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CrossTalk proposal:

Blood Flow Pulsatility in LVAD Patients is essential to Maintain Normal Brain Physiology

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1 Biographies

Eric J. Stöhr trained in exercise science in Germany and
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joined Columbia University Irving Medical Center in 2016 where he studies advanced heart
failure patients. His research aims at understanding the interaction between the heart muscle
dynamics and arterial function in health and disease. Joshua Z. Willey is a vascular neurologist
with a research interest in cerebrovascular physiology and disease with mechanical circulatory
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Columbia University Medical Center where he is now an Assistant Professor of Neurology.

21 For the first time in history, some humans live without a palpable pulse (Purohit *et al.*, 2018). This remarkable physiology is the consequence of surgical implantation of a continuous-flow left 22 ventricular assist device (CF-LVAD) in patients with end-stage heart failure. This CF-LVAD 23 creates a low oscillatory blood flow profile in the aorta that results in significantly reduced 24 pulsatility in all arterial compartments (Castagna et al., 2017, Figure 1A and 1B). Despite 25 26 remarkable gains in quality of life and longevity, complications that affect not only morbidity 27 such as gastrointestinal bleeding, but also mortality such as strokes, are still prevalent in CF-28 LVAD patients. Low pulsatility has been proposed as a major culprit in contributing to these 29 adverse events (Mancini & Colombo, 2015; Goldstein et al., 2018). In this CrossTalk, we present the current arguments in favour of maintaining an appropriate amount of arterial pulsatility, in 30 particular in the cerebral circulation, to lower risk in these patients. 31

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33 Cerebral microcirculation and O₂ kinetics

A macro-circulatory link between cardiac output, aortic stiffness and arterial pulsatility with the 34 brain is well-established (Mitchell et al., 2011; Jefferson et al., 2015). At the level of the 35 microcirculation, it is thought that the healthy circulation already presents with absence of pulse 36 pressure (O'Rourke & Hashimoto, 2007), and hence CF-LVADs would not create a different 37 environment for gas exchange from normal physiology. However, even in healthy individuals, 38 39 measurements of arteriolar haemodynamics have revealed pulsatile patterns (Rappaport et al., 1959; Shore, 2000). An important implication is that a pulsatile velocity profile entails that 40 cerebral transit time (CTT) slows in the diastolic phase and facilitates the oxygen gradient for 41 gas exchange. In CF-LVAD patients, the increased diastolic blood velocity may result in an 42 overall elevated mean blood velocity (Brassard et al., 2011; Castagna et al., 2017, and Figure 43

1B), thereby impairing oxygen kinetics (Wardlaw et al., 2002). However, data on absolute blood 44 velocities are scarce, or their interpretation currently lacks confidence because the assessment of 45 46 cerebral blood velocities, even in the pre-arteriolar circulation, has typically not been performed with the necessary angle correction of the Doppler signal. Whatever the real O₂ kinetics in CF-47 LVAD, it is known that cerebral blood flow is also regulated for reasons other than O_2 48 49 requirements (Mintun et al., 2001). Thus, the low pulsatile, diastolic-dominant haemodynamics of CF-LVAD impact on cerebral artery properties beyond gas exchange, as discussed in the 50 51 following paragraphs.

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53 Cerebral auto-regulation

54 Cerebral autoregulation has been proposed to take effect across a more narrow range of perfusion pressure than previously thought (Willie et al., 2014). Consequently, the low systolic blood 55 pressure and low-to-normal mean arterial pressure coupled with a normal cardiac output mean 56 57 that CF-LVAD patients may find themselves on an unusual point of the perfusion-cerebral blood flow (CBF) curve, with high flow into a low-resistance cerebral circulation (Cornwell et al., 58 2014). The high-flow low-resistance is directly caused by the low-pulsatile haemodynamics of 59 CF-LVAD. Notwithstanding, cerebral auto-regulation may be preserved in CF-LVAD patients 60 61 (Ono et al., 2012; Cornwell et al., 2014), independent of end-tidal CO₂ concentrations (Cornwell et al., 2014). However, some remaining differences to normal brain physiology can be noted. For 62 instance, the variance in CBF was most similar between healthy individuals and CF-LVAD 63 patients, while patients with pulsatile devices responded significantly differently to a sit-to-stand 64 65 challenge (Cornwell et al., 2014). These intriguing findings may indicate a meaningful role of added pulsatility in the context of LVAD and justify a more detailed investigation into the 66

dynamics of perfusion pressure (i.e. pulse pressure) and cerebral autoregulation in the setting of low absolute pressures (Ono *et al.*, 2017). Rather than being disturbed itself, the maintained cerebral autoregulation in CF-LVAD may cause a reduction in pulsatility since the total flow is already high.

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72 Endothelial function, bleeding and aortic stiffness

Pulsatility of *flow* against the cyclical stretch of the arterial wall is a critical contributor to 73 endothelial production of nitric oxide and cardiovascular health (Hahn & Schwartz, 2009). The 74 high occurrence of bleeding events such as GI bleeding and haemorrhagic strokes indicate a 75 primary problem with endothelial integrity. A recent study confirms elegantly that a staggering 76 77 proportion of LVAD patients have cortical microbleeds in a pattern similar to cerebral amyloid angiopathy, a condition with high rates of arteriolar fragility (Yoshioka et al., 2017). 78 Furthermore, reduced pulsatility appears responsible for the marked reduction in endothelial 79 80 nitric oxide bioavailability in CF-LVAD patients when compared to those on support with pulsatile device (Witman et al., 2015). While shear rate has not been measured in the cerebral 81 82 circulation of CF-LVAD patients, it is conceivable that it would be higher than normal in the diastolic phase of the cardiac cycle, a circumstance that, when present in the carotid artery, has 83 been associated with adverse cerebral events in non-LVAD populations (Mutsaerts et al., 2011). 84 In addition, the high diastolic flow likely contributes to increased arterial stiffness observed in 85 CF-LVAD patients by markedly attenuating the normal systolic-diastolic stretch and recoil cycle 86 (Ambardekar et al., 2015; Patel et al., 2017). It is important to underline that in pulsatile 87 88 circulations, aortic stiffness increases the transmission of pulsatility to the periphery, and, if exceeding normal pulsatility, is detrimental to the brain and other end-organs (Webb et al., 89

2012). Paradoxically, this means that the reduced Windkessel effect in CF-LVAD patients 90 because of the larger diastolic flow and increased aortic stiffness might be beneficial in some 91 individuals via a mild augmentation of pulsatile dynamics transmitted to the periphery, which 92 would otherwise be harmful to end-organs. Finally, elegant insight into bleeding-associated 93 complications in CF-LVAD - which may include blood-brain-barrier disruption and cortical 94 95 microbleeds - has been provided by Vincent et al. (2018). These authors showed that the loss of von Willebrand-Factor from the high shear forces within the mechanical device was, at least in 96 part, offset by increased arterial pulsatility, which promoted new vWF release from the 97 98 endothelium. Hence, mild increases in arterial pulsatility may mitigate bleeding risk in CF-LVAD patients. 99

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101 Additional considerations

Two common misconceptions related to CF-LVAD physiology, and specifically pulsatility, deserve attention. First, it is commonly assumed that CF-LVADs should produce perfectly continuous flow if the aortic valve does not open (Floras *et al.*, 2015). This assumption overlooks the role of fluctuations of the intra-ventricular pressure within each cardiac cycle. The resulting changes in pressure-gradient between LVAD inflow and aortic outflow graft creates variability in pump flow between systole and diastole and thereby generates arterial pulsatility (Khalil *et al.*, 2008; Pagani, 2008).

Second, the absolute blood volume in relation to the pulsatility is often ignored. Although pulsatility is typically reduced with a higher LVAD speed, the concomitant increase in cardiac output may have significant effects beyond that of reduced pulsatility. Acutely, a larger flow into the cerebral circulation will result in increased resistance and possibly higher pressure. In any

case, it is important to consider cardiac output in relation to the local peripheral vasodilation and 113 vasoconstriction. Studies examining the effects of pulsatile cardiopulmonary bypass reported that 114 the number of perfused vessels in the microcirculation was increased compared with a 115 continuous-flow circulation (O'Neil et al., 2012; Inamori et al., 2013). Importantly, the authors 116 also reported, "pulsatility resulted in a reduction in the prevalence of pathologic hyper-117 118 dynamically perfused vessels" (O'Neil et al., 2012). This observation strongly supports a role of pulsatility independent of blood volume since the latter was not significantly different between 119 120 pulsatile and continuous-flow bypass.

One final comment relates to the newest generation of CF-LVADs. Whether the recent improvements in outcomes, including the reduced incidence of stroke in HeartMate 3 patients (Mehra *et al.*, 2018), can be attributed to the added pulsatility and the greater load-sensitivity of the device itself – and hence greater intrinsic pulsatile oscillation within one cardiac cycle (Pagani, 2008) – remains to be confirmed. Collectively, the presented evidence suggests that CF-LVAD patients are currently not exposed to a normal brain physiology and that mild increases in arterial pulsatility may be beneficial.

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272 Figures

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Figure 1. The schematic of the continuous-flow left ventricular assist device (CF-LVAD) shows the inflow cannula connection to the LV apex and the anastomosis of the outflow cannula to the ascending aorta (A). Representative pressure and flow profiles in the carotid artery and middle cerebral artery (*highlighted in yellow*) show the significant differences in pulsatility (B). LVAD schematic reproduced with permission from St Jude Medical. (B) was modified from Castagna *et al.* (2017) and was originally distributed under the terms of the Creative Commons Attribution 4.0 International License (http://creativecommons.org/licenses/by/4.0/).



"outflow cannula": blood is redirected into the ascending aorta, where it mixes with blood ejected through the aortic valve (if opening).

"inflow cannula": suction from the LVAD unloads the dilated left ventricle.

