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## A Local Search Method for Pattern Classification\*

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**Abstract.** We present a new method to compute depth-three threshold circuits for pattern classification problems. The first layer of the circuits is calculated from a sample set  $S$  of the classification problem by a local search strategy that minimises the error on  $S$  for each individual gate. The local search is based on simulated annealing with the logarithmic cooling schedule  $c(k) = \Gamma / \ln(k + 2)$ . The parameter  $\Gamma$  depends on  $S$  and the neighbourhood relation is determined by the classical Perceptron algorithm. The approach is applied to the recognition of focal liver tumours.

### 1 Introduction

The paper describes method of computing depth-three threshold circuits for pattern recognition purposes. The approach is applied to focal liver tumour recognition, where the CT images are classified by the threshold circuit without any pre-processing. From a general point of view, the threshold circuits are designed for binary classifications of points from an  $n$ -dimensional space. This problem has been studied for a long time and is closely related to algorithms solving systems of linear inequalities.

AGMON proposed in 1954 [2] a simple iteration procedure to find solutions of linear inequalities  $l^j(\vec{z}) = \vec{a}^j \cdot \vec{z} + b^j \geq 0$ ,  $j = 1, \dots, m$ . In pattern recognition, AGMON's method became popular as the classical Perceptron algorithm [16]. For sets  $S$  of  $n$ -dimensional vectors  $\vec{x}$  that are separable by a linear threshold function into "positive" and "negative" examples, MINSKY and PAPERT [13] proved the following convergence property: If  $\vec{w}^*$  is a unit vector solution to the separation problem, then the Perceptron algorithm converges in at most  $1/\sigma^2$  iterations, where  $\sigma := \min_{[\vec{x}, \eta] \in S} |\vec{w}^* \cdot \vec{x}|$ ,  $\eta \in \{+, -\}$ . The parameter  $\sigma$  can be exponentially small in terms of the dimension  $n$ .

In general, the simple Perceptron algorithm performs well even if the sample set is not consistent with any weight vector  $\vec{w}$  of linear threshold functions,

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see [9]. For our problem of CT-image classification, one can hardly assume that positive and negative examples are separable by a single linear threshold function. In order to reduce the classification error, we try to compute a bounded-depth circuit consisting of linear threshold functions. The threshold functions, in particular the gates of the first level, are determined by a learning procedure from positive and negative examples  $S$  of the classification problem.

HÖFFGEN [12] has shown that finding a linear threshold function that minimises the number of misclassified examples is NP-hard in the case of arbitrary sample sets. In our approach, we utilise a combination of logarithmic simulated annealing and the Perceptron algorithm for this computationally hard minimisation problem. The combination has been studied in [6] for samples generated by non-linear threshold functions. The approach belongs to the class of local search methods [1].

To our knowledge, the first paper on learning-based methods applied to X-ray diagnosis was published by ASADA ET AL. [7]. Since then, the research has been concentrating on using commercially available neural networks for medical image classification [8, 10, 14, 15, 18].

In a number of papers, feature extraction is used in learning-based classification methods [14, 17]. In [14], for example, a high classification rate of nearly 98% is reported, where the Wisconsin breast cancer diagnosis (WBCD) database of 683 cases is taken for learning and testing. The approach is based on feature extraction from image data and uses nine visually assessed characteristics for learning and testing. Among the characteristics are the uniformity of cell size, the uniformity of cell shape, and the clump thickness.

The paper continues the research from [3]. In the present paper, we describe the computation of depth-three threshold circuits from positive and negative examples that are designed to recognise focal liver tumours. The input are fragments of CT images of size  $119 \times 119$  with an 8 bit grey scale in DICOM standard format [11]. Therefore, the input size is  $n = 14161$  and the input values range from 0 to 255. For the learning procedure, we used 400 positive (focal liver tumours) and 400 negative (normal liver tissue) examples. The circuits were tested on  $100 + 100$  examples (different from the learning set), and we obtained a correct classification of about 94%.

## 2 A Simulated Annealing-Based Heuristic

We assume that rational numbers are represented by pairs of binary tuples of length  $d$  and denote the set of linear threshold functions by

$$\mathcal{F} := \bigcup_{n \geq 1} \mathcal{F}_n, \text{ where } \mathcal{F}_n = \left\{ f(\vec{x}) : f(\vec{x}) = \sum_{i=1}^n w_i \cdot x_i \geq \vartheta_f \right\},$$

where  $w_i$  and  $x_i$  are equal to  $\pm(p_i, q_i)$  for  $p_i, q_i \in \{0, 1\}^d$ .

The functions from  $\mathcal{F}$  are used to design single-output circuits  $\mathcal{C}$  of threshold functions: A circuit  $\mathcal{C}$  is defined by the underlying acyclic directed graph  $\mathcal{G} = [E, V]$ ,  $E \subset V \times V$ . The graph  $\mathcal{G}$  has  $n$  input nodes labelled by variables  $x_1$ ,

$\dots, x_n$ , and  $|V| - n$  nodes  $v_f$  labelled by threshold functions  $f \in \mathcal{F}$ , where the number of incoming edges of  $v_f$  has to be consistent with the number of variables of  $f$ . Finally, one  $v_f$  is chosen as the output  $v_{out}$  of  $\mathcal{C}$ .

The depth of  $\mathcal{C}$  is the maximum number of edges on a path from an input node  $x_i$  to the output node  $v_{out}$ . The nodes that are not input nodes are called gates. The function  $F(\mathcal{C})$  computed by  $\mathcal{C}$  is defined as follows: The gates of the first level output 1 or 0 depending on whether or not  $\sum_{i=1}^n w_i \cdot x_i \geq \vartheta_f$ . In the same way, the gates at higher levels have Boolean outputs only. Therefore, when all paths from input nodes to  $v_{out}$  are of the same length, the gates at level 2, 3, .. do compute Boolean threshold functions. Thus, we have  $F(\mathcal{C}) : \{0, 1\}^{n \cdot d} \rightarrow \{0, 1\}$ .

In the present paper, the maximum depth of  $\mathcal{C}$  is three; circuits of depth one are simply the elements of  $\mathcal{F}_n$ , and in Section 3 we consider circuits of depth two and three, respectively. In our application, each of the threshold functions from the first level is equally important for the overall classification result of the depth-three circuit. Therefore, the weights at the input lines of second level functions (gates) can be normalised to the value 1 and only the threshold values depend on the sample set  $S$ .

For a given sample set  $S$ , we assume  $S = \{[\vec{x}, \eta]\}$  for  $\eta \in \{+, -\}$  and  $\vec{x} = (x_1, \dots, x_n)$  where  $x_i = (p_i, q_i)$ ,  $p_i, q_i \in \{0, 1\}^d$ . Furthermore, we consider a particular number  $n$  of variables only and we take the set  $\mathcal{F} := \mathcal{F}_n$  as the configuration space.

The objective of our optimisation procedure is to minimise the number  $|S\Delta f|$  of misclassified examples,  $S\Delta f := \{[\vec{x}, \eta] : f(\vec{x}) < 0 \& \eta = + \text{ or } f(\vec{x}) > 0 \& \eta = -\}$ . The objective function is defined by  $\mathcal{Z}(f) := |S\Delta f|$ , and  $\mathcal{F}_{\min}(S)$  denotes the set of minimum-error solutions.

Given  $f = \sum_{i=1}^n w_i \cdot x_i \geq \vartheta_f$ , the neighbourhood relation  $\mathcal{N}_f$  is suggested by the Perceptron algorithm [16] and defined by

$$w_i(f') := w_i - y_j \cdot x_{ij} / \sqrt{\sum_{i=1}^n w_i^2}, \quad j \in \{1, 2, \dots, m\}, \quad (1)$$

for all  $i$  simultaneously and for a specified  $j$  that maximises  $|y_j - \vartheta_f|$ , where  $y_j = \sum_{i=1}^n w_i \cdot x_{ij}$ . The threshold  $\vartheta_{f'}$  is equal to  $\vartheta_f + y_j / \sqrt{\sum_{i=1}^n w_i^2}$ .

Given a pair  $[f, f']$ ,  $f' \in \mathcal{N}_f$ , we denote by  $G[f, f']$  the probability of generating  $f'$  from  $f$  and by  $A[f, f']$  the probability of accepting  $f'$  once it has been generated from  $f$ .

To speed up the local search for minimum error solutions, we take a non-uniform generation probability where the transitions are forced into the direction of the maximum deviation. We used this approach before [4] in the context of equilibrium computations. The non-uniform generation probability

is derived from the Perceptron algorithm: For the current hypothesis  $f$  we set:

$$U(\vec{x}) := \begin{cases} -f(\vec{x}), & \text{if } f(\vec{x}) < \vartheta_f \text{ and } \eta(\vec{x}) = +, \\ f(\vec{x}), & \text{if } f(\vec{x}) \geq \vartheta_f \text{ and } \eta(\vec{x}) = -, \\ 0, & \text{otherwise.} \end{cases} \quad (2)$$

For  $f' \in \mathcal{N}_f$  we set  $G[f, f'] := U(\vec{x}) / \sum_{\vec{x} \in S_{\Delta_f}} U(\vec{x})$ . Thus, preference is given to the neighbours that maximise the deviation. Now, our heuristic can be summarised in the following way:

1. The initial hypothesis is defined by  $w_i = 1$ ,  $i = 1, 2, \dots, n$  and  $\vartheta = 0$ .
2. For the current hypothesis, the probabilities  $U(\vec{x})$  are calculated; see (2).
3. To determine the next hypothesis  $f_k$ , a random choice is made among the elements of  $\mathcal{N}_{f_{k-1}}$  according to the definition of  $G[f, f']$ .
4. When  $\mathcal{Z}(f_k) \leq \mathcal{Z}(f_{k-1})$ , we set  $A[f_{k-1}, f_k] := 1$ .
5. When  $\mathcal{Z}(f_k) > \mathcal{Z}(f_{k-1})$ , a random number  $\rho \in [0, 1]$  is drawn uniformly.
6. If  $A[f_{k-1}, f_k] := e^{-(\mathcal{Z}(f_k) - \mathcal{Z}(f_{k-1}))/c(k)} \geq \rho$ , the function  $f_k$  is the new hypothesis. Otherwise, we return to 3 with  $f_{k-1}$ .
7. The computation is terminated after a predefined number of steps  $K$ .

Hence, instead of following unrestricted increases of the objective function, our heuristic tries to find another "initial" hypothesis when the difference of the number of misclassified examples is too large.

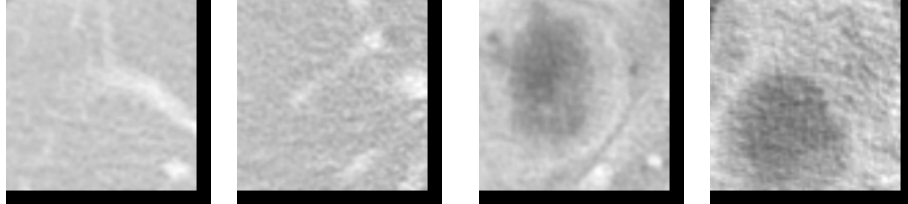
The crucial parameter  $c(k)$  is defined by  $c(k) = \Gamma / \ln(k + 2)$ ,  $k = 0, 1, \dots$ . The parameter  $\Gamma$  depends on the underlying energy landscape. When  $\Gamma$  is larger than or equal to the maximum value of the minimum escape depth from local minima, one can prove the convergence to minimum-error solutions for a more general neighbourhood relation that provides the reversibility of the configuration space. In this case, the convergence analysis from [5] indicates a time complexity of roughly  $n^{\Gamma + O(1)}$ , i.e., after  $n^{\Gamma} + \log^{O(1)}(1/\delta)$  transitions the confidence that a minimum-error threshold function has been computed is larger than  $1 - \delta$ .

### 3 Implementation and Results

The heuristic was implemented in C++ and we performed computational experiments on SUN Ultra 5/333 workstations with 128 MB RAM. In the experiments, we used fragments of CT images of size  $119 \times 119$  with 8 bit grey levels. From 400 positive (with focal liver tumours) and 400 negative examples (normal tissue) several independent hypotheses of the type  $w_1 \cdot x_1 + \dots + w_n \cdot x_n \geq \vartheta$  were calculated for  $n = 14161$ . We tested the hypotheses simultaneously on 100 positive and 100 negative examples. The test examples were not presented to the algorithm during the training phase.

In Figure 1 and Figure 2, typical representatives of negative and positive examples are shown. It is important to note that the CT examinations were

performed with comparable imaging parameters, as can be seen from the brightness and contrast of the examples.



Normal liver tissue: Negative examples.

Focal liver tumour: Positive examples.

**Figure 1**

**Figure 2**

Table 1 summarises typical results for circuits of depth 1, ..., 3 (Due to the long run-time, only a few experiments have been performed so far, and therefore it is difficult to present average values). Each function (gate) from the first level was trained on a random choice of 100+100 examples out of 400+400 examples. The examples were learned with zero error after about 25000 to 35000 changes of the hypothesis for a single linear threshold function (gate from the first level). The results are for  $\Gamma = 60$ .

The depth-three circuit consists of three sub-circuits of depth two, where each depth-two circuit has 11 threshold functions at the first layer. The output gate of the depth-three circuit is a simple majority function. Thus, the depth-three circuit consists of  $3 \cdot (11 + 1) + 1 = 37$  linear threshold functions (gates). Each of the threshold functions of the first level (i.e., each input gate) has  $n = 14161$  inputs, i.e., the total number of input lines that are connected to the 14161 input nodes (pixel values) is  $3 \cdot 11 \cdot 14161 = 467313$ .

Depth of Circuits	Learning Run-Time	Errors on		Errors on		Percentage of Errors
		POS	NEG	T_POS	T_NEG	
1	$\approx 275$ min	0	0	32	36	34%
2	$\approx 3000$ min	0	0	13	17	15%
3	$\approx 9000$ min	0	0	4	8	6%

**Table 1**

The test on a single image from the 100 + 100 test examples is performed within a few seconds. The parameter settings " $\Gamma = 60$ ", "100 out of 400", and "11" for the number of gates at the first layer of depth-two (sub-)circuits were determined by computational experiments.

We think that one reason for the good classification rate of 94% is the homogeneous imaging technique that was used to obtain the training and test material.

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