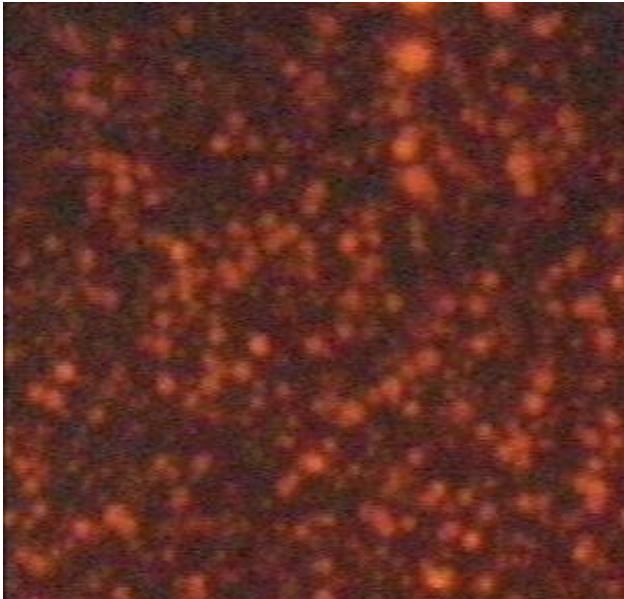
# FORMULATION OF DRUG LOADED PAA-CHOLESTEROL NP



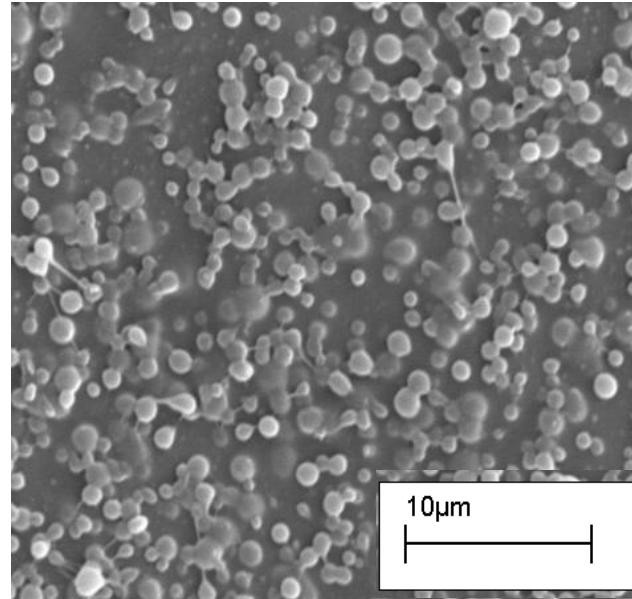
## ELECTROSPRAY

Electrospray is a method of liquid atomization that consists in the dispersion of a solution into small charged droplets by an electric field.

Doxorubicin loaded (9%) PAA-cholesterol nanoparticles

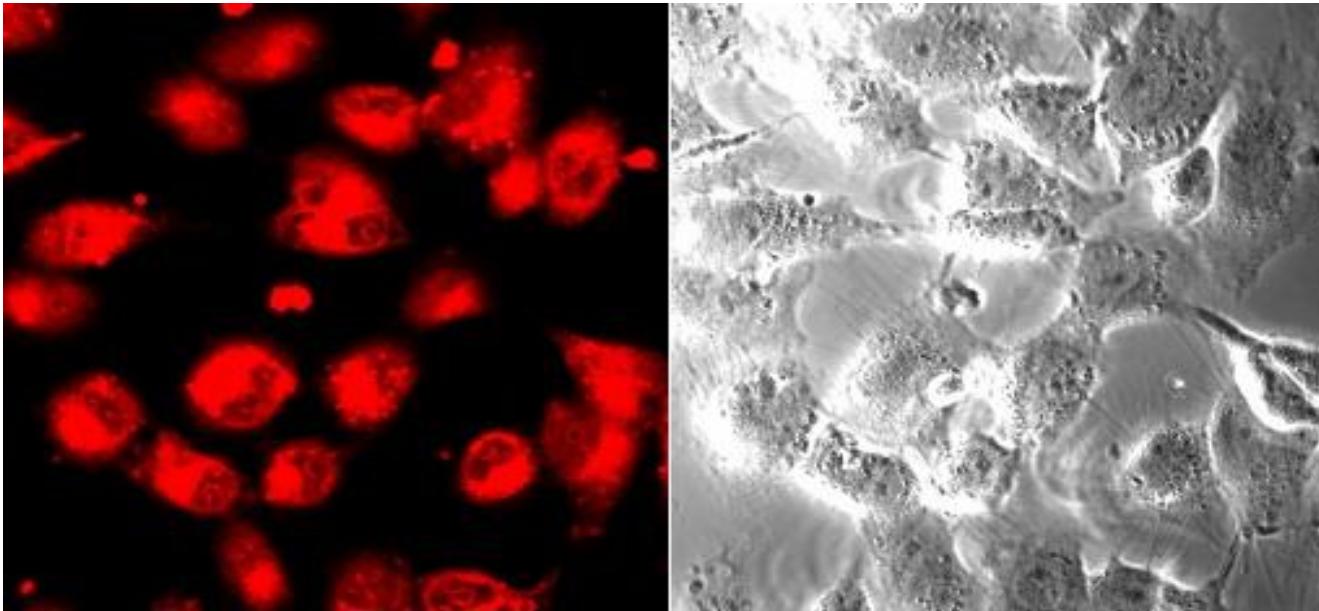


Tamoxifen loaded (5%) PAA-cholesterol nanoparticles



# FORMULATION OF DRUG LOADED PAA-CHOLESTEROL NP

## ELECTROSPRAY



Cellular uptake of doxorubicin-loaded and fluorescent PAA-cholesterol nanoparticles with confocal laser scanning microscopy.

After 1 hour the nanoparticles were internalized in the cells.



# FORMULATION OF DRUG LOADED PAA-CHOLESTEROL NP

## SOLVENT INJECTION METHOD

PAA-cholesterol nanoparticles were formulated by the solvent injection method from water-ethanol mixtures.

The nanoparticles showed no hemolytic activity tested on in vitro red blood cell.

Sample	D (nm)	PI	PZ (mV)
ISA23-SSChol	<b><math>60 \pm 10</math></b>	<b>0.26</b>	<b><math>-14.86 \pm 0.99</math></b>

D = average diameter.

PI = polydispersity index.

PZ = zeta potential

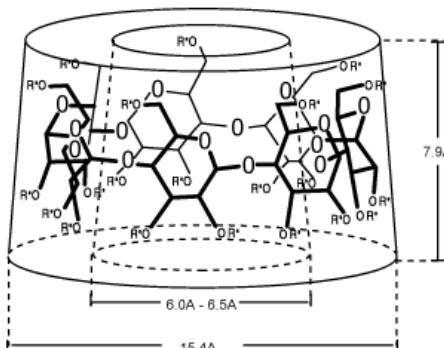
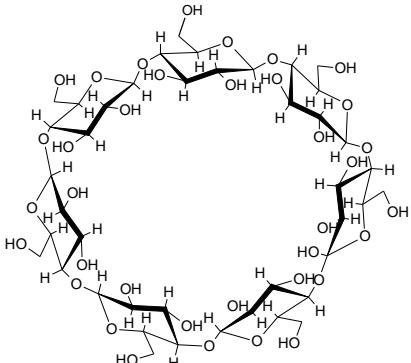
# BIOMEDICAL AND RELATED APPLICATIONS OF SECOND GENERATION POLYAMIDOAMINES

1. Synthesis and properties of PAAs
2. PAAs as cytoplasmic delivery vehicles of immunotoxines
3. PAA-cholesterol nanoparticles
- 4. PAA- $\beta$ -Cyclodextrin nanoparticles**
5. Conclusions



# PAA- $\beta$ -CYCLODEXTRIN NANOPARTICLES

Unsubstituted  $\beta$ -cyclodextrin ( $\beta$ -CD) is poorly soluble in water and often gives nearly insoluble complexes with hydrophobic molecules.



Characteristics	$\beta$ -CD
Units	7
PM	1135
Water solubility	1.85 (g/100 mL)
Cavity volume	262 Å
$[\alpha]_D$ 25°C	162.5 + 0.5
pK <sub>a</sub>	12.2

Many chemical modifications have been proposed for increasing the solubility of  $\beta$ -CD and its complexes in aqueous media but only relatively few examples of  $\beta$ -CD conjugates with biocompatible hydrophilic synthetic polymers can be found in literature.

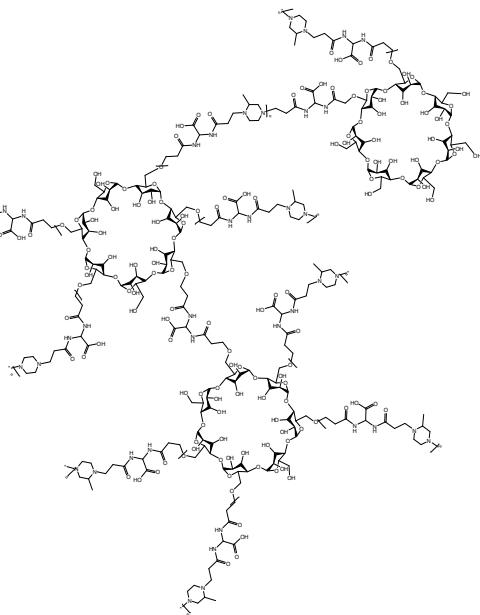
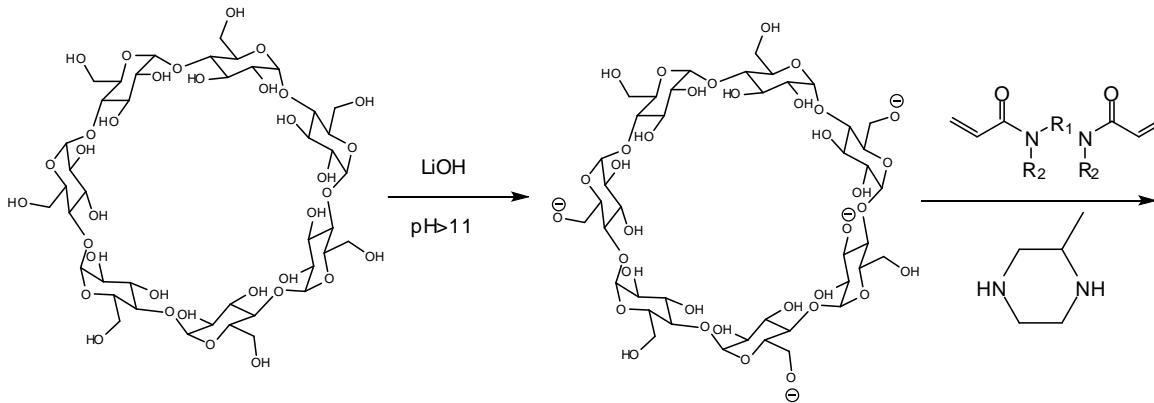


Szejtli, J. *Chem. Rev.* 1998, 98, 1743.

Salmaso, S.; Semenzato, A.; Calicetti, P.; Hoebelke, J.; Sonico, F.; Dubernet, C.; Couvreur, P. *Bioconjugate Chem.* 2004, 15, 997.

# PAA- $\beta$ -CYCLODEXTRIN NANOPARTICLES

$\beta$ -CD-PAA copolymers can be obtained as hyperbranched soluble products, or as crosslinked nanoparticulated products.



In water at 20-25°C and pH  $\geq 11$ , approximately 5 hydroxyl groups per  $\beta$ -CD molecule undergo Michael-type addition to bis-acrylamides.

This means that  $\beta$ -CD acts as multifunctional monomer in stepwise polyadditions to bisacrylamides.



# SYNTHETIC STRATEGIES

## FLORY-STOCKMAYER EQUATION

### Kinetic control

$$p_c = \frac{1}{\{r[1 + \rho(f - 2)]\}^{1/2}}$$

### Stoichiometric control

$$r_c = \frac{1}{1 + \rho (f - 2)}$$

$r$  = ratio between the number of functions of the multifunctional monomer and the total number of the same functions

$f$  = number of functions of the multifunctional monomer

$r$  = starting ratio among the complementary functions ("a" and "b")

$p_c$  = reaction conversion degree at which gelling takes place;

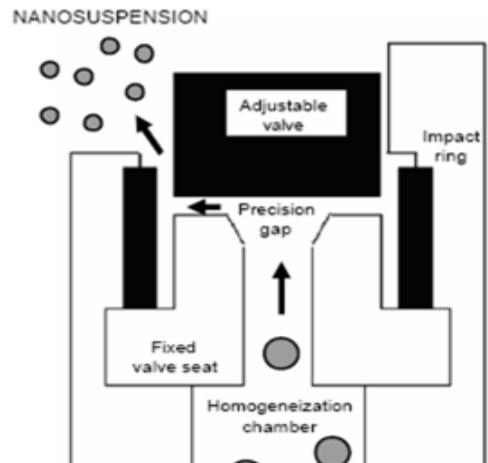
$r_c$  = critical functiona ratio. Below this value cross-linking cannot take place.



# PAA- $\beta$ -CD NANOPARTICLES

## HIGH PRESSURE HOMOGENIZATION (HPH)

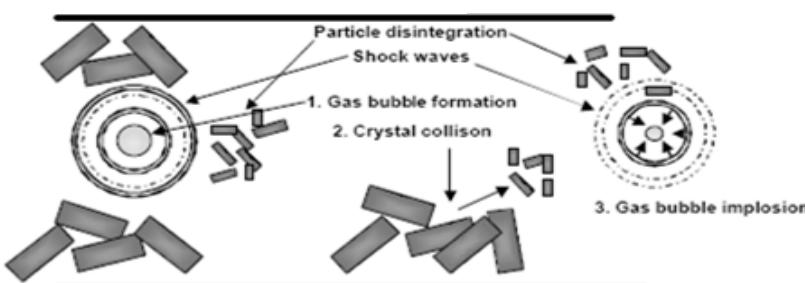
High pressure homogenizer



PAA micro- and nanogels are obtained by high pressure homogenization of hydrogel suspensions.

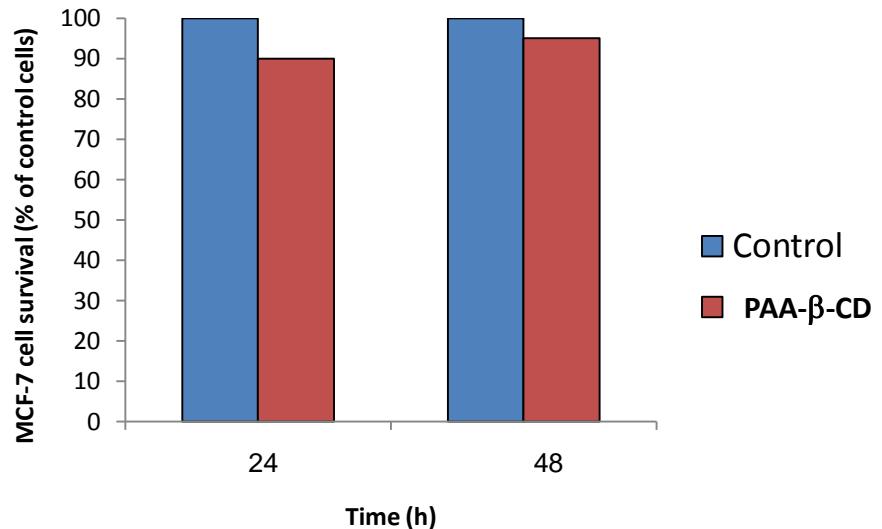
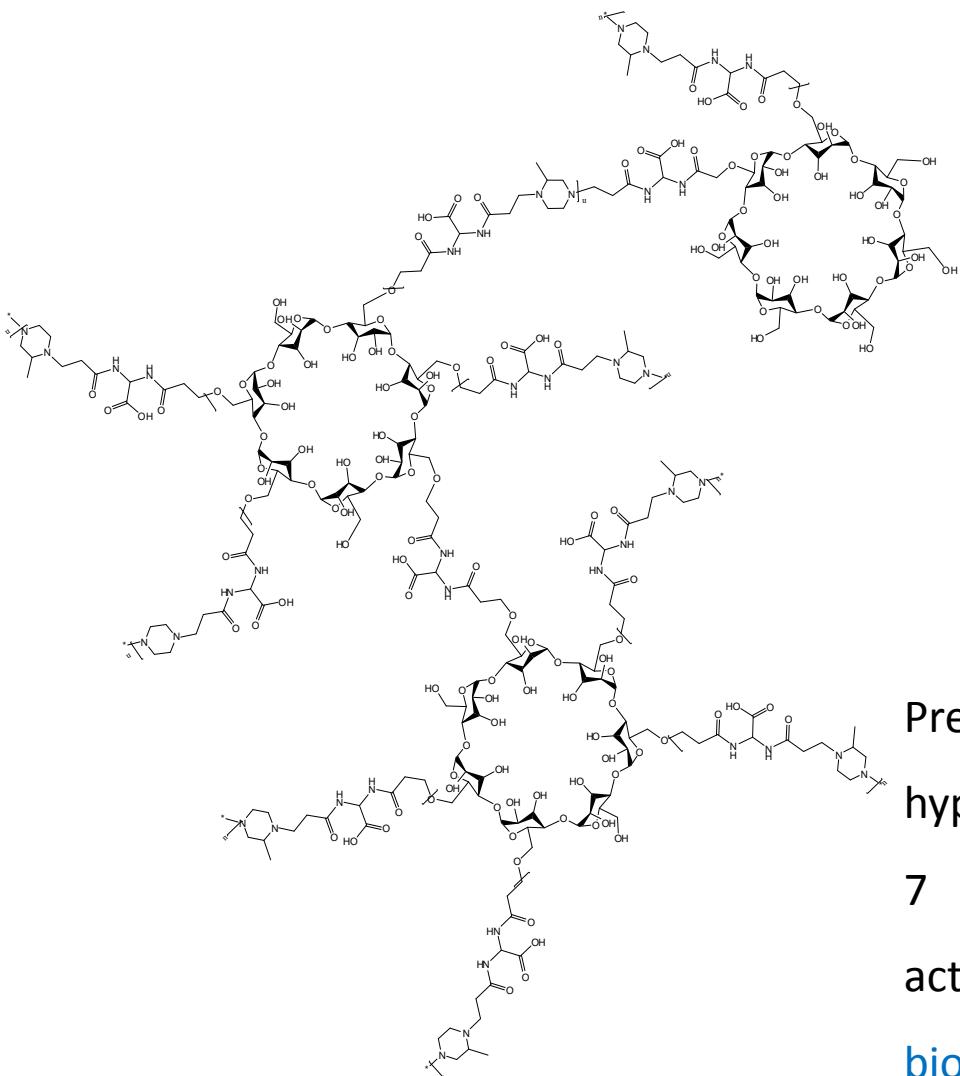
Procedure:

- 1) mechanical grinding at 12000 rpm
- 2) Homogenization cycles at 2000 – 5000 KPa



Particles rupture in precision gap during HPH process

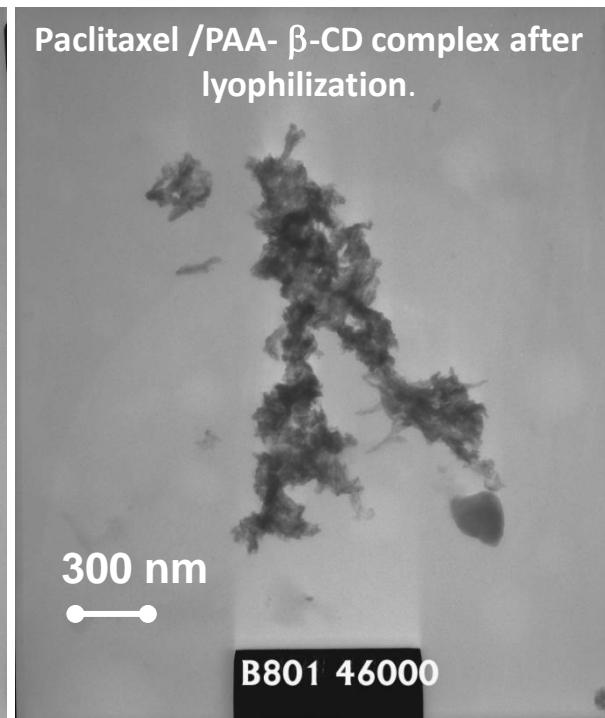
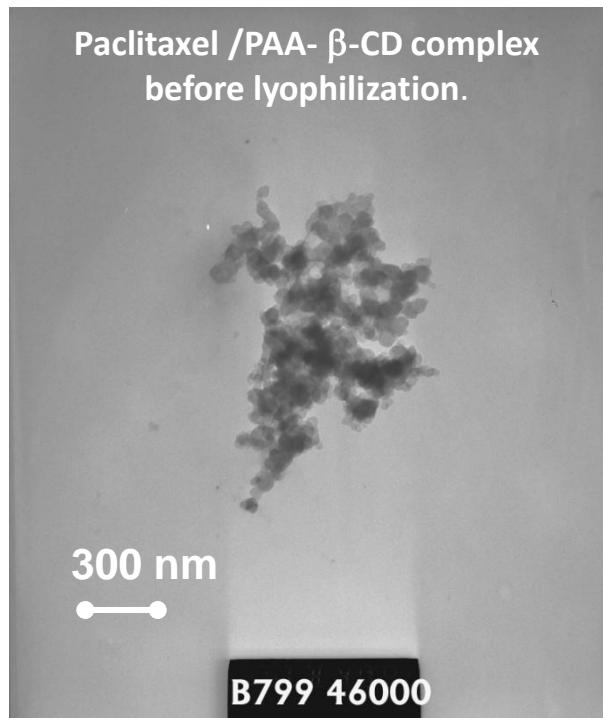
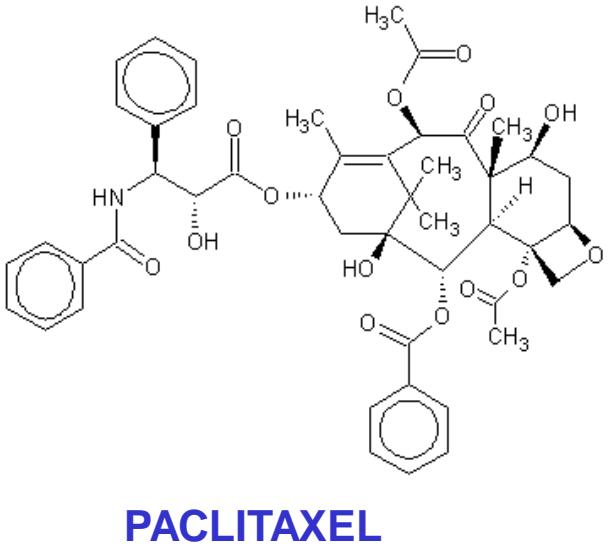
# TOXICITY



Preliminary biological evaluations carried out for hyperbranched PAA- $\beta$ -CD including In-vitro MCF-7 cell viability tests and In-vivo haemolytic activity (human RBC), have confirmed the biocompatibility of the polymer.



## PAA- $\beta$ -CD/PACLITAXEL NP



PAA- $\beta$ -CD can be loaded with Paclitaxel up to 5% of their own weight forming nanoparticles with diameter < 500 nm



## PAA- $\beta$ -CD/PACLITAXEL NP

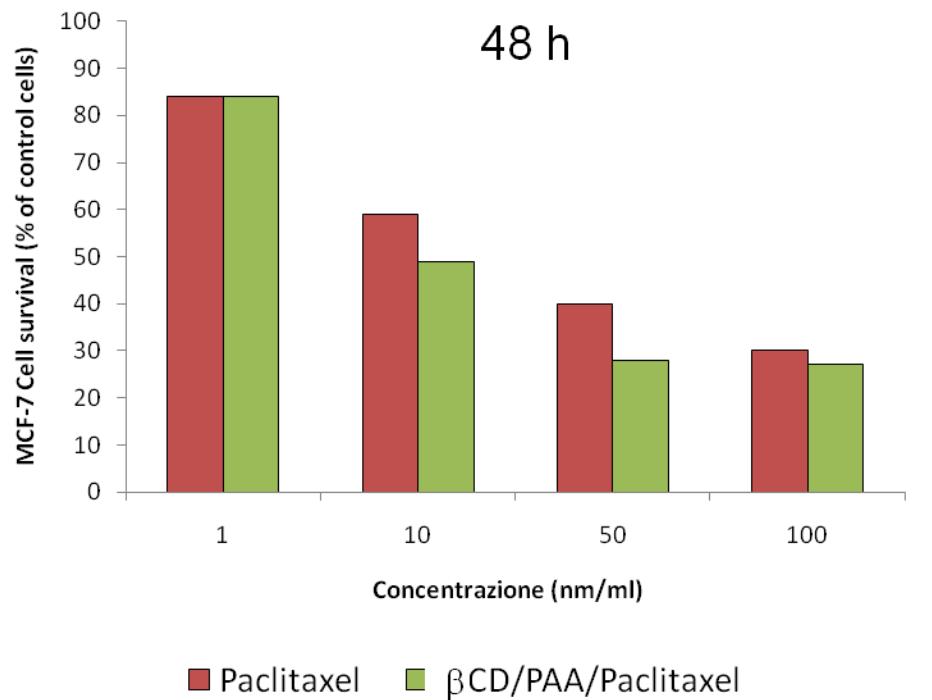
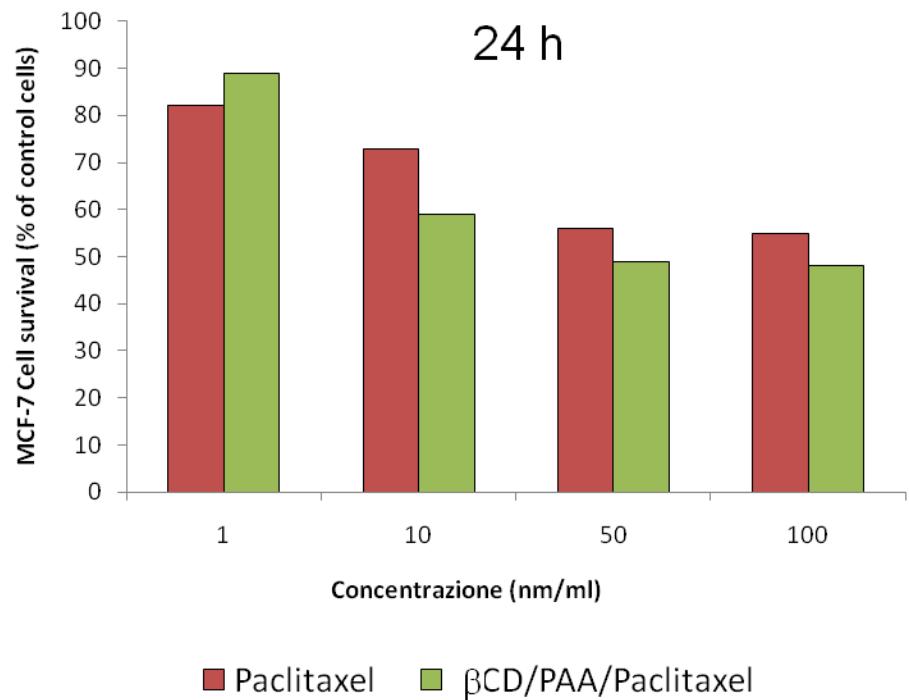


Native “solution”

The same “solution” after  
lyophilisation an  
redissolution in water.



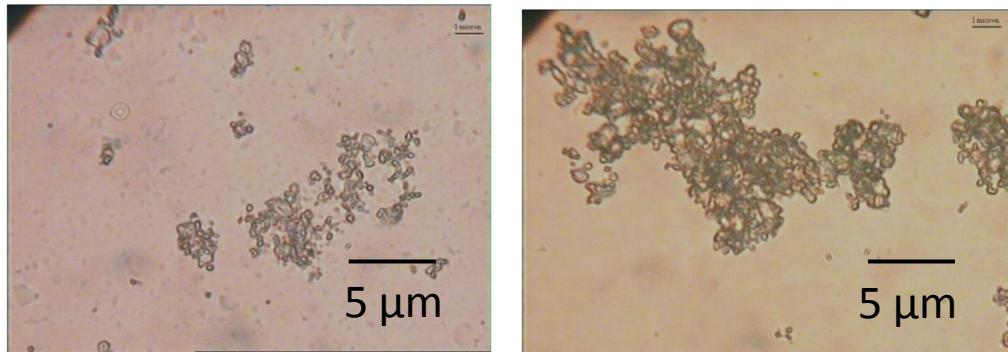
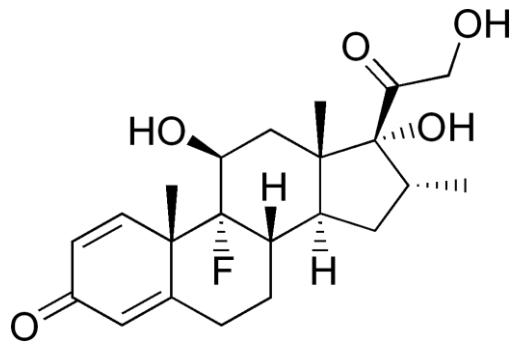
# PAA- $\beta$ -CD/PACLITAXEL NP: TOXICITY



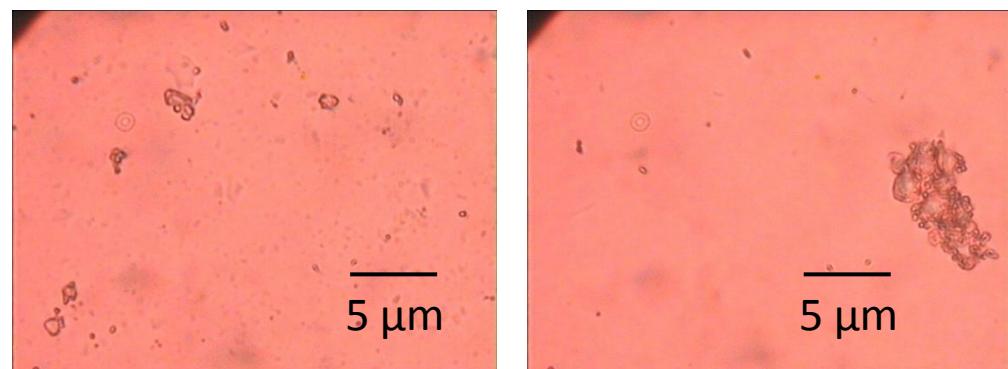
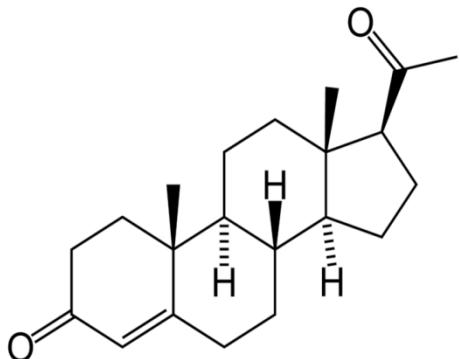
Paclitaxel even complexed by the polymeric system, maintains its efficiency in the inhibition of cancer cell growth (In vitro MCF-7 cell cultures).



## PAA- $\beta$ -CD NANOPARTICLES



DEXAMETHASONE



PROGESTERONE



# BIOMEDICAL AND RELATED APPLICATIONS OF SECOND GENERATION POLYAMIDOAMINES

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2. PAAs as cytoplasmic delivery vehicles of immunotoxines
3. PAA-cholesterol nanoparticles
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5. **Conclusions**



# CONCLUSIONS

PAAs constitute a very versatile family of ionic polymers that are easily synthesized and can be designed to be biocompatible and degradable in the body fluids.

They warrant potential, *inter alia*, as intracytoplasmic delivery vehicles of protein, as nanoparticles for the release of lipophilic drugs and many other applications in the nanomedicine field.

As a final observation, the unique combination of biotechnologically relevant properties of PAAs are still waiting to be fully exploited.



# ACKNOWLEDGMENTS

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**THANK YOU  
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