

Enhancement of Emotion Recognition using Feature Fusion and the Neighborhood Components Analysis

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Abstract: Feature fusion is a common approach to improve the accuracy of the system. Several attempts have been made using this approach on the Mahnob-HCI database for affective recognition, achieving 76% and 68% for valence and arousal respectively as the highest achievements. This study aimed to improve the baselines for both valence and arousal using feature fusion of HRV-based, which used the standard Heart Rate Variability analysis, standardized to mean/standard deviation and normalized to [-1,1], and cvxEDA-based feature, calculated based on a convex optimization approach, to get the new baselines for this database. The selected features, after applying the sequential forward floating search (SFFS), were enhanced by the Neighborhood Component Analysis and fed to kNN classifier to solve 3-class classification problem, validated using leave-one-out (LOO), leave-one-subject-out (LOSO), and 10-fold cross validation methods. The standardized HRV-based features were not selected during the SFFS method, leaving feature fusion from normalized HRV-based and cvxEDA-based features only. The results were compared to previous studies using both single- and multi-modality. Applying the NCA enhanced the features such that the performances in valence set new baselines: 82.4% (LOO validation), 79.6% (10-fold cross validation), and 81.9% (LOSO validation), enhanced the best achievement from both single- and multi-modality. For arousal, the performances were 78.3%, 78.7%, and 77.7% for LOO, LOSO, and 10-fold cross validations respectively. They outperformed the best achievement using feature fusion but could not enhance the performance in single-modality study using cvxEDA-based feature. Some future works include utilizing other feature extraction methods and using more sophisticated classifier other than the simple kNN.

1 INTRODUCTION

Although the standard HRV analysis (Task Force of the European Society of Cardiology the North American Society of Pacing Electrophysiology, 1996) was not suitable to ECG signals in the Mahnob-HCI database for affect recognition (Soleymani et al., 2012) due to signal length requirements, the Neighborhood Components Analysis (NCA) (Goldberger et al., 2005) could refine the quality of the features, improving the accuracy from about 43% and 48% to 69% and 71% for valence and arousal respectively to solve 3-class classification problem (Ferdinando et al., 2017a). Further, (Ferdinando and Alasaarela, 2017) extracted features using the cvxEDA, a convex optimization approach to analyze EDA signal, (Greco et al., 2016) from Galvanic Skin Response (GSR) or Electrodermal Activity (EDA) signals from this database for valence and arousal recognition achiev-

ing accuracies up to 75% and 77% respectively.

Previously, others have already applied feature fusion for emotion recognition using the Mahnob-HCI database to solve 3-class problem in valence and arousal. Soleymani et al. (Soleymani et al., 2012) provided the baselines, i.e. 76% and 68% for valence and arousal respectively by combining features from EEG and eye gaze using SVM. Zhu et al. (Zhu et al., 2014) fused EEG and audio/video signals and achieved up to 58% and 61% for valence and arousal correspondingly using the same classifier. Wiem and Lachiri (Wiem and Lachiri, 2017) used features from ECG, Resp, Temp and GSR, and SVM with various kernel, achieving 57% and 55% for valence and arousal respectively. Using EEG and several physiological signals, Shu and Wang (Shu and Wang, 2017) achieved 59% for valence and 66% for arousal on SVM. Overall, the best accuracies were achieved by Soleymani et al. and this work served

as references. Another reference was the highest accuracy from single-modality achieved by Ferdinando and Alasaarela (Ferdinando and Alasaarela, 2017). Aiming to improve the baselines, we fused features from the standard HRV analysis, analyzed using the standard HRV analysis (Task Force of the European Society of Cardiology the North American Society of Pacing Electrophysiology, 1996) and the cvxEDA (Greco et al., 2016), to develop a multi-modal affect recognition. The new set of features was subject to feature selection using the sequential forward floating search (SFFS) method, followed by the NCA (Goldberger et al., 2005) to enhance the features quality.

The kNN classifier was used to solve 3-class classification problem in valence and arousal, validated using leave-one-out (LOO), leave-one-subject-out (LOSO), and 10-fold cross validations to accommodate validation from the previous studies. The best result from each dimensionality was selected based on significance test using t-test with 0.05 significance level. The final result from each validation was the best result with the lowest dimensionality, assessed with algorithm proposed in (Ferdinando et al., 2017a) and compared to the previous results.

2 MATERIAL AND METHODS

Figure 1 shows the block diagram of this study. There were two dimensionality reduction processes applied to the fused features. After the dimensionality reduction process, the features were fed to a classifier and an algorithm was used to select the best result with the lowest dimensionality.

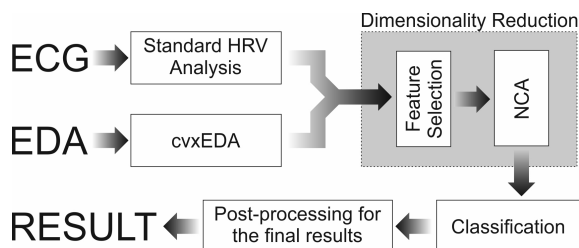


Figure 1: Block diagram of this study.

2.1 Database

Both ECG and EDA signals used in this study were from the Mahnob-HCI database for affect recognition. Recorded from 30 subjects stimulated by pictures and videos, the Mahnob provides synchronized measurement to enable multimodal affect recognition study (Ferdinando et al., 2016). To be more specific,

the signals were downloaded from database server under *Selection of Emotion Elicitation*, providing 513 samples from 26 subjects because samples from some of the subject were corrupted.

2.2 Feature Extraction

During the experiments, there were 30 seconds before and after the stimulated phase called *relaxing phase* when the subjects were not emotionally stimulated. A synchronization pulse was used to mark the beginning and the end of stimulation phase. Features from ECG signals were derived from ECG signal before the stimulation, called *baseline*, and during the stimulation, called *response*.

Feature indices from standard HRV analysis were (Ferdinando et al., 2017a):

- RMS of the Successive Difference between adjacent R-R intervals (RMSSD).
- Standard Deviation of the Successive Difference between adjacent R-R intervals (SDSD).
- Standard Deviation of all NN intervals (SDNN).
- Number of pairs of adjacent NN intervals differing by more than 50 ms (NN50).
- Number of pairs of adjacent NN intervals differing by more than 20 ms (NN20).
- NN50 count divided by the total number of NN intervals (pNN50).
- NN20 count divided by the total number of NN intervals (pNN20).
- Power spectral density for very low frequency (VLF), low frequency (LF), high frequency (HF), and total power.
- Ratio of HF to LF.
- Poincar analysis (SD1 and SD2).
- Ratio of response to baseline features.

The acquired features were standardized based on mean and SD, and also normalized to [-1,1] to get three sets of HRV-based features, i.e. standardized features, normalized features, and joined standardized and normalized features.

Features from EDA were extracted using a optimization approach, called cvxEDA (Greco et al., 2016), which was applied to EDA from the Mahnob and provided good performance for both valence and arousal (Ferdinando and Alasaarela, 2017). The cvxEDA can be applied directly to raw signal and splits it into phasic, tonic, and noise. Similar to ECG signal, features from EDA were also calculated using baseline and response point of view. Feature indices from EDA were (Ferdinando and Alasaarela, 2017)

- nSCR1, number of significant SCR within 5-second non-overlap window, divided by number of window.
- nSCR2 = number of significant SCR within 5 second non-overlap window, divided by length of the signal in seconds.
- nSCR3 = number of significant SCR divided by length of the signal in seconds.
- Area under curve (AUC) of phasic and tonic signals.
- 14 items of statistical distribution: mean, standard deviation, Q1, median, Q3, IQR, percentile 2.5, percentile 10, percentile 90, percentile 97.5, maximum, skewness, and kurtosis.
- Power in 0-0.1 Hz, 0.1-0.2 Hz, 0.2-0.3 Hz, 0.3-0.4 Hz.
- Ratio of response to baseline features.

The three sets of HRV-based features were fused individually to cvxEDA-based feature, resulting three sets of fused features for the next process.

2.3 Dimensionality Reduction

Prior to feeding the fused features to classifier, a sequential forward floating search (SFFS) method was used to select a set of features having high discriminant values from the three sets of fused features utilizing kNN to evaluate its performance. Next, the Neighborhood Components Analysis (NCA) (Goldberger et al., 2005) was used to calculate a projection matrix able to transform the selected features into certain space such that the distances among features belong to the same class were decreased while increasing distances among features belong to different classes. The NCA calculation used the implementation in the *drtoolbox* written for Matlab¹. The projection matrix also reduced the dimensionality of the features in the new space to [2,9] (Ferdinando and Alasaarela, 2017).

2.4 Classifier and Validation

We used the kNN classifier to compare our results with the other previous studies appropriately and validated using 10-fold cross, leave-one-out (LOO), and leave-one-subject-out (LOSO) validation methods. For 10-fold cross validation, 20% of the samples were held out for validation while the rest of the samples were subject to training and testing purpose with 1000 repetitions and new resampling for every repetition to get the average as close as possible to the true value.

¹<https://lvdmaaten.github.io/drtoolbox/>

In the LOO validation, one sample is excluded to validate the model built using the remaining samples. This process continues to each sample and the average is reported. Generally, the LOSO validation is similar to the LOO but the excluded samples are from one of the subjects.

2.5 Post-processing

The results were grouped according to the dimensionality. One result must be chosen to represent the results of that dimensionality. We used t-test with 0.05 significance level to assess if the differences among the results within the same dimensionality was significant or not. Later, an algorithm was used to select the best result with the lowest dimensionality for each validation (Ferdinando et al., 2017a):

1. Find the best accuracy (namely, A1).
2. If the best accuracy is occurred at the lowest dimensionality, then the best result is found (the best result = A1).
3. Otherwise, find the second-best accuracy (namely, A2) from the lower dimensionality and compare A1 to A2 using t-test with significance level 0.05.
4. If the difference is statistically significant, then the best results is found (the best result = A1).
5. If the difference is not statistically significant, then the second-best turns to the best accuracy. Repeat process from step 2 until it reaches the lowest dimensionality.

3 RESULTS AND DISCUSSIONS

3.1 Fused Feature Evaluation

After applying the SFFS to fused features of standardized HRV-based, normalized HRV-based, and cvxEDA-based features, it was found that none of standardized HRV-based features were selected in both valence and arousal. It seemed using ordinary mean and standard deviation, instead of median and median absolute deviation (MAD) or median and interquartile range (IQR), were not suitable to the distribution, so that the standardized features captured less information about valence and arousal than the ones from the others. Consequently, there were no experiment from fused features of standardized HRV-based and cvxEDA-based features. The SFFS reduced the dimensionalities from 168 to 14 and from 168 to 11 for valence and arousal respectively.

3.2 Recognition Results

Figure 2 shows the valence accuracy based on LOO validation of the fused features with and without applying the NCA, and also the baseline from (Soleymani et al., 2012). The proposed method offered better accuracy than the baseline, even without applying the NCA. Applying the algorithm in (Ferdinando et al., 2017a), the difference between 82.4% (8D) and 81.8% (4D) was evaluated using t-test at 0.05 significance level and found that 82.4% (8D) was the best result with the lowest dimensionality. Similar phenomenon occurred in arousal, see Figure 3, where the performance without applying the NCA already outperformed the baseline. Since the highest performance was already in the lowest dimensionality, it became the best result with the lowest dimensionality.

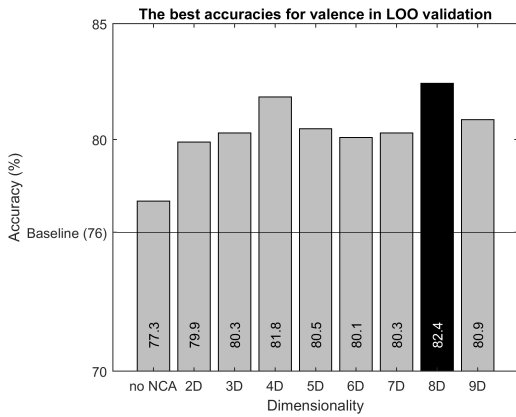


Figure 2: The best accuracy for valence with and without involving the NCA using kNN classifier in LOO validation and the baseline from (Ferdinando and Alasaarela, 2017) showed that the NCA improved the accuracies of system.

Now, we compare these achievements to the some previous studies. Table 1, visualized in Figure 4, compare the current results to the original baseline from the database (Soleymani et al., 2012) and the same system using cvxEDA-based features only (Ferdinando and Alasaarela, 2017), which presented the result based on LOO validation. For valence, our result outperformed the one from both previous studies. For arousal, our result was slightly above the system used cvxEDA-based features only (Ferdinando and Alasaarela, 2017) but outperformed the one from the database owner (Soleymani et al., 2012).

Figure 5 shows the accuracy for valence in 10-fold cross validation and the baseline from (Ferdinando and Alasaarela, 2017) because no previous studies used 10-fold cross validation. Both implementation with and without involving the NCA outperformed the baseline significantly, confirmed using t-test at 0.05 significance level. Applying supervised dimen-

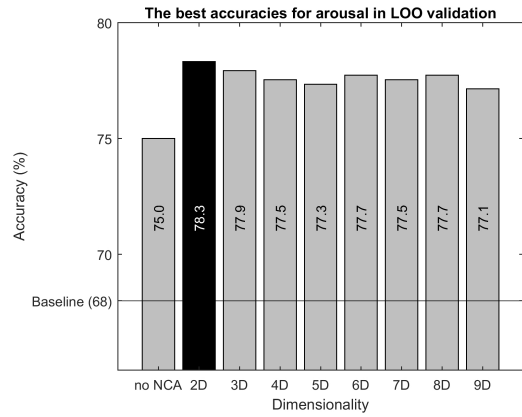


Figure 3: The best accuracy for arousal with and without involving the NCA using kNN classifier in LOO validation and the baseline from (Ferdinando and Alasaarela, 2017) showed that the NCA improved the accuracies of system.

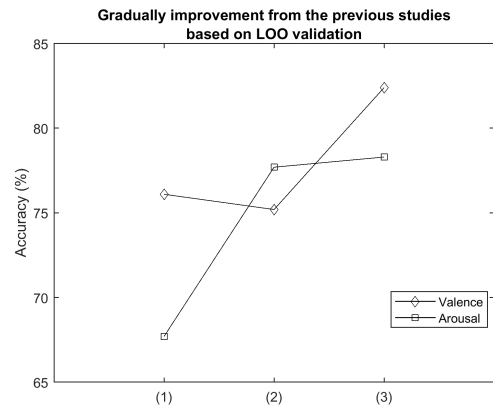


Figure 4: Visual representation of improvements for valence and arousal from the previous studies based on LOO validation (1): all peripheral physiological signals (Soleymani et al., 2012), (2): EEG+Gaze (Soleymani et al., 2012), (3): EDA (Ferdinando and Alasaarela, 2017), (4): current results.

sionality reduction to the fused features boosted the accuracy but kept the standard deviation accuracy almost unchanged. On the other hand, the NCA failed to boost all accuracies for arousal as only some of them outperformed the baseline while the other were below the baseline, see Figure 6. Using the algorithm to select the best result with the lowest dimensionality as proposed in (Ferdinando et al., 2017a), the best performances were achieved at 79.6 ± 3.7 (8D) and 77.7 ± 3.8 (2D) for valence and arousal respectively.

Table 2, visualized in Figure 7, compared the current results to the previous studies based on 10-fold cross validation. As shown in the previous studies, it was easier to recognize arousal than the other but findings in this study presented the opposite. The accuracies were also gradually improved significantly,

Table 1: Performance comparison to the original baseline from the owner of the database (Soleymani et al., 2012) and the other previous study (Ferdinando and Alasaarela, 2017) in leave-one-out (LOO) validation.

	(Soleymani et al., 2012)	(Ferdinando and Alasaarela, 2017)	Current Results
Input Signals	EEG+Gaze	EDA	HRV+EDA
Valence	76.1	75.2	82.4
Arousal	67.7	77.7	78.3

Table 2: Compare the performance with the previous study for 10-fold cross validation.

Input Signals	ECG ¹	ECG, HRV ²	EDA ³	HRV+EDA ⁴
Valence	64.1 ± 7.4	68.6 ± 4.4	74.6 ± 3.8	79.6 ± 3.7
Arousal	66.1 ± 7.4	70.7 ± 4.3	77.3 ± 3.6	77.7 ± 3.9

¹ Results from (Ferdinando et al., 2017b)

² Results from (Ferdinando et al., 2017a)

³ Results from (Ferdinando and Alasaarela, 2017)

⁴ Results from proposed method

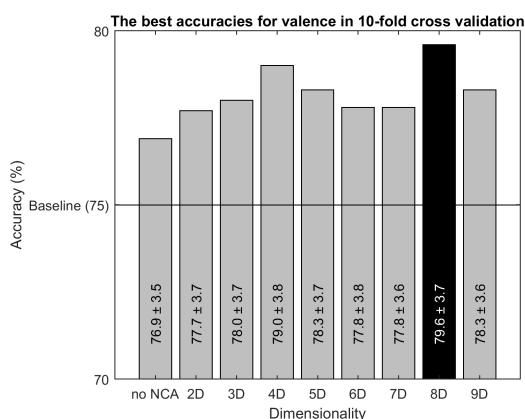


Figure 5: The best accuracy for valence with and without involving the NCA using kNN classifier in 10-fold cross validation after 1000 iterations and the baseline from (Ferdinando and Alasaarela, 2017) showed that the NCA enhanced the accuracies very well.

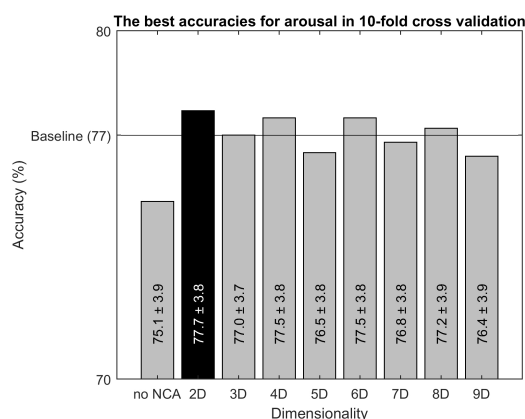


Figure 6: The best accuracy for arousal with and without involving the NCA using kNN classifier in 10-fold cross validation after 1000 iterations and the baseline from (Ferdinando and Alasaarela, 2017) showed that the NCA did not enhance all accuracies, see 3D, 5D, 7D, and 9D.

except for arousal, see Figure 7. It indicated the NCA could not improve the accuracy anymore. To get better accuracy, another feature extraction method is needed or other modalities are used. The fused features also kept the standard deviation unchanged, indicating the same consistency among the repetitions.

The results based on the LOSO validation for both valence and arousal are displayed in Figure 8 and 9 respectively. The results in Figure 8 presented the same facts as in Figure 4, where all of them outperformed the baseline. What stands out from Figure 8 was the best result with the lowest dimensionality was represented by 4D instead of 8D, although the later has higher performance. Significance test between 82.7 ± 8.5 (8D) and 81.9 ± 8.8 (4D) resulted no significance difference, bringing consequence that 81.9 ± 8.8 (4D) was chosen. It was interesting to note here that the di-

mensionalities, which outperformed the baseline for arousal were exactly the same as in the other validation method, compare Figure 6 and 9.

Table 3, visualized in Figure 10, revealed several interesting results. Firstly, the NCA could improve the quality of the fused features and boost the accuracy for valence to 82%. Unfortunately, there was no significant improvement from (Ferdinando and Alasaarela, 2017) for arousal. Applying the NCA to the fused features failed to improve the performance. Secondly, the standard deviation of the current results were close to (Ferdinando and Alasaarela, 2017), which used cvxEDA-based feature only.

Table 3: Compare the performance with the previous study for LOSO validation.

Input Signals	ECG ¹	ECG, HRV ²	EDA ³	HRV+EDA ⁴
Valence	61.7 ± 14.1	70.7 ± 4.9	75.5 ± 7.7	81.9 ± 8.8
Arousal	69.6 ± 12.4	73.5 ± 4.4	77.8 ± 8.0	78.7 ± 9.5

¹ Results from (Ferdinando et al., 2017b)

² Results from (Ferdinando et al., 2017a)

³ Results from (Ferdinando and Alasaarela, 2017)

⁴ Results from proposed method

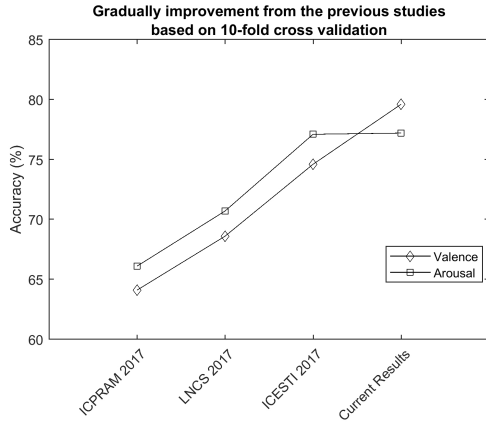


Figure 7: Visual representation of improvements for valence and arousal from the previous studies based on 10-fold cross validation.

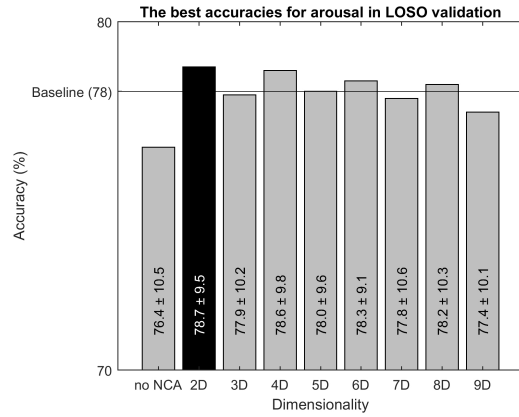


Figure 9: The best accuracy for arousal with and without involving the NCA using kNN classifier in LOSO validation and the baseline from (Ferdinando and Alasaarela, 2017).

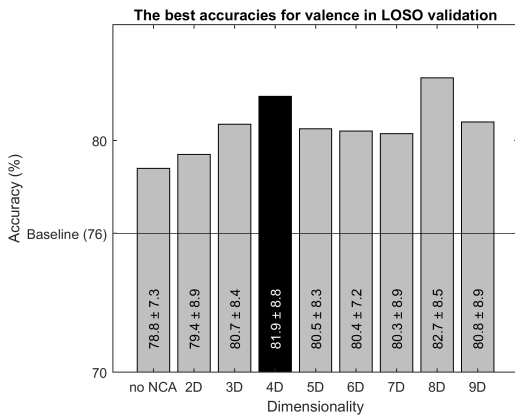


Figure 8: The best accuracy for valence with and without involving the NCA using kNN classifier in LOSO validation and the baseline from (Ferdinando and Alasaarela, 2017). Although 82.7 ± 8.5 (8D) was higher than 81.9 ± 8.8 (4D), the later was selected as the best result with the lowest dimensionality through the proposed algorithm in [LNCS 2017].

4 CONCLUSIONS

Performances of affect recognition using feature fusion of HRV-based and cvxEDA-based features in-

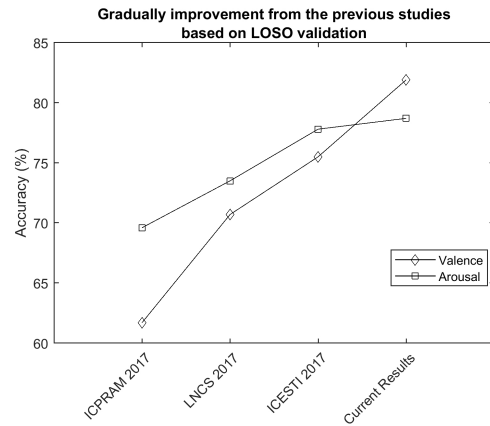


Figure 10: Visual representation of improvements for valence and arousal from the previous studies based on LOSO validation.

volving the NCA were presented. The HRV-based features involved in this study were from the normalized one only while the other conveyed information about valence and arousal insufficiently, confirmed by the SFFS. The fused features contained a lot of un-useful features as most of them were discarded by the SFFS, leaving 14 and 11 features for valence and arousal respectively.

For valence, the fused features without applying the NCA offered better performance than the previous

studies in all validation methods, so also the enhanced features after applying the NCA. For arousal, feature fusion did not work as good as for valence. However, applying the NCA enhanced them to work better but not at all dimensionality. Results presented here were the best results with the lowest dimensionality. Overall, feature fusion of normalized HRV-based and cvxEDA-based features together with feature enhancement using the NCA offered new baselines for both valence and arousal in three validation methods.

Our results in arousal were only slightly above the best ones from the previous studies based on LOO and LOSO validation, and was similar to the one based on 10-fold cross validation. Using other feature extraction method is recommended to enhance the performance in all validation methods and employing more sophisticated classifier other than the simple kNN are left for future works.

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REFERENCES

- Ferdinando, H. and Alasaarela, E. (2017). Emotion recognition using cvxEDA-based features. In *Proceeding of the 3rd International Conference on Electrical Systems, Technology and Information (ICESTI) 2017*. MATEC Web of Conference.
- Ferdinando, H., Seppänen, T., and Alasaarela, E. (2016). Comparing features from ECG pattern and HRV analysis for emotion recognition system. In *2016 IEEE Conference on Computational Intelligence in Bioinformatics and Computational Biology, CIBCB 2016, Chiang Mai, Thailand, October 5-7, 2016*, pages 1–6.
- Ferdinando, H., Seppänen, T., and Alasaarela, E. (2017a). Emotion recognition using neighborhood components analysis and ecg/hrv-based features. In M. De Marsico, G. S. di Baja, A. F., editor, *Lecture Note on Computer Science: Pattern Recognition Applications and Methods*. Springer Berlin Heidelberg, Berlin, Heidelberg. Accepted.
- Ferdinando, H., Seppänen, T., and Alasaarela, E. (2017b). Enhancing emotion recognition from ECG signals using supervised dimensionality reduction. In *Proceedings of the 6th International Conference on Pattern Recognition Applications and Methods, ICPRAM 2017, Porto, Portugal, February 24-26, 2017.*, pages 112–118.
- Goldberger, J., Hinton, G., Roweis, S., and Salakhutdinov, R. (2005). Neighbourhood components analysis. In Saul, L. K., Weiss, Y., and Bottou, L., editors, *Advances in Neural Information Processing Systems 17*, pages 513–520. MIT Press.
- Greco, A., Valenza, G., Lanata, A., Scilingo, E. P., and Citi, L. (2016). cvxeda: A convex optimization approach to electrodermal activity processing. *IEEE Trans. Biomed. Engineering*, 63(4):797–804.
- Shu, Y. and Wang, S. (2017). Emotion recognition through integrating eeg and peripheral signals. In *Proceeding of the IEEE International Conference on Acoustics, Speech and Signal Processing (ICASSP)*. IEEE.
- Soleymani, M., Lichtenauer, J., Pun, T., and Pantic, M. (2012). A multimodal database for affect recognition and implicit tagging. *IEEE Trans. Affective Computing*, 3(1):42–55.
- Task Force of the European Society of Cardiology the North American Society of Pacing Electrophysiology (1996). Heart rate variability standards of measurement, physiological interpretation, and clinical use. *Circulation*, 93(5):1043–1065. HRV autonomic risk factors.
- Wiem, M. B. H. and Lachiri, Z. (2017). Emotion classification in arousal valence model using mahnob-hci database. *International Journal of Advanced Computer Science and Applications*, 8(3).
- Zhu, Y., Wang, S., and Ji, Q. (2014). Emotion recognition from users’ eeg signals with the help of stimulus videos. In *Proceeding of IEEE International Conference on Multimedia and Expo (ICME)*. IEEE.