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# Spark plasma sintered Ti6Al4V-ZrO2 bio-composites: optimization of ball milling and turbula mixing of powders and their subsequent sintering parameters 

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#### Abstract

The use of Ti6A14V as a biomaterial has been limited due to the dissociation of V and Al ions into the surrounding environment which can cause inflammations, cell damage and toxicity. To prohibit these undesirable challenges, the addition of $\mathrm{ZrO}_{2}$ into Ti 6 Al 4 V was proposed because ZrO 2 is biocompatible, it has good wear and corrosion resistant properties, it has low affinity to bacterial colonization and it has high fracture toughness. The aim of this work is to determine the optimum powder synthesising parameters by Tubular mixer and ball mill for fabrication of sintered composites. Powder mixtures were prepared by $49 \mathrm{rpm}, 72 \mathrm{rpm}$ and 74 rpm for 2,4 and 8 hours followed by spark plasma sintering at $1100^{\circ} \mathrm{C}$ at heating rate of $100^{\circ} \mathrm{C} / \mathrm{min}$ for 10 min and pressure of 50 MPa .from the results obtained it was discovered that Tubular mixing of $90 \mathrm{Vol} \% \mathrm{Ti} 6 \mathrm{Al} 4 \mathrm{~V}$ and $10 \mathrm{Vol} \% \mathrm{ZrO}_{2}$ at 72 rpm and ball milling of 90 $\mathrm{Vol} \% \mathrm{Ti} 6 \mathrm{Al} 4 \mathrm{~V}$ and $10 \mathrm{Vol} \% \mathrm{ZrO}_{2}$ at 74 rpm speed have proved to produce homogeneous admixed powders, which can further produce fully dense SPS compacts with higher microhardness values.


## 1.Introduction

Ti6A14V is a grade of titanium alloy which is considered suitable for the fabrication of implants. This alloy was developed to improve the properties of commercially pure titanium such as low strength and wear resistance for hard tissue replacements [1].Ti6Al4V properties range from good biocompatibility, good mechanical properties to good corrosion and wear resistance as such, it was considered a superior metallic biomaterial compared to cobalt-alloys and stainless [2]. However, it was discovered by Manivasagam [3] that under a biological environment such as the human body it releases toxic metal ions of vanadium and aluminium thus leading to diseases such as Alzheimer. This release of toxic ions occurs even though the metal is protected by the surface oxide layers from the environmental attack; as such this was a clear indication that the corrosion resistance of Ti6Al4V is not sufficient and may results in the implant failure. To hinder the release of these ions and the formation of debris which can go into the blood, the addition of $\mathrm{ZrO}_{2}$, which possesses high fracture toughness, high wear resistance, high strength and excellent biocompatibility to Ti6A14V was
proposed [3]. The bio-composite was fabricated by Spark Plasma Sintering, a powder metallurgy technology based on simultaneous application of high temperature, high axial pressure, and low-mode (low voltage, high current) field (plasma) associated with an electric current on powders through a graphite die and plungers. In comparison with the conventional sintering methods, it offers products with fine microstructures and high density at relatively low sintering temperatures, very short sintering times and easy control of the sintering conditions [4]. Hence the work was aimed at studying the effect of the ad-mixed and milled powder metallurgy preparation methods on the densification and microhardness of Ti6A14V-ZrO 2 bio-composites produced via SPS.

## 2. Materials and Methods

Ti6A14V (average particle size of $18.94 \mu \mathrm{~m}$ ) and $\mathrm{ZrO} 2(65,26 \mu \mathrm{~m})$ powders were utilized as the starting materials for this research. The two powders were mixed and milled in a dry environment using a Turbular shaker mixer (T2F) and planetary ball mill (RETSCH PM 400 MA-type) at a speed of 49 and $72 / 74 \mathrm{rpm}$ for 2,4 and 8 hours with the powder ratio of $90 \mathrm{Vol} \% \mathrm{Ti} 6 \mathrm{Al} 4 \mathrm{~V}$ and $10 \mathrm{Vol} \% \mathrm{ZrO}$. The morphology and powder particle size distribution (PSD) of the mixed and milled powders were examined using scanning electron microscope (SEM) and particle size analyser (Microtrac s3500). The amount of mixed powders required to produce a 40 mm diameter and 5 mm thickness of Ti6A14VZrO 2 Nano structured bio-composites were poured into graphite die and then sintered using a spark plasma-sintering machine (HHPD-25 FCT GmbH Germany).

The optimized powders were sintered at $1100^{\circ} \mathrm{C}$ at a heating rate of $100^{\circ} \mathrm{C} / \mathrm{min}$ and 50 Mpa pressure in vacuum condition. The relative densities of the samples were measured using an OHAUS density kit and by Archimedes principle of the staring powders constituents using the rule of mixtures. The samples were prepared for metallography following the metallographic standard procedure prescribed for griding and polishing for Ti6A14V-ZrO2. The samples were etched using kroll etchant for 30 seconds and the microstructure was analysed using a (Tescan) scanning electron microscope. The Vickers micro hardness (Hv20) was measured by a micro-hardness tester machine (model falcon 500 series) whereby each sample was indented 10 times. The samples were labelled based on the ZrO 2 ratio added to Ti6Al4V, the mixing/milling speed, the mixing/milling time and the type of mixing process. For example, $10-49-2 \mathrm{~T}$ means that this sample has $10 \mathrm{Vol} \% \mathrm{ZrO} 2$ added, it was mixed at 49 rpm for 2 hours in a Turbula mixer and $10-49-2 \mathrm{~B}$ means the sample has $10 \mathrm{Vol} \% \mathrm{ZrO} 2$ at a speed of 49 rpm for 2 hours in a ball mill.

## 3. Results and Discussion

### 3.1 SEM results



Figure 1: SEM Micrographs of as-received (a) Ti 6 Al 4 V and (b) $\mathrm{ZrO}_{2}$ powders.
The SEM results of as-received powders are shown in figure 1, revealed that the Ti6A14V powder is spherical and non- porous while the $\mathrm{ZrO}_{2}$ powders are doughnut shaped, hollow and porous.

### 3.1.1 Turbular mixing.

Figure 2 illustrates SEM Micrographs of (a)10-49-2T ,(b) 10-49-4T, (c) 10-49-8T, (d)10-72-2T,(e)10-$72-4 \mathrm{~T}$ and (f) 10-72-8T.In the obtained results, it is evident that the doughnut-like shape of ZrO 2 particles was strongly broken down in all Turbula admix powders due to the combination of motion of rotation, translation and inversion as well as the impact of the balls that led to the effective reduction of the particle size of the product during mixing. The ZrO 2 particles are homogeneously distributed in the Ti6A14V particles. Furthermore, an interesting trend discovered in these SEM results was the powders became more homogenous with an increase in speed and time from $49-72 \mathrm{rpm}$ and $2-8$ hours.


Figure 2: SEM Micrographs of (a)10-49-2T,(b)10-49-4T,(c)10-49-8T,(d)10-72-2T,(e)10-72-4Tand (f) 10-72-8T.

### 3.1.2 Ball milling

Figure 3 illustrate the SEM Micrographs of (a)10-49-2B,(b)10-49-4B,(c)10-49-8B,(d)10-74-2B,(e)10-$74-2 \mathrm{~B}$ and (f) 10-74-8B. An interesting trend discovered in these results was that satellites of Ti6A14V have agglomerated in the unbroken hallow ZrO 2 powder particles, this trend is more evidential in
(c)10-49-8B, additionally the results indicate that the $\mathrm{ZrO}_{2}$ powder particles are gradually homogeneously distributed in the Ti6Al4V particles as the speed and time of milling increases. According to these results, it is evident that $\mathrm{ZrO}_{2}$ powder particles are also broken down during ball milling but only at high speeds such as 74 rpm .


Figure 3: SEM Micrographs (a)10-49-2B,(b)10-49-4B,(c)10-49-8B,(d)10-74-2B,(e)10-74-2B and (f) 10-74-8B.

### 3.2 PSD results



Figure 4: shows the particle size distribution of received powders and mixed powders
The obtained PSD results showed that the $\mathrm{ZrO}_{2}$ powder has coarse particle size of $65 \mu \mathrm{~m}$ while Ti6A14V has fine particle size of $19 \mu \mathrm{~m}$ as shown in figure 4. It was discovered that the PSD results compliments the SEM results whereby the Turbula mixed powders have the lowest values of average particle size than that of ball milled powders (illustrated in figure 4). A pattern was also discovered in these results where there is a continuous reduction in powder particle size reduction as we increase mixing/milling speed and time. Moreover, the SEM results alongside with the PSD results indicate that 72 rpm and 74 rpm are the optimum mixing/milling speed since they produce powders with low particle size distribution than powders mixed/milled at 49 rpm . The samples from the optimised speeds of 72 rpm and 74 rpm were considered to be the best choice to sinter $\mathrm{Ti} 6 \mathrm{Al} 4 \mathrm{~V}-\mathrm{ZrO}_{2}$ bio-composites.

### 3.3 Sintered Composites Results

SEM Micrographs of sintered Ti6A14V-ZrO2 composites, which were mixed and milled at the speed of 72 rpm and 74 rpm , are illustrated by figure 5 . The microstructure of all sintered samples contains a pool of Ti with island of ZrO 2 and they also contain micro pours that lead to crack propagation during metallographic preparation.



Figure 5: SEM Micrographs of sintered composites (a) 10-72-2T,(b)10-72-4T, (c)10-72-8T, (d)10-742B, (e) 10-74-4B and (f) 10-74-8B.

### 3.4 Densification

Table 1 illustrate that density increase with increasing with sintering temperature, this is because porosity decreases when the atoms are bonded together during sintering. Considering the above statement, this could be one of the reasons that the Standard sample (Ti6A14V) sintered at 1000 has low densification value of $99.6 \%$ and the $\mathrm{Ti} 6 \mathrm{Al} 4 \mathrm{~V}-\mathrm{ZrO} 2$ bio-composite samples sintered at 1100 have high densification values of $100 \%$.

Table 1: Densities of Sintered samples.

| Sample <br> name | Holding <br> Time, <br> min | Pressure, <br> MPa | Heating <br> Rate, <br> ${ }^{\mathbf{}} \mathbf{C} / \mathbf{m i n}$ | Sintering <br> temperature <br> $\left({ }^{\circ} \mathbf{c}\right)$ | Densification <br> $\%$ |
| :--- | :--- | :--- | :---: | :---: | :---: |
| Standard <br> sample <br> (Ti6A14V) | 10 | 50 | 100 | 1000 | 99.6 |
| $\mathbf{1 0 - 7 2 - 2 T}$ | 10 | 50 | 100 | 1100 | 100 |
| $\mathbf{1 0 - 7 2 - 4 T}$ | 10 | 50 | 100 | 1100 | 100 |
| $\mathbf{1 0 - 7 2 - 8 T}$ | 10 | 50 | 100 | 1100 | 100 |
| $\mathbf{1 0 - 7 4 - 2 B}$ | 10 | 50 | 100 | 1100 | 100 |
| $\mathbf{1 0 - 7 4 - 4 B}$ | 10 | 50 | 100 | 1100 | 100 |
| 10-74-8B | 10 | 50 | 100 | 1100 | 100 |

### 3.5 Hardness

Figure 6 Is Microhardness of sintered composites (10-72-2T, 10-72-4T and 10-72-8T) and (10-74-2B, $10-74-4 \mathrm{~B}$ and $10-74-8 \mathrm{~B}$ ) the results shows that mixed samples have the highest microhardness values than the ball milled samples. A trend was observed where microhardness values increase as the mixing and milling time increases from 2 to 8 hours. This could be due to high powder homogeneity as speed and time increased and thus producing a well dense sintered sample. Theoretically, sintering rates increases with increasing reduction in powder particle size, hence the increase in microhardness values as the mixing time increase.


Figure 6: Hardness values of sinterd samples.

## 4. Conclusion

In conclusion Turbular mixing using balls has proved to be more effective than ball milling in producing homogeneously distributed powder mixtures with finer particles, which can be facilitated in the production of fully dense composites. Furthermore, the optimisation of mixing, milling and sintering parameters done in this paper could be utilised as a reference during further work based on $\mathrm{Ti} 6 \mathrm{Al} 4 \mathrm{~V}-\mathrm{ZrO}_{2}$ bio-composites.

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