

Spring 3-28-2012

Blood Flow Through the Aorta in a Mouse Model of Atherosclerosis

J. Hough
Monash University

P. Assemat
Monash University

K.K.W. Siu
Monash University

J.A. Armitage
Monash University

K. Contreras
Monash University

See next page for additional authors

Follow this and additional works at: <http://dc.engconfintl.org/cfdmedicine>

 Part of the [Biomedical Engineering and Bioengineering Commons](#)

Recommended Citation

J. Hough, P. Assemat, K.K.W. Siu, J.A. Armitage, K. Contreras, A. Aprico, A. Dart, J. Ching-Dusting, and K. Hourigan, "Blood Flow Through the Aorta in a Mouse Model of Atherosclerosis" in "Computational Fluid Dynamics (CFD) in Medicine And Biology in Conjunction With the Seventh International Biofluid Mechanics Symposium", D. Elad, Tel Aviv Univ.; D. Bluestein, Stony Brook Univ.; D. Dooly, Imperial College London; M. Gharib, California Inst. Of Technology; P. Hunter, The Univ. of Auckland; M. Engelman, ANSYS, Inc. Eds, ECI Symposium Series, (2013). <http://dc.engconfintl.org/cfdmedicine/2>

This Conference Proceeding is brought to you for free and open access by the Proceedings at ECI Digital Archives. It has been accepted for inclusion in Computational Fluid Dynamics (CFD) in Medicine And Biology in Conjunction With the Seventh International Biofluid Mechanics Symposium by an authorized administrator of ECI Digital Archives. For more information, please contact franco@bepress.com.

Authors

J. Hough, P. Assemat, K.K.W. Siu, J.A. Armitage, K. Contreras, A. Aprico, A. Dart, J. Ching-Dusting, and K. Hourigan

Blood Flow Through the Aorta in a Mouse Model of Atherosclerosis

J. Hough¹, P. Assemat¹, K. K. W. Siu^{2,3}, J. A. Armitage⁴, K. Contreras¹, A. Aprico⁵, A. Dart⁵, J. Chin-Dusting⁵, [K. Hourigan¹](#)

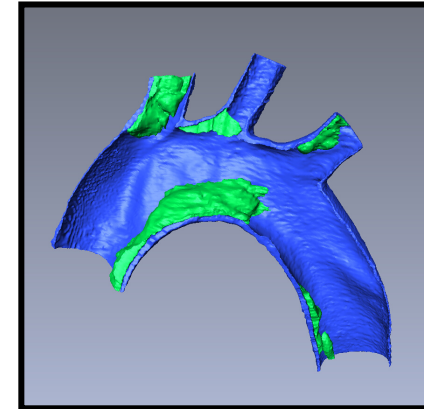
¹*Department of Mechanical and Aerospace engineering & Division of Biological Engineering, Monash University, Melbourne, Australia*

²*Monash Biomedical Imaging, Monash University, Clayton, Australia*

³*Australian Synchrotron, Clayton Australia*

⁴*Department of Anatomy and Developmental Biology, Monash University, Melbourne, Australia*

⁵*Baker IDI Heart and Diabetes Institute, Melbourne, Australia*



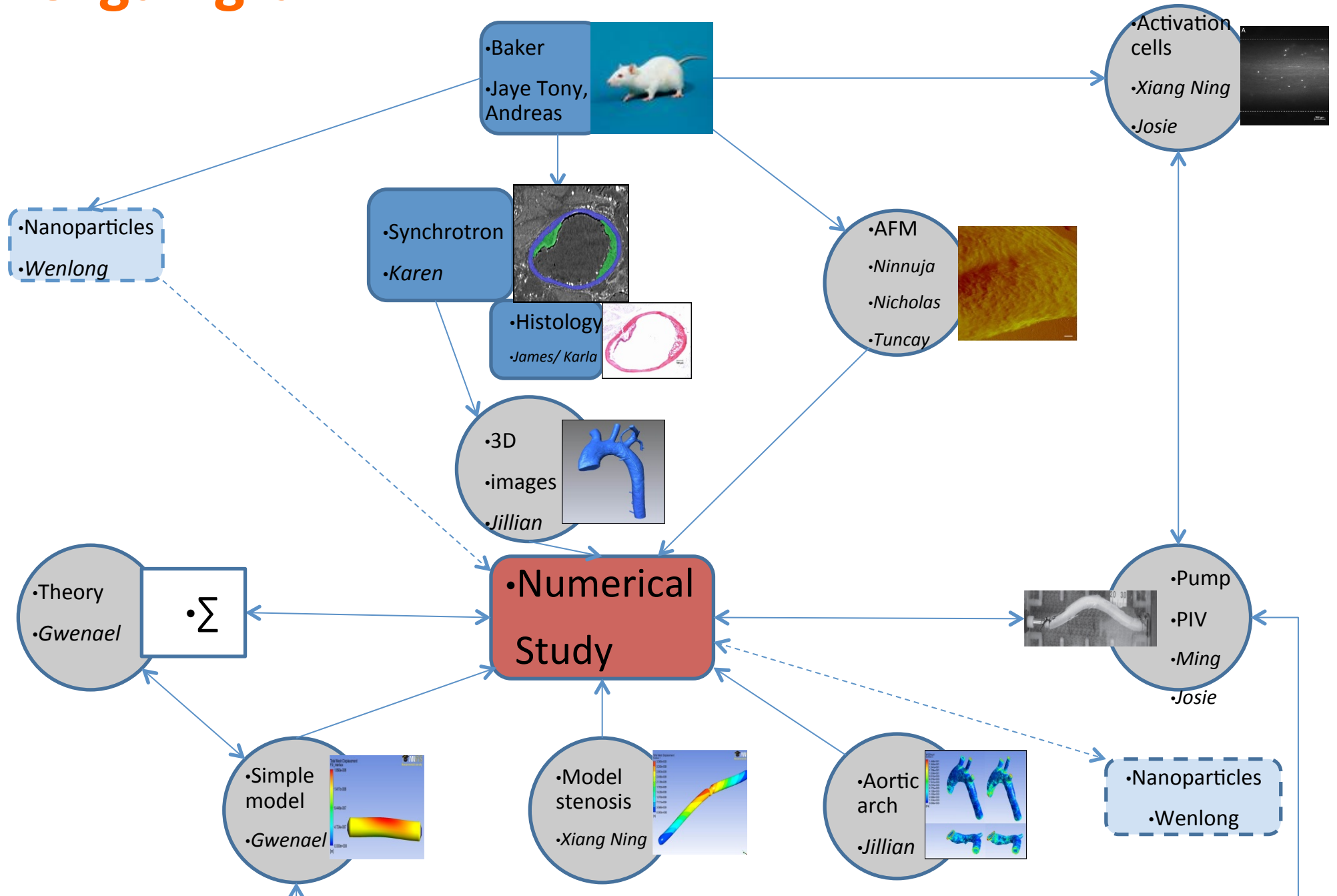
ECI Conference on Computational Fluid Dynamics (CFD) in Medicine and Biology / Seventh International Biofluid Mechanics Symposium

March 25-30, 2012, Crowne Plaza Dead Sea, Ein Bokek, Dead Sea, Israel

Outline of the Presentation

- ⇒ • **Context of current research**
- **Atherosclerosis overview**
- **Computed Tomographic X-ray Velocimetry**
 - Synthetic: Stenosis**
 - In vitro: Thrombi**
 - In vivo: Heart**
- **CFD**
 - Idealised stenoses**
 - Mouse aorta**
- **Conclusions**

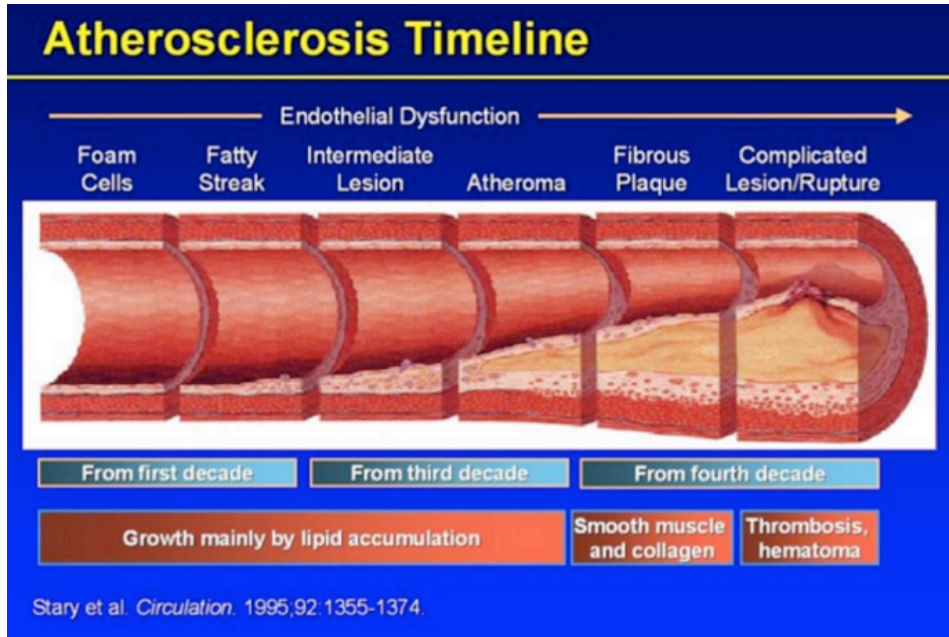
Organigram



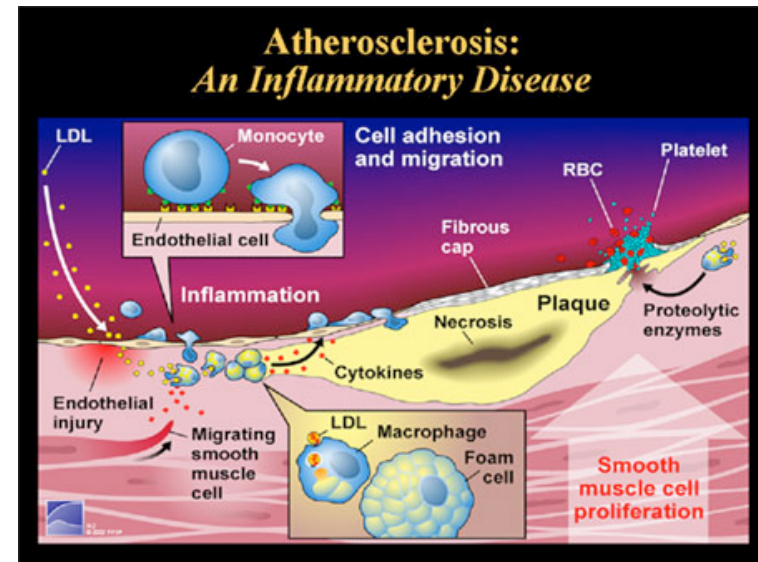
Outline of the Presentation

- Context of current research
- ⇒ • Atherosclerosis overview
- Computed Tomographic X-ray Velocimetry
 - Synthetic: Stenosis
 - In vitro: Thrombi
 - In vivo: Heart
- CFD
 - Idealised stenoses
 - Mouse aorta
- Conclusions

Sequence of progression of atherosclerosis



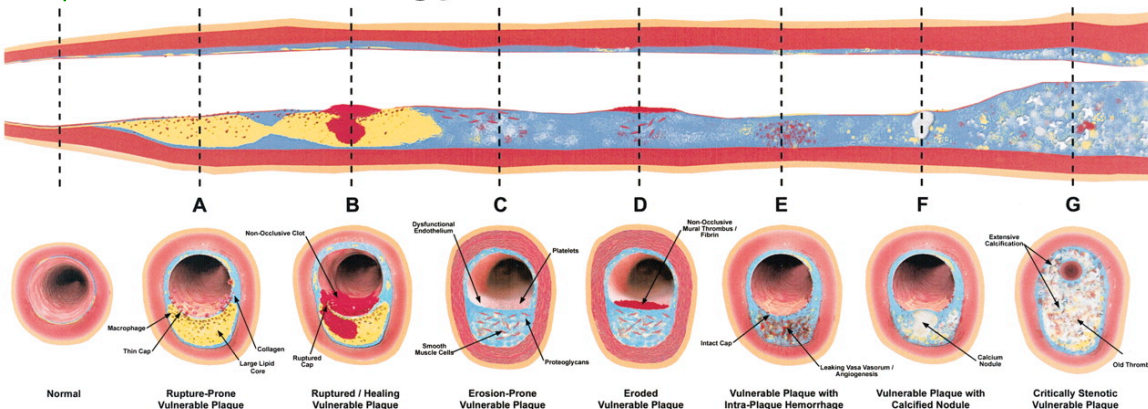
Biomolecular activity in atherosclerosis



www.lancastria.net

www.coastalcimt.com

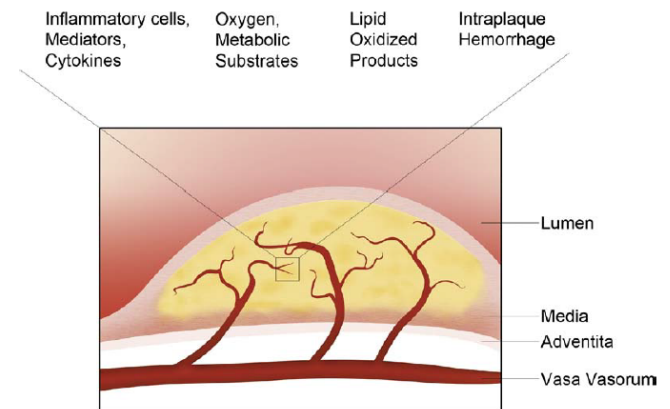
Different Types of Vulnerable Plaque



www.vp.org



Contribution of plaque angiogenesis to lesion growth



Caplice, N. & Martin, K., *J. Am. Coll. Cardiol.*, 3 (1 2), 2010

Refer to review paper:

Stabilisation of atherosclerotic plaques

Position Paper of the European Society of Cardiology (ESC) Working Group on Atherosclerosis and Vascular Biology

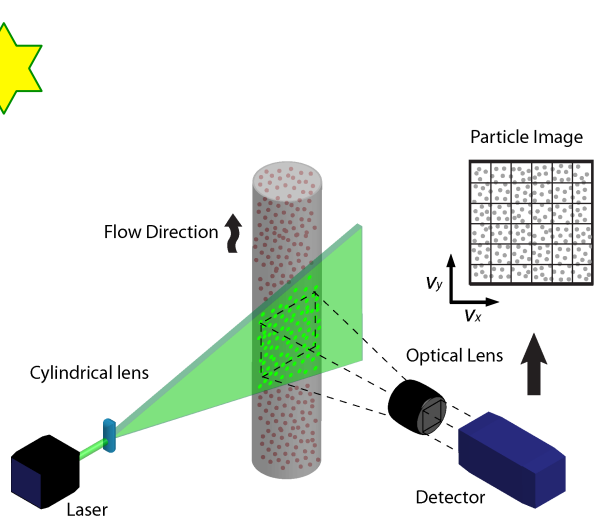
Thrombosis and Haemostasis 2011; 106: 1–19

Seppo Ylä-Herttuala; Jacob Fog Bentzon; Mat Daeme; Erling Falk; Hector M. Garcia-Garcia; Joerg Herrmann; Imo Hofer; J. Wouter Jukema; Rob Krams; Brenda R. Kwak; Nikolaus Marx; Marek Naruszewicz; Andrew Newby; Gerard Pasterkamp; Patrick W. J. C. Serruys; Johannes Waltenberger; Christian Weber; Lale Tokgözoğlu

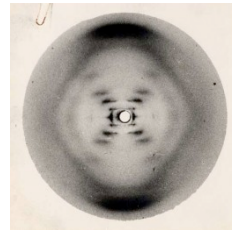
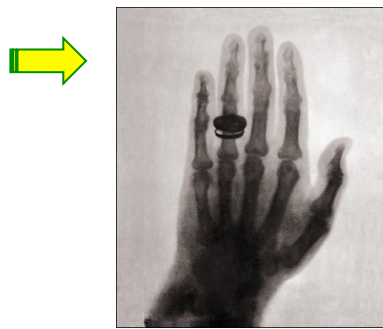
Outline of the Presentation

- Context of current research
- Atherosclerosis overview
- ⇒ • Computed Tomographic X-ray Velocimetry
 - Synthetic: Stenosis
 - In vitro: Thrombi
 - In vivo: Heart
- CFD
 - Idealised stenoses
 - Mouse aorta
- Conclusions

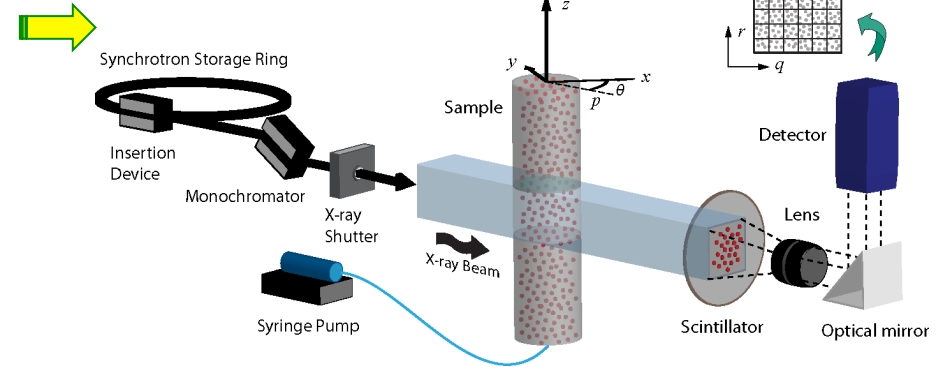
From PIV to Computed Tomographic X-ray Velocimetry



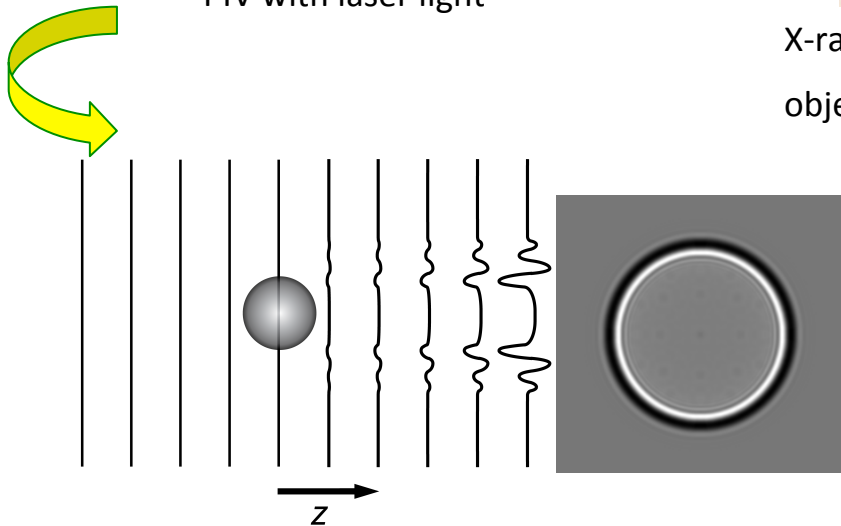
PIV with laser light



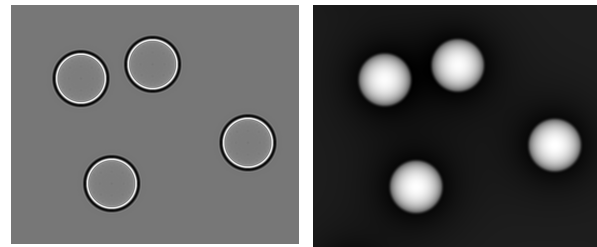
X-rays: opaque and small objects



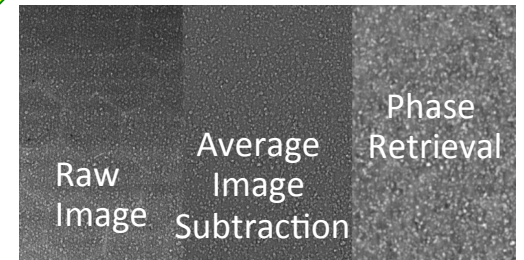
Experimental setup for CTXV



Phase contrast imaging increases signal from weakly absorbing objects

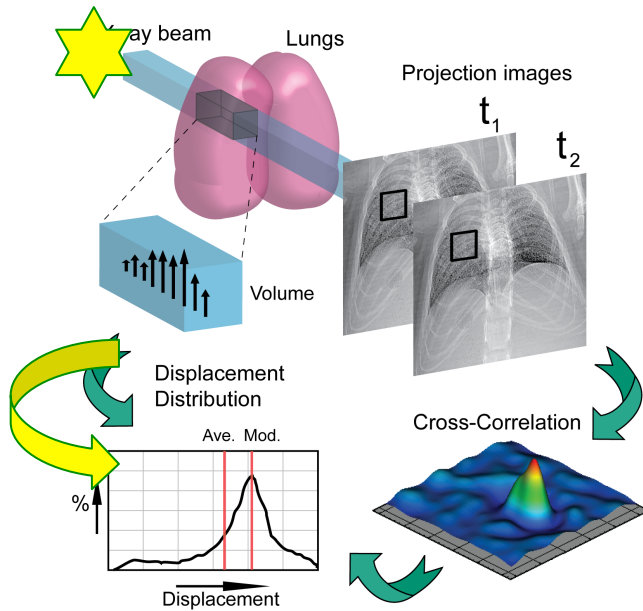


Phase retrieval algorithm allows for recovery of projected thickness

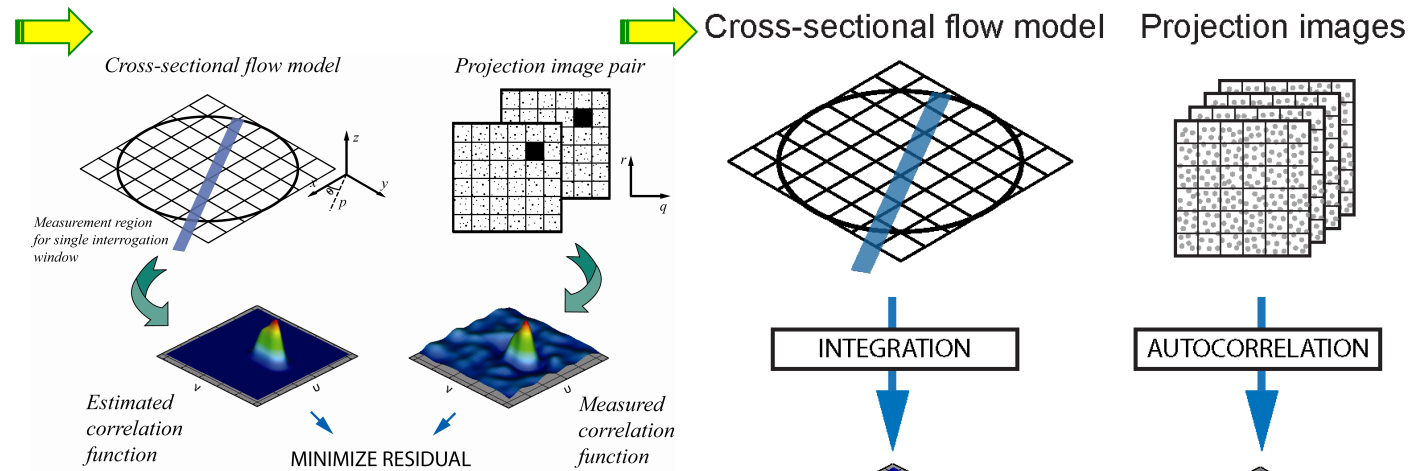


Pre-processing improves images for analysis

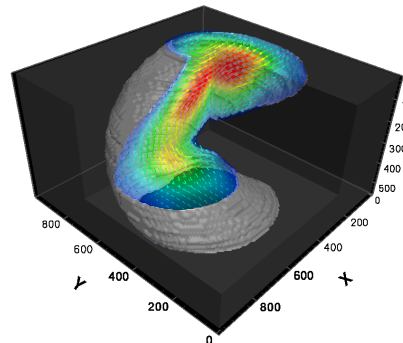
From PIV to Computed Tomographic X-ray Velocimetry (ctd)



The cross-correlation contains VOLUMETRIC motion information



Non-linear iterative algorithm is to reconstruct the 3D velocity profile from the 2D cross-correlations



Estimated cross correlation function

Forward projection estimates cross-correlation function

Dubsky, S., Jamison, R., Higgins, S., Siu, K., Hourigan, K. & Fouras, A., *Computed Tomographic X-ray Velocimetry for simultaneous 3D measurement of velocity and geometry in opaque vessels*, Experiments in Fluids, 2012, 52:543–554.

Outline of the Presentation

- **Context of current research**
- **Atherosclerosis overview**
- **Computed Tomographic X-ray Velocimetry**



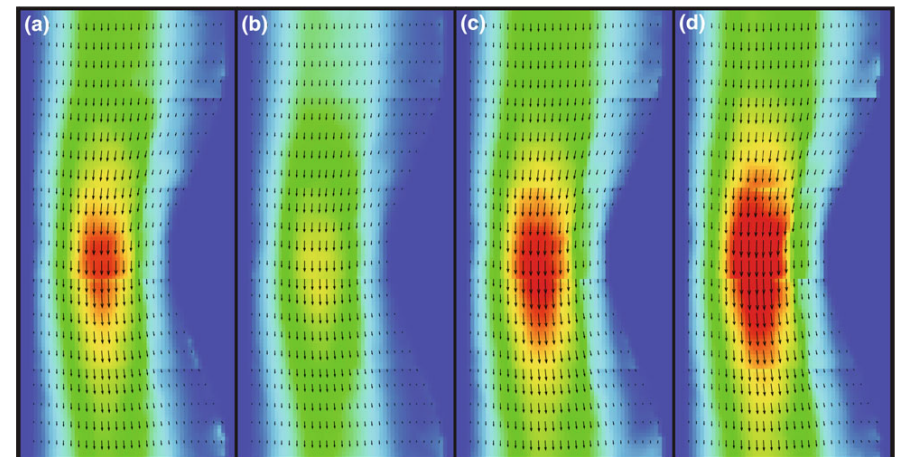
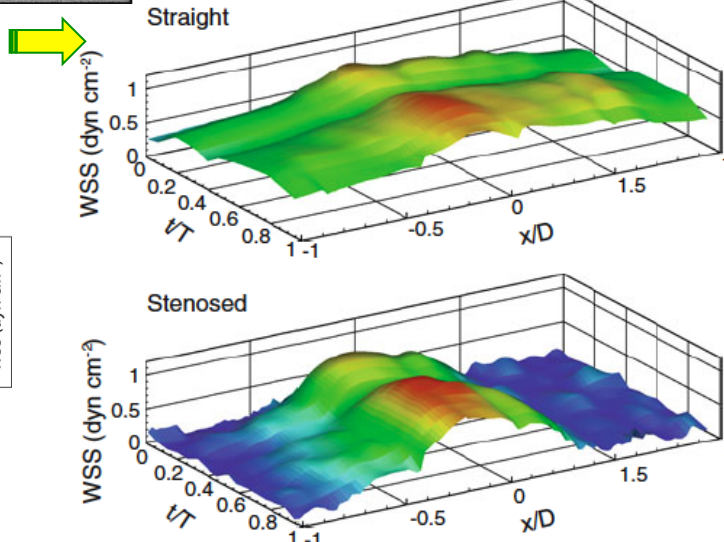
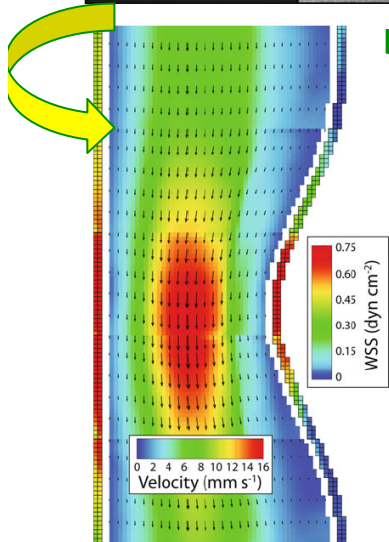
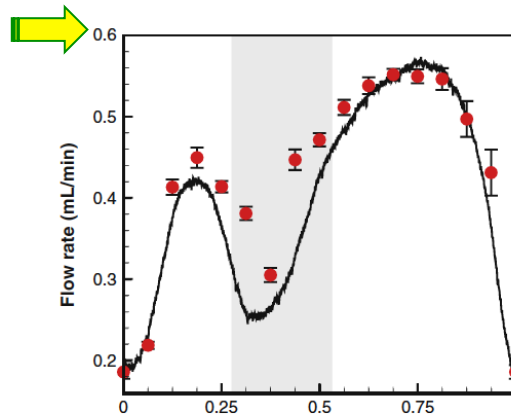
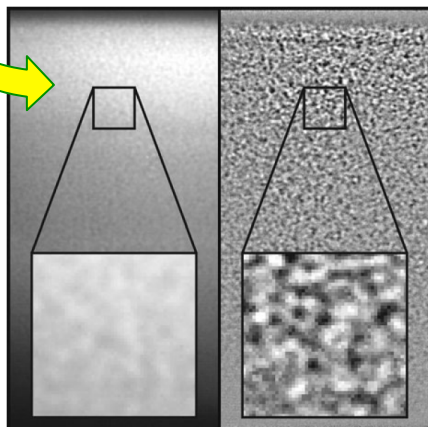
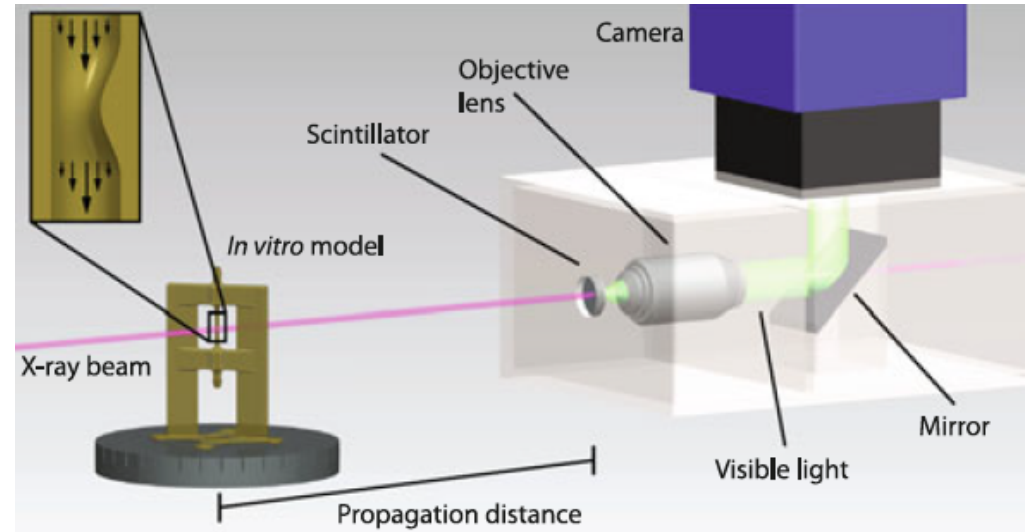
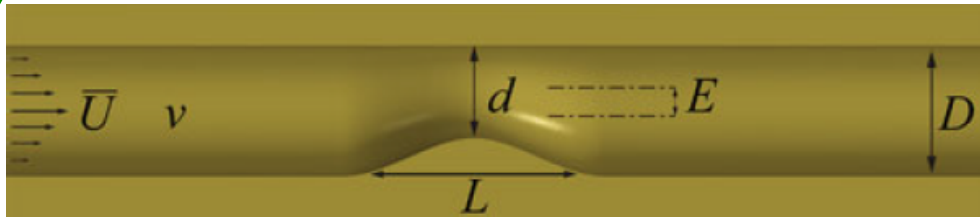
Synthetic: Stenosis

In vitro: Thrombi

In vivo: Heart

- **CFD**
 - Idealised stenoses**
 - Mouse aorta**
- **Conclusions**

X-ray PIV (2D) measurement of flow in a synthetic stenosed vessel



Jamison, R.A., Dubsky, S., Siu, K.W., Hourigan, K., Fouras, A., *X-ray velocimetry and haemodynamic forces within a stenosed femoral model at physiological flow rates*, *Annals of Biomedical Engineering*, 39 (6), 1643-1653, 2011.

Outline of the Presentation

- **Context of current research**
- **Atherosclerosis overview**
- **Computed Tomographic X-ray Velocimetry**

Synthetic: Stenosis



In vitro: Thrombi

In vivo: Heart

- **CFD**

Idealised stenoses

Mouse aorta

- **Conclusions**

The evolution of thrombi geometry



Platelets Can Promote Inflammation & Plaque Instability

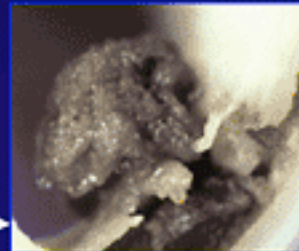
Activated Platelets



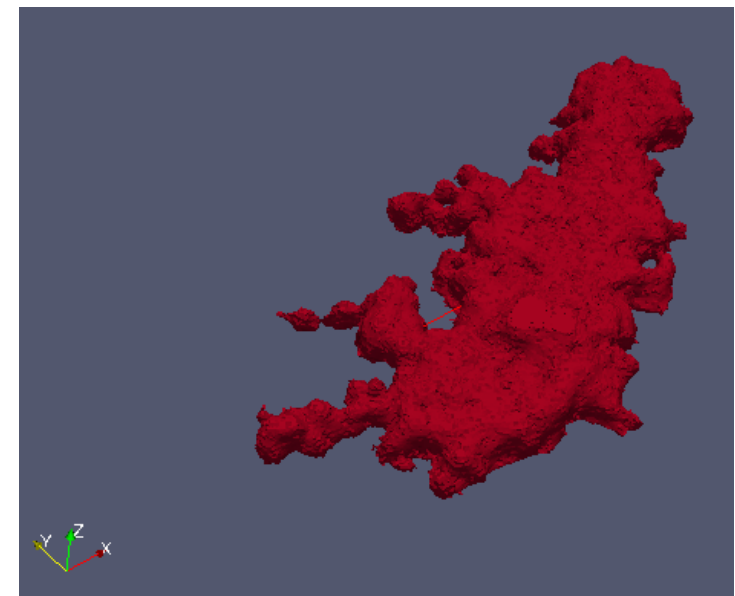
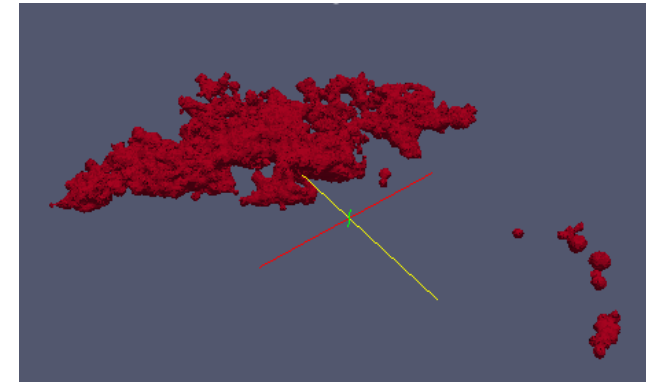
Inflammatory Mediators

- CD40L
- Platelet-derived growth factor
- Platelet factor 4
- RANTES
- Thrombospondin
- Transforming growth factor- β
- Nitric Oxide

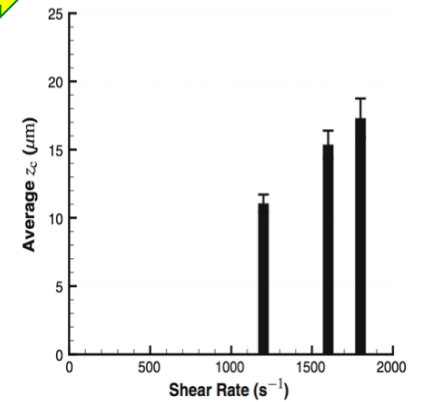
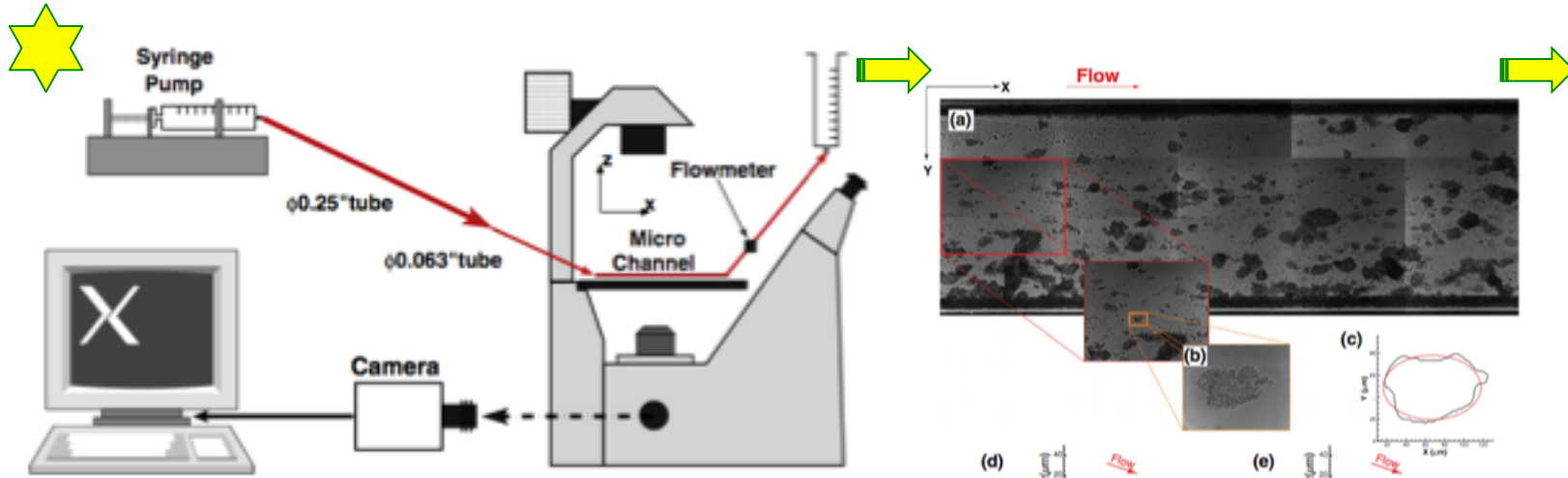
Plaque Rupture & Thrombosis



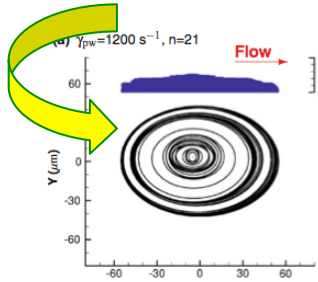
Libby, P. *Circ.* 2001;103:1718-1720.



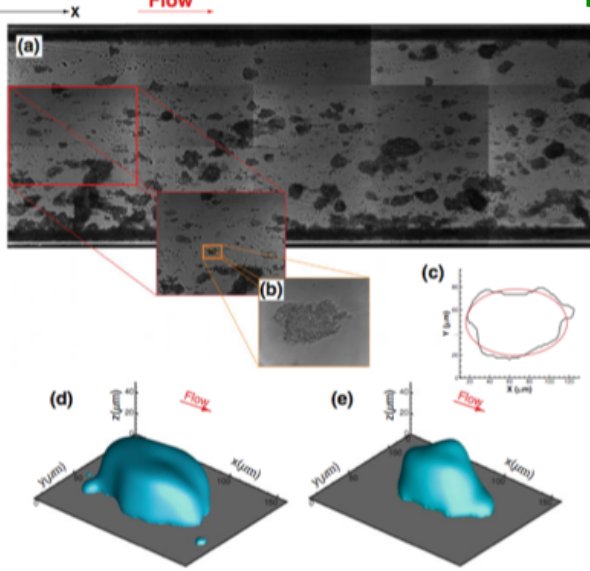
Effect of haemodynamic forces on thrombi geometry



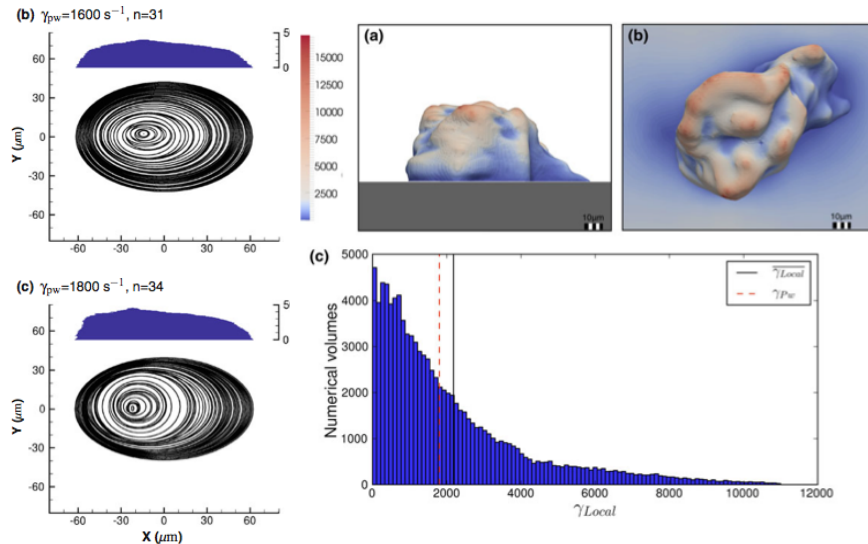
Average centroid height (z_c) of mature platelet aggregations increases with shear rate



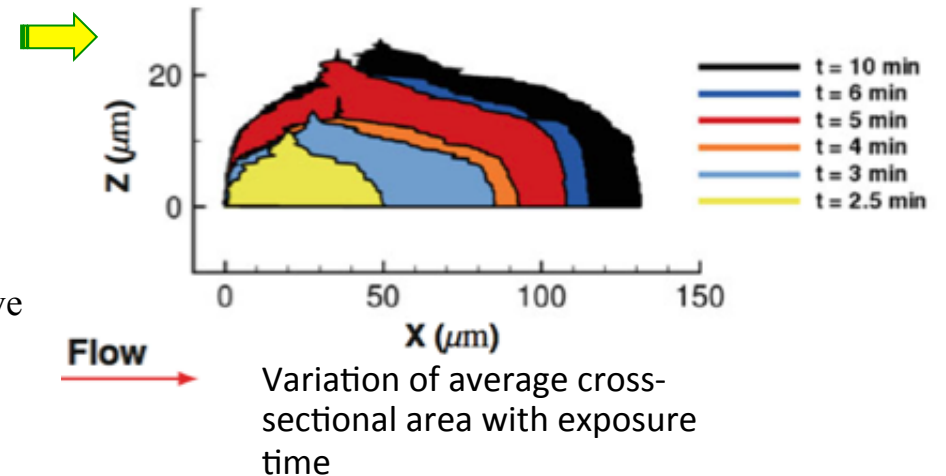
The three-dimensional profiles for the average platelet aggregations at each shear rate



Measurement of platelet aggregation geometries using bright field scanning microscopy and image reconstruction

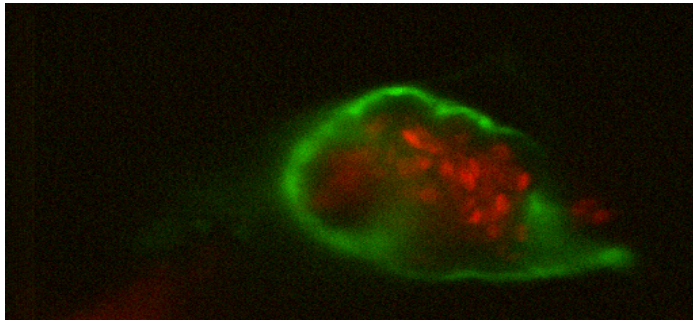


Local shear rate distribution around a representative mature platelet aggregation

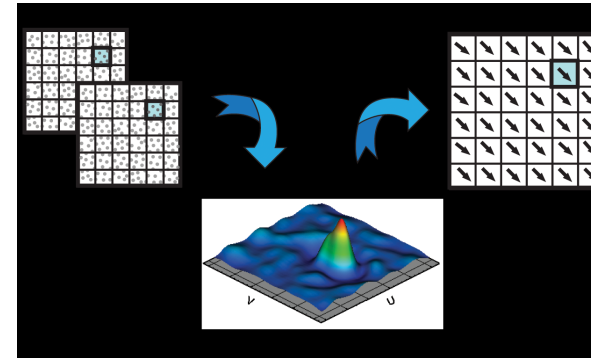


Variation of average cross-sectional area with exposure time

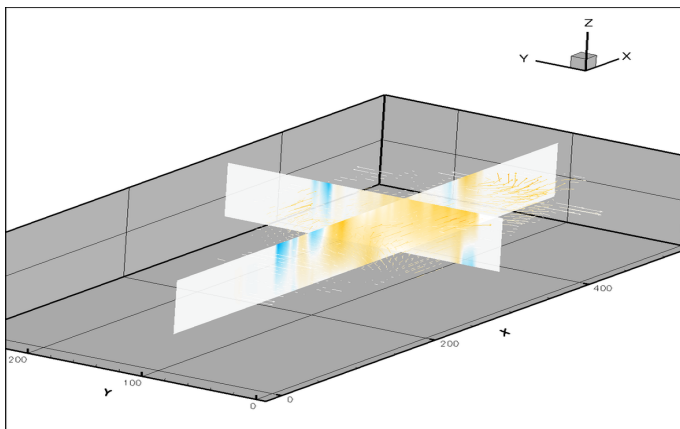
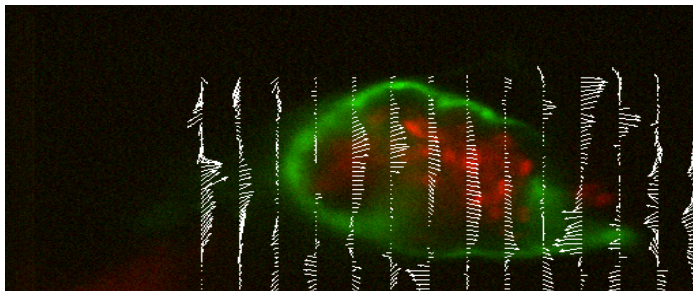
Extending to 3-Dimensional analysis of *in vivo* flows



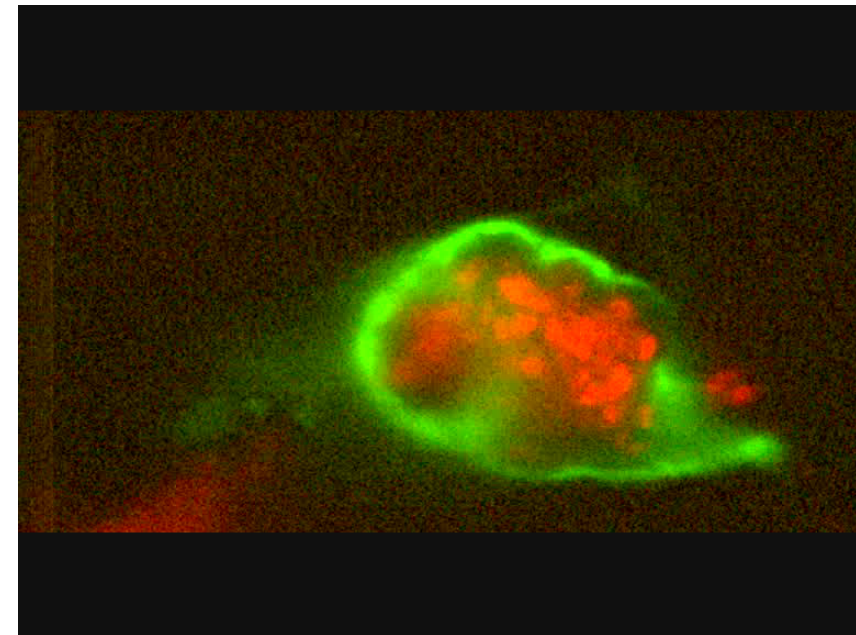
Zebra fish heart: tissue, blood



Particle Image Velocimetry



2d -> 3d velocity fields



Small, beating, compliant, non-Newtonian blood

Outline of the Presentation

- **Context of current research**
- **Atherosclerosis overview**
- **Computed Tomographic X-ray Velocimetry**

Synthetic: Stenosis

In vitro: Thrombi

In vivo: Heart

- **CFD**

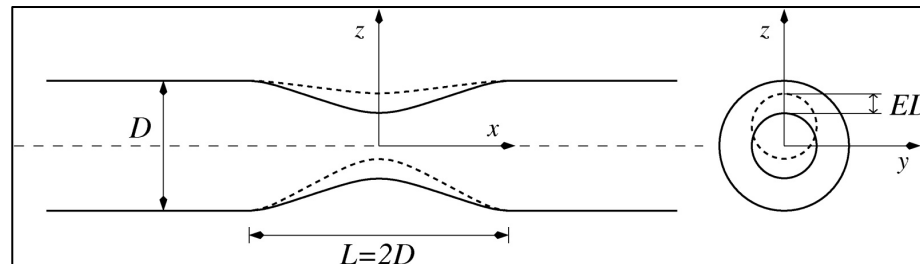
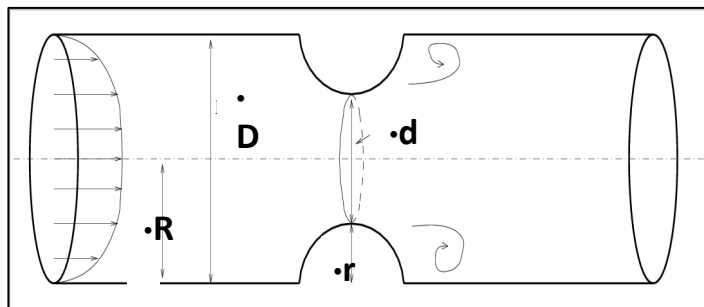


Idealised stenoses

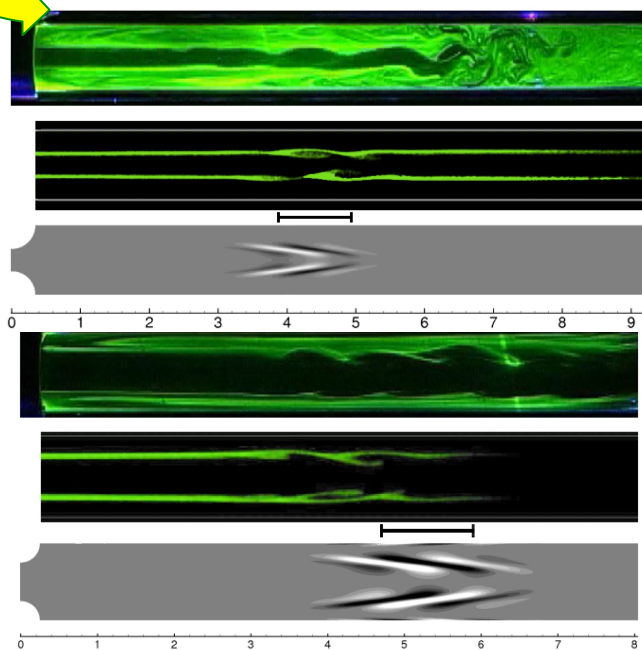
Mouse aorta

- **Conclusions**

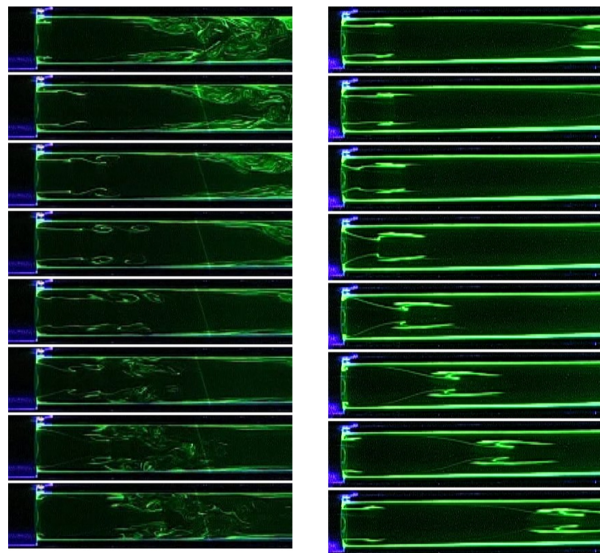
CFD in idealised stenosed vessels – see Poster by Griffith et al.



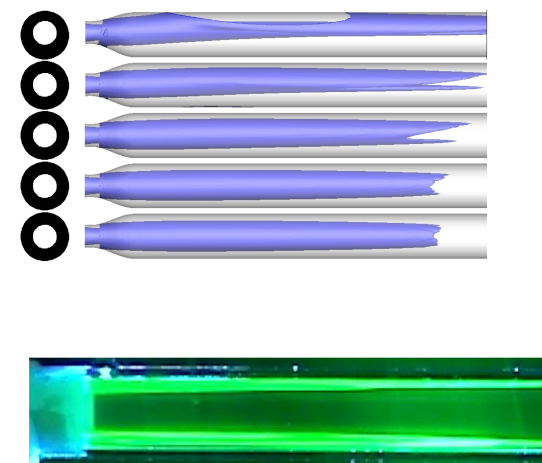
Steady inflow



Pulsed inflow



Eccentric stenosis



Griffith, M.D., Leweke, T., Thompson, M.C. & Hourigan, K. 2008 Steady inlet flow in stenotic geometries: convective and absolute instabilities. *Journal of Fluid Mechanics* **616**, 111-133.

Griffith, M.D., Leweke, T., Thompson, M.C. & Hourigan, K. 2009 Pulsatile flow in stenotic geometries: flow behaviour and stability. *Journal of Fluid Mechanics* **622**, 291-320.

Griffith, M.D., Thompson, M.C., Leweke, T. & Hourigan, K. 2010 Convective instability in steady stenotic flow: optimal transient growth and experimental observation. *Journal of Fluid Mechanics* **655**, 504-514.

Outline of the Presentation

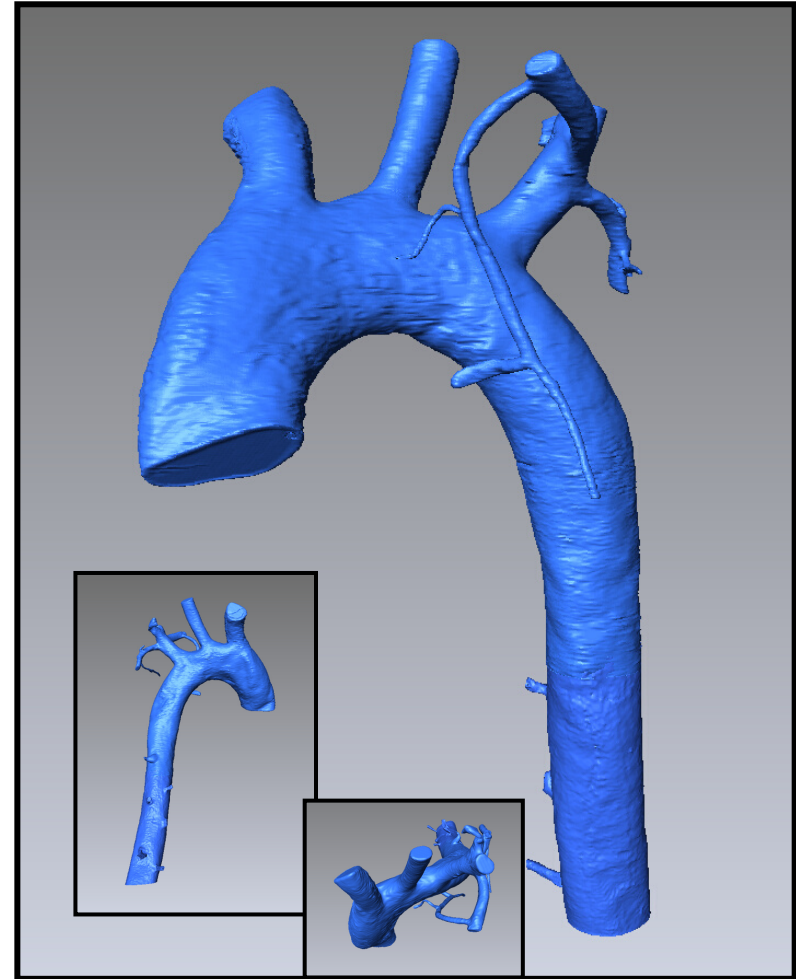
- **Context of current research**
- **Atherosclerosis overview**
- **Computed Tomographic X-ray Velocimetry**
 - Synthetic: Stenosis**
 - In vitro: Thrombi**
 - In vivo: Heart**
- **CFD**
 - Idealised stenoses**
 -  **Mouse aorta**
- **Conclusions**

CFD in the model from a mouse

Mouse aorta geometry



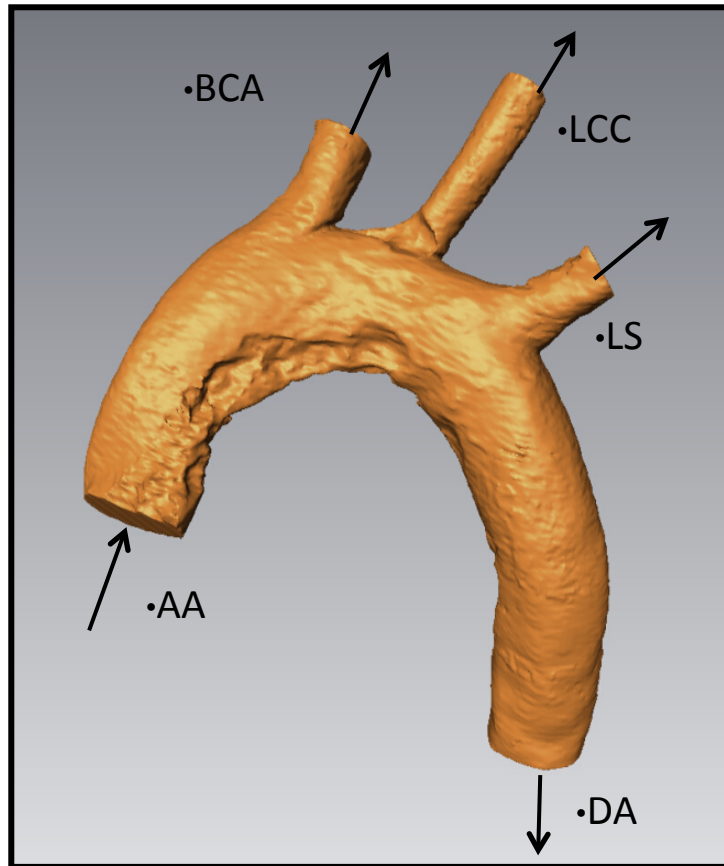
Two-dimensional slice in Avizo showing a section of the aortic arch of an Apo E-deficient mouse. The image has been segmented, vessel (blue), plaque (green) and lumen (brown).



Mouse aorta geometry.



Vessel geometry: CAD

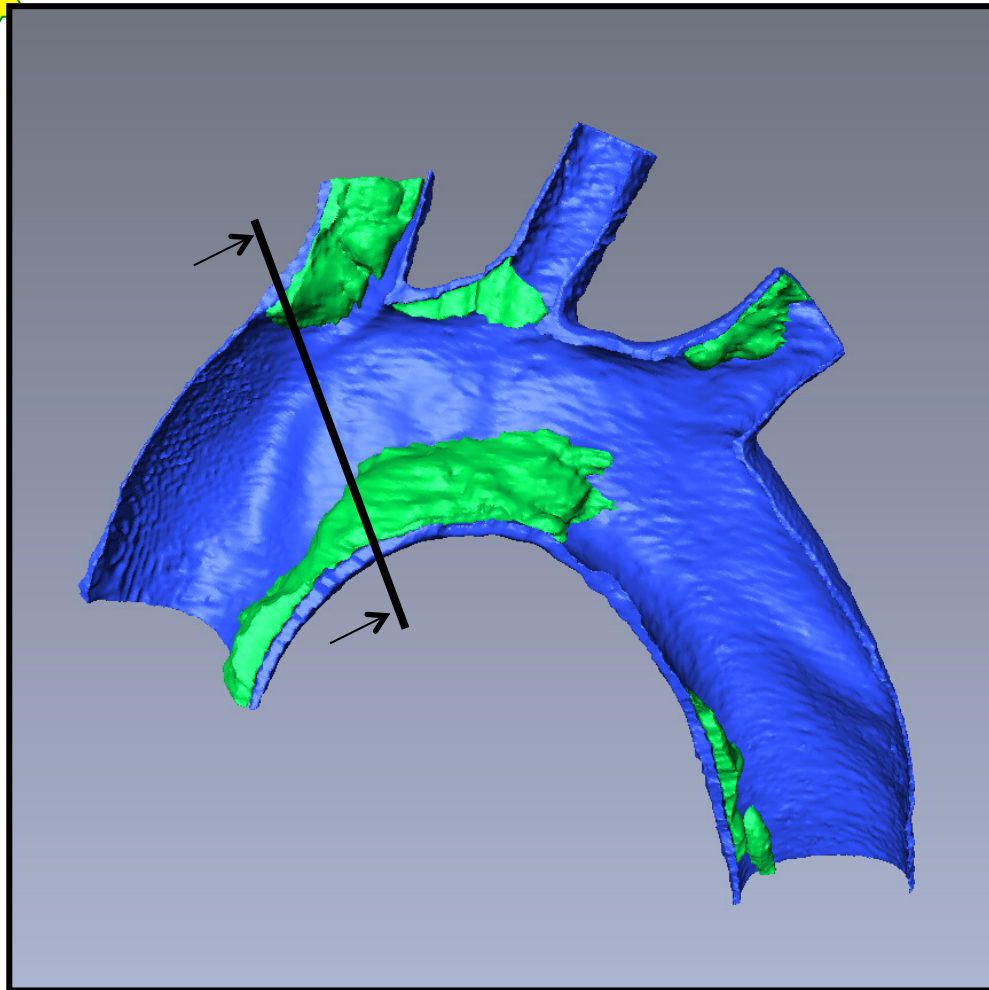


	Ascending Aorta (AA)	Brachiocephalic Artery (BCA)	Left Common Carotid Artery (LCC)	Left Subclavian Artery (LS)	Descending Aorta (DA)
Diameter, D (mm)	0.83	0.56	0.33	0.38	0.82
Flow Rate, Q (mL/min) [7]	12.02	1.87	1.35	1.06	7.74
Reynolds Number, Re	95	22	27	18	62

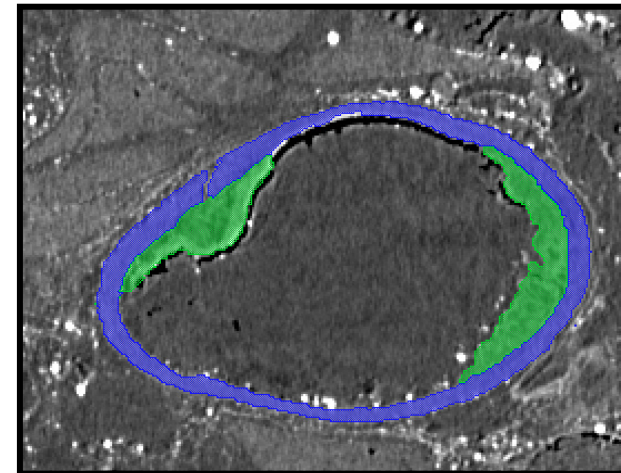
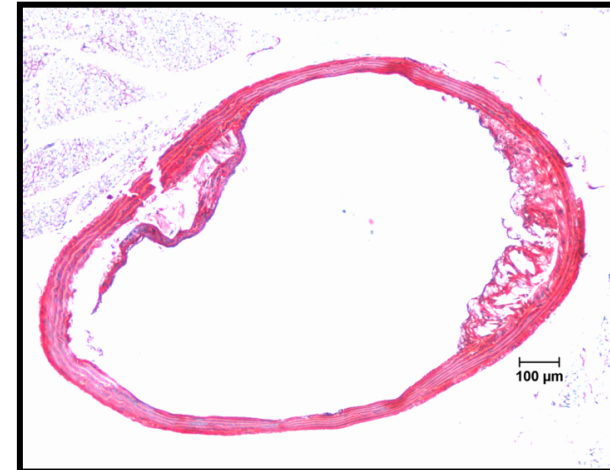
The lumen of the vessel which has been segmented and cropped, ready for meshing in ICEM CFD.

Dimensions of the aorta and its main branches measured from the reconstructed three-dimensional geometry. The flow rates used as boundary conditions were obtained from Huo et al. (2008).

Plaque locations



Section of the ApoE-deficient mouse aorta demonstrating the location of the plaques (green) on the inner curvature of the aorta and on the upstream side of the three main branch points.

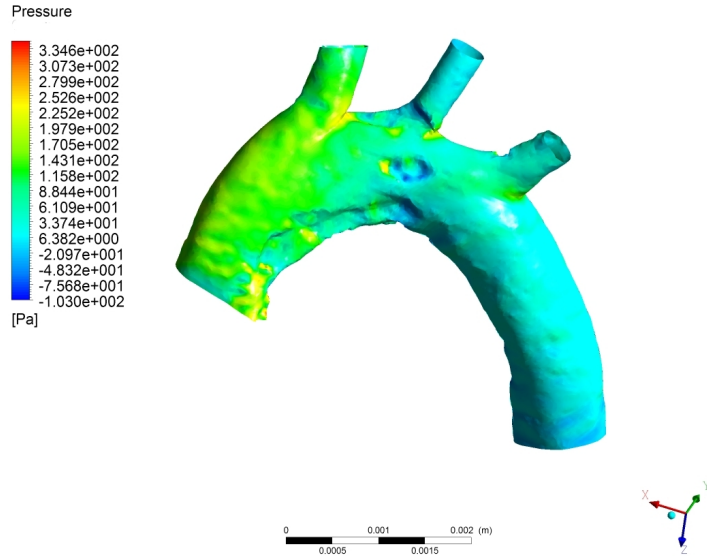


a) Histology of a cross-section of the AA and BCATwo plaques are visible, one with a well defined fibrous cap (provided by J. Armitage).
b) Related two-dimensional slice in Avizo with the wall and plaque segmented.

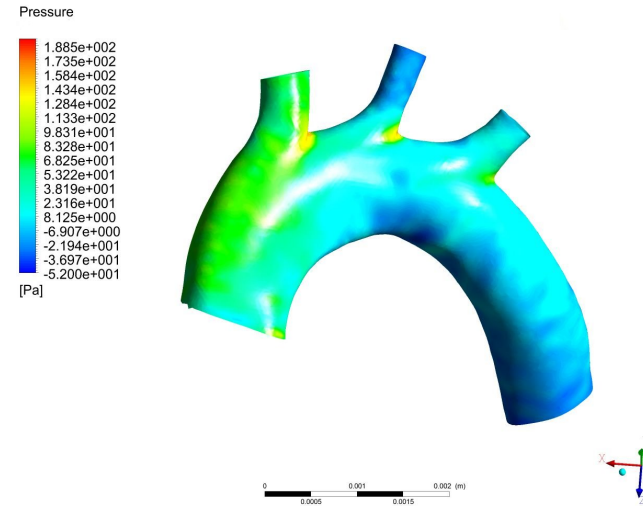
Surface pressure



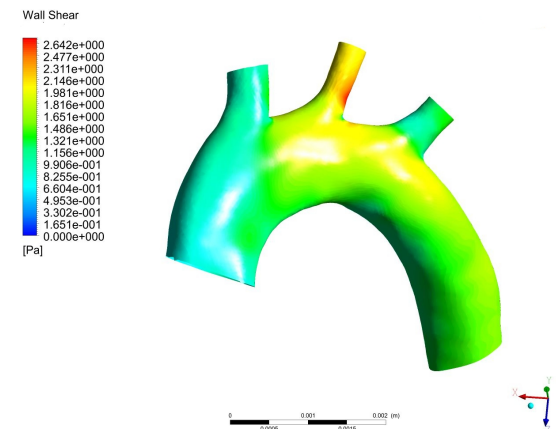
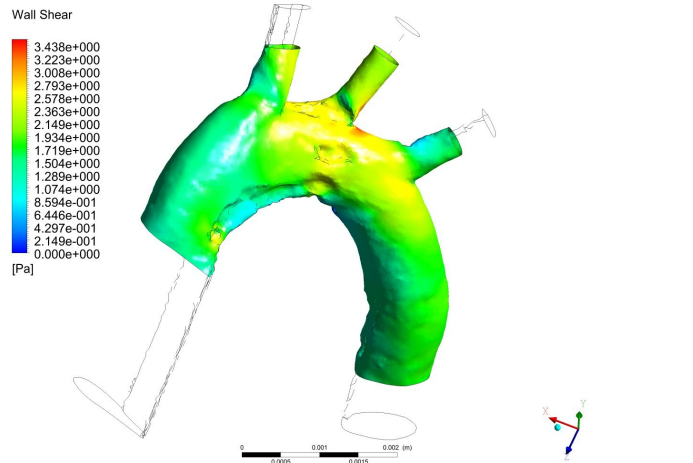
Plaque present



Plaque "removed"



Wall shear stress



Wall shear stress (exaggerated contours)

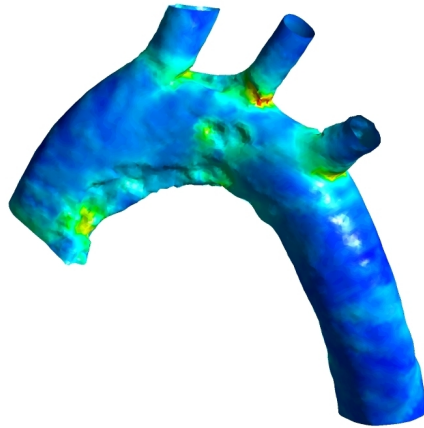
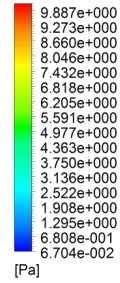


Plaque present

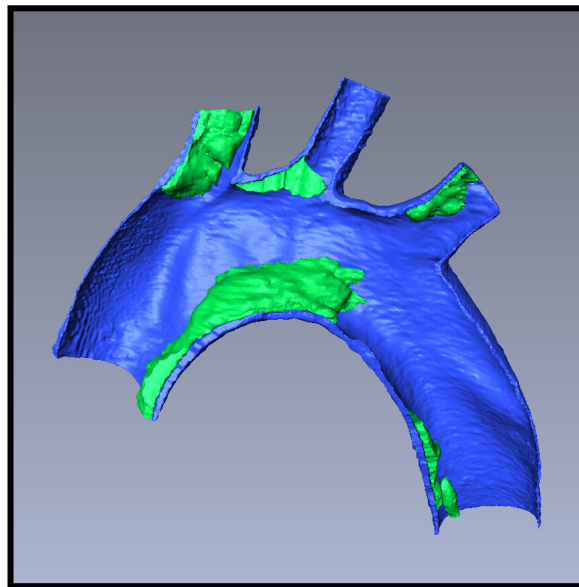
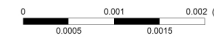
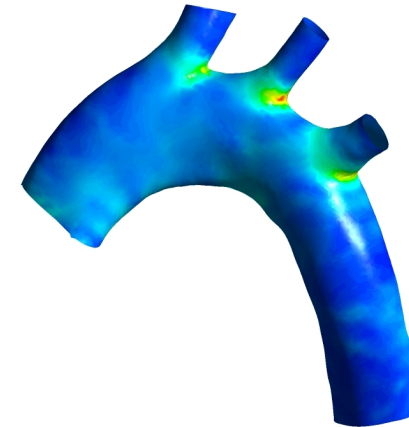
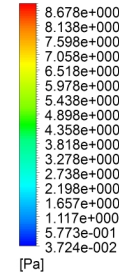


Plaque "removed"

WSShuo



WSShuo



c.f. plaque locations

Outline of the Presentation

- **Context of current research**
- **Atherosclerosis overview**
- **Computed Tomographic X-ray Velocimetry**

Synthetic: Stenosis

In vitro: Thrombi

In vivo: Heart

- **CFD**

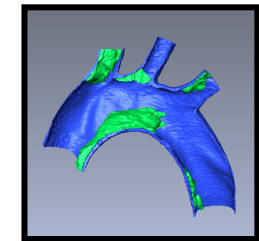
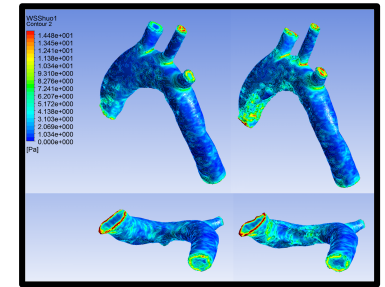
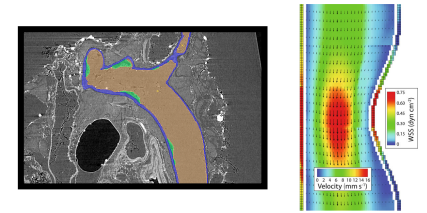
Idealised stenoses

Mouse aorta

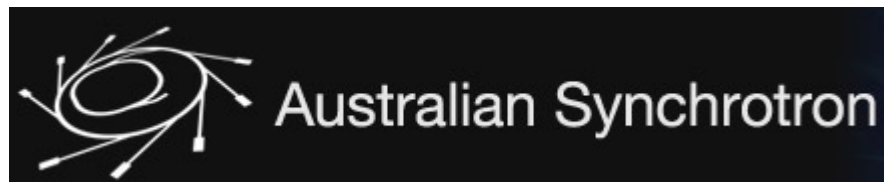
-  • **Conclusions**

Conclusions

- X-ray CT Velocimetry + CFD can be used to determine tissue geometries, blood flow velocity fields, WSS, etc
- In accordance with the literature, plaques were found to develop on the inner curvature of the aortic arch and the upstream side of the main branches in Apo E-deficient mice
- The WSS results are consistent with those found by others in arteries without plaque
- As an extension to previous work, the flow around plaque has been investigated, with altered WSS distributions observed
- Work is in progress looking at the deformation of the arterial wall and plaque by incorporating the elastic properties of the materials (coupled solver, AFM, Biodynamic tester)
- X-ray CT+Velocimetry + *in vivo*, functional nanoparticles will also be investigated
- Part of a broader program in lung/brain/cardiovascular, imaging, cfd, nanotechnology, drug delivery, devices,



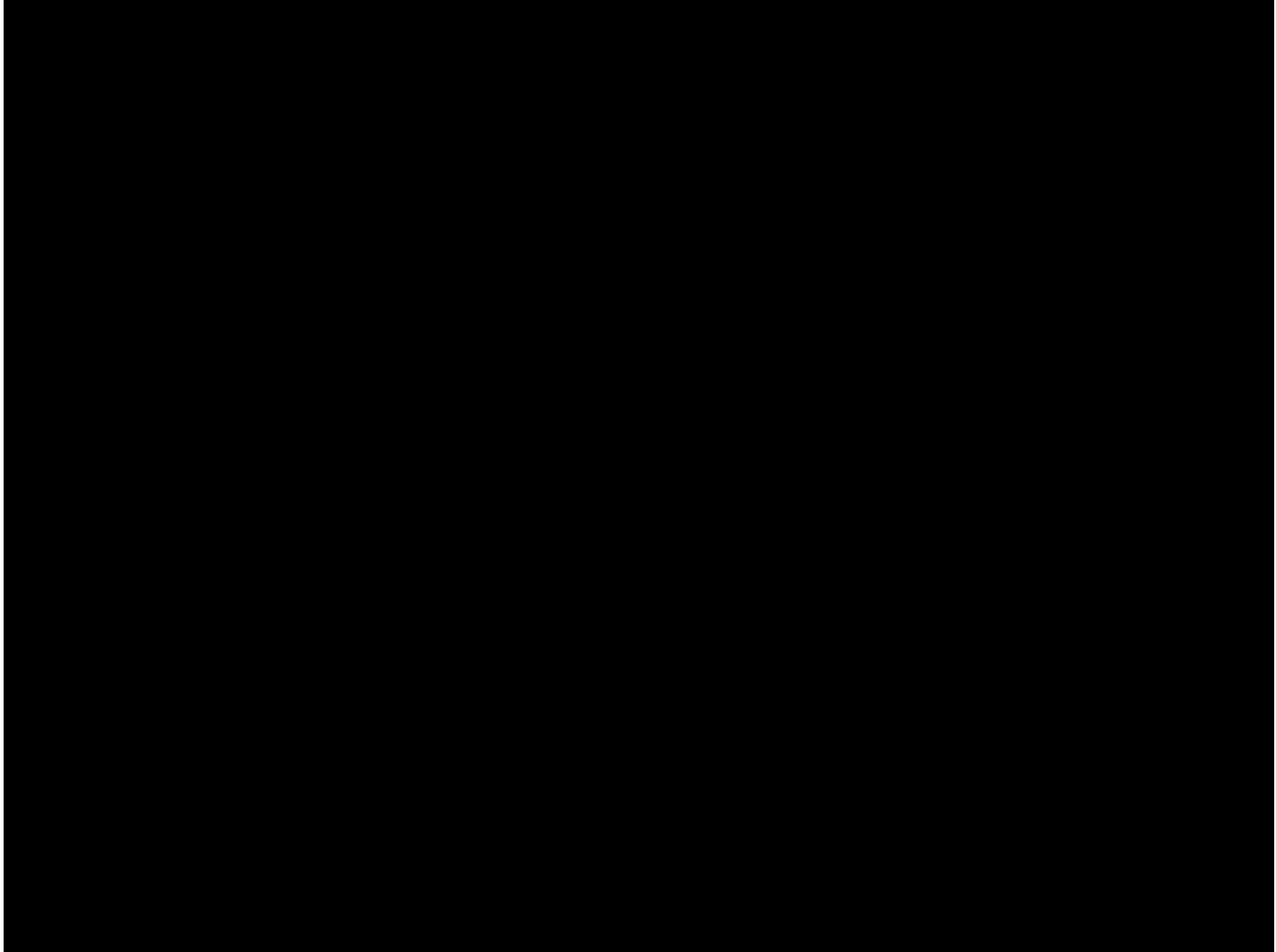
Acknowledgements



Swiss Light Source

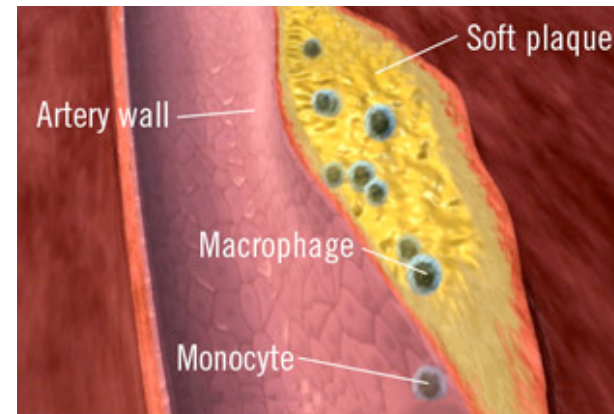
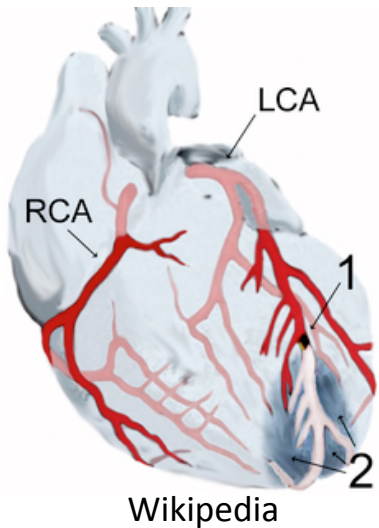
Multidisciplinary research – one needs to wear many hats





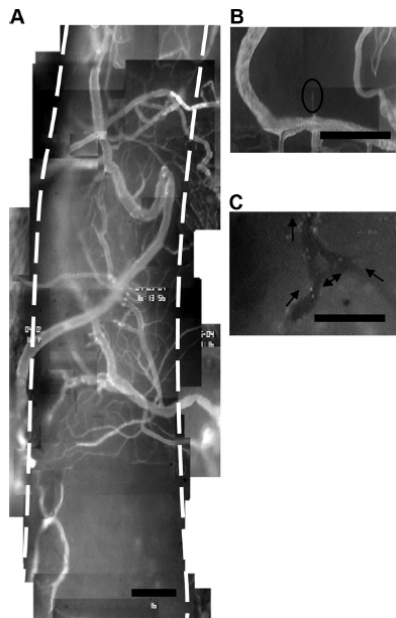
Myocardial Infarction

- Results from the interruption of blood supply to a part of the heart, causing heart cells to die
- Most commonly due to occlusion (blockage) of a coronary artery following the rupture of a vulnerable atherosclerotic plaque
- vulnerable plaque rupture causes as many as 85% of all heart attacks.



© 2007 Prescient Medical, Inc. All rights reserved.

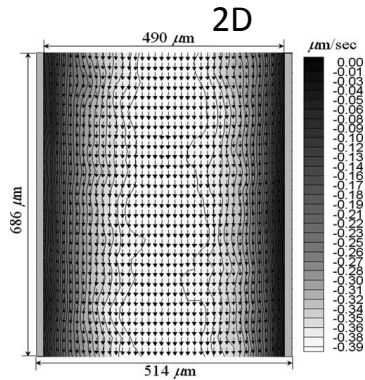
- As cholesterol are absorbed by the artery, proteins called "cytokines" are released. The cytokines cause inflammation and make the arterial wall sticky, resulting in the attraction of immune-system cells to the area. The immune-system cells are called "monocytes."
- When the monocytes enter the arterial wall, they differentiate into "macrophage" cells and begin to absorb fat droplets. Over time, these fat-filled cells form a plaque – what researchers now call "vulnerable plaque."



Microvessels in atherosclerosis as important entry pathways for leukocytes to lesions.

Eriksson, Circulation 2011, 124:2129-2138

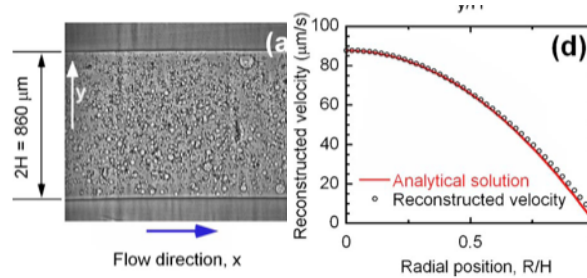
Computed Tomographic X-ray Velocimetry of Biofluid Flows



Kim GB, Lee SJ (2006) *X-ray PIV measurements of blood flows without tracer particles*. Exp Fluids 41:195-2006



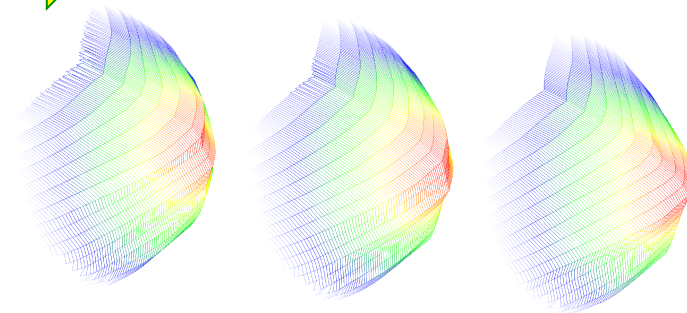
Axisymmetric



Im KS, Fezzaa K, Wang YJ, Liu X, Wang J, Lai MC (2007) *Particle tracking velocimetry using fast X-ray phase-contrast imaging*. Appl Phys Lett 90: Artn 091919



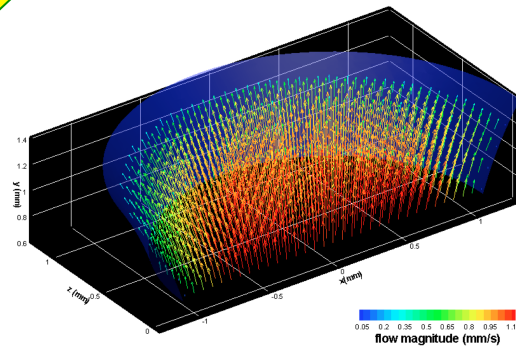
3D, planar symmetry assumed



Fouras A, Disting J, Lewis R, Hourigan K (2007) *Three-dimensional synchrotron X-ray particle image velocimetry*. J Appl Phys 102: Artn 064916



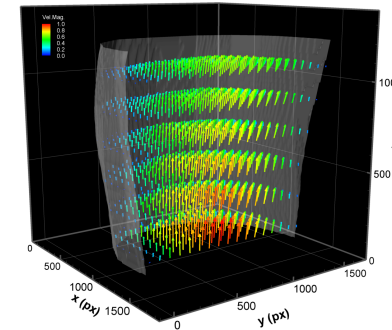
Axisymmetric



Irvine SC, Paganin DM, Jamison A, Dubsky S, Fouras A (2010) *Vector tomographic X-ray phase contrast velocimetry utilizing dynamic blood speckle*. Opt Express 18:2368-2379



3D, Axisymmetric

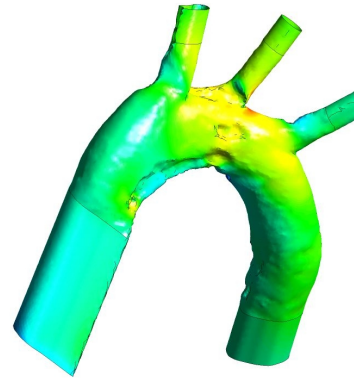
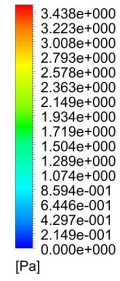


Dubsky, S., R.A. Jamison, S.C. Irvine, K.K.W. Siu, K. Hourigan, and A. Fouras, *Computed tomographic X-ray velocimetry*. Applied Physics Letters, 2010. 96(2)

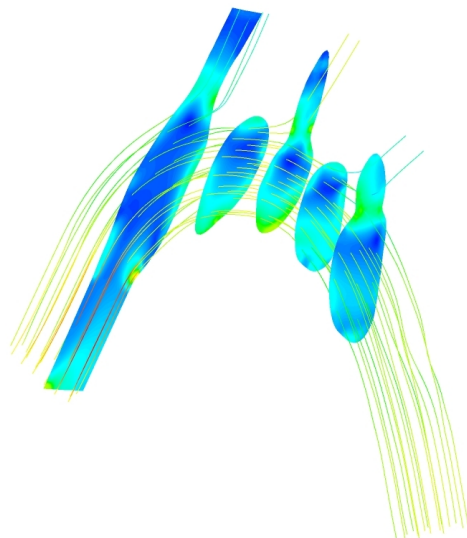
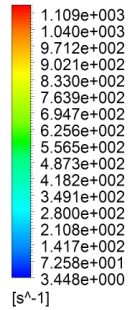
	Ascending Aorta (AA)	Brachiocephalic Artery (BCA)	Left Common Carotid Artery (LCC)	Left Subclavian Artery (LS)	Descending Aorta (DA)
Flow Rate, Q (mL/min) [7]	12.02	1.87	1.35	1.06	7.74
Diameter, D (mm) [7]	1.3	0.85	0.64	0.64	-
Reynolds Number [7]	61	14	14	11	-
Experimental Diameter, D (mm)	0.83	0.56	0.33	0.38	0.82
Experimental Reynolds Number, Re	95	22	27	18	62

Table 1: Comparison of diameter and Reynold's number from experimental findings and the values stated in Huo et al (2008). The experimental dimensions of the aorta and its main branches were measured from the reconstructed three-dimensional geometry. The flow rates used as boundary conditions were obtained from Huo et al (2008). In the Reynolds number calculations ($Re = \rho Q D / (6 \times 10^6 A \mu)$), Q is the flow rate, A is the surface area and D is the equivalent diameter of the artery. The density (ρ) is 1235 kg/m^3 and the dynamic viscosity (μ) is 0.004 Pa.s .

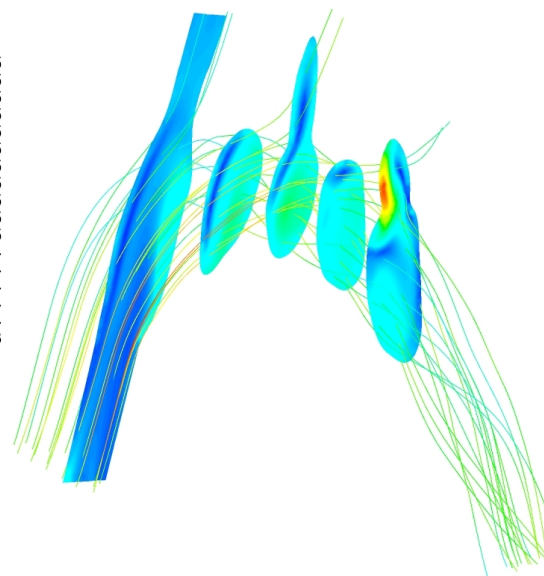
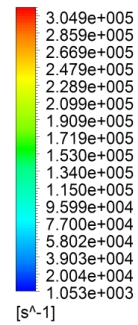
Wall Shear

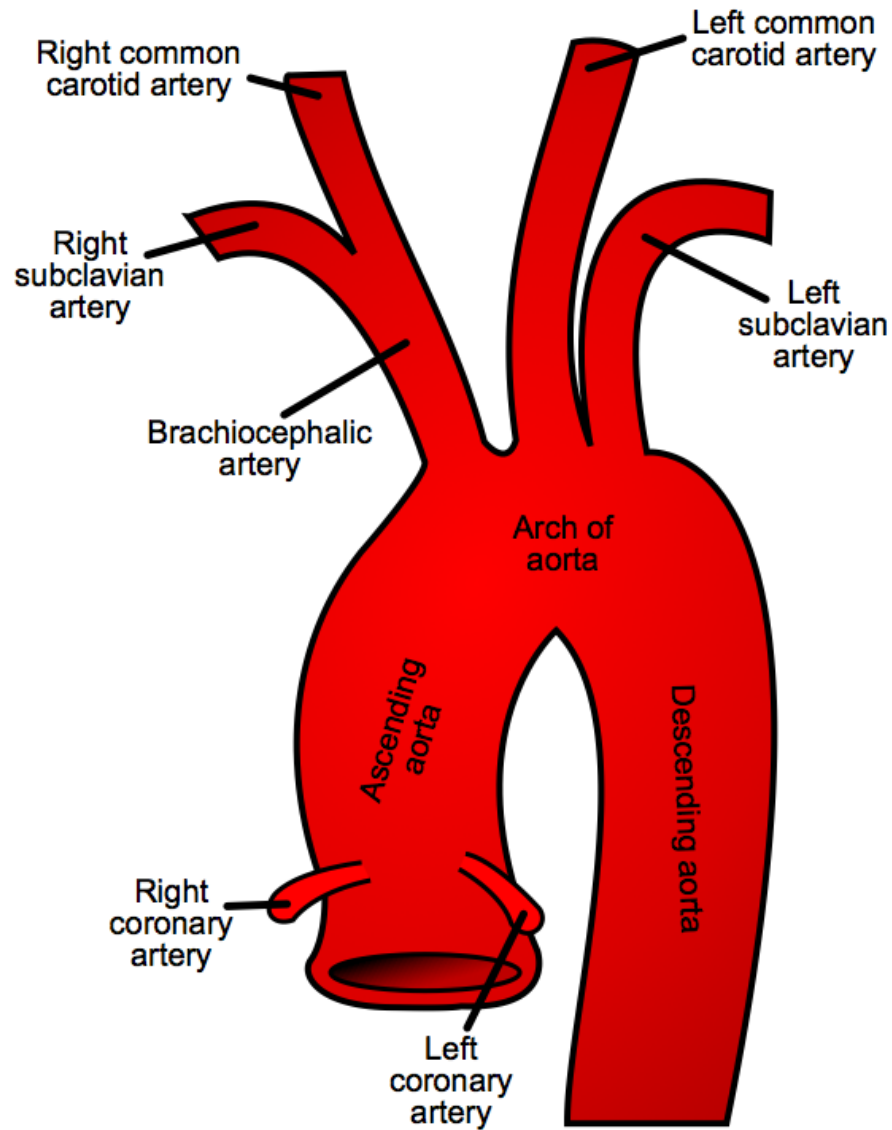


Vorticity



Vorticity





•<http://upload.wikimedia.org/wikipedia/commons/thumb/e/e6/Gray506.svg/250px-Gray506.svg.png>