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**INTEGRATED MASTER IN BIOENGINEERING – SPECIALIZATION IN
MOLECULAR BIOTECHNOLOGY**

Moving into advanced nanomaterials.

**Toxicity of TiO₂ nanoparticles immobilized in clay
on human cell line.**

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ABSTRACT

Titanium dioxide nanoparticles (TiO₂ NPs) are the most extensively studied metal oxide nanoparticle worldwide. Despite the inconsistency of biological effects observed *in vitro* after exposure to TiO₂ NPs, many studies have demonstrated their capacity to induce cytotoxicity and genotoxicity in various cultured cell lines.

Nanoparticle toxicity has been associated to their small size and consequent high surface area and reactivity. In an attempt to overcome this issue and maintain the advantages of nanoparticles, immobilization of nanoparticles on the surface of inorganic supports has been recently performed, in particular on clays minerals, resulting in the creation of nanocomposites.

Taking all into account, the main goal of the present work was to evaluate *in vitro* toxicity of rutile TiO₂ NPs immobilized in high purity kaolinite clay (C-TiO₂), in a hepatocellular carcinoma human cell line (HepG2). For a full understanding of the effects of this nanocomposite and its single elements, a primary characterization was performed using field emission scanning electron microscope and dynamic light scattering. Nanomaterials uptake by HepG2 was also analyzed by means of flow cytometry. For the cytotoxicity evaluation it was initially established to use the MTT, Alamar blue, Neutral red uptake and LDH assays, however, after interference analysis, only MTT and Alamar blue were found to be suitable assays for the present materials. Cytotoxicity was evaluated after exposure to different concentrations of the three materials prepared in complete and serum free media for three exposure times (3, 6 and 24 hours). The comet assay was further used for the genotoxicity assessment (non-cytotoxic concentrations for 3 and 24 hours).

Results show that all studied materials were internalized by HepG2 cells in both media types (complete and serum free) and for both periods of exposure. In addition, analyzed materials induced significant mitochondrial and potential redox dysfunction of the hepatocytes in a dose-dependent manner. TiO₂ NPs preferentially induced decrease in viability after 24 hours of exposure in serum free medium and in almost all periods of exposure in complete medium; both nanokaolin and C-TiO₂ nanocomposite could significantly decrease the HepG2 viability for both media and also in almost all periods of treatment. Furthermore, TiO₂ NPs, nanokaolin and C-TiO₂ nanocomposites also affected DNA integrity in a dose-dependent manner both after 3 and 24 hours of exposure.

Thereby, the present results suggest that kaolinite mineral is not a desirable substrate for the immobilization of nanoparticles and that, in accordance to what has been

previously stated by other authors, rutile TiO₂ NPs may present cytotoxic and genotoxic effects.

To overcome the toxic effects observed, other organically modified kaolinite clays must be studied in order to find a suitable substrate for nanoparticle immobilization; this will be essential for the development of biocompatible and safe nanocomposites.

Keywords: nanocomposites, nanoparticles, TiO₂, kaolinite, cytotoxicity, genotoxicity, HepG2 cell line

RESUMO

Entre as nanopartículas de óxido de metal mais estudadas em todo o mundo estão as nanopartículas de dióxido de titânio (NPs TiO₂). Muitos estudos *in vitro* têm demonstrado que estas nanopartículas são capazes de induzir citotoxicidade e genotoxicidade em várias linhas celulares, embora exista alguma inconsistência relativamente aos efeitos biológicos observados.

A toxicidade das nanopartículas tem sido associada ao seu tamanho reduzido e consequente elevada área de superfície e reatividade. Na tentativa de superar este problema e manter as vantagens das nanopartículas, foi recentemente desenvolvida a técnica de imobilização de nanopartículas na superfície de suportes inorgânicos, em particular em minerais de argilas, resultando na criação de nanocompósitos.

Neste contexto, o principal objetivo do presente trabalho foi avaliar *in vitro* a toxicidade das NPs TiO₂ de rútilo imobilizadas em argila de caulinite de elevada pureza (C-TiO₂), numa linha hepatocelular de carcinoma humano (HepG2). Para compreender os efeitos destes nanocompósitos e dos seus elementos individuais, realizou-se uma caracterização primária usando as técnicas microscópio eletrónico de varredura de emissão de campo e dispersão dinâmica de luz. A internalização dos nanomateriais pelas células HepG2 foi analisada por citometria de fluxo. Para a avaliação da citotoxicidade, foi inicialmente estabelecido o uso dos ensaios MTT, Alamar Blue, internalização do vermelho neutro e LDH, mas a análise das interferências revelou que apenas os ensaios MTT e Alamar Blue seriam adequados para os materiais em estudo. A citotoxicidade foi avaliada após a exposição a diferentes concentrações dos três materiais preparados em meio completo e incompleto em três períodos de exposição (3, 6 e 24 horas). O ensaio cometa foi utilizado para a avaliação de genotoxicidade (concentrações não citotóxicas para 3 e 24 horas).

Os resultados mostram que todos os materiais estudados foram internalizados pelas células HepG2 em ambos os tipos de meio (completo e incompleto) e nos dois períodos de exposição. Além disso, todos os materiais analisados foram capazes de alterar significativamente a atividade mitocondrial e o potencial redox dos hepatócitos de uma forma dependente da dose. As NPs TiO₂ induziram preferencialmente uma diminuição da viabilidade após 24 horas de exposição em meio incompleto e em quase todos os períodos de exposição em meio completo; tanto a nanocaulinite como os nanocompósitos C-TiO₂ foram capazes de diminuir significativamente a viabilidade das HepG2 em ambos os meios e também em quase todos os períodos de tratamento. Adicionalmente, as NPs TiO₂,

nanocaulinite e os nanocompósitos C-TiO₂ também afetaram a integridade do DNA de uma forma dose-dependente após 3 e 24 horas de exposição.

Deste modo, estes resultados sugerem que o mineral caulinite não é um substrato adequado para a imobilização de nanopartículas e que, à semelhança do que já foi descrito por outros autores, as NPs TiO₂ de rútilo podem ser citotóxicas e genotóxicas.

Para superar os efeitos tóxicos observados, devem ser estudadas outras argilas de caulinite organicamente modificadas, de forma a identificar um substrato adequado para a imobilização de nanopartículas; isto será essencial para o desenvolvimento de nanocompósitos biocompatíveis e seguros.

Palavras-chave: nanocompósitos, nanopartículas, TiO₂, caulinite, citotoxicidade, genotoxicidade, linha celular HepG2

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LIST OF ABBREVIATIONS

AB	Alamar blue assay
BSA	Bovine Serum Albumin
C-TiO ₂	Titanium dioxide nanoparticles immobilized in clay
DLS	Dynamic light scattering
DMEM	Dulbecco's modified Eagle's medium
DMSO	Dimethyl sulfoxide
ENMs	Engineered nanomaterials
FBS	Fetal bovine serum
FE-SEM	Field-emission scanning electron microscopy
FSC	Forward scatter channel
HEPES	4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid
HepG2	Hepatocellular carcinoma human cell line
HSCs	Hepatic stellate cells
INT	2-(4-Iodophenyl)-3-(4-nitrophenyl)-5-phenyltetrazoliumchlorid
JRC	European Commission's Joint Research Centre
LDH	Lactate dehydrogenase
LDV	Laser Doppler velocimetry
LMP	Low melting point
MMS	Methyl methanesulfonate
MONPs	Metal oxide nanoparticles
MTT	3-[4,5-dimethylthiazol-2-yl]-2,5 diphenyl tetrazolium bromide
NMP	Normal melting point
NRU	Neutral red uptake
PBS	Phosphate buffered saline
ROS	Reactive oxygen species
SEM	Scanning electron microscopy

SSC	Side scatter channel
TEM	Transmission electron microscopy
tDNA	Comet tail intensity
TiO ₂ NPs	Titanium dioxide nanoparticles
UV	Ultraviolet

I. INTRODUCTION

1. Statement of the problem

In recent times, nanotechnology is growing in rapid pace, discovering innovative and attractive nanomaterials with specific properties for several applications (Iavicoli *et al.*, 2011; Savolainen *et al.*, 2013). Within the existing nanomaterials, the most used are the metal oxide nanoparticles (Djurisic *et al.*, 2014), being the titanium dioxide nanoparticles (TiO₂ NPs) the most extensively studied (both on material characterization and toxic properties) due to its low cost production and unique properties, including small size, large surface area, high stability, anticorrosive, excellent optical and electrical properties and photocatalytic activity (Gupta and Tripathi, 2011; Menard *et al.*, 2011; Fresegna *et al.*, 2014). Textile industries, biotechnology, pharmaceutical and cosmetics are prominent areas of TiO₂ NPs applications, leading to the increasing worldwide distribution of these nanoparticles (Gupta and Tripathi, 2011; Marquez-Ramirez *et al.*, 2012; Botelho *et al.*, 2014). However, the available studies on the toxicity of TiO₂ NPs show contradictory results (Shi *et al.*, 2013; Iavicoli *et al.*, 2011; Iavicoli *et al.*, 2012a).

Owing to the distinctive properties derived by the nano-sized particles, some reports have been demonstrating that nanoparticles are more toxic when compared to larger micro-sized particles (Kocbek *et al.*, 2010; Roy *et al.*, 2014). Recent advances in the production of nanomaterials lead to the development of new structures, namely of nanoparticles immobilized in microstructures that, by presenting new physico-chemical features, must be tested in regards to their toxic potential (Aono *et al.*, 2012). Concerning TiO₂ NPs, these have already been developed in conjugation with modified clays, but to our knowledge there are no earlier toxicological studies on these novel nanocomposites (Aranda *et al.*, 2008; Manova *et al.*, 2010). In this way, *in vitro* studies are required to evaluate the biological effects of these nanostructures in order to understand if they present increased toxicity or biocompatibility as compared to TiO₂ NPs alone.

2. Research questions

In this context, the main goal of the present work was to evaluate *in vitro* cytotoxicity and genotoxicity of a nanocomposite (here designed C-TiO₂) constituted by TiO₂ NPs (NM-104 rutile obtained from the European Commission's Joint Research Centre (JRC) (Rasmussen *et al.*, 2014)) and high purity kaolinite clay in a hepatocellular carcinoma human cell line (HepG2). For a matter of comparison, both TiO₂ and kaolinite single particles were also studied.

Thus, to achieve this main objective, the following specific goals were established:

1. Nanomaterial characterization: Characterization of primary particle size, size distribution and particle morphology using field emission scanning electron microscope (FE-SEM), as well as the evaluation of the hydrodynamic particle size, polydispersity - via dynamic light scattering (DLS) - and zeta-potential (by laser Doppler velocimetry – LDV) of the nanomaterials under evaluation (TiO₂ NPs, kaolinite clay and C-TiO₂ nanocomposites);
2. Nanomaterial uptake: Exploratory analysis of nanomaterials internalization on HepG2 cells after exposure to different concentrations and time periods by means of flow cytometry;
3. Interferences studies: Evaluation of the possible interferences between nanomaterials and the cytotoxicity (3-[4,5-dimethylthiazol-2-yl]-2,5 diphenyl tetrazolium bromide (MTT), neutral red uptake (NRU) and Alamar blue (AB) and lactate dehydrogenase (LDH) activity assays) and genotoxicity assays under evaluation. This stage was essential to identify which of them were suitable for toxicity assessment of the studied materials, and to obviate possible interference between materials and assay reading by introducing alterations to assay protocols;
4. In vitro cytotoxicity and genotoxicity of C-TiO₂, kaolinite and TiO₂ nanomaterials on HepG2 cell line: Assessment of the cytotoxic and genotoxic effects of the different nanomaterials on HepG2 cell line. Cell viability was evaluated after cell exposure to different concentrations (and time periods) of the studied materials, by employing MTT and AB cytotoxicity assays. Additionally, for the genotoxicity assessment, comet assay was performed after cell exposure for the different nanomaterials non-cytotoxic concentrations and time periods.

3. Organization of the dissertation

The dissertation is constituted by the following topics:

1. State of the art, presents general concepts on nanotechnology and nanotoxicology, a literature review of the nanomaterials under study and their possible related effects as well as innovative aspects of the research;
2. Methodology, provides a detailed explanation of the methods used for the nanomaterial characterization, and the methodologies used for each cytotoxic and genotoxic assays under evaluation, after a full study of the possible nanomaterial interference on the assays;

3. Results and Discussion, debates the results obtained with basis on knowledge described in the scientific literature;
4. Conclusions and future perspectives, summarizes the main results and conclusions discussed in the previous section, presents suggestions for future work and appreciations of the work developed.

This dissertation also includes appendices with supplementary data.

II. STATE OF ART

1. The Nano World

Nanotechnology is an interdisciplinary field of science that is considered as a fundamental technology of the 21st century (Frohlich, 2013; Laroui *et al.*, 2013). The interconnection of different fields of knowledge integrating physics, chemistry, engineering, biology and medicine, allows nanotechnology to study and manipulate materials at nano scale, producing innovative structures, materials and/or devices with distinctive properties and functionalities (Laroui *et al.*, 2013; OCDE, 2014).

The industry of nanotechnology is in global expansion (Baker *et al.*, 2014; Djuricic *et al.*, 2014), being estimated that, by now, in 2015, there would be around 2 million nanotechnology workers worldwide, and the value of products incorporating nanotechnology as a key component would reach around 1 trillion dollars (Roco, 2011). With the systematic introduction of new products, the nanotechnology market is doubling every 3 years. The same author has extrapolated that, by the year of 2020, the number of nanotechnology workers worldwide and product market value will increase to 6 million people and 3 trillion dollars, respectively.

In the last years, several sectors such as electronics, textiles, food, agriculture, environmental protection, cosmetics and healthcare (including drug delivery systems, regenerative medicine and diagnostics) have been revolutionized with the introduction of different types of engineered nanomaterials (ENMs) (SCENIHR, 2007; Conde *et al.*, 2014). The European Union defines ENMs as structures, agglomerates or aggregates, where 50% or more of the particles have at least one dimension, in the size range 1-100 nm (EPC, 2011; Lin *et al.*, 2014). In addition, there is a specific definition of particle at a nano scale which includes a piece of matter with demarcated physical boundaries with the same size range as defined earlier, commonly defined as nanoparticles. The European Commission also recommends that these broad definitions should include any material with natural (e.g. forest fires, mineral composites, volcanic ash, viruses), incident (e.g. cooking smoke, diesel exhaust, industrial effluents) or engineered (quantum dots, carbon nanotubes, lipid and metallic nanoparticles) origin (Lidén, 2011). Generally, engineered nanoparticles are better characterized than the environmental nanoparticles, allowing a better correlation between their physicochemical properties and their effects in biological systems (Frohlich, 2013).

Despite the implementation of ENMs being a sustainable and profitable alternative to traditional materials, it is important to consider the possible impact on environmental and human health (Mitrano *et al.*, 2015; Martirosyan and Schneider, 2014). The large scale applications of ENMs increases the extension of exposure, influencing the life cycle of these nanomaterials. Nanomaterials can be released into the environment during different stages:

production process and manufacture, usage, recycling or disposal (Djurisic *et al.*, 2014). While the manufacturing of these materials is performed in controlled conditions, the use and disposal of these products by the consumer are life cycle stages that cannot yet be controlled (Mitrano *et al.*, 2015). Once in the environment, ENMs experience different transformations (e.g., deposition, adsorption, agglomeration, aggregation, redox reactions) that possibly interfere with their reactivity and toxicity (Martirosyan and Schneider, 2014). As such, it is necessary to conduct a complete risk assessment of these nanomaterials, which must include their entire life cycle, in order to understand their biological impact and fate in the environment (Piccinno *et al.*, 2012; Martirosyan and Schneider, 2014).

2. Nanotoxicology: looking at the risks of TiO₂ NPs exposure to human health

Nanotoxicology is a branch of bionanoscience which evaluates the potential toxic impact of nanomaterials on human and environmental health, resulting from the interaction of these materials with biological and ecological systems (Ai *et al.*, 2011; Love *et al.*, 2012; Sarkar *et al.*, 2014). Some materials, harmless in its bulk form, become cytotoxic when presented at the nano scale. This adverse phenomenon is related to the high surface to volume ratio and consequent increase surface reactivity of the nanoparticles (Frohlich, 2013). One key goal of nanotoxicology is to understand the impact of existing nanoparticles in different biological systems and ultimately to help scientists to synthesize safer nanoparticles, or at least understand the impact of existing nanoparticles in different biological systems. For this purpose, the physicochemical properties of nanomaterials must be well characterized, and the analysis of its effects on biological systems must be carried out using appropriate models (Love *et al.*, 2012).

2.1. What are TiO₂ NPs?

Metal oxide nanoparticles (MONPs) are the group of ENMs with the largest share of manufacture and application worldwide (Djurisic *et al.*, 2014). These nanoparticles offer unique optical and magnetic functionalities, and are therefore appealing for several applications, including material science, engineering and biomedical applications (Falugi *et al.*, 2012; Teske and Detweiler, 2015).

Currently, one of the most studied and most abundantly produced MONPs around the world are TiO₂ NPs (Menard *et al.*, 2011; Li *et al.*, 2014).

In its bulk form, titanium dioxide is frequently characterized as a non-combustible, thermally stable, odourless and poorly soluble particulate (Iavicoli *et al.*, 2011; Marquez-Ramirez *et al.*, 2012). Titanium dioxide is obtained from the iron mineral ilmenite, a naturally

occurring crystal that can exist in three major crystalline forms: rutile, anatase and brookite (Banerjee, 2011; Park *et al.*, 2014). Despite that, only rutile and anatase are generally used in titanium dioxide applications (Iavicoli *et al.*, 2011; Becker *et al.*, 2014). Although both rutile and anatase possess a tetragonal crystal system (Figure 1), rutile has a denser arrangement of the atoms (Iavicoli *et al.*, 2011). This phase is the most common and stable phase in nature, while anatase is metastable at room temperature, exhibiting the highest photocatalytic activity and chemical reactivity when compared to rutile form (Menard *et al.*, 2011; Becker *et al.*, 2014). Commonly, TiO₂ NPs are a mixture of both rutile and anatase forms (Becker *et al.*, 2014).

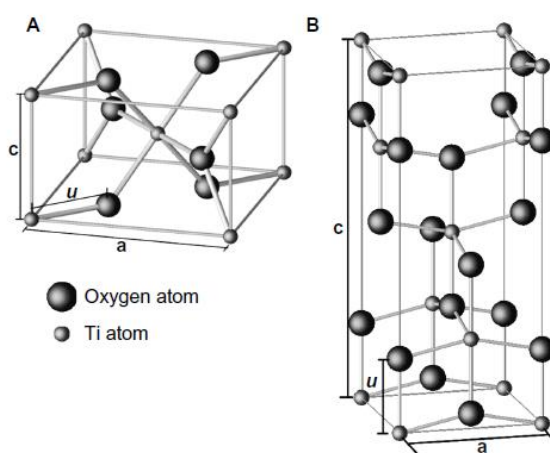


Figure 1. Tetragonal crystal structure of (A) rutile and (B) anatase TiO₂ forms (Banerjee, 2011).

Due to their unique and distinctive properties, including high stability, anticorrosive, biocompatibility, excellent optical performance and electrical properties, photocatalytic activity and low cost production, TiO₂ NPs are broadly used in a variety of applications (Jaeger *et al.*, 2012; Lagopati *et al.*, 2014). These include industry, waste water treatment, medicine, pharmaceuticals and cosmetics (Warheit, 2013; Botelho *et al.*, 2014). They are also applied in several industrial materials as a white pigment in paints, inks, rubber, plastics, car materials, papers and food additives (Horie *et al.*, 2010; Martirosyan and Schneider, 2014).

Cosmetics are the largest application area for TiO₂ NPs (Fig. 2.A), representing 59.4% of the total product application. These nanoparticles are commonly used in sunscreens for protecting skin cells from ultraviolet (UV) light damage, as well as white dye in toothpastes (Fenoglio *et al.*, 2009; Becker *et al.*, 2014). Additionally, they have been used in skin care products to treat some dermatologic diseases such as acne vulgaris, atopic dermatitis and hyperpigmented skin lesions, among others (Shi *et al.*, 2013).

More recently, TiO₂ NPs have been explored in several areas of biomedical research including prosthetic implants (e.g. as coating material due to their antimicrobial and mechanical properties), photodynamic therapy for cancer, drug delivery systems, cell imaging, biosensors and genetic engineering (Marquez-Ramirez *et al.*, 2012; Yin *et al.*, 2013; Martirosyan and Schneider, 2014).

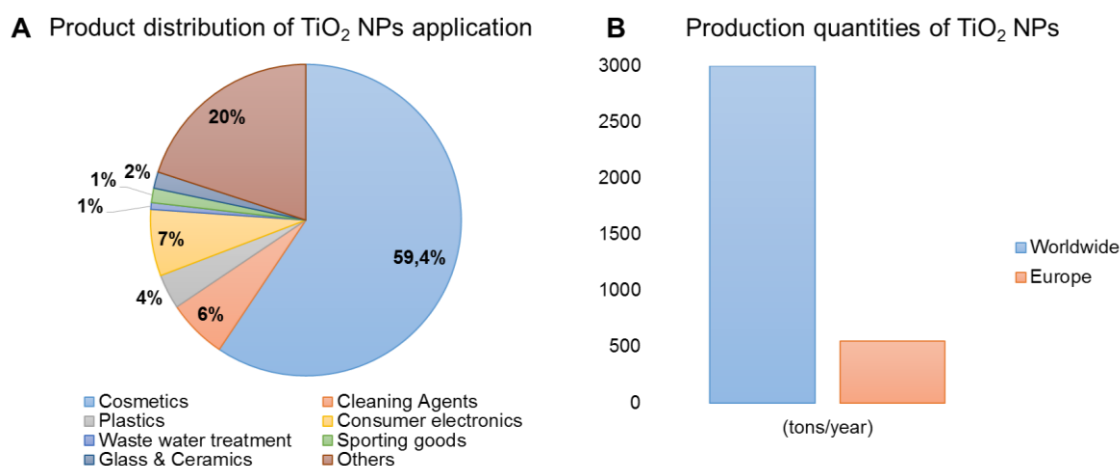


Figure 2. Percentages of product applications (A) and production quantities of TiO₂ NPs (B) (based on data presented by Sun *et al.* (2014) (graph A) and Piccinno *et al.* (2012) (graph B)).

With the increased demand for TiO₂ NPs among nanotechnology products, the amount of production of these ENMs is massive. As represented in the figure 2.B, according to Piccinno *et al.* (2012), around 3000 tons of TiO₂ NPs are produced per year worldwide, while in Europe, from these quantity, only 550 tons per year are produced. Thereby, a significant release of TiO₂ NPs into the environment is expected, increasing environmental and, consequently, human exposure (Botelho *et al.*, 2014; Djuricic *et al.*, 2014). Individuals primarily exposed to TiO₂ NPs are not only the consumers of these applications, but also the workers who may contact, directly or indirectly, with these nanoparticles during research, synthesis or further treatment and application of these materials (Klien and Godnic-Cvar, 2012).

Most of the TiO₂ NPs physicochemical properties that make them so valuable for the mentioned applications are also related to their bioavailability and toxicity in humans (Shi *et al.*, 2013). The main physicochemical properties of particles associated to their toxicity include size, shape, surface characteristics and also inner structure (Roy *et al.*, 2014; Becker *et al.*, 2014; Park *et al.*, 2014). Besides the reactivity and consequent toxicity which may be related to the small size of TiO₂ NPs (as also with the majority of nanoparticles, as mentioned above) (Wang *et al.*, 2014), is important to consider the influence of the proteins with the nanoparticles in biological conditions. Actually, nanoparticles when introduced in

biological medium will unavoidably interact with the human plasma proteins, leading to the formation of a protein corona, which result from the adsorption of these proteins to nanoparticles surface. Consequently, this protein corona will interfere with the physicochemical properties of the nanoparticles (e.g. size, agglomeration state), possibly interfering with the cellular uptake of particles (Allouni *et al.*, 2015). Therefore, researchers have been concerned about the possible harmful effects derived from TiO₂ NPs exposure in human health (Shi *et al.*, 2013).

For several applications such as sunscreens, different authors verified that surface modifications of TiO₂ NPs leads to an improvement of their properties (e.g. UV attenuation), in comparison with uncoated particles (Rahim *et al.*, 2012). Additionally, to prevent agglomeration and increase the dispersibility and stability of these nanoparticles in different organic solvents, some researchers have been employing different surface coatings (e.g. polyethylene glycol) (Rahim *et al.*, 2012; Janer *et al.*, 2014). Depending on the coatings and surface modifications applied in different applications, nanoparticles can present higher biocompatibility and possibly decrease their acute toxicity (Naqvi *et al.*, 2010).

2.2. Human Exposure to TiO₂ NPs: uptake, biodistribution and accumulation

Human exposure to TiO₂ NPs may occur during both manufacturing and use (Klien and Godnic-Cvar, 2012). Although the real effects on human health derived from nanoparticles exposure remain unclear, it is important to consider the multiple scenarios of uptake and biodistribution of the nanoparticles in the human body, to better evaluate and predict the possible toxicological effects (Magdolenova *et al.*, 2012).

The human body has several portals of entry that protect the organism against pathogens and harmful materials from the external environment (Arora *et al.*, 2012). The major portals of entry of TiO₂ NPs in the human body are the respiratory tract, the skin and hair follicles, the gastrointestinal tract and the circulatory system (Wang *et al.*, 2014) (Figure 3).

In occupational settings, inhalation is the major route of exposure to TiO₂ NPs (Shi *et al.*, 2013). The respiratory system is the portal of entry with the largest surface area in direct contact with the environment being, in the majority of exposure scenarios, the main route of entrance of nanoparticles (Kim *et al.*, 2012). After inhalation, nanoparticles can pass through the lung epithelium and reach the blood and lymph systems (Magdolenova *et al.*, 2012). In addition, inhalation of TiO₂ NPs has been also related to the deposition of these particles in the brain, since they can pass through the olfactory bulb (Huerta-Garcia *et al.*, 2014).

Dermal exposure is related to the use of cosmetics and sunscreens that contain these MNOPs (Burnett and Wang, 2011). Skin is considered the first mechanical barrier that protects the organism against toxic agents, including nanoparticles (Krug and Wick, 2011). Depending on the nanoparticle features, they can penetrate into the dermis, enter via bloodstream or lymphatic system and reach other organs that can be potentially affected (Magdolenova *et al.*, 2012). Nevertheless, several studies demonstrated no evidence of TiO₂ NPs penetration through the human skin into the body, under normal conditions (healthy skin without burns or cuts) (Shi *et al.*, 2013).

The ingestion of drug carriers, food products, water or beverages containing TiO₂ NPs are examples of sources of exposure to these nanoparticles in the gastrointestinal tract (Martirosyan and Schneider, 2014).

In medical applications, intravenous, intraperitoneal or even subcutaneous injection of TiO₂ NPs are the main route of entry into the circulatory system (Shi *et al.*, 2013). The small size of TiO₂ NPs allows internalization by cells and transcytosis across epithelial and endothelial cell barriers into the blood and lymph circulation (Huerta-Garcia *et al.*, 2014). TiO₂ NPs can form a protein corona after interacting with human plasma proteins, coagulation factors, platelets and red or white blood cells. This protein corona may interfere with the distribution, metabolism and excretion of these nanoparticles and, therefore, with their possible toxic effects (Allouni *et al.*, 2015).

After entering the systemic circulation, TiO₂ NPs can be biodistributed and bioaccumulated in organs and tissues of the body including liver, lung, spleen, kidney, heart, bone marrow and lymph nodes (Becker *et al.*, 2014; Roy *et al.*, 2014). It has also been demonstrated that high doses of TiO₂ NPs in the circulation are able to cross blood brain barrier, blood-testis and also the blood placenta barrier in pregnant women (Martirosyan and Schneider, 2014).

There are two main clearance pathways of TiO₂ NPs from the human body: via kidneys/urine and bile/faeces. A large fraction of internalized TiO₂ NPs can be rapidly excreted, however, not all of these nanoparticles will be totally eliminated, since some of them may accumulate in some tissues or organs, especially after continuous exposure. The physicochemical properties of the particles, dosage, time and route of exposure may interfere with the rate of absorption, biodistribution, metabolism and excretion of these MNOPs in the human body. Some studies reveal pathological lesions in several organs and low clearance of TiO₂ NPs after exposure to high doses and for short periods that often correspond to unrealistic particle levels of exposure. Therefore, further studies are needed

to better understand the effects of the TiO₂ NPs exposure in the normal biological function and anatomical morphology (Shi *et al.*, 2013).

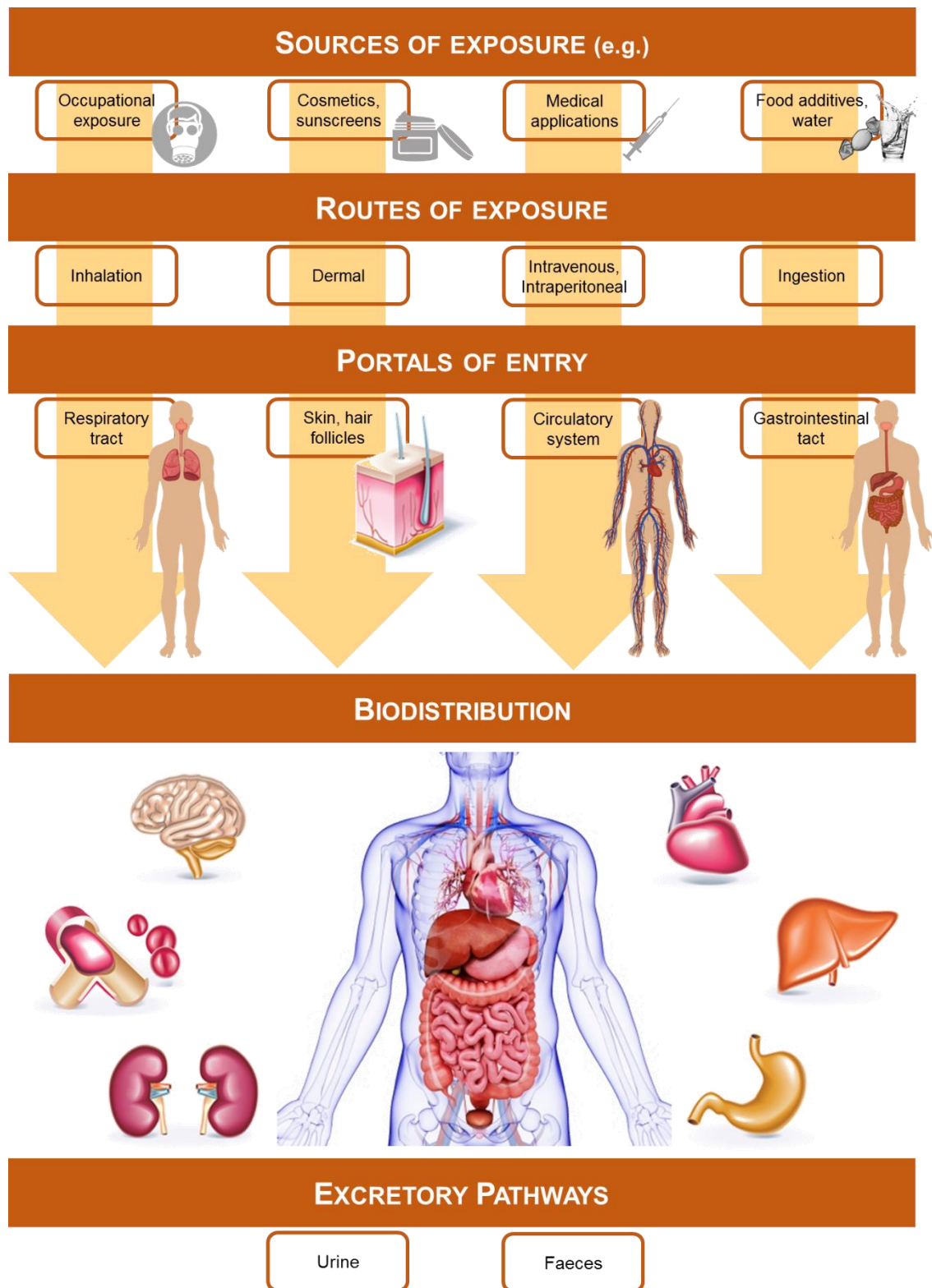


Figure 3. Toxicokinetics of TiO₂ NPs within the human body with indication of possible sources of exposure, based on the information reported along the text.

The liver is the second largest organ of the human body, playing a critical role in the metabolic (e.g. cholesterol and intestinal lipid metabolism) and clearance function (Wallace *et al.*, 2008).

The liver is mainly constituted by parenchymal cells, representing approximately 80% of the liver volume (Figure 4). About 6.5% of the remaining volume corresponds to non-parenchymal cells. Hepatocytes are the major parenchymal cells types in the liver, while the hepatic stellate cells (HSCs), liver sinusoidal endothelial cells and Kupffer cells (specialized macrophages in the liver) are the main non-parenchymal cell types (Bartneck *et al.*, 2014; Wang *et al.*, 2015). All these liver cells are promising targets for nanomedicine applications, due to their critical functions in the liver disease progression (Giannitrapani *et al.*, 2014).

This highly vascular and protective organ is involved in the detoxification of the TiO₂ NPs in the body (Roy *et al.*, 2014). Due to its physiological and anatomical characteristics, the liver is the major organ of nanoparticle accumulation and TiO₂ NPs are no exception (Shi *et al.*, 2013).

One possible reason for the nanoparticle accumulation is the high number of liver macrophages, which represents around 80-90% of total macrophages of the body. Once in the blood circulation, nanoparticles form a protein corona after interacting non-specifically with the serum proteins, which is further recognized by the Kupffer cells on the hepatic sinusoid, leading to nanoparticle accumulation. The larger the particle size, the greater the uptake by the Kupffer cells, decreasing the circulation time of these nanoparticles (Wang *et al.*, 2015). Additionally, there are other factors besides particle size that interfere with the cellular uptake of nanoparticles, for instance particles surface charge. Generally, hepatocytes are able to internalize positive charged nanoparticles, while Kupffer cells and endothelial cells tend to internalize the negative charged ones (Wang *et al.*, 2015). Beyond that, the surface charge of nanoparticles also interferes with the extracellular immobilization of nanoparticles by immune cells (Bartneck *et al.*, 2014; Giannitrapani *et al.*, 2014).

To avoid the nanoparticle accumulation on the liver and minimize nanoparticle cellular uptake by Kupffer cells, several biodegradable and biocompatible surface coating materials (e.g. polyethylene glycol) have been used (Giannitrapani *et al.*, 2014). Nonetheless, despite the numerous targeting approaches studied so far, the effect of nanoparticle properties at the cellular level in the liver is still uncertain (Wang *et al.*, 2015).

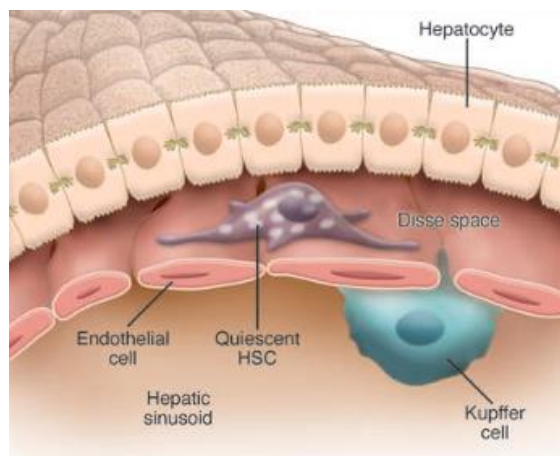


Figure 4. Major cells presented in a normal liver. Hepatocytes are parenchymal cells, while the hepatic stellate cells (HSCs), liver sinusoidal endothelial cells and Kupffer cells are non-parenchymal cells. HSCs are present in the space of Disse, which is a small region between the hepatic sinusoid and hepatocytes (adapted from Iredale (2007)).

Few studies of hepatic toxicity of TiO₂ NPs have been performed in the last years. According to Iavicoli *et al.* (2011), four studies made on hepatic cells identified the production of reactive oxygen species (ROS) as one of the predominant toxic effects related to *in vitro* TiO₂ NPs exposure. More recent studies are in agreement with these results. For instance, Shukla *et al.* (2014) demonstrated that oxidative stress is an important mechanism of toxicity after TiO₂ NPs exposure, triggering DNA damage mechanisms and initiating the expression of apoptotic proteins, resulting in hepatic injury. These confirm the results obtained in other studies reporting genotoxic effects (Petković *et al.*, 2011; Kermanizadeh *et al.*, 2012) and loss in hepatic functions (Natarajan, 2015).

It is important to take into account that *in vitro* hepatic systems might not be the more accurate liver model once these cells lose key liver specific functions and are not representative of realistic *in vivo* conditions (Kermanizadeh *et al.*, 2013). Notwithstanding, several authors claim that the use of mammalian cell line is the best option to access the toxicological effect of a certain engineered nanomaterial in cells and tissues (Suh *et al.*, 2009). Actually, the cancer cell line demonstrates increased uptake levels of nanoparticles and are more sensitive to nanomaterial toxicity, when compared with long-lived cell lines and primary cultures (Joris *et al.*, 2013). One of the widely used *in vitro* hepatic model is the HepG2 cell line. It is an extremely well characterized cell line and it is commonly used in nanotoxicological studies as a surrogate model of human hepatocytes (Jones and Grainger, 2009).

2.3. TiO₂ NPs interaction with biological systems: *in vitro* and *in vivo* evidence

As aforementioned, the unique properties of TiO₂ NPs make them an attractive option for several everyday nanotechnology-based products and applications, being the most vastly manufactured nanoparticle in the world (Liang *et al.*, 2009). Meanwhile, the major challenge in using this type of particles is to guarantee their safety to human health and environment, after inclusion in consumer products (Djurisic *et al.*, 2014; Lin *et al.*, 2014).

The main aspects to take into account during the evaluation of nanoparticle cytotoxicity and genotoxicity is the proper characterization of these materials, including morphology, crystal structure, purity, size distribution, surface area, chemical composition (surface chemistry and charge), and the degree of aggregation and agglomeration as well as the release of metal ion in biological media (Djurisic *et al.*, 2014). In addition to these, the coating and surface modification of the nanoparticle is another important feature to take into account (Klien and Godnic-Cvar, 2012). Thereby, a detailed characterization of the nanomaterial properties is essential for both *in vitro* and *in vivo* studies, to perceive their influence in the biological systems.

One of the major problems associated with *in vitro* studies with nanoparticles are related to the nanoparticles instability and their tendency to form aggregates (non-reversible grouping of nanoparticles) and agglomerates (reversible grouping of nanoparticles) in biological solutions. The same phenomenon occurs to TiO₂ NPs without surface modifications, since they tend to form aggregates and agglomerates due to their small size and also due to solution properties (e.g. conductivity and ionic strength) (Love *et al.*, 2012). Thus, to overcome this issue, is important to perform suitable medium dispersion to correctly evaluate the cytotoxic effects of the TiO₂ NPs (Fujita *et al.*, 2009).

For some researchers, TiO₂ NPs are considered to be a nontoxic mineral, being even used as negative control in many *in vitro* and *in vivo* studies (Liu *et al.*, 2013). However, others investigators demonstrated opposite effects, since their studies suggest that TiO₂ NPs may induce higher toxicity potential, especially when compared to their bulk materials (Jaeger *et al.*, 2012).

Due to their small size, TiO₂ NPs can penetrate the cells, which may disrupt their normal function (Liu *et al.*, 2013). The most studied mechanisms of nanoparticle cell internalization include endocytosis, membrane fluidity and direct passage through channels or adhesive junctions (e.g. tight junctions) (Roy *et al.*, 2014). Once inside the cells, some reports indicate the occurrence of cyto and genotoxic effects, depending on the TiO₂ NPs concentration and also their exposure time.

Despite the inconsistency of biological effects observed *in vitro* after exposure to TiO₂ NPs, many studies have demonstrated the capacity of TiO₂ NPs to induce cytotoxicity and genotoxicity in various cultured cell lines (Shi *et al.*, 2013; Prasad *et al.*, 2014). Increased ROS production, reduction in cell viability and proliferation, and DNA damage have been frequently related to these nanoparticles in mammalian cells (Huerta-Garcia *et al.*, 2014). In fact, the photocatalysis activity of TiO₂ NPs conjugated with their reduced size has been related to increased ROS production and subsequent biological damage (Fujita *et al.*, 2009; Horie *et al.*, 2010).

Additionally, other studies have reported that exposure to TiO₂ NPs leads to lipid peroxidation, caspase activation followed by micronuclei formation, DNA damage directly or indirectly via oxidative stress, chromatin condensation and inflammatory responses (Valdiglesias *et al.*, 2013; Botelho *et al.*, 2014). While some authors reported the occurrence of cell death via apoptosis, others have not demonstrated this phenomenon induced by TiO₂ NPs (Jaeger *et al.*, 2012; Roy *et al.*, 2014). Conflicting results have also been described in the study of oxidative stress response, mitochondrial dysfunction and plasma membrane damage.

In the same way as *in vitro* studies, *in vivo* studies of TiO₂ NPs exposure carried out on hamsters, rats, and mice also show inconsistent results (Iavicoli *et al.*, 2012b; Prasad *et al.*, 2014). One topic that remains controversial is the genotoxicity of TiO₂ NPs (Shi *et al.*, 2013). While some *in vivo* genotoxicity studies showed that TiO₂ NPs increase the expression of inflammatory cytokines, mRNA expression of toll like receptors and DNA deletions in different organs and also in the reproductive system, other authors does not report the same effect (Ursini *et al.*, 2014). These opposite results may be due to different TiO₂ NPs, exposure times and/or doses applied by the investigators, as previously notice for *in vitro* studies. Therefore, further *in vivo* studies should be carried out with relevant doses (which occur in occupational and environmental exposure conditions) in order to understand the real effects of TiO₂ NPs exposure (Martirosyan and Schneider, 2014).

Since most researchers use TiO₂ NPs with different crystal phase, size, surface coating and dosage, it is difficult to compare and truly understand the predictive value of some *in vitro* and *in vivo* studies (Janer *et al.*, 2014). As such, only after a proper assessment of the TiO₂ NPs properties and living models under evaluation, is possible to make a precise interpretation of results obtained in the performed studies (Frohlich, 2012; Park *et al.*, 2014). Therefore, despite the debatable aspects of TiO₂ NPs cytotoxicity and genotoxicity, these nanomaterials should be treated as potentially hazardous.

3. Moving forward with nanocomposites

3.1. The need for new materials

The fact that nanoparticles induce more damage and are more biologically active when compared to larger micro-sized particles (Roy *et al.*, 2014; Allouni *et al.*, 2015) encouraged the emergence of an innovative area of nanotechnology: nanoarchitectonics. Nanoarchitectonics is a technology system which assembles nanostructure units (discrete functional parts which have one or more dimensions of the order of 100 nm or less) (SCENIHR, 2007) into a novel structure functionality through mutual interactions among units (Aono *et al.*, 2012). This field of nanomaterials introduced innovations in the design and constructions systems in nanoelectronics, nanomachinery, energy conversion, and more recently in nanomedicine (Gonzalez-Alfaro *et al.*, 2011; Kujawa and Winnik, 2013). New nanostructured materials have been developed as electro and photocatalysts (e.g. removal of non-filterable pollutants and dissolved organic compounds from water such as dyes, halogenated organic compounds and pesticides, resulting from industrial and agricultural applications), rechargeable batteries, solar cells and fuel cells (Aranda *et al.*, 2008; Aono *et al.*, 2012). Most of these nano, or even micro scale materials have been produced utilizing synthetic techniques based on soft-chemical nanoarchitectonics, including colloid chemistry and supermolecular nanoarchitectonic processes (Aono *et al.*, 2012). Currently, colloidal systems have been studied as new nanostructure complexes for therapeutic and diagnostic applications and also for development of new materials for regenerative medicine (Kujawa and Winnik, 2013; Kim *et al.*, 2014).

Composites are materials constituted with two or more components. These can be formed through a combination of materials with different physicochemical structures which contribute to the appearance of uncommon properties difficult to obtain from the individual components. Composite materials present two main phases: continuous matrix phase and the filler material embedded to the matrix which corresponds to the dispersed phase (Olad, 2011).

Nanocomposites are commonly defined as composite materials, where at least one of the phase components dimension is at the nanometre range (Jeon and Baek, 2010; Wohlleben *et al.*, 2011; Choi *et al.*, 2013). Similarly to the composites, nanocomposites can be classified as polymeric, ceramic and metallic, according to the matrix composition (Camargo *et al.*, 2009; Choi *et al.*, 2013).

Recently, the use of biocompatible and antibacterial polymeric nanocomposites in several applications has been increasing, for example, for water purification membranes,

thin films for wound dressing and biosensors (Santos *et al.*, 2012). Nanocomposites have already been considered an attractive option for several biomedical fields including tissue engineering, oral implant and orthopaedic applications (Choi *et al.*, 2013).

The degradation and consequent release of the embedded nanomaterials into the environment is a probable ending of nanocomposites life cycle (i.e., since the manufacture, consumer product use to disposal and/or recycling), representing a potential hazard aspect of these applications (Froggett *et al.*, 2014). Thereby, more studies are required to understand the potential toxicological effects derived from exposure to these nanocomposites.

In spite of the numerous advantages and potential applications regarding the polymeric nanocomposites, some researchers have identified some disadvantages associated to these structures. The main problems arise from the non-homogeneous distribution of the particles in the polymer matrix, limited degree of exfoliation and tendency to aggregation, especially in nanocomposites containing fibers, tubes or spherical particles (Keledi *et al.*, 2012).

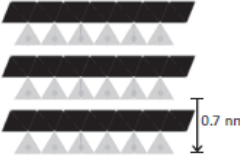
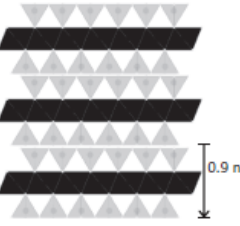
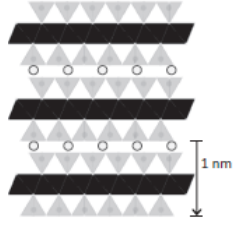
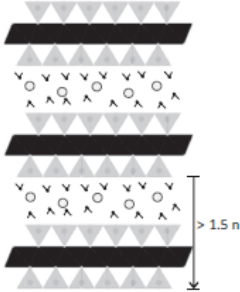
The immobilization of nanoparticles on the surface of inorganic or organic supports results in the creation of nanocomposites. These new nanoarchitectonic structures also present high surface area as well as increased porosity due to their topochemical characteristics (Aranda *et al.*, 2008). The most widely used supports include zeolites, activated carbon, silica and also natural or synthetic clay minerals like montmorillonite, vermiculite and sepiolite (Aranda *et al.*, 2008; Gonzalez-Alfaro *et al.*, 2011).

3.2. Clay minerals

Layered silicates are natural or synthetic minerals characterized by a regular laminar structure made of alumina and silica with high surface area (Pavlidou and Papaspyrides, 2008; Maisanaba *et al.*, 2015). Among the existing layered silicates, the clays are one of the most commonly used in the preparation of polymer nanocomposites since they greatly improve the polymeric matrix properties, due to their high surface to volume ratio (Arora and Padua, 2010; Olad, 2011). Clay minerals are one of the most abundant natural mineral at the surface of the earth and is presented as a nanosized layer, with a particle size less than 2 nm and layer thickness of 1 nm (Davidovic *et al.*, 2011). The layered structure of clays are built from two sheets, tetrahedral (in which a silicon atom is surrounded by four oxygen atoms) and octahedral (in which a metal like aluminium or magnesium is surrounded by eight oxygen atoms), fused together at the oxygen atoms. The rearrangements of these sheets fused together form different types of groups: kaolinite (one tetrahedral fused to one

octahedral sheet) and phyllosilicate (two tetrahedral fused to one octahedral sheet) (Table 1) (Olad, 2011; Dawson and Oreffo, 2013).

Table 1. Types of arrangements of clay layered silicates (based on Dawson and Oreffo (2013) and Maisanaba *et al.* (2015)).

	Layered silicate	Structure	General formula	Layer thickness (nm)	
Type of arrangement (tetrahedral:octahedral sheets)	Kaolinite (1:1)		$Al_2Si_2O_5(OH)_5$	0.7	
					$Al_2Si_4O_{10}(OH)_2$
	Phyllosilicates (2:1)	Vermiculite		$(Mg, Fe^{2+}, Al)_3(Al, Si)_4O_{10}(OH)_2 \cdot 4(H_2O)$	
		Smectite		Montmorillonite: $M_x(Al_{4-x}Mg_x)Si_8O_{20}(OH)_4$ Hectorite: $M_x(Mg_6-xLi_x)Si_8O_{20}(OH)_4$ Saponite: $M_xMg_6(Si_8-xAl_x)O_{20}(OH)_4$	> 1.5

Kaolinite is one relevant class of clay minerals in which the layers are held together through hydrogen bonding, as well as dipole-dipole and van der Waals interactions. This clay mineral does not tend to expand in water, but certain compounds (e.g. amides, urea), induce kaolinite swelling due to the formation of hydrogen bonds with the inter-layer surface. The high level of organization and degree of stacking of the layers allows them to be positive

charged in acidic conditions and negative charged at pH around 7 (Dawson and Oreffo, 2013; Maisanaba *et al.*, 2015).

The basic 2:1 structure without any substitution is named pyrophyllite (Pavlidou and Papaspyrides, 2008; Maisanaba *et al.*, 2015). This type of phyllosilicate is electrostatically neutral, not showing any ion within the inter layers and neither expanding in water such as kaolinite. In its turn, when the aluminium cations are partially substituted by divalent magnesium or iron cations in the neutral pyrophyllite, the smectite layered silicate is formed. The negative charge originated by this substitution is well balanced with the sodium and calcium ions presented in the inter layer (Olad, 2011). Among the different types of smectites, montmorillonite, hectorite and saponite are the most commonly used in the preparation of polymer nanocomposites (Pavlidou and Papaspyrides, 2008).

The weak forces holding the clay layers close to each other (e.g. electrostatic and van der Waals forces), the charge density and cation radius and the degree of hydration of the inter layer influences the distance between the layers, called inter layer spacing (Tang *et al.*, 2012; Mittal, 2009). The lateral dimensions of the clay and its capacity to disperse into separate layers is crucial for the interactions between the polymer matrix and the clay in a nanocomposite. As such, the thickness of the clay layer strongly interferes with the polymer properties. Several researchers reports that 1 nm of layer thickness strongly improves the polymer properties, however as the dispersing between layers increases, the internal forces for agglomeration of individual layers also rises (Olad, 2011).

3.3. TiO₂ NPs-clay nanocomposites

Titanium dioxide is considered to have excellent resistance to corrosion in different environments, a low density and also the highest strength to weight ratio, which allows many potential applications, especially for titanium-based nanocomposite materials (Shahadat *et al.*, 2015). In fact, titanium-based organic or inorganic matrix materials have been considered more advantageous comparing to other materials because of their thermal and chemical stability (Aranda *et al.*, 2008; Shahadat *et al.*, 2015). There are several applications concerning titanium-based nanocomposites, for example removal and recovery of inorganic or organic pollutants, modified electrodes, catalysts, solar and microbial fuel cells, adsorbents, gas sensors, biosensors and biomedical applications (Mallakpoura and Shahangia, 2012). Older reports have considered titanium based nanocomposites, for instance degradable polymer-TiO₂ NPs nanocomposites, as environment-friendly and safe (Reijnders, 2009).

To overcome and even restrain the release of TiO₂ NPs into the environment, it has been proposed to immobilize them in crystalline substrates, facilitating the manipulation of these nanoparticles (Tokarsky *et al.*, 2012). It has been considered that immobilization with proper mineral nanomaterials is a good strategy to diminish the possible release of these nanoparticles into the environment (Tokarčíková *et al.*, 2014).

For some applications, such as photocatalytic materials (Stathatos *et al.*, 2012; Zhang *et al.*, 2014), TiO₂ NPs can be supported on materials that should be chemically inert or participate in the chemical processes that help improving the material function. One strong example of support material for TiO₂ NPs are natural and synthetic clays (Vimonses *et al.*, 2010; Tokarčíková *et al.*, 2014). In the last years, a huge attention has been given to TiO₂ NPs supported on inorganic clay minerals, especially for photocatalysis applications (Chong *et al.*, 2009; Vimonses *et al.*, 2010). Several authors claim that the synthesis of TiO₂ NPs embedded in porous clays structures avoid the formation of aggregates (Chen *et al.*, 2013; Yang *et al.*, 2013). The small size of TiO₂ NPs (4–30 nm) leads to the formation of aggregates in suspension, decreasing its effective surface area and photocatalytic efficiency. Thereby, clay minerals are able to maintain a large surface area and enhance the photocatalytic efficiency of the photocatalysts (Chong *et al.*, 2009). Additionally, clay minerals are considered to be stable supports, protecting the TiO₂ NPs from erosion (Kibanova *et al.*, 2009) and they can also act as electron acceptors or donors (Zhang *et al.*, 2014), as well as, are capable of catalyse several chemical reactions including polymerization, reduction, decomposition or acid–base reactions (Mallakpoura and Shahangia, 2012). Resulting from its improved properties, studies have been reporting that TiO₂-clay nanocomposites exhibit more photocatalytic activity than the single TiO₂ NPs (Belessi *et al.*, 2007; Kibanova *et al.*, 2009).

Beyond the different types of clay minerals, there are various that have demonstrated to be suitable matrix for anchoring of TiO₂ NPs. Montmorillonite is the most commonly used (Vimonses *et al.*, 2010) comparing to other clay minerals, such as vermiculite, kaolinite, saponite and hectorite (Tokarčíková *et al.*, 2014). However, the interaction forces of kaolinite minerals makes this a suitable substrates for the immobilization and support of TiO₂ NPs (Chong *et al.*, 2009; Tokarčíková *et al.*, 2014) (see figure 5). It was already mentioned in the literature that this nanocomposite is not dangerous either for the environment or human health, however this must be better evaluated and clarified.

In addition to combining the best properties of both components, it has been stated that micro-sized particles induce less toxicity than the nano-size ones (Kocbek *et al.*, 2010;

Roy *et al.*, 2014). In this context, nanocomposites gain more prominence, since they are obviously larger than the single nanoparticles and, consequently, present fewer toxic effects than most nanoparticles in biological systems.

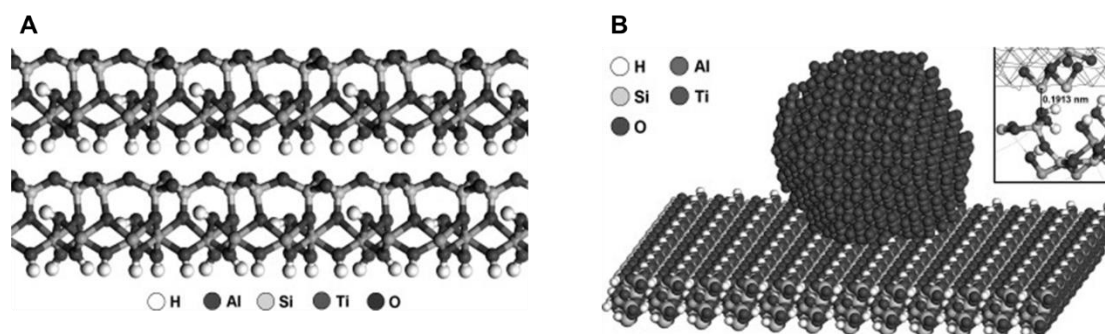


Figure 5. (A) Structure of kaolinite. (B) Model of TiO_2 nanoparticle anchored in the kaolinite clay structure. The upper right corner shows the newly formed Titanium–Oxygen bond between TiO_2 nanoparticle and the kaolinite mineral (adapted from Tokarčíková *et al.* (2014)).

3.4. Toxicity of clay based nanocomposites

So far, few studies have been made regarding the *in vitro* characterization of cellular responses to clay materials or clay based nanocomposites (Dawson and Oreffo, 2013). Generally, available studies demonstrated the occurrence of minimal loss of cell viability or proliferation for cells exposed to clays or materials incorporating this mineral. For instance, Zhuang *et al.* (2007) shown normal stromal cells morphology and proliferation after exposure to polymeric-clay scaffolds (i.e. gelatin – montmorillonite – chitosan) and Depan *et al.* (2009) observed also normal function of fibroblast after the presence of chitosan galactid acid montmorillonite composites. More recent studies performed by Li *et al.* (2010) verified no genotoxicity of exfoliated montmorillonite in Chinese hamster ovary cells, as well as, no long accumulation of this clay in any specific organ, after this being absorbed into the body.

In addition, other authors have demonstrated normal cellular responses and also cell adhesion and proliferation enhancements dependent on the clay concentration on polymeric substrates (Dawson and Oreffo, 2013). Studies performed in several cell lines including HepG2, human umbilical vein endothelial cells and skin fibroblasts cultured on the surface of poly-N-isopropylacrylamide hydrogels with certain specific clay concentrations, shown that the cellular adhesion and proliferation was strongly dependent on the clay content in the hydrogel, up to a critical concentration (Haraguchi *et al.*, 2006). Moreover, Zia *et al.* (2011) also evaluated the cytotoxicity of chitin based polyurethane bio-nanocomposites with different bentonite nanoclay (clay consisting mostly of

montmorillonite) concentrations, and realized that polymers with 2% of clay content were the preferred candidate for the surgical materials that were developing. The addition of the nanoclay drastically improved the tensile strength and also decreased the elongation at break of the biomaterial.

Most of the studies that look at clay induced-cytotoxicity found that significant effects were only observed after exposure to high concentrations of this mineral. For example, Han *et al.* (2011a) verified moderate cytotoxicity of clay minerals modified with an amine functional group in different cell types only at 1000 µg/mL. However, there are authors that described significant loss of A549 lung epithelial cells viability at much lower concentrations (25 µg/mL) after 24 hours of exposure to other nanoclays (Verma *et al.*, 2012). Another study observed both decrease of cell viability and ROS generation but at even lower concentrations of nanoclay (1 µg/mL) in HepG2 liver cell line (Lordan *et al.*, 2011). These authors also mentioned that the nanoclays tended to aggregate in the cell culture medium, which appeared to be correlated to the toxicity mechanisms observed (Lordan *et al.*, 2011).

In view of this, more studies are required to elucidate the potential mechanisms of cytotoxicity of certain clay formulations and their biocompatibility in living systems. One important aspect to take into account is the possible clay interactions with the components of the cell culture media, which may interfere with cell-clay interaction, influencing the cell viability (Dawson and Oreffo, 2013). Besides, is also needed to understand what are the possible pathways of biodistribution, bioaccumulation and cellular uptake of clay minerals particles in the human organism, and also their real impact on the environment (Reijnders, 2009; Dawson and Oreffo, 2013).

III. METHODOLOGY

1. Chemicals

MTT (CAS No. 298-93-1), neutral red dye (CAS No. 553-24-2), rezasurin (CAS No. 62758-13-8), Triton X-100 (CAS No. 9002-93-1), 2-mercaptoethanol (CAS No. 60-24-2), low melting point (LMP) agarose (CAS No. 39346-81-1), Tris-HCl (CAS No. 1185-53-1), 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid (HEPES) (CAS No. 7365-45-9), methyl methanesulfonate (MMS) 99% (CAS No. 66-27-3) and bovine serum albumin (BSA) (CAS No. 9048-46-8) were purchased from Sigma-Aldrich Co. Dimethyl sulfoxide (DMSO) (CAS No. 37-68-5), acetic acid (glacial) 100% (CAS No. 64-19-7), ethanol absolute (CAS No. 64-17-5), NaOH (CAS No. 1310-73-2), NaCl (CAS No. 7647-14-5) and KOH (CAS No. 105033) were bought from Merck KGaA. Cell culture media components and SyberGold were all Invitrogen™ and purchased from Thermo Fisher Scientific Inc. LDH protein from rabbit muscle (CAS No. 9001-60-9) and Tris base (CAS No. 77-86-1) were purchased from Calbiochem, while KCl (CAS No. 7447-40-7) and Na₂EDTA (CAS No. 6381-92-6) were purchased from Prolab. Finally, high purity 2-(4-Iodophenyl)-3-(4-nitrophenyl)-5-phenyltetrazoliumchlorid (INT) (CAS No. 146-68-9), phosphate-buffered saline (PBS) buffer (CAS No. 10049-21-5) and normal melting point (NMP) agarose were supplied from VWR chemicals, Lonza Group AG and Bionline, respectively.

2. Nanomaterial preparation and characterization

Nanomaterials suspensions under study (rutile TiO₂ NPs (NM-104)), high purity kaolinite clay and TiO₂ NPs immobilized in high purity kaolinite clay (C-TiO₂) were supplied by the Ceramic for Smart System Group of the Electroceramic Department, Instituto de Ceramica y Vidrio, CSIC, Madrid, Spain. The C-TiO₂ nanocomposite was prepared in accordance with the method previously described in the patent "Procedimiento para la dispersión de nanopartículas en seco y la obtención de estructuras jerárquicas y recubrimientos" (Fernandez *et al.*, 2010).

For the nanomaterial preparation, these were suspended in incomplete (serum-free media) and complete HepG2 cell culture media (300 µg/mL for TiO₂ NPs, 2700 µg/mL for kaolinite clay and 3000 µg/mL for C-TiO₂ nanocomposite). Afterwards, the suspensions were homogenized in a microfluidizer (Model LM10, Microfluidics International Corporation) at 12500 Psi, for three times, in order to obtain a correct homogenization. This procedure was performed in an interaction chamber with Y geometry (single-slotted) with suspensions placed in an ice-water bath.

Primary particle size, size distribution and particle morphology were characterized by Field-Emission Scanning Electron Microscopy (FE-SEM) with a resolution of 1.5 nm,

working at 20 kV with a current intensity of 10 μ A (Model S-4700, Hitachi Ltd. Corporation). Information on size distribution was calculated from measuring over 100 nanoparticles in random fields of view in addition to images that show general morphology of the nanoparticles.

Average hydrodynamic size and polydispersity index (PDI) of suspensions were measured by DLS, while zeta potential was determined by Laser Doppler Velocimetry (LDV) configuration, using a Zetasizer Nano-ZS equipped with 4.0 mW, 633 nm laser (Model ZEN 3600, Malvern Instruments Ltd.). For this evaluation, the nanomaterials suspensions were diluted into a 0.01 μ g/mL concentration.

Prior to each toxicity treatment and interference analysis, nanomaterials suspensions were sonicated in water bath for 5 min. Serial dilutions were carried out to obtain the different nanomaterial concentrations tested and sonicated in water bath for an additional 5 min prior to testing.

3. Cell culture

Hepatocellular carcinoma human cell line (HepG2) is a continuous cell line derived from a 15 years old Caucasian male who presented a well differentiated hepatocellular carcinoma. This cell line was obtained from the European Collection of Cell Cultures and was cultured in nutrient mixture DMEM (Dulbecco's modified Eagle's medium) medium with L-Glutamine (1%), antibiotic and antimycotic solution (1%), supplemented with 10% heat-inactivated fetal bovine serum (FBS).

Once cells reached 80% confluence in the T-flasks, they were transfer to new flasks with fresh medium. For that, culture medium was removed and the cell layer was washed with PBS. After this procedure, the confluent monolayer of cells was trypsinized (Trypsin 0.25%/EDTA 0.02% in PBS without Ca^{2+} , Mg^{2+}) and incubated at 37 °C for approximately 1 min. After cell detachment, trypsin was inactivated with cell culture media and the suspension was transferred to a conic tube and centrifuged for 5 min at 365 x g. The supernatant was discarded and the pellet resuspended in cell culture medium. The suspension was transferred to new T-flasks, and fresh new complete medium was added (subcultivation ratio of 1:3). Cells were incubated in a humidified atmosphere with 5% CO_2 and 37 °C.

All these procedures were performed in a laminar-flow chamber to ensure sterile conditions. All materials were manipulated using appropriate procedures in order to prevent external contamination.

3.1. Exposure conditions

To study nanoparticle uptake, cells were seeded at 2.5×10^4 cells per well in 96-well plates and allowed to adhere for 24 h at 37 °C. For the cellular internalization of the nanomaterials, 100 μ L of different suspensions of nanomaterials (25 and 300 μ g/mL for TiO₂ NPs; 225 and 2700 μ g/mL for kaolinite clay and 250 and 3000 μ g/mL for C-TiO₂ nanocomposite), both in complete (supplemented with FBS) and incomplete (without FBS) media, were incubated with cells for two periods of time (3 and 24 h). Cells not exposed to nanomaterials were used as negative control, for both media types. After the incubation period, treatment was removed from wells and cells detached with trypsin (1 min at 37 °C). Cell culture media was used to inactivate the trypsin and, subsequently, the content of each well was collected into microtubes and centrifuged (5 min at 3200 x g). The resulting pellet was resuspended in PBS for cytometry for final analysis in the flow cytometer.

For cytotoxicity assessment, cells were seeded at 2.5×10^4 cells per well in 96-well plates and allowed to adhere for 24 h at 37 °C. For each assay and each nanomaterial, 100 μ L of different suspensions of nanomaterials (5, 25, 50, 100, 200 and 300 μ g/mL for TiO₂ NPs; 45, 225, 445, 900, 1800 and 2700 μ g/mL for kaolinite clay and 50, 250, 500, 1000, 2000 and 3000 μ g/mL for C-TiO₂ nanocomposite), both in complete and incomplete medium, for different periods of time (3, 6 and 24 h) were evaluated. Complete or incomplete media was used as negative control and Triton X-100 (1%) in complete/incomplete media was used as positive control.

For genotoxicity assessment, cells were seeded at 2×10^5 cells per well in 12-well plates and then incubated for 24 h at 37 °C. For each nanomaterials, different concentrations were tested (5, 25 and 50 μ g/mL for TiO₂ NPs; 45, 225 and 445 μ g/mL for kaolinite clay and 50, 250 and 500 μ g/mL for C-TiO₂ nanocomposite) in both complete and incomplete medium, for two periods of exposure (3 and 24 h). Complete/incomplete media was used as negative control and MMS 100 μ M in complete/incomplete medium was used as positive control. Afterwards, the medium was removed from the wells, followed by washing the wells with PBS and finally cells were detached with trypsin (1 min at 37 °C). After inactivating the trypsin with cell culture media, the content of each well was collected into microtubes and three successive centrifugations were performed (3 min at 7500 x g). Between the 1st and 2nd centrifugations the pellet was resuspended in PBS and cell density was calculated in a Neubauer improved counting chamber (BLAUBRAND® Neubauer improved by BRAND®). The calculated volume with 2.5×10^4 cell/mL was transferred to a microtube with PBS and centrifuged to pellet cells.

4. Nanomaterial uptake

Cellular uptake of nanomaterials in HepG2 cells was evaluated by means of flow cytometry using a BD Accuri™ C6 Flow Cytometer equipped with BD Accuri C6 software (BD Biosciences). The analysis was carried out on the basis of the size and the complexity of the cells by measuring the forward scatter (FSC) and the side scatter (SSC). Figure 6 represents an exemplificative SSC-FSC plot; two regions were established for analysis (R4 and R5): events in R5 stand for cells that have incorporated the nanomaterials while events in R4 correspond to cells with normal inner complexity (without internalized materials).

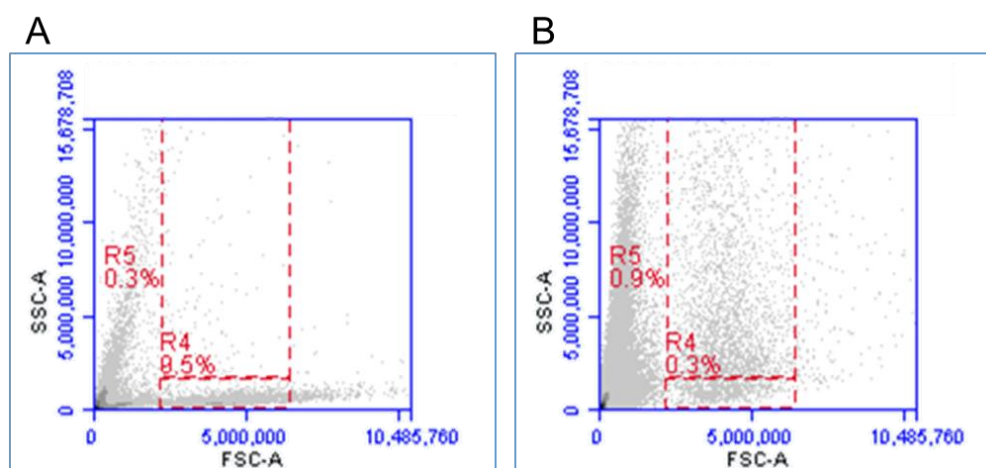


Figure 6. Plots obtained from the flow cytometry analysis: (A) Control sample (cells not exposed to nanomaterials); (B) HepG2 cells exposed to 25 µg/mL of TiO₂ NPs in incomplete medium. R4: HepG2 cells with no nanomaterial uptake; R5: HepG2 cells with internalized nanomaterials.

The percentage of cells with nanomaterials was calculated according to the following formula:

$$\% \text{Cells with Nanomaterials} = \frac{\text{Counts of events on the R5 gate}}{\text{Total counts of events on both R4 and R5 gates}} \times 100$$

5. Cellular viability and membrane integrity

In the present work, the cytotoxic effects of the different nanomaterials under study (TiO₂ NPs, kaolinite clay and C-TiO₂) were evaluated on HepG2 cell line. For the cell viability analysis it was proposed to employ MTT (Mosmann, 1983), NRU (Borenfreund and Puerner, 1985) and AB (Borra *et al.*, 2009) assays and for membrane integrity evaluation the LDH cytotoxicity assay. To evaluate if these assays were appropriate for the evaluation of nanoparticle toxicity, several interference studies were performed prior to cytotoxicity assessment.

5.1. Interference studies

To reveal possible interferences between nanomaterials and cytotoxicity assays experimental procedures, two main sets of experiments were conducted: (1) to analyze the influence of materials presence on optical measurements (light-absorption interference) and (2) to address possible nanomaterials reactivity with assay components (catalytic interference).

5.1.1. Optical interference: Evaluation of the nanomaterials interference with the light-adsorption

An exploratory analysis of nanomaterials absorbance spectrum was performed prior to the analysis of interference with early and final products of the cytotoxicity assays. Nanomaterials suspensions were prepared in water at different concentrations (0, 5, 25, 50, 100, 200 and 300 µg/mL for TiO₂ NPs; 0, 45, 225, 445, 900, 1800 and 2700 µg/mL for kaolinite clay and 0, 50, 250, 500, 1000, 2000 and 3000 µg/mL for C-TiO₂ nanocomposite) and analyzed by UV-Visible spectroscopy (ATi Unicam UV2 UV/Vis Spectrometer).

For MTT and NRU assays, light absorption interference was analyzed in the presence of dissolving agents (DMSO and fixative solution, for MTT and NRU assay, respectively) and reaction end-products (formazan dissolved in DMSO and neutral red dissolved in fixative solution). End-products were obtained by incubating live cells with MTT and NRU dyes. The nanomaterials suspensions were prepared in solvents and end-products at different concentrations (0, 25, 100 and 300 µg/mL for TiO₂ NPs; 0, 225, 900 and 2700 µg/mL for kaolinite clay and 0, 250, 1000 and 3000 µg/mL for C-TiO₂ nanocomposite). In turn, for the AB assay, the nanomaterials suspensions were prepared in both resazurin and resorufin (obtained after reduction with formic acid until obtain a pink colour).

The interference of the nanomaterials dispersions with the optical detection of the INT reduction during the LDH assay was performed by using oxidized and reduced INT. The reduced INT was obtained by adding 2-mercaptoethanol until obtain a red colour. To verify that the INT was entirely reduced, cells were exposed to Triton-X100 (1%) for 10 min and LDH assay was performed in the presence of reduced INT, prepared previously; light absorption was measured continuously at 492 nm using a Cambrex ELx808 microplate reader (Biotek, KC4) for 30 min at 37 °C, to observe a possible increase in absorbance due to INT reduction. The nanomaterials suspensions (0, 25, 100 and 300 µg/mL for TiO₂ NPs; 0, 225, 900 and 2700 µg/mL for kaolinite clay and 0, 250, 1000 and 3000 µg/mL for C-TiO₂ nanocomposite) were prepared by serial dilution in reduced and oxidized INT.

Absorbance was measured at 570 nm and 540 nm for MTT and NRU, respectively, at 570 nm with a reference wavelength of 630 nm for the AB assay, and at 490 nm for the LDH assay using a Cambrex ELx808 microplate reader (Biotek, KC4).

5.1.2. Catalytic interference: reactivity of the nanomaterials with the assay components

Nanomaterials reactivity with dyes was determined by incubating 100 μ L of nanomaterials suspensions 0, 25, 100 and 300 μ g/mL for TiO₂ NPs; 0, 225, 900 and 2700 μ g/mL for kaolinite clay and 0, 250, 1000 and 3000 μ g/mL for C-TiO₂ nanocomposite) prepared in complete and incomplete media with MTT, NRU and AB assays reagents in the absence of cells (4 h of incubation for MTT and AB, and 3 h for NRU). The absorbance was measured at the end of the incubation.

In case of LDH assay, positive control wells with only 100 mU of LDH protein (from rabbit muscle) were also included. The assay was carried according to the kit manufacturer's instructions (Cytotoxicity Detection Kit LDH, Cat. no. 11644793001, Roche Diagnostics Corp). Light absorption was measured continuously at 490 nm with a reference wavelength of 655 nm using a Cambrex ELx808 microplate reader (Biotek, KC4) for 1 h at 37 °C.

5.1.3. Interference on the enzymatic activity of LDH

For the LDH assay, an additional experiment was carried out to understand the possible interference of nanomaterials on the enzymatic activity of LDH, by either inactivating or adsorbing the LDH protein. Four concentrations of nanomaterials suspensions were tested (0, 25, 100 and 300 μ g/mL for TiO₂ NPs; 0, 225, 900 and 2700 μ g/mL for kaolinite clay and 0, 250, 1000 and 3000 μ g/mL for C-TiO₂ nanocomposite). For each concentration different units of LDH protein from rabbit muscle (20, 50, 100 and 500 mU) were tested in a 96-well plate and four periods of exposure were assessed (0, 15 min, 60 min, 3 and 24 h). After these time periods, 100 μ L of the kit reaction buffer was added and the remaining assay was carried according to the kit manufacturer's instructions (Cytotoxicity Detection Kit LDH, Cat. no. 11644793001, Roche Diagnostics Corp). Spectrophotometric absorption was taken at 490 nm with a reference wavelength of 655 nm using a Cambrex ELx808 microplate reader (Biotek, KC4).

6. Cytotoxicity assessment protocols

6.1. MTT

At the end of the exposure period, the treatment was removed and 100 μL of MTT reagent, prepared in incomplete medium (0.5 mg/mL), was added to the treated 96-well plates and incubated for 4 h at 37 $^{\circ}\text{C}$ in the dark. After removing the MTT, the formazan was solubilized with 200 μL DMSO. Thereafter, the plates were centrifuged (Universal 320, Hettich) at 4000 x g for 10 min and 100 μL of the supernatant were transferred to a new plate for the final reading. Absorbance was measured at 570 nm (MTT) using a Cambrex ELx808 microplate reader (Biotek, KC4).

6.2. Alamar Blue

The Alamar Blue reagent (200 μL), prepared in incomplete medium (20 $\mu\text{g}/\text{mL}$), was added to the treated 96-well plates after removing the treatment at the end of the exposure period and then incubated for 4 h at 37 $^{\circ}\text{C}$ in the dark. Similarly to MTT, the plates were centrifuged (Universal 320, Hettich) at 4000 x g for 10 min and 100 μL of the supernatant were transferred to a new plate for the final reading. Spectrophotometric absorbance was taken at 570 nm with a reference wavelength of 630, using a Cambrex ELx808 microplate reader (Biotek, KC4).

7. DNA integrity

7.1. Interference studies

To evaluate the possible interactions of nanomaterials with alkaline comet assay, two conditions were tested for each type of medium (complete or incomplete) and each type of nanomaterial (TiO_2 NPs, kaolinite clay or C- TiO_2 nanocomposite): (1) negative control (cells in cell culture medium); (2) lysis test (100 μL of nanomaterials at the highest concentrations under evaluation (300, 2700 and 3000 $\mu\text{g}/\text{mL}$ for TiO_2 NPs, kaolinite clay and C- TiO_2 nanocomposite, respectively) added just before running the assay).

7.2. Genotoxicity assessment protocol: Alkaline Comet Assay

Cells (in pellet) were embedded in 200 μL 0.6% LMP agarose gel (for the lysis test in the interferences assay, 100 μL of LMP agarose at 1.2% was used as it was added 100 μL of nanomaterials) and 5 μL drops were placed on microscope slides precoated with 1% agarose (the technique was carried out using a medium throughput system 12 gel comet assay unit, Severn Biotech Ltd®). After gel solidification, the slides were placed in a coplin

jar and immersed in lysis solution (NaCl 2.5 M, Na₂EDTA 100 mM, Tris-base 10 mM, NaOH 10 M, pH 10, supplemented with Triton-X 100 1%) during 1 h, to lyse the cells and separate DNA from histones. For unwinding of DNA, all slides were immersed in electrophoresis solution (Na₂EDTA 1 mM, and NaOH 0.3 M) in the electrophoresis platform for 40 min (with a cooler underneath the platform), followed by electrophoresis for 20 min (1.15 V/cm). Neutralization was performed with cold PBS (pH 7.2) for 10 min and cold deionized water for 10 min. Slides were fixed with ethanol 70% and 96% for 15 min each at room temperature and gels were dried overnight. As represented in figure 7, just before analysis, slides were stained with SyberGold in TE buffer (Tris-HCl 10 mM and EDTA 1 mM). Slides were visualized with a Nikon Eclipse E400 microscope attached to an epi-fluorescence illuminator Nikon C-SHG1 power supply for HG 100 W, with 250x magnification (Filter G-2A). Slides were analyzed using the Comet Assay IV Software (Perceptive Instruments). At least 100 cells were scored (50 for each replicate gel). The percentage of DNA in the comet tail (% tDNA) was used as DNA damage parameter.

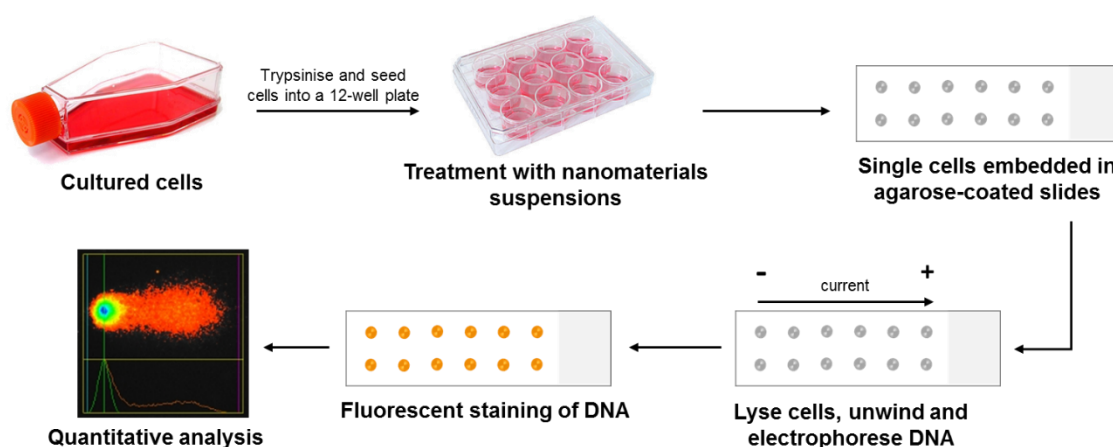


Figure 7. General procedure of the comet assay, based on the protocol described in the text.

8. Statistical analysis

Statistical analyzes were performed using SPSS for Windows statistical package (version 23.0). Non-parametric tests, Mann–Whitney U-test (differences among groups) and Spearman's correlation (associations between two variables) were used for the statistical analysis of data. A minimum of three independent experiments (in viability assays, three replicated were analyzed in each experiment) were performed for each experimental condition tested. Experimental data were expressed as mean \pm standard error and a p-value of 0.05 was considered significant.

IV. RESULTS AND DISCUSSION

1. Nanomaterial characterization

With the development of nanotoxicology it has become clear that the physicochemical characterization of nanosized materials is an essential step for the risk assessment of these materials on environment and human health. A proper evaluation of the nanomaterials properties is a basic stage for screening of the mechanisms of toxicity derived from exposure to these materials (Lopez-Serrano *et al.*, 2014; Guadagnini *et al.*, 2013).

In this work, a primary characterization of C-TiO₂ nanocomposite was performed, as well as of their individual constituents: TiO₂ NPs and kaolinite mineral. Those materials were characterized after dispersion in water and biological media to understand their behaviour in the conditions as these are presented to cells. Besides, dispersion in culture media may alter original physico-chemical properties. In these conditions, nanomaterials may suffer several alterations regarding the size (e.g. altered aggregation or agglomeration state, adsorbed proteins), the particle charge, among others (Oh and Park, 2014).

The particle size is the most basic characteristic of nano-sized materials and is crucial to understand the possible mechanisms of distribution and retention of the particles in living tissues (Cho *et al.*, 2013). The most common methods for size determination are microscopy (for instance, transmission electron microscopy (TEM) and scanning electron microscopy (SEM)) and light scattering techniques, such as dynamic light scattering (DLS). While microscopy techniques allow an accurate assessment of size and morphology of the particle by image analysis, DLS measures the size and size distribution but in relevant aqueous or biological solutions (Dhawan *et al.*, 2009).

Figure 8 presents four FE-SEM micrographs of different scale magnifications of the TiO₂ NPs under evaluation. Although most existing TiO₂ NPs are a mixture of rutile anatase forms (Becker *et al.*, 2014), the present nanoparticles were only constituted by the rutile form. These nanoparticles were obtained from the JRC repository (NM-104) and are characterized as being thermal and hydrophilic. As represented in figure 8.C, these rutile TiO₂ NPs were found to be nearly spherical agglomerates with different particle size.

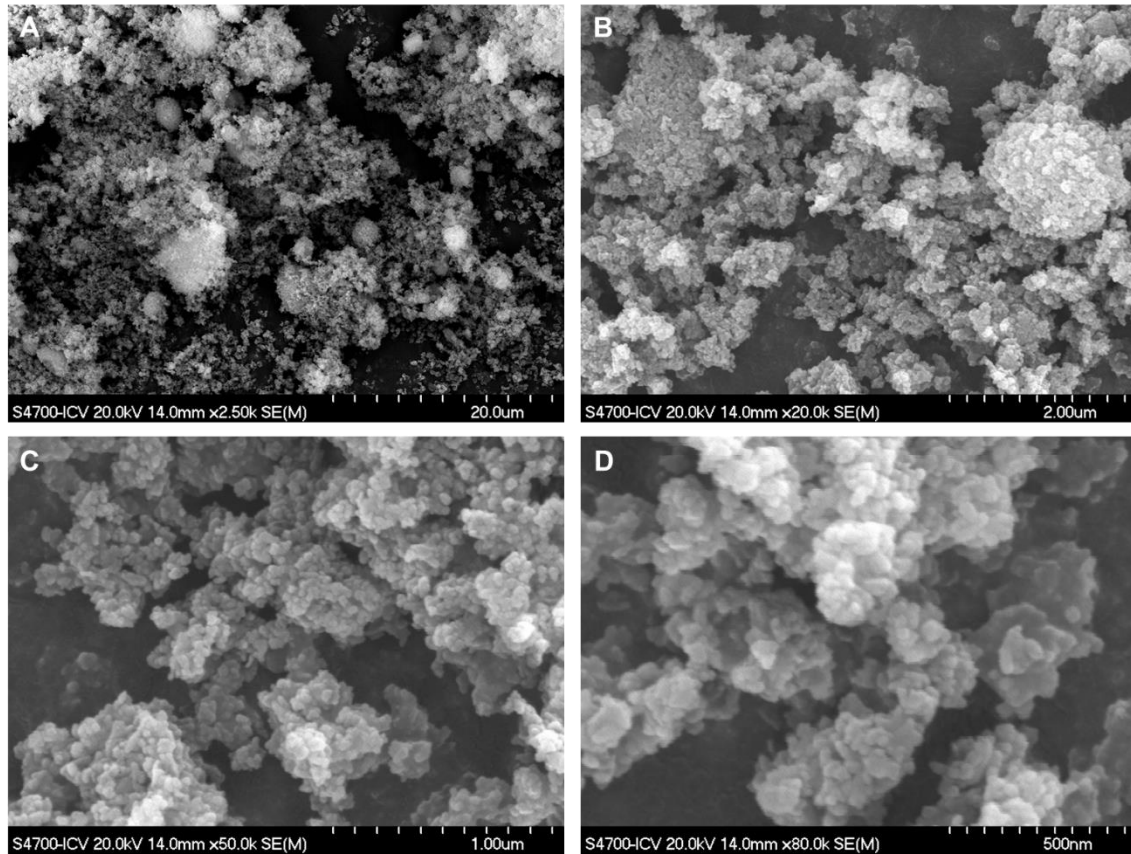


Figure 8. FE-SEM micrographs from TiO₂ NPs in four magnification scales: (A) 20.0 μm; (B) 2.0 μm; (C) 1.0 μm; and (D) 500 nm. Particles were supplied by the Ceramic for Smart System Group of the Electroceramic Department, Instituto de Ceramica y Vidrio, Madrid, Spain.

Regarding the clay mineral, it was a high purity kaolinite mineral with laminar structure of alumina and silica with a general formula of $\text{Al}_2\text{Si}_2\text{O}_5(\text{OH})_5$, as already mentioned in previous sections. Kaolinite is a 1:1 clay mineral structure with layer thickness of 0.7 nm and its layers are held together by weak hydrogen bonding along with dipole-dipole and van der Waals interactions (Maisanaba *et al.*, 2015).

Layered silicate structures generally crystallizes into micro and nano-sized particles (Dawson and Oreffo, 2013), as was also noted in this work. The studied kaolinite clay presented agglomerates of particles with a spherical morphology and with irregular laminar shape (Fig. 9.A and 9.B). The agglomerates were formed by plates of nano-sized kaolinite (Fig. 9.C and 9.D).

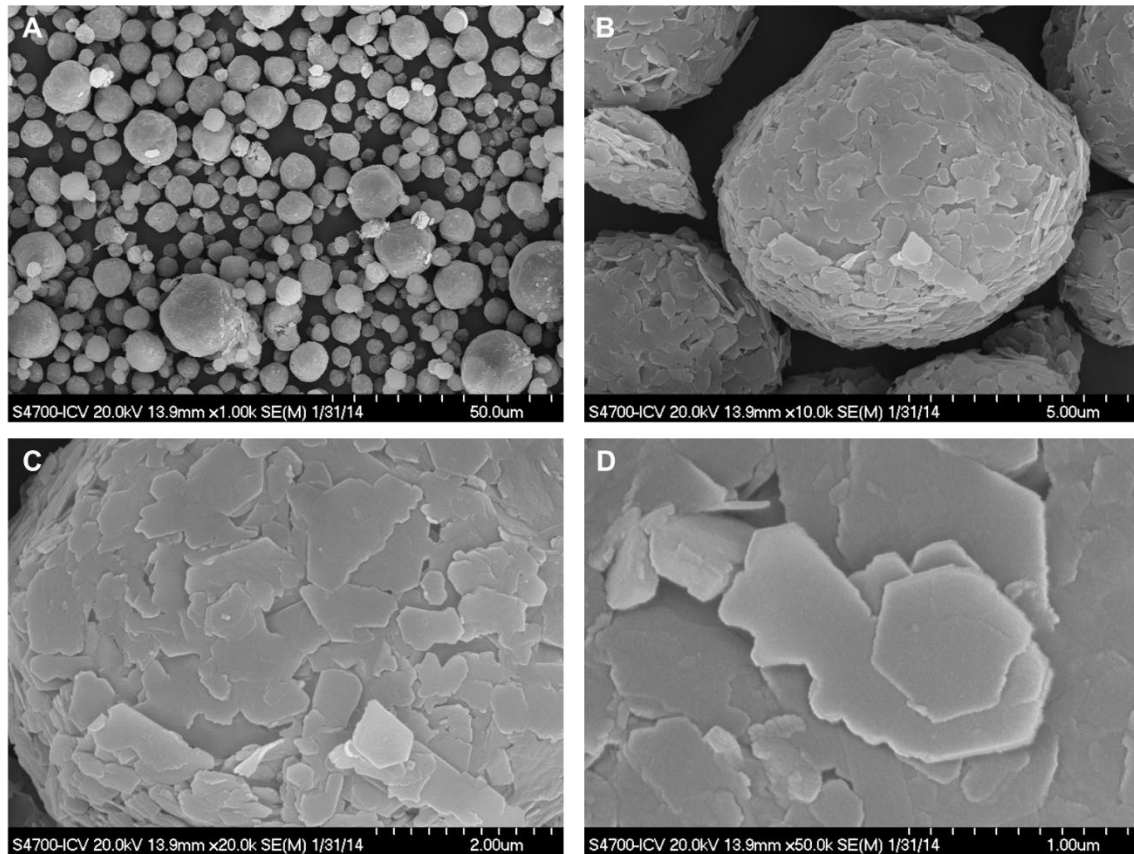


Figure 9. FE-SEM micrographs from kaolinite agglomerate particles in four magnification scales: (A) 50.0 μm ; (B) 5.0 μm ; (C) 2.0 μm ; and (D) 1.0 μm . Particles were supplied by the Ceramic for Smart System Group of the Electroceramic Department, Instituto de Ceramica y Vidrio, Madrid, Spain.

The nanokaolin layered silicates represented 90% of the C-TiO₂ nanocomposite constitution. The remaining 10% were for the rutile TiO₂ NPs, immobilized on the nanokaolin for the formation of these nanocomposites. Figure 10 illustrates the FE-SEM images obtained from the C-TiO₂ nanocomposites. Through the magnifications of the figures 10.B and 10.C it is possible to distinguish the nanokaolin clay (Fig. 10.B.2) from the TiO₂ NPs (Fig.10.B.1), as well as the TiO₂ NPs immobilized on the kaolinite laminar structures (Fig.10.B.1 and Fig.10.C.1). These micrographs show that these nanocomposites were not spherical.

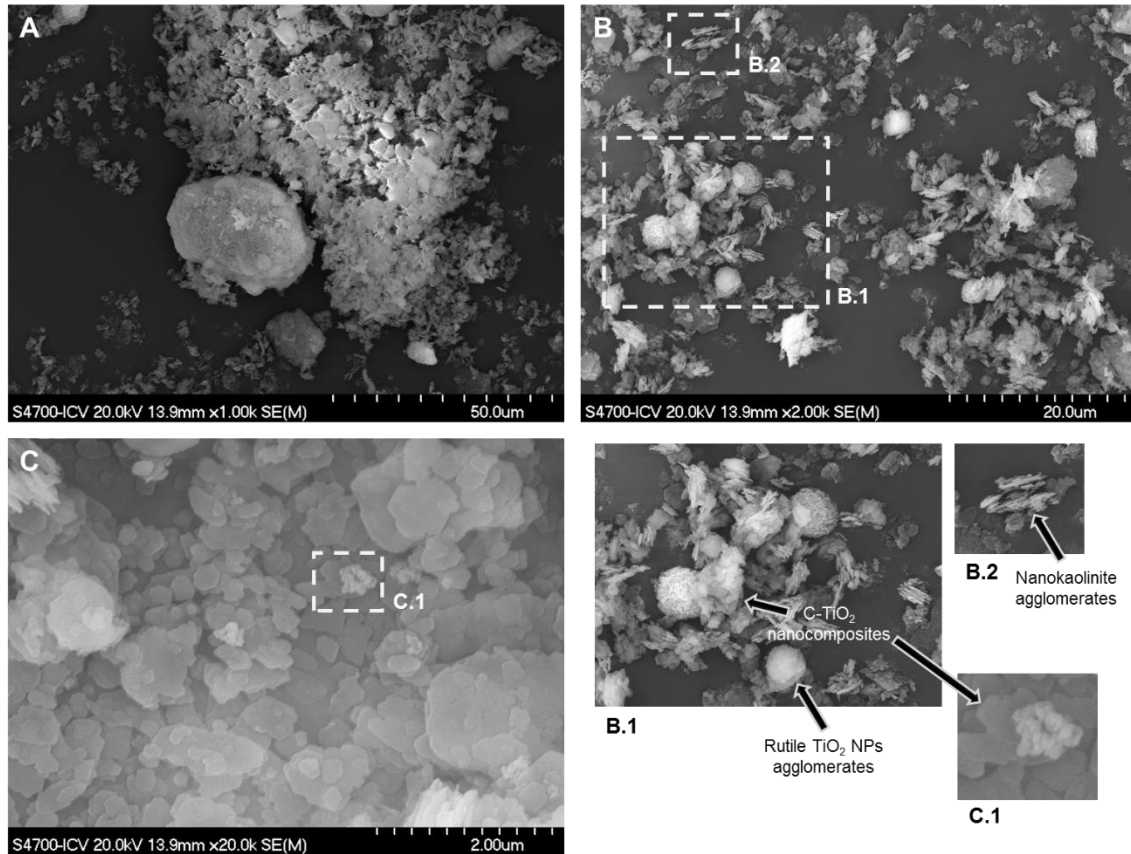


Figure 10. FE-SEM micrographs from C-TiO₂ nanocomposites in four magnification scales: (A) 50.0 μm; (B) 20.0 μm; and (C) 2.0 μm. Composites were supplied by the Ceramic for Smart System Group of the Electroceramic Department, Instituto de Cerámica y Vidrio, Madrid, Spain.

From the TiO₂ NPs and kaolinite micrographs (Figures 8 and 9) it was also possible to determine their size distribution, as represented in the figure 11. The TiO₂ NPs presented a size range from 0.01 to 0.1 μm, being the 0.04, 0.05 and 0.06 μm the most prevalent sizes (Fig. 11.A). This size range is coincident with the one reported by the JRC, that characterize the NM-104 nanoparticles with a particle size from 0.01 to 0.03 μm (Rasmussen *et al.*, 2014). The present analysis also confirms that this examined material is qualified as an ENM according to the European Commission definition (EPC, 2011).

On the other hand, the kaolinite particle agglomerates exhibited a superior size range between 0.1 to 1.4 μm, with most of them showing a predominant size 0.6 and 0.7 μm (Fig. 11.B).

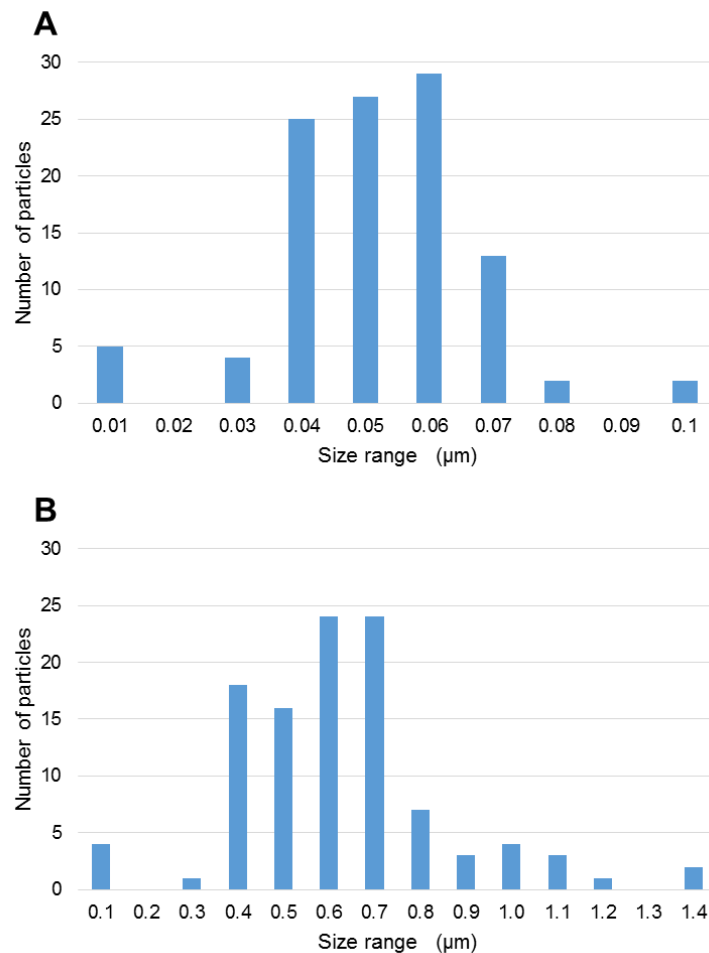


Figure 11. Size distribution of (A) TiO₂ NPs and (B) kaolinite mineral obtained from image analysis of FE-SEM micrographs.

The primary particle size is sometimes a misleading parameter particularly when considering the aggregation and/or agglomeration propensity of most nanomaterials in biological medium (due to the salts and proteins in their constitution) (Verma *et al.*, 2012). Therefore, the hydrodynamic size, polydispersity index (PDI) and zeta-potential of the C-TiO₂ nanocomposite and its individual components were evaluated by DLS to understand the nanomaterials behaviour and aggregation after dispersion in liquids.

DLS measures the Brownian motion which determines the hydrodynamic diameter of particles. The Brownian motion is defined as “the random movement of particles in a liquid due to the bombardment by molecules that surround them” (Malvern, 2004). It is the speed of particles movements into the liquid that enables the determination of size (Appendix A; Fig. A 1). While small particles move quickly, the large ones move slowly in the liquid (Malvern, 2004). As particles tend to aggregate in aqueous state, DLS size measurements show higher size than individual particles (Dhawan *et al.*, 2009). Another parameter given by the DLS technique is the PDI, that indicates if a nanoparticle sample is

monodisperse (small PDI values) or polydisperse (high PDI values) in the liquid solution (Appendix A; Fig. A 2).

Several studies demonstrate that nanoparticles stability varies in different liquid media, depending on the ionic strength and protein composition of the solution. For instance, nanoparticles stable in water can form large aggregates in physiological solutions or similar conditions, reducing their stability (Pavlin and Bregar, 2012). For this reason, nanomaterials characterization in relevant media is essential for toxicity evaluation, since interaction with biological fluids components may influence nanomaterial behaviour and communication with cells (Balog *et al.*, 2015; Allouni *et al.*, 2015). Culture media or FBS contain simple ions and peptides that can exhibit different charge groups at physiological conditions, contributing to a formation of a transient or permanent protein corona (Pavlin and Bregar, 2012). Pavlin and Bregar (2012) and his co-workers establish that proteins from the media strongly affects the stability of the nanoparticles, i.e., the protein corona formation and opsonisation around nanoparticles may destabilized the nanoparticles suspensions and contribute to a certain degree of flocculation and sedimentation of the nanoparticles.

In this regard, the DLS is a useful technique to evaluate the nanomaterials properties in relevant biological media, giving more “realistic” information of the nanomaterials behaviour than others techniques, for example TEM or SEM (Balog *et al.*, 2015).

In addition to hydrodynamic size, Zetasizer Nano-ZS also provides the value of zeta potential in solutions with different pH and ionic strength measured by the LDV configuration. Zeta potential plays an important role in the nanoparticle characterization since it delivers an indirect measure of the net charge of the particle and is also a parameter of particle diffusion degree in the medium (Dukhovich, 2004). In fact, the zeta potential is defined as the existing potential between particle surface and the dispersing liquid, giving the potential stability of the colloidal system (Malvern, 2004; Salgın *et al.*, 2012) (Appendix A; Fig. A 3). The larger the absolute values of zeta, the greater the ability of nano-sized particles to disperse; conversely, as the zeta potential is close to zero, the particles become unstable and tend to aggregate (Murdock *et al.*, 2008). Basically, the high absolute value of zeta potential enables a stable suspension of the materials due to the strength derived from the electrostatic repulsion force (Verma *et al.*, 2012).

The studied nanomaterials were characterized after dispersion in water, the cell culture media supplemented with bovine serum and also in serum-free cell culture media. In all aqueous solutions, TiO₂ NPs exhibited the smallest hydrodynamic size, when compared to the remaining materials (Table 2). As expected, C-TiO₂ nanocomposite presented higher size than the TiO₂ NPs and nanokaolin.

Curiously, the C-TiO₂ nanocomposite tended to agglomerate more in water than in the both tested biological media, presenting the size of 7289 nm and a PDI of 1, which means that, in water, the C-TiO₂ nanomaterials are strongly polydispersed. In cell culture media, it presented higher size in serum free medium (2419 nm) than in complete media (470 nm); however the PDI was very similar in both media.

Similarly to the nanocomposite, both TiO₂ NPs and kaolinite clay presented higher hydrodynamic sizes in incomplete medium than in complete medium. These results suggest that the absence of serum leads to an increase in the agglomeration state, i.e., serum proteins allowed a better dispersion of these materials, which can be proven by the obtained PDI for each material. Actually, they appeared to be more stable and monodispersed in complete medium than in serum free medium.

Table 2. TiO₂ NPs, kaolinite mineral and C-TiO₂ nanomaterial characterization. Average hydrodynamic size and polydispersity index (PDI) of particles in suspension in water, incomplete and complete HepG2 culture media were determined by dynamic light scattering (DLS), while ζ – potential was measured by laser Doppler velocimetry (LDV) configuration.

		DLS		LDV	
		Average hydrodynamic size (nm)	PDI	ζ – potential	pH
	H2O*	196.7	0.308	41.6	6.63
TiO₂ NPs	HepG2 incomplete medium*	447.2	0.635	**	7.58
	HepG2 complete medium*	236.6	0.223	**	7.80
	H2O*	508.4	0.244	-39.0	6.86
Kaolinite	HepG2 incomplete medium*	2675.0	0.617	**	7.72
	HepG2 complete medium*	447.5	0.474	**	7.91
	H2O*	7289.0	1.000	10.4	6.56
C-TiO₂	HepG2 incomplete medium*	2419.0	0.433	**	7.62
	HepG2 complete medium*	470.0	0.471	**	7.82

* measured at 0.01 $\mu\text{g}/\text{mL}$

** media components did not allow a correct assessment of the ζ – potential of the materials

As reported in the literature, proteins adsorbed by nanomaterials to their surface may influence key parameters such as their hydrodynamic size and, sometimes, colloid stability (Baalousha, 2009). As observed in the present work, other previously published studies have demonstrated that TiO₂ NPs create larger agglomerates in cell culture medium than in water, which result in increased hydrodynamic size (Valdiglesias *et al.*, 2013; Wang *et al.*, 2014). Adsorption of proteins may, on one hand, increase the size of nanoparticles

but also contribute to the stability of the dispersion as observed in this work, since the TiO₂ NPs presented lower values in complete medium than in incomplete medium.

Regarding the zeta potential in water, the TiO₂ NPs showed the largest absolute value (ζ – potential of 41.6) and, therefore, were found to be the most stable suspension, while the C-TiO₂ nanocomposite were the less stable (ζ – potential of 10.4).

When attempting to perform zeta potential measurements in the LDV configuration, it was found that the ionic strength of the solution impacted measurement reproducibility as the high salt content would interfere with the electrodes in the capillary tube. Additionally, when other media components, such as fetal bovine serum, were present, it would give a very broad distribution of charges with a peak close to 0 mV due to the wide distribution of charges from both particles and proteins (Murdock *et al.*, 2008).

2. Nanomaterial uptake

An exploratory analysis of the uptake of studied nanomaterials by HepG2 was performed to better understand the possible cytotoxic effect assessed further on. Two periods of exposure (3 and 24 h) and two media types (serum free and FBS supplemented) were evaluated to clarify the influence of serum proteins on nanomaterial internalization by hepatocytes over time.

Results obtained show that after 3 hours of exposure to TiO₂ NPs, these were able to be internalized by HepG2 cells in both media (Figs. 12.A and 12.B). However, in incomplete medium it was observed a significantly higher percentage of material uptake for the lowest concentration (~75%) than the one observed for the same conditions in complete medium (~10%) suggesting that the presence of FBS strongly interferes with TiO₂ NPs internalization by preventing it when nanoparticles are present in small amounts.

Additionally, for incomplete medium (and 300 µg/mL in complete medium) it was observed higher TiO₂ NPs uptake after 3 hours of exposure than after 24 hours period. This can be either due the fact that HepG2 cells started to identify these nanoparticles, avoiding their internalization or due to a dynamic equilibrium that has been reached after this period of exposure (Murugan *et al.*, 2015; Oh and Park, 2014).

Cell internalization of TiO₂ NPs has been described in different human cell lines (Valdiglesias *et al.*, 2013; Jaeger *et al.*, 2012), namely HepG2 (Shukla *et al.*, 2013; Petković *et al.*, 2011). Some authors support that internalization of TiO₂ NPs with different range of primary sizes, shapes or crystal phases (anatase, rutile or both forms), may occur in several mammalian cells (Janer *et al.*, 2014). These previous publications describe concentration

dependent increase of TiO₂ NPs cellular internalization over time (after 3 and 6 h) in complete medium (Valdiglesias *et al.*, 2013; Shukla *et al.*, 2013); yet, none of these authors performed an analysis of the internalization pattern in complete and incomplete media.

Regarding the nanokaolin, it was observed increased cellular uptake in complete medium than in serum free medium (Figs. 12.C and 12.D), suggesting that the presence of serum proteins improves kaolinite internalization by HepG2.

Results obtained for the internalization of C-TiO₂ nanocomposites in complete medium were very similar to the ones observed for the nanokaolin (Figs. 12.D and 12.F). Once these nanocomposites are mostly constituted by kaolinite, it is in fact expected that these behave similarly.

However, in incomplete medium, increased uptake of C-TiO₂ nanomaterials in HepG2 was observed when compared to what was seen for kaolinite. This can be related to differences in size and stability of the nanocomposite in complete and incomplete media.

In fact, the size of the nanomaterial is an important parameter for the uptake (Tenzer *et al.*, 2011). Usually smaller particles sizes or even smaller agglomerates have higher cellular uptake than larger agglomerates (Prasad *et al.*, 2014).

In addition to the size parameter, the real influence of the protein corona in the cellular internalization mechanism of nanomaterials is not fully understood. Human serum albumin and γ -globulins included in FBS used to supplement the complete medium often coat micro-sized materials forming a protein corona, modifying the size, agglomeration state, surface charge of the nanomaterials, potentially interfering with their cellular uptake (Allouni *et al.*, 2015). These proteins are recognized as safe by the HepG2 cells, simplifying the entrance of nano and micro-sized particles. In this context, some authors report that nanoparticles suspended in the presence of serum proteins show higher uptake while others observed the same phenomenon but in serum free biological solution (Allouni *et al.*, 2015). In the present work, this same singularity was found: TiO₂ NPs were better internalized by HepG2 cells in incomplete medium while for nanokaolin and C-TiO₂ nanocomposite the opposite was observed.

Protein adsorption to nanomaterials is a dynamic process that tends to increase over time of exposure. In *in vitro* systems models, as used herein, cells are attached to the bottom of the well, which leads to less contact of the adsorbed materials with cells since increased protein adsorption retains the particle in the biological suspensions for longer periods. Thereby, serum free medium will increase the fast sedimentation of the nanomaterials, providing an early cell-nanomaterial contact (Allouni *et al.*, 2015). In the

absence of serum proteins, the cellular uptake may be resultant from direct recognition of the materials at the cell surface instead of the recognition of the protein corona in media supplemented with serum proteins (Allouni *et al.*, 2015), as possibly happened with the TiO₂ NPs for shorter times of exposure.

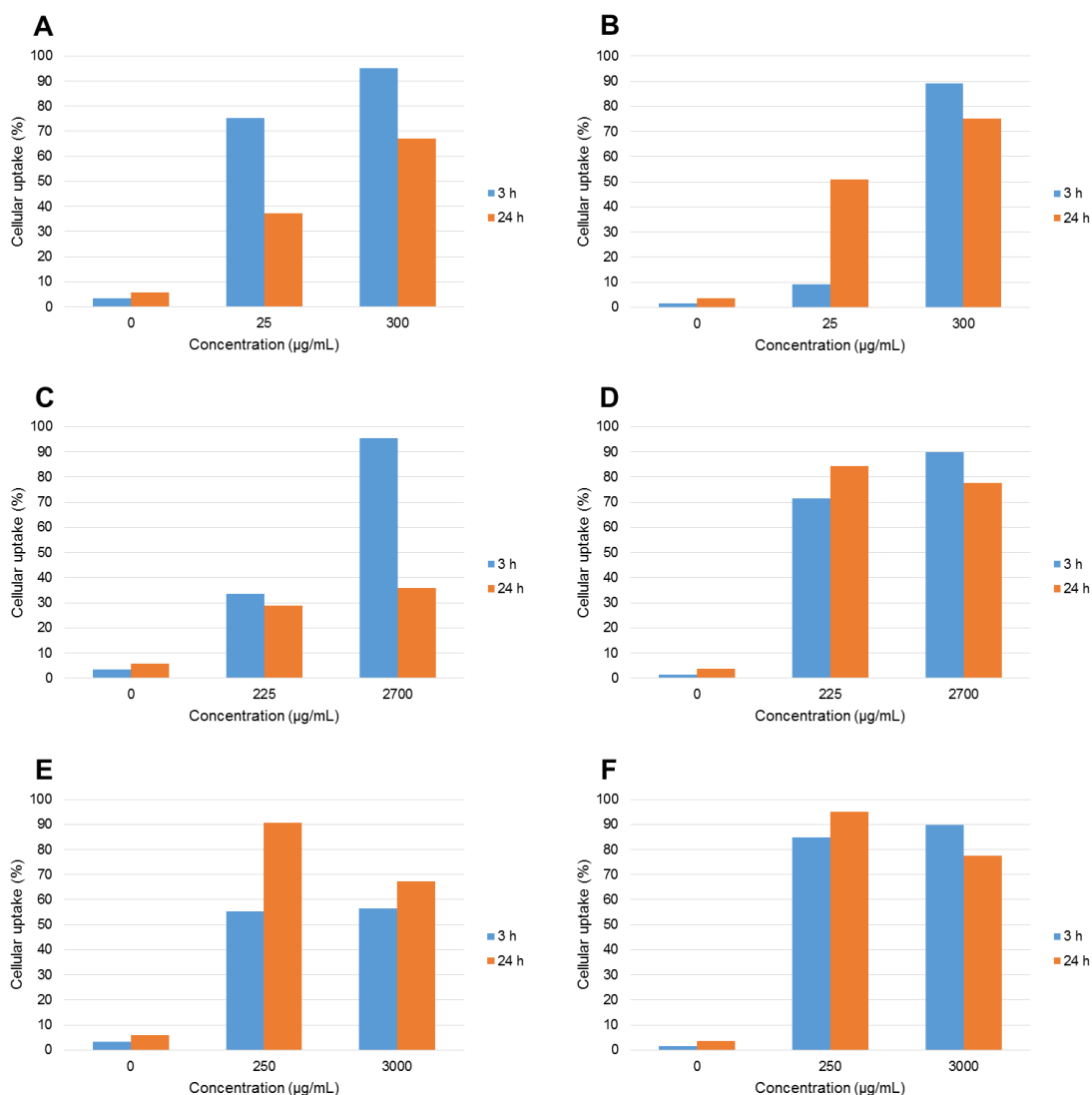


Figure 12. Cellular uptake of TiO₂ NPs, nanokaolin and C-TiO₂ nanocomposites by HepG2 cells as analyzed by flow cytometry. (A) TiO₂ NPs in incomplete medium; (B) TiO₂ NPs in complete medium; (C) Nanokaolin in incomplete medium; (D) Nanokaolin in complete medium; (E) C-TiO₂ nanocomposite in incomplete medium; (F) C-TiO₂ nanocomposite in complete medium.

Still, concerning the kaolinite mineral, possibly due to their constitution, this material could induce more protein adsorption than the TiO₂ NPs, which can be related to their increase cellular uptake by the HepG2 cells in FBS supplemented medium. This explains why the C-TiO₂ nanocomposite, mostly constituted by kaolinite, were better internalized in complete medium.

3. *In vitro* cytotoxicity of the nanomaterials in the HepG2 cell line

In the present work, it was intended to evaluate the cytotoxic effects of different nanomaterials (TiO₂ NPs, nanokaolin and C-TiO₂ nanocomposite) on hepatocellular carcinoma human cell line. For this purpose, four cytotoxic assays were chosen: MTT, NRU and AB assays for cellular viability and LDH assay for membrane integrity evaluation.

The most common method for cell viability determination is the MTT assay (Love *et al.*, 2012). MTT is a sensitive, quantitative and reliable colorimetric assay (Vega-Avila and Pugsley, 2011) that allows the detection of mitochondrial activity (Kroll *et al.*, 2009). Dehydrogenase is a mitochondrial enzyme capable to reduce the water soluble MTT reagent (yellow) into formazan (dark purple) crystals, which are subsequently solubilized by DMSO and quantitated by colorimetry (Takhar and Mahant, 2011) (schematic representation of the MTT principle presented in appendix B, Fig. B 1).

Another assay also widely used for measure the cellular viability is the AB assay (Love *et al.*, 2012). Alamar Blue is a cell viability indicator of the redox potential of cells (Takhar and Mahant, 2011). The main reagent of this technique is resazurin (7-hydroxy-10-oxidophenoxazin-10-ium-3-one). Resazurin is water soluble, non-toxic and stable in culture medium and that easily crosses the cell membrane (Rampersad, 2012). Viable cells reduce resazurin (blue) into resorufin (red), generating a quantitative measure for cytotoxicity of the cells (Takhar and Mahant, 2011) (see schematic representation of the AB principle in the appendix B, Fig. B 2).

AB works similarly as MTT since it is based on the conversion of resazurin to resorufin by mitochondrial enzymes (e.g. NADPH, NADH and cytochromes). Nonetheless, in addition to mitochondrial reductases, other enzymes (e.g. diaphorases, flavin reductase, among others) located in the cytoplasm and the mitochondria may also be able to reduce resazurin. Thereby, AB assay may imply an impairment of cellular metabolism but it is not necessarily related to mitochondrial dysfunction (Rampersad, 2012).

Since nanoparticles are frequently internalized and stored inside the lysosomes, this organelle is, consequently, one main target for nanoparticle accumulation possibly leading to lysosomal dysfunction. This possible destabilization of the lysosome membrane can induce oxidative stress through ROS generation, mitochondria damage and cell death (Frohlich, 2013). As such, lysosome dysfunction is often evaluated using the NRU cytotoxicity assay.

Neutral red (3-amino-7-dimethylamino-2-methylphenazine hydrochloride) is a weak cationic dye that evaluates the integrity of the lysosomes (Kroll *et al.*, 2009; Takhar and

Mahant, 2011). Neutral red is able to enter in the cells by non-ionic diffusion and accumulate in the lysosomes of viable cells (Kroll *et al.*, 2009; Takhar and Mahant, 2011), where it becomes positively charge and is thus retained inside these organelles. When the integrity of the lysosome membrane is changed, it loses the ability to retain the dye inside (see schematic representation of the NRU principle in the appendix B, Fig. B 3). Therefore, this sensitive assay evaluates cytotoxicity through neutral red reduction, evaluating the cell integrity and growth inhibition, providing an estimation of the number of viable cells in culture (Repetto *et al.*, 2008).

The determination of total LDH content in the extracellular medium is the principle of the LDH assay and intends to evaluate the cytoplasmic membrane integrity of cells and, subsequently, is an indicator of apoptosis and/or necrosis through physical damage of the cell membrane (Love *et al.*, 2012). This colorimetric and enzymatic assay measures the level of LDH released from damaged cells (Han *et al.*, 2011b) that catalyse the reaction represented in the appendix B Fig. B 4. NAD⁺ is reduced to NADH/H⁺ catalysed by the LDH conversion of lactate to pyruvate. Secondly, H/H⁺ from NADH/H⁺ is transferred to the INT yellow salt which is oxidized to a red formazan (Kroll *et al.*, 2009; Takhar and Mahant, 2011).

Most of the cytotoxic assays were developed for the evaluation of conventional drug compounds *in vitro*. In fact, researchers have realized that not all cytotoxicity assays are appropriate for the evaluation of nanoparticle toxicity (Frohlich, 2013) as several nanoparticles are capable to interfere with these methods (Love *et al.*, 2012). For instance, the binding and possible inactivation of assay components involved and the interference with colorimetric detection are examples of nanoparticle interference on the cytotoxic assays (Frohlich, 2013). For a correct assessment of the cytotoxicity of the nanoparticles under evaluation, possible nanoparticle-assay interactions need to be identified.

3.1. Interference studies

To reveal possible interferences between materials and cytotoxicity assays experimental procedure, three sets of experiments were conducted: (1) light-absorption interference of the nanomaterials in water; (2) light absorption interference with the early and final assay components; and (3) interference on the catalytic activity of the assay (Wang *et al.*, 2012; Guadagnini *et al.*, 2013). The first two experiments intended to analyze the influence of materials presence on absorbance measurements while the third addressed possible nanomaterials reactivity with assay components. For the LDH assay, an additional experiment was conducted, evaluating the interference of nanomaterials on the enzymatic activity of LDH (Han *et al.*, 2011b; Kroll *et al.*, 2012; Holder *et al.*, 2012).

In this first set of experiments, all nanomaterials seemed to interfere with light-absorption when suspended in water, as the absorbance increased with the increase of nanomaterial concentration (Figure 13). However, for nanokaolin and C-TiO₂, this tendency is observed only up to the 4th concentration for nanokaolin (900 µg/mL) and the 3th concentration for C-TiO₂ (500 µg/mL); at higher concentrations the signal decreases or stabilizes. This exploratory analysis suggested that both nanokaolin and C-TiO₂ nanomaterials interfere with light-absorption in a concentration dependent manner at the lower tested concentrations. Light absorption of rutile TiO₂ NPs was also concentration dependent but was found to be lower than the observed for the remaining nanomaterials under evaluation (with the exception of the highest tested concentration, in which the signal was similar to the other nanomaterials).

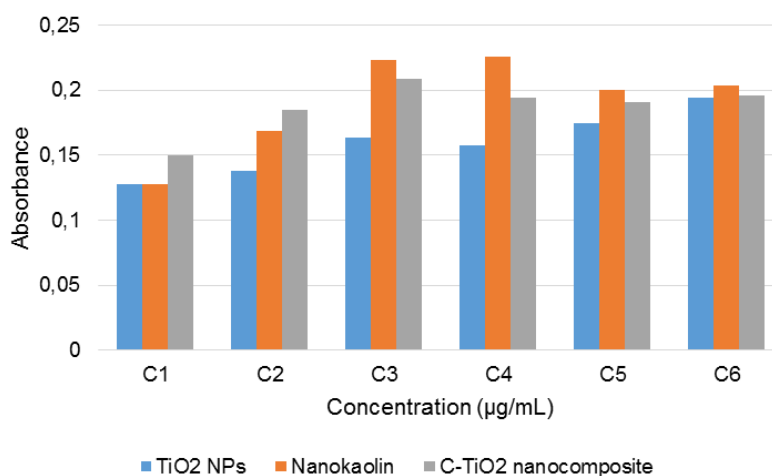


Figure 13. Evaluation of the nanomaterials interference with the light-adsorption in water. Concentrations (µg/mL): TiO₂ NPs: C1 – 5, C2 – 25, C3 – 50, C4 – 100, C5 – 200, C6 – 300; Nanokaolin: C1 – 45, C2 – 225, C3 – 450, C4 – 900, C5 – 1800, C6 – 2700; C-TiO₂: C1 – 50, C2 – 250, C3 – 500, C4 – 1000, C5 – 2000, C6 – 3000.

The remaining interferences studies were carried out separately for the cellular viability and the membrane integrity assays.

In all viability assays under evaluation (MTT, AB and NRU), the tested materials were capable to interfere with both early and final products of the respective assays (Figure 14) introducing bias in the final result.

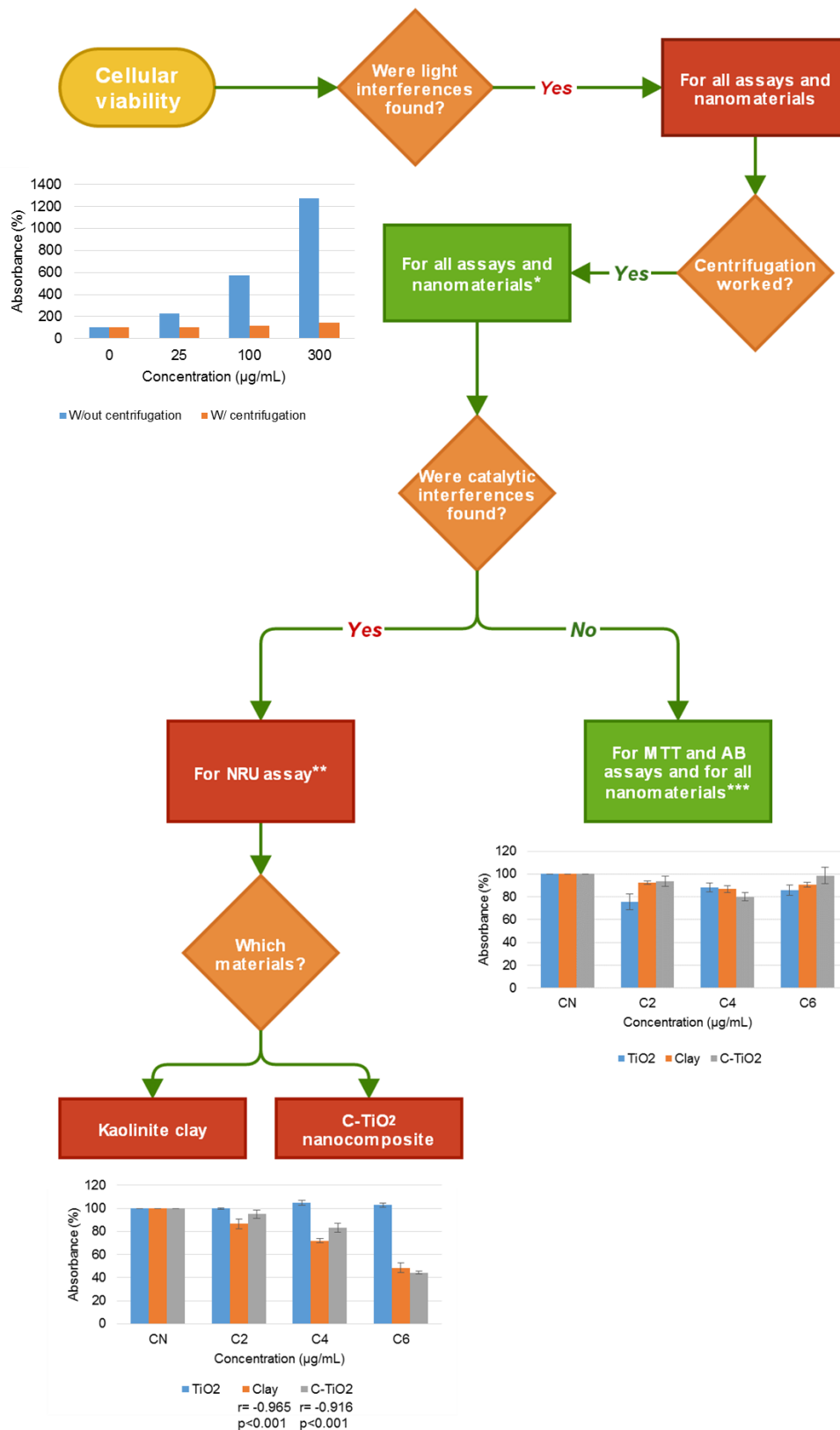


Figure 14. Schematic representation of the cellular viability (MTT, AB and NRU assays) interference studies. *As results were found to be similar in early and final products, only MTT results for the final product (DMSO) are presented; **Since the results in incomplete and complete medium were similar, only results in complete media were presented; ***Only MTT results in complete media are shown since results for MTT and AB catalytic interference were found to be similar.

To obviate this interference due to nanomaterial presence in assay reading, the plates were centrifuged before absorbance measurements. This procedure was enough to diminish or completely eliminate the optical interference of these nanomaterials since, after centrifugation, the absorbance obtained was similar to the one of negative controls (without nanomaterials in the early and final products of the assays).

Regarding the nanomaterials reactivity with the assay components, all nanomaterials concentrations exhibited a similar signal compared to the negative control for the MTT and AB assays in both media, which attested that no catalytic interference was found for all nanomaterials under evaluation. In opposition, for the NRU assay, the nanokaolin and C-TiO₂ nanocomposite could react with the NRU assays components, possibly adsorbing to them, leading to a decrease in signal. Since there is no possible alteration of the protocol to eliminate the catalytic interference, the NRU assay could not be applied to evaluate cell viability of HepG2 cells when exposed to the nanomaterials under evaluation.

Concerning the LDH assay, no optical interference was found for the TiO₂ NPs when suspended in both oxidized and reduced INT (early and final components of the LDH assay) (see figure 15). However, kaolinite layered silicate and C-TiO₂ nanocomposite were capable of interfere with light absorbance measurements. Similarly to the previous studies for the viability assays, to overcome such interferences, a centrifugation step was added before absorbance measurements. Despite the signal lowered tremendously, the centrifugation was not enough to eliminate the nanokaolin and C-TiO₂ light interference with this cytotoxicity assay as a decrease in absorbance was still observed with the increase in nanomaterial concentrations.

None of the presented materials shown catalytic interferences with the LDH assays over an hour of continuous measurements.

As this is an enzymatic assay, it was also evaluated if the nanomaterials could inactivate or adsorb the LDH protein present in the supernatant, decreasing the final measured absorbance. To do so, nanomaterials were suspended in incomplete and complete media and different units of LDH protein from rabbit muscle were added to the suspensions and absorbance was measured over time. In the absence of serum proteins, all nanomaterials were capable of interfering with enzymatic activity of the LDH protein over time, decreasing its signal, irrespective of the units of LDH protein present on the media tested. Possibly, LDH proteins were adsorbed to materials surface and ceased to be able to reduce the INT compound, inducing false negatives, i.e., the assay would indicate that the integrity of the cellular membrane was not damaged when, in the reality, the LDH was

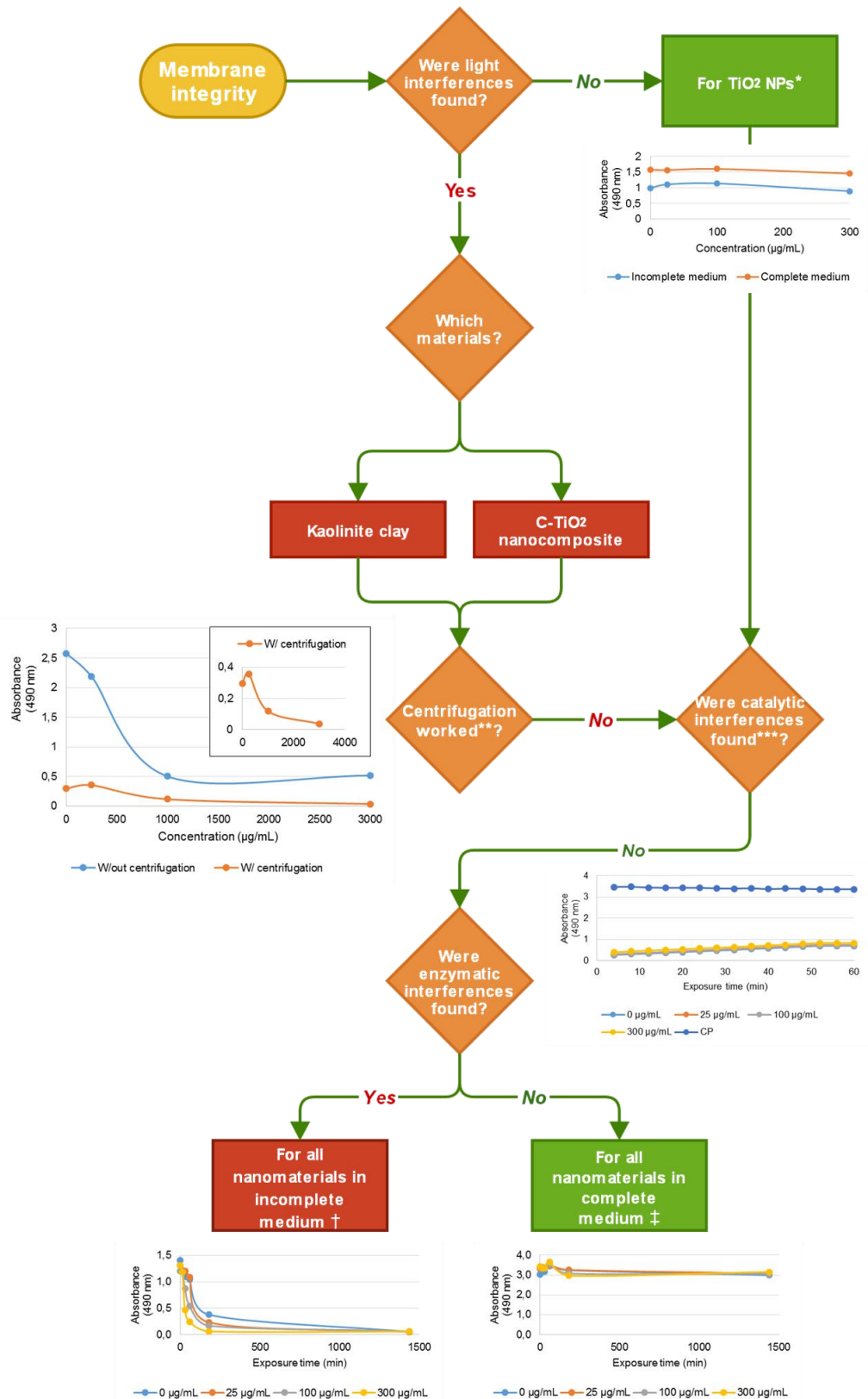


Figure 15. Schematic representation of the membrane integrity (LDH assay) interference studies. *,** As results were found to be similar in early and final products, only reduced INT results are presented; ***Only TiO₂ NPs results in complete media are shown since all nanomaterials exhibited similar catalytic interference; †,‡ Since the results were similar for all nanomaterials and mU of LDH protein, only some results were presented.

simply not available to convert lactate to pyruvate due to nanomaterials adsorption. In complete medium (with FBS proteins) this effect was not observed, possibly due to the presence of a protein corona formed by the FBS proteins around the materials that avoided LDH adsorption.

Results obtained in interference studies suggest that nanokaolin and C-TiO₂ nanocomposites were able to adsorb NRU and LDH assay components, decreasing the signal in both assays with the increase of particles concentrations. As these interferences could not be eliminated by protocol alterations, only MTT and AB assays were found to be suitable for further *in vitro* cytotoxicity study.

Current reports specify that MONPs interact with assay components or dyes or even with optical readouts due to the high adsorption or scattering of nanoparticles, distorting the assay outcome on the viability assessment (Kroll *et al.*, 2012). Different factors such as size, shape, crystallinity and concentration of the nanomaterial might influence the light detection of the colorimetric assays, owing to the nanomaterial interaction with the dyes, modifying their emission intensity. Generally, optical interference depends on the particle composition and also with its concentrations (the higher the concentration, the greater the interference) (Kroll *et al.*, 2012; Guadagnini *et al.*, 2013). These sort of interference has already been stated for TiO₂ NPs. A recent work reported that TiO₂ NPs could interfere with the NRU and MTT assays, increasing the signal reading for these dyes, which could be related to the light-absorbing properties of this nanoparticle (Guadagnini *et al.*, 2013).

Some authors demonstrated that LDH could be adsorbed and even inactivated for different metal nanoparticles, with special emphasis on TiO₂ NPs (Han *et al.*, 2011b; Guadagnini *et al.*, 2013). Nanoparticles may interact with proteins present on the biological solutions which may allow an increased reactivity with cytokines or enzymes from the cytotoxic assays, such as the LDH. With regard to metal based nanoparticles, they could induce a metal-catalysed oxidation of the LDH protein, non-specifically inactivating this molecule (Han *et al.*, 2011b). This occurrence may impair the correct evaluation of the membrane integrity assessment after nanomaterial exposure (Guadagnini *et al.*, 2013).

In respect of nanokaolin or even TiO₂ NPs immobilized in clay minerals, in accordance with the found literature, no interference studies regarding the toxicity assays have been made so far for these materials. Hence, the present work presents innovative results regarding the nanokaolin and nanocomposite interference on the proposed cytotoxicity assays (MTT, AB, NRU and LDH assays).

Is of paramount importance to assess possible nanomaterial interference with the toxicity assays methods prior to analysis of cellular responses in mammalian cell lines such

as the HepG2. The necessary protocol modifications must be introduced to eliminate or reduce the observed interferences in order to obtain a correct toxicological evaluation (Guadagnini *et al.*, 2013).

3.2. Cellular viability

After studying the nanomaterial capacity to interfere with the assays, a deeper analysis was carried out concerning the mitochondrial activity and potential redox of HepG2 hepatocytes after exposure to rutile TiO₂ NPs, nanokaolin clay and C-TiO₂ nanocomposite. The purpose of the present dissertation was to apprehend if the C-TiO₂ was a biocompatible nanomaterial for human and environmental applications. In addition, this study also evaluated toxicity of kaolinite mineral and TiO₂ NPs.

TiO₂ NPs induced a significant dose-dependent decrease in viability of the liver cells only after 24 hours of exposure to these nanoparticles ($p < 0.014$) in incomplete medium, measured by the MTT assay (Fig. 16.A).

In complete medium, a significant dose-dependent decrease in viability of HepG2 cells was observed in all studied periods of exposure to TiO₂ NPs ($p < 0.001$) (Fig. 16.B). This means that, the presence of FBS proteins in the medium was associated to more evident alterations in the mitochondrial activity and, consequently, lower viability of these hepatic cells.

Regarding the obtained results in AB assay (Figure 17), TiO₂ NPs induced a significant dose-dependent decrease in HepG2 viability only after 24 hours of treatment in incomplete medium ($r = -0.563$; $p < 0.001$), consistent with the results obtained on the MTT assay.

In complete medium, a decrease in viability was observed only for the first two periods of exposure ($p < 0.001$ and $p = 0.002$ for 3 and 6 h, respectively). These results suggest that the hepatic cells could possibly recover their redox potential functionality after a 24 hours period, in the presence of FBS proteins. However, as previously observed, the mitochondrial activity was still compromised.

Despite the inconsistent *in vitro* biological effects related to TiO₂ NPs, many studies have demonstrated the capacity of TiO₂ NPs to induce cytotoxicity in various cultured cell lines (Shi *et al.*, 2013; Prasad *et al.*, 2014).

Towards the toxicity evaluation on hepatocytes cells, Gaiser *et al.* (2013) found no cytotoxic on C3A hepatocytes after exposure to rutile with minor anatase TiO₂ NPs up to 625 µg/cm², using the Alamar Blue and LDH assays. Decrease in the cell viability was only

detected for high concentrations. These authors concluded that these TiO₂ NPs were non cytotoxic for C3A hepatocytes up to high doses (Gaiser *et al.*, 2013). These results were consistent with the ones obtained by Kermanizadeh *et al.* (2013) for the same cell line and using exclusively mitochondrial activity assays.

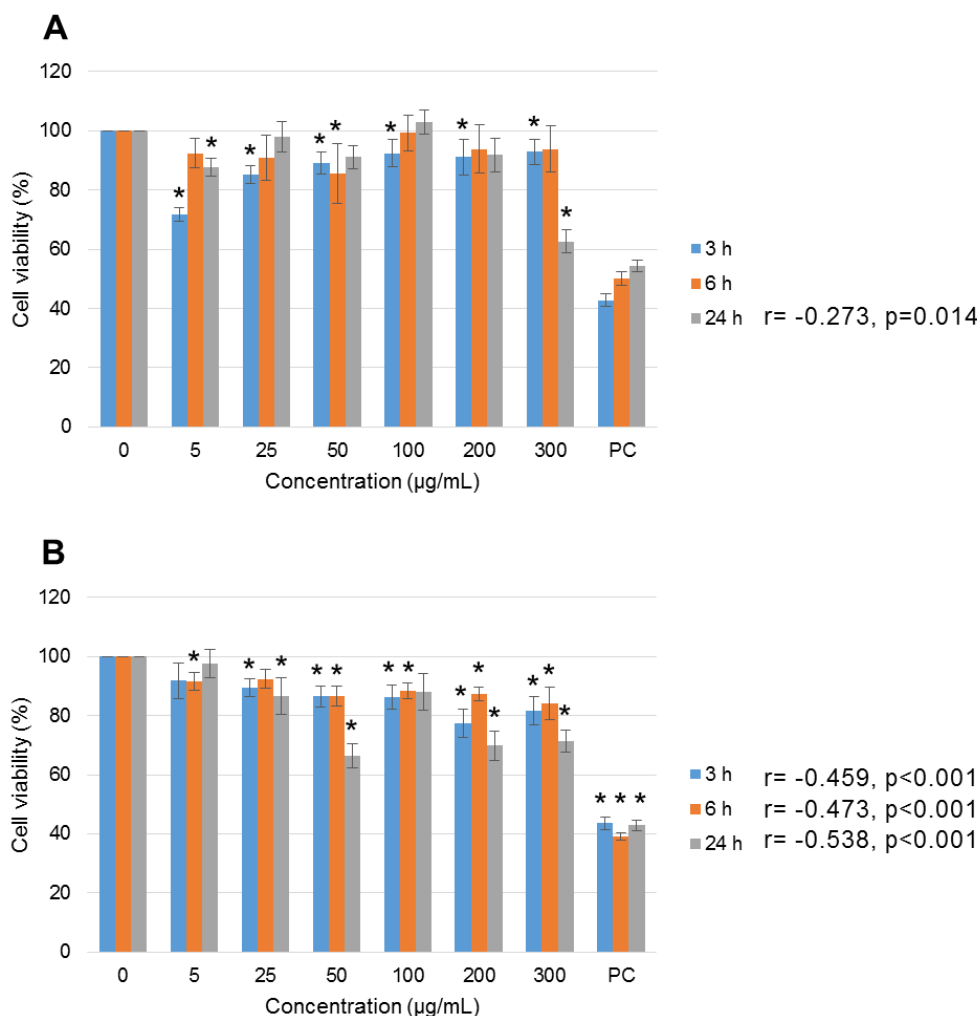


Figure 16. MTT assay performed in HepG2 cells after exposure to TiO₂ NPs suspended in (A) incomplete and (B) complete media. PC: Positive control (Triton X-100 1%). Bars present standard error of the mean. Values were normalized considering negative control as 100%. * $p < 0.05$, significant difference with regard to the corresponding negative control. For each period was performed a correlation analysis between TiO₂ NPs concentrations and cellular viability were r value represent the correlation coefficient and p value the statistical significance of the correlation.

With respect to studies performed on HepG2 cell line, some demonstrated that TiO₂ NPs (mainly constituted with anatase) did not induce significant decrease in cell viability in medium supplemented with FBS in any concentration tested (until 100 µg/mL) after 24 hours of exposure (Prasad *et al.*, 2014). Others demonstrated negligible loss in the HepG2 viability after 6 hours of exposure while, for longer time periods (24 and 48 h) only concentrations of 20 to 80 µg/mL induce significant cytotoxicity through MTT and NRU

assays assessment (Shukla *et al.*, 2013). However, previous reports showed opposite results relating no reduced viability of HepG2 cells for either anatase or rutile TiO₂ NPs (Petkovic *et al.*, 2011).

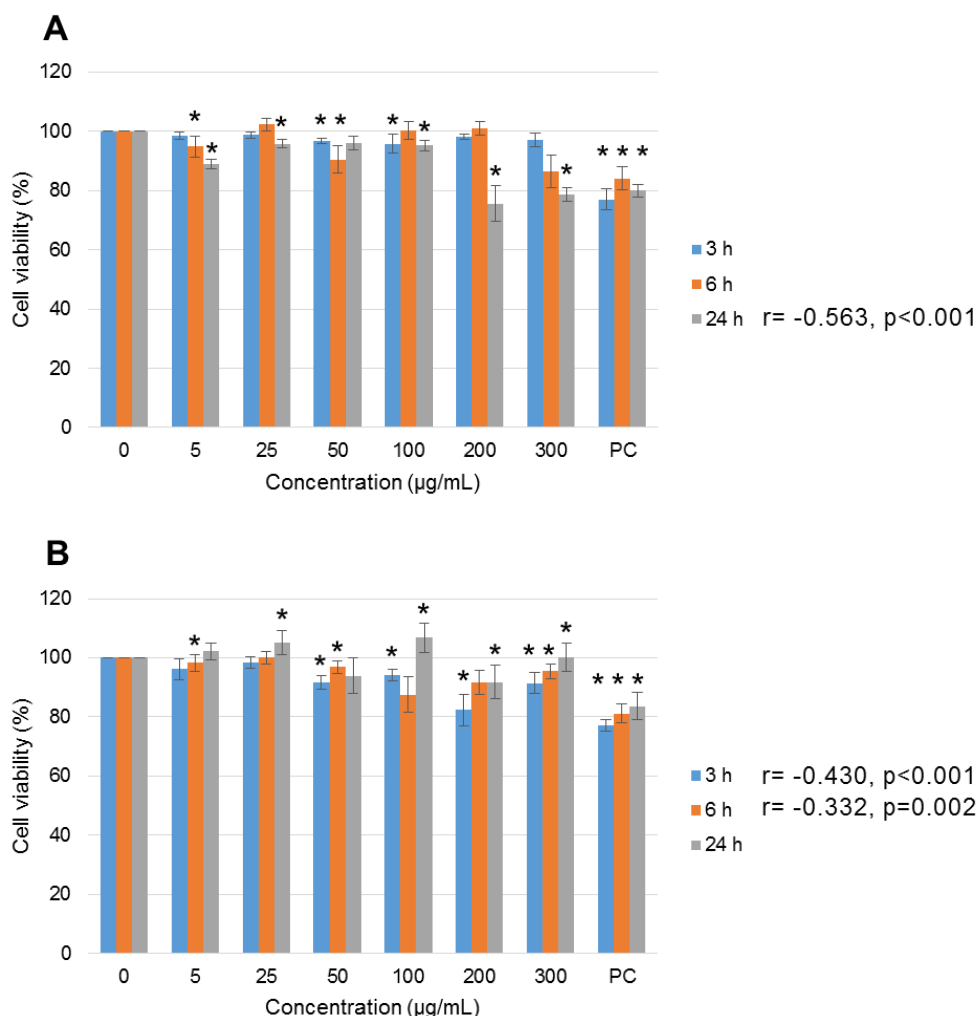


Figure 17. AB assay performed in HepG2 cells after exposure to TiO₂ NPs suspended in (A) incomplete and (B) complete media. PC: Positive control (Triton X-100 1%). Bars present standard error of the mean. Values were normalized considering negative control as 100%. * p < 0.05, significant difference with regard to the corresponding negative control. For each period was performed a correlation analysis between TiO₂ NPs concentrations and cellular viability were r value represent the correlation coefficient and p value the statistical significance of the correlation.

As far as it is known, there are not many papers reporting cytotoxic studies with rutile TiO₂ NPs on hepatic cell lines. According to the previous papers, TiO₂ NPs with a mixture of both rutile and anatase presented some similar results to the ones observed on this work, i.e., for longer periods of exposure and for high doses these nanoparticles could induce *in vitro* damage on hepatic cells. However, the rutile TiO₂ NPs used here also exhibited adverse effects on the mitochondrial activity for short periods of exposure and in several

cases low concentrations of these nanoparticles could induce damage for both mitochondrial and potential redox activities.

Differences between human cell lines plays an important part in TiO₂ NPs toxicity assessment (Prasad *et al.*, 2014). While studies performed on A549 lung cell line shown lack of cytotoxic effects regarding the cell viability and membrane damage, other studies on BEAS-2B bronchial epithelial cell line found high cytotoxicity also in cell viability reduction and membrane integrity after exposure to TiO₂ NPs (mainly constituted by anatase) (Ursini *et al.*, 2014). These results were coherent with the ones obtained by Ekstrand-Hammarstrom *et al.* (2012) that obtained lower toxicity on five different types of TiO₂ NPs (either anatase or rutile), and also with Moschini *et al.* (2013) for MTT and NRU analysis, despite the efficient internalization in A549 in both studies.

In neuronal cell lines, such as SHSY5Y, no effect on viability was also measured by MTT and NRU assays after exposure to two types of TiO₂ NPs (Valdiglesias *et al.*, 2013).

The differences between studies can be related to the variation on the production and preparation of the TiO₂ NPs, as well as the comparison of nanoparticle's toxicity with different particle size, degree of aggregation, incubation and/or exposure conditions (i.e. dosage and periods of treatment) (Iavicoli *et al.*, 2011). The conjugation of the mentioned factors may lead to contradictory results. Therefore, the knowledge concerning the toxicity of TiO₂ NPs is still far from being completely understood.

Taking into consideration the results obtained in the present work, and despite some reports that did not observe cytotoxic effects derived from TiO₂ NPs exposure, results here obtained suggest that these nanoparticles should not be considered as negative controls in nanotoxicological studies, as some authors have suggested (Liu *et al.*, 2013).

In relation to the clay mineral under evaluation, nanokaolin induced a significant dose-dependent decrease in viability of HepG2 cells (assessed by MTT assay), in all studied periods of exposure in incomplete medium ($p < 0.001$), in contrast to the observed for TiO₂ NPs exposure (Fig. 18.A). These results advocate that kaolinite clay is able to alter mitochondrial activity rapidly (just after 3 h of exposure) and continuously.

A similar tendency was observed in complete medium, with the exception of the 6 hours of kaolinite exposure (Fig. 18.B).

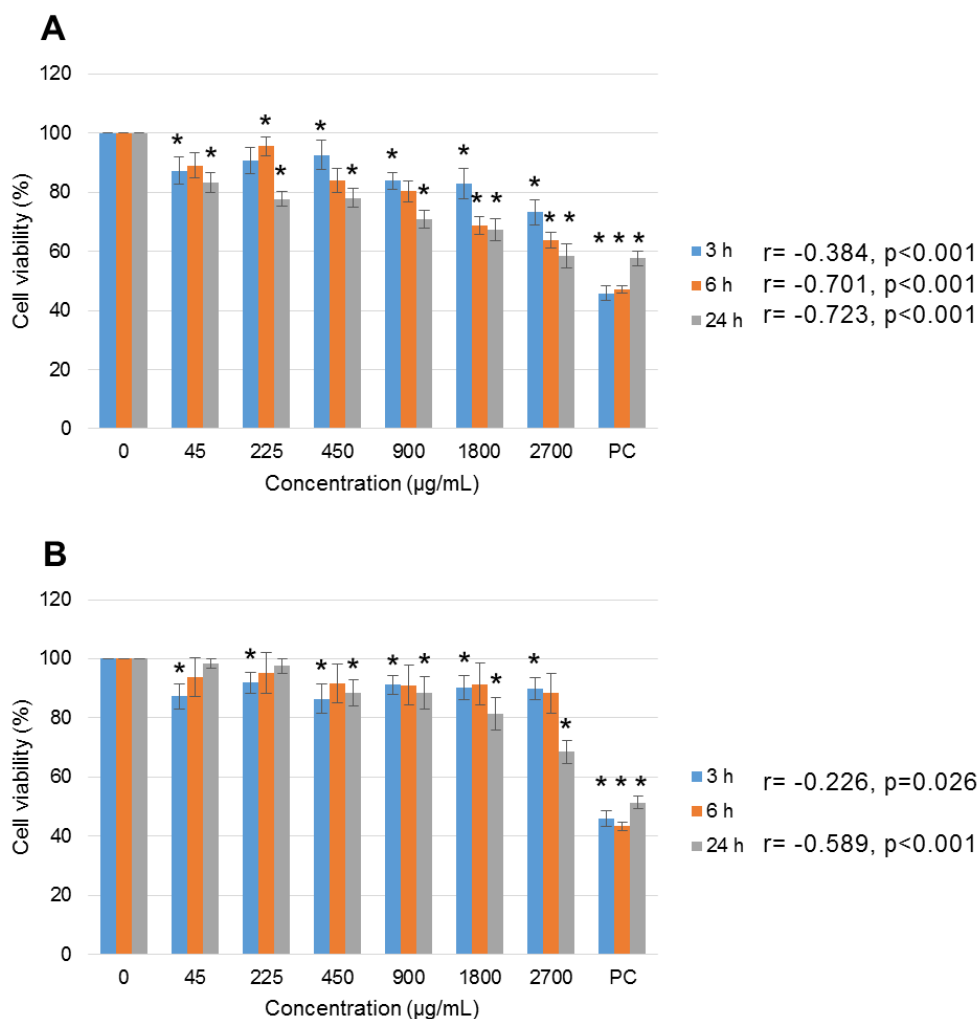


Figure 18. MTT assay performed in HepG2 cells after exposure to nanokaolin suspended in (A) incomplete and (B) complete media. PC: Positive control (Triton X-100 1%). Bars present standard error of the mean. Values were normalized considering negative control as 100%. * $p < 0.05$, significant difference with regard to the corresponding negative control. For each period was performed a correlation analysis between nanokaolin concentrations and cellular viability were r value represent the correlation coefficient and p value the statistical significance of the correlation.

In respect to the AB assay, kaolinite induced a dose-dependent decrease in the cell viability (measured by the redox potential of the HepG2 cells) in both incomplete (Fig. 19.A) and complete medium (Fig. 19.B), which, along with the results obtain for the MTT assay, corroborates that these particles are cytotoxic to HepG2 cells.

Despite the multiple functionalities of the clay minerals, the use of nanoclays raises some concerns since there is still few information about the toxicity that these nanomaterials can induce (Jones and Grainger, 2009).

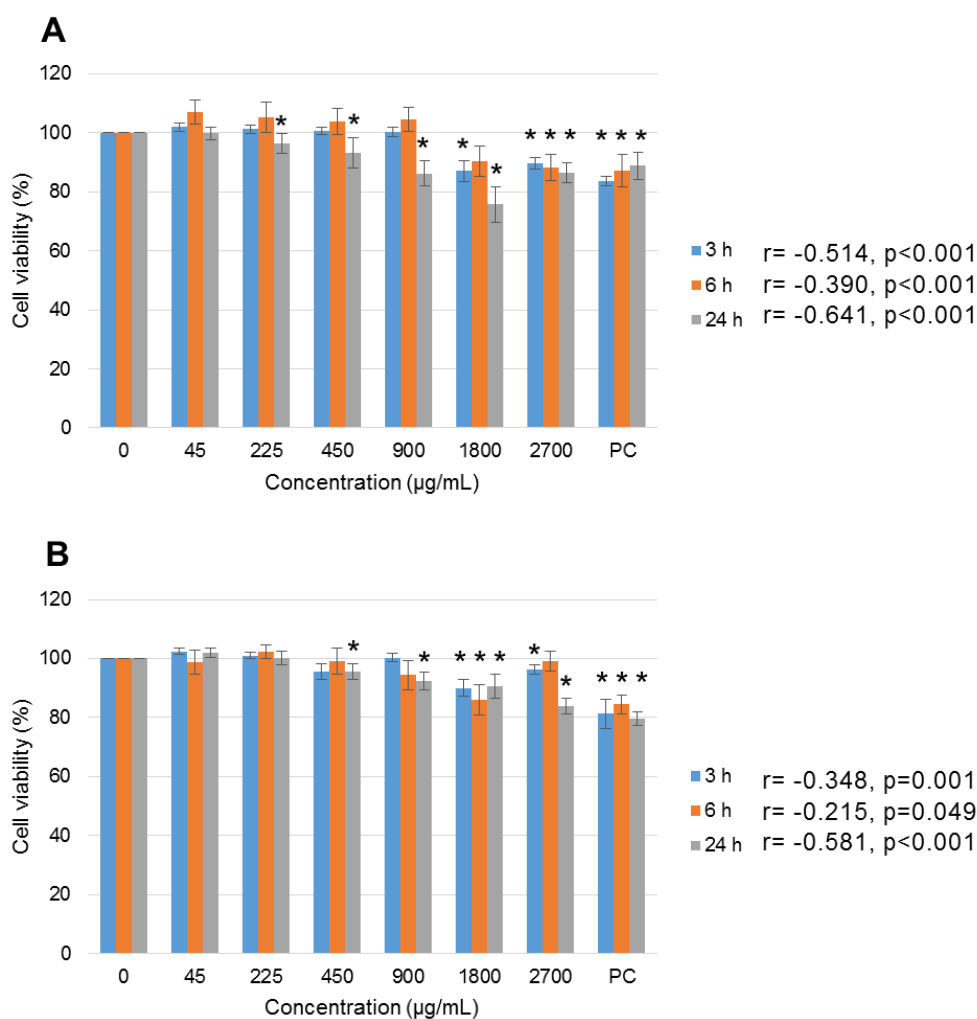


Figure 19. AB assay performed in HepG2 cells after exposure to nanokaolin suspended in (A) incomplete and (B) complete media. PC: Positive control (Triton X-100 1%). Bars present standard error of the mean. Values were normalized considering negative control as 100%. * $p < 0.05$, significant difference with regard to the corresponding negative control. For each period was performed a correlation analysis between nanokaolin concentrations and cellular viability were r value represent the correlation coefficient and p value the statistical significance of the correlation.

Several studies already demonstrated that some types of clays are able to cause cytotoxicity in different cell lines, and even induce cell death. Most of the studies show that clay induces cytotoxicity only at high concentrations. For example, Han *et al.* (2011a) verified moderate cytotoxicity of clay minerals modified with an amine functional group in different cell types only at 1000 µg/mL (Han *et al.*, 2011a). However, other authors have described significant loss of A549 lung epithelial viability after 24 hours of exposure to different nanoclays at lower concentrations (25 µg/mL) (Verma *et al.*, 2012). Another study observed the same effect but in even inferior concentrations of nanoclay (1 µg/mL), in HepG2 liver cell line, as well as the significant generation of ROS (Lordan *et al.*, 2011). These authors also mentioned that the ultra-small sized clays particles tended to aggregate in the cell culture medium, which appeared to be correlated with the observed toxicity

mechanisms. In spite of this data, there are still few toxicological studies in the literature about clays in HepG2 cell line (Abdel-Wahhab *et al.*, 2015).

Recent reports illustrated no significant cytotoxic effect in intestinal Caco-2 cell line after being exposed to selected concentrations of a specific type of modified montmorillonite clay after 24 and 48 hours of exposure. However, the same group shown the opposite results on the same type of clay but with different organic modification, for relatively low concentrations (Maisanaba *et al.*, 2014). The same author studied the same clay particles in the HepG2 liver cell line and observed similar effects (Maisanaba *et al.*, 2013).

After evaluating the cytotoxicity of their single components, the impact of C-TiO₂ nanocomposite on the cellular viability of hepatocytes was also analyzed using the MTT and AB assays.

Results of MTT assay (Figure 20) show that C-TiO₂ induced mitochondrial imbalance for increased concentrations of these material, regardless of the presence of serum proteins in the biological media.

In the case of AB assay (Figure 21), it was demonstrated that C-TiO₂ nanocomposite lowered the cell viability of the hepatic cell line under study also in a dose-dependent way, with the exception for the shorter treatment period in complete medium. Possibly the FBS proteins have some positive influence on the redox potential of the liver cells in the first hours of exposure.

As aforementioned, the C-TiO₂ nanocomposite was mainly constituted by nanokaolin. Probably for this reason, similarly to what was observed for the kaolinite clay mineral, the C-TiO₂ induced a dose-dependent decrease in the cell viability (in both assays) of the HepG2 cell line in both serum supplemented and serum free medium.

One important aspect to take into account is the possible interactions between clay and cell culture media components, including serum (Dawson and Oreffo, 2013). Although the uptake results showed that FBS proteins apparently improved kaolinite internalization, these proteins did not protect cells from both mitochondrial or redox potential dysfunction since both nanokaolin and C-TiO₂ nanomaterials could cause cytotoxicity damage on liver cells in both biological media tested.

Altogether, results suggest that kaolinite laminar structure has the biggest contribution to the cytotoxicity of C-TiO₂ nanocomposites.

Thereby, these results suggest that kaolinite is not a suitable clay substrate for the immobilization of other nanomaterials (for instance the TiO₂ NPs), since increased

concentrations of kaolinite induce a significant decrease in the cell viability in the HepG2 cell line, which was also observed on the C-TiO₂ nanocomposites.

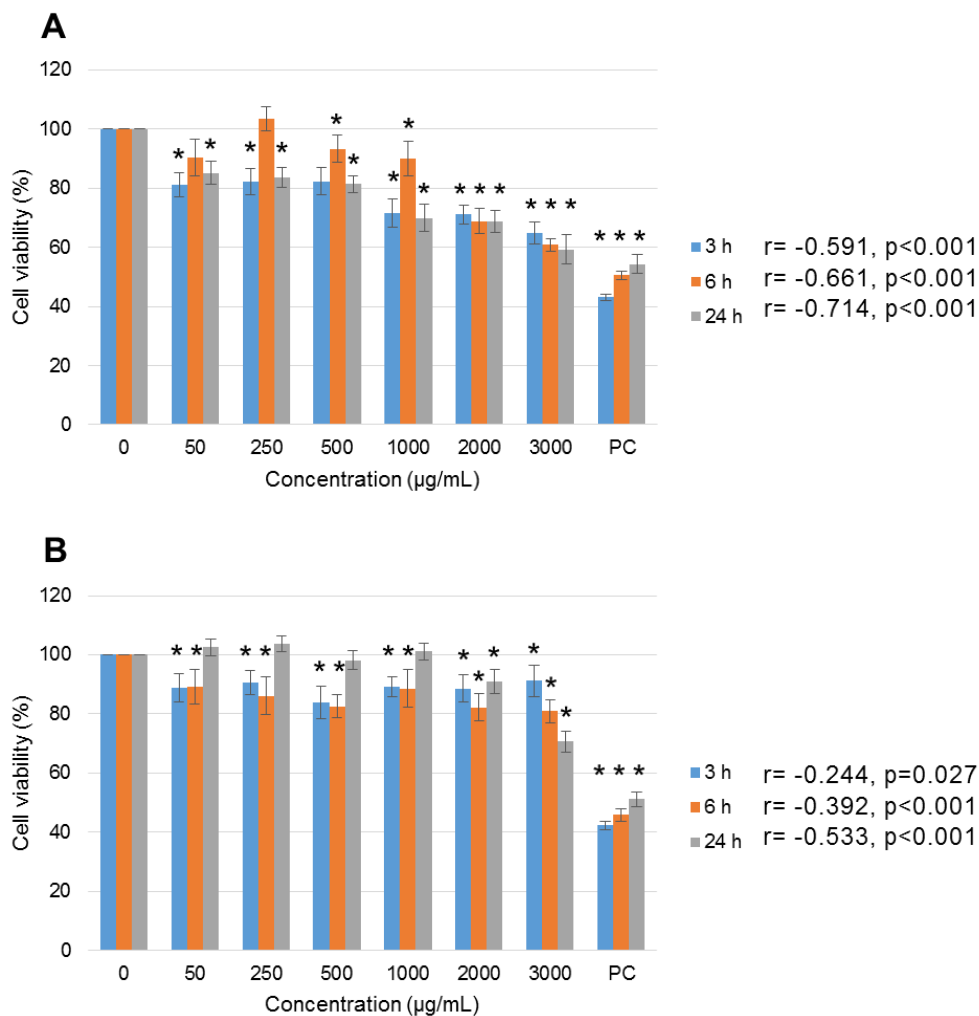


Figure 20. MTT assay performed in HepG2 cells after exposure to C-TiO₂ nanocomposites suspended in (A) incomplete and (B) complete media. PC: Positive control (Triton X-100 1%). Bars present standard error of the mean. Values were normalized considering negative control as 100%. * $p < 0.05$, significant difference with regard to the corresponding negative control. For each period was performed a correlation analysis between C-TiO₂ concentrations and cellular viability were r value represent the correlation coefficient and p value the statistical significance of the correlation.

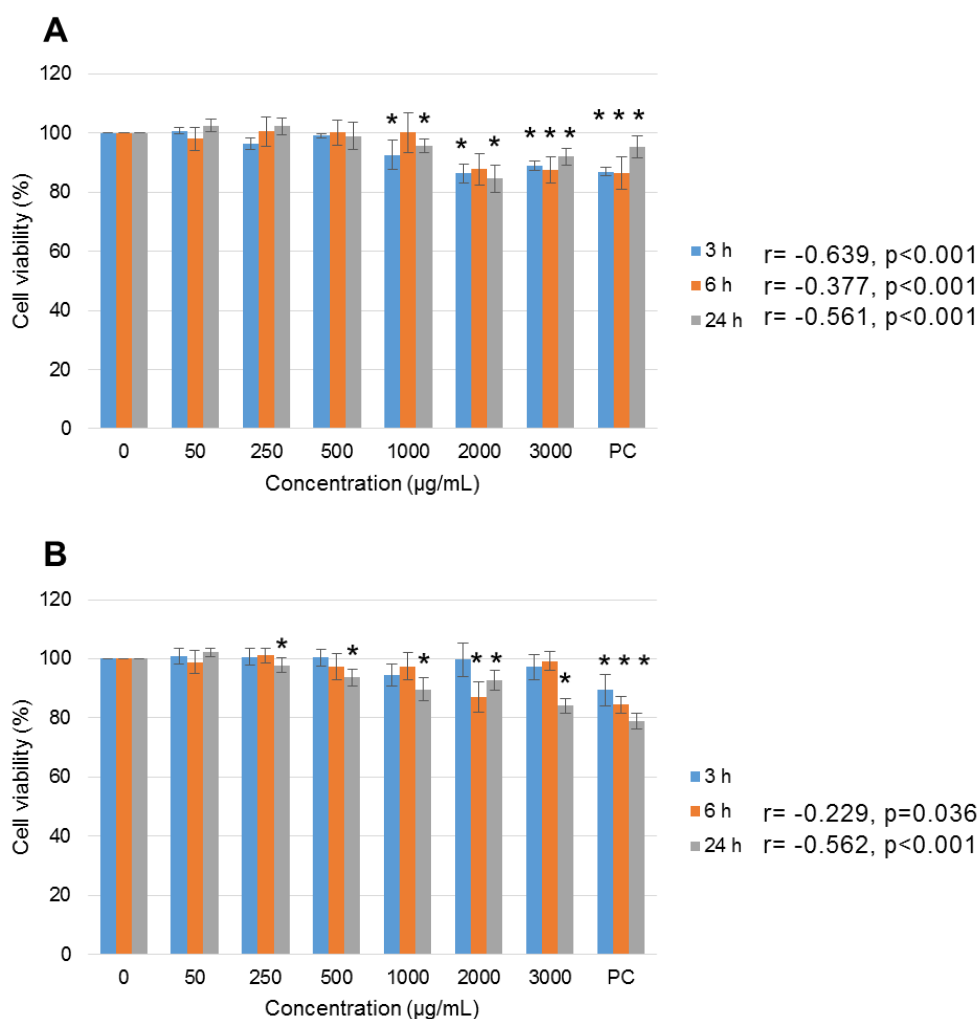


Figure 21. AB assay performed in HepG2 cells after exposure to C-TiO₂ nanocomposites suspended in (A) incomplete and (B) complete media. PC: Positive control (Triton X-100 1%). Bars present standard error of the mean. Values were normalized considering negative control as 100%. * $p < 0.05$, significant difference with regard to the corresponding negative control. For each period was performed a correlation analysis between C-TiO₂ concentrations and cellular viability were r value represent the correlation coefficient and p value the statistical significance of the correlation.

4. *In vitro* genotoxicity of the nanomaterials in the HepG2 cell line

To understand the genotoxic potential of rutile TiO₂ NPs, nanokaolin clay and the conjugation of both nanomaterials (C-TiO₂ nanocomposite), the alkaline comet assay was selected.

Similarly to cytotoxicity assays, interference studies were performed before assessing the DNA damage derived from *in vitro* nanomaterial exposure. The following section will describe in detail the observed interferences and also the adopted strategies to avert them.

4.1. Interference studies

There are different mechanisms associated to the capacity of the nanomaterials to interfere with genotoxic comet assay, by: (1) associating to the DNA nucleoid, affecting its performance during electrophoresis and (2) inducing breaks in the naked DNA. Thereby, in order to estimate the nanomaterials capacity to damage DNA in cells it is important to evaluate the interaction of these with the alkaline comet assay. The presence of nanomaterials during the comet assay can interfere with the sensibility of the assay, misleading the results (Magdolenova *et al.*, 2012).

During the lysis step of the alkaline comet assay, cells are embedded in a solution with high concentration of NaCl and 1% of Triton X-100, responsible for membrane disruption, removing the cytoplasm and nuclear proteins and, therefore, exposing non-nucleosomal DNA. In this stage, the nanomaterials may interact with the unprotected DNA and cause additional DNA damage (Karlsson, 2010).

As represented in figure 22, when comparing the negative control (cells non-exposed to nanomaterials) in incomplete medium with the lysis test, all nanomaterials seem to cause additional damage on the DNA, interfering with the assay.

In opposition, in the presence of FBS there were no major differences between the lysis test of all materials and the negative control, showing that all tested nanomaterial did not to interfere with the alkaline comet assay in complete medium. To reduce the risk of interferences observed in serum free medium, extensive washing of the wells was performed after the nanomaterials exposure, in order to remove nanomaterials.

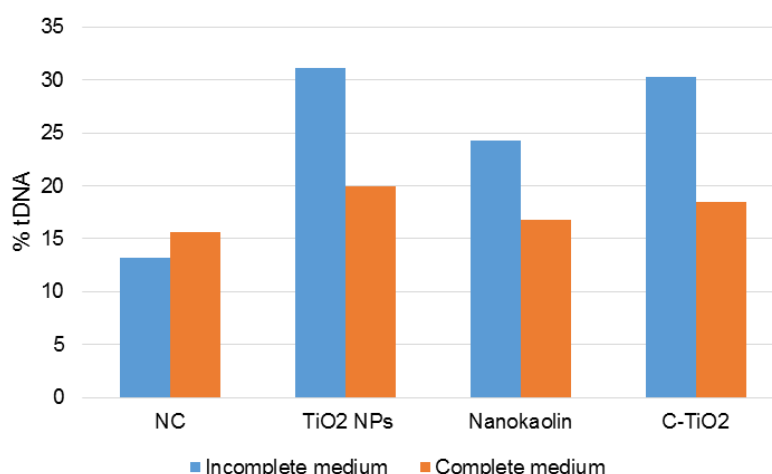


Figure 22. Possible interactions of TiO₂ NPs, nanokaolin clay and C-TiO₂ nanocomposites with alkaline comet assay in incomplete and complete media. In the lysis test, nanomaterials were added just before the assay. NC: cells non-exposed to nanomaterials; tDNA: tail intensity.

4.2. DNA integrity

The alkaline comet assay is one of the most common test systems to assess genotoxicity (Love *et al.*, 2012; Chang *et al.*, 2013). This version of comet assay allows the detection of two types of DNA damage: SSBs (single strand breaks) and ALSs (alkali-labile sites). As the name implies, SSBs denote single breaks on the DNA strands, while ALSs represent a loss of pyrimidine and purines bases from the sugar in the DNA backbone (Karlsson, 2010; Kain *et al.*, 2012).

Comet assay results showed that after exposure to TiO₂ NPs, cells presented higher levels of tail DNA in complete medium rather than in the absence of serum proteins. Regardless, increase in DNA damage with increasing dosage of TiO₂ NPs was observed for both media and periods of exposure (Figs. 23.A and 23.B).

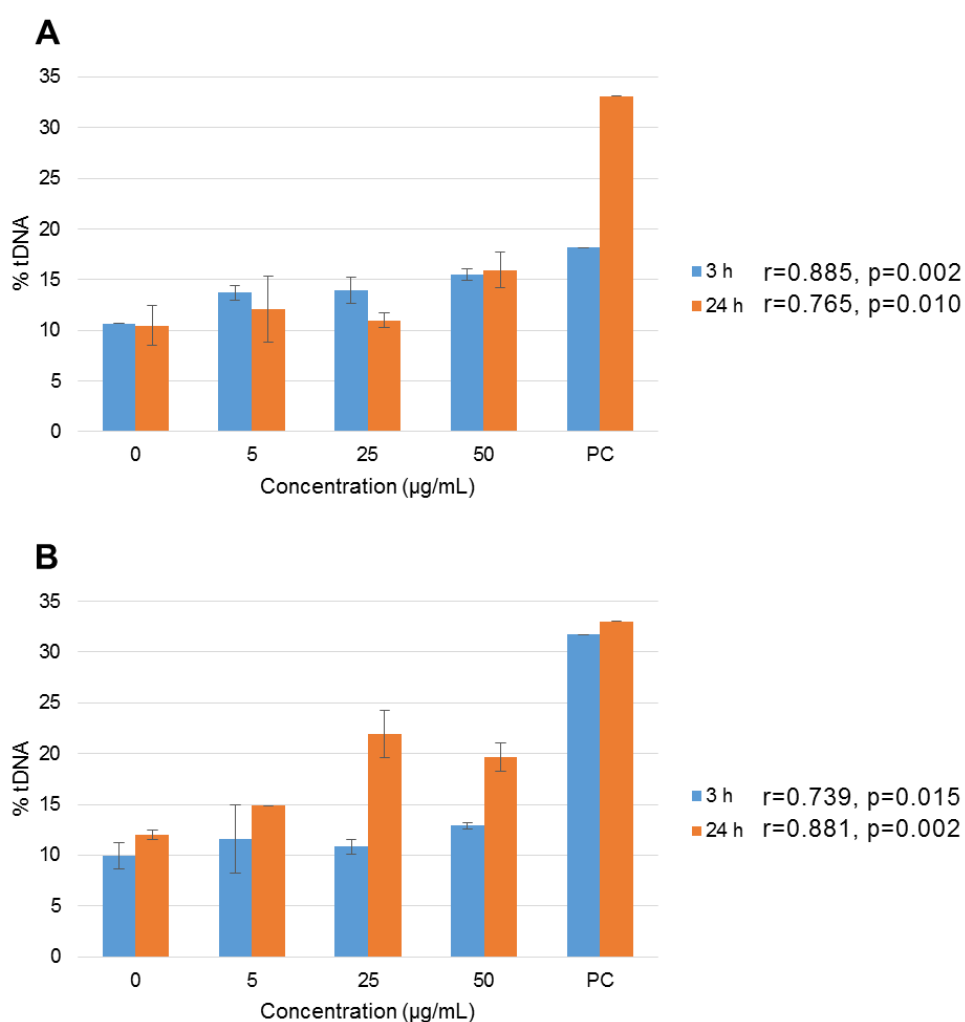


Figure 23. Effect of TiO₂ NPs on DNA damage of HepG2 cells analyzed by alkaline comet assay in (A) incomplete and (B) complete media. PC: Positive control (MMS 100 µM). Bars present standard error of the mean. tDNA: tail intensity.

Once again, the physicochemical characterization of the TiO₂ NPs plays a crucial role on their toxicity but, in this case, on the DNA damage derived from the exposure to these nanoparticles. Petkovic *et al.* (2011) shown in his work that the genotoxic potential of TiO₂ NPs depends on its particle size and crystalline structure. In fact, anatase TiO₂ NPs induced stronger DNA damage than the rutile ones in HepG2 cell line. These results were confirmed later with the same hepatocyte cell line (Petković *et al.*, 2011). Also using the HepG2 cell line, Prasad *et al.* (2014) observed that increased concentration of TiO₂ NPs mostly constituted by anatase suspended in medium supplemented with 10% of FBS induced increase DNA damage (Prasad *et al.*, 2014).

Other studies on mammalian cell lines (for instance human gastric epithelial AGS cell line, A549 lung cell line, lymphocytes) also observed genotoxic effects for different sized anatase and rutile TiO₂ NPs by using comet assay (Botelho *et al.*, 2014; Kang *et al.*, 2008; Jugan *et al.*, 2012).

According to the review authored by Karlsson (2010), TiO₂ NPs are the most well studied metal-based nanoparticle up to date and most studies on their genotoxicity using the alkaline comet assay reported an increase in damage compared with non-exposed controls, in different cell lines, including A549, lymphocytes, BEAS-2B, Caco-2, among others.

Another study looking at the genotoxicity of the TiO₂ NPs studied here (NM-104) showed that these did not cause significant DNA damage on intestinal Caco-2 cell line. In fact, the same study evaluated other TiO₂ NPs with distinct crystal phases and noticed that anatase and anatase/rutile (NM-102 and NM-105, respectively) were the most hazardous nanoparticles in comparison to NM-104, in accordance with the *in vitro* comet assay results. The only cell line in which was observed DNA damage derived from NM-104 exposure was the dermal cell line NHEK (Norppa *et al.*, 2013).

Concerning nanokaolin and C-TiO₂ nanomaterials, both induced similar effects on the DNA integrity on the hepatic cells. Similarly to TiO₂ NPs, nanokaolin clay and C-TiO₂ nanocomposite induced more damage in complete medium (Figs. 24.B and 25.B). In this case, these nanomaterials could induce more SSBs and ALSs breaks on the HepG2 DNA even after 3 hours of exposure, in contrary to what was observed in incomplete medium, where increase of DNA damage was only detected after 24 hours of exposure (Figs. 24.A and 25.A). For both materials, a high correlation coefficient and significant p value was obtained for 24 hours of exposure in incomplete medium ($r=0.867$; $p=0.001$).

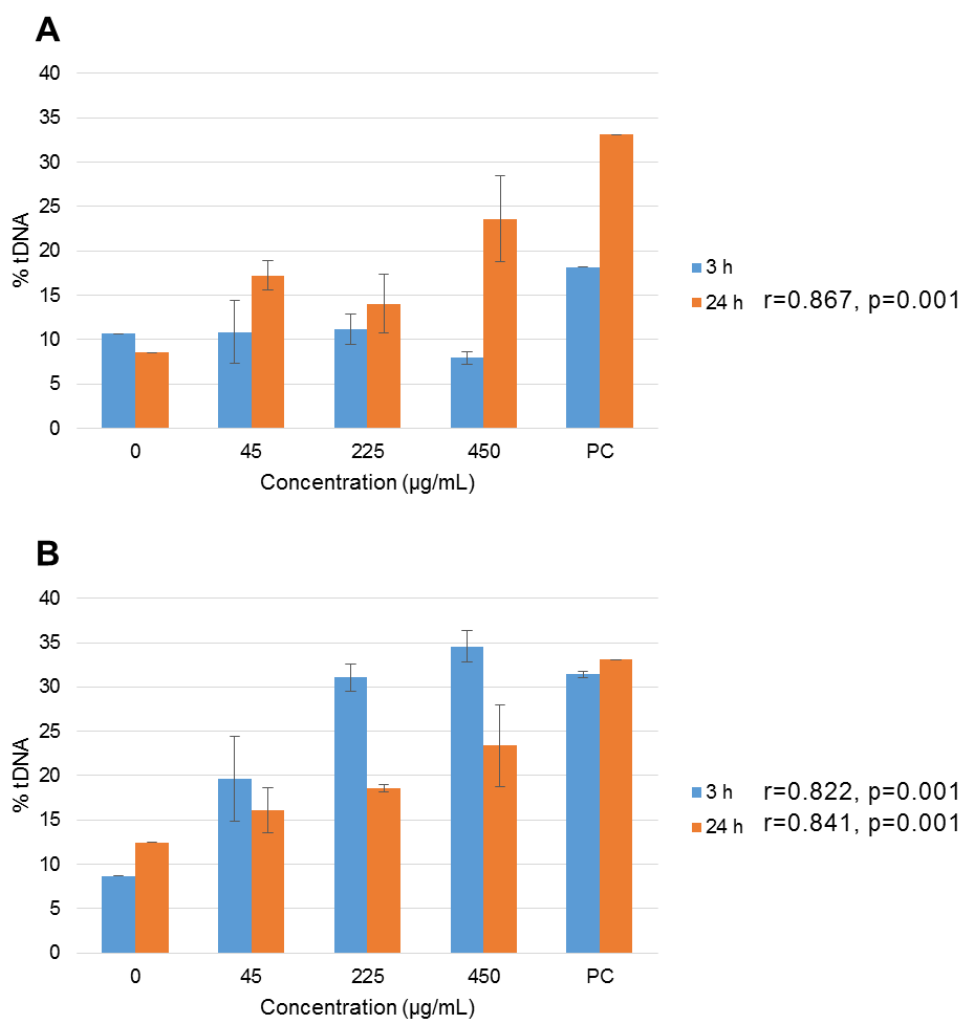


Figure 24. Effect of nanokaolin on DNA damage of HepG2 cells analyzed by alkaline comet assay in (A) incomplete and (B) complete media. PC: Positive control (MMS 100 µM). Bars present standard error of the mean. tDNA: tail intensity.

Previous studies have already demonstrated that clays commonly found in soils (e.g. smectites) can react with pesticides and modify their genotoxicity in mammalian cells; pesticides alone did not cause genotoxicity, while, when coupled to redox-modified clays, triggered environmental genotoxicity (Sorensen *et al.*, 2005). On the contrary, more recent studies performed by Li *et al.* (2010) showed no genotoxicity of exfoliated montmorillonite (a 2:1 clay mineral type). Another study also demonstrated that a chemically modified montmorillonite clay mineral (cloisite) could not induce *in vitro* damage on the DNA of Caco-2 cell line exposed for more than 24 hours (Sharma *et al.*, 2010); however, other author demonstrated the opposite effect on the same cell line (Sharma *et al.*, 2010). Two recent studies proved to occur DNA strand break on hepatic HepG2 cells in a time dependent manner, also measured by the comet assay, after exposure to organomodified cloisite clays (Maisanaba *et al.*, 2013; Houtman *et al.*, 2014).

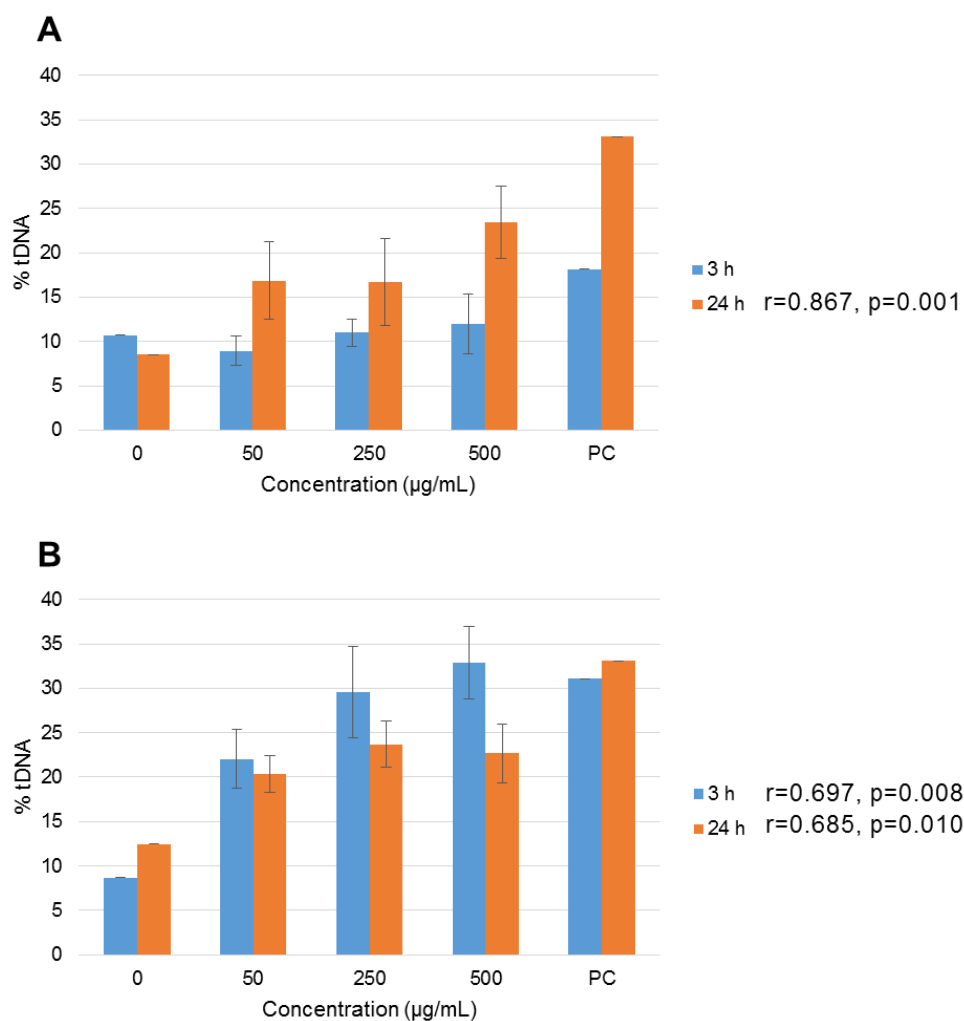


Figure 25. Effect of C-TiO₂ nanocomposites on DNA damage of HepG2 cells analyzed by alkaline comet assay in (A) incomplete and (B) complete media. PC: Positive control (MMS 100 µM). Bars present standard error of the mean. tDNA: tail intensity.

Results obtained herein indicate, once again, that kaolinite is not a suitable clay substrate for the immobilization of other nanomaterials, since, in opposition to what has been previously reported, high concentrations of clay induced a significant increase in DNA damage of HepG2 cell line.

V. CONCLUSIONS AND FUTURE PERSPECTIVES

One of the main concerns of nanotechnology applications is that nanoparticles might be more toxic, and therefore more hazardous than larger particles and bulk materials, due to their large surface area and consequent enhanced chemical reactivity and also cellular internalization (Tucci *et al.*, 2013).

In the last years, TiO₂ NPs have been extensively studied to investigate their potential toxicological effects due to their increased environmental and occupational exposure (Tucci *et al.*, 2013). In order to monitor and control the release of TiO₂ NPs, it has been developed the technique of immobilization of these nanoparticles into crystalline substrates, such as inorganic clay minerals, facilitating their manipulation, restraining their release and diminishing their threat into the environment and human health (Tokarsky *et al.*, 2012; Tokarčíková *et al.*, 2014). Clay minerals have been distinguished as the materials of the 21st century due to their relatively low cost, availability and environmental sustainability (Maisanaba *et al.*, 2015). Among the existing clay minerals, kaolinite, commonly found in soils, has been reported has an excellent substrate for immobilizing MONPs (Tokarsky *et al.*, 2012). The formation of the TiO₂ NPs supported in kaolinite mineral created nanocomposites that combines the properties of both components (Tokarsky *et al.*, 2012; Tokarčíková *et al.*, 2014).

The liver is an organ of nanoparticle accumulation and clearance and, for that reason, is susceptible to nanomaterials toxicity (Petkovic *et al.*, 2011; Prasad *et al.*, 2014). In addition, the hepatocytes include an abundance of cellular organelles associated with metabolic and secretory functions, such as high number of mitochondria that helps providing high energy levels to support the numerous metabolic function of the liver (Rolfe, 2013).

In the current work it was applied an *in vitro* model system to surrogate human hepatocytes, the HepG2 cell line. *In vitro* studies constitute an initial stage of the toxicological evaluation (Joris *et al.*, 2013) and for each type of nanomaterials is crucial to perform cytotoxicity studies because of their distinctive biological response (Lewinski *et al.*, 2008). Conflicting results found in the literature highlight the need for a greater consistency on all experimental procedures such as detailed physicochemical characterization of the materials, dispersion protocol, dosage of the materials, periods of exposure, cell culture medium constitution, interference assays and cytotoxicity assays protocols.

In this regard, the present study measured the cellular interaction and biological responses of human hepatocytes after exposure to TiO₂ NPs immobilized in nanokaolin laminar structures. To achieve this main goal, a set of experiments were performed in order to evaluate the cellular uptake, viability and DNA damage on hepatic cells. In addition, all

proposed assays were tested in regards of the possible interference of this nanocomposite and/or its individual components with optical, catalytic and even enzymatic performance.

To overcome possible interferences of the C-TiO₂ nanocomposite and its single elements on the cytotoxicity assessment, a set of experiments were performed and, when possible, alterations on the classic assays protocols were done. Only the NRU assay was not suitable for viability assessment since both nanokaolin clay and C-TiO₂ nanocomposite exhibited light and catalytic interferences; for membrane integrity assessment, LDH was also not adequate since all materials suspended in incomplete medium enzymatically interfered with the assay. Thereby, MTT and AB were the only cytotoxic assays compatible with the all TiO₂ NPs, nanokaolin and C-TiO₂ nanocomposite.

While there is an outlook that the incorporation of single nanoparticles on nanocomposites may decrease their biological damage (COST, 2012), the present *in vitro* study suggests that kaolinite is not a suitable substrate for the immobilization of nanoparticles, as well as that TiO₂ NPs may not be harmless for human applications as some previous studies reported. Both cytotoxic and genotoxic effects were observed on the HepG2 hepatic cell line after exposure to C-TiO₂ nanocomposites and its single elements. The figure 26 summarizes the main toxicological mechanisms identified in the present *in vitro* assessment. All nanomaterials could induce mitochondrial and potential redox dysfunction of the hepatocytes, after internalization in these hepatic cells. Lastly, the HepG2 DNA was also affected after longer periods of exposure to TiO₂ NPs, nanokaolin clay and C-TiO₂ nanocomposite even in the presence of serum proteins in the biological media.

A possible strategy to overcome the cytotoxic and genotoxic effects of naked kaolinite observed in this study is to chemically modify the kaolinite particles with organic compounds (Maisanaba *et al.*, 2014). Even so, further toxicity studies must be performed in organoclay particles to understand if the chemical modification allows the creation of a more compatible kaolinite mineral and, therefore, a more convenient material for the incorporation of nanoparticles for future and safer nanocomposite applications.

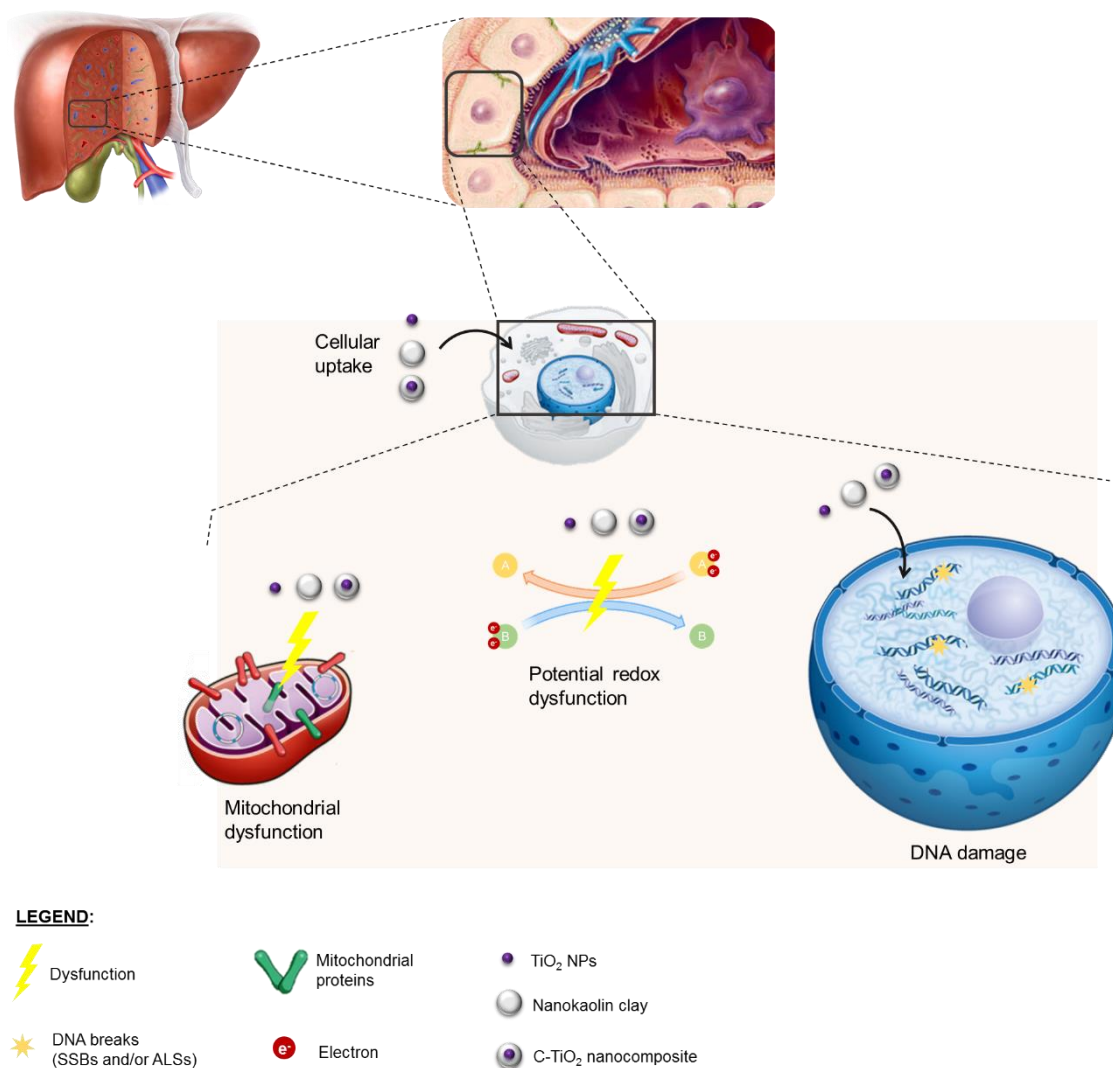


Figure 26. General mechanisms of toxicity on the hepatocyte cell line under study (HepG2) caused by TiO_2 NPs, nanokaolin clay and C- TiO_2 nanocomposite in the presence or absence of serum proteins in the biological medium.

After selecting the appropriate clay mineral for the immobilization of TiO_2 NPs or other nanoparticles, the following step is to perform *in vivo* studies. The first stage for *in vivo* studies is to choose an appropriate animal model with similar metabolic and physiological system background to humans in order to evaluate the biological effects of nanoparticles in real situations.

The current innovative study represents a primordial toxicity evaluation of the nanocomposites using mineral clays structures on human exposure, moving towards to a safer application of these new materials.

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VII. APPENDICES

Appendix A

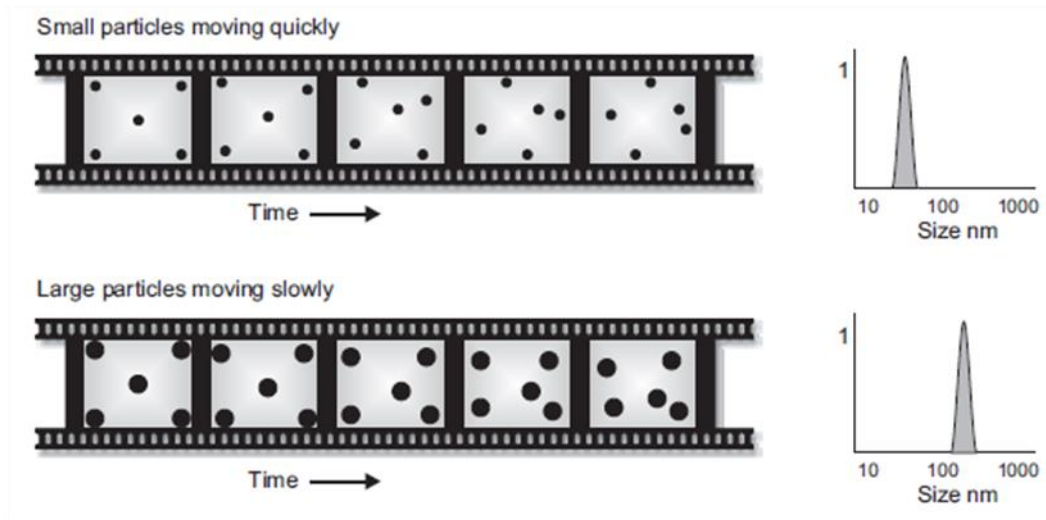


Figure A 1. Principle of hydrodynamic particle size measured by DLS (from Malvern (2004)).

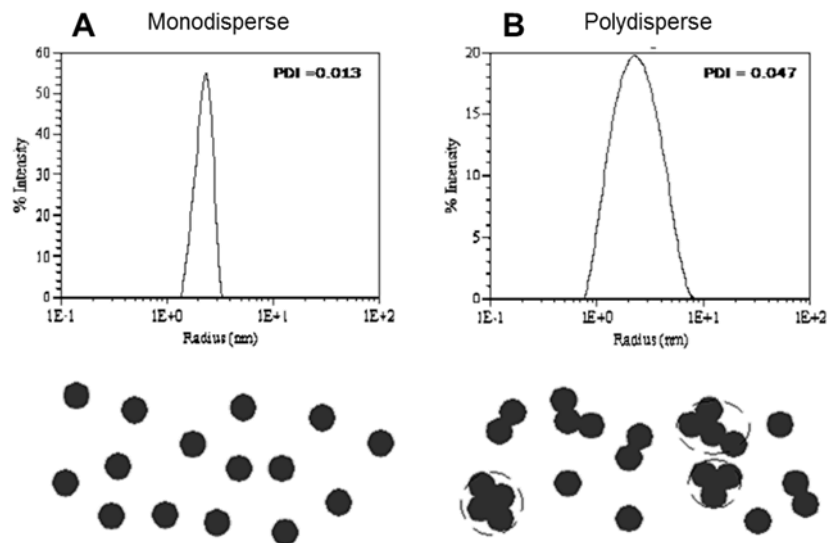


Figure A 2. Principle of polydispersity index (PDI). (A) Monodisperse sample; (B) Polydisperse sample.

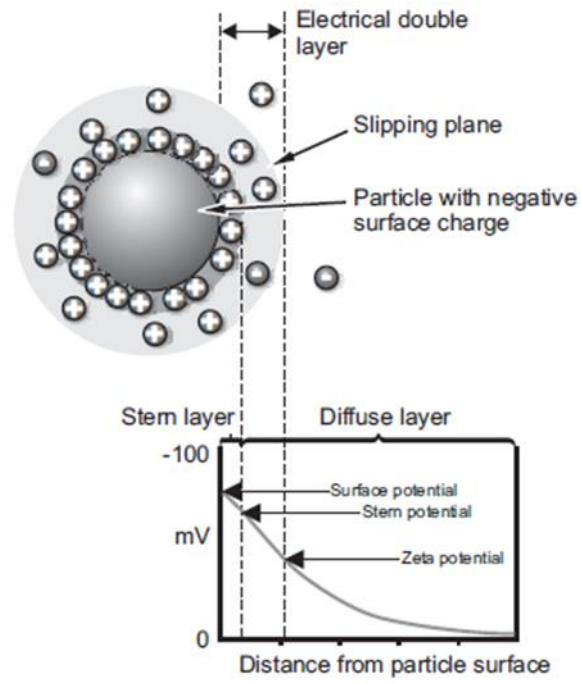


Figure A 3. Principle of zeta potential (from Malvern (2004)).

Appendix B

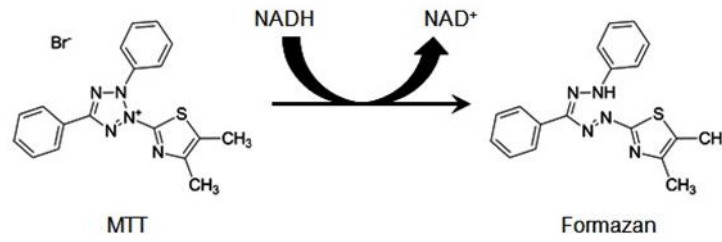


Figure B 1. Principle of the MTT methodology (from Riss *et al.* (2004)).

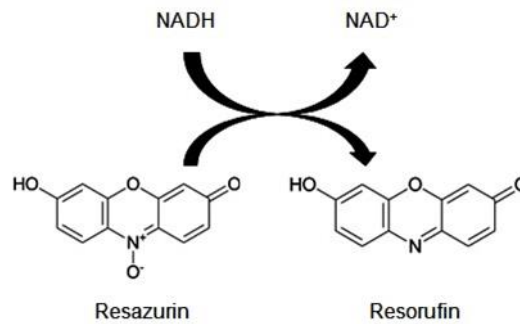


Figure B 2. Principle of the Alamar Blue methodology (from Riss *et al.* (2004)).

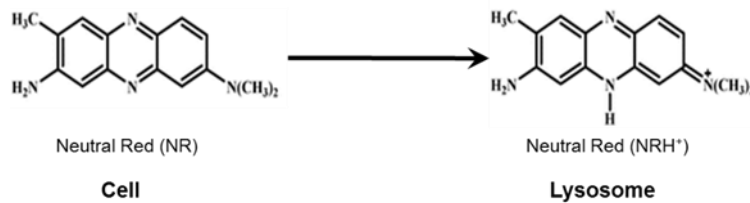


Figure B 3. Principle of the Neutral Red uptake methodology (based on Repetto *et al.* (2008)).

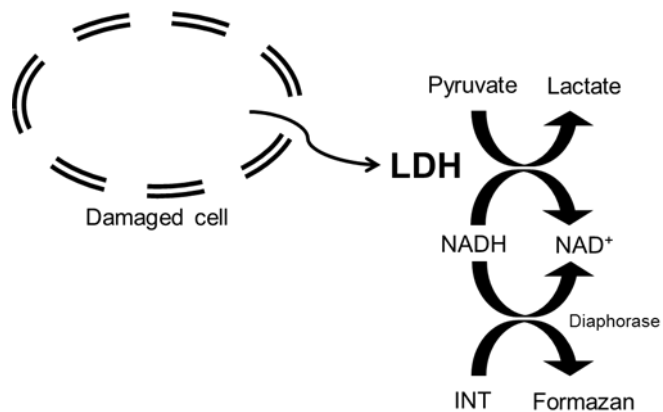


Figure B 4. Principle of the lactate dehydrogenase (LDH) reaction inside the cell (adapted from Thermo (2015)).