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Optics Letters

Natural convection induced by an optically fabricated and actuated microtool with a thermoplasmonic disk

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2 Two-photon polymerization was employed for fabricating microtools amenable to optical trapping and manipulation. A disk feature was included as part of the microtools and further functionalized by electron-beam deposition. The nanostructured gold layer on the disk facilitates off-resonant plasmonic heating upon illumination with a laser beam. As a consequence, natural convection characterized by the typical toroidal shape resembling that of Rayleigh-Bénard flow can be observed. A velocity of several $\mu\text{m} \cdot \text{s}^{-1}$ is measured for $2 \mu\text{m}$ microspheres dispersed in the surroundings of the microtool. To the best of our knowledge, this is the first time that thermoplasmonic-induced natural convection is experimentally demonstrated using a mobile heat source. © 2018 Optical Society of America

OCIS codes: (120.6810) Thermal effects; (310.1860) Deposition and fabrication; (140.7010) Laser trapping; (230.4000) Microstructure fabrication.

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3 Recent developments in photolithographic techniques have widened fabrication possibilities and, thus, the applications of microstructures that are now becoming ubiquitous in scientific explorations in the micro- and nano-regimes. Microtools can increase the efficiency of processes that are otherwise difficult to achieve with conventional “macrotools” due to the inherent disparity in size between the macrotools and certain samples and specimens. Furthermore, microstructures can act as a mediator between a specimen and an actuator to minimize damage, especially when dealing with biological samples [1].

Two-photon polymerization (2PP) is a microfabrication technique that relies on the non-linear interaction between a tightly focused femtosecond pulsed light and a photosensitive resin. Two-photon absorption is initiated within the beam’s focal volume and leads to the polymerization of the photoresist in the target region, while minimizing the polymerization in the

out-of-focus regions [2]. A near-infrared (NIR) beam is usually employed to trigger crosslinking, since most resins are transparent in the NIR region, allowing the beam to focus with minimal intensity loss through the photoresist volume. The focused beam is then 3D scanned in the photoresist, which leads to polymerization along the beam’s path and, thus, enables the fabrication of microstructures. Direct laser writing (DLW) using 2PP has been employed for the fabrication of microfluidic devices [3], implantable biomedical devices [4], and hydrogel scaffolds for tissue engineering [5]. DLW is extremely advantageous for rapid prototyping, as it allows fast design and fabrication iterations.

Along with topological design optimization, the functionalization of microtools by chemical or physical treatment allows them to be tailored to more specific tasks. Remote manipulation of microtools can be done by optical trapping, while additional light-matter interaction mechanisms can be used to initiate the intended function of the microtools. In most cases, the trapping beams are spatially separated from the illumination beam used to trigger the additional effect, making them independently configurable. Successful demonstrations of manipulating functionalized microtools include indirect optical manipulation of live cells [6,7], puncturing of cells with embedded carbon nanotubes [8], light confinement and guiding to inaccessible areas in microfluidics [9], rotary motion of micro-rotors by transfer of linear momentum [10], spin angular momentum [11], and orbital angular momentum [12]. Targeted material delivery has been demonstrated by embedding a metal layer inside the body of a hollow microtool, which enabled a draw-and-eject function via thermally induced fluid motion [13].

Under illumination, metallic nanostructures enhance light-to-thermal energy conversion via plasmonic absorption, which makes them viable heat sources in the nano- and micro-regimes. The field of thermoplasmonics has been growing continuously since the early 2000 s when plasmonic heating was demonstrated for photothermal microscopy [14] and photothermal therapy [15]. Recently, thermoplasmonic structures have been employed for different applications such as localized optical heating [16], trapping [17,18], and biosensing [19].

In this Letter, we report the fabrication of a microtool with a thermoplasmonic disk. Using spherical trapping handles, the microtool can be moved to a target location, after which the heating can be activated on demand by a user. The increase in local temperature manifests in thermophoretic effects and the occurrence of natural convection. We are especially interested in an enhanced convection, as this can lead to increased mass flow rates, which are at the same time directed. This is of great interest in lab-on-a-chip systems, as it provides a fundamental understanding of energy conversion on the microscale, and potentially enables direct applications for material delivery and micro-mixing, which are both challenging in microfluidic systems. The generation of plasmon-induced convection is experimentally demonstrated. To the best of our knowledge, this is the first time the actual convection flow induced by thermoplasmonics with the aid of a mobile heat source is reported.

The microtools are fabricated by DWL using a 2PP-based microfabrication system (Nanoscribe Photonic Professional GT, Nanoscribe GmbH, Germany). The 3D design is done in SolidWorks and then transferred to the DeScribe software, where it is digitally sliced in 2D layers and, subsequently, transformed into hatched lines. The fabrication involves scanning the beam focus layer by layer along the hatched lines by moving the stage where the substrate is mounted. We set the slicing and hatching distances to 200 nm and fixed the power scaling to correspond to a 16 mW average power at the aperture objective. The stage velocity was set to $200 \mu\text{m} \cdot \text{s}^{-1}$. We used the Nanoscribe IPL-80 as photoresist to print on glass substrates. Our microtool has three spherical trapping handles (8 μm diameter) and a disk (10 μm diameter, 2 μm thickness). The microtool was designed in this way to attain minimal size while allowing for stable optical trapping through its spherical handles. To allow selective metal coating of the disk, a mask covering the spherical handles and connecting parts was designed and 3D-printed on top of the microtools. The printing of nine microtools with masks takes approximately 4 h. After fabrication, the glass substrate containing the printed microtools is immersed for 20 min in isopropanol to ensure the removal of uncrosslinked photoresist. For fabricating metal-coated microtools, 1 nm of titanium as an adhesive layer followed by a 10 nm layer of gold were deposited on the disks by a physical vapor electron-beam (e-beam) deposition (Wordentec QCL800). The metal layer obtained after gold e-beam deposition is exploited for off-resonant plasmonic heating. After metal coating, the microtools were harvested from the substrate using a syringe with a $100 \times 100 \mu\text{m}^2$ square capillary tube, as described in Ref. [13]. The microtools were then transferred into a Hellma cuvette ($250 \times 250 \mu\text{m}^2$ inner cross section, 20 mm length) containing 0.125% polystyrene microspheres (2 μm diameter Polybead[®] Microspheres, PolySciences, Inc.) and 1% Tween 80 in Milli-Q water ($18.2 \text{M}\Omega \cdot \text{cm}$).

Optical trapping was performed in our Biophotonics Workstation (BWS) that employs counter-propagating (CP) beams to control and actuate particles [Fig. 1(a)] [20,21]. A CP beam relies on scattering forces for trapping instead of the gradient force used in more common optical tweezers [22]. As such, the CP trapping geometry does not require high numerical aperture (NA) objectives and, thus, accommodates a long working distance, which allows for the insertion of an additional objective for side imaging. In our BWS, the CP beams are generated using a proprietary illumination module and a

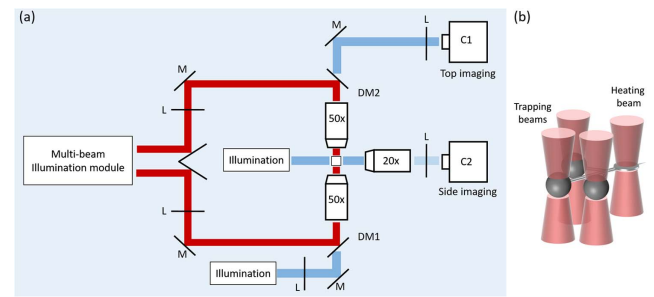


Fig. 1. (a) Schematic diagram of the Biophotonics Workstation. A 1070 nm laser is used for both optical trapping and heating. (b) Schematic representation of a microtool with CP trapping and heating beams.

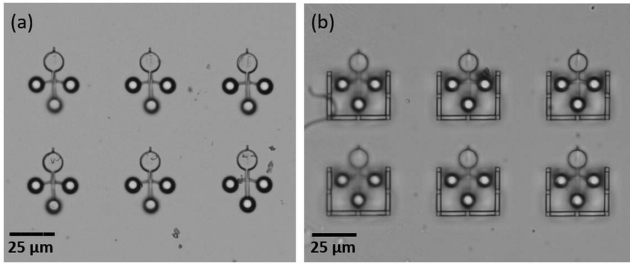
continuous-wave NIR laser (IPG Photonics, $\lambda = 1070 \text{ nm}$, 40 W maximum input power). The beams are then relayed onto the sample using two opposing objectives (Olympus LMPLN, 50 \times IR, WD = 6.0 mm NA = 0.55). A LabView-based graphical user interface (GUI) is used to generate multiple traps displayed as overlay graphics on real-time images acquired with the top camera. Displacement of the microtool in the $x - y$ plane is executed by dragging the trap overlays to the desired location, while manipulation on the z -axis is performed by changing the intensity ratio of the top and bottom beams. The size of the beam spots can also be adjusted from the GUI. In addition to the top-view recording, side imaging is available in the setup using a 20 \times microscope objective (Mitutoyo Plan Apo, 20 \times , WD = 20 mm, NA = 0.42). In our experiments, three CP beams were generated for trapping the microtool, and a fourth CP beam was directed at the disk to induce heating [Fig. 1(b)]. The trapping and heating beam spot sizes were set to 10 μm . In our experiments, the total optical power reaching the microtool is in the order of tens of milliwatts equally divided into the heating and trapping CP beams. The uncertainty arises from the losses in the measurement system. One of the challenges in illuminating the coated disk is the recoil of the microtool due to beam reflection, but this is minimized by trapping the microtool with the aid of the spherical handles.

The videos used for particle tracking consist of 840 frames recorded at 21 frames per second, corresponding to a duration of 40 s. The videos were recorded using the side-view camera from the time the heating beam was turned on. Particle tracking was performed using the Spot Tracking plugin in the Icy image analysis software. Only the particles that remain in focus in the imaging plane for at least 525 frames were taken into account for subsequent data analysis in order to minimize calculation errors due to out-of-plane displacements. The first 525 frames (25 s) of all tracks obtained were used for further data processing. The mean square displacements (MSDs) of individual particles were calculated from the coordinates of the particles using the freely available Matlab tool msdalyzer [23]. In our experiments, we analyze and compare particle trajectories for microtools with both uncoated and coated disks.

Examples of the 3D-printed microtools employed in this Letter are shown in Fig. 2. Each microtool has three spherical handles that allow optical trapping and manipulation. As seen in Fig. 2(b), the mask printed on top of the microtools during

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F1:2
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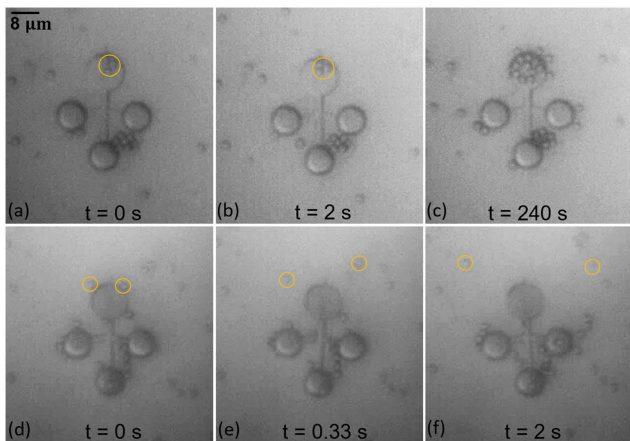


F2:1 **Fig. 2.** 40× bright field images of 3D-printed microtools (a) without
 F2:2 and (b) with masks for subsequent metal coating.

189 the fabrication process selectively exposes the disk feature for
 190 metal coating.

191 Control experiments were performed with uncoated micro-
 192 tools. Figure 3 shows one uncoated microtool just before (a),
 193 and 2 s (b) and 240 s (c) after the heating beam was turned on.
 194 The microspheres located in the immediate vicinity of the trap-
 195 ping spheres and disk were trapped when the laser was turned
 196 on. Leaving the trapping and heating beams on for four min-
 197 utes resulted in some additional aggregation of microspheres
 198 around the trapping spheres and disk, but no significant motion
 199 was observed for microspheres farther from the microtool.
 200 Although the uncoated disk can serve as a heat source by light
 201 absorption, the generated heat is not enough to effect global
 202 motion in the fluid.

203 In contrast, illumination of the gold-coated microtools re-
 204 sulted in the immediate expulsion of microspheres away from
 205 the disk, as can be seen from Figs. 3(d)–3(f). This can be ex-
 206 plained by the increase in temperature around the disk upon
 207 illumination. The metal-coated disk serves as an efficient heat
 208 source by virtue of off-resonant plasmonic heating. Energy
 209 absorption is greatly enhanced with the aid of the plasmonic
 210 nanostructures, which have been previously used as heat
 211 sources [24]. Due to thermophoretic effects, the microspheres
 212 that were initially near the disk tend to move in the direction of
 213 the temperature gradient—from the hotter disk to the cooler



F3:1 **Fig. 3.** Top-view BF images of microtools at different time points
 F3:2 after turning on the heating beam. The microspheres slowly aggregate
 F3:3 around the disk in the presence of the uncoated microtool (a)–(c), but
 F3:4 are rapidly pushed away in the presence of the gold-coated microtool
 F3:5 (d)–(f).

214 area around it. Factors affecting thermophoresis have been exten-
 215 sively studied [25], as well as its applications to thermopho-
 216 retic trapping of nano-objects by plasmonic heating [18,26].

217 For the gold-coated microtools, thermophoretic diffusion is
 218 a consequence of disk heating. When the disk is illuminated, it
 219 heats up by plasmonic absorption and generates a convection
 220 flow that drags particles towards the microtools which leads to
 221 their movement from the bottom to the top of the microcham-
 222 ber. Thermophoresis prevents the microspheres from getting
 223 into the immediate surroundings of the disk.

224 Figure 4 shows a schematic of the microsphere motion for
 225 the uncoated (a) and coated (b) microtools when the disk is
 226 actuated using the heating beam.

227 For characterizing particle motion, the MSDs were calcu-
 228 lated from the side-view recordings. A linear MSD versus time
 229 relation indicates that the particles are in Brownian motion
 230 [27–29], in which case the MSD at any given time is given
 231 by Einstein’s equation for Brownian motion in 2D:

$$\rho(t) = 4Dt, \tag{1}$$

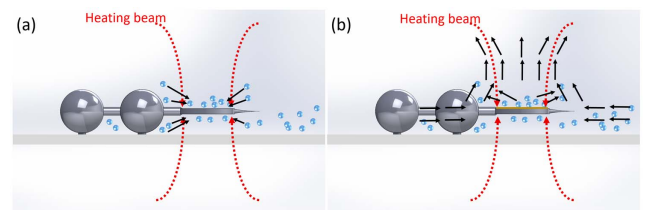
232 where $\rho(t)$ is the MSD, D is the diffusion coefficient, and t is
 233 the time. In the case of directed motion, the MSD increases
 234 faster with time, which manifests in a positive curvature in
 235 the MSD versus time plot. Thus, in the case of a directed
 236 trajectory, the particle MSD is given by [29]

$$\rho(t) = 4Dt + v^2t^2, \tag{2}$$

237 where v is the drift velocity, and the other parameters are the
 238 same as in Eq. (1).

239 Individual particle trajectories over a period of 40 s in the
 240 presence of an uncoated tool are shown in Fig. 5(a). From the
 241 linear fit of the average particle MSD versus time experimental
 242 data points, the diffusion coefficient was calculated to be
 243 $2.98 \pm 1.73 \mu\text{m}^2 \text{s}^{-1}$. The highly erratic individual particle
 244 trajectories and the linear increase of the average MSD with
 245 time [Fig. 5(c)] indicate that, in this case, the motion of the
 246 microspheres is highly associated to Brownian motion.
 247 Sedimentation due to gravity and convection induced by heat-
 248 ing the disk do not have a significant effect on particle motion
 249 in the bulk of the solution. While particles near the beams will
 250 tend to slowly move towards the disk due to the gradient force
 251 introduced by the heating beam, this does not lead to any col-
 252 lective movement of particles towards the microtool within the
 253 time period considered.

254 For the coated microtool, illumination of the disk led to
 255 natural convection characterized by the typical toroidal shape
 256 resembling that of Rayleigh–Bénard flow, as depicted in the
 257 particle trajectories shown in Fig. 5(b) and in the flow pattern
 258 shown in Fig. 5(d). The local increase in temperature leads to a



F4:1 **Fig. 4.** Schematic of microsphere movement after the heating beam
 F4:2 is turned on to illuminate the disk of (a) uncoated and (b) gold-coated
 F4:3 microtools.

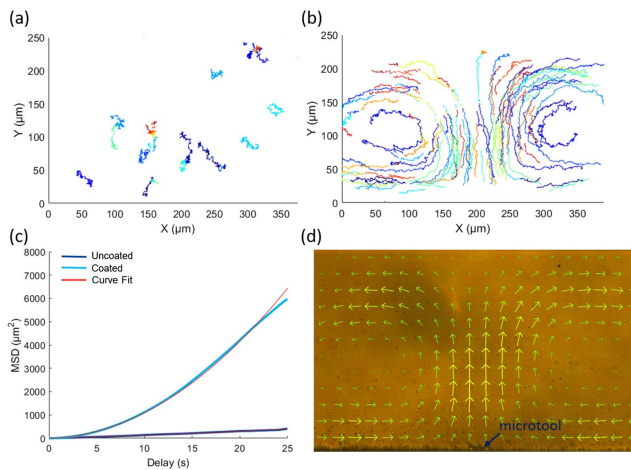


Fig. 5. Individual particle trajectories calculated from the side-view imaging in the presence of (a) uncoated and (b) gold-coated microtools for a duration of 40 s. (c) MSD comparison for coated and uncoated microtools. (d) Flow pattern in the measurement chamber generated by heating a gold-coated disk microtool.

decrease in the fluid density around the disk, which then generates natural convection currents. Distant microspheres outside the field of view were dragged by the fluid flow towards and away from the microtool radially and vertically. This “migration” cannot be associated with the gradient force of the optical traps alone, as demonstrated by the reference experiments using uncoated microtools. By fitting the MSD versus time curve according to Eq. (2), we calculated a diffusion coefficient of $2.74 \pm 0.11 \mu\text{m}^2 \text{s}^{-1}$, which is in good agreement with that of microspheres in the presence of the uncoated microtool. From the same fit, the average particle velocity was found to be $3.14 \pm 0.02 \mu\text{m s}^{-1}$. This average particle velocity is higher or comparable with previously reported results [26,30,31]. The convection pattern we obtained [Fig. 5(d)] is similar to the simulation results presented in Roxworthy *et al.* for an array of gold bowtie nanoantennas (BNAs) patterned on top of an indium-tin-oxide (ITO) layer [31]. However, in their case, the temperature increase was associated with the optical absorption of the ITO layer in NIR, while the BNAs merely had the role of enhancing the heat absorption of ITO. In our case, the temperature increase arises from the Joule effect on the gold nanolayers.

Microtools with gold-coated disks were successfully fabricated and employed for localized heating in a straight and closed microchannel. Spherical handles included as part of the microtool design enable optical trapping and manipulation of the microtools, which further facilitates precise actuation. By illuminating the disk with a laser beam, we demonstrate off-resonant plasmonic heating, which leads to natural convection in the system. Upon short-term illumination of the gold-coated disk (<2 s), nearby microspheres are immediately repelled due to the creation of thermophoretic gradients. Further heating of the disk induces a natural convective flow that spans several hundreds of micrometers. Illumination of similar microtools without gold coating on the disk does not lead to any significant motion in the system. This suggests that the natural convective flow observed can be attributed to the off-resonant plasmonic heating of the disk, rather than any other effects related to

the presence of the microtool or laser beam. To the best of our knowledge, this represents the first direct observation of natural convection induced by means of off-resonant plasmonic heating with the aid of a mobile heat source. This approach could prove valuable for understanding and controlling micro-mixing and material delivery in microfluidic devices.

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